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Biomaterials for bone tissue engineering scaffolds: a review

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Bone tissue engineering has been continuously developing since the concept of "tissue engineering" has been proposed. Biomaterials that are used as the basic material for the fabrication of scaffolds play a vital role in bone tissue engineering. This paper first introduces a strategy for literature search. Then, it describes the structure, mechanical properties and materials of natural bone and the strategies of bone tissue engineering. Particularly, it focuses on the current knowledge about biomaterials used in the fabrication of bone tissue engineering scaffolds, which includes the history, types, properties and applications of biomaterials. The effects of additives such as signaling molecules, stem cells, and functional materials on the performance of the scaffolds are also discussed.

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1. Introduction

Bone and its associated diseases, accounting for half of chronic diseases in people over 50 years old, still remain an important clinical challenge. Although bones have a certain healing and/or regeneration capacity, it cannot be accomplished by itself for large segmental bone defects. Large bone defects or injuries, caused by old age, traffic accident, fracture nonunion, bone tumor resection, *etc.*, are serious problems in orthopaedics, and they bring great harms to health and the quality of life. Autologous bone grafting is still regarded as the "gold standard" for repairing bone defects. However, the drawbacks of autologous bone grafting include secondary damages, high donor site morbidity, limitation of special shape, insufficiency of autogenous bone and so on. These weaknesses limit its widespread use in clinical settings.

The term "tissue engineering" was first used in 1987.⁵ It is the utilization of a combination of multidisciplinary approaches to improve or replace biological tissues. In recent years, with the rapid development of tissue engineering technology, bone tissue engineering has become a hopeful approach for repairing bone defects. Scaffolds play a crucial role in bone tissue engineering. Their purpose is to mimic the structure and function of the natural bone extracellular matrix (ECM), which can provide a three-dimensional (3D) environment to promote the adhesion, proliferation, and differentiation and to have adequate physical properties for bone repair. An ideal scaffold should be biodegradable, biocompatible, bioactive, osteoconductive and

osteoinductive. Artificial bone scaffolds with biomaterials and additives, such as drugs, growth factors (GFs) and stem cells, have been useful for bone repair.

The biomaterials (biomedical materials), which are basic components of scaffolds, play an important role in bone tissue engineering. Archaeological findings showed that materials such as human or animal bones and teeth, corals, shells, wood, and several metals (gold, silver and amalgam) were used for the replacement of missing human bones and teeth.6 For example, in the ancient times, the Etruscans learnt to replace damaged teeth with artificial graft obtained from the bones of oxen. In the early 1960s, the limitations of biological bone substitute materials resulted in the emergence of a multidisciplinary field called "Biomaterials". Biomaterials are used for the evaluation, treatment, augmentation, repair or replacement of tissues or organs of the body. Ancient alternative materials are mostly bioinert (biologically inert), and these materials interact less with the surrounding tissues and are even toxic to humans. An ideal biomaterial should be non-cytotoxic, printable, biodegradable, bioactive, and osteoconductive in vivo. Due to the various needs of scaffolds, composite materials composed of two or more materials with excellent properties are widely used in bone tissue engineering.

Numerous natural and synthetic polymers such as calcium phosphates, calcium carbonate, and bioactive glasses have been used to fabricate scaffolds. Recent outstanding approaches include the addition of conductive polymers (CPs), inducerons (signaling molecules, unlike bone morphogenetic protein 2 (BMP-2)) and mechanical signals (elastic polymer networks such as hydrogels) to bone tissue engineering scaffolds. With the integration, intercrossing and development of the fields of medicine, biology, materials and other disciplines, biomaterials have been extensively used in the fabrication of bone tissue engineering scaffolds.⁸

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This article gives a brief introduction to the descriptions of the hierarchical structure, chemical composition of natural bone and strategies for bone tissue engineering. It aims to outline the history, types, properties and development methods of common biomaterials used to fabricate scaffolds. Further, the review also highlights the biomaterial scaffolds with additives. Finally, it examines the combination of advanced technology and biomaterials, and emphasizes the challenges and opportunities of biomaterials in bone tissue engineering scaffolds.

Materials and methods

All studies (*in vitro* and *in vivo*) concerning the application of biomaterials to manufacture scaffolds for bone tissue engineering were researched in duplicate in the Medline (PubMed) online database. The PubMed search was performed to look for articles published in English between January 1, 2010 and January 1, 2019. The Medical Subject Heading (abbreviated as MeSH) terms "bone and bones", "biocompatible materials" and "tissue scaffolds" were used together with the keywords "bone tissue engineering", "biomaterials" and "scaffolds" to apply the following search strategy:

((("Bone and Bones[Mesh] OR (bone[All Fields]) OR (bones [All Fields]) OR ("bones and bone" [All Fields]) OR ("bones and bone tissues" [All Fields]) OR (bone [All Fields] AND (tissue [All Fields] OR tissues[All Fields])) OR ("bone tissue"[All Fields]) OR ("bone tissues" [All Fields])) AND ("biocompatible materials"[Mesh] OR ("biocompatible materials"[All Fields]) OR ((material[All Fields]) AND (biocompatible[All Fields])) OR (biomaterials[All Fields]) OR (biomaterial[All Fields]) OR ("bioartificial materials"[All Fields]) OR ("bioartificial material"[All Fields]) OR ((material[All Fields]) AND (bioartificial[All Fields]))) AND ("tissue scaffolds" [Mesh] OR ((scaffold [All Fields] OR scaffolds[All Fields] OR scaffolding[All Fields] OR scaffoldings [All Fields]) AND tissue[All Fields]) OR ("tissue scaffold"[All Fields]) OR ("tissue scaffolding"[All Fields]) OR ("tissue scaffoldings"[All Fields]))) OR ((bone tissue engineering) AND (biomaterials) AND (scaffolds))) AND ("2010/01/01" [Date-Publication]: "2019/01/01" [Date-Publication]). 9,10

