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## Biosafety evaluation of dual-responsive neutroblots

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The toxicity effects of paclitaxel (PTX)-loaded magnetic neutrophil-hybrid swimming microrobots ("neutroblots") *in vivo* were assessed after intravenous administration to mice. The mice after 72 hours exhibited minimal immunotoxicity and liver and kidney toxicity at an administration dose of  $3 \times 10^6$  PTX-loaded neutroblots. The minor toxicity of drug-loaded neutroblots holds considerable promise for biomedical applications.

## Introduction

Swimming micro/nanorobots as an innovative modality have attracted considerable attention due to their unprecedented features as well as promising potential, particularly in the areas of the active targeted delivery of therapeutic agents.<sup>1–3</sup> Swimming micro/nanorobots enable controllable propulsion in various fluids by the conversion of chemical or physical energy

into mechanical motion.<sup>4–8</sup> Compared with conventional therapeutic micro/nanoparticles which rely on passive diffusion in biological fluids, swimming micro/nanorobots allow for the transportation of diverse therapeutic agents toward the hard-to-reach areas.<sup>9,10</sup> Among various swimming micro/nanorobots, magnetically actuated micro/nanorobots that are driven by an external magnetic field with uniform intensity have exhibited an impressive propulsion performance in various complex biological fluids ranging from blood flow to the vitreous of eyes.<sup>11–13</sup> With the efficient and precise mobility, the magnetic swimming micro/nanorobots are capable of conducting various tasks, including genome editing, non-invasive surgery, and environmental remediation.<sup>14–19</sup> However, the major magnetic swimming micro/nanorobots still have inherent limitations such as poor biocompatibility and biodegradability. With the rapid development in the field of biomedicine, swimming micro/nanorobots with biocompatible and biomimetic surfaces for favourable interfaces and interactions with natural biological subjects are urgently required.

To overcome these issues, diverse natural cell-hybrid magnetic swimming micro/nanorobots were developed in the past decade, and their movement behavior in biological fluids and biomedical applications has been investigated.<sup>20</sup> Sharing the unique biological functions of natural cells, diverse types of cells, such as red blood cells, macrophages, and neutrophils, have been utilized to develop swimming micro/nanorobots.<sup>21,22</sup> Particularly, neutrophil-hybrid magnetic swimming microrobots, namely neutroblots, have exhibited efficient magnetic propulsion and chemotaxis along the gradient of inflammatory factors for active therapy of glioma *in vivo*.<sup>23</sup> Although considerable progress has been accomplished on neutroblots, safety concerns are still remaining in its potential for immunogenicity and its relatively poor *in vivo* stability. There are no reports involving the safety evaluation of neutroblots *in vivo*.

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California Institute of Technology. His research interests are focused on the development of the next-generation of swimming micro/nanorobots for precision medicine. He is a recipient of the MIT Technology Review 35 Innovators under 35 in China list.

Here, we report the pharmacology and toxicity of the systematic administration of neutroblots in mice. To investigate the toxicological effect of drugs from neutroblots in the body, neutroblots were encapsulated with paclitaxel (PTX) – a typical antitumor drug that also causes considerable side effects to normal tissues. According to a previous report, the PTX-loaded neutroblots by intravenous injection exhibited a remarkable therapeutic effect toward glioma *in vivo* upon the administration dose of  $10^6$  neutroblots per mouse.<sup>23</sup> The corresponding PTX dose from neutroblots is equivalent to that of the free PTX toward mice. Inheriting the biocompatibility and biodegradability of natural neutrophils, drug-loaded neutroblots are not susceptible to uptake by normal cells, accomplishing negligible toxicity *in vivo* which is essential to neutroblots for practical biomedical usages.

## Materials and methods

### Materials

Percoll was purchased from Biosharp Biotechnology Co., Ltd. Fe(acac)<sub>3</sub>, gelatin, NaOH, hexanoic anhydride, 1,2-hexadecanediol, coumarin 6, dibenzyl ether, oleic acid, oleylamine, 1,1'-di-*n*-octadecyl-3,3,3',3'-tetramethylindocarbocyanine perchlorate (DiI), Hoechst 33342, and 1,1-dioctadecyl-3,3,3,3-tetramethylindocarbocyanine iodide (DiR) were purchased from Shanghai Yeasen Biotechnology Co., Ltd. Polycarbonate porous membranes (400 nm, 200 nm) were purchased from Whatman. Phosphotungstic acid was purchased from Beijing Solarbio Biotechnology Co., Ltd. RPMI 1640, DMEM, fetal blood serum (FBS), and PBS were purchased from Biosharp Biotechnology Co., Ltd. ELISA Kits (mouse TNF- $\alpha$ , IP-10, IFN- $\alpha$ , C3, IL-6, and histamine) were purchased from Shanghai Fanyin Biotechnology Co., Ltd.

