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RNA BioMolecular Electronics: towards new tools for biophysics and biomedicine

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The last half-century has witnessed the birth and development of a new multidisciplinary field at the edge between materials science, nanoscience, engineering, and chemistry known as Molecular Electronics. This field deals with the electronic properties of individual molecules and their integration as active components in electronic circuits and has also been applied to biomolecules, leading to BioMolecular Electronics and opening new perspectives for single-molecule biophysics and biomedicine. Herein, we provide a brief introduction and overview of the BioMolecular electronics field, focusing on nucleic acids and potential applications for these measurements. In particular, we review the recent demonstration of the first single-molecule electrical detection of a biologically-relevant nucleic acid. We also show how this could be used to study biomolecular interactions and applications in liquid biopsy for early cancer detection, among others. Finally, we discuss future perspectives and challenges in the applications of this fascinating research field.

Introduction

From before the 1980s and especially during the 90s, materials science in general, and nanoscience and nanotechnology in particular, have promised multiple applications enabled by an unprecedented control of matter. One of them is the ultimate miniaturization of electronic components and circuits to the

scale of individual molecules. This exciting field is known as Molecular Electronics.

Molecular Electronics started almost 50 years ago when Aviram and Ratner predicted the first molecular rectifier (Fig. 1, top) in their seminal theoretical work.¹ During the last half century, a myriad of theoretical and experimental results have been published studying the many aspects of molecular electronics.

Theories for how charges transfer and transport in molecules developed^{2–8} in parallel with the experimental developments. The multiple theoretical and experimental methods used during the years, beyond the scope of this perspective, can be found in

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Angela Piso is an undergraduate student majoring in Biology at the University of Massachusetts Lowell. She is a pre-medical student interested in tying research into her future career as a doctor. Angela hopes to one day work in the field of oncology. In addition to her work in the lab, she is also an EMT. She provides emergency care to both her university's campus and local communities.



Tiba Qattan is an honors Biology student at the University of Massachusetts Lowell. As an immersive scholar, she worked with the Chemistry Department on a project that utilizes the STM break junction technique in various applications. The project employs nanoscience technologies to develop biosensors and understand biomolecular interactions. She recently got accepted to the Baccalaureate MD Pathway program this

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Juan M. Artes Vivancos is an assistant professor in the Department of Chemistry at the University of Massachusetts Lowell. After obtaining a PhD from the University of Barcelona working in single-molecule biophysics, he was a postdoctoral associate at the ECE Department of the University of California, Davis, developing new electrical methods for detecting oligonucleotides. He was

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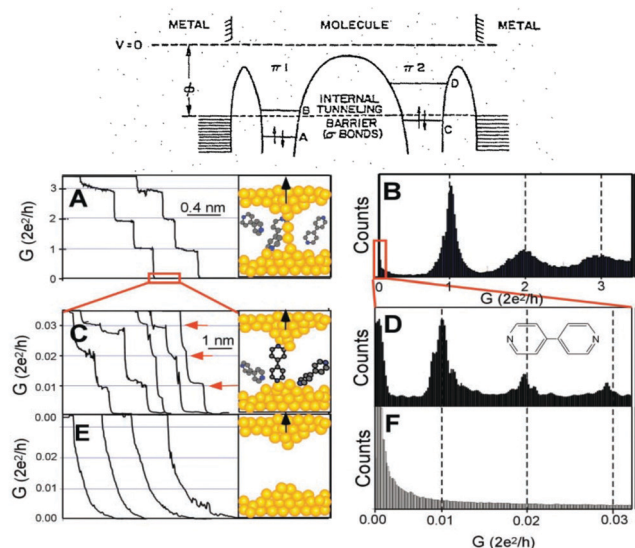


Fig. 1 Top: Aviram and Ratner's proposed molecular diode diagram. Reproduced with permission from ref. 1. Bottom: The STM-BJ current-distance method applied to bipyridine. (A) Conductance of a gold contact formed between a gold STM tip and a gold substrate decreases in quantum steps near multiples of G_0 ($=2e^2/h$) as the tip is pulled away from the substrate. (B) A corresponding conductance histogram constructed from 1000 conductance curves as shown in (A) shows well-defined peaks near $1G_0$, $2G_0$, and $3G_0$ due to conductance quantization. (C) When the contact shown in (A) is completely broken, corresponding to the collapse of the last quantum step, a new series of conductance steps appears if molecules such as 4,4'-bipyridine are present in the solution. These steps are due to the formation of the stable molecular junction between the tip and the substrate electrodes. (D) A conductance histogram obtained from 1000 measurements as shown in (C) shows peaks near $1 \times$, $2 \times$, and $3 \times 0.01G_0$ that are ascribed to one, two, and three molecules, respectively. (E and F) In the absence of molecules, no such steps or peaks are observed within the same conductance range. Reproduced with permission from ref. 19.

BioMolecular Electronics

Shortly after opening the door for reliable single-molecule conductance measurements, biomolecules were considered as the subject of these studies, too, primarily short peptides³² and oligonucleotides.³³ This quickly expanded to larger biomolecules,^{34–36} including redox proteins^{26,37} and even some larger complexes.³⁸ We briefly review a protein example below before focusing on oligonucleotides and BioMolecular Electronics applications.

