



Cite this: *Chem. Commun.*, 2016, 52, 5884

Received 14th January 2016,
Accepted 29th March 2016

DOI: 10.1039/c6cc00353b

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An ultrasensitive and incubation-free electrochemical immunosensor using a gold-nanocatalyst label mediating outer-sphere-reaction-philic and inner-sphere-reaction-philic species†

Chiew San Fang,^a Kyung Hwan Oh,^a Aram Oh,^b Kwangyeol Lee,^b Seonhwa Park,^a Sinyoung Kim,^c Jin Kyoong Park^a and Haesik Yang^{*a}

This communication reports a new nanocatalytic scheme based on the facts that the redox reaction between a highly outer-sphere-reaction-philic (OSR-philic) species and a highly inner-sphere-reaction-philic (ISR-philic) species is slow and that an OSR- and ISR-philic Au-nanocatalyst label can mediate the two different types of redox species. This scheme allows highly sensitive and incubation free detection of creatine kinase-MB.

The direct electron transfer between an electrode and a redox species occurs within a few nanometers. This fundamental principle has been widely harnessed to design simple and sensitive electrochemical biosensors.^{1–3} For example, specific binding of a target (bio)molecule can induce the close approach of a redox label to an electrode along with a conformational change of the redox label-conjugated probe molecule, which in turn allows the direct transfer of electrons, and thereby a high electrochemical signal can be obtained.^{4,5} However, it is not easy to apply this principle to common sandwich-type biosensors, particularly when the biosensing layer that exists between an electrode and a redox label is not thin enough for direct electron transfer to occur. In the case of redox nanoparticle or catalytic nanoparticle (nanocatalyst) labels, the additional layers (on the labels) that are required to immobilize probe molecules and to minimize the aggregation of the nanoparticle labels make direct electron transfer less feasible.⁶

Instead of direct electron transfer, one way to obtain fast electron transfer between an electrode and a redox label is to employ an electron mediator that could shuttle electrons between them.⁷ When a redox enzyme is used as a redox label in a sandwich-type immunosensor, an electron mediator can efficiently shuttle electrons and allow fast enzymatic reactions to occur provided that a

redox enzyme label is specifically bound to an immunosensing electrode within a few tens of nanometers.^{8–10} Contrary to the case of redox enzymes, the mediated electron transfer between a metal nanocatalyst label and an electrode has rarely been investigated. Importantly, it is not easy to simultaneously obtain both a fast redox reaction between an electron mediator and a substrate in the presence of a metal nanocatalyst label and *vice versa*, especially when the difference between their formal potentials is large.

To obtain a high electrochemical signal-to-background ratio in a biosensor using mediated electron transfer between a nanocatalyst label and an electrode, the following requirements need to be met: (i) the electron mediator should undergo a fast electrochemical reaction at the electrode and a fast catalytic reaction on the nanocatalyst, (ii) the electrochemical reaction of the substrate for the catalytic reaction should be very slow at the electrode, and (iii) the direct reaction (electron transfer) between the electron mediator and the substrate should be very slow, even though the difference in the formal potential between the mediator and the substrate is large.

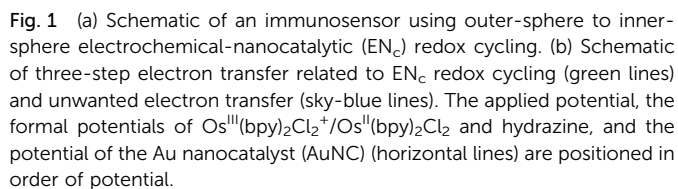
Redox reactions of inorganic complexes are classified into outer-sphere reactions and inner-sphere reactions,¹¹ and this classification can be extended to redox reactions between an organic electron donor and an acceptor¹² and redox reactions at electrodes.¹³ Furthermore, the authors previously reported that redox species can be classified into species that undergo outer-sphere reactions (OSR-philic species) and species that undergo inner-sphere reactions (ISR-philic species).^{14,15} Electron mediators such as ferrocene, $\text{Fe}(\text{CN})_6^{3-}$, the Ru complex, and the Os complex that undergo fast outer-sphere reactions are highly OSR-philic.¹⁶ In many cases, the redox reaction between a highly OSR-philic species and a highly ISR-philic species is slow, even though the formal potentials of the two redox species are quite different. For example, the redox reaction between OSR-philic $\text{Ru}(\text{NH}_3)_6^{3+}$ and ISR-philic tris(2-carboxyethyl)phosphine is slow.¹⁴ Nevertheless, the slow reaction can be accelerated by OSR- and ISR-philic species such as 4-aminophenol: the indirect redox reaction between $\text{Ru}(\text{NH}_3)_6^{3+}$ and tris(2-carboxyethyl)phosphine readily occurs *via* electron mediation of 4-aminophenol.¹⁴ Most inner-sphere reactions are slow at indium-tin oxide (ITO) electrodes,¹⁷ but many of them are fast at