The follow-up period or sample size is not limited. Meta analyses and systematic reviews were not included. Scientific research regarding the following topics was not considered: scaffolds for assisted positioning of transplants and help with surgical planning before the surgery.

2.1 Study selection

Two of the authors individually selected the titles and abstracts of the articles obtained by the above-mentioned search. Then, the selected studies were independently carefully sifted by both of the reviewers. Any disagreement was determined through discussions between them.

2.2 Data extraction

Two of the authors separately summarized the search and sought consensus among other authors in the process. The

undermentioned information was recorded: the publication information including the author's name and publication data, the biomaterials applied to manufacture scaffolds and their important characteristics.

3. Structure, mechanical properties and materials of natural bone

3.1 Hierarchical structure of bone

As the main part of the human skeletal system, bone plays a crucial role in providing structure, supporting mechanical movement, protecting organs, and producing and hosting blood cells. It has a complex hierarchical structure based on the length and width scale, which consists of the macro scale (trabecular bone, also known as cancellous or spongy bone, and compact bone, also named cortical bone), microscale and submicroscale (haversian canals, osteons and lamellae), nanoscale (fibrillar collagen) and sub-nanoscale (such as minerals, collagen and so on), as shown in Fig. 1.¹¹ The structure of natural bone has been presented in various articles.¹¹⁻²¹ Compact bone is nearly solid, except for ~3–5% of rooms for canaliculi, osteocytes and so on.¹⁸ However, trabecular bone is an interconnected porous network and has a higher bone surface-to-bone volume (BS/BV) ratio than compact bone.

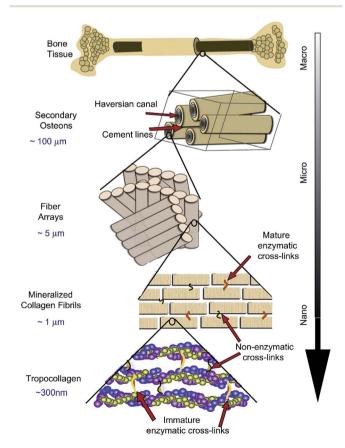


Fig. 1 Hierarchical structure of natural bone. Reproduced from ref. 11 with permission from Elsevier, copyright 2011.

RSC Advances Review

Table 1 Mechanical properties of natural bone

	Modulus (GPa)		Strength (MPa)		Poisson's ration
Compact bone	Longitudinal	17.9 ± 3.9	Tension	135 ± 15.6	0.4 ± 0.16
•	· ·		Compression	205 ± 17.3	
	Transverse	10.1 ± 2.4	Tension	53 ± 10.7	0.62 ± 0.26
			Compression	131 ± 20.7	
	Shear	3.3 ± 0.4	Shear	65 ± 4.0	
Trabecular bone	Vertebra	0.067 ± 0.045		2.4 ± 1.6	
	Tibia	0.445 ± 0.257		5.3 ± 2.9	
	Femur	0.441 ± 0.271		6.8 ± 4.8	

Table 2 Chemical composition of bone (wt%)

Inorganic Phase	Organic Phase
$HA \approx 60$ $H_2O \approx 9$ Carbonate ≈ 4 Citrate ≈ 0.9 $Na^+ \approx 0.7$ $Mg^{2^+} \approx 0.5$ Cl^-	Collagen≈20 Noncollagenous proteins≈3 Traces: polysaccharides, lipids, and cytokines Primary bone cell: osteoblasts, osteocytes, and osteoclasts
Others: K ⁺ , F ⁻ , Zn ²⁺ , Fe ²⁺ , Cu ²⁺ , Sr ²⁺ , and Pb ²⁺	

3.2 Mechanical properties of bone

The mechanical properties of natural bone vary greatly with respect to age and the body part. Young's modulus and yield stress of natural bone are anisotropic. A complete understanding of the mechanics of living bones remains an important scientific challenge. Table 1 shows the mechanical properties of natural bone obtained from the reported data.¹⁸ The longitudinal direction of the compact bone is robuster and stiffer than its transverse direction. The trabecular bone has a porous structure, and the porosity and arrangement of the individual trabeculae determine its mechanical properties.

3.3 Natural composition of bone

The understanding of the material components of natural bone plays a crucial role in the selection of scaffold materials. Natural bone consists of cells, ECM assembled from collagen fibrils and

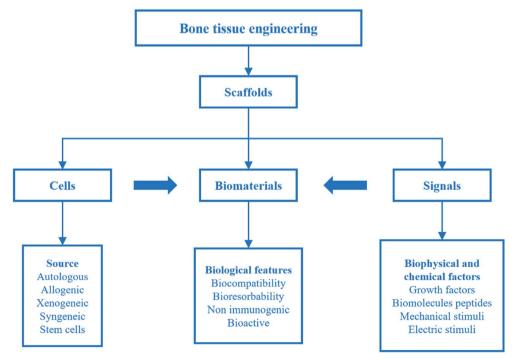


Fig. 2 Strategies for bone tissue engineering. Reproduced from ref. 22 with permission from Springer, copyright 2018.

