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## Introduction

Photodynamic therapy (PDT) is a clinically approved therapeutic modality that has been extensively applied to treat cancer because of its temporal–spatial controllability and minimal side effects.<sup>1–6</sup> The PDT mechanism relies on the conversion of an excited photosensitizer (PS) to molecular oxygen, under light irradiation, to generate ROS.<sup>7–12</sup> To date, various advanced PSs have been developed, but several obstacles impede their acceptance in biomedicine.<sup>13–16</sup> For example, PSs often undergo  $\pi$ – $\pi$  stacking, which reduces the singlet oxygen quantum yield.<sup>17,18</sup> Moreover, the inferior tissue penetration capability of the light sources currently used with PSs (<800 nm) reduces the PDT efficiency in deep-seated tumors.<sup>19–21</sup> Dark cytotoxicity in PSs is undesired and avoiding it is critical for reducing treatment side effects.<sup>22–24</sup> Thus, these challenges motivated us to

develop novel photosensitizers for a safer and more effective PDT process.

Coordination-driven self-assembly involves the spontaneous formation of metallacycles with tunable sizes and shapes.<sup>25–29</sup> Recently, the construction of metallacycle-based PSs has aroused continued interest in biomedicine.<sup>30–33</sup> Metallacycle-based PSs demonstrate unique advantages that can effectively address issues encountered in traditional PS systems. For example, their rigid macrocyclic structure can effectively preserve ROS production through an anti-quenching effect.<sup>34</sup> Furthermore, the presence of heavy atoms can improve PDT efficiency by promoting the intersystem crossing (ISC) process.<sup>35</sup> By incorporating well-designed fluorescent ligands, the absorption/emission wavelengths have been recently shifted into the near-infrared (NIR) region, which can improve the diagnosis and phototherapy of deep-seated tumors.<sup>36,37</sup> Despite these results, solving the inherent dark cytotoxicity of heavy metals remains largely unexplored, which greatly limited their translation from the laboratory to clinical use.

Herein, we explore molecular engineering on Ru acceptors to develop highly efficient and NIR absorptive/emissive (800–1000 nm) Ru(II) metallacycle-based PSs with low dark toxicity and high phototoxicity indices (PIs). A series of Ru(II) metallacycles (**Ru1–Ru4**) were designed using the self-assembly of fluorescent ligands (**L**) and tunable  $\pi$ -expanded ruthenium acceptors (**A1–A4**) (Scheme 1). With the advantage of long-wavelength absorption/emission, **Ru1–Ru4** were capable of deep-tissue fluorescence imaging and ROS production (~7 mm) compared with

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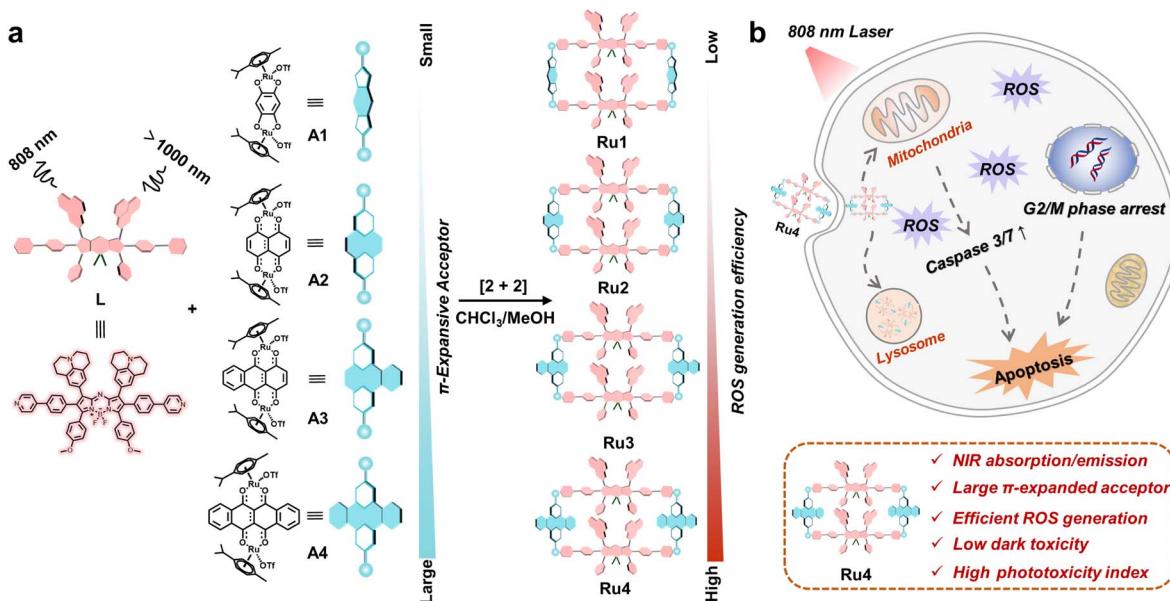
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**Scheme 1** Schematic illustration of the design and antitumor mechanism of **Ru1–Ru4**. (a) The design, chemical structure and properties of **Ru1–Ru4**, which are excited at 808 nm and emitted over 1000 nm. (b) The underlying antitumor mechanism illustrates the internalization of **Ru4** into A549 cells through the endocytic pathway and subsequently induces mitochondria-mediated apoptosis and cell cycle arrest in the G2/M phase.

visible-light-activated metallacycles ( $\sim 1 \text{ nm}$ ). Moreover, the *in vitro* anticancer results indicated that **Ru1–Ru4** displayed high selectivity between A549 and 16HBE cells, and remarkable anticancer activity even under hypoxic conditions. Among the Ru(II) metallacycles in this study, **Ru4** had the largest steric bulk and highest electron density at the acceptor site. It demonstrated the highest PI ( $\sim 146$ ) and ROS generation ( $\sim 20$ -fold compared to its ligand), which could be attributed to its smallest ligand bending angle ( $\theta, 149.4^\circ$ ), and the lowest singlet–triplet energy gap ( $\Delta E_{\text{ST}}$ , 0.62 eV) of the studied metallacycles. Therefore, **Ru4** was selected to investigate the anticancer mechanism in detail. *In vivo* studies on PDT efficacy were then conducted, which demonstrate that **Ru4** is a highly efficient PDT agent with low side effects.