## Methods

### Preparation and characterization

**Preparation of EM@nanogels.** EM@nanogels were fabricated *via* a camouflage process among *E. coli* outer membrane vesicles and nanometer scale gelatin particles, named nanogels. Nanogels were produced by dissolving amphiphilic gelatin and hydrophobic Fe<sub>3</sub>O<sub>4</sub> nanoparticles<sup>24</sup> into the water–chloroform mixed dispersant, chloroform phase with 6 mg of paclitaxel (PTX) or without, and then the dispersant was heated to evaporate chloroform. Magnetic nanoparticles were prepared as described in the literature. The amphiphilic gelatin gathered on the interface between the water and chloroform, and, with chloroform evaporated, the gelatin aggregated around chloroform nanodroplets with Fe nanoparticles and eventually formed nanogel particles. The *E. coli* outer membrane vesicles were obtained by an ultracentrifugation method with 1 50 000 g for 2 h. Then, the nanogels and *E. coli* outer membrane vesicles were mixed and forced to pass through a polycarbonate membrane with a pore size of 200 nm under external pressure. After the extruding process, EM@nanogels were collected by 9800 g centrifugation 2 times.

**Isolation of neutrophils.** Neutrophils were collected from the murine bone marrow of KM or ICR mice. The RPMI 1640 medium was applied to flush the inner cavity of the mice tibia bone to obtain a bone marrow dispersion containing leukocytes, and then a discrete density gradient centrifugation means using the commercial Percoll mixture was applied to collect neutrophils from the interfaces of 71% and 61% volume fraction Percoll. More centrifugations would be applied to remove Percoll and red blood cells if necessary.

**Preparation of neutroblots.** For the preparation of neutroblots, the neutrophils were cultured with EM@nanogels for 30 min at 37 °C. EM@nanogels were phagocytosed by neutrophils to form neutroblots. Excess EM@nanogels were separated by centrifugation.

**TEM of neutroblots.** Neutroblots were dehydrated step by step and dispersed in acetone. The resin was added to the acetone dispersion of neutroblots on a rotating shaking table. After the resin was cured, the sections were sliced and stained with uranyl acetate and lead citrate. Finally, the sectioned samples of neutroblots were observed by transmission electron microscopy H-7650 (Hitachi, Japan).

**CLSM of neutroblots.** Cou6 loaded EM@nanogels were used to prepare neutroblots. The nucleus of neutroblots was labelled by Hoechst 33342. DiI was used to label the cell membrane of neutroblots. The 3D images were captured and reconstructed using a Leica SP5 Confocal microscope.

**Fe amount of neutrophils, neutroblots and neutroblots loaded with nanogels.** The Fe amount was evaluated using ICP-AES.

### Magnetic motion

**Magnetic field setup.** The magnetic field system contains a signal generator, a signal amplifier, a data acquisition card, Helmholtz coils, and a microscope. The magnetic field using in this experiment is the rotating magnetic field.

**Trajectories and velocity of neutroblots.** The movie of the motion of neutroblots was recorded. Trajectories of neutroblots were analyzed using ImageJ plugin Manual Tracker/Mtrack2. The velocity was calculated based on trajectories and motion time.

#### Plasma cytokine level test

KM mice (male, 6–8 weeks) were used in this experiment. The mice were intravenously injected with neutroblots loaded with PTX ( $3 \times 10^6$  cells per mouse). Before injection, a blood sample was collected as the control group (0 h). After scheduled times (12, 24, 48, and 72 h), blood samples were collected from the Kunming mice. The plasma was separated after centrifugation of the blood sample (3000 rpm, 30 min). ELISA kits were used to test plasma cytokine levels.

***In vivo* distribution of neutroblots.** KM mice (male, 6–8 weeks) were used in this experiment. Neutroblots ( $3 \times 10^6$  cells per mouse, labelled with DiR) were intravenously injected into mice. After injection, the mice were anesthetized by isoflurane. Then, the mice were imaged using the PERKINELMER IVIS Spectrum.

#### Liver function test and renal function test

A blood sample was collected from the KM mice injected with neutroblots ( $3 \times 10^6$  cells per mouse) after different time intervals. The tests were conducted by the laboratory department of the hospital of Harbin Institute of technology.

**Pathological section of main organs after the injection of neutroblots.** KM mice (male, 6–8 weeks) were used in this experiment. The mice were intravenously injected with neutroblots ( $3 \times 10^6$  cells per mouse). Before injection, a blood sample was collected as the control group (0 h). After scheduled times (12, 24, 48, and 72 h), the main organs (brain, heart, liver, spleen, lungs, and kidneys) were separated and fixed. The sections were stained with H&E, and the images were captured using OLYMPUS IX-73 inverted microscope with DP74 CCD camera.

All the animals were treated in accordance with the Guide for Care and Use of Laboratory Animals. Animal experiments were approved by the experimental animal welfare ethics committee of the Harbin Institute of technology (No. IACUC-2022032).