Proteins: the case of azurin

The STM-BJ approach¹⁹ was used to perform conductance measurements on the redox protein azurin (Fig. 2).²⁶ Azurin is a small protein from *Pseudomonas aeruginosa* that constituted the benchmark for charge transfer in proteins during the 90s in theoretical and experimental research (electrochemical and photochemical bulk studies).^{39–41} The results showed current steps comparable to those found in studies performed on organic molecules with simpler structures, indicating that azurin can establish a junction bridging two electrodes.²⁶ Conductance

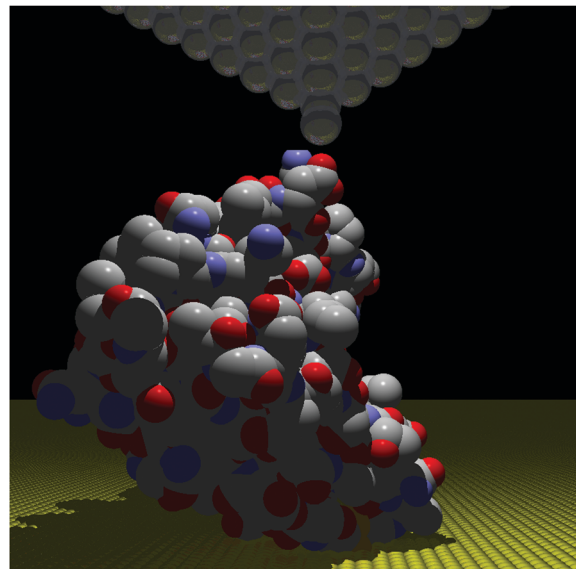


Fig. 2 Idealized all atom representation of an azurin junction contacted between two STM electrodes. Figure built using the pdb structure 1AZU,⁴⁷ RasMol,⁴⁸ and PoV-Ray.⁴⁹

histograms obtained at different electrochemical potentials demonstrated that azurin conductance is related to the redox behavior of the protein, as control measurements performed on non-redox Zn-azurin showed no such dependence. The dependence of azurin conductance on electrochemical potentials is consistent with a multistep charge transport model.⁷ A numerical version of the model⁴² was used to fit the data and obtain parameters describing the charge transport (CT) process. The conductance in the junction is controlled by the alignment of the Fermi levels of the electrodes with the energy level of the redox center, in analogy to a field effect transistor. This constituted a proof of concept transistor based on a single protein. Further research helped to obtain other parameters, like the transition voltage,^{43,44} studying azurin mutants,^{14,45} and azurin interacting with the redox partner.⁴⁶ Developments over the last decades show that STM-assisted molecular junctions are a vital tool for molecular and bioelectronics. These applications to study single protein conductance opened the doors for future investigations on more complex biological samples that constitute ongoing research.

Nucleic acids

Just ten years after the discovery of the structure of DNA,⁵⁰ it was suggested that the stacking of the orbitals of the bases of double stranded DNA (dsDNA) could lead to conductive behavior.⁵¹ Since then, several theoretical and experimental studies have addressed the question of the electronic conductance in DNA, leading to exciting findings and a still ongoing discussion.

DNA CT has been an active field of study for many years. How the charges move through oligonucleotides is a question that has been addressed using diverse techniques, including



bulk and single-molecule approaches, in environments ranging from ultra-high vacuum to solid-state configurations in air, as well as experiments in buffer and electrochemical environments.^{33,34,52–60}

DNA bases have been found to participate and mediate CT in optical, electrochemical, and single-molecule approaches.⁵³ However, in a recent study, it is suggested that CT could also be mediated by the backbone.⁶⁰ Further research is needed to demonstrate if the backbone is playing any direct role in the DNA CT process. Despite not having a clear, unified picture of the CT process in DNA, it is now clear that CT plays an essential role in some DNA biological processes.^{53,61} For example, CT in DNA is fundamental in DNA oxidative processes, like oxidative damage and its repair related to many widespread diseases.⁶¹ But, probably due to the different variety of conditions, various lengths, and sequences used in the experiments, results of DNA conductance reported in the literature spanned a vast range differing in orders of magnitude. Just to cite some examples, DNA was reported to be insulating,^{54,62} semiconducting,⁵⁶ conducting,⁵⁷ and even superconducting.⁵⁸

Nevertheless, despite all these different results, discarding disagreements due to diverse experimental conditions and extreme molecular differences, some consensus was achieved about the mechanisms for CT in individual DNA molecules. Fig. 3 shows the different determinants for single-molecule DNA conductance. In general, except in one report,⁶⁰ it has been observed that a double-helix is needed to transport charges due to the base stacking providing the orbitals with energy levels mediating the transfer. Initially, the electronic conductance was believed to depend mainly on sequence and length, based on the results observed in DNA³³ and other progressively longer molecules.⁶⁴ GC-rich sequences tended to give a smoother decay of G with the distance, suggesting a hopping charge transfer, while ATs introduced a higher resistance for the charges, suggesting a tunneling charge transport mechanism. Similarly, a transition from tunneling to hopping is suggested with increasing lengths. Several variations and subtleties on these two extremes have been proposed over the years (*i.e.* see ref. 12, 65 and 66), but discussing the particular details is beyond the scope of this perspective. Theoretical studies suggested from early years that effects such as the structure and conformation of DNA may modulate the conductance.^{6,67} After a decade of single-molecule DNA measurements, new effects were described (Fig. 3c), suggesting that the conformation of the sequence^{59,68–70} and the delocalization of the density of electronic states^{59,63} over more than one base pair also play essential roles in determining the conductance of DNA oligonucleotides. As a consequence of the base stacking being the central mediator of the CT process, mismatches in the base-pairing can profoundly affect oligonucleotides' conductance.^{34,71} The conductance of the molecule can change by an order of magnitude, depending on the nature of the base substitution.³⁴