^a Department of Chemistry and Chemistry Institute for Functional Materials, Pusan National University, Busan 46241, Korea. E-mail: hyang@pusan.ac.kr; Fax: +82 51 516 7421; Tel: +82 51 510 3681

^b Department of Chemistry, Korea University, Seoul 02841, Korea

^c Department of Laboratory Medicine, Yonsei University College of Medicine, Seoul 03722, Korea

† Electronic supplementary information (ESI) available: Experimental details and more supporting data. See DOI: 10.1039/c6cc00353b



Herein, we report an ultrasensitive, incubation-free electrochemical immunosensor using the outer-sphere to inner-sphere redox cycling that involves an ITO electrode, an electron mediator, an AuNC label, and a strong reductant. Four OSR-philic electron mediators [$\text{Ru}(\text{NH}_3)_6^{3+}$, $\text{Os}(\text{bpy})_2\text{Cl}_2^+$, ferrocenemethanol (FcMeOH), and $\text{Fe}(\text{CN})_6^{3-}$] were tested and compared in terms of high signal-to-background ratios. $\text{Os}(\text{bpy})_2\text{Cl}_2^+$ was chosen as the optimum electron mediator, and hydrazine, a strong reductant, was used as a substrate for a fast catalytic reaction on AuNC. Electrochemical measurement conditions, including applied potential, concentration of $\text{Os}(\text{bpy})_2\text{Cl}_2^+$, and concentration of hydrazine, were optimized. These optimum conditions were applied to a sandwich-type immunosensor for the detection of creatine kinase-MB (CK-MB).^{18–28}

Fig. 2a shows cyclic voltammograms of the four OSR-philic metal complexes obtained at ITO electrodes in phosphate-buffered saline (PBS). The voltammograms show near-reversible behavior, even at low electrocatalytic ITO electrodes, indicating that electrochemical oxidation and reduction of the metal complexes are fast. The formal potential increases in the sequence of $\text{Ru}(\text{NH}_3)_6^{3+}/\text{Ru}(\text{NH}_3)_6^{2+}$, $\text{Os}(\text{bpy})_2\text{Cl}_2^+/\text{Os}(\text{bpy})_2\text{Cl}_2$, $\text{Fe}(\text{CN})_6^{3-}/\text{Fe}(\text{CN})_6^{4-}$, and $\text{FcMeOH}^+/\text{FcMeOH}$. Fig. 2b represents cyclic voltammograms of the four complexes obtained in the presence of hydrazine at AuNC-modified ITO electrodes. In the case of $\text{Os}(\text{bpy})_2\text{Cl}_2$, highly increased oxidation currents were observed above 0.0 V (curve (ii) of Fig. 2b). The sigmoidal behavior is due to the electrochemical-nanocatalytic (EN_c) redox cycling involving

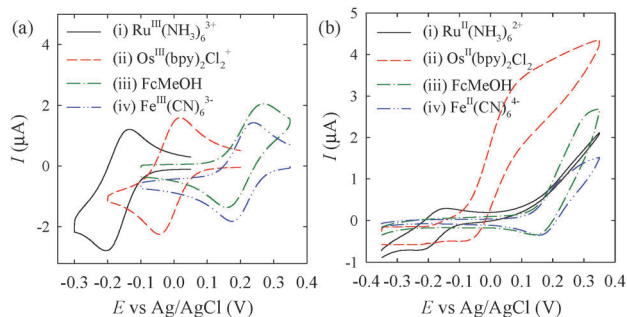


Fig. 2 (a and b) Cyclic voltammograms recorded (at a scan rate of 20 mV s^{-1}) using (a) bare ITO electrodes in PBS (pH 7.4) containing $100 \mu\text{M}$ (i) $\text{Ru}^{\text{III}}(\text{NH}_3)_6^{3+}$, (ii) $\text{Os}^{\text{III}}(\text{bpy})_2\text{Cl}_2^+$, (iii) ferrocenemethanol (FcMeOH), and (iv) $\text{Fe}^{\text{III}}(\text{CN})_6^{3-}$ and (b) ITO electrodes modified with adsorbed AuNC, in PBS (pH 7.4) containing 1.0 mM hydrazine and $100 \mu\text{M}$ (i) $\text{Ru}^{\text{III}}(\text{NH}_3)_6^{3+}$, (ii) $\text{Os}^{\text{III}}(\text{bpy})_2\text{Cl}_2^+$, (iii) FcMeOH, and (iv) $\text{Fe}^{\text{III}}(\text{CN})_6^{4-}$.