## Results and discussion

### Fabrication and characterization of neutroblots

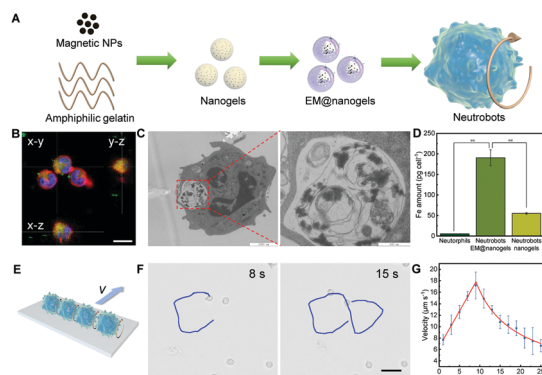
The preparation of neutroblots contains three steps including the synthesis of gelatin-based nanogels, preparation of *E. coli* membrane-coated nanogels (EM@nanogels), and phagocytosis of EM@nanogels into neutrophils (Fig. 1A).  $\text{Fe}_3\text{O}_4$  nanoparticles ( $\text{Fe}_3\text{O}_4$  NPs) and PTX-loaded gelatin nanogels were fabricated utilizing an emulsion/solvent evaporation method as described in a previous report.<sup>23</sup> Furthermore, the *E. coli* membrane, acting as a multifunctional scaffold that prevents the intracellular release of PTX and activates neutrophils to engulf EM@nanogels, was fused onto the nanogel through

co-extruding of the nanogel and *E. coli* membrane nanovesicles. The resulting neutroblots were obtained by the phagocytosis of EM@nanogels using neutrophils. To confirm the presence of EM@nanogels inside the neutroblots, coumarin 6 (Cou6)-labeled EM@nanogels were introduced into the fabrication process of neutroblots. The three dimensional confocal laser scanning microscopy image in Fig. 1B illustrated the green fluorescence from Cou6 inside the neutroblots, indicating the successful incorporation of EM@nanogels toward neutroblots. Next, the ultrastructure analysis of neutroblots using ultramicrotomy was conducted to visualize the subcellular distribution of EM@nanogels. The ultrathin TEM section image of neutroblots in Fig. 1C displayed a significant number of EM@nanogels inside the neutroblots. The corresponding enlarged TEM image displayed that these particles were aggregated and encapsulated in a phagosome membrane inside the cytoplasm of neutroblots. Inductively coupled plasma/mass spectrometry (ICP-MS) analysis was conducted to further quantify the iron phagocytosis by the neutroblots. As shown in Fig. 1D, an up an uptake of 190.5 ng of iron per 1000 neutroblots was observed from the EM@nanogels, while the neutroblots that were prepared with bare nanogels rather than EM@nanogels had an uptake of 55.1 ng per 1000 cells. The near 4-fold elevation in the amount of iron clearly verifies that the coating of the *E. coli* membrane can effectively enhance the phagocytosis of EM@nanogels by neutrophils.

The magnetically actuated propulsion of neutroblots upon application of an external rotating magnetic field with a uniform intensity is attributed to the interaction between neutroblots and the substrate (Fig. 1E). The capability of PTX-loaded neutroblots to efficiently locomote *in vitro* was first examined. The microscopic images in Fig. 1F illustrate the movement of neutroblots under the rotating magnetic field with a frequency of 30 Hz and an intensity of 15 mT in 15 s. The corner trajectory of neutroblots was achieved by the manipulation of the direction of the rotating magnetic field. Moreover, the velocity of neutroblots can be controlled by operating the frequency of the rotating magnetic field. As shown in Fig. 1G, the average velocity increases from  $7.7 \mu\text{m s}^{-1}$  at 1 Hz to  $17.2 \mu\text{m s}^{-1}$  at 9 Hz. It should be noted that the intensity of the employed rotating magnetic field plays a minor role in the toxicity toward normal cells.

### Dynamic distribution of neutroblots *in vivo*

To investigate the safety profile of neutroblots *in vivo*, PTX-loaded neutroblots were injected through the caudal vein in a dose of  $3 \times 10^6$  neutroblots per mouse according to a previous report.<sup>23</sup> Such a dose was comparable to the number of neutrophils in the whole mouse, and the dose cannot be elevated anymore. In this case, the distribution of injected neutroblots *in vivo* as a function of time was first studied. To visualize the dynamic distribution *in vivo*, the neutroblots were loaded with a DiR fluorescent dye. IVIS Spectrum *in vivo* imaging instruments were used to continuously characterize the change of the fluorescence intensity of mice in 60 min. As shown in Fig. 2, the real-time change of the fluorescence



**Fig. 1** Fabrication, characterization and magnetic propulsion of neutroblots. (A) Scheme of the preparation of neutroblots. (B) CLSM images of neutroblots (Cou6-EM@nanogels, Hoechst 33342-nucleus, and DiI-cell membrane). (C) TEM image of a neutroblot. Scale bar, 2  $\mu\text{m}$ . The enlarged image shows EM@nanogels inside the neutroblot. Scale bar, 500 nm. (D) Fe amount of neutrophils, neutroblots and neutroblots with nanogels.  $** p < 0.01$ . (E) Scheme of the magnetic motion of neutroblots under a rotating magnetic field. (F) Controlled motion of a single neutroblot under a magnetic field. (G) Motion velocity of single rolling neutroblots under RMF with different frequencies (15 mT).

