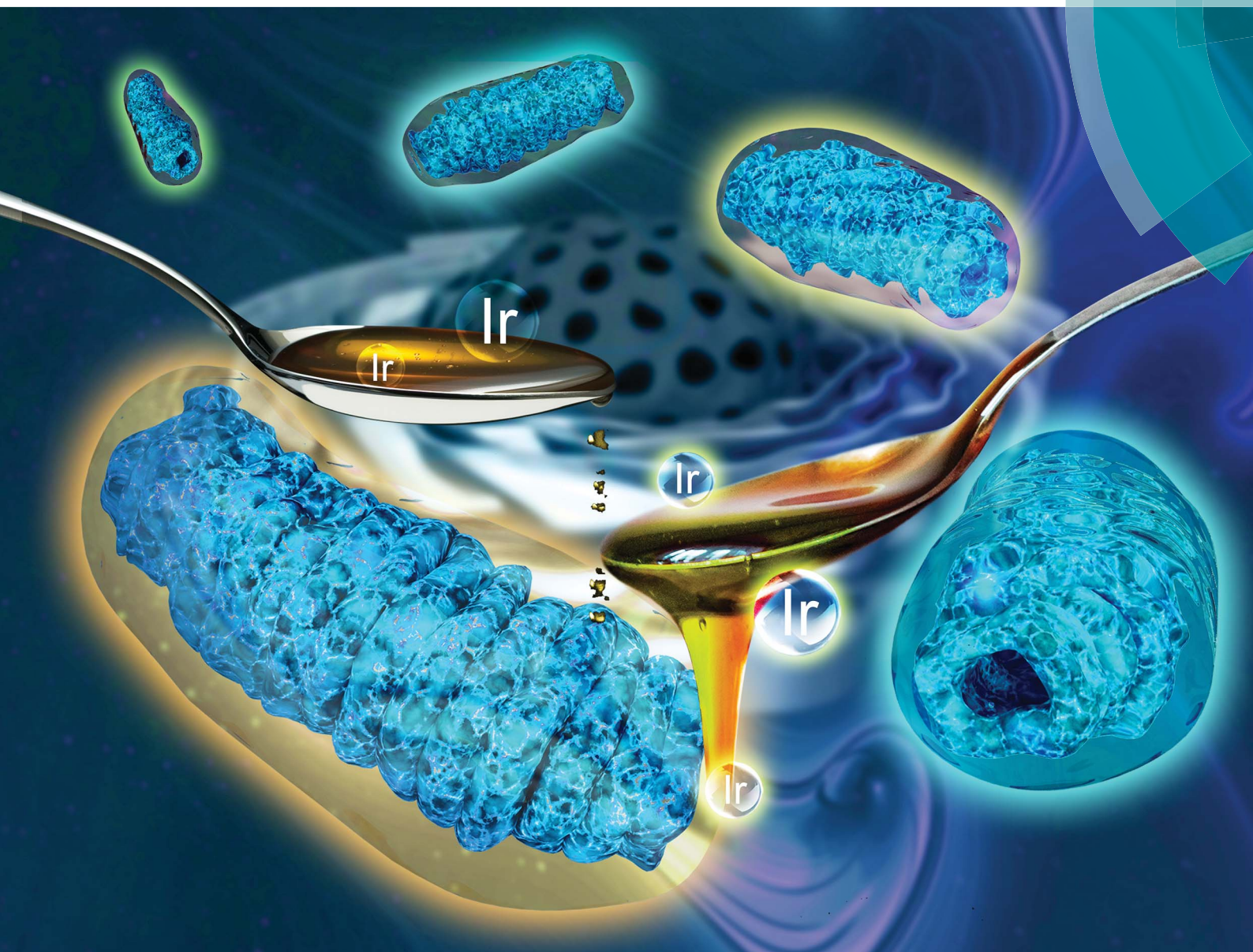


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Monitoring mitochondrial viscosity with anticancer phosphorescent Ir(III) complexes via two-photon lifetime imaging†

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Precise quantitative measurement of viscosity at the subcellular level presents great challenges. Two-photon phosphorescence lifetime imaging microscopy (TPPLIM) can reflect micro-environmental changes of a chromophore in a quantitative manner. Phosphorescent iridium complexes are potential TPPLIM probes due to their rich photophysical properties including environment-sensitive long-lifetime emission and high two-photon absorption (TPA) properties. In this work, a series of iridium(III) complexes containing rotatable groups are developed as mitochondria-targeting anticancer agents and quantitative viscosity probes. Among them, **Ir6** ($[\text{Ir}(\text{ppy-CHO})_2(\text{dppe})]\text{PF}_6$; ppy-CHO: 4-(2-pyridyl) benzaldehyde; dppe: *cis*-1,2-bis(diphenylphosphino)ethene) shows satisfactory TPA properties and long lifetimes (up to 1 μs). The emission intensities and lifetimes of **Ir6** are viscosity-dependent, which is mainly attributed to the configurational changes in the diphosphine ligand as proved by ^1H NMR spectra. **Ir6** displays potent cytotoxicity, and mechanism investigations show that it can accumulate in mitochondria and induce apoptotic cell death. Moreover, **Ir6** can induce mitochondrial dysfunction and monitor the changes in mitochondrial viscosity simultaneously in a real-time and quantitative manner via TPPLIM. Upon **Ir6** treatment, a time-dependent increase in viscosity and heterogeneity is observed along with the loss of membrane potential in mitochondria. In summary, our work shows that multifunctional phosphorescent metal complexes can induce and precisely detect microenvironmental changes simultaneously at the subcellular level using TPPLIM, which may deepen the understanding of the cell death mechanisms induced by these metalloc compounds.

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Introduction

Recently, organometallic iridium complexes have been reported to exhibit potent anticancer effects.¹ On the other hand, phosphorescent iridium complexes have been widely investigated for bioimaging and biosensing due to their superior photophysical properties, *e.g.*, high quantum yields, large Stokes shifts and long emission lifetimes.² Moreover, the phosphorescence of iridium complexes is reported to be sensitive to the environmental changes, such as oxygen,³ viscosity⁴ and pH.⁵ By careful structural tuning and molecular design, iridium complexes can locate in specific cell organelles to achieve bioimaging applications at the subcellular levels.⁶

The fluorescence lifetime of a fluorophore depends on its molecular environment but not concentration, and fluorescence lifetime imaging (FLIM) can reflect the alterations in microenvironments with high accuracy.⁷ In the FLIM technique, molecular rotors with viscosity-dependent lifetimes can map cellular viscosity quantitatively.^{8,9} Most of the FLIM probes have nanosecond lifetimes similar to cellular background autofluorescence (usually below 10 ns), which limits their contrast and sensitivity. Owing to their high spin-orbit coupling associated with the heavy metal ion, metal complexes are ideal candidates for phosphorescence lifetime imaging microscopy (PLIM) with emission lifetimes up to microseconds.^{10–12} The accuracy can be increased due to the expanded linear correlation scope and totally depleted background emission by imposing a time delay between excitation and detection.¹³ Moreover, two-photon phosphorescence lifetime imaging microscopy (TPPLIM) that uses excitation by the near-infrared (NIR) light with deep penetration depth offers the possibility of eliminating the background fluorescence effectively and reflects micro-environmental changes of the chromophore in a quantitative manner.^{10–12} On the other hand, anticancer fluorescent agents that can induce and monitor therapeutic effects

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in real-time have attracted much attention as they can avoid the interference between drugs and probes.¹⁴ These anticancer agents that can reflect the changes in the microenvironment of subcellular organelles are highly desirable as they can give more insight into the mechanism investigation.¹⁵

The mitochondrion is the energy factory and a key regulator of cell death signaling.¹⁶ Intracellular viscosity affects protein-protein interactions in cellular membranes,¹⁷ and it has been demonstrated to be associated with many diseases, *e.g.*, atherosclerosis,¹⁸ diabetes¹⁹ and Alzheimer's disease.²⁰ Furthermore, the viscosity in the mitochondrial matrix is closely related to mitochondrial network organization, mitochondrial respiration, metabolite diffusion and mitochondrial metabolism.^{17,21,22} Recently, some fluorescent molecular rotors featuring intramolecular rotational dynamics have been designed to sense intracellular viscosity. They usually have low quantum yields due to the internal rotation, while the fluorescence recovers as the viscosity increases and the rotation gets restricted.^{8,9,21–23} Quantitative measurement of viscosity can be achieved using ratio-metric viscosity monitors with both viscosity-dependent and -independent emissive bands.^{9,21} Moreover, viscosity probes for specific organelles are also accomplished by introducing targeting groups.^{22,24}

Subcellular viscosity probes with long lifetimes up to microseconds suitable for TPPLIM remain undeveloped. Iridium complexes containing phosphine ligands are widely explored as catalysts²⁵ and phosphorescent materials,^{26,27} while their bioimaging or therapeutic properties are barely revealed. In this work, we introduce rotational groups into the emissive iridium complexes that can aggregate in mitochondria due to their lipophilic and cationic characteristics. As these complexes possess viscosity-sensitive two-photon absorption (TPA) properties and long emission lifetimes, we anticipate that they can reflect the changes in the subcellular microenvironments more precisely when they are performing the anticancer functions. Herein, six phosphorescent cyclometalated Ir(III) complexes **Ir1–Ir6** with the general formula $[\text{Ir}(\text{C-N})_2(\text{P-P})]\text{PF}_6$ ($\text{C-N} = 2\text{-phenylpyridine}$ (**Ir1–Ir3**) or $4\text{-(2-pyridyl)benzaldehyde}$ (**Ir4–Ir6**); $\text{P-P} = \text{bis-(diphenylphosphino)methane}$ (L_1 in **Ir1** and **Ir4**), $\text{bis-(diphenylphosphino)ethane}$ (L_2 in **Ir2** and **Ir5**) or $\text{bis-(diphenylphosphino)ethylene}$ (L_3 in **Ir3** and **Ir6**); Fig. 1a) were developed as mitochondria-targeting anticancer viscosity probes. **Ir1–Ir6** contain diphosphine ligands with rotatable phenyl substitutions, and the cyclometalated ligands in **Ir4–Ir6** also contain a rotatable aldehyde group.^{9,28} Among them, **Ir6** displays high TPA properties and competent viscosity sensitivity. We demonstrate that **Ir6** can localize to mitochondria and induce mitochondrial dysfunction leading to apoptotic cell death. At the same time, **Ir6** can monitor the changes in mitochondrial viscosity quantitatively in a real-time manner using TPPLIM. We find that the viscosity of dysfunctional mitochondria is significantly increased in a heterogeneous fashion. In conclusion, our work demonstrates the potential of phosphorescent anticancer metallocompounds in inducing and accurately revealing microenvironmental changes at the subcellular levels.

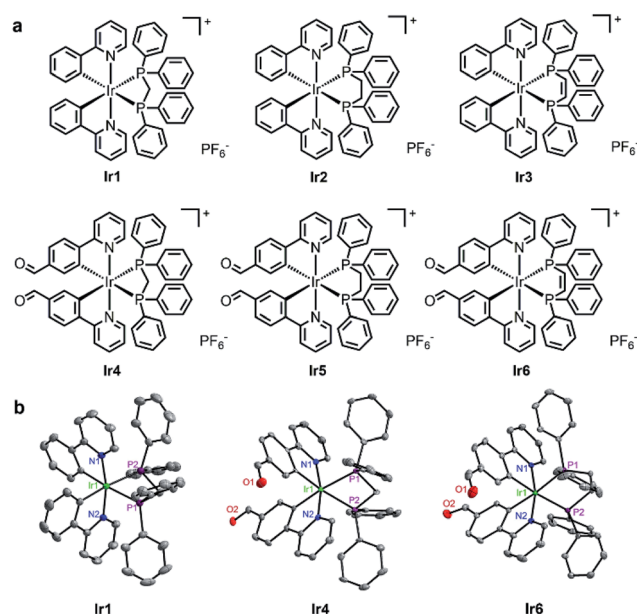


Fig. 1 (a) Chemical structures of **Ir1–Ir6**. (b) X-ray crystal structures of **Ir1**, **Ir4** and **Ir6** with thermal ellipsoids set at 30% probability. The H atoms, counterions, and solvent molecules are omitted for clarity.

Results and discussion

Synthesis and characterization

Ir1–Ir3 were synthesized using literature methods²⁷ and **Ir4–Ir6** were obtained similarly (Scheme S1†). Briefly, two equivalents of the bis-diphenylphosphine ligand and the corresponding cyclometalated Ir(III) dimer were refluxed in $\text{CH}_2\text{Cl}_2\text{--CH}_3\text{OH}$ for 6 h (**Ir1–Ir3**) or in dimethylformamide for 72 h (**Ir4–Ir6**), followed by anion exchange with NH_4PF_6 , purification by column chromatography and recrystallization. The complexes were characterized by ESI-MS (Fig. S1–S6†), ^1H NMR spectroscopy (Fig. S7–S12†) and elemental analysis. **Ir1–Ir6** were stable for at least 3 days as measured in a mixed solvent of dimethyl sulfoxide- d_6 ($\text{DMSO-}d_6$) and D_2O by ^1H NMR spectroscopy (Fig. S13†). **Ir1**, **Ir4** and **Ir6** were also characterized by X-ray crystal diffraction (Fig. 1b and Table S1†). The iridium centers in **Ir1**, **Ir4** and **Ir6** adopt a distorted octahedral geometry with the two nitrogen atoms of the C-N ligands being trans to each other. The two phosphorus atoms of the P-P ligand are trans to the carbon atoms of the C-N ligands.