Despite this consensus, there are several remaining unknowns about the electrical conductance of DNA; What is the precise role of the backbone? Which one is the CT mechanism for each length? Is there a mechanism explaining

DNA electrical conductance

- Sequence
- Length
- Structural/Conformational
- Delocalization length

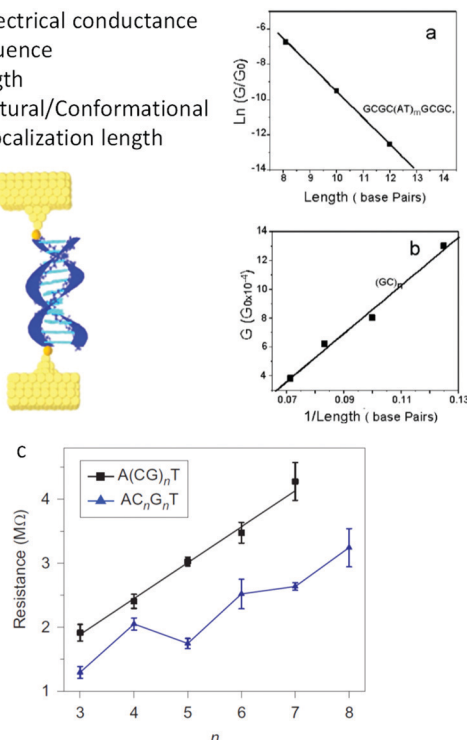


Fig. 3 Factors determining DNA conductance. (a) Natural logarithm of DNA conductance vs. length (total number of base pairs). The solid line is a linear fit that reflects the exponential dependence of the conductance on length. The decay constant is determined from the slope of the linear fit. (b). Conductance of (GC)_n vs. 1/length (in total base pairs). Reproduced with permission from ref. 33. (c) Resistance of alternating (black squares) and stacked (blue triangles) G DNA sequences versus the number of CG in the sequences. The stacked sequences have smaller resistance values than alternating sequences, and an oscillation is superimposed on the linear trend. Error bars are standard deviations calculated from three to four sets of experiments for each individual sequence. Reproduced with permission from ref. 63. The scheme in the left was adapted with permission from ref. 59.

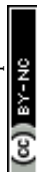
all the effects? Is it possible to predict the electrical conductance from the DNA sequence in complex structures such as DNA origami or other NA nanostructures?

Further research is necessary to complete our understanding since experiments with individual oligonucleotides keep showing surprising results (see below).

DNA:RNA: a different length and sequence dependence

One would expect DNA:RNA hybrid molecules (a DNA chain hybridized with an RNA) would have similar or identical conductance as a dsDNA with the same sequence, but the initial experiments with simple GC-rich DNA:RNA sequences showed recently that their electrical conductance was one order of magnitude higher than the one of dsDNA for the same sequence.⁷²

Fig. 4 shows simulations done to rationalize the experimental results showing DNA:RNA having one order of



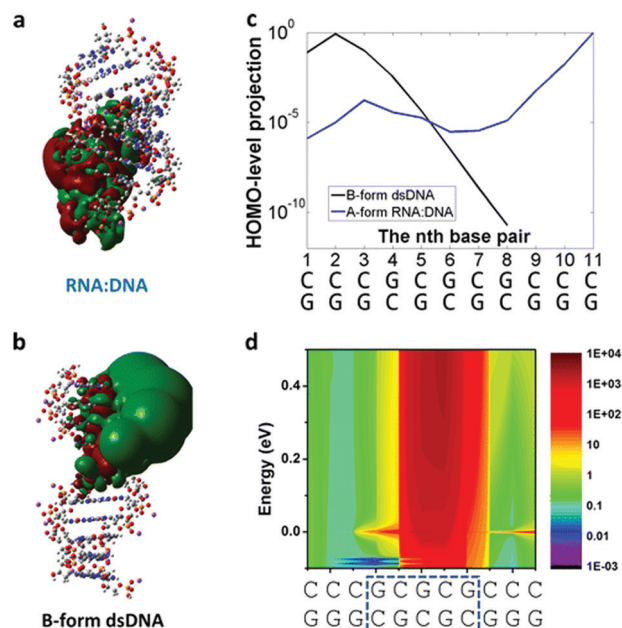


Fig. 4 DNA:RNA conductance in GC-rich sequences. Results from charge-transport simulations of 11-bp RNA:DNA and B-form dsDNA. (a and b) 3D isosurface of the HOMO orbital (isovalue = 2×10^{-5}) on the oligonucleotide structures for RNA:DNA and B-form dsDNA. (c) Projection of the HOMO level onto each of the base pairs in the A-form RNA:DNA (blue solid line) and B-form dsDNA (black solid line). There is no contribution to the HOMO level for the 9th to 11th base pairs in dsDNA. (d) 2D representation of the ratio of the total density of states (DoS) along the molecule between RNA:DNA hybrids and B-form dsDNA for an energy ranging from HOMO–0.1 to 0.5 eV above HOMO level. Reproduced with permission from ref. 72.

magnitude higher conductance than the dsDNA counterpart.⁷² Briefly, results and simulations demonstrated that this different conductance is mainly due to DNA:RNA hybrids being in the A-form (Fig. 4a) conformation, while dsDNA is in the B-form (Fig. 4b). In contrast with some early theoretical calculations that suggested the opposite trend⁶ (it is worth noting that this study did not include the backbone in the computation), A-form is more compact and allows for the delocalization of the HOMO over more base pairs (see Fig. 4),^{59,72} resulting in a higher conductance.

