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Carbon dots for highly effective photodynamic inactivation of multidrug-resistant bacteria†

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For addressing the ever increasing challenge of multidrug-resistant (MDR) bacterial infections, specifically designed and prepared carbon dots (CDots) of small carbon nanoparticles with surface functionalization–passivation by oligomeric polyethylenimine were found to be readily activated by visible light to effectively and efficiently inactivate MDR bacterial strains. The inactivation was evaluated under various combinations of experimental conditions (dot concentrations, light intensities, and treatment times), with the results collectively suggesting CDots as a new class of promising agents for combating MDR bacteria. Mechanistic origins and implications of the observed strong antibacterial actions as relevant to the photoexcited state processes in CDots and the photodynamically induced cellular damages leading to the death of the bacterial cells were explored, with the results discussed.

Infectious diseases caused by ever increasing antibiotic-resistant bacteria represent one of the most serious threats to public health globally.^{1,2} Among the multidrug resistant (MDR) pathogens that have emerged over the recent decades, MDR *Enterococci* are ranked second only to *Staphylococci* as aetiological agents for hospital acquired infections (HAI).^{3,4} *Enterococci* are the leading causes for bacteremia, urinary tract infections, and surgical wound infections,^{4–6} with *E. faecium* and *E. faecalis* responsible for the majority of enterococcal infections.^{2,7–10} These strains have acquired strong resistance capabilities through multiple mechanisms, and their resistance

to virtually all existing antibiotics in clinic^{9,11} presents particularly tough challenges for countermeasure strategies. In fact, not only are *Enterococci* able to recruit and maintain a variety of gene clusters for MDR, but also serve as donors of the resistance gene clusters to other pathogenic microorganisms,^{12,13} thus driving the spread and evolution of antibiotic resistance.

In the fight to control MDR pathogens, alternative to the development of new drugs and therapeutic paradigms have been approaches based on antimicrobial agents and mechanisms that are beyond the bacterial resistance. One approach proven effective has been photodynamic inactivation (PDI), in which a photo-sensitizer is employed to generate reactive oxygen species (ROS) under light illumination for their damaging multiple cellular components and ultimately killing the bacterial cells.^{14,15} Organic dyes have traditionally been used as photo-sensitizers, but more recently nanoscale materials have shown great promise as effective PDI agents for their many unique and advantageous characteristics, such as the robust photoexcited state processes for more effective and efficient ROS generation, photostability for repeated PDI actions, among others. In fact, recent reports on the PDI activities of semiconductor quantum dots (QDs) against MDR bacteria have generated some excitement in the research communities and also in the news media,^{16,17} despite the fact that the reported results for the QDs were generally suggesting the toughness of MDR bacterial strains in comparison with their non-resistant counterparts.^{16,17} For example, in the well publicized study of CdTe QDs for PDI against drug-resistant *Staphylococcus aureus*, *Escherichia coli*, *Klebsiella pneumoniae*, and *Salmonella typhimurium*, only a maximum of 80% or 92% (less than one log) of the bacterial cells were killed with 35 nM CdTe QDs after 6 hours of illumination with the normal light intensity or 8 hours of illumination with triple the normal light intensity, respectively.¹⁶ The inactivation was attributed to the light-activated redox species (LARS) interfering with the redox homeostasis of the bacterial cells. Competing with semiconductor QDs are the structurally rather simple carbon nanomaterials dubbed carbon dots (CDots, Fig. 1),^{18,19} which have recently

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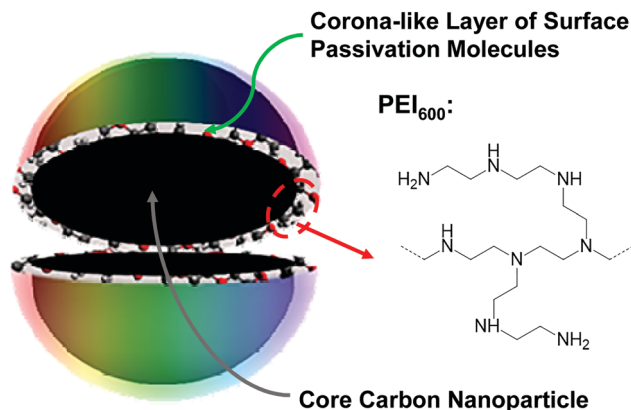