## Results and discussion

### Design, synthesis and characterization of Ru(II) metallacycles

Aza-boron-dipyrromethene (aza-BODIPY) was selected as the donor precursor owing to its high molar extinction coefficient and tunable emission wavelength.<sup>38</sup> By introducing julolidine and anisole as strong electron-donating groups and phenyl-pyridine as the ruthenium coordinating group into the aza-BODIPY core, a fluorescent ligand (**L**) with NIR absorption/emission features was successfully synthesized (Scheme 1). As depicted in Fig. S1,<sup>†</sup> the energy bandgap in **L** was approximately 1.86 eV, which demonstrated that the emission wavelength of **L** was extended to the NIR-II range. Moreover, **L** also exhibited a low  $\Delta E_{\text{ST}}$  value (1.23 eV). The structure of **L** was confirmed using nuclear magnetic resonance (NMR) spectroscopy and mass spectrometry (Fig. S2–4<sup>†</sup>).

Metallacycles **Ru1–Ru4** were then constructed using the self-assembly of **L** with  $\pi$ -expansive ruthenium acceptors (**A1–A4**) (Scheme 1). **Ru1–Ru4** were characterized using  $^1\text{H}$ -NMR

spectroscopy, two-dimensional correlated spectroscopy (COSY), 2D-rotating frame Overhauser effect spectroscopy (ROESY) and electrospray ionization time-of-flight mass spectrometry (ESI-TOF-MS). The pyridyl proton  $\text{H}_1$  peak displayed an upfield shift (from 8.64 to 8.09 ppm for **Ru1**, 8.64 to 8.27 ppm for **Ru2**, 8.64 to 8.37 ppm for **Ru3**, and 8.64 to 8.43 ppm for **Ru4**) compared to the same peak in free **L** (Fig. 1a and S5–8<sup>†</sup>). The change in the chemical shift can be attributed to a loss of electron density when the ligand coordinated to the Ru(II) acceptor. The  $^1\text{H}$ – $^1\text{H}$  COSY and ROESY spectra further supported the unambiguous assignment of the proton peaks in these metallacycles (Fig. S9–16<sup>†</sup>). ESI-TOF-MS spectra for **Ru1–Ru4** were found to possess multiple prominent peaks for the assigned [2 + 2] assembly with charge states resulting from the loss of the triflate ( $\text{OTf}^-$ ) counterions (Fig. 1b and S17–20<sup>†</sup>). Peaks at  $m/z = 831.38, 856.23, 881.40$ , and 906.64 corresponded to  $[\text{M} - 4\text{OTf}]^{4+}$  for **Ru1–Ru4**, respectively. All the assigned peaks matched well with simulated theoretical distributions, indicating that **Ru1–Ru4** possessed the expected 1 : 1 ratio of building blocks.

### Photophysical and photodynamic properties and stability studies

The ultraviolet-visible (UV-vis) absorption spectra of **Ru1–Ru4** are shown in Fig. 2a. Free **L** exhibited two broad absorption bands with peaks at  $\sim 650$  and 830 nm. After **L** was coordinated with the Ru(II) acceptors, and the absorption peak at 830 nm was red-shifted (24, 38, 7, and 15 nm for **Ru1**, **Ru2**, **Ru3**, and **Ru4**, respectively). The molar absorption coefficients ( $\epsilon$ ) of **Ru1–Ru4** were  $1.25 \times 10^4, 2.19 \times 10^4, 1.76 \times 10^4$ , and  $1.70 \times 10^4 \text{ M}^{-1} \text{ cm}^{-1}$ , respectively (Fig. S21<sup>†</sup>). Furthermore, the maximum emission wavelengths of **L** and **Ru1–Ru4** in dichloromethane