Review RSC Advances

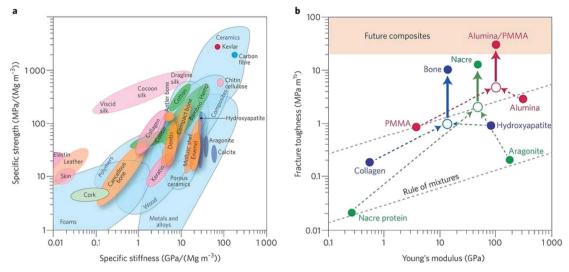


Fig. 3 Performance of natural and synthetic materials. (a) Ashby chart of strength and stiffness for natural and synthetic materials. (b) Calculation for natural and synthetic materials. Reproduced from ref. 17 with permission from Nature Publishing Group, copyright 2014.

hydroxyapatite (HA), and bound minerals. Collagen and HA together account for \sim 95% of natural bone under dry conditions.²¹ The composition of natural bone is presented in Table 2.¹⁹ Biological apatites deviate from the stoichiometric composition of HA and contain certain amounts of ion substitution impurities such as Na⁺, Mg²⁺, Cl⁻, K⁺, F⁻, and Zn²⁺. HA is the major inorganic component of human skeleton.

4. Bone tissue engineering

Although human bones have a certain self-healing ability, they are powerless for large bone defects. To overcome the problems, bone tissue engineering is proposed on the basis of tissue engineering. Bone tissue engineering aims to induce new tissue repairing and regeneration by the synergy of cells, signals and scaffolds.⁸ A scaffold composed of biomaterials is a carrier of cells and signals. It plays a key role in bone tissue engineering. Strategies for bone tissue engineering are shown in Fig. 2.²²

For the large-sized tissues and origins with different shapes, it is necessary to design a temporary support to provide spaces for cell proliferation, differentiation and growth. The support is called scaffold, transplant, template or artificial ECM. As noticed before, an ideal scaffold should have biocompatibility, suitable mechanical properties, high porosity and gradient pore structure. As the new tissue grows, the implanted scaffold gradually degrades until the new tissue completely replaces it. The design and fabrication of scaffolds with customization can be obtained by computer-aided design and computer-aided manufacturing (CAD/CAM) technology. Biomaterials are an important part of the scaffolds, and an ideal biomaterial should possess the following characteristics: (1) biocompatibility; (2) biodegradability; (3) easy printing and processing. During the last decades, researchers have shown increasing interest towards biomaterials for their application in bone tissue engineering scaffolds.

Generally, the obtained scaffolds should be biologically investigated. The main approaches of biological research *in*

vitro as forecasting test before pre-clinical can be divided into two main categories: (1) *in vitro* culture experiments such as scaffold toxicity tests, animal or human cells (such as BMSCs,²³ hMSCs,²⁴ *etc.*) and (2) *in vivo* animal experiments (such as repairing of femur defects in rats).²⁵ Scaffolds with non-toxic, good biocompatibility are the basis of bone repair and regeneration, in which biomaterials play an important role in the excellent performance of the scaffolds.

5. Various biomaterials for bone tissue engineering scaffolds

5.1 History of biomaterials

In the long history of human development, tissues and organs have evolved with respect to function after millions of years, but humans have been using artificial substitutes to repair damaged tissues only for decades. In the year 659 AD, the Chinese first used dental amalgam to repair defects in teeth.²⁶ The limitations of bone replacement materials have resulted in the utilization of synthetic alternative materials for bone repair, replacement and enhancement. "Biomaterials" appeared in the early 1960s.⁷ The history of using biomaterials for scaffolds based on three different generations is briefly introduced below.⁸

The first generation of biomaterials appeared in the 1960s.²⁷ It aimed to achieve the performance of the biomaterial to match the replaced tissue with the least toxic reaction to the host. They are generally bioinert, and interact minimally with the surrounding tissues. The first generation of biomaterials mainly includes: metals (such as titanium or titanium alloys), synthetic polymers (such as PMMA and PEEK) and ceramics (such as alumina and zirconia).

The most important feature of the second-generation biomaterials is their bioactive nature, and some could be biodegradable *in vivo*. They consist of synthetic and natural polymers (*e.g.* collagen), calcium phosphates, calcium carbonate, calcium sulfates, and bioactive glasses.

RSC Advances

properties of biocompatible metalitic seaffolds Bioactive and corrosion resistance Good porous and biodegradable implant alloys Filannium and titanium Bourable, biocompatible, incompatible, classicity for rabecome properties (such as the shape memory and superelastic effects) Filannium and overy similar modulus of classicity for rabecome properties (such as the shape memory and superelastic effects) Filannium and pimer Similarity to ECM, specific degradation rares and good bone organic materials, Excellent piocompatibility Denaturalized collagen Filannium and pimer Similarity to ECM, specific degradation rares and good bone organic materials, Excellent piocompatibility Denaturalized collagen Filannium and pimer Silk fibroin Silk fibroin will be compatibility of resistance to bacteria Polysaccharide with negative charge, and can rousalink and print by injection Filannium and titanium Filannium	Biomaterials	Characteristics	Advantages	Disadvantages	Ref.
Fantalum Bioactive and corrosion Extensively used as implant Indicated	Metal	properties of biocompatible	properties	C	
Magnesium Good porous and biodegradable implant similar to human bone liodegradable (highly corrosion resistant and trainium alloy highly corrosion resistant and eys winith roudulus of elasticity, for trabecular bone monoy and superelastic effects) brother including propertice (such as the shape memory and superelastic effects) brother including propertice (such as the shape memory and superelastic effects) brother including propertice effects) brother including propertice (such as the shape better than any other metals for comparity to ECM, specific degradation rates and good brother including propertice of the degradation rates and good brother including propertice of the degradation rates and good brother including propertice of the degradation rates and good brother including propertice of the degradation rates and good brother including propertice of the degradation rates and good brother including propertice of the degradation rates and good brother including propertice of the degradation rate and good brother including propertice of the degradation rate and good brother including propertice of the degradation rate and good brother including propertice of the degradation rate and good brother including propertice of the degradation rate and good brother including propertice of the degradation rate and good brother including propertice of the propertice of the degradation rate and good propertice of the pr	Tantalum	Bioactive and corrosion	Extensively used as implant	Almost no degradation lead to a second surgery for	28-32
PLA, PGA and PLGA PEA, PGA and	Magnesium		similar to human bone	Toxicity risk caused by metal	33-39
elasticity for trabecular bone Particular mechanical properties (such as the shape memory and superelastic effects) Natural polymer Similarity to ECM, specific degradation rates and good biological properties Eccellent biocompatibility Denaturalized collagen Denaturalized collagen Excellent biocompatibility and resistance to bacteria Hyaluronic acid Olymer Synthetic polymer PLA, PGA and PLGA Excellent crystallinity and mechanical properties PVA Hydroylated synthetic polywinyl acetate PPF Has numerous nonsaturable double bonds and the resistines mechanical properties Cannot perform medical reactions with living tissue Cannot perform medical reactions with living tissue Low modulus of elasticity, and high damping capacity, better match the properties of natural bone better than any other metals Biocompatibile pheropetics of natural bone better than any other metals Biocompatibile Degradation Degradation Silk fibroin attentials. Excellent biocompatibility and resistance to bacteria Polysaccharide with positive charge, and can crosslink and print by injection Glycosaminoglycan with negative charge, and ean crosslink and print by injection Glycosaminoglycan with negative charge, and ean crosslink and print by injection Glycosaminoglycan with negative charge, and ean crosslink and print by injection Glycosaminoglycan with negative charge, and ean crosslink and print by injection Glycosaminoglycan with negative charge, and ean crosslink and print by injection Glycosaminoglycan with negative charge, and ean crosslink and print by injection Glycosaminoglycan with negative charge, and ean crosslink and print by injection Glycosaminoglycan with negative charge, and ean crosslink and print by injection Glycosaminoglycan with negative charge, and ean crosslink and print by injection Glycosaminoglycan with negative charge, and ean crosslink and print by injection Changeable mechanical and physical properties which relatively difficult are relatively difficult are relatively difficult are relatively difficult ar		highly corrosion resistant	· ·	Non-biodegradable	40-44
Natural polymer Similarity to ECM, specific degradation rates and good biological properties Collagen Important part of natural bone organic materials. Excellent biocompatibility of penaturalized collagen Gelatin Denaturalized collagen Silk fibroin with outstanding mechanical properties Polysaccharide with positive charge, biocompatibility and resistance to bacteria Alginate Alg	Nickel-titanium alloy (nitinol)	elasticity for trabecular bone Particular mechanical properties (such as the shape memory and superelastic	pseudo-elasticity, and high damping capacity, better match the properties of natural bone better than any	nitinol, the relatively high stiffness of titanium can cause stress shielding and	45-48
Distriction and handling are relatively difficult Secolation Denatural part of natural bone organic materials. Various forms of scaffolds Excellent biocompatibility (e.g., sheets) Forming blends through Cross-linking Silk fibroin Silk fibroin with outstanding mechanical properties Polysaccharide with positive charge, biocompatibility and resistance to bacteria and print by injection Polysaccharide with negative charge, and can crosslink and print by injection Hyaluronic acid Glycosaminoglycan with negative charge, biocompatibility, forming hydrogel through cross-linking Changeable mechanical and phydrogel through cross-linking Polysaccharide with regative charge, biocompatibility, forming hydrogel through cross-linking Changeable mechanical and physical properties Polysical properties Changeable mechanical and physical properties Polysical properties Changeable mechanical and physical properties Changeable mechanical properties Changeable mechanical and physical properties Changeable mechanical properties Changeable mechanical and physical properties Changeable mech	Natural polymer	degradation rates and good	Biocompatible	Low mechanical strength	
Gelatin Denaturalized collagen constituting and mechanical properties charge, and can rosslink gegradability and negative charge, and can crosslink gegradability properties charge, bicompatibility, forming hydrogel through crosslinking Synthetic polymer PLA, PGA and PLGA Excellent crystallinity and mechanical applications PVA Hydroxylated synthetic polyming archanical properties classing polymyl acetate polyvinyl acetate double bonds and the crosslinks may be toxic properties POR Excellent crystallinity and mechanical properties double bonds and the crosslinks may be toxic properties Gearantic Cannot perform medical reactions with living tissue constitutions and the crosslinks may be toxic properties Estimerer ceramic Cannot perform medical reactions with living tissue constitutions and properties consulted and properties an	Collagen	Important part of natural bone organic materials.	Various forms of scaffolds	· ·	49–51