Another surprise in the first DNA:RNA conductance reports was the length dependence of adenine-stacked sequences.⁷³ Adenine-rich sequences favored a tunneling component and a sharp decay of the conductance for increasing lengths in dsDNA measurements³³ but resulted in nearly length-independent and a long-range conductance⁷³ in DNA:RNA hybrids (Fig. 5).

The behavior of AT-rich sequences shown in Fig. 5 reflects virtually the same conductance for sequences ranging from eleven to twenty-one base pairs. This is indicative of a hopping CT mechanism,⁷³ but a deeper analysis of this length dependence resulted in the conclusion that the most likely mechanism is hopping with the hopping site being delocalized over several base pairs.⁶³ Specifically, it is 1.3 nm, or five bases for the sequence shown in Fig. 5.⁷³

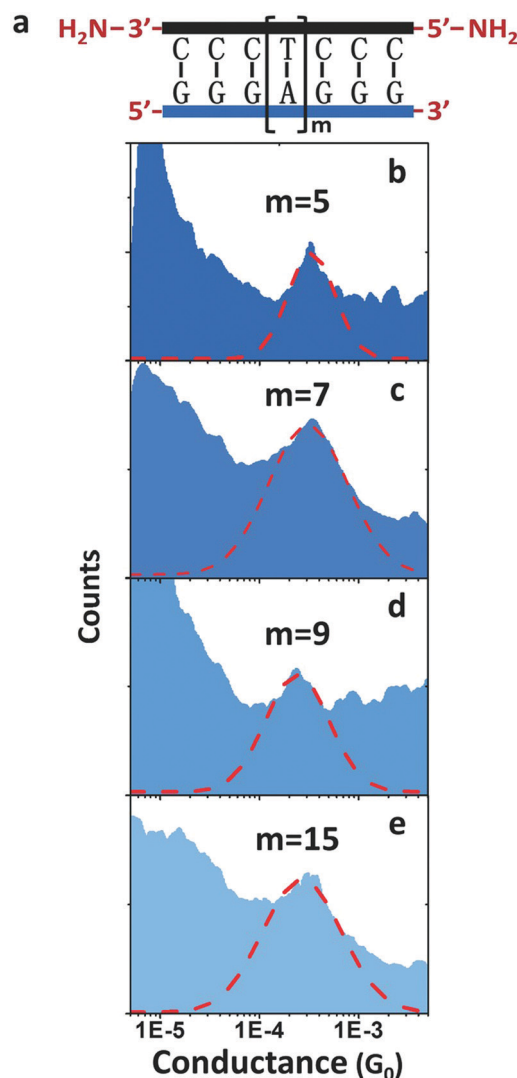
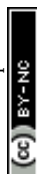


Fig. 5 DNA:RNA conductance in adenine-rich sequences. Conductance measurements of adenine-stacked RNA:DNA hybrids. (a) Illustration of the GGG-Am-GGG RNA:DNA hybrids. (b–e) Conductance histograms of four RNA:DNA hybrids ($m = 5, 7, 9$, and 15 , respectively). Red dashed line shows the Gaussian fitting of each peak. Reproduced with permission from ref. 73.

In summary, STMBJ measurements in individual oligonucleotides have established the main determinants for single-molecule conductance in dsDNA and DNA:RNA hybrids.^{59,71–73} However, some knowledge gaps remain and more studies are needed to characterize the CT process in oligonucleotides completely; *e.g.*, the conductance of dsRNA or those from sequences containing uracil have not been systematically studied yet. Nevertheless, the research has already paved the way for single-molecule devices, biosensors, and several other applications (see below). In the following sections, we introduce some emerging applications of BioMolecular Electronics. The initial ones correspond to new applications recently reported, while others are potential applications representing ongoing research.



Some examples of applications and potential applications: a single-molecule biosensor for foodborne bacteria

The electrical detection of individual RNA molecules in solution described above allows for the ultra-sensitive detection of sequences in complex environments.^{71,74} Knowing the particular target sequence (*i.e.*, specific for some organism), one can design a complementary probe functionalized to bind electrodes and close the “circuit” (Fig. 6), with the conductance detected being characteristic for the target sequence and sensitive to changes in length,⁷² conformation,⁵⁹ and changes in the base-pairing.³⁴

Traditional approaches for detecting microorganisms often require time-consuming cell-culturing steps before detection and identification, and, while nucleic acid-based methods provide better specificity (mutants, different strains, and pathogenic serotypes can be differentiated), the detection of nucleic acids almost always requires enzymatic amplification through

approaches such as PCR.⁷⁵ The electrical detection of RNA can obviate the need for amplification steps and enable the detection of particular sequences in complex and dilute environments (Fig. 6).⁷¹

Fig. 6 shows the first single-molecule electrical detection approach applied to particular *E. coli* strains. These experiments focused on identifying specific strains of *Escherichia coli*.⁷⁶ Many *E. coli* strains are pathogenic and produce one or more forms of Shiga toxin.⁷⁷ This approach targeted a particular region of mRNA that partially encodes for the Shiga toxins. RNA was specifically targeted instead of DNA for different reasons, as introduced above:

- RNA transcription within the cells naturally amplifies these targets during the interphase of the cell cycle, thus naturally creating more RNA for detection, which in turn may remove the necessity of performing PCR-based amplification or cell-culturing steps.
- Many pathogens have RNA genomes⁷⁸
- RNA fragments can provide direct information about gene activity and cell viability.