In CH_2Cl_2 , CH_3CN and PBS at 298 K, **Ir1–Ir6** show intense absorption bands at 250–340 nm assigned to spin-allowed intraligand (^1IL) transitions and less intense absorption bands at 350–480 nm assigned to a mixture of spin-allowed and spin-forbidden metal-to-ligand charge transfer transitions ($^1\text{MLCT}/^3\text{MLCT}$) (Fig. S14†).²⁷ Upon excitation at 405 nm, **Ir1–Ir3** exhibit weak luminescence with the maxima at *ca.* 480 nm, which is consistent with literature reports.²⁷ When bulky aldehyde groups are introduced into the C-N ligands, **Ir4–Ir6** display much stronger emission at *ca.* 550 nm and longer lifetimes (up to 1 μs) compared with **Ir1–Ir3** (ESI, Table S3†).



Viscosity-sensitive emission properties

The emission responses of **Ir1–Ir6** to viscosity were measured in mixed methanol–glycerol solvents representing different viscosities. **Ir1–Ir6** exhibit viscosity-dependent phosphorescence intensities and lifetimes (Fig. 2a–c; S15 and S16†), which may be attributed to the rotatable aromatic rings on diphosphine ligands and aldehyde groups.^{9,28} The impact of viscosity on emission properties is more pronounced for **Ir4–Ir6** than that observed for **Ir1–Ir3**. For example, the maximum emission intensity of **Ir6** is enhanced by *ca.* 6.4-fold in 90% glycerol compared with that measured in methanol, which can be easily observed by the naked eye (Fig. 2a and b). The lifetime of **Ir6** increases from 0.54 μ s to 2.17 μ s as the viscosity increases from 0.55 cP (centipoise) to 259 cP. A linear correlation is obtained between the lifetimes ($\log \tau$) of **Ir6** and solvent viscosity parameters (Fig. 2c), and the linear detection range coincides with the range of cellular viscosities reported.^{9,21,22,24}

To elucidate the relationship between structural restriction and viscosity-responsive emission, we measured the temperature-dependent NMR spectra and emission (Fig. 2d–f and S17†). Interestingly, a linear correlation is obtained between the lifetime ($\log \tau$) of **Ir6** and temperature (K), which shows that restricting molecular rotation by reducing the temperature can increase the emission lifetime of **Ir6**. In NMR spectra, three kinds of H atoms are assigned on the dppe ligand: group i is from the C=C double bond, and groups ii and iii are on the benzene rings (Fig. 2d). From the ¹H NMR spectra measured at different temperatures, it can be seen that the chemical shifts as well as the shape and width of the peaks assigned to these H atoms have changed, which indicates that the chemical environments of these H atoms are affected by restricted rotation. Furthermore, the ¹H–¹H NOESY spectra indicate that the interactions between the H atoms of group ii/iii and group i become stronger as the temperature decreases, which implies that the distances between these H atoms are reduced at lower temperature. In summary, these results show that the viscosity-dependent emission of **Ir6** may partially be attributed to the alterations in molecular configurations under restricted environments.

In order to confirm the specificity of the emission response of complexes towards viscosity, we also tested the influence of other factors on the lifetime of **Ir6**. The lifetime of **Ir6** exhibits small response to polarity, solvent type, glutathione and human serum albumin (HSA), indicating its selectivity for viscosity (Fig. S18–S20†).

The two-photon absorption (TPA) cross-sections of **Ir6** were determined using rhodamine 6G as the reference (Table S3 and Fig. S21†).²⁹ The maximum TPA cross-section ($\delta_{\max}$, λ_{ex} = 750 nm) was measured to be 444 GM, which is comparable to the TPA cross-sections reported for other two-photon phosphorescent iridium probes.^{5,30–32}

Cytotoxicities, cellular uptake and localization

The *in vitro* cytotoxicities of **Ir1–Ir6** and cisplatin were evaluated in A549 (human lung adenocarcinoma), HeLa (human cervical carcinoma) and LO2 (human hepatic) cells after 48 h treatment

(Table S4†). Generally, the order of *in vitro* antiproliferative activity of the compounds can be considered as **Ir3** > **Ir1** > **Ir2** > **Ir6** > **Ir4** > **Ir5** > cisplatin.

Due to their intrinsic emission, we can observe the cellular uptake and localization of phosphorescent iridium complexes by confocal microscopy, which is closely related to their anti-cancer mechanisms. **Ir1–Ir3** with low quantum yields exhibit no obvious cellular emission, and the green phosphorescence of **Ir4–Ir6** is mainly maintained in the cytoplasm of A549 cells after 1 h incubation (Fig. S22†). Inductively coupled plasma mass spectrometry (ICP-MS) measurement shows that **Ir1–Ir6** tend to accumulate in the mitochondria of A549 cells (Fig. 3a).

As **Ir6** displays appropriate cytotoxicity and the best linear response to viscosity, we choose it as a model compound in the subsequent investigations.

A high colocalization is observed for **Ir6** and Mito-Tracker Deep Red (MTDR), which is consistent with the results obtained by ICP-MS. Moreover, the Pearson's colocalization coefficient obtained for **Ir6** with MTDR (0.93) is much higher than that obtained for **Ir6** with Lyso-Tracker Deep Red (LTDR, 0.28), which further confirms that **Ir6** can be used for specifically imaging mitochondria (Fig. 3b).

Induction of apoptotic cell death

Cell death can occur through various pathways (*e.g.*, apoptosis and necrosis) that are characterized by defined morphological alterations and biochemical hallmarks.³³ The cell death modes induced by **Ir6** were first investigated by morphological observations. Control cells exhibit normal morphology with a plump and homogeneous nuclear staining pattern (Fig. S23†). Cells treated with **Ir6** display typical morphological apoptotic characteristics including cell shrinkage, membrane blebbing, condensed chromatin, and brightly stained and fragmented nuclei.³⁴ Transmission electron microscopy (TEM) also shows that **Ir6**-treated cells exhibit typical apoptotic characteristics, such as hyperchromatin and vacuolar degeneration (Fig. 3c). From the TEM picture, we can also see that **Ir6**-treatment causes abnormal mitochondrial morphology. In the untreated cells, normal mitochondria show a normal tubular structure. In the cells treated with **Ir6**, the normal shape of mitochondria disappears and mitochondria with disrupted cristae can be observed.

The externalization of phosphatidylserine (PS) on the outer leaflet of the cells is an indication of early apoptosis.³⁵ Annexin V staining shows a concentration-dependent increase in the proportion of apoptotic cells in **Ir6**-treated cells, and apoptotic cells increase from $4.79 \pm 0.1\%$ to $38.0 \pm 1.4\%$ after **Ir6** (20 μ M, 24 h) treatment (Fig. S24†). Confocal microscopic observation also shows that after **Ir6** (5 μ M, 24 h) treatment, the proportions of cells at both early (annexin V-positive and propidium iodide (PI)-negative) and late (annexin V- and PI-positive) stages of apoptosis are increased significantly (Fig. S25†). Compared with the control cells, treatment of **Ir6** (10 μ M, 6 h) causes up to 2.4-fold increases in caspase-3/7 activity in A549 cells (Fig. S26†). These results indicate that **Ir6** induces caspase-mediated apoptotic cell death.



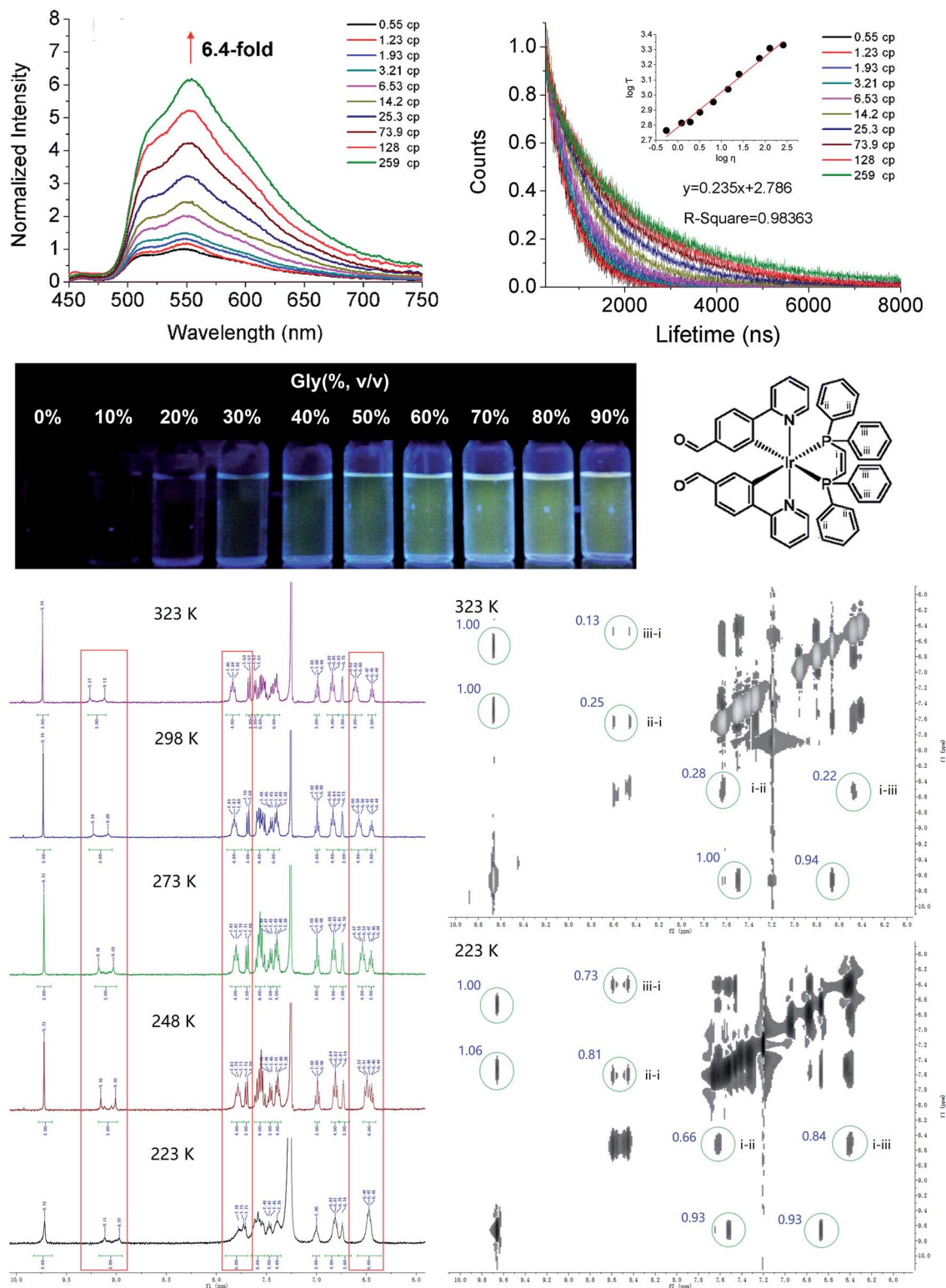


Fig. 2 (a and b) Emission intensity and (c) lifetime of **Ir6** (20 μM) in mixtures of CH_3OH and glycerol (percentage of glycerol = 0%, 10%, 20%, 30%, 40%, 50%, 60%, 70%, 80%, and 90%, v/v). The calculated viscosity parameters are indicated. $\lambda_{\text{ex}} = 405$ nm. (d) To analyze the temperature-dependent NMR spectra of **Ir6**, three kinds of H atoms are assigned on the dppe ligand: group (i) is from the C=C double bond, and groups (ii) and (iii) are on the benzene rings. (e) ^1H NMR spectra of **Ir6** in CDCl_3 at different temperatures. (f) ^1H - ^1H NOESY spectra of **Ir6** in CDCl_3 at different temperatures. The integrals of the peaks showing the interactions between (i) and (ii)/(iii) are marked in blue.



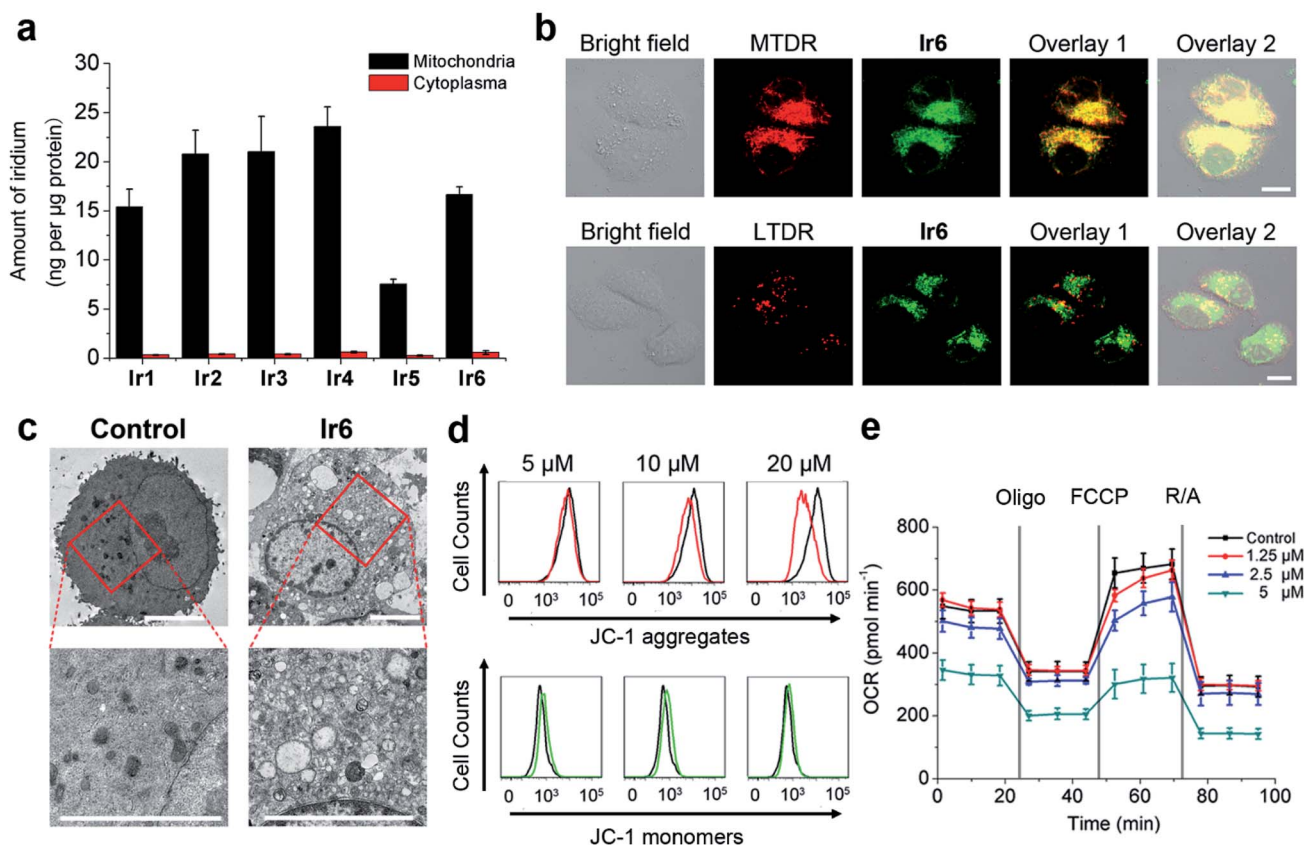


Fig. 3 (a) Detection of iridium in the extracts of A549 cells treated with Ir1–Ir6 (20 μM , 1 h). (b) Cellular colocalization microscopy image of A549 cells incubated with Ir6 (20 μM , 1 h) and MTDR/LTDR (200 nM, 30 min). $\lambda_{\text{ex}} = 405 \text{ nm}$ (Ir6)/633 nm (MTDR/LTDR); $\lambda_{\text{em}} = 550 \pm 20 \text{ nm}$ (Ir6)/665 $\pm 20 \text{ nm}$ (MTDR/LTDR). Overlay 1: overlay of the 2nd and 3rd columns. Overlay 2: overlay of the 1st and 4th columns. Scale bars: 10 μm . (c) TEM images of A549 cells incubated with Ir6 (20 μM , 24 h). The images in the lower panel are the enlarged images from the red boxes. Scale bars: 5 μm . (d) Representative result of MMP detection by JC-1 staining and flow cytometry. A549 cells were treated with Ir6 at indicated concentrations for 4 h. $\lambda_{\text{ex}} = 488 \text{ nm}$; $\lambda_{\text{em}} = 527 \pm 20 \text{ nm}$ (JC-1 monomers) and $590 \pm 20 \text{ nm}$ (JC-1 aggregates). The black and colored lines represent the control and Ir6-treated samples, respectively. (e) Respiratory profiles of A549 cells treated with Ir6 (3 h) under basal conditions, and after the addition of oligomycin (Oligo, 0.75 μM), trifluoromethoxy carbonylcyanide phenylhydrazide (FCCP, 1.0 μM) and rotenone/antimycin A (R/A, 0.5 μM each) measured by a Seahorse XF24 Extracellular Flux Analyzer.

To further investigate the cancer cell selectivity of Ir6, we compared the anticancer activities of Ir6 on human hepatoblastoma cells (HepG2) and LO2 cells from the same organ. A higher cytotoxicity of Ir6 is observed in HepG2 cells than in LO2 cells at all the doses tested (Fig. S27a†). Higher iridium levels are detected in mitochondria isolated from HepG2 cells than in mitochondria from LO2 cells, which may explain the higher cytotoxicity observed in HepG2 cells (Fig. S27b†). Furthermore, an about 1.7-fold increase in caspase-3/7 activity can be detected in HepG2 cells treated with Ir6 (10 μM) while caspase-3/7 activation is not so obvious in LO2 cells (Fig. S27c†).

Induction of mitochondrial dysfunction

As Ir6 could localize to mitochondria, we then investigated the impact of Ir6 on mitochondrial integrity. The mitochondrial membrane potential (MMP) can be measured by 5,5',6,6'-tetrachloro-1,1'-3,3'-tetraethyl-benzimidazolylcarbocyanine iodide (JC-1) staining. At high MMPs, JC-1 exists in its aggregate form and emits red fluorescence, while it exists as a monomer and emits green fluorescence at low MMPs.³⁶ Compared with the

control group, a collapse in MMPs is observed in Ir6-treated A549 cells as indicated by the decrease in the ratio of red/green fluorescence of JC-1 (Fig. 3d and S28†). Compared with the control group, Ir6-treated cells show a significant decrease in ATP levels as measured by the CellTiter-Glo® luminescent cell viability assay (Fig. S29†). Subsequently, we used the Seahorse XF24 extracellular flux analyzer to measure the oxygen consumption rate (OCR) which is indicative of the mitochondrial oxidative phosphorylation (OXPHOS) status.³⁷ Compared with the control cells, Ir6-treated cells display a decrease in basal respiration, ATP production and non-mitochondrial respiration, along with an increase in proton leak (Fig. 3e and S30†). These results indicate that Ir6-treatment can impair the energetic and metabolic status of mitochondria. Mitochondria are the main sites where cellular oxidative stress is produced, and defects in mitochondrial functionality often lead to the elevation of the level of ROS.³⁸

The ROS levels were evaluated using the 2',7'-dichlorodihydrofluorescein diacetate (DCFH-DA) assay. DCFH-DA is non-fluorescent but can be oxidized to the highly fluorescent 2',7'-



dichlorofluorescein (DCF) in the presence of ROS. An obvious concentration-dependent increase in fluorescence intensity of DCF can be detected in **Ir6**-treated cells (Fig. S31†). Compared with the control cells, a *ca.* 34.9-fold increase in the mean fluorescence intensity (MFI) of DCF is observed in A549 cells treated with **Ir6** (20 μ M, 6 h). Moreover, the fluorescence of DCF colocalizes well with that of the mitochondria-specific dye MTDR, which indicates that ROS are mainly generated in mitochondria (Fig. S32†). These results collectively indicate that **Ir6** can cause mitochondrial dysfunction and a massive production of ROS.

Tracking of mitochondrial viscosity *via* TPPLIM

As previous experiments show, **Ir6** can cause mitochondrial dysfunction, and a linear response relationship exists between its lifetime and environmental viscosity. We then use TPPLIM to track the dynamic changes in mitochondrial viscosity and investigate its correlation with mitochondrial physiological status. A time-dependent increase in the integrated phosphorescence lifetime is observed in **Ir6**-treated A549 cells in 4 h (Fig. 4a). As **Ir6** can image mitochondrial viscosity, it can be

applied to track the changes in mitochondrial viscosity in real time.

The average lifetime increases from about 1410 ns to 1792 ns and the viscosity of mitochondria is calculated to be varying from about 35 cP to 100 cP, which is consistent with the viscosity parameters reported in the literature.²² Under the same conditions, the collapse in MMP in **Ir6**-treated A549 cells is also detected with JC-1 staining. The fluorescence ratio (green/red) is calculated to increase from 0.45 to 0.95, indicating the loss of MMP (Fig. 4c). Interestingly, with the extension of incubation time, the decrease in the red/green fluorescence ratios of JC-1 and the increase in the calculated viscosity value show the same trend, which indicates that the changes in viscosity parameters can reflect the mitochondrial physiological status (Fig. 4d). The emission intensity and lifetime of **Ir6** in A549 cells were also recorded by confocal microscopy in a real-time manner. As the incubation time increases, an obvious increase in the emission intensity and lifetime of **Ir6** can be observed (Movie S1†).

It is known that the responses of different mitochondria in a cell to external stimuli are different, but the detection methods for mitochondrial heterogeneity are limited.^{39,40} We

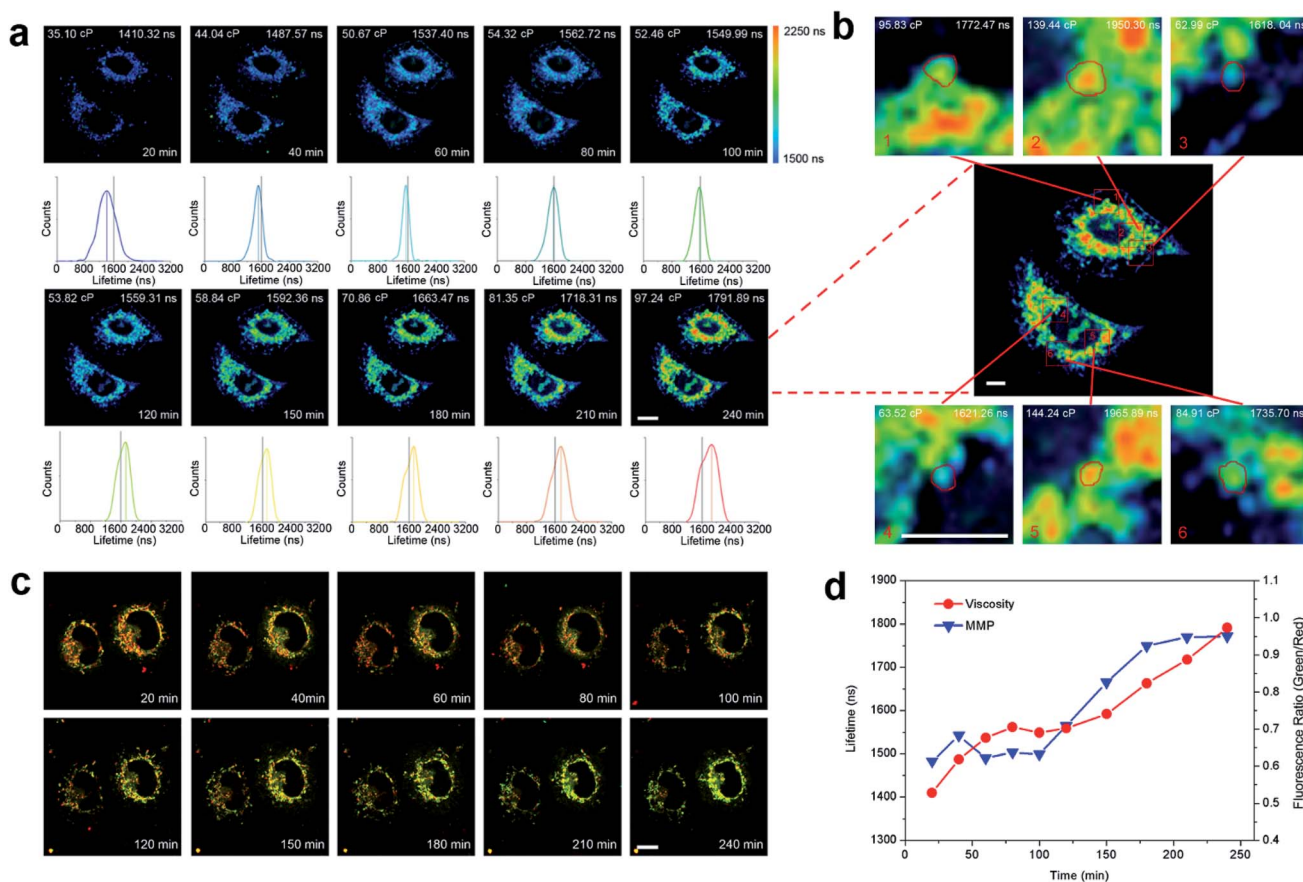


Fig. 4 (a) Mitochondrial viscosity in **Ir6**-treated A549 cells detected by TPPLIM. The cells were treated with **Ir6** (20 μ M) and subjected to imaging at different time intervals. (b) Determination of mitochondrial heterogeneity. A549 cells were treated with **Ir6** (20 μ M) for 4 h. The enlarged images are from the red boxes. The lifetime and viscosity are calculated from the spots in the red circle. $\lambda_{\text{ex}} = 750$ nm (**Ir6**); $\lambda_{\text{em}} = 550 \pm 20$ nm (**Ir6**). (c) Confocal microscopy image of JC-1 in **Ir6**-treated A549 cells. $\lambda_{\text{ex}} = 488$ nm; $\lambda_{\text{em}} = 530 \pm 20$ nm (JC-1 monomers)/ 590 ± 20 nm (JC-1 aggregates). (d) Calculated lifetimes of **Ir6** and fluorescence ratio of JC-1 (green)/JC-aggregates (red). Scale bars: 10 μ m (a and c)/5 μ m (b).



integrated the emission lifetimes of different spots in the cell and calculated the corresponding viscosity values. It can be seen that the lifetimes of different spots vary from 1618 ns to 1966 ns and the corresponding viscosity values range from *ca.* 63 cP to *ca.* 144 cP (Fig. 4b). The results show that TPPLIM can provide a relatively accurate quantitative method to detect mitochondrial heterogeneity.

In vivo imaging of zebrafish

Two-photon excitation imaging is attractive for *in vivo* applications due to the penetrability of the long wavelength photo source. Thus, we investigated the *in vivo* imaging capability of **Ir6** using zebrafish larvae. **Ir6** can effectively image zebrafish under both one- and two-photon excitation (Fig. S33†). Besides, the phosphorescence lifetimes reveal varied viscosities in different tissues of zebrafish larvae (Fig. S34†). The surface of the eyes and torso exhibits a shorter lifetime (*ca.* 500 ns). The interior of the eyes, head and spine shows a longer lifetime (*ca.* 1300 ns). The result demonstrates that **Ir6** has potential for application in TPPLIM *in vivo*.

Conclusions

In this work, we designed six cyclometalated Ir(III) complexes containing diphosphine ligands as mitochondria-targeting anticancer agents. Among them, the lifetime of the **Ir6** complex exhibits a specific response to the environmental viscosity and **Ir6** has potent TPA properties. **Ir6** can effectively accumulate in mitochondria and specifically label mitochondria. Moreover, **Ir6** can induce apoptosis mediated by caspase activation. As expected, **Ir6** can impair the energetic/metabolic status of mitochondria and cause massive production of mitochondrial ROS. Owing to its viscosity-responsive phosphorescence lifetimes, **Ir6** is capable of monitoring the changes in mitochondrial viscosity using TPPLIM in real-time. At the same time, the heterogeneity of mitochondria can be detected during the process of damage using TPPLIM. In conclusion, our work provides a new clue for the design of small molecule-based anticancer agents that can induce and monitor therapeutic effects by quantitative detection of microenvironmental changes at the subcellular level.

Experimental section

Synthetic protocol and characterization

[Ir₂(ppy)₄Cl₂] and [Ir₂(ppy-CHO)₄Cl₂]. These compounds were synthesized using literature methods.⁴¹ Briefly, IrCl₃·3H₂O (1.00 g, 2.84 mmol) and ppy (0.967 g, 6.25 mmol) or ppy-CHO (1.145 g, 6.25 mmol) were refluxed in 2-ethoxyethanol (100 mL) for 18 h. After cooling to room temperature and filtration, the residue was washed with methanol and ether. [Ir₂(ppy)₄Cl₂] and [Ir₂(ppy-CHO)₄Cl₂] were obtained as yellow and orange solids, respectively.

[Ir(ppy)₂L₁](PF₆) (Ir1**)**. **Ir1** was synthesized by reacting [Ir₂(ppy)₄Cl₂] (0.200 g, 0.186 mmol) with **L₁** (0.157 g, 0.410 mmol) according to literature methods.²⁷ Yield: 0.299 g

(78%). ¹H NMR (400 MHz, *d*₆-DMSO) δ 8.11–8.02 (m, 4H; H1, 5, 16, 20), 7.89 (d, *J* = 7.7 Hz, 2H; H28, 29), 7.74 (dd, *J* = 15.3, 7.6 Hz, 6H; H24, 17–19), 7.57 (t, *J* = 7.2 Hz, 6H; H7–9, 12–14), 7.13 (t, *J* = 7.3 Hz, 2H; H26, 31), 7.06 (t, *J* = 7.4 Hz, 2H; H23, 34), 6.98 (t, *J* = 7.5 Hz, 6H; H21, 25, 32, 36, 24, 33), 6.87 (t, *J* = 8.5 Hz, 4H; H6, 10, 11, 15), 6.62 (t, *J* = 6.6 Hz, 2H; H22, 35), 6.30 (d, *J* = 5.0 Hz, 2H; H27, 30), 5.94 (t, *J* = 9.9 Hz, 2H; H37). ESI-MS (CH₃OH): *m/z* calcd for [M – PF₆]⁺, 885.22; found: 885.3. Elemental analysis calcd (%) for C₄₇H₃₈IrN₂P₃F₆·H₂O: C, 53.87; H, 3.85; N, 2.67; found: C, 53.93; H, 3.78; N, 2.63.

[Ir(ppy)₂L₂](PF₆) (Ir2**)**. **Ir2** was synthesized by reacting [Ir₂(ppy)₄Cl₂] (0.200 g, 0.186 mmol) with **L₂** (0.163 g, 0.410 mmol) according to literature methods.²⁷ Yield: 0.249 g (64%). ¹H NMR (400 MHz, *d*₆-DMSO) δ 7.94 (d, *J* = 8.2 Hz, 2H; H1, 20), 7.85 (d, *J* = 7.7 Hz, 2H; H5, 16), 7.73 (dd, *J* = 15.6, 7.0 Hz, 6H; H2–4, 17–19), 7.64 (t, *J* = 7.7 Hz, 2H; H28, 29), 7.47 (t, *J* = 7.3 Hz, 2H; H8, 13), 7.36 (t, *J* = 7.3 Hz, 4H; H7, 9, 12, 14), 7.05 (t, *J* = 7.4 Hz, 4H; H23, 26, 31, 34), 6.96 (t, *J* = 7.3 Hz, 2H; H24, 33), 6.90 (t, *J* = 7.4 Hz, 4H; H21, 25, 32, 36), 6.64 (t, *J* = 8.4 Hz, 4H; H6, 10, 11, 15), 6.47 (t, *J* = 6.6 Hz, 2H; H22, 35), 6.22 (d, *J* = 4.6 Hz, 2H; H27, 30), 3.92 (dt, *J* = 23.3, 12.6 Hz, 2H; H37, 38), 2.92 (d, *J* = 9.3 Hz, 2H; H37, 38). ESI-MS (CH₃OH): *m/z* calcd for [M – PF₆]⁺, 899.23; found: 899.3. Elemental analysis calcd (%) for C₄₈H₄₀IrN₂P₃F₆: C, 55.22; H, 3.86; N, 2.68; found: C, 54.97; H, 3.79; N, 2.59.

[Ir(ppy)₂L₃](PF₆) (Ir3**)**. **Ir3** was synthesized by reacting [Ir₂(ppy)₄Cl₂] (0.200 g, 0.186 mmol) with **L₃** (0.162 g, 0.410 mmol) according to literature methods.²⁷ Yield: 0.279 g (72%). ¹H NMR (400 MHz, *d*₆-DMSO) δ 8.97–8.76 (m, 2H; H37, 38), 7.85 (dd, *J* = 16.3, 8.2 Hz, 6H; H1, 5, 16, 20), 7.78 (d, *J* = 7.7 Hz, 2H; H3, 18), 7.59 (dd, *J* = 12.9, 7.1 Hz, 4H; H4, 28, 29, 17), 7.50 (t, *J* = 7.3 Hz, 4H; H7, 9, 12, 14), 7.42 (d, *J* = 5.8 Hz, 2H; H8, 13), 7.07 (dd, *J* = 13.3, 6.9 Hz, 4H; H23, 26, 31, 34), 6.99 (t, *J* = 7.3 Hz, 2H; H24, 33), 6.90 (t, *J* = 7.1 Hz, 4H; H21, 25, 32, 36), 6.64–6.29 (m, 6H; H6, 10, 11, 15, 2, 19), 6.20 (dd, *J* = 7.1, 2.1 Hz, 2H; H27, 30). ESI-MS (CH₃OH): *m/z* calcd for [M – PF₆]⁺, 897.22; found: 897.3. Elemental analysis calcd (%) for C₄₈H₃₈IrN₂P₃F₆: C, 55.33; H, 3.68; N, 2.68; found: C, 54.96; H, 3.62; N, 2.64.