Silk fibroin mechanical properties mechanical properties chitosan Polysaccharide with positive charge, biocompatibility and resistance to bacteria Alginate Polysaccharide with negative charge, and can crosslink and print by injection Hyaluronic acid Glycosaminoglycan with negative charge, biocompatibility, forming hydrogel through cross-linking Synthetic polymer PLA, PGA and PLGA FDA-approved materials for clinical applications PCL Excellent crystallinity and mechanical properties PVA Hydroxylated synthetic polywil acetate Hydroxylated synthetic polywil acetate PVA Hydroxylated synthetic polywil acetate Hydrox	Gelatin		Forming blends through		52-55
Chitosan Polysaccharide with positive charge, biocompatibility and resistance to bacteria Alginate Polysaccharide with negative charge, and can crosslink and print by injection Hyaluronic acid Glycosaminoglycan with negative charge, piocompatibility, forming hydrogel through cross-linking Synthetic polymer Charge PDA-approved materials for clinical applications clinical applications PLA, PGA and PLGA FDA-approved materials for clinical applications PCL Excellent crystallinity and mechanical properties PVA Hydroxylated synthetic polyvinyl acetate PVA Hydroxylated synthetic polyvinyl acetate PVA Hydroxylated synthetic crosslinks may be toxic consistinks may be toxic degradation PCF Connot properties a shape, porosity and degradation rate crosslinks may be toxic degradation PCF Connot properties a shape, porosity and degradation rate crosslinks may be toxic degradation and accordance of the polyvinyl acetate crosslinks may be toxic degradation and physical properties believe the polyvinyl and constant the polyvinyl and print properties a shape, porosity and degradation rate crosslinks may be toxic degradation and physical properties believe the polyvinyl and print polyvinyl acetate crosslinks may be toxic degradation rate POF Connot perform medical properties a polyvinyl acetate crosslinks may be toxic degradation and physical properties and rates of degradation and physical prop	Silk fibroin		cross mixing		56-58
Alginate Polysaccharide with negative charge, and can crosslink and print by injection Hyaluronic acid Glycosaminoglycan with negative charge, piocompatibility, forming hydrogel through cross-linking Synthetic polymer PLA, PGA and PLGA PLA, PGA and PLGA Excellent crystallinity and mechanical properties PVA Hydroxylated synthetic polywil acetate PVA Hydroxylated synthetic polywil acetate PVA Has numerous nonsaturable double bonds and the crosslinks may be toxic POPL Remarkable mechanical Robert Strength and rates of degradation Robert Strength and rates of degradation with living tissue Robert Cannot perform medical reactions with living tissue Robert Strength and rates of degradation with living tissue Robert Strength and rates of degradation with living tissue Robert Strength and rates of degradation with living tissue Robert Strength and rates of degradation with living tissue Robert Strength and rates of degradation with living tissue Robert Strength and rates of degradation with living tissue	Chitosan	Polysaccharide with positive charge, biocompatibility and			59
Hyaluronic acid Glycosaminoglycan with negative charge, biocompatibility, forming hydrogel through cross- linking Changeable mechanical and physical properties Changeable mechanical and physical properties PLA, PGA and PLGA PLA, PGA and PLGA FDA-approved materials for clinical applications Clinical applications Changeable mechanical and physical properties PCL Excellent crystallinity and mechanical properties Biolinert ceramic POPU Remarkable mechanical properties Cannot perform medical propertors Cannot perform medical propertors Cannot perform medical properties Cannot perform medical properties Functionalization and functionalization and functionalization and degradability functionalization and degradation Possible adverse tissue reactions acused by acidic degradation reactions acused by acidic degradation Possible adverse tissue reactions alization and Possible adverse tissue reactions alization and begradability hydroxplete strength and print performing physroylation degree Poly urethane (PU) Remarkable mechanical properties Cannot perform medical reactions with living tissue Fas, 63-66 functionalization and degradability hydroxplete mechanical and prossible adverse tissue reactions alization and degradation Possible adverse tissue reactions acused by acidic degradation Possible adverse tissue reactions caused by acidic degradation Possible adverse tissue reactions a	Alginate	Polysaccharide with negative charge, and can crosslink			60-62
Changeable mechanical and physical properties reactions caused by acidic degradation PLA, PGA and PLGA POn-Nydroplobic and operation degradation PLA, PGA and PLGA PLA, PGA and PLGA PO-90 PLA, PGA and PLGA PON-Nydroplobic and Non-hydropholic and shortage of cell adhesion PLA, PGA and PLGA PO-90 PLA, PGA and PLGA PON-Nydroplobic and Non-hydropholic and shortage of cell adhesion PO-90 PLA, PGA and PLGA PO-	Hyaluronic acid	Glycosaminoglycan with negative charge, biocompatibility, forming hydrogel through cross-	functionalization and		58,63-6
clinical applications crystallinity tunable by changing hydroxylation degree PCL Excellent crystallinity and mechanical properties by injection PVA Hydroxylated synthetic polyvinyl acetate implants with various characteristics such as shape, porosity and degradation rate double bonds and the crosslinks may be toxic elegradation POP Remarkable mechanical properties Bioinert ceramic Clinical applications crystallinity tunable by shortage of cell adhesion changing hydroxylation degree Pop Sexcellent crystallinity and An crosslink in situ and print pogradation rate in years 70–73 Ability to manufacture implants with various characteristics such as shape, porosity and degradation rate Adjustable mechanical strength and rates of degradation Folyurethane (PU) Remarkable mechanical properties Bioinert ceramic Cannot perform medical reactions with living tissue	Synthetic polymer		0	reactions caused by acidic	
mechanical properties by injection PVA Hydroxylated synthetic Ability to manufacture 74–77 polyvinyl acetate implants with various characteristics such as shape, porosity and degradation rate PPF Has numerous nonsaturable double bonds and the crosslinks may be toxic degradation Polyurethane (PU) Remarkable mechanical properties Bioinert ceramic Cannot perform medical reactions with living tissue By injection 1 Ability to manufacture 74–77 Ability to manufacture 9 Ability to manufacture 94 Adjustable mechanical 98 Adjustable mechanical 98	PLA, PGA and PLGA	* *	crystallinity tunable by changing hydroxylation	J 1	67-69
polyvinyl acetate implants with various characteristics such as shape, porosity and degradation rate PPF Has numerous nonsaturable double bonds and the crosslinks may be toxic degradation Polyurethane (PU) Remarkable mechanical properties Bioinert ceramic Cannot perform medical reactions with living tissue implants with various characteristics such as shape, porosity and degradation 78,79 Adjustable mechanical strength and rates of degradation 80–82 80–82	PCL			Degradation rate in years	70-73
PPF Has numerous nonsaturable double bonds and the crosslinks may be toxic degradation Polyurethane (PU) Remarkable mechanical properties Bioinert ceramic Cannot perform medical reactions with living tissue Adjustable mechanical strength and rates of degradation 80–82	PVA	Hydroxylated synthetic	implants with various characteristics such as shape, porosity and		74-77
Polyurethane (PU) Remarkable mechanical properties Bioinert ceramic Cannot perform medical reactions with living tissue	PPF	double bonds and the	Adjustable mechanical strength and rates of		78,79
reactions with living tissue	Polyurethane (PU)	Remarkable mechanical	8		80-82
	Bioinert ceramic	Cannot perform medical			