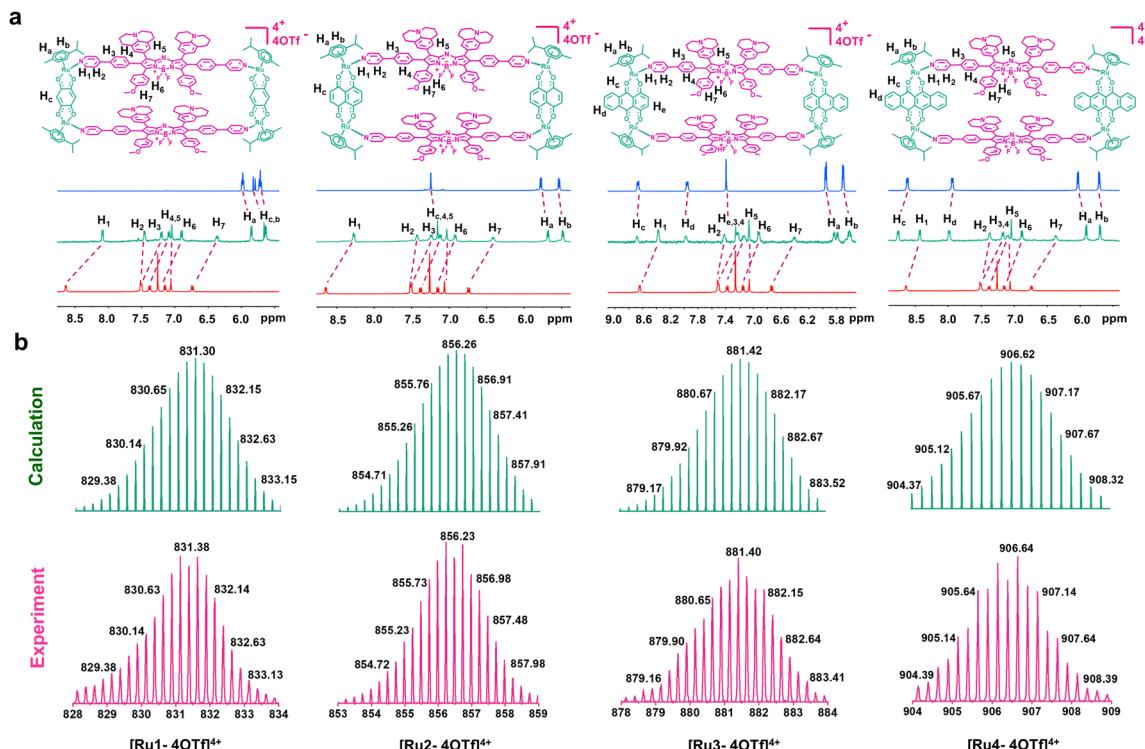


Fig. 1 Chemical structure and characterization of Ru1–Ru4. (a) Chemical structures and partial <sup>1</sup>H NMR spectra of Ru1–Ru4. (b) Experimental (magenta) and calculated (green) ESI-TOF-MS spectra of Ru1–Ru4.

were 1008, 1108, 1050, 1093, and 1085 nm, respectively (Fig. 2b). The bathochromic shift of the absorption and emission wavelengths for **Ru1–Ru4** could be attributed to the N–Ru coordination bond formation, which facilitated intramolecular charge transfer (ICT) in **L**. The chemical stability and photostability of **Ru1–Ru4** were assessed by monitoring changes in the absorption spectra. As depicted in Fig. S22–24,<sup>†</sup> **Ru1–Ru4** exhibited high chemical stability in the medium and a high photostability under continuous laser irradiation. Tissue-mimicking materials (1% intralipid) were used to assess the deep optical penetration ability of **Ru1–Ru4**, with a previously reported visible-light absorption/emission counterpart (**Ru-M**, Ex: 450 nm)<sup>39</sup> used as the control. The fluorescence signals from **Ru1–Ru4** could be observed at a penetration depth of 7 mm owing to the long absorption/emission wavelengths of **Ru1–Ru4**. Conversely, the FL signal of **Ru-M** became almost imperceptible when the penetration depth increases to 1 mm (Fig. 2c and S25<sup>†</sup>).

To investigate the effect of different  $\pi$ -expanded Ru(II) acceptors on the PDT potential of the metallacycles, 2',7'-dichlorodihydrofluorescein diacetate (DCFH-DA) was used to evaluate their ROS-production abilities.<sup>40</sup> **L** or **Ru1–Ru4** were co-incubated with DCFH-DA and irradiated at 488 nm for 60 s. The fluorescence intensity at 525 nm increased significantly with the irradiation time. Notably, the DCF fluorescence intensity increased 31-fold after 60 s of laser irradiation in the presence of **Ru4**, which was higher than that of **L** (1.5-fold) or other Ru(II) metallacycles (4-fold for **Ru1**, 9-fold for **Ru2**, and 18-fold for **Ru3**) (Fig. 2d and S26<sup>†</sup>). Additionally, 1,3-diphenylisobenzofuran (DPBF), hydroxyphenyl fluorescein (HPF) and dihydroethidium (DHE) were used

to detect  $^1\text{O}_2$ , hydroxyl radicals ( $\text{OH}^\bullet$ ), and superoxide anions ( $\text{O}_2^-$ ), respectively. Under laser irradiation, the absorbance of DPBF at 416 nm and the fluorescence intensity of HPF at 516 nm remained relatively unchanged, while the fluorescence intensity of DHE at 595 nm significantly increased (Fig. S27–29<sup>†</sup>). Among them, the increase in  $\text{O}_2^-$  generated by **Ru4** (3.0-fold) exceeded that of **Ru1** (1.2-fold), **Ru2** (1.5-fold), and **Ru3** (2.6-fold). To explore the anti-quenching ROS ability of the Ru(II) metallacycles, DCFH-DA was incubated with **L** or **Ru4**, and the emission spectra were recorded in dimethyl sulfoxide/water. When the water fraction ( $f_w$ ) was increased from 0% to 90%, the fluorescence intensity of DCF induced by **Ru4** increased rapidly compared with the intensity observed in **L** and DCFH-DA solutions (Fig. 2e and S30<sup>†</sup>). To evaluate whether the metallacycles can efficiently generate ROS in deep tissue, DCFH-DA incubated with either **Ru4** or **Ru-M** was placed under 1% intralipid and exposed to laser irradiation. As shown in Fig. 2f, g and S31,<sup>†</sup> **Ru4** efficiently generated ROS, even when the depth increased to 7 mm. In comparison, **Ru-M** cannot generate ROS beyond depths of 1 mm. Subsequently, we evaluated the capacity of **Ru4** to generate ROS at the cellular level. After co-incubation with DCFH-DA, A549 cells treated with **Ru4** and exposed to 808 nm laser irradiation displayed strong green fluorescence (Fig. 2h). A549 cells co-incubated with **Ru4** and DHE exhibited typical red fluorescence under laser irradiation, indicating that DHE was exposed to  $\text{O}_2^-$  (Fig. S32<sup>†</sup>). These results suggested that **Ru4**, which was a sterically bulky and electron-rich acceptor, can efficiently generate ROS.