Fig. 1 A cartoon illustration on the structure in CDots in general and PEI₆₀₀-CDots specifically.

emerged to represent a new class of highly effective PDI agents under visible/natural light against a number of bacterial strains.^{20–24} In the work reported here, specifically designed and prepared CDots with visible-light activation were found to be able to kill drug resistant *E. faecium* and *E. faecalis* efficiently and quantitatively.

CDots are generally defined as small carbon nanoparticles with various surface passivation schemes,^{19,25} and the dot structure may be viewed as a special core-shell configuration, each with a “hard” carbon nanoparticle core and a “soft” shell of organic species for the passivation function (Fig. 1). In this work, oligomeric polyethylenimine (molecular weight ~600, PEI₆₀₀) was used for the surface functionalization-passivation of pre-processed and selected small carbon nanoparticles, thus the resulting dots denoted as PEI₆₀₀-CDots. The small carbon nanoparticles of averaging around 5 nm in diameter were harvested from commercially acquired carbon nanopowders (purity >99%), which according to the supplier were produced by the high-temperature carbonization of plant materials. The protocol for the harvesting included the oxidative acid treatment of the as-supplied carbon nanopowders, followed by a combination of solvent-dispersing and centrifuging steps and then solvent removal to obtain the targeted small carbon nanoparticles.²⁶ The nanoparticles thus harvested were then dispersed in PEI₆₀₀ melt for microwave energy-induced thermal reactions, in which the nanoparticles were functionalized by PEI₆₀₀ through radical addition²⁷ and/or other surface attachment modes.²³ The PEI₆₀₀-CDots prepared in the thermally induced functionalization reactions were found to be highly stable in terms of their optical properties remaining unchanged after their exposure to visible light for many hours or storage under ambient conditions for many months.

The sample characterization by using a series of instrumental methods yielded results that confirmed the dot structure as defined (Fig. 1), namely carbon nanoparticle cores of around 5 nm in average diameter surface-passivated by PEI moieties in the CDots (sizes mostly 4–8 nm, Fig. 2). The observed UV/vis absorption spectrum of PEI₆₀₀-CDots in an aqueous solution (Fig. 2) is similar to that of the aqueous suspended precursor

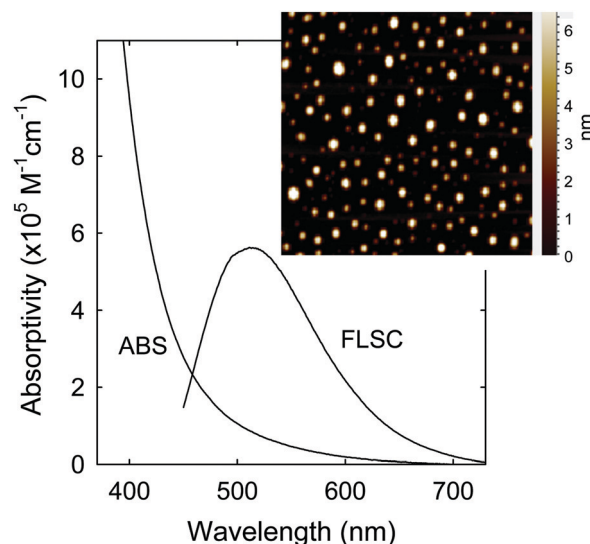


Fig. 2 Optical absorption (ABS) and fluorescence (FLSC) spectra of PEI₆₀₀-CDots in aqueous solution. Inset: Representative AFM images for the CDots.