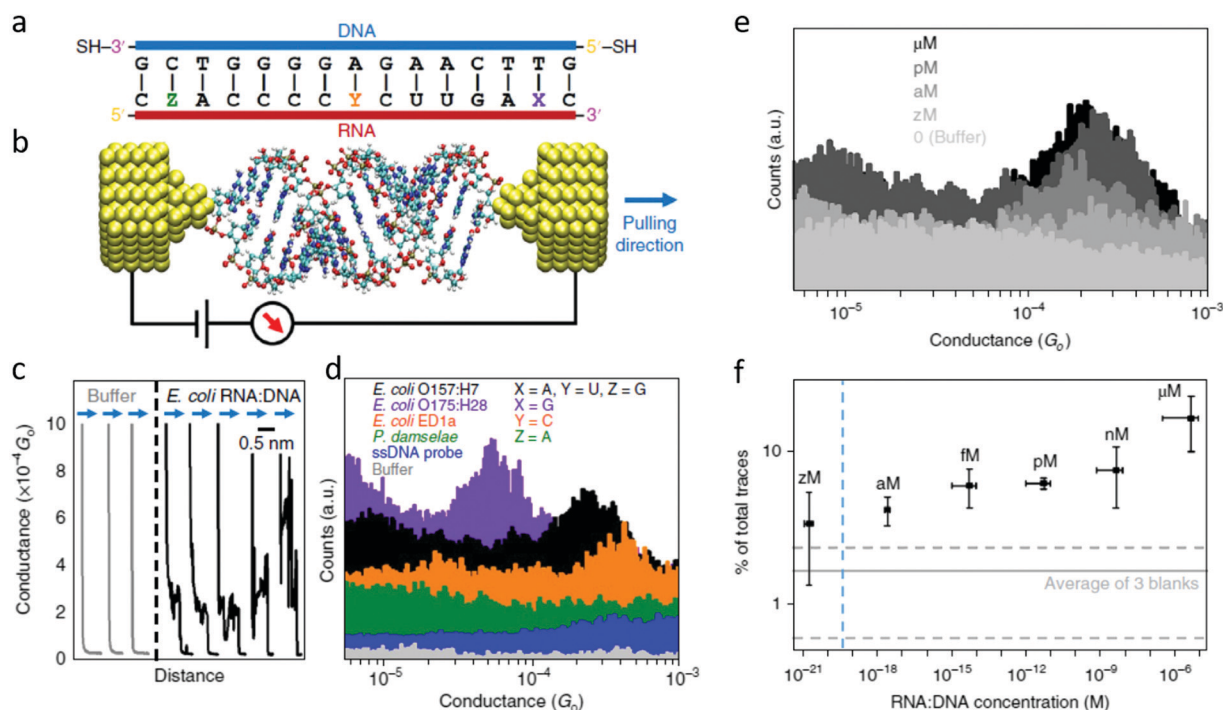


Fig. 6 The first single-molecule electrical study on a biologically-relevant oligonucleotide. (a) Schematic of the 15 bp RNA:DNA sequences studied. The blue side represents the DNA probe with thiol linkers, and the red side represents the RNA sequences targeted. For *E. coli* O157:H7 $X = A$, $Y = U$, and $Z = G$ (perfectly matched). In the other three cases a mismatch is present. For *E. coli* O157:H28 $X = G$, for *E. coli* ED1a $Y = C$ and for *Photobacterium damsela* $Z = A$. (b) Idealized schematic of the experimental set-up showing the RNA:DNA molecule bound between two gold electrodes. (c) Representative conductance versus distance traces obtained from the O157:H7 hybrids during break junction measurements. The black curves (with steps) are measured when a molecule binds between the electrodes; and the grey curves occur when no molecules bind. All curves are offset horizontally for clarity. (d) Conductance histograms for the four RNA:DNA hybrids and two control experiments performed for the single-stranded DNA probe and blank buffer. Histograms are offset vertically for clarity. A total of 5000 traces were collected for each sample. (e) Representative histograms measured at various concentrations of the O157:H7 sequence. The control experiment in buffer solution shows no peak in the histogram. (f) Dependence of trace selection on the concentration of target molecules, showing the percentage of traces with steps at varying concentrations. Horizontal error bars show the final RNA:DNA hybrid concentration range from three independent experiments. Vertical error bars represent the percentage of curves showing steps from three independent measurements. Dashed horizontal lines represent the typical percentage of curves selected in sodium phosphate buffer without adding RNA:DNA hybrids. The vertical dashed line depicts the theoretical concentration where a single molecule would exist in the sample volume. Adapted with permission from ref. 71.