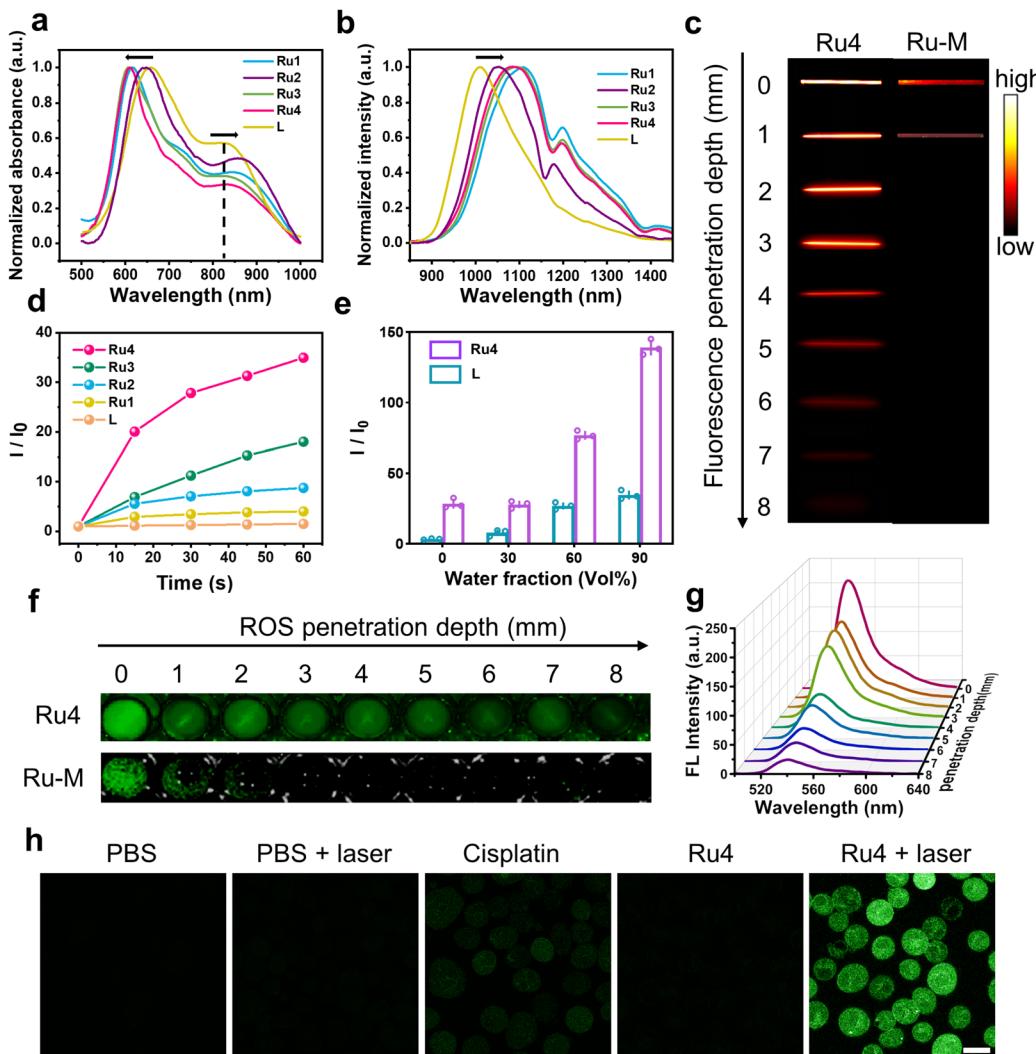


Fig. 2 *In vitro* photophysical properties of Ru1–Ru4. (a) Normalized absorbance and (b) emission spectra ( $\lambda_{\text{ex}} = 808 \text{ nm}$ ) of Ru1–Ru4 in DCM. (c) Fluorescence images of Ru4 (10  $\mu\text{M}$ ) and Ru-M (10  $\mu\text{M}$ ) at various depths under 808 nm laser irradiation. (d) Comparison between the fluorescence intensity of DCFH-DA incubated with L (20  $\mu\text{M}$ ) and Ru1–Ru4 (10  $\mu\text{M}$ ), respectively. (e) Comparison between the ROS generation capacity of L (20  $\mu\text{M}$ ) and Ru4 (10  $\mu\text{M}$ ) with different  $f_w$ . (f) The DCF fluorescence imaging of Ru4 (10  $\mu\text{M}$ ) and Ru-M (10  $\mu\text{M}$ ) at various depths. (g) Fluorescence spectra at different depths to monitor ROS generation by Ru4 under 808 nm laser irradiation. (h) Inverted fluorescence microscope images of A549 cells incubated with DCFH-DA after various treatments. Scale bar: 20  $\mu\text{m}$ .

### In vitro anticancer activity

Based on the promising photophysical properties, the anti-cancer efficacies of Ru1–Ru4 were evaluated using 3-[4,5-dimethylthiazol-2-yl]-2,5-diphenyl tetrazolium bromide (MTT) assays of A549, cisplatin-resistant A549 (A549/DDP), and 16HBE cells. The cells were co-incubated with different concentrations of Ru1–Ru4, A1–A4, and L and further treated with or without light, and the results are summarized in ESI Tables 1 and 2.† Under dark conditions, with the exception of Ru2, the metallacycles were inactive against A549 cells. Ru4 exhibited the lowest cytotoxicity ( $\text{IC}_{50} = 305.6 \mu\text{M}$ ), which could be attributed to the steric bulk and the electron-rich acceptor properties preventing exchange with biomolecules.<sup>41–43</sup> In contrast, under light irradiation, Ru4 was the most effective compound for the eradication of A549 cells ( $\text{IC}_{50} = 3.6 \mu\text{M}$ ). Ru1–Ru4 exhibited

good anticancer activity against cisplatin-resistant A549 cells and maintained high phototoxicity even under hypoxic conditions. Specifically, the PI of Ru4 can reach as high as 146. In addition, Ru4 demonstrated good selectivity for A549 cells with a calculated selectivity index (SI) of 2.7, which was higher than that of cisplatin (0.4), and Ru1–Ru3 (1.4, 1.0, and 0.9). These results indicated that Ru4 was superior to cisplatin and other metallacycles in maintaining excellent antitumor effects, being selective between A549 and 16HBE cells and possessing a high PI.