carbon nanoparticles, characterized by significant photon-harvesting in the visible spectrum, and the observed fluorescence emission spectra and quantum yields (~20% at 400 nm excitation) are comparable to those of other CDots reported previously.²⁶

Visible light-induced PDI activities of PEI₆₀₀-CDots against MDR *E. faecalis* (resistant to tetracycline, nalidixic acid, and low-level streptomycin and erythromycin) and *E. faecium* (resistant to tetracycline, erythromycin, nalidixic acid, and low-level ciprofloxacin) were evaluated, with excellent outcomes. Experimentally, each strain in PBS buffer at a concentration of 10^7 – 10^8 CFU mL⁻¹ was treated with 1.9 μM PEI₆₀₀-CDots under visible light of 400–800 nm (11 W LED – light intensity ~4.8 mW cm⁻²) for 30 min, resulting in average viable cell reductions of ~6.0 log for *E. faecalis* and ~6.3 log for *E. faecium* (Fig. 3), close to complete inactivation. In the dark controls, the same treatment of PEI₆₀₀-CDots without light exposure had no effects on the bacterial cells. Also no effects were found for the exposure of *E. faecalis* and *E. faecium* to the visible light in the absence of any CDots.

The evaluation results also suggested dependencies of the PDI effectiveness on various combinations of parameters and conditions, including the dot concentration, light intensity, and exposure time. Fig. 3 shows the PDI results on MDR *E. faecalis* and *E. faecium* by PEI₆₀₀-CDots at dot concentration of 1.9 μM with 30 min exposure of visible light at two levels of intensity. The treatment at higher light intensity of ~7.8 mW cm⁻² (17 W LED) resulted in the complete inactivation of both *E. faecalis* and *E. faecium*, achieving ~8.0 log and ~7.1 log viable cell reduction, respectively (Fig. 3), while at the lower light intensity of ~4.8 mW cm⁻² (11 W LED), ~6.0 log and ~6.3 log viable cell reduction for *E. faecalis* and *E. faecium* was achieved, respectively (Fig. 3). In another combination to keep the light intensity at ~4.8 mW cm⁻², a much lower dot concentration of



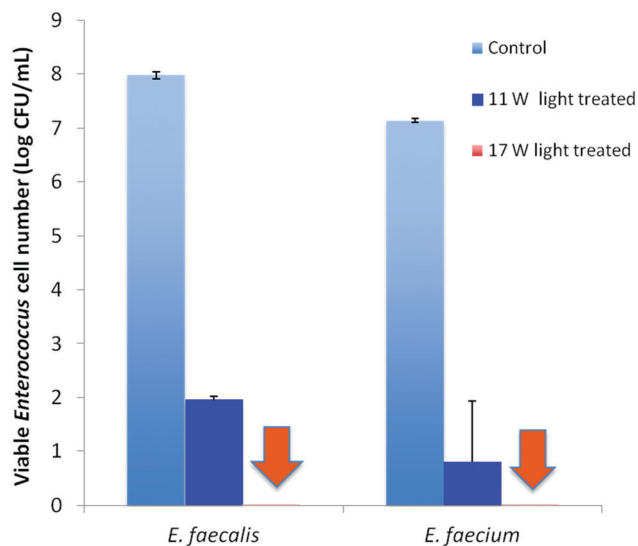


Fig. 3 The logarithmic viable cell numbers in the samples upon treatments with $1.9 \mu\text{M}$ PEI₆₀₀-CDots under illumination of visible light from 11 W ($\sim 4.8 \text{ mW cm}^{-2}$) and 17 W ($\sim 7.6 \text{ mW cm}^{-2}$) LEDs for 30 min, along with the control samples. (Note: the two arrows indicate the position of the columns where all bacterial cells were killed under illumination with the 17 W LED.)