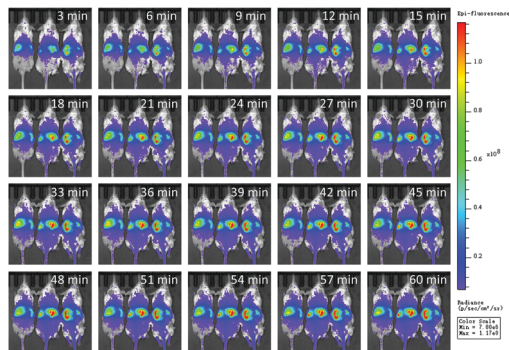


Fig. 2 *In vivo* distribution of neutroblots after injection into mice ( $3 \times 10^6$  cells per mouse) at different processing timescales. Scale bar, 10 mm.

intensity displayed that the fluorescence intensity in liver rapidly increased in first 30 min, consistent with the existing judgment that the liver is the main detoxification organ in mammals.<sup>25</sup> After that, there was negligible change in the fluorescence intensity of the mouse except the liver, the above changes could be obtained by reading the numerical changes of ROIs. These changes indicated that mice are metabolizing, and decomposing DiR injected into the body, implying that neutroblots can be excreted from the body through the normal metabolic pathway of mammals. The results shown in Fig. 2 prove that neutroblots had a normal metabolic pathway in mammals and did not affect the survival of mice in the experiment.

### Effects of neutroblots toward liver *in vivo*

Next, the toxicity of neutroblots toward liver *in vivo* was studied by collecting the blood samples of mice injected with neutroblots to detect their liver functions. Alanine aminotransferase (ALT) and aspartate aminotransferase (AST) are important enzymes in the liver.<sup>26</sup> Evaluating the content of liver enzymes in the serum can evaluate liver injury and dysfunction. Mice without the injection of neutroblots were used as the control group. In the liver function test, Fig. 3A shows the serum ALT concentration test. Elevated ALT usually shows liver injury. After injecting neutroblots without PTX, the ALT concentration was  $14 \text{ U L}^{-1}$  at 12 hours, which increased briefly compared with the ALT concentration of the control group ( $9.3 \text{ U L}^{-1}$ ). At 24 hours, it decreased to  $10.7 \text{ U L}^{-1}$ , which has no significant difference with the concentration of the control group.

At 48 hours and 72 hours, the ALT concentration was  $8.3$  and  $8 \text{ U L}^{-1}$  respectively, which was lower than the ALT concentration of the control group. After the injection of PTX-loaded neutroblots, the concentrations of ALT at 12, 24, 48 and 72 hours were  $9.7$ ,  $7.3$ ,  $9.7$  and  $10.3 \text{ U L}^{-1}$ , respectively, which have no significant difference with that in the control group. Moreover, the test of serum AST in Fig. 3B shows that the AST concentration in the control group was  $29.7 \text{ U L}^{-1}$ . After the injection of neutroblots without PTX, the concentration of AST slightly increased at 12 hours. The concentrations of AST in the PTX-free neutroblots and PTX-loaded neutroblots groups were  $34.7$  and  $36.3 \text{ U L}^{-1}$ , respectively, and, decreased at 24 hours,

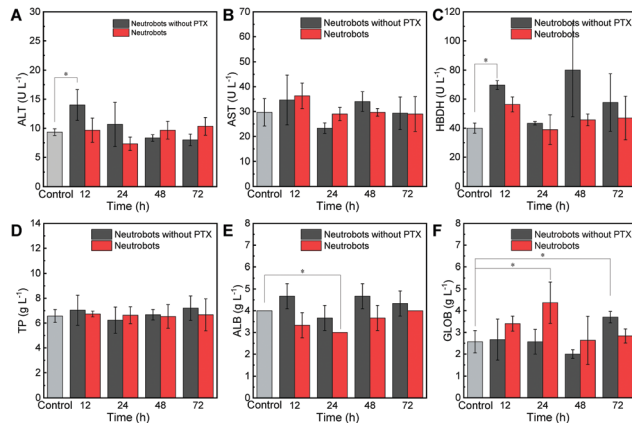


Fig. 3 Liver function tests of KM mice injected with neutroblots at specific time points after injection. Mice of the control group with no injection, and mice injected with  $3 \times 10^6$  neutroblots loaded with PTX or not. (A) Serum alanine aminotransferase (ALT) concentration, (B) serum aspartate aminotransferase (AST) concentration, (C) serum  $\alpha$ -hydroxybutyrate dehydrogenase (HBDH) concentration, (D) serum total protein (TP) concentration, (E) serum albumin (ALB) concentration, and (F) serum globulin (GLOB) concentration.  $N = 3$ ,  $* p < 0.05$ .

the concentrations of AST were  $23.3$  and  $29 \text{ U L}^{-1}$ , respectively. There was no significant change in the AST concentration at 48 hours and 72 hours. The AST test results showed that neutroblots had no obvious damage to the liver. Furthermore,  $\alpha$ -hydroxybutyrate dehydrogenase (HBDH) is a kind of cell death marker. Acute hepatitis and heart and kidney injury may cause the increase of HBDH.<sup>27</sup> After the injection of neutroblots, HBDH in the PTX free neutroblots group and the PTX loaded neutroblots group increased slightly (Fig. 3C). Compared with the HBDH concentration in the control group ( $40 \text{ U L}^{-1}$ ), HBDH in the PTX free neutroblots group increased to  $80 \text{ U L}^{-1}$  at 48 hours and then decreased to  $57.7 \text{ U L}^{-1}$  at 72 hours. In the PTX loaded neutroblots group, HBDH reached  $56.3 \text{ U L}^{-1}$  at the highest and decreased rapidly after 12 hours. The results from 24 hours to 72 hours have no significant difference to those in the control group, indicating that a very short process of cell damage may be caused after the injection of neutroblots. There is a small fluctuation in the HBDH concentration, and it quickly returns to the normal range in a short time. In order to test the liver function, the contents of the serum total protein (TP), albumin (ALB) and globulin (GLOB) were measured at the same time. Fig. 3D shows that the TP after the injection of neutroblots is moderate and maintained in a stable range, which is similar to the value of the control group. The injection of neutroblots has no effect on the total serum protein. Fig. 3E shows that ALB fluctuated slightly after the injection of neutroblots. After the increase of ALB in the PTX free neutroblots group, it was maintained at a similar amount to that in the control group. After the injection of PTX loaded neutroblots, ALB decreased briefly and returned to a range similar to that of the control group at 48 hours. Fig. 3F shows that the GLOB concentration increased briefly after the injection of PTX loaded neutroblots, which