### Theoretical calculations of metallacycles

These promising results inspired us to explore the relationship between the macrocycle structure and the photophysical properties using theoretical calculations. The geometric

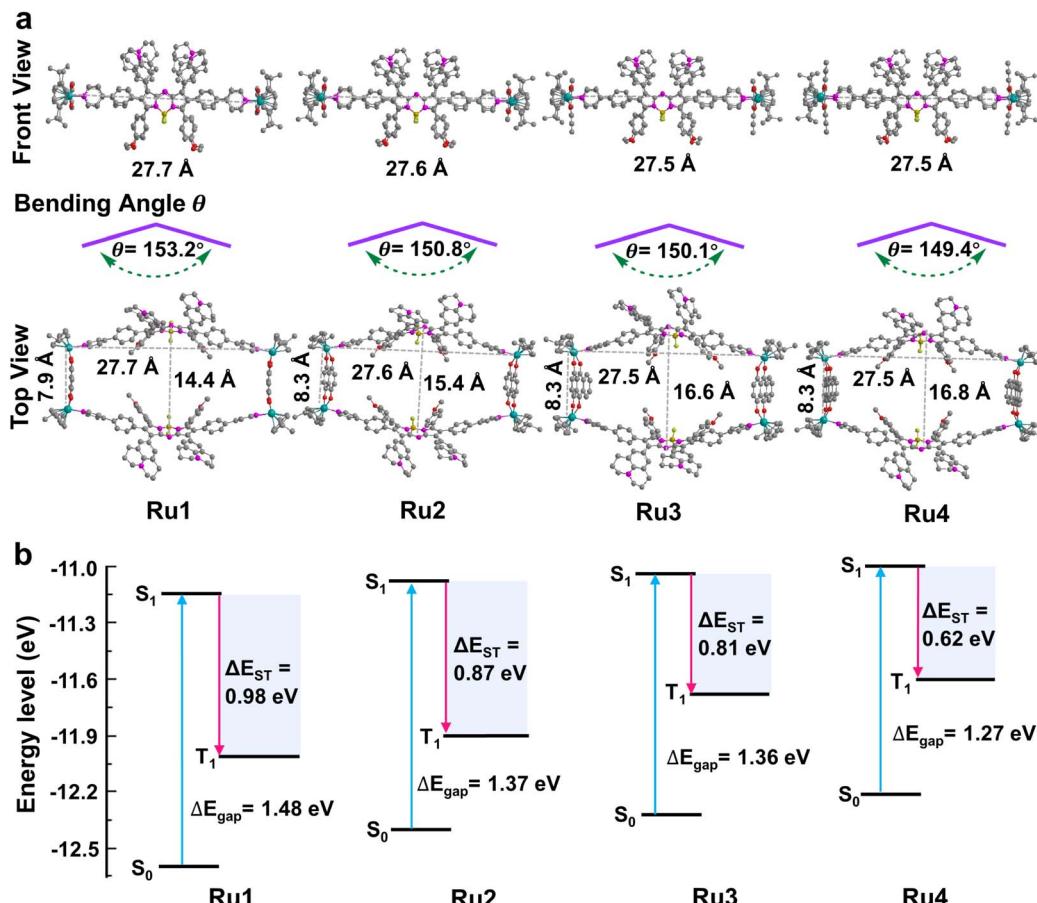


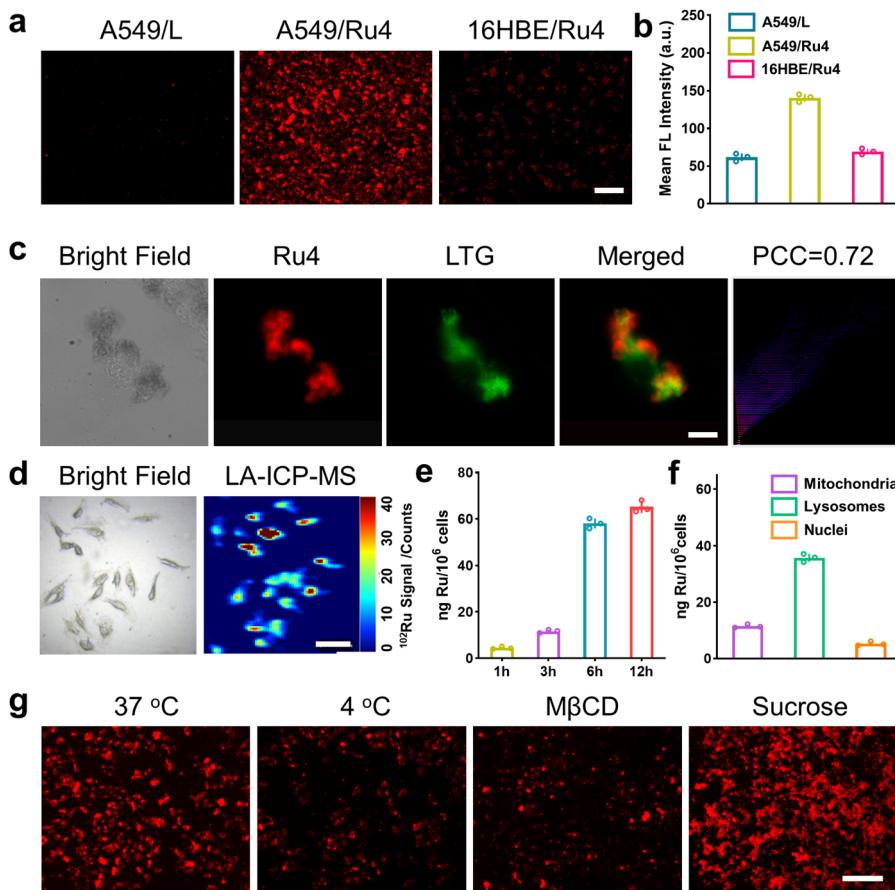
Fig. 3 Theoretical calculations of Ru1–Ru4. (a) Optimized structure of metallacycles and the bending angle  $\theta$  of L in metallacycles; hydrogen atoms in the structure are omitted for clarity. (b) Calculated HOMO and LUMO of Ru1–Ru4 at the B3LYP/6-31G(d) level. Excitation energy of the excited triplet state was determined under the B3LYP/6-31G(d) level by time-dependent DFT.  $\Delta E_{\text{gap}}$  and  $\Delta E_{\text{ST}}$  between singlet and triplet states are also presented in the figure.

conformations of **Ru1–Ru4** were optimized using density functional theory (DFT) with a 6-31G(d) basis set in Gaussian 16.<sup>44–46</sup> The rectangular structure in **Ru4** ( $27.5 \times 16.8 \text{ \AA}$ ) was larger than that in **Ru1** ( $27.7 \times 14.4 \text{ \AA}$ ), **Ru2** ( $27.6 \times 15.4 \text{ \AA}$ ), and **Ru3** ( $27.5 \times 16.6 \text{ \AA}$ ) (Fig. 3a). The bending angle  $\theta$  (dihedral angle  $\angle N1-N2-B1-N3$  that represents the angle between the phenylpyridine modified groups on both sides of the azabODIPY core) decreased in the order of free L ( $176.0^\circ$ ) > **Ru1** ( $153.2^\circ$ ) > **Ru2** ( $150.8^\circ$ ) > **Ru3** ( $150.1^\circ$ ) > **Ru4** ( $149.4^\circ$ ), which was expected, given the large cavity in the structure of **Ru4** (Fig. 3a and S33†). These results suggested that the increase in the degree of  $\pi$ -expansion of the Ru(II) acceptors enhanced the degree of twist in L, which improved the ICT effect and generation of ROS.<sup>47</sup> The electronically excited structures and related photophysical properties were computed using a TD-DFT method. As shown in Fig. 3b and Table S3,† the HOMO–LUMO energy gaps of L, **Ru1**, **Ru2**, **Ru3**, and **Ru4** were determined to be 1.86, 1.48, 1.37, 1.36, and 1.27 eV, respectively. **Ru1–Ru4** exhibited a lower  $\Delta E_{\text{gap}}$  than free L owing to the introduction of Ru-pyridyl coordination bonds and the electron-deficient nature of the transition metal.  $\Delta E_{\text{ST}}$  was also investigated to evaluate the ROS generation efficiency. As shown in

Fig. 3b, **Ru4** has the smallest  $\Delta E_{\text{ST}}$  (0.62 eV) of the Ru(II) metallacycles, suggesting that the sterically bulky and electron-rich Ru(II) acceptor can enhance the ISC of **Ru4** and improve the efficiency of ROS production. The theoretical calculations were in good agreement with the experimental data and the results supported our design concept that efficient ROS generation can be achieved by engineering the acceptor in Ru(II) metallacycles.

#### Evaluation of cell uptake and localization of Ru4

We firstly evaluated the octanol/water partition coefficient ( $\log P_{\text{o/w}}$ ) of **Ru1–Ru4** and L.<sup>48</sup> As shown in Table S4,† all these compounds demonstrated similar  $\log P$ . The cellular uptake and localization of **Ru4** were further investigated using A549 cells. After incubation with **Ru4**, the cells showed a strong red fluorescence signal and the corresponding mean fluorescence intensity increased with the incubation time (Fig. S34†). Moreover, **Ru4** demonstrated a much stronger fluorescence signal than L in A549 cells as well as in normal 16HBE cells (Fig. 4a, b and S34†). These results could be attributed to the unique shape and positive charge of the metallacycles, which are beneficial for cell uptake and selectivity towards A549 cells. An



**Fig. 4** Cellular uptake and localization of **Ru4** in A549 cells. (a) Fluorescence images of cells treated with **Ru4** (10  $\mu$ M) and L (20  $\mu$ M), respectively. Scale bar: 300  $\mu$ m. (b) Semi-quantitative analysis of the fluorescence imaging in Fig. 4a. (c) Colocalization assay of **Ru4** (10  $\mu$ M) using LTG. Scale bar: 10  $\mu$ m. (d) LA-ICP-MS imaging of  $^{102}\text{Ru}$  in A549 cells incubated with **Ru4** (10  $\mu$ M). Scale bar: 50  $\mu$ m. (e) ICP-MS results showing the Ru content in A549 cells over time. (f) Subcellular distribution of Ru concentration in A549 cells measured using ICP-MS. (g) Cellular uptake mechanism studies of **Ru4** (10  $\mu$ M) at 4  $^{\circ}$ C and 37  $^{\circ}$ C, M $\beta$ CD and sucrose, respectively. Scale bar: 300  $\mu$ m.

intracellular localization test was performed and, after 9 hours of incubation, the red fluorescence signal of **Ru4** and green fluorescence from LysoTracker® Green (LTG) overlapped, showing a Pearson correlation coefficient (PCC) of 0.72 (Fig. 4c and S35 and 36 $\dagger$ ). Laser ablation inductively coupled plasma MS (LA-ICP-MS) for the A549 cells also showed a strong signal corresponding to  $^{102}\text{Ru}$  (Fig. 4d). Moreover, ICP-MS verified that **Ru4** uptake increased with incubation time and reached 65.2 ng per million cells at 12 h (Fig. 4e). The calculated Ru content in the lysosomes was 35.8 ng per million cells, which was higher than that observed in the mitochondria and the nuclei (Fig. 4f). To investigate the cellular uptake mechanism of **Ru4**, cellular fluorescence imaging was done at low temperatures or with various metabolic and endocytic inhibitors. The intracellular red fluorescence of **Ru4** dropped significantly at 4  $^{\circ}$ C or with metabolic inhibitors, suggesting that **Ru4** was internalized into the cell through energy-dependent processes (Fig. 4g and S37 $\dagger$ ). Pretreatment with methyl- $\beta$ -cyclodextrin (M $\beta$ -CD) resulted in a decrease in the intracellular red fluorescence intensity, indicating that **Ru4** was internalized into cancer cells *via* the energy-dependent caveolae-mediated endocytosis pathway.