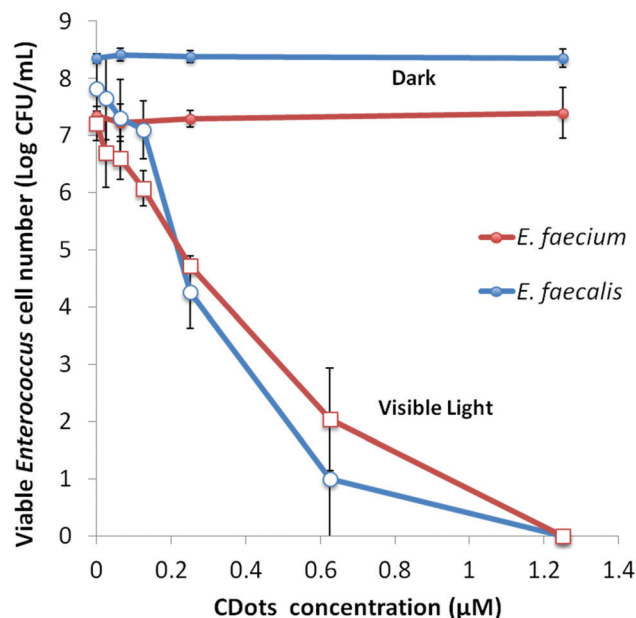


Fig. 4 The logarithmic viable cell numbers in the samples upon the treatment with different concentrations of PEI₆₀₀-CDots under visible light for 1 h, along with the samples treated with the same CDots in dark.

$0.62 \mu\text{M}$ could be coupled with a longer light exposure time of 90 min to achieve the similarly effective inactivation, with viable cell reductions of $\sim 7.0 \log$ for *E. faecalis* and $\sim 7.1 \log$ for *E. faecium*.

Under the same light intensity and exposure time ($\sim 4.8 \text{ mW cm}^{-2}$ for 60 min), the evaluations on variable dot concentrations show that the meaningful inactivation of more than 1 log could be achieved with the dot concentration as low as $0.12 \mu\text{M}$ in the samples containing 10^7 – 10^8 CFU mL^{-1} of *E. faecalis* or *E. faecium*, while complete eradication of bacterial cells in the samples was achieved at dot concentration of $1.25 \mu\text{M}$ (Fig. 4). And the concentration dependency of CDots' PDI was clearly observed for both strains (Fig. 4).

The results presented above collectively suggest that the CDots of relatively simple chemical compositions and nano-scale structures could readily be activated under visible light for highly effective killing of MDR bacteria, specifically the highly ranked MDR *E. faecium* and *E. faecalis*. While there are no comparable results available on PDI actions of conventional semiconductor QDs and related nanomaterials against the same MDR bacterial strains, the high performances of CDots are apparent, with the quantitative inactivation achieved at relatively low concentrations coupled with the exposure to simple household light sources. Among similar uses of conventional semiconductor QDs, the recently reported CdTe QDs for PDI against several drug-resistant bacterial strains resulted in only about one log bacterial cell reduction.¹⁶ The obviously high performance levels of CDots demonstrated in the PDI of the MDR *Enterococci* strains make these simple carbon nanomaterials extremely promising in the development of countermeasures to control MDR bacteria. Beyond the high performance, the CDots platform also offers other major advantages. Unlike many popular

yet highly toxic conventional semiconductor QDs due to their containing Cd (cadmium) or other heavy metals, CDots are known as being benign and nontoxic *in vitro* and *in vivo*,^{28–30} thus offering excellent opportunities for broad applications in many healthcare settings and human living environments.

For PDI, the strong optical absorptions of CDots for photon-harvesting in the visible spectrum represent a major advantage. The estimated molar absorptivities for CDots with core carbon nanoparticles in sizes of 5 nm in diameter are around $5 \times 10^5 \text{ M}^{-1} \text{ cm}^{-1}$ at 400–450 nm (Fig. 2). Mechanistically, upon photoexcitation of CDots there are rapid charge transfer and separation in the dots (Fig. 5), and the electrons and holes thus produced are trapped at various surface defect sites that are stabilized by the passivation of the organic moieties (Fig. 1).²⁵ The redox pairs likely serve the antibacterial function that is similar to or even more potent than that of the ROS produced in the traditional photosensitization, responsible in a major part for the observed high inactivation performance of the CDots. There have been experimental results suggesting that radiative recombinations of the electrons and holes (the population of the emissive excited states, Fig. 5) for the observed bright and colorful fluorescence emissions in CDots are rapid, namely the redox pairs are short-lived.³¹ Thus, their potent antibacterial activities must be on a fast time scale, probably requiring the dots next to the targeted bacterial cells. In this regard, the PEI moieties with abundant amino groups on the dot surface (Fig. 1) could be protonated at near neutral pH in the buffer solution and positively charged to facilitate the “binding” of PEI₆₀₀-CDots to the *Enterococci* cells, similar to what were found in the interactions of CDots with other bacteria.²⁰

The emissive excited states in CDots (Fig. 5) are relatively longer lived, averaging on the order of 5–10 ns,³¹ capable of the same ROS



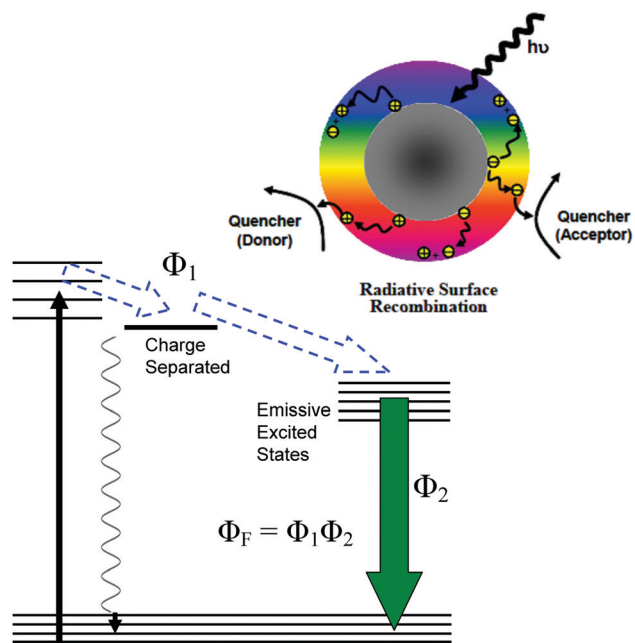


Fig. 5 Upper: Cartoon illustration on the photoexcited state processes in CDots, including the rapid charge separation, and the trapping of electrons and holes thus formed (which can be quenched by external electron acceptor and donor, respectively) and their radiative recombinations. Lower: The energy diagram for the same processes, with the observed fluorescence quantum yield Φ_F as a product of Φ_1 (denoting the overall yield for the charge separation and radiative recombinations) and Φ_2 (the yield of radiative process).

generation as that with traditional photosensitization. The high fluorescence quantum yields of PEI₆₀₀-CDots suggest relatively inefficient competing processes for the excited state energies, which must have benefited the ROS generation by the CDots (essentially bound to the targeted bacterial cells) to be more competitive and efficient. The combination of the ROS-like (by the initially formed redox pairs from the rapid charge separation following photoexcitation) and classical ROS actions on different time scales may be credited for the observed uniquely effective PDI against the MDR *Enterococci*.

The photo-generated ROS are known to damage various cell components such as carbohydrates, DNA, and/or lipids and proteins, leading to the cell death.^{32–34} For CDots, their photodynamic

killing of cancer cells has been demonstrated.^{35–37} In this work, the elevated intracellular ROS level was detected in both *E. faecalis* and *E. faecium* cells upon their treatment with PEI₆₀₀-CDots, increasing 3.8 and 3.2 fold in comparison to control samples, respectively, after the cells were treated with 1.2 μ M CDots for 1 h.