was  $4.4 \text{ g L}^{-1}$  at 24 hours, compared with  $2.6 \text{ g L}^{-1}$  in the control group, which may be due to the transient immune response. Then it rapidly decreased to  $2.6 \text{ g L}^{-1}$  at 48 hours, indicating that the injection of neutrophils had only a transient effect on the globulin content. Based on the above results, the effect of neutrotoxs injected into mice on liver function can be ignored and did not cause the increase of transaminase and drastic changes in the serum protein concentration, indicating that neutrotoxs have very little toxicity to the liver.

### Toxicity evaluation of neutrotoxs toward kidney *in vivo*

Blood urea nitrogen (BUN) and serum creatinine (CREA) are markers of renal function<sup>28</sup> and UREA/CREA. The kidney is responsible for the drug metabolism and is vulnerable to damage. BUN may be affected by the protein intake and metabolic status. Fig. 4A shows the CREA concentration in blood, and there was no significant change in the content of creatinine, while the BUN value decreased slightly, which is shown in Fig. 4B. There may be many reasons for the decrease in BUN, except for the impaired renal function, so it can be considered that the renal function of the mice was not affected. Fig. 4C shows UREA/CREA values in blood, similar with BUN results, UREA/CREA values were decreasing. As an increased UREA/CREA indicates the impaired kidney function, the decreased result also has few things to do with the kidneys. Fig. 4D shows the blood glucose concentration, and all data were in a normal range. In summary, injected neutrotoxs are not toxic to the kidneys.

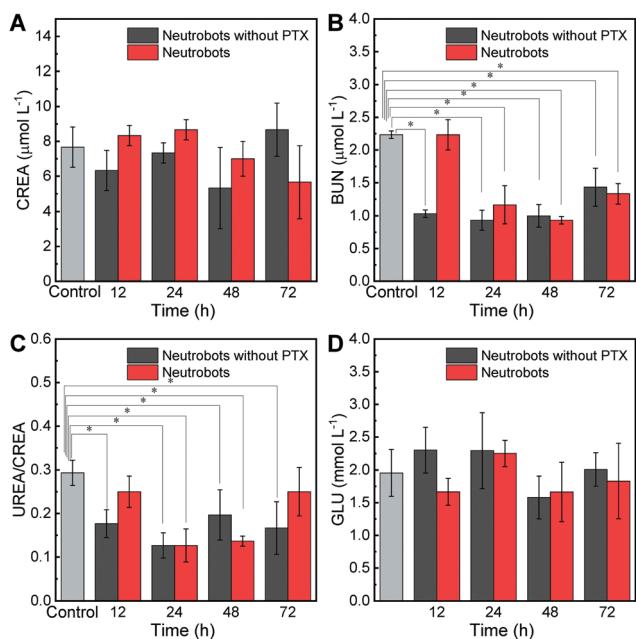


Fig. 4 Renal function tests of KM mice injected with neutrotoxs at specific time points after injection. Mice of the control group with no injection, and mice injected with  $3 \times 10^6$  neutrotoxs loaded with or not. (A) Serum creatinine (CREA) concentration, (B) blood urea nitrogen (BUN) concentration, (C) urea creatinine ratio (UREA/CREA), and (D) serum glucose (GLU) concentration.  $N = 3$ ,  $* p < 0.05$ .

### Evaluation of immunotoxicity caused by neutrotoxs *in vivo*

It is not only necessary to characterize the metabolism of neutrotoxs in mice, but also to analyze whether neutrotoxs will cause additional immune responses in mice, such as incremental immune rejection. Therefore, the following experiments were designed: the contents of various cytokines and immune factors in the mouse serum were detected within 72 hours after the injection of  $3 \times 10^6$  neutrotoxs, to judge whether the injection of neutrotoxs caused an additional immune response. Six kinds of cytokines were tested; they were tumor necrosis factor- $\alpha$  (TNF- $\alpha$ ), interferon g-inducible protein 10 (IP-10), IFN- $\alpha$ , complement components (C3), interleukin-6 (IL-6), and histamine.

The test results are shown in Fig. 5, indicating that the contents of six cytokines were within the normal range. TNF- $\alpha$  is used in the immune system for cell signaling. During an inflammatory response, macrophages or leukocytes release TNF- $\alpha$  as a communication between immune cells.<sup>29</sup> The stable TNF- $\alpha$  content indicated that the injection of neutrotoxs did not cause severe inflammation and subsequent cytokine release (Fig. 5A). IP-10, also known as the CXC motif chemokine ligand 10 (CXCL10), has chemical attraction to monocytes/macrophages, T cells, *etc.*, and promotes the adhesion of T cells to endothelial cells, antitumor activity and inhibition of bone marrow colony formation and angiogenesis.<sup>30</sup> After neutrotoxs were injected into mice, IP-10 was stable at 0–72 h, indicating that neutrotoxs had a negligible effect on the immune system and the fluctuation is very small (Fig. 5B). IFN- $\alpha$  is a type I interferon, which plays an important role in inflammation, immune regulation, and other reactions and has anti-tumor activity.<sup>31</sup> After neutrotoxs were injected into the body, IFN- $\alpha$  shows a slightly down-regulation at 0 to 24 h, from 20.7 to  $15.5 \text{ pg mL}^{-1}$ , and then return to  $21.8 \text{ pg mL}^{-1}$  at 48 h (Fig. 5C). IFN- $\alpha$  shows a stable level after the injection. Complement component 3 (C3) plays a key role in the complement system

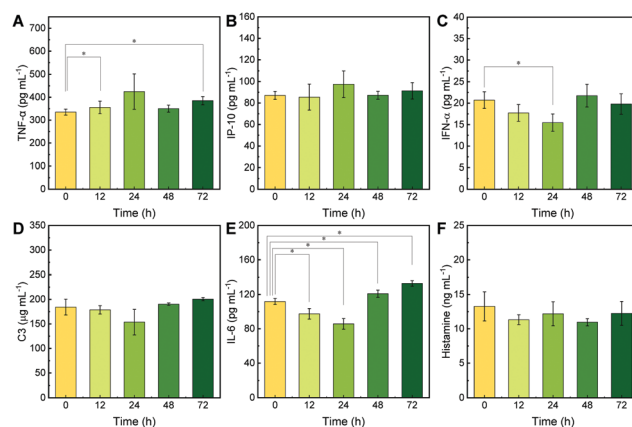


Fig. 5 Plasma cytokine levels in mice after injection with neutrotoxs loaded with PTX ( $3 \times 10^6$  cells per mouse) and different processing timescales. (A) Tumor necrosis factor- $\alpha$  (TNF- $\alpha$ ) levels, (B) interferon g-inducible protein 10 (IP-10) levels, (C) IFN- $\alpha$  levels, (D) complement component (C3) levels, (E) interleukin-6 (IL-6) levels, and (F) histamine levels;  $N = 3$ ,  $* p < 0.05$ .

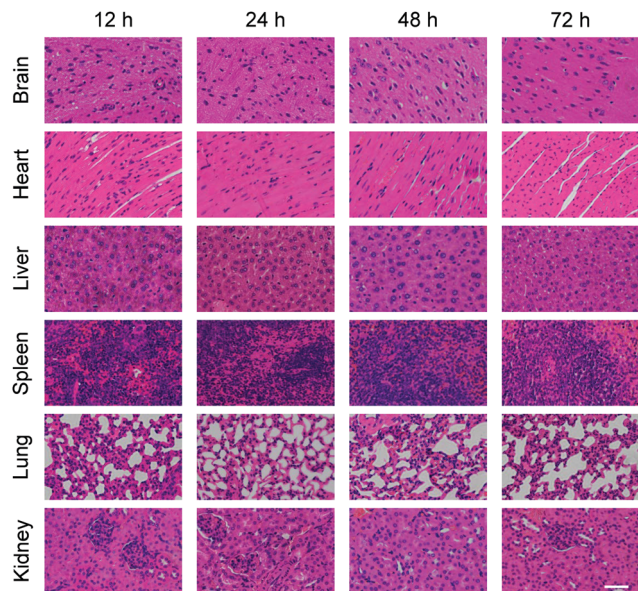


Fig. 6 Pathological section of main organs (brain, heart, liver, spleen, lungs and kidneys) separated from mice after injection with PTX free neutrocytes and different processing timescales. Scale bar, 50  $\mu\text{m}$ .

and is conducive to innate immunity. The C3 elevation is common in the early stage of acute inflammation.<sup>32</sup> After injection into the mice, the small fluctuation of C3 caused by neutrocytes indicates that the impact time of neutrocytes on the internal environment is short and can return to normal after 72 hours (Fig. 5D). Interleukin-6 (IL-6) can be used as a pro-inflammatory factor and anti-inflammatory factor. As an inflammatory marker, IL-6 is an important mediator of the acute inflammatory response.<sup>33</sup> After the injection of neutrocytes into

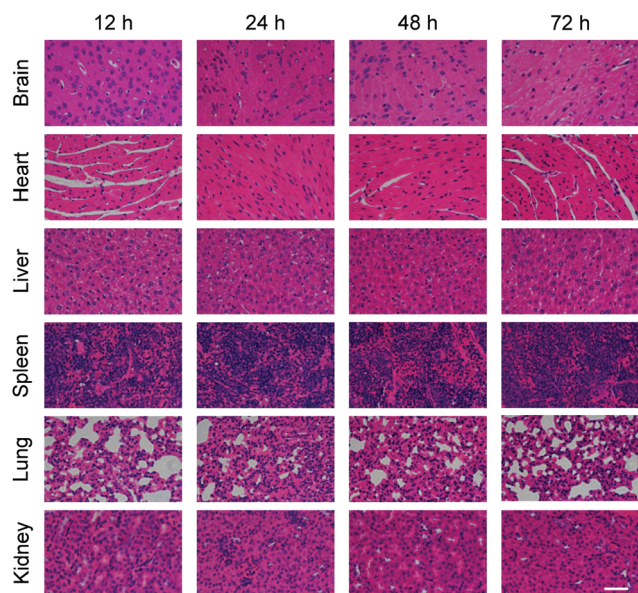


Fig. 7 Pathological section of main organs (brain, heart, liver, spleen, lungs and kidneys) separated from mice after injection with neutrocytes loaded with PTX and different processing timescales. Scale bar, 50  $\mu\text{m}$ .

the mice, the concentration of IL-6 decreased slightly, and gradually returned to a slightly higher level, which may be due to the early weak inflammation caused by many neutrocytes (Fig. 5E). Histamine is a central neurotransmitter involved in inflammatory responses and increases capillary permeability.<sup>34</sup> It can promote the entry of neutrocytes into tissues and provide conditions for neutrocytes to function. Histamine keeps a stable level from 0 to 72 h (Fig. 5F). A variety of cytokine tests showed that the injection of neutrocytes did not cause significant fluctuations of cytokines *in vivo*. After the injection of neutrocytes, the cytokines in the mouse serum remained stable. The above results show that the injection of neutrocytes does not cause serious side effects such as inflammation or an inflammatory factor storm, and it is safe as an injection.

Besides the concentration test of cytokines, pathological sections were made for the organs obtained after the dissection of mice in each experimental group. The results are shown in Fig. 6 and 7. Fig. 6 shows the pathological sections of mice injected with neutrocytes without PTX. Fig. 7 shows the pathological sections of mice injected with neutrocytes loaded with PTX. The optical microscope photographs of the pathological sections of six main organs showed that the morphology of each organ of the experimental group was normal and was not damaged by neutrocytes.

No differences were observed between pathological sections collected from mice injected with neutrocytes with PTX (Fig. 7) and without PTX (Fig. 6). In summary, the injection of neutrocytes into mice would not cause additional immune rejection, would not damage the normal tissues and organs of mice, and could be excreted along the general metabolic pathway. It should be noted that the toxicity evaluation of PTX-loaded neutrocytes *in vivo* was conducted in healthy mice according to previous reports,<sup>35,36</sup> the minor effect on the tissue histopathology, activity of liver, kidney, and immunity, suggesting that the treatment of PTX-loaded neutrocytes is safe in the mouse model. More in-depth studies for the evaluation of neutrocytes including the toxicity profile with an expanded period *in vivo*, metabolic pathway, and molecular mechanism will be carried out in future research.

## Conclusions

In conclusion, the toxicological properties of PTX-loaded neutrocytes administered by injection were evaluated for 72 hours upon the administration dose of  $3 \times 10^6$  neutrocytes per mouse according to a previous report. Compared with the widely acknowledged toxicity of PTX to the body, the data indicate that the delivery of PTX using neutrocytes caused minor effects on the functions of the immune system, liver, and kidney. Although these investigations were not carried out to support the advancement of clinical candidates, they reflected that the neutrocytes might be feasible for the safe delivery of therapeutic levels of the drug. Future studies will focus on the dynamic pharmacology, pharmacokinetics of various drug-loaded

neurobots with repeated administration, and the risk for juvenile animals.

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## Author contributions

Z. W. conceived the project. Z. W. supervised the studies. H. Z. and Z. L. prepared and characterized the neurobots. H. Z. and L. Z. performed the magnetic movement experiments. H. Z. and Y. J. drew the schematic illustrations. H. Z. and L. W. conducted the *in vivo* experiments. Z. W. and H. Z. interpreted data and wrote the manuscript. All the authors reviewed the manuscript.

## Conflicts of interest

There are no conflicts to declare.

