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A multi-valent polymyxin-based fluorescent probe for the detection of Gram-negative infections†

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A multi-branched fluorogenic probe for the rapid and specific detection of Gram-negative bacteria is reported. Three Gram-negative-targeting azido-modified polymyxins were clicked onto a trivalent scaffold functionalised with the environmental green-emitting fluorophore 7-nitrobenz-2-oxa-1,3-diazole. The probe allowed wash-free detection of target bacteria with increased sensitivity and lower limits of detection compared to mono-valent probes.

Introduction

Bacterial infections (from both antibiotic-resistant and susceptible species) remain a major cause of death globally, with an estimated 13.7 million infection-related deaths in 2019 (of which approx. 10 million were from sepsis).¹ The most predominant organisms (in order of deaths caused, excluding TB) are *Staphylococcus aureus*, *Escherichia coli*, *Streptococcus pneumoniae*, *Klebsiella pneumoniae*, *Pseudomonas aeruginosa* and *Acinetobacter baumannii*, four of which are Gram-negative and are responsible for many life-threatening infections, such as sepsis, wound infections, urinary tract infections and pneumonia.^{2–4}

Unfortunately, the accurate and rapid identification of infections remains a challenge as current diagnostic techniques often rely on invasive biopsies and microbial culture, which causes a delay between patient sampling and diagnoses.⁵ Consequently, pre-emptive treatments are commonly employed, which typically leads to overuse of broad-spectrum antibiotics with serious adverse side-effects (*e.g.* deafness with aminoglycosides,⁶ nephrotoxicity with glycopeptides,⁷ *etc.*). This approach also promotes the utilisation of “last resort” highly potent antibiotics thereby driving the antimicrobial resistance problem.^{8,9}

The development of tools and methodologies for the rapid and accurate identification of pathogenic agents is crucial to prevent this “butterfly effect”, and therefore allow early bedside decision of tailored treatments. One approach to achieve this goal is to create targeted reporters that can label pathogens and be visualised in real time, for example by the attachment of a fluorophore to a targeting ligand with specific affinity for a class of pathogens,^{10–13} generating highly pathogen-specific imaging probes with high potential for clinical diagnosis.^{14–17}

Antibiotics specific to classes of pathogens (*i.e.* targeted to a specific Gram status) have become popular targeting ligands for the design of fluorescent probes to detect bacterial infections,^{18–21} with broad applications in disease diagnostics, resistance mechanisms studies and drug susceptibility assessment.^{22–26} Probes targeting Gram-negative bacteria^{27–30} specifically can be designed using polymyxins, a class of naturally occurring cationic cyclic lipopeptides. These compounds selectively bind to the outer membrane of Gram-negative bacteria *via* interactions with lipid A, a key component of the lipopolysaccharide (LPS).^{19,31,32} The long aliphatic chain of unmodified polymyxins is able to insert into the membrane giving enhanced (entropically driven) binding. This chain can be removed to develop non-cytotoxic imaging probes while keeping the cyclic peptide structure, essential for specific membrane recognition, thus enabling the development of targeted imaging probes for Gram-negative bacteria. In previous work, “switch-on” fluorescent probes, designed by derivatization of the antibiotic polymyxin B (PMB) with green- or red-emitting solvato-fluorogenic dyes, were used to detect Gram-negative pathogens with good

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(see ESI[†]). The active ester was reacted with **2** in presence of DIPEA to yield the azide module **5** (Scheme 1). The tri-branched scaffold was based on a tris(hydroxymethyl)aminomethane (TRIS) scaffold that was modified with three propargyl groups to enable CuAAC. Thus, the amine group of TRIS was functionalised with the commercially available ethylene glycol linker BocNH-(EG)₂-CO₂H, with amide bond formation on this hindered amine position efficiently promoted by the coupling agent EEDQ under microwave irradiation, cleanly affording **7** (Scheme 2). The hydroxyl groups were alkylated with propargyl bromide under microwave heating to yield the corresponding tris-alkyne, which was then deprotected using TFA (see ESI[†]). The resulting crude amine was used in an SNAr reaction with NBD-Cl to give the NBD-functionalised fluorescent tri-branched scaffold **8** in a 4-step sequence with only a single final purification needed (34% yield over 4 steps). Finally, CuAAC between the tris-alkyne platform and three equivalents of **5** was performed using the CuI/THPTA catalytic system under microwave irradiation. Completion of the reaction was monitored using LC-MS to maximise the formation of the tri-functionalised compound over the partially (mono- or bi-) functionalised scaffold. The final bacterial-targeting probe **NBD-Tris(PMB7)** was then purified by preparative RP-HPLC (see ESI[†]). The copper-catalysed azide-alkyne cycloaddition (CuAAC) provided a clean, efficient, and high yielding reaction, even when constructing multi-branched scaffolds with biologically complex ligands.