Both intracellular and extracellular ROS are capable of disrupting cell membranes,^{38,39} and the resulting cell structural damages can be visualized by using electron microscope. In the transmission electron microscopy (TEM) imaging experiment, the structural changes in the CDots-treated *E. faecium* cells were probed in reference to the untreated control cells. As compared in Fig. 6, while the treated cells still maintained their shape, without obvious disruption in cell morphology, there were apparently significant changes in the cytoplasm with the distinct condensed areas (the light area mostly in the center of cell, Fig. 6). The condensation of the cytoplasm must be due to the denaturing and precipitation of proteins and other cytoplasmic constituents induced by the PDI treatment with CDots, as similar condensed cytoplasm was observed in cells treated by other bactericidal agents,^{40–42} for which an example is the condensation in *Listeria innocua* cells treated with electrolyzed water and acidic sanitizers.⁴¹ Also consistent with the cell membrane damages and increased permeability was the observed release of more extracellular vesicles by the treated cells than the control cells.

In conclusion, CDots as structurally and composition-wise simple carbon-based nanomaterials could readily be activated by visible light to inactivate effectively and efficiently different strains of MDR *Enterococcus*. Mechanistically the inactivation is credited to the photodynamic effect, for which a special advantage of CDots is for the initially produced redox pairs upon photoexcitation to contribute substantially to the killing of the targeted bacterial cells (in addition to the actions of ROS generated in processes similar to those found in traditional photosensitization). The reported results further establish CDots as a new class of promising visible/natural light-activated broad spectral antibacterial agents, including especially their being capable of killing MDR bacterial pathogens in addition to various non-resistant bacterial species previously reported. With their simple structure and composition and their preparation from benign and abundant precursors, CDots may find broad applications in combating MDR bacterial infections through effective inactivation of MDR pathogens at various contaminated sites in their spread/transmission routes.

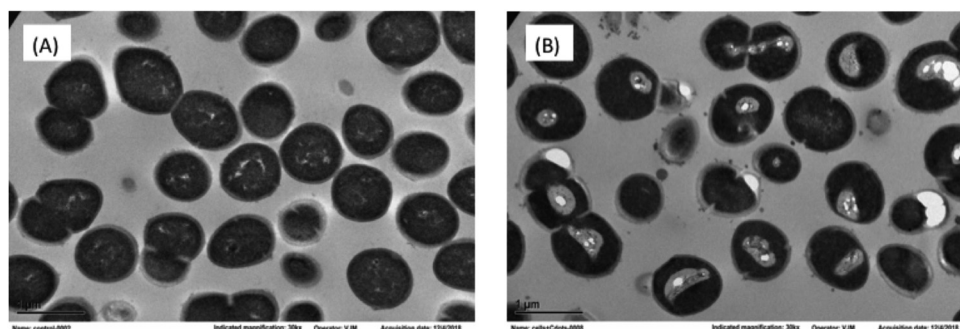


Fig. 6 TEM images of *E. faecium* cells (A) without treatment, and (B) post-treatment with 1.2 μ M PEI₆₀₀-CDots under the 11 W visible LED for 1 h.



Conflicts of interest

There are no conflicts to declare.