Note that this approach is entirely different from electrical sequencing technologies based on ionic currents; the charge transports through the bases, parallel to the strand in this case, while in sequencing approaches, one aims either to block the ionic current in a nanopore with the NA or to measure the CT perpendicular to each base. This single-molecule biosensor can detect known sequences quickly and sensitively, but is not designed to figure out new sequences. Recently, some efforts have been developed to adapt this technology to sequencing applications, using BioMolecular Electronics with the aid of machine learning data treatment.⁷⁹

As a single-biomolecule sensor, this application shows remarkable specificity able to discern single-base mismatches. The histograms in Fig. 6d show that changes in an individual base can dramatically affect electrical conductance. While the wild-type (perfect match) sequence for the pathogenic *E. coli* O157:H7 results in a conductance around $2.5 \times 10^{-4} G_0$ (with G_0 being the conductance quantum, $G_0 = 2e^2/h$), changing an adenine to guanine close to the 3' in the RNA fragment causes the conductance to drop to a fifth of that value, allowing for detecting of this other pathogenic *E. coli* strain. In contrast, when guanine is exchanged for an adenine close to 5' (a *P. damsela* sequence), the conductance is not detectable in this experimental range. Another surprising result was found when changing uracil in the central part of RNA for a cytosine (a sequence for the non-pathogenic *E. coli* ED1), resulting in an electrical conductance of $5 \times 10^{-4} G_0$. This is remarkable since it is counter-intuitive; affecting the base pairing in the middle of the sequence, instead of affecting the CT pathway, somehow favors it. This manifests that the conductance is a complex magnitude difficult to predict from the starting sequence and was explained thanks to molecular dynamics simulations coupled to *ab initio* CT calculations. The computations showed that this particular change affected the molecule's energy levels, bringing it closer to the energy level of the electrodes, resulting in a situation closer to resonance and thus a higher electrical conductance.⁷¹

Besides the high specificity allowing the distinction of different sequences from different strains differing in only one base pair, this method also has the advantage of extremely high sensitivity. Fig. 6e shows conductance histograms obtained from experiments performed at different RNA concentrations ranging from extremely low (zM, 10^{-21} M) to micro. The selectivity (number of conductance traces included in the histogram) scales proportionally with the concentration. A titration for the selectivity (Fig. 6f) allows finding the limit of detection for this proof-of-concept single-molecule sensor to be in the attomolar range. Table 1 shows a comparison of the Limit of Detection (LOD) of this novel biosensor to typical sensor performance indicators in the literature.

This, together with other indicators of sensor performance (the possibility of detecting the target RNA in the presence of interfering sequences⁷¹ and complex environments⁷⁴), shows a proof-of-concept single-molecule biosensor that has enormous potential impact in diverse fields related to human health. This method's possible future benefits go from detecting potential

Table 1 Sensor performance: limit of detection (LOD) in concentration units for different sensing technologies

Technology	LOD
Chemical sensors	nM ⁸²
Electrochemical biosensors	fM ⁸³
SPR	pM–nM ⁸⁴
STM-based single-biomolecule electrical detection	aM ⁷¹

pathogens before they cause catastrophic epidemics to the early detection of biomarker sequences related to cancer (see the last section).

Some present roadblocks for these new applications are the lack of single-molecule conductance measurements for RNA from human origin and the challenges in miniaturizing these single-molecule devices, despite recent advances in miniaturization and microfabrication of electromechanical molecular break-junctions systems.^{80,81} See the last section for more details.

Electrical measurement of biomolecular interactions at the single-molecule level

The advances described above are not limited to engineering applications in biosensors and nano detectors but could also open new possibilities for single-molecule biophysical measurements. Biomolecular interactions and their analysis are at the core of a wide range of disciplines like biochemistry, biotechnology, and medicinal chemistry. These dynamic interactions are the key to all cellular functions and understanding those interactions between biomolecules could be vital to elucidate the molecular basis of many diseases. Single-molecule techniques (mostly optical approaches) have emerged as powerful tools for deciphering these interactions.⁸⁵

Comparing single-molecule results with the known behavior of the cellular interactions in bulk has also remained a challenge for scientists over the years. STM-BJ methods could also be used to study the fundamentals of biophysical interactions at the single-molecule level. Therefore, BioMolecular Electronics methods based on scanning probe microscopies are promising single-molecule approaches for measuring electron transport between biomolecules and in biomolecular complexes. This molecular-level biophysical study could also be a concept validation for different single biomolecule-based sensors, not necessarily based on nucleic acids, if using interactions such as the one between antigen and antibody (Ag–Ab).

Measuring Ag–Ab interactions

Antigen–antibody interactions are a textbook example of biomolecular interactions.⁸⁶ The strength of the interaction between antibody (Ab) and antigen (Ag) depends on the affinity and the specificity of the binding.^{86,87} In addition, depending on the number of binding sites and conformations at the molecular level, the strength of the binding may vary.⁸⁸

There exist several bulk methods for detecting these Ag–Ab interactions. These include immuno-rolling circle amplification,^{89–91} immuno-hybridization chain reaction,⁹² electrochemical impedance



Antibodies are Y-shaped proteins with different binding domains (Fig. 7). They can form a conducting bridge by binding a pair of electrodes,⁹⁷ making the system perfect for STM-BJ measurements. By measuring the electrical conductance of individual Ag-Ab complexes, one could get a molecular fingerprint to characterize them. Fig. 7 shows an idealized diagram of a single-molecule junction formed between an antibody and two electrodes. Measurements in the presence and absence of the antigen could help elucidate if the antigen affects the conductance pathway, and this may demonstrate a single-biomolecule biosensor based on Ag-Ab interactions. This kind of single-biomolecule electrical biosensors could be invaluable for human health and environmental monitoring.¹⁰¹

A far more complex system with crucial biomolecular interactions is the RNA-Induced Silencing Complex (RISC). The RISC

is a multiprotein complex that uses the siRNA or miRNA as a template for recognizing complementary mRNA.¹⁰² When it finds a complementary strand, it activates RNase to cleave mRNA. siRNAs function post-transcriptionally by base-pairing to the mRNA 3'-untranslated regions to repress protein synthesis.^{102,103} The main components of the RISC are the nucleic acids, the proteins DICER, TRBP (RNA binding protein), PACT, and, most importantly, Argonaute 2 (AGO2).¹⁰⁴ BioMolecular Electronics measurements could also be used for having a complete understanding of these dynamic processes and measuring the interactions between different components of the RISC complex.¹⁰⁵

Some recent studies support the fact that some phase-separated systems inside the cell are associated with transcription regulation and other biological functions. Processing bodies (P-bodies) are one of these phase-separated cytoplasmic ribonucleoprotein complexes, primarily composed of translationally repressed mRNAs and proteins.¹⁰⁶ They are induced by cellular stress and related to mRNA decay.¹⁰⁶ These phase-separated systems are associated with many diseases,¹⁰⁷ including cancer, neurodegeneration, and some infectious diseases.

Fig. 8 shows an advanced potential application of BioMolecular Electronics, where a nucleic acid bound between electrodes, in turn, binds to Ago2. With such a system, one could have a clear insight into the binding geometry between the different components of the RISC complex and obtain electrical fingerprints for each case. One could construct the respective conductance histograms and get electrical fingerprints by measuring the conductance values for ds RNA and Ago2–dsRNA complexes. These fingerprints could be related to single-complex thermodynamic and kinetic information of these complexes responsible for gene silencing. This information could be crucial to predicting the design and delivery strategies for silencing human disease factors using RNAi.

In the future, the application of single-molecule techniques for the measurement of gene expression in individual cells

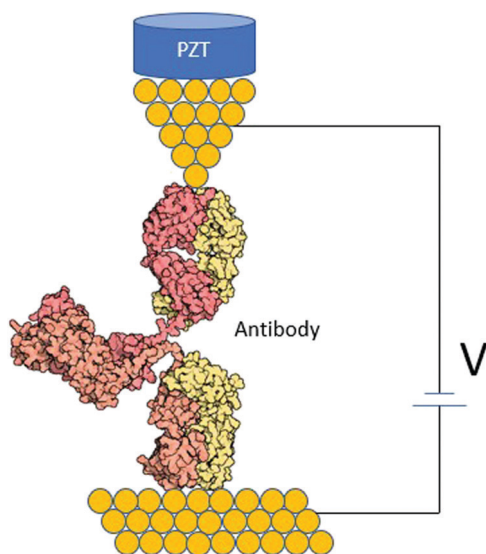


Fig. 7 STM biomolecular break junction formed by an individual antibody between two gold electrodes.

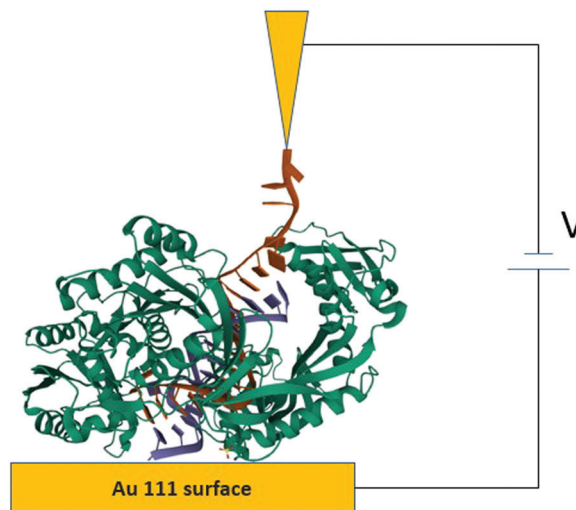


Fig. 8 STM-BJ measurement of a Argonaute-siRNA complex at the single-complex level.

could provide many new insights into the field of gene silencing.¹⁰⁸

A potential biomedical application: electrical cancer detection in liquid biopsies

Cancer is a significant healthcare problem and constitutes one of the most frequent causes of death globally.¹⁰⁹ Unfortunately, many cancer cases are recognized too late, and this late-stage diagnosis results in higher fatality rates. Thus, there is a clear need for detection methods capable of detecting early stages since this could enable early treatments, potentially saving many lives.¹¹⁰