The optical properties of the tri-branched probe **NBD-Tris(PMB7)** were initially investigated to evidence their emissive character in lipophilic media. The compound showed a similar behaviour to other known NBD derivatives (ESI[†], Fig. S1) and to the monomeric probe **NBD-PMB9**,³³ with an intense absorption band at 464 nm, and broad green emission ($\lambda_{\text{max}} = 545$ nm) (Fig. 1, top). The large band tailing beyond 600 nm and its large Stokes' shift are characteristic of the NBD fluorophore.



Fig. 1 Top: Normalised absorption (continuous line) and emission (dashed line) spectra of **NBD-Tris(PMB7)** in DMSO. Bottom: Evolution of the fluorescence intensity of solutions of **NBD-Tris(PMB7)** (5 μ M) with increasing percentages of DMSO in PBS upon excitation at 475 nm.

We explored the sensitivity of the probe to the solvation environment by increasing the DMSO content of aqueous solutions of the probe. DMSO was selected to generate different lipophilic environments, whilst maintaining good probe solubility. The absorption and emission wavelengths were practically unaffected by the polarity and proticity changes (Fig. S2, ESI[†]), however, in accordance with the well-known solvato-fluorogenic character of NBD (*i.e.* known sensitivity to the



Scheme 2 Synthesis of the tri-branched polymyxin probe **NBD-Tris(PMB7)**. Reagents and conditions: (i) BocNH-(EG)₂-CO₂H, EEDQ, EtOH, 100 °C (MW), 2 h. (ii) Propargyl bromide, KOH, DMF, 120 °C (MW), 4 h. (iii) TFA, CH₂Cl₂, r.t., 1 h. (iv) NBD-Cl, Et₃N, MeOH, r.t., 16 h. (v) **5**, CuI, THPTA, DMF, 70 °C (MW), 1 h.



hydrogen bonding. As such, in **NBD-PMB9**, the fluorophore is more likely to be exposed to unfavourable interactions with the peptide and with water molecules, which may limit the fluorescence increase. In contrast, with two diethylene glycol spacers attached *via* the TRIS platform, the NBD moiety in **NBD-Tris(PMB7)** may be more sterically shielded from unfavourable interactions, therefore leading to a stronger brightness increase. This is a further benefit of the tri-branched structure in our probe design, and allowed wash-free, selective fluorescent labelling of Gram-negative bacteria with low levels of cross-labelling. In bacterial assays, the tri-branched probe also showed higher sensitivity compared to the monovalent analogues based on **PMB9** and the shorter **PMB7** targeting ligands. This allowed up to 4-times more sensitive detection of Gram-negative bacteria, promoted synergistically by the presence of three PMB binding units and the greater solvato-fluorogenic properties of the NBD unit.

This new tri-branched tool could open the way to more precise optical detection of Gram-negative infections. Future iterations of the tri-branched probes could lead to the incorporation of three fluorophores to increase signal amplification, and the synthesis of multi-modal probes with additional diagnostic or therapeutic functionality. This also warrants further investigation of tri-branched fluorescent probes on *in vivo* infection models and clinical samples.

Author contributions

Conceptualization, M. K., M. R.-R., R. S., M. B.; synthesis M. K., M. R.-R., J. C., M. S., A. M.-F, photophysical characterization M. K.; biological validation, R.S.; writing – original draft preparation, M. K., R. S., M. R.-R, J. C.; writing – review and editing, M. K., R. S., M. R.-R., J. C., A. M.-F., M. B. All authors have read and agreed to the published version of the manuscript.

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Data availability

The data supporting this article have been included as part of the ESI.†

Conflicts of interest

The authors declare no conflict of interest.