83-86

Table 3 (Contd.)

Biomaterials	Characteristics	Advantages	Disadvantages	Ref.
Aluminum, e.g., α - aluminum oxide (Al ₂ O ₃)	Improve mechanical properties; lack of biological			
aluminum oxide (Al ₂ O ₃)	activity			
Zirconia	Interconnected structures;			87-89
	lack of chemical bonds and			
	biological reactions between			
Dia antina annonia	living tissues			
Bioactive ceramic	Can show medical reactions with living tissue after			
	implantation			
НА	The main inorganic	Highly biocompatible, non-		6,85,90,91
	component of natural bone	toxic and osteoconductive		
Tricalcium phosphate (TCP),	The ratio of calcium to	Biocompatibility, no	α-TCP has excessive	56,92-95
e.g., beta-tricalcium	phosphorus is close to	rejection and can provide	dissolution and rapid	
phosphate (β-TCP)	natural bone tissue	calcium and phosphorus for new tissue	degradation	
		new tissue	Degradation rate and osteogenic speed are	
			inconsistent	
Calcium sulfate (CaSO ₄)	CaSO ₄ is a good material to			96-99
	choose after tumor resection			
Akermanite (ca, Si, Mg)	Excellent mechanical			100-102
	properties and controllable			
	degradation rate			
	Better osteogenic differentiation and			
	increased gene expression			
	compared to β-TCP			
Diopside (MgCaSi ₂ O ₆)	Low temperature and fast			103-106
	firing and good thermal			
	expansion properties			
Bioactive glasses (BGs)	The main components for			107-113
	Na ₂ O, CaO, SiO ₂ and P ₂ O ₅ ; brittleness			

The third generation of biomaterials are designed to induce specific beneficial biological responses by the addition of instructive substances based on the second-generation biomaterials with excellent properties and/or new biomaterials with outstanding performance. Some of the instructive substances include, but are not limited to, biological factors or external stimuli.

5.2 Simple biomaterial scaffolds

Biomaterials such as metals, natural polymers, synthetic polymers, ceramics, and their composites have been widely used in biomedical fields for decades. Fig. 3a indicates the values (normalized by density) of stiffness and the strength of various materials by an Ashby plot.¹⁷ Natural materials, except silk that exhibits excellent toughness, have much lower values of strength and toughness than engineering materials. However, many natural materials have a toughness value that far exceeds their composition and their homogeneous mixture (as shown by the dashed line in Fig. 3b).¹⁷ Selection of matrix material plays a crucial role in the properties of bone scaffolds. Various polymers have been developed to fabricate bone tissue engineering scaffolds. An overview of different biomaterials including their characteristics, advantages, and disadvantages is given in Table 3.

5.3 Composite biomaterial scaffolds

Composite biomaterials are designed to combine two or more materials. The purpose of using composite materials is mainly to improve the processability, printing performance, mechanical properties and bioactivity of the scaffolds. Ti6Al4V, HA, β-TCP and BG are widely used as bioactive biomaterials due to specific biological reactions between scaffolds and living tissues. Bioresorbable biomaterials applied in bone tissue engineering are generally natural polymers (such as collagen, gelatin, silk fibroin, and chitosan), synthetic polymers (such as PLA, PGA, and PCL) and ceramic (such as HA, β-TCP, and BGs). Scaffolds containing additives (such as GFs) have been used in clinical applications because of their excellent bone regeneration capabilities. The general composite biomaterial scaffolds with additives (signaling molecules, stem cells, functional materials, and so on) for bone tissue engineering are summarized in Table 4, which include metal matrix composites, polymer matrix composites, ceramic matrix composites, and functional composites.

Bioactive metal matrix composites are widely used in clinical medical settings because of their outstanding mechanical properties, excellent biocompatibility, thermal stability, and corrosion resistance. Titanium, tantalum and their respective **RSC Advances** Review

Table 4 Summary of composites materials used to manufacture scaffolds for bone tissue engineering

Туре	Raw materials	Additives	Study outcome	Ref.
Metal	Ti6Al4V		Young's modulus similar to human natural bone,	114,115
matrix			improved the mechanical shielding	
composites	Ti6Al4V	Tantalum (Ta)	Better bone ingrowth in Ta-coated scaffolds	116
	Ti6Al4V	Simvastatin/Hydrogel	Significantly improved neovascularization,	117
			osteointegration and bone ingrowth	
	Ti6Al4V	HA/pDA	Significantly promoted bone regeneration and improved	118
	Ti6Al4V/Fibrin glue	Vascular endothelial growth factor	osteointegration and osteogenesis Significantly enhanced both osteogenesis and	119
	110A14V/F101111 glue	(VEGF) and BMP-2	angiogenesis for a single factor or dual factors, but	119
		(VEGI) and Bivil 2	synergistic effects of two-factor combination can	
			observe angiogenesis but lack osteogenesis	
Polymer	Bioactive glass (BG)	Collagen-glycosaminoglycan (CG)		120
matrix			the problem of inadequate graft vascularization in	
composites			tissue engineering	
	Poly(L/DL lactide) (PLDL)/PCL	Osteogenon-drug	8 1 ,	121
			adhesion and cell differentiation	
	PEG/PU	BMSCs	The polymer matrix is highly thermally stable,	23
			regulatable, degradable at an acidic pH (5.8),	
			biodegradable, cell compatible and has excellent	
	PLA	Bioactive organically modified glass	porosity The fibers are coated with different ormoglass	122
	LA	(ormoglass)	components and their properties (roughness, stiffness	122
		(omiogiass)	and morphology) are adjusted by altering the trial	
			parameters	
	Poly(D,L-Lactide) (PDLLA)	BGs and CuO/ZnO		123
			PDLLA, composite scaffolds can be obtained with	
			improved bioactivity	
Ceramic	Titanium dioxide	PLGA/gentamicin	Confirmed the effective antibacterial activity of the	124
matrix			released gentamicin and the compatibility of the	
composites	НА/β-ТСР	BMP-2	scaffold on osteoblast-like cells(MG-63) Real application possibilities for bone tissue	125
	TIA, p TOI	DMI 2	engineering purposes	123
	β-ТСР	Iron-containing	Iron maybe help to promote the bone conduction	126
	•	o .	properties of calcium phosphate (CaP) ceramics	
	n-HA/poly(D,L-lactide-co-	hMSCs		24
	glycolide) (PLAGA)			
	HA/Poly(D,L-lactic acid)-co-	BMSCs/rhBMP-2	Making the scaffolds suitable for evaluating bone	25
	poly-(ethylene glycol)-co-		regeneration approaches based on cell/the PELA/HA	
Eupational	poly(D,L-lactic acid) (PELA)	Tomporature	scaffolds with 500 ng of rhBMP-2	107
	Photocrosslinking of PCL and bioactive polydopamine	Temperature	The capacity to automatically fit into irregular defects and superior bioactivity because of polydopamine-	12/
	coating		coating	
	Polypyrrole (PPy), HA, gelatin	Electrical stimulation	Good mechanical properties, higher protein adsorption	128
	and mesoporous silica			
	PLGA	Black phosphorus (BP)/SrCl $_2$	The obtained scaffolds had good biocompatibility and	129
			good bone regeneration ability under near-infrared	
			(NIR) irradiation <i>in vivo</i> in rats	
		hMSCs and electrical stimulation	Enhanced cell adhesion and growth	130
	Gelatin/bioactive glass	Poly(3,4- ethylenedioxythiophene):poly(4-	Adding PEDOT stabilizes the structure of scaffolds and	131
		styrene sulfonate) (PEDOT:PSS) and	enhances the cellular properties of mesenchymal stem cells	
		electrical stimulation	COLD	
	Transglutaminase cross-	BMP-2, matrix rigidity and	The combination of hydrogel hardness and BMP-2 has	132
	linked gelatin (TG-Gel)	mechanical signaling	a synergistic effect on cellular osteogenic differentiation	

alloys are considered to be the preferred biomaterials for scaffolds. However, the high costs of manufacturing scaffolds limit their widespread development. Ti6Al4V is an outstanding representative of metal matrix composites. Young's modulus of the suitable porous Ti6Al4V scaffolds can be similar to natural bone and improve the mechanical shielding to the living tissue.114,115 The Ti6Al4V scaffolds can significantly increase

bone ingrowth, osteointegration, and osteogenesis by covering the tantalum coating,116 adding simvastatin/hydrogel,117 or polydopamine-assisted hydroxyapatite coating (HA/pDA),118 as summarized in Table 4. Although metal matrix composites, such as Ti6Al4V, have many outstanding advantages; the nonbiodegradable properties of metal matrix composites fundamentally limit their potential to become ideal materials.

Review

(a) Malleable at
T > 56 °C

2 on

1 cm

1 cm

1 cm

1 cm

1 cm

Stirring
Solvent
evaporation
W: PVA

O/W emusion

BP-Srchi/PLGA
microspheres

8 w

N/R irradiation

8 w

Sr^h

Fig. 4 Functional composite bone tissue engineering scaffolds. (a) Effect of temperature on the scaffolds. Reproduced from ref. 127 with permission from Elsevier, copyright 2014. (b) Effect of near-infrared light on the scaffolds. Reproduced from ref. 129 with permission from Elsevier, copyright 2018.

In recent years, the application of polymer matrix composites and ceramic matrix composites has made great progress in bone tissue engineering scaffolds. Polymer composites have various excellent properties, such as biodegradability and mechanical properties. 122-131 Ceramic materials, especially HA, are the main inorganic constituents of natural bone.19 Composite materials composed of ceramic materials and polymer materials have desirable properties for the manufacturing of scaffolds for bone tissue engineering. 125,126,130,131 The composite scaffolds with additives (signaling molecules, stem cells and functional materials) have superior performance compared to just composite scaffolds (Table 4). The composite scaffolds with additives could further enhance the performance of the scaffolds. As shown in Fig. 4a, scaffolds with bioactive polydopamine coating have the capacity to automatically fit into irregular defects at higher temperatures. Wang et al. fabricated BP-SrCl₂/PLGA scaffolds for rat femoral defects, and the nearinfrared light-triggered platform significantly enhanced bone regeneration, as seen in Fig. 4b.129

6. Conclusion

In this paper, the summarized literature, which involves biomaterials for bone tissue engineering scaffolds, has been reviewed. The application and properties of various biomaterials used to fabricate scaffolds have also been elaborated. In particular, composite materials such as metal matrix composites, polymer matrix composites, ceramic matrix composites, and functional composites have been discussed. It was found that additives such as signaling molecules, stem cells, and functional materials can enhance the performance of the

scaffolds. Although it was impossible forty years ago to find a material that is not repelled by living tissue, nowadays biomaterials have been used for bone repair. Improved performance of ideal biomaterials is required for their positive interactions with host tissues. The approaches for bone regeneration will make giant steps with the exploitation of novel biomaterials and new strategies, particularly the deep integration of nanotechnology, stem cell science and other fields.

Abbreviations

3D	Three-dimensional
ECM	Bone extracellular matrix
GFs	Growth factors
CPs	Conducting polymers
MeSH	Medical subject heading
BS/BV	Bone surface to bone volume
HA	Hydroxyapatite
n-HA	Nano-hydroxyapatite
CAD	Computer-aided design
CAM	Computer-aided manufacturing
PMMA	Poly(methyl methacrylate)
PEEK	Polyether ether ketone
PLA	Poly(lactic acid)
PGA	Poly(glycolic acid)
PLGA	Poly(lactic-co-glycolic acid)
PVA	Poly(vinyl alcohol)
PPF	Poly(propylene fumarate)
PU	Polyurethane
Al_2O_3	α-Aluminum oxide
TCP	Tricalcium phosphate
β-ТСР	beta-tricalcium phosphate
CaP	Calcium phosphate
$CaSO_4$	Calcium sulphate
HA/	polydopamine-assisted hydroxyapatite coating
pDA	
Ta	Tantalum
CG	Collagen-glycosaminoglycan
PLDL	Poly(L/DL lactide)
BP	Black phosphorus
NIR	Near-infrared
BMSCs	Bone marrow stromal cells
PEG	Poly-(ethylene glycol)
PDLLA	Poly(D,L-Lactide)
BMP-2	Bone morphogenetic protein 2
VEGF	Vascular endothelial growth factor
PELA	Poly(D,L-lactic acid)-co-poly-(ethylene glycol)-co-
	poly(D,L-lactic acid)
PLAGA	Poly(D,L-lactide-co-glycolide)

rhBMP- Recombinant human bone morphogenetic protein-2

PSS poly(3,4-ethylenedioxythiophene): poly(4-styrene

Human mesenchymal stem cells

TG-Gel Transglutaminase cross-linked gelatin

PPy/Alg Polypyrrole/alginate

sulfonate)

hMSCs

PEDOT

Conflicts of interest

There are no conflicts to declare.

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