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References

- W. H. Organization, *Antimicrobial Resistance: Global Report on Surveillance*, the WHO Document Production Services, Geneva, Switzerland, 2014.
- L. B. Rica, *J. Infect. Dis.*, 2008, **197**, 1079–1081.
- A. I. Hidron, J. R. Edwards, J. Patel, T. C. Horan, D. M. Sievert, D. A. Pollock, S. K. Fridkin, T. National Healthcare Safety Network and F. Participating National Healthcare Safety Network, *Infect. Control Hosp. Epidemiol.*, 2008, **29**, 996–1011.
- D. R. Schaberg, D. H. Culver and R. P. Gaynes, *Am. J. Med.*, 1991, **91**, 72S–75S.
- T. G. Emori and R. P. Gaynes, *Clin. Microbiol. Rev.*, 1993, **6**, 428–442.
- W. R. Jarvis, *CDC*, 1996, 1–7.
- C. A. Arias, G. A. Contreras and B. E. Murray, *Clin. Microbiol. Infect.*, 2010, **16**, 555–562.
- B. Hota, *Clin. Infect. Dis.*, 2004, **39**, 1182–1189.
- M. M. Huycke, D. F. Sahm and M. S. Gilmore, *Emerging Infect. Dis.*, 1998, **4**, 239–249.
- R. M. van Harten, R. J. L. Willems, N. I. Martin and A. P. A. Hendrickx, *Trends Microbiol.*, 2017, **25**, 467–479.
- B. L. Hollenbeck and L. B. Rice, *Virulence*, 2012, **3**, 421–433.
- S. Chang, D. M. Sievert, J. C. Hageman, M. L. Boulton, F. C. Tenover, F. P. Downes, S. Shah, J. T. Rudrik, G. R. Pupp, W. J. Brown, D. Cardo, S. K. Fridkin and T. Vancomycin-Resistant Staphylococcus aureus Investigative, *N. Engl. J. Med.*, 2003, **348**, 1342–1347.
- A. J. Ray, N. J. Pultz, A. Bhalla, D. C. Aron and C. J. Donskey, *Clin. Infect. Dis.*, 2003, **37**, 875–881.
- D. E. J. G. J. Dolmans, D. Fukumura and R. K. Jain, *Nat. Rev. Cancer*, 2003, **3**, 380–387.
- L. B. Josefsen and R. W. Boyle, *Met.-Based Drugs*, 2008, **2008**, 276109.
- C. M. Courtney, S. M. Goodman, J. A. McDaniel, N. E. Madinger, A. Chatterjee and P. Nagpal, *Nat. Mater.*, 2016, **15**, 529–534.
- C. M. Courtney, S. M. Goodman, T. A. Nagy, M. Levy, P. Bhusal, N. E. Madinger, C. S. Detweiler, P. Nagpal and A. Chatterjee, *Sci. Adv.*, 2017, **3**, e1701776.
- Y. P. Sun, *US Pat.* 7,829,772 B2, 2010.
- Y. P. Sun, B. Zhou, Y. Lin, W. Wang, K. A. S. Fernando, P. Pathak, M. J. Meziani, B. A. Harruff, X. Wang, H. F. Wang, P. J. G. Luo, H. Yang, M. E. Kose, B. L. Chen, L. M. Veca and S. Y. Xie, *J. Am. Chem. Soc.*, 2006, **128**, 7756–7757.
- D. I. Abu Rabe, M. M. Al Awak, F. Yang, P. A. Okonjo, X. Dong, L. R. Teisl, P. Wang, Y. Tang, N. Pan, Y. P. Sun and L. Yang, *Int. J. Nanomed.*, 2019, **14**, 2655–2665.
- M. M. Al Awak, P. Wang, S. Wang, Y. Tang, Y. P. Sun and L. Yang, *RSC Adv.*, 2017, **7**, 30177–30184.
- X. Dong, A. E. Bond, N. Pan, M. Coleman, Y. Tang, Y. P. Sun and L. Yang, *Int. J. Nanomed.*, 2018, **13**, 8025–8035.
- Y. Hu, M. M. Al Awak, F. Yang, S. Yan, Q. Xiong, P. Wang, Y. Tang, L. Yang, G. E. LeCroy, X. Hou, C. E. Bunker, L. Xu, N. Tomlinson and Y. P. Sun, *J. Mater. Chem. C*, 2016, **4**, 10554–10561.
- M. J. Meziani, X. Dong, L. Zhu, L. P. Jones, G. E. LeCroy and F. Yang, *ACS Appl. Mater. Interfaces*, 2016, **8**, 10761–10766.
- L. Cao, M. J. Meziani, S. Sahu and Y. P. Sun, *Acc. Chem. Res.*, 2013, **46**, 171–180.
- G. E. LeCroy, S. K. Sonkar, F. Yang, L. M. Veca, P. Wang, K. N. Tackett, J. J. Yu, E. Vasile, H. J. Qian, Y. M. Liu, P. Luo and Y. P. Sun, *ACS Nano*, 2014, **8**, 4522–4529.
- X. Y. Ren, W. X. Liang, P. Wang, C. E. Bunker, M. Coleman, L. R. Teisl, L. Cao and Y. P. Sun, *Carbon*, 2019, **141**, 553–560.
- J.-H. Liu, Y. Wang, G.-H. Yan, F. Yang, H. Gao, Y. Huang, H. Wang, P. Wang, L. Yang, Y. Tang, L. R. Teisl and Y.-P. Sun, *J. Nanosci. Nanotechnol.*, 2019, **19**, 2130–2137.
- Y. Wang, P. Anilkumar, L. Cao, J. H. Liu, P. G. Luo, K. N. Tackett, 2nd, S. Sahu, P. Wang, X. Wang and Y. P. Sun, *Exp. Biol. Med.*, 2011, **236**, 1231–1238.
- S. T. Yang, X. Wang, H. Wang, F. Lu, P. G. Luo, L. Cao, M. J. Meziani, J. H. Liu, Y. Liu, M. Chen, Y. Huang and Y. P. Sun, *J. Phys. Chem. C*, 2009, **113**, 18110–18114.
- W. Liang, C. E. Bunker and Y.-P. Sun, *ACS Omega*, 2020, **5**, 965–971.
- L. J. Marnett, *Carcinogenesis*, 2000, **21**, 361–370.
- E. R. Stadtman and R. L. Levine, *Ann. N. Y. Acad. Sci.*, 2000, **899**, 191–208.
- S. Yla-Herttuala, *Ann. N. Y. Acad. Sci.*, 1999, **874**, 134–137.
- J. Ge, M. Lan, B. Zhou, W. Liu, L. Guo, H. Wang, Q. Jia, G. Niu, X. Huang, H. Zhou, X. Meng, P. Wang, C. S. Lee, W. Zhang and X. Han, *Nat. Commun.*, 2014, **5**, 4596.
- P. Juzenas, A. Kleinauskas, P. G. Luo and Y. P. Sun, *Appl. Phys. Lett.*, 2013, **103**, 063701.
- Z. M. Markovic, B. Z. Ristic, K. M. Arskin, D. G. Klisic, L. M. Harhaji-Trajkovic, B. M. Todorovic-Markovic, D. P. Kepic, T. K. Kravic-Stevovic, S. P. Jovanovic, M. M. Milenkovic, D. D. Milivojevic, V. Z. Bumbasirevic, M. D. Dramicanin and V. S. Trajkovic, *Biomaterials*, 2012, **33**, 7084–7092.
- Y. N. Slavin, J. Asnis, U. O. Häfeli and H. Bach, *J. Nanobiotechnol.*, 2017, **15**, 65.
- L. Wang, H. He, Y. Yu, L. Sun, S. Liu, C. Zhang and L. He, *J. Inorg. Biochem.*, 2014, **135**, 45–53.
- T. Dai, A. Gupta, Y.-Y. Huang, R. Yin, C. K. Murray, M. S. Vrahas, M. E. Sherwood, G. P. Tegos and M. R. Hamblin, *Antimicrob. Agents Chemother.*, 2013, **57**, 1238–1245.
- L. Feliciano, J. Lee and M. A. Pascall, *J. Food Sci.*, 2012, **77**, M182–187.
- B. Sampathkumar, G. G. Khachatourians and D. R. Korber, *Appl. Environ. Microbiol.*, 2003, **69**, 122–129.