## Notes and references

- W. Gao, R. Dong, S. Thamphiwatana, J. Li, W. Gao, L. Zhang and J. Wang, *ACS Nano*, 2015, **9**, 117–123.
- J. Li, B. Esteban-Fernández de Ávila, W. Gao, L. Zhang and J. Wang, *Sci. Robot.*, 2017, **2**, eaam6431.
- M. Sitti, *Nat. Rev. Mater.*, 2018, **3**, 74–75.
- T. Xu, W. Gao, L.-P. Xu, X. Zhang and S. Wang, *Adv. Mater.*, 2017, **29**, 1603250.
- T. Xu, F. Soto, W. Gao, R. Dong, V. Garcia-Gradilla, E. Magaña, X. Zhang and J. Wang, *J. Am. Chem. Soc.*, 2015, **137**, 2163–2166.
- R. Dong, Y. Cai, Y. Yang, W. Gao and B. Ren, *Acc. Chem. Res.*, 2018, **51**, 1940–1947.
- R. Dong, Y. Hu, Y. Wu, W. Gao, B. Ren, Q. Wang and Y. Cai, *J. Am. Chem. Soc.*, 2017, **139**, 1722–1725.
- F. Mou, Q. Xie, J. Liu, S. Che, L. Bahmane, M. You and J. Guan, *Natl. Sci. Rev.*, 2021, **8**, nwab066.
- M. Wan, H. Chen, Q. Wang, Q. Niu, P. Xu, Y. Yu, T. Zhu, C. Mao and J. Shen, *Nat. Commun.*, 2019, **10**, 966.
- M. Zhou, Y. Xing, X. Li, X. Du, T. Xu and X. Zhang, *Small*, 2020, **16**, 2003834.
- J. Yu, D. Jin, K.-F. Chan, Q. Wang, K. Yuan and L. Zhang, *Nat. Commun.*, 2019, **10**, 5631.
- X. Yang, W. Shang, H. Lu, Y. Liu, L. Yang, R. Tan, X. Wu and Y. Shen, *Sci. Robot.*, 2020, **5**, eabc8191.
- J. Liu, S. Yu, B. Xu, Z. Tian, H. Zhang, K. Liu, X. Shi, Z. Zhao, C. Liu, X. Lin, G. Huang, A. A. Solovev, J. Cui, T. Li and Y. Mei, *Appl. Mater. Today*, 2021, **25**, 101237.
- H. Wang and M. Pumera, *Chem. Rev.*, 2015, **115**, 8704–8735.
- F. Mou, X. Li, Q. Xie, J. Zhang, K. Xiong, L. Xu and J. Guan, *ACS Nano*, 2020, **14**, 406–414.
- T. Yu, A. G. Athanassiadis, M. N. Popescu, V. Chikkadi, A. Güth, D. P. Singh, T. Qiu and P. Fischer, *ACS Nano*, 2020, **14**, 13673–13680.
- M. Li, X. Wang, B. Dong and M. Sitti, *Nat. Commun.*, 2020, **11**, 3988.
- M. Pacheco, B. Jurado-Sánchez and A. Escarpa, *Angew. Chem., Int. Ed.*, 2019, **58**, 18017–18024.
- K. Yuan, B. Jurado-Sánchez and A. Escarpa, *Angew. Chem., Int. Ed.*, 2021, **60**, 4915–4924.
- B. Esteban-Fernández de Ávila, W. Gao, E. Karshalev, L. Zhang and J. Wang, *Acc. Chem. Res.*, 2018, **51**, 1901–1910.
- F. Zhang, R. Mundaca-Urbe, H. Gong, B. Esteban-Fernández de Ávila, M. Beltrán-Gastélum, E. Karshalev, A. Nourhani, Y. Tong, B. Nguyen, M. Gallot, Y. Zhang, L. Zhang and J. Wang, *Adv. Mater.*, 2019, **31**, 1901828.
- Y. Dai, X. Bai, L. Jia, H. Sun, Y. Feng, L. Wang, C. Zhang, Y. Chen, Y. Ji, D. Zhang, H. Chen and L. Feng, *Small*, 2021, **17**, 2103986.
- H. Zhang, Z. Li, C. Gao, X. Fan, Y. Pang, T. Li, Z. Wu, H. Xie and Q. He, *Sci. Robot.*, 2021, **6**, eaaz9519.
- S. Sun, H. Zeng, D. B. Robinson, S. Raoux, P. M. Rice, S. X. Wang and G. Li, *J. Am. Chem. Soc.*, 2004, **126**, 273–279.
- F. Zaefarian, M. R. Abdollahi, A. Cowieson and V. Ravindran, *Animals*, 2019, **9**, 63.
- R. J. Church and P. B. Watkins, *J. Dig. Dis.*, 2019, **20**, 2–10.
- A. Zinellu, P. Paliogiannis, C. Carru and A. A. Mangoni, *Clin. Exp. Med.*, 2021, DOI: [10.1007/s10238-021-00777-x](https://doi.org/10.1007/s10238-021-00777-x).
- B. R. Griffin, S. Faubel and C. L. Edelstein, *Ther. Drug Monit.*, 2019, **41**, 213–226.
- J. A. Baugh and R. Bucala, *Curr. Opin. Drug Discovery Dev.*, 2001, **4**, 635–650.
- P. Romagnani and C. Crescioli, *Clin. Chim. Acta*, 2012, **413**, 1364–1373.
- S. Pasquali and S. Mocellin, *Curr. Med. Chem.*, 2010, **17**, 3327–3336.
- J. R. Delanghe, R. Speeckaert and M. M. Speeckaert, *Pathology*, 2014, **46**, 1–10.
- M. Mihara, M. Hashizume, H. Yoshida, M. Suzuki and M. Shiina, *Clin. Sci.*, 2011, **122**, 143–159.
- L. Maintz and N. Novak, *Am. J. Clin. Nutr.*, 2007, **85**, 1185–1196.
- B. E.-F. De Ávila, P. Angsantikul, J. Li, M. Angel Lopez-Ramirez, D. E. Ramírez-Herrera, S. Thamphiwatana, C. Chen, J. Delezuk, R. Samakapiruk, V. Ramez, M. Obonyo, L. Zhang and J. Wang, *Nat. Commun.*, 2017, **8**, 272.
- M. Wan, Q. Wang, R. Wang, R. Wu, T. Li, D. Fang, Y. Huang, Y. Yu, L. Fang, X. Wang, Y. Zhang, Z. Miao, B. Zhao, F. Wang, C. Mao, Q. Jiang, X. Xu and D. Shi, *Sci. Adv.*, 2020, **6**, eaaz9014.