the ITO electrode, $\text{Os}(\text{bpy})_2\text{Cl}_2^+/\text{Os}(\text{bpy})_2\text{Cl}_2$, AuNC, and hydrazine (Fig. 1a). Three-step electron transfer from hydrazine to the ITO electrode occurs (Fig. 1b) during the EN_c redox cycling because AuNCs are OSR- and ISR-philic species. On the other hand, the current increase caused by $\text{Ru}(\text{NH}_3)_6^{2+}$ was observed at potentials much higher than its formal potential (curve (i) of Fig. 2b). Current increases caused by FcMeOH and $\text{Fe}(\text{CN})_6^{4-}$ (curves (iii) and (iv) of Fig. 2b) were also observed, but the increase occurred at potentials much higher than that of $\text{Os}(\text{bpy})_2\text{Cl}_2$ (curve (ii) of Fig. 2b). To compare the signal-to-background ratios, chronocoulometric data were obtained at 0.16 V in the presence of electron mediators and hydrazine (for measuring background levels) and in the presence of the electron mediator, hydrazine, and adsorbed AuNC (for measuring signal levels) (Fig. S2 of the ESI†). The signal-to-background ratio of $\text{Os}(\text{bpy})_2\text{Cl}_2^+$ (624) was the highest among the four metal complexes. Thus, $\text{Os}(\text{bpy})_2\text{Cl}_2^+$ was finally selected as the electron mediator.

To investigate the background level in more detail, more cyclic voltammograms and chronocoulograms were obtained and compared (Fig. 3a and c). In the cyclic voltammogram obtained in a solution of hydrazine (curve (i) of Fig. 3a), capacitive currents were mainly observed. The voltammogram obtained in a solution of $\text{Os}(\text{bpy})_2\text{Cl}_2$ (curve (ii) of Fig. 3a) was similar to that obtained in a solution of $\text{Os}(\text{bpy})_2\text{Cl}_2$ and hydrazine (curve (iii) of Fig. 3a). The chronocoulometric signal obtained in a solution of hydrazine (curve (vi) of Fig. 3c) was somewhat higher than that of $\text{Os}(\text{bpy})_2\text{Cl}_2^+$ (curve (vii) of Fig. 3c) and lower than that of $\text{Os}(\text{bpy})_2\text{Cl}_2^+$ and hydrazine (curve (viii) of Fig. 3c). However, these chronocoulometric signals were much lower than the chronocoulometric signal obtained in the presence of AuNC (Fig. 3d), indicating that the electrochemical oxidation of hydrazine was very slow at the ITO electrode and that the direct redox reaction between $\text{Os}(\text{bpy})_2\text{Cl}_2^+$ and hydrazine was also slow. The chronocoulometric signal obtained in a solution of hydrazine in the presence of AuNC (curve (xi) of Fig. 3d) was much higher than that obtained in the absence of AuNC (curve (vi) of Fig. 3c). This indicates that hydrazine is oxidized at AuNC more easily than at the ITO electrode. It is interesting to note that the chronocoulometric signal obtained in a solution of hydrazine and $\text{Os}(\text{bpy})_2\text{Cl}_2^+$ in the presence of AuNC (curve (ix) of Fig. 3c) was

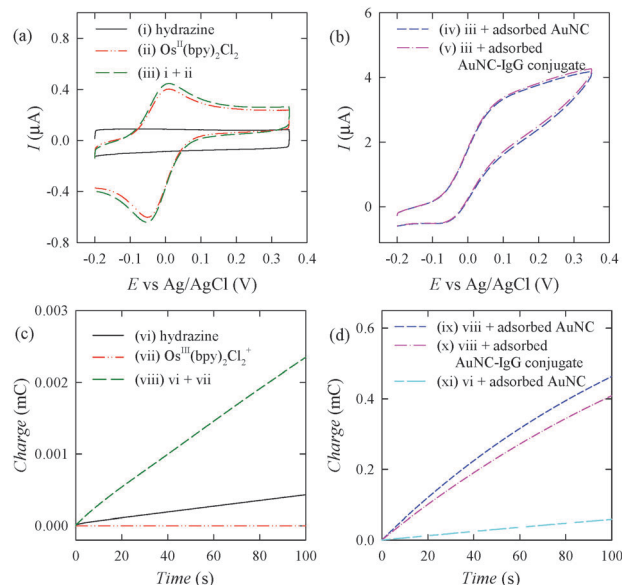


Fig. 3 (a and b) Cyclic voltammograms recorded (at a scan rate of 20 mV s^{-1}) using (i, ii and iii) bare ITO electrodes, (iv) an ITO electrode modified with adsorbed AuNC, and (v) an ITO electrode modified with an adsorbed AuNC-antibody conjugate in PBS containing (i) 1.0 mM hydrazine, (ii) $100 \mu\text{M}$ $\text{Os}^{\text{III}}(\text{bpy})_2\text{Cl}_2^+$, and (iii, iv and v) 1.0 mM hydrazine and $100 \mu\text{M}$ $\text{Os}^{\text{III}}(\text{bpy})_2\text{Cl}_2^+$. (c and d) Chronocoulograms recorded (at an applied potential of 0.20 V) using (vi, vii and viii) bare ITO electrodes, (ix) an ITO electrode modified with adsorbed AuNC, and (x) an ITO electrode modified with an adsorbed AuNC-antibody conjugate in PBS (pH 7.4) containing (vi) 1.0 mM hydrazine, (vii) $100 \mu\text{M}$ $\text{Os}^{\text{III}}(\text{bpy})_2\text{Cl}_2^+$, and (viii, ix and x) 1.0 mM hydrazine and $100 \mu\text{M}$ $\text{Os}^{\text{III}}(\text{bpy})_2\text{Cl}_2^+$.

higher than that obtained in a solution of hydrazine in the presence of AuNC (curve (xi) of Fig. 3c). These results indicate that the EN_c redox cycling involving $\text{Os}(\text{bpy})_2\text{Cl}_2^+/\text{Os}(\text{bpy})_2\text{Cl}_2$ significantly increases the electrochemical signal.

The catalytic activity of AuNC may deteriorate significantly after an antibody is adsorbed onto AuNC. To obtain a high electrochemical signal, the catalytic activity of an AuNP-labelled antibody should be similar to that of bare AuNC. The cyclic voltammogram obtained in the presence of adsorbed AuNC (curve (iv) of Fig. 3b) was similar to that obtained in the presence of an adsorbed AuNC-labelled antibody (curve (v) of Fig. 3b). Moreover, there was no significant difference between the chronocoulometric signal obtained in the presence of adsorbed AuNC (curve (ix) of Fig. 3d) and that obtained in the presence of an adsorbed AuNC-labelled antibody (curve (x) of Fig. 3d). These results clearly indicate that most of the catalytic activity of AuNC remained even after the antibody was adsorbed onto AuNC.

The performance of the EN_c redox-cycling scheme was evaluated using immunosensors that detect CK-MB and mouse IgG (Fig. 1a). Avidin-modified ITO electrodes were used to immobilize antibodies because the modified electrodes show very low nonspecific binding to many labelled antibodies. The immobilized antibody captures the target and then the AuNC-labelled antibody. The EN_c redox cycling involving the ITO electrode, $\text{Os}(\text{bpy})_2\text{Cl}_2^+/\text{Os}(\text{bpy})_2\text{Cl}_2$, AuNC, and hydrazine occurs upon specific binding of the AuNC-labelled antibody to the captured target. The electrochemical oxidation of

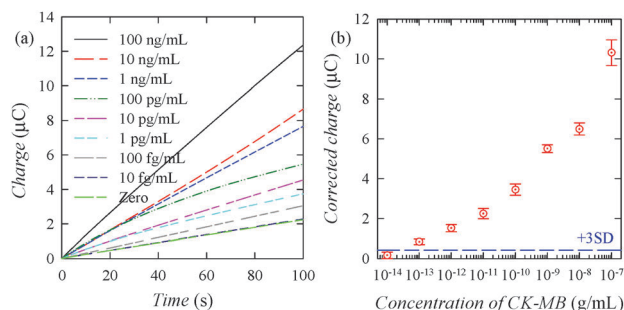


Fig. 4 (a) Chronocoulograms obtained (at an applied potential of 0.16 V) using immunosensing electrodes in PBS containing 1.0 μM $\text{Os}^{\text{III}}(\text{bpy})_2\text{Cl}_2^+$ and 1.0 mM hydrazine for detecting various concentrations of CK-MB spiked in PBS. (b) Calibration plot: concentration dependence of the charges at 100 s in panel (a). Each experiment was carried out using three different immunosensing electrodes for the assay of the same sample. The data were subtracted by the mean value obtained from seven measurements at zero concentration. The dashed line corresponds to three times the standard deviation (SD) of the charge at zero concentration.

$\text{Os}(\text{bpy})_2\text{Cl}_2$ triggers the EN_c redox cycling. Consequently, outer-sphere to inner-sphere redox cycling occurs in the sequence of a highly OSR-philic ITO electrode, highly OSR-philic $\text{Os}(\text{bpy})_2\text{Cl}_2^+$ / $\text{Os}(\text{bpy})_2\text{Cl}_2$, OSR- and ISR-philic AuNC, and highly ISR-philic hydrazine (Fig. 1a). Ultimately, a high electrochemical signal for the nanocatalytic reaction is achieved without an incubation period.

Fig. 4a shows concentration-dependent chronocoulograms obtained at an applied potential of 0.16 V in PBS containing $\text{Os}(\text{bpy})_2\text{Cl}_2^+$ and hydrazine after the immunosensing electrodes were treated with PBS containing various concentrations of CK-MB and then with carbonate buffer containing AuNC-labelled anti-CK-MB IgG. The charge data increased with increasing concentration of CK-MB. Fig. 4b shows a calibration plot drawn with the charge data measured at 100 s in the chronocoulograms (Fig. 4a). The calculated detection limit was approximately 20 fg mL^{-1} for CK-MB, indicating that the immunosensor is highly sensitive and that the nonspecific binding of the AuNC-labelled antibody to the immunosensing electrode is very low. Fig. S3a of the ESI† shows concentration-dependent chronocoulograms obtained after the immunosensing electrodes were treated with PBS containing various concentrations of mouse IgG and then with PBS containing AuNC-labelled antimouse IgG. Fig. S3b of the ESI† shows a calibration plot drawn with the charge data measured at 100 s in the chronocoulograms. The calculated detection limit was approximately 20 fg mL^{-1} for mouse IgG, reconfirming that the EN_c redox cycling allowed ultrasensitive detection. In the case of another cardiac target (myoglobin), the chronocoulometric signal was similar to that of zero CK-MB (Fig. S4 of the ESI†), indicating that the immunosensor is selective.

To validate the applicability of the immunosensor using the EN_c redox cycling, 15 clinical serum samples were tested using the immunosensor. Each test was carried out using three different immunosensing electrodes for the assay of the same sample, and the charges at 100 s obtained from the chronocoulograms were plotted against the known concentrations of CK-MB (Fig. S5 of the ESI†). The charge increased with increasing concentration of CK-MB

with good reproducibility, indicating that the immunosensor is practically appealing.

In conclusion, we have developed a new nanocatalytic scheme using outer-sphere to inner-sphere EN_c redox cycling that allows high signal amplification. When the EN_c redox cycling was applied to a sandwich-type immunosensor for the detection of CK-MB, the calculated detection limit was approximately 20 fg mL^{-1} , indicating that the immunosensor is highly sensitive. The results for clinical serum samples showed that the immunosensor is practically appealing.

This work was supported by the National Research Foundation of Korea (2015R1A2A2A01002695, 2015M2A8A5021905, and 2012-M3C1A1-048862).