[Ir(ppy-CHO)₂L₁](PF₆) (Ir4**)**. [Ir₂(ppy-CHO)₄Cl₂] (0.200 g, 0.168 mmol) and **L₁** (0.143 g, 0.372 mmol) were refluxed in dimethyl formamide for 72 h. After cooling to room temperature, the solution was evaporated to 5 mL under reduced pressure before being instilled into saturated aqueous solution of NH₄PF₆. The resulting turbid liquid was filtered to obtain light yellow solids. The crude product was purified by column chromatography on silica gel (CH₂Cl₂ : CH₃OH = 99 : 1, v/v) and recrystallized by diffusion of diethyl ether into acetonitrile. The final product was obtained as yellow crystals. Yield: 0.274 g (75%). ¹H NMR (400 MHz, *d*₆-DMSO) δ 9.74 (s, 2H; H27, 30), 8.24 (d, *J* = 8.1 Hz, 2H; H28, 29), 8.15 (dd, *J* = 9.1, 7.5 Hz, 4H; H1, 5, 16, 20), 7.89 (t, *J* = 7.7 Hz, 2H; H3, 18), 7.70 (t, *J* = 8.5 Hz, 4H; H2, 4, 11, 19), 7.65–7.50 (m, 8H; H7–9, 12–14, 26, 31), 7.15 (t, *J* = 7.3 Hz, 2H), 6.99 (t, *J* = 7.0 Hz, 4H), 6.84 (dt, *J* = 13.5, 7.9 Hz, 6H), 6.77 (d, *J* = 2.5 Hz, 2H), 6.05 (t, *J* = 10.1 Hz, 2H). ESI-MS (CH₃OH): *m/z* calcd for [M – PF₆]⁺, 941.20; [M – PF₆ + CH₃OH]⁺, 973.23; [M – PF₆ + 2CH₃OH]⁺, 1005.26; found: 941.3,

973.3, 1005.3. Elemental analysis calcd (%) for $C_{49}H_{38}IrN_2O_2 \cdot P_3F_6$: C, 53.73; H, 3.53; N, 2.58; found: C, 53.96; H, 3.50; N, 2.51.

[Ir(ppy-CHO)₂L₂](PF₆) (Ir5). Ir5 was synthesized adopting a similar procedure to that described for Ir4 by using L₂ instead of L₁ as the ligand. Yield: 0.225 g (61%). ¹H NMR (400 MHz, *d*₆-DMSO) δ 9.74 (s, 2H; H27, 30), 8.17–8.07 (m, 4H; H1, 5, 16, 20), 7.80 (dd, *J* = 13.6, 6.6 Hz, 4H; H3, 18, 26, 31), 7.68 (t, *J* = 8.6 Hz, 4H; H2, 4, 17, 19), 7.58 (d, *J* = 7.9 Hz, 2H; H28, 29), 7.46 (t, *J* = 7.4 Hz, 2H; H7, 13), 7.31 (t, *J* = 7.1 Hz, 4H; H6, 8, 12, 14), 7.07 (t, *J* = 7.3 Hz, 2H; H23, 34), 6.91 (t, *J* = 7.0 Hz, 4H; H21, 25, 32, 36), 6.72 (d, *J* = 2.8 Hz, 2H; 24, 33), 6.69–6.56 (m, 6H; H6, 10, 11, 15, 22, 35), 3.98 (dd, *J* = 30.1, 10.1 Hz, 2H; H37, 38), 3.02 (d, *J* = 9.2 Hz, 2H; H37, 38). ESI-MS (CH₃OH): *m/z* calcd for [M – PF₆]⁺, 955.22; [M – PF₆ + CH₃OH]⁺, 987.25; [M – PF₆ + 2CH₃OH]⁺, 1019.27; found: 955.3, 987.3, 1019.3. Elemental analysis calcd (%) for $C_{50}H_{40}IrN_2O_2P_3F_6 \cdot 3H_2O$: C, 54.59; H, 3.67; N, 2.55; found: C, 54.37; H, 3.93; N, 2.46.

[Ir(ppy-CHO)₂L₃](PF₆) (Ir6). Ir6 was synthesized adopting a similar procedure to that described for Ir4 by using L₃ instead of L₁ as the ligand. Yield: 0.247 g (67%). ¹H NMR (400 MHz, *d*₆-DMSO) δ 9.75 (s, 2H; H27, 30), 8.98–8.82 (m, 2H; H37, 38), 8.03 (t, *J* = 7.2 Hz, 4H; H1, 5, 16, 20), 7.78 (dt, *J* = 15.5, 8.1 Hz, 6H; H2–4, 17–19), 7.59 (t, *J* = 8.2 Hz, 4H; H26, 28, 29, 31), 7.48 (dd, *J* = 10.6, 5.8 Hz, 6H; H7–9, 12–14), 7.11 (t, *J* = 7.4 Hz, 2H; H23, 34), 6.92 (t, *J* = 7.1 Hz, 4H; H21, 25, 32, 36), 6.70–6.60 (m, 4H; H22, 24, 33, 35), 6.48 (t, *J* = 8.6 Hz, 4H; H6, 10, 11, 15). ESI-MS (CH₃OH): *m/z* calcd for [M – PF₆]⁺, 953.20; [M – PF₆ + CH₃OH]⁺, 985.23; [M – PF₆ + 2CH₃OH]⁺, 1017.26; found: 953.3, 985.3, 1017.4. Elemental analysis calcd (%) for $C_{50}H_{38}IrN_2O_2P_3F_6$: C, 54.70; H, 3.49; N, 2.55; found: C, 54.26; H, 3.38; N, 2.47.

Real-time tracking of mitochondria by TPPLIM

A549 cells were seeded in 35 mm culture dishes (Corning) and incubated for 24 h. The growth medium was replaced by PBS with Ir6 (20 μ M) and DMSO (1%, v/v) before visualization by confocal microscopy. The confocal microscope is connected to an incubator that provides a constant temperature (37 °C) and CO₂ (5%). The luminescence intensity and phosphorescence lifetime of Ir6 under two-photon excitation were collected, respectively. The phosphorescence lifetime value is given by Becker & Hickl SPCImage. λ_{ex} = 750 nm (TPM); λ_{em} = 550 $\pm$ 20 nm.

Conflicts of interest

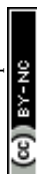
The authors declare no conflict of interest.

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