### Cell death mechanisms

Based on the excellent anticancer activity of **Ru4**, we investigated the mechanisms of cell death. A549 cells treated with **Ru4** under 808 nm laser irradiation showed 35.6% apoptosis, indicating the enhanced cytotoxicity of **Ru4** (Fig. 5a). To visualize the effect of **Ru4** on cell death, co-staining of calcein AM and propidium iodide was performed to distinguish between live (green) and dead (red) cells. $^{49}$  As for **Ru4** or laser irradiation alone, strong green fluorescence from calcein AM and weak red fluorescence from propidium iodide were observed (Fig. S38 $\dagger$ ). In comparison, the combination of **Ru4** and the laser together results in a strong propidium iodide signal, indicating the high ROS efficacy of **Ru4**. As **Ru4** mainly accumulated in lysosomes, acridine orange (AO) was used to evaluate lysosomal membrane integrity. $^{50}$  As shown in Fig. 5b and S39, $\dagger$  when A549 cells were incubated with **Ru4** and subjected to laser irradiation, the red fluorescence produced by AO largely disappeared. **Ru4** is also partially localized in the mitochondria, and JC-1 dye was used to evaluate the mitochondrial membrane potential (MMP) after PDT. Compared with the control groups, the **Ru4**-treated group under 808 nm laser irradiation showed intense green

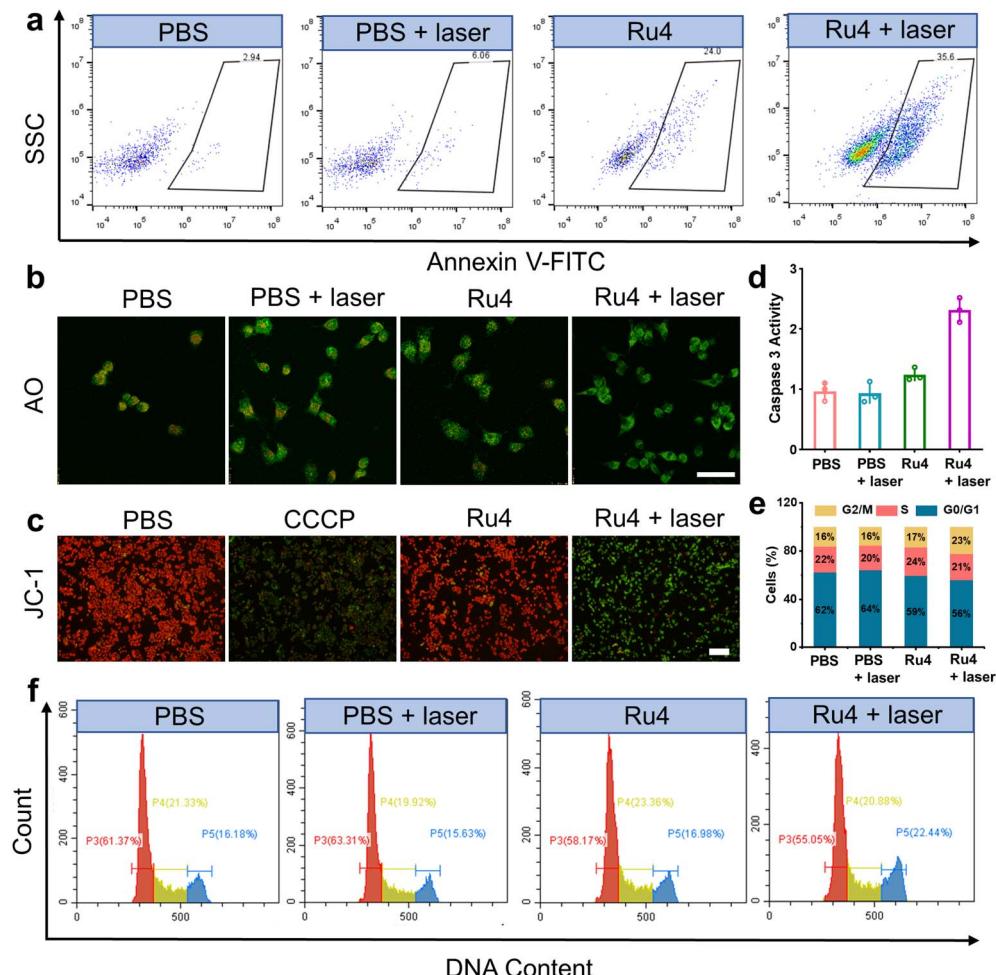


Fig. 5 Cell death mechanisms of **Ru4** in A549 cells. (a) Flow cytometry measuring cell apoptosis of A549 cells with PBS, PBS + laser, **Ru4** (10  $\mu$ M) and **Ru4** (10  $\mu$ M) + laser. (b) Confocal fluorescence imaging of AO stained A549 cells after different treatments. Scale bar: 20  $\mu$ m. (c) Fluorescence imaging of JC-1 labelled A549 cells treated with PBS, CCCP (10  $\mu$ M), **Ru4** (10  $\mu$ M), and **Ru4** (10  $\mu$ M) + laser. (d) Caspase 3 activity in A549 cells after various treatments. (e) Histogram depicting cell cycle distribution after various treatments. (f) Flow cytometry analysis of the cell cycle of A549 cells after various treatments.

fluorescence (Fig. 5c and S40†). Mitochondrial damage often triggers downstream activation of the caspase cascade and apoptosis. As shown in Fig. 5d, the **Ru4**-treated group under laser irradiation showed a 2.2-fold increase in caspase 3 activity as compared to that in the **Ru4** alone group. Subsequently, flow cytometry results indicated that the number of cells accumulated in the G2/M phase increased from 16.98% to 22.44% upon treatment with **Ru4** and laser irradiation. Conversely, the number of cells in the S phase hardly increased (Fig. 5e and f). These results demonstrated that **Ru4** under laser irradiation induced cell cycle arrests in the G2/M phase under laser irradiation.