A promising approach for early detection is the use of cancer biomarkers in body fluids through liquid biopsies.¹¹¹ Liquid biopsy is an analytically sensitive body fluid test that allows analyzing body fluids such as blood samples for cancer-specific biomarkers. It can be used to discriminate tumor cells easily among billion healthy cells.¹¹² Blood samples, or other body fluids, can contain circulating free tumor nucleic acids (ctNA) such as circulating tumor DNA (ctDNA) or circulating tumor RNA (ctRNA) that can be used as cancer biomarkers.¹¹² The amount of circulating tumor DNA in blood can range from 0.01% up to 1%,¹¹² an extremely low level compared to wild-type cell-free DNA. This, combined with a low frequency of mutations relative to wild-type sequences, makes ctDNA detection in blood or other body fluids challenging.¹¹² Detecting RNA may be relatively easier because transcription allows RNA to be amplified naturally and produces more RNA for detection. Moreover, RNA provides information about the particular cellular state.⁷¹

Nanotechnology could help to address these challenges. For example, the STM-BJ recently allowed the first demonstration of detection and identification of RNA from *E. coli* via single-molecule conductance⁷¹ (see above), and this could be an ideal method for liquid biopsy because it is non-invasive, highly sensitive, and could be helpful to detect cancers without the use of surgery.¹¹² Fig. 9 shows the proposed approach; after sampling body fluids, the liquid biopsy sample could be used for single-biomolecule electrical detection targeting cancer biomarkers with minimal preprocessing.⁷⁴

The main hypothesis behind this particular application is that the sequences of ctNAs can be used to detect cancers. Recent omics studies suggest that this is the case, such as the

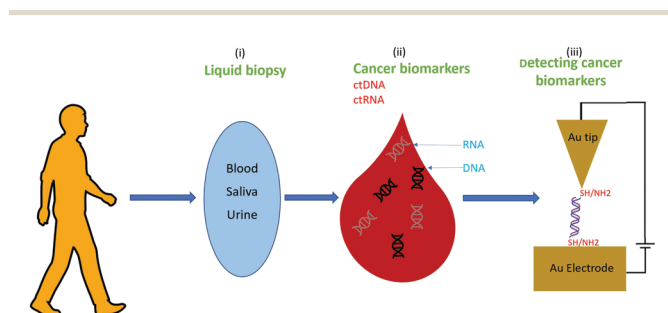


Fig. 9 A biomedicine application: cancer detection via single-biomolecule electrical detection in liquid biopsies.

Pan-Cancer Analysis of Whole Genomes (PCAWG) of the International Cancer Genome Consortium (ICGC) and The Cancer Genome Atlas (TCGA)¹⁰⁹ (see Fig. 10). PCAWG reports the comprehensive and integrative analysis of 2658 whole-cancer genomes across 38 tumor types.^{109,113} Fig. 10 shows a recent analysis of the distribution of cancer biomarkers and their mutations across cancer types.¹¹³ At the top of the list, one finds the proto-oncogene KRAS, TERT, and BRAF accounting for most of the mutations detected in dangerous adenocarcinomas like the pancreatic one. We propose using STM-BJ to detect Kras mRNA mutant fragments as a proof-of-concept application of single-molecule electrical detection of a biomarker for early cancer detection. This could be extended to many other biomarkers, and the detection paralleled after miniaturizing the single-biomolecule sensor to cover several different cancer types. Since the conductance of mRNA is expected to decrease with an increasing length of the sequence,⁷² it is critical to find the minimum specific size because it will allow for a higher signal-to-noise ratio in the conductance measurement. At the same time, the chosen sequence needs to be specific only for the required gene.

It is worth mentioning that this approach is different from sequencing and is not targeting the discovery of new biomarkers. In this case, we propose BioMolecular Electronics for the fast electrical screening of liquid biopsy samples in single-molecule experiments (targeting already discovered common cancer biomarkers). We study the unique electrical fingerprints of the biomarkers that may appear in many cancer types with the objective of detecting cancers electrically. This could be extended to the parallel detection of many biomarkers in miniaturized devices that could simultaneously cover several different cancer types.

We are doing some preliminary analysis on wild-type and mutated KRAS sequences (a common cancer biomarker). GC content, melting temperatures, and secondary structure information can be found using the IDT Oligoanalyzer tool.¹¹⁴ In addition, the minimum specific length is found using the NCBI Blast tool.¹¹⁵ Multiple alignments Blast results

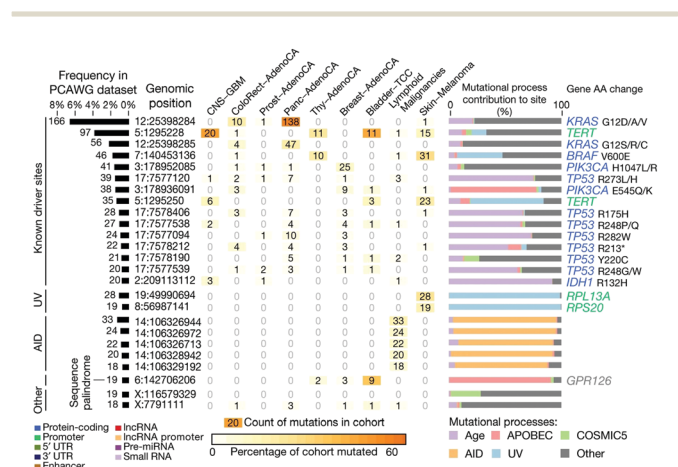


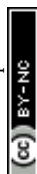
Fig. 10 Candidate cancer biomarkers found in the recent literature.¹¹³ Reproduced with permission from ref. 113.



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