Notes and references

- 1 A. A. Lubin and K. W. Plaxco, *Acc. Chem. Res.*, 2010, **43**, 496.
- 2 F. Ricci and K. W. Plaxco, *Microchim. Acta*, 2008, **163**, 149.
- 3 K. W. Plaxco and H. T. Soh, *Trends Biotechnol.*, 2011, **29**, 1.
- 4 J. C. Cunnning, N. J. Brenes and R. M. Crooks, *Anal. Chem.*, 2014, **86**, 6166.
- 5 J. Hu, T. Wang, J. Kim, C. Shannon and C. J. Easley, *J. Am. Chem. Soc.*, 2012, **134**, 7066.
- 6 J. Das and H. Yang, *J. Phys. Chem. C*, 2009, **113**, 6093.
- 7 W. Schuhmann, *Rev. Mol. Biotechnol.*, 2002, **82**, 425.
- 8 A. Singh, S. Park and H. Yang, *Anal. Chem.*, 2013, **85**, 4863.
- 9 G. Dutta, S. Kim, S. Park and H. Yang, *Anal. Chem.*, 2014, **86**, 4589.
- 10 G. Dutta, S. Park, A. Singh, J. Seo, S. Kim and H. Yang, *Anal. Chem.*, 2015, **87**, 3574.
- 11 H. Taube, *Angew. Chem., Int. Ed.*, 1984, **23**, 329.
- 12 S. V. Rosokha and J. K. Kochi, *Acc. Chem. Res.*, 2008, **41**, 641.
- 13 A. J. Bard, *J. Am. Chem. Soc.*, 2010, **132**, 7559.
- 14 M. R. Akanda, Y.-L. Choe and H. Yang, *Anal. Chem.*, 2012, **84**, 1049.
- 15 H. Yang, *Curr. Opin. Chem. Biol.*, 2012, **16**, 422.
- 16 P. Chen and R. L. McCreery, *Anal. Chem.*, 1996, **68**, 3958.
- 17 M. Choi, K. Jo and H. Yang, *Bull. Korean Chem. Soc.*, 2013, **34**, 421.
- 18 W. J. Kim, B. K. Kim, A. Kim, C. Huh, C. S. Ah, K. H. Kim, J. Hong, S. H. Park, S. Song, J. Song and G. Y. Sung, *Anal. Chem.*, 2010, **82**, 9686.
- 19 L. Piras and S. Reho, *Sens. Actuators, B*, 2005, **111–112**, 450.
- 20 C. L. Yuan, S. S. Kuan and G. G. Gullbault, *Anal. Chem.*, 1981, **53**, 190.
- 21 A. M. J. Haque, J. Kim, G. Dutta, S. Kim and H. Yang, *Chem. Commun.*, 2015, **51**, 14493.
- 22 J. R. Peela, A. M. Jarari, A. Hai, A. K. Rawal, S. D. Kolla, S. Sreeksar, L. Khurana and N. R. Sidhanathi, *Ibnosina J. Med. Biomed. Sci.*, 2010, **2**, 190.
- 23 A. J. S. Ahammad, Y. H. Choi, K. Kok, J. H. Kim, J. J. Lee and M. Lee, *Int. J. Electrochem. Sci.*, 2011, **6**, 1906.
- 24 E. V. Suprun, A. L. Shilovskaya, A. V. Lisitsa, T. V. Bulko, V. V. Shumyantseva and A. I. Archakov, *Electroanalysis*, 2011, **23**, 1051.
- 25 A. Qureshi, Y. Gurbuz and J. H. Niazi, *Sens. Actuators, B*, 2012, **171–172**, 62.
- 26 M. Pedrero, S. Campuzano and J. M. Pingarron, *Electroanalysis*, 2014, **26**, 1132.
- 27 J. P. Park, M. K. Park and J. W. Yun, *Biomarker*, 2011, **16**, 1.
- 28 J. Lee, Y. S. Choi, Y. Lee, H. J. Lee, J. N. Lee, S. K. Kim, K. Y. Han, E. C. Cho, J. C. Park and S. S. Lee, *Anal. Chem.*, 2011, **83**, 8629.
- 29 J. Das, K. Jo, J. W. Lee and H. Yang, *Anal. Chem.*, 2007, **79**, 2790.
- 30 M. R. Akanda, M. A. Aziz, K. Jo, V. Tamilvan, M. H. Hyun, S. Kim and H. Yang, *Anal. Chem.*, 2011, **83**, 3926.
- 31 A. N. Asanor, W. W. Wilson and P. B. Oldham, *Anal. Chem.*, 1998, **70**, 1156.
- 32 M. R. Akanda, H.-A. Joung, V. Tamilvan, S. Park, S. Kim, M. H. Hyun, M.-G. Kim and H. Yang, *Analyst*, 2014, **139**, 1420.
- 33 M. R. Akanda, V. Tamilvan, S. Park, K. Jo, M. H. Hyun and H. Yang, *Anal. Chem.*, 2013, **85**, 1631.
- 34 J. Jeong, J. Das, M. Choi, J. Jo, M. A. Aziz and H. Yang, *Analyst*, 2014, **139**, 5814.
- 35 S. Park and H. Yang, *Analyst*, 2014, **139**, 4051.
- 36 S. Noh and H. Yang, *Electroanalysis*, 2014, **26**, 2727.