References

- 1 K. S. Ikuta, L. R. Swetschinski, G. Robles Aguilar, F. Sharara, T. Mestrovic, A. P. Gray, N. Davis Weaver and E. E. Wool, *et al.*, *Lancet*, 2022, **400**, 2221–2248.
- 2 J. O'Neill, The Rev on AMR, H. M Government/Wellcome Trust, 2016.
- 3 R. Laxminarayan, P. Matsoso, S. Pant, C. Brower, J.-A. Røttingen, K. Klugman and S. Davies, *Lancet*, 2016, **387**, 168–175.
- 4 M. S. Mulani, E. E. Kamble, S. N. Kumkar, M. S. Tawre and K. R. Pardesi, *Front. Microbiol.*, 2019, **10**, 539.
- 5 P. Naucélér, A. Huttner, C. H. van Werkhoven, M. Singer, P. Tattevin, S. Einav and T. Tängdén, *Clin. Microbiol. Infect.*, 2021, **27**, 175–181.
- 6 R. E. Brummett and R. B. Morrison, *Arch. Otolaryngol., Head Neck Surg.*, 1990, **116**, 406–410.
- 7 R. E. Campbell, C. H. Chen and C. L. Edelstein, *Kidney Int. Rep.*, 2023, **8**, 2211–2225.
- 8 M. Exner, S. Bhattacharya, B. Christiansen, J. Gebel, P. Goroncy-Bermes, P. Hartemann, P. Heeg, C. Ilschner, A. Kramer, E. Larson, W. Merckens, M. Mielke, P. Oltmanns, B. Ross, M. Rotter, R. M. Schmithausen, H. G. Sonntag and M. Trautmann, *GMS Hyg. Infect. Control*, 2017, **12**, Doc05.
- 9 U. Theuretzbacher, *Curr. Opin. Microbiol.*, 2017, **39**, 106–112.
- 10 J. A. Kim, D. J. Wales and G.-Z. Yang, *Prog. Biomed. Eng.*, 2020, **2**, 042001.
- 11 H. M. Schouw, L. A. Huisman, Y. F. Janssen, R. H. J. A. Slart, R. J. H. Borra, A. T. M. Willemsen, A. H. Brouwers, J. M. van Dijk, R. A. Dierckx, G. M. van Dam, W. Szymanski, H. H. Boersma and S. Kruijff, *Eur. J. Nucl. Med. Mol. Imaging*, 2021, **48**, 4272–4292.
- 12 P. Giacomo, R. Sheryl, K. Susanne and R. Thomas, *J. Nucl. Med.*, 2020, **61**, 1419.
- 13 H. Kobayashi, M. Ogawa, R. Alford, P. L. Choyke and Y. Urano, *Chem. Rev.*, 2010, **110**, 2620–2640.
- 14 A. A. Ordonez, M. A. Sellmyer, G. Gowrishankar, C. A. Ruiz-Bedoya, E. W. Tucker, C. J. Palestro, D. A. Hammoud and S. K. Jain, *Sci. Transl. Med.*, 2019, **11**, eaax8251.
- 15 M. M. Welling, A. W. Hensbergen, A. Bunschoten, A. H. Velders, H. Scheper, W. K. Smits, M. Roestenberg and F. W. B. van Leeuwen, *Clin. Transl. Imaging*, 2019, **7**, 125–138.
- 16 Z. Wang and B. Xing, *Chem. Commun.*, 2022, **58**, 155–170.
- 17 Y. Huang, W. Chen, J. Chung, J. Yin and J. Yoon, *Chem. Soc. Rev.*, 2021, **50**, 7725–7744.
- 18 P. Pristovšek and J. Kidrič, *J. Med. Chem.*, 1999, **42**, 4604–4613.
- 19 T. Velkov, P. E. Thompson, R. L. Nation and J. Li, *J. Med. Chem.*, 2010, **53**, 1898–1916.
- 20 Z. Z. Deris, J. D. Swarbrick, K. D. Roberts, M. A. K. Azad, J. Akter, A. S. Horne, R. L. Nation, K. L. Rogers, P. E. Thompson, T. Velkov and J. Li, *Bioconjug. Chem.*, 2014, **25**, 750–760.
- 21 B. Yun, K. D. Roberts, P. E. Thompson, R. L. Nation, T. Velkov and J. Li, *Sensors*, 2017, **17**, 2598.