### In vivo anticancer application

The outstanding *in vitro* results of **Ru4** prompted us to further explore the feasibility of anti-tumor activity in the A549 tumor-bearing nude mice. When the xenograft tumor volumes reached around 100  $\text{mm}^3$ , the mice were randomly

divided into five groups: (i) physiological saline (group 1), (ii) physiological saline and laser irradiation (group 2), (iii) cisplatin (group 3), (iv) **Ru4**-injected only (group 4), and (v) **Ru4**-injected and laser irradiation (group 5). For group 5, 12 hours after intratumoral injection of metallacycle **Ru4** (1 mg **Ru4** per kg body weight), the A549 tumor was irradiated with a laser (808 nm, 1 W  $\text{cm}^{-2}$ , and 10 min). The same laser dose and the same **Ru4** dose were used for group 2 and group 3. The tumor volumes and the body weight of the mice were recorded at 2 day intervals for a total of 16 days. As shown in Fig. 6a, b and S41,† the tumor volume of the **Ru4** group treated with the laser reduced to 95% of the original volume on the 16 day, while the tumor volume of the mice treated with cisplatin and only **Ru4** increased 7-fold and 9-fold respectively in the same period. Importantly, no significant weight loss was observed during the treatment (Fig. 6c), indicating that **Ru4** has minimal side effects upon treatment. Moreover, the tumors treated with the **Ru4** + laser group can effectively prolong the survival time of mice compared with

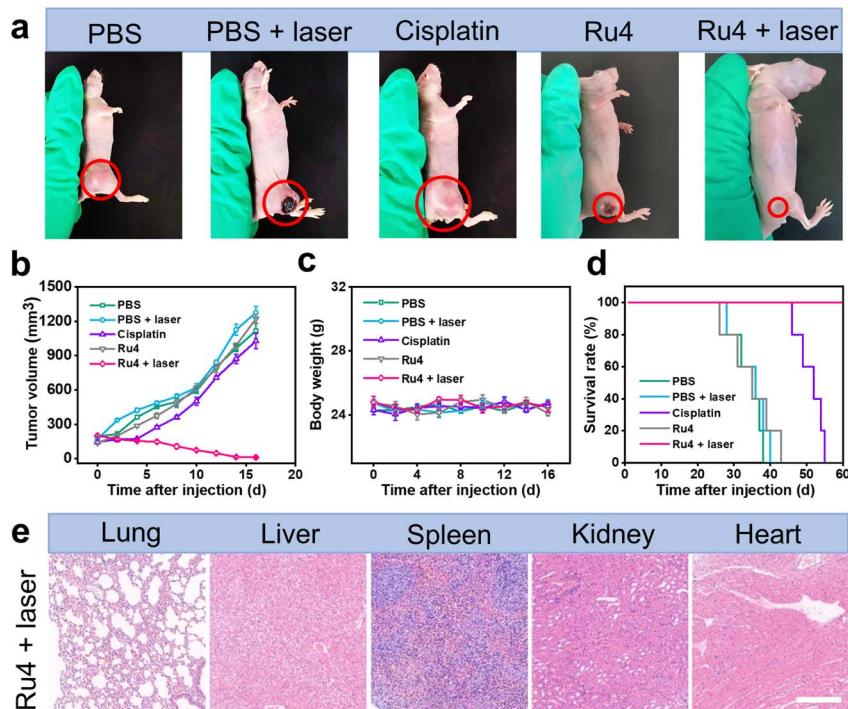


Fig. 6 *In vivo* PDT effect of Ru4 in A549 tumor-bearing mice. (a) Representative photographs of A549 tumors treated with PBS, PBS + laser, cisplatin (10  $\mu$ M), Ru4 (10  $\mu$ M), and Ru4 (10  $\mu$ M) + laser (808 nm, 1 W  $\text{cm}^{-2}$ ). (b) Tumor growth inhibition curves. (c) Body weight change curves of mice after various treatments. (d) Survival rate of the A549 tumor-bearing mice after different treatments. (e) Histological examination of the primary organs of mice treated with Ru4 (10  $\mu$ M) + laser (808 nm, 1 W  $\text{cm}^{-2}$ ). Scale bar: 50  $\mu$ m.

the other tested groups (Fig. 6d). In addition, histological examination of the major organs (lung, liver, spleen, kidney and heart) of mice by hematoxylin and eosin (H&E) staining showed no obvious organ damage (Fig. 6e and S42<sup>†</sup>). Overall, **Ru4** is effective for the treatment of cancer by PDT *in vivo*, and has no side effects.

## Conclusions

In conclusion, we applied molecular engineering to Ru(II) acceptors in metallacycles to develop a series of metallacycle-based PSs. Among them, **Ru4** exhibited the lowest dark toxicity, strongest ROS generation ability, highest PI, and excellent deep-tissue fluorescence and ROS penetration. Theoretical calculations verified that introducing sterically bulky and electron-rich moieties at the Ru(II) acceptor position can reduce the bending angle of the ligand and  $\Delta E_{\text{ST}}$  of the metallacycles. In addition, we also studied the antitumor mechanism *in vitro* and antitumor effect *in vivo* of **Ru4** thoroughly. Therefore, this study provides a convenient and important strategy for developing high-efficiency metallacycle-based photosensitizers for potential clinical applications.

## Data availability

All the data supporting this article have been included in the main text and the ESI.<sup>†</sup>

## Author contributions

Yao Sun and P. J. S. conceived the project and designed the experiments. C. L., L. T. and Chang Liu designed, synthesized and characterized the materials. J. Y. and W. T. carried out the theoretical calculation. C. L., L. T. and Y. X. performed the *in vitro* and *in vivo* studies. Yao Sun, J. L., Yan Sun and P. J. S. wrote the manuscript. All authors analyzed and discussed the results and have given approval to the final version of the manuscript.

## Conflicts of interest

There are no conflicts to declare.

## Acknowledgements

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