

Cite this: *Mater. Adv.*, 2023,
4, 52

COVID-19 mitigation: nanotechnological intervention, perspective, and future scope

Arpita Adhikari,^{†a} Dibyakanti Mandal,^b Dipak Rana,^{ib}*^c Jyotishka Nath,^{‡a} Aparajita Bose,^d Sonika,^e Jonathan Tersur Orasugh,^{*fg} Sriparna De^{*h} and Dipankar Chattopadhyay^{ib}*^a

COVID-19 infections and severe acute respiratory syndrome (SARS) have caused an unprecedented health crisis across the globe with numerous deaths, as well as causing a tremendous economic crash worldwide. To combat this acute pathogenic coronavirus strain, a vital strategy of safe and effective diagnostic and therapeutic measures is highly important and demanding at present. Instead of conventional diagnosis tools, nanotechnology offers inspiring options for therapeutic applications that can ward off the disease from spreading further and remove the threat of this virus causing future pandemics. Physicochemically tuned nanomaterials can be exploited in upgrading detection schemes for viral antigens, nano-vaccines, and inhibitors of the cytokine storm, which are vital in the fight against COVID-19. The one-of-a-kind nanoscale biosynthesis of synthetic nanoparticles can efficiently imitate and interact with the structurally similar spike proteins present on the viral surface. Given this, we envision the precise and concurrent amalgamation of nanoscience and nanotechnology, leading to new avenues that can disrupt the development of viruses and limit the length of the viral lifespan. Current and developing nanotechnology approaches enable the development of therapeutic and precautionary pathways to curb this disease and identify crucial methods in the field of nanoscience for developing upcoming antiviral systems. In this review article, we also present a synopsis of the latest studies on the efficacy of nanoparticles (NPs) as antiviral or diagnostic devices against most viruses. Engineered NPs capable of tempering the patient's immune response can have a pronounced impact in mitigating inflammatory reactions as well as the design of potent nano-vaccines and drugs against viral pandemics such as COVID-19. In summary, state-of-the-art approaches based on nanotechnology can be critically deployed to counter future pandemics including COVID-19 and function at the forefront in tackling various new dangerous viral threats.

Received 30th June 2022,
Accepted 4th October 2022

DOI: 10.1039/d2ma00797e

rsc.li/materials-advances

^a Department of Polymer Science and Technology, University of Calcutta, 92 A.P.C. Road, Kolkata 700 009, India. E-mail: dcpst@caluniv.ac.in^b Department of Microbiology, Faculty of Life Sciences, PDM University, Sector 3A, Bahadurgarh, Haryana 124 507, India^c Department of Chemical and Biological Engineering, University of Ottawa, 161 Louis Pasteur St., Ottawa, ON, K1N 6N5, Canada. E-mail: rana@uottawa.ca^d Department of Chemistry, University of Calcutta, 92 A.P.C. Road, Kolkata 700 009, India^e Department of Physics, Rajiv Gandhi University, Rono Hills, Doimukh, Arunachal Pradesh 791 112, India^f Department of Chemical Sciences, University of Johannesburg, Doornfontein, Johannesburg 2028, South Africa^g DST-CSIR National Centre for Nanostructured Materials, Council for Scientific and Industrial Research, Pretoria 0001, South Africa. E-mail: JOrasugh@csir.co.za^h Department of Allied Health Sciences, Brainware University, Barasat, Kolkata 700 125, India. E-mail: sd.ah@brainwareuniversity.ac.in[†] Present address: Faculty of Engineering, Indian Institute of Technology, Kharagpur 721 302, India.[‡] Present address: Department of Chemistry, Southern Methodist University, Dallas, TX 75205, USA.

1. Introduction

The world is under threat from a relentless minuscule enemy, which was unknown to mankind but is now causing serious illness and infections. As countries across the globe initiate unparalleled techniques to dampen the further spread of COVID-19, a major startling conclusion is that there is still no clear way out of this viral disease. Community scrutiny, rapid testing, contact tracing, social distancing, and swift clinical care are the rudimentary prevention schemes being employed worldwide. However, we do not understand exactly how long these measures need to be imposed or what extent of relaxation will cause the virus to resurge. Numerous contagious diseases spread by viruses have recently come to light, such as SARS-CoV, Ebola virus, and dengue virus, resulting in the demand for advanced antiviral treatments and personal protection equipment (PPE) to combat these contagious agents.¹ A cornerstone strategy for maintaining a healthy environment includes



appropriate use of disinfectants (cleaning, disinfecting, and hand hygiene) and protective respirator face masks to act as a safeguard for the nose and mouth of the wearer, preventing the spread of droplets carrying viruses or other infectious pathogens. In this context when regular health aid is provided, health professionals prescribe critical care for patients and ensure that the infection is prevented, and infection prevention and control (IPC) measures are carried out and followed in healthcare facilities to curb healthcare-related infections. To prevent infection in healthcare facilities, the WHO suggests the application of contact and droplet precautions by healthcare employees for the treatment of COVID-19 patients.^{2,3} The WHO also endorses

that airborne measures be taken in these settings, emphasizing that the right use of PPE kits is essential, including face protection, goggles, masks and face shields, gloves, gowns, head coverings, and rubber boots. Furthermore, exploration in the fields of nanoscience and nanotechnology can serve to add an extra protective shield to prevent infection colonization in healthcare professionals.^{4,5} To date, numerous viral diseases have surfaced in the global community, which have turned out to be a serious threat to the population. Besides the common cold, diseases conditions including influenza, herpes virus, viral encephalitis, herpes keratitis, neonatal disseminated infections, prolonged distress, and sometimes persistent infections of hepatitis viruses



Arpita Adhikari

Dr Arpita Adhikari obtained her PhD from the Department of Polymer Science and Technology at the University of Calcutta, India. She is presently working as a Research Associate at the Electronics and Electrical Communication Engineering Department at IIT Kharagpur. She has engineered conducting polymers with certain morphological arrangements such as nanorods and nanoribbons and their various metal nanocomposites, which exhibited considerable efficiency for sensor applications in her PhD tenure. She is currently engaged in the preparation of various quantum dots and 2D materials for energy, biomedical and sensing applications. E-mail: https://arpita.adhikari2011@gmail.com.



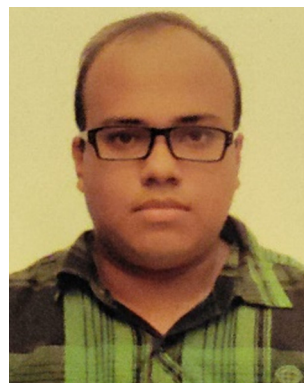
Dibyakanti Mandal

Dr Dibyakanti Mandal is an internationally known molecular virologist. He is presently working as an Associate Professor in the Department of Microbiology at PDM University, Bahadurgarh (Delhi-NCR). Dr Mandal did his PhD on the Molecular Characterization of Human Immunodeficiency Virus Type-1 from Calcutta University, Kolkata. He then worked as a Postdoctoral Fellow and Staff Scientist at University of Iowa, USA. His research is focused on understanding the pathogenesis of RNA viruses including HIV, influenza, coronavirus, RSV and Chandipura virus. He has published research works in reputed journals such as Nucleic Acids Research, Journal of Virology, and AIDS Research and Human Retroviruses. He also serves as an editorial and reviewer board member of several international biomedical journals. E-mail: https://dkmandal2000@yahoo.com.



Dipak Rana

Dipak Rana is presently a Senior Research Scientist in the Industrial Membrane Research Institute, Dept. of Chemical and Biological Engineering, University of Ottawa, Canada. Dr Rana has been a member of various organizations, such as the Indian Chemical Society, Society for Polymer Science, Society of Plastics Engineers, and American Chemical Society. He was awarded a PhD in Science from Jadavpur University, Calcutta, when he was working at the Indian Association for the Cultivation of Science, Calcutta, India. Dr Rana has published over 275 professional papers with a total citation count of over 13 125 and h-index of 60 from Scopus. E-mail: https://ranadipak@hotmail.com.



Jyotishka Nath

Jyotishka Nath completed his Master's in Chemistry from IIT (ISM) Dhanbad, India. He submitted his Master's thesis on the 'Synthesis and Characterization of Cd(II) Metal-Organic Frameworks'. After graduation, he pursued an internship at the University of Calcutta, where he explored conductive polymers and their nanocomposites for various sensing applications. He worked as an intern at IISER Kolkata, where he performed RAFT polymerization to synthesize biopolymers from cholic acid-based monomers. He worked as a research and development personnel at Kanopy Techno Solutions Pvt. Ltd. He is now a Graduate Student at Southern Methodist University in Dallas, Texas. E-mail: https://jyotishka95@gmail.com.



(namely hepatitis B virus (HBV) and hepatitis C virus (HCV)) or human immunodeficiency virus (HIV) can ultimately lead to severe immunodeficiency diseases, and in some cases even cancer. Thus, considerable struggles have been encountered in attempts to effectively deal with these viral diseases.^{6,7}

Nanotechnology and nanoscience as a whole involve the development, progress, and utilization of atomic and molecular

structures, which have one of their dimensions in the nano-scale (1–100 nm), involving different constitutions, shapes, structures, size, and surface properties. Nanotechnology-based cutting-edge technology has emerged with the potential to reveal significant alternatives that can constrain the spread of virions. The synergism of nanoparticles in the fields of physics, chemistry, biology, materials science, and medicine



Aparajita Bose

Ms Aparajita Bose is currently pursuing her Master's from the University of Calcutta, India. She has completed her Bachelor's from Amity University, Kolkata, India. She has previously worked on synthesizing and characterizing various nanomaterials and studied their anticancer activity. In the future, she plans to work extensively in the field of nanoscience and pursue a PhD in the same. E-mail: https://aparajitabose00@gmail.com.



Sonika

Dr Sonika is working as an Assistant Professor on the regular post in the Department of Physics, Rajiv Gandhi University, Rono Hills, Doimukh, Itanagar, Arunachal Pradesh, India. She received BSc and MSc degrees from Ch. Charan Singh University, Meerut, India in 2002 and 2004, respectively. She has been awarded PhD degree from the Department of Physics, Aligarh Muslim University, Aligarh, India in 2010. She was a Research Associate at Nuclear Physics Division, Bhabha Atomic Research Centre, Mumbai, India (April 2014–March 2016) and also was Post-Doctoral Fellow at Theory Division, Saha Institute of Nuclear Physics, Kolkata, India (October 2010–September 2011). She has also teaching experience of about 06 years after completing the PhD. She has published several research papers in the reputed international journals. Her main research work is associated with Nuclear Structure, Nuclear Reaction, Accelerators and Instrumentation for Nuclear Physics. Her current research interest is Energy Harvesting, Nano Technology, Nano Materials, Advanced polymers, Nuclear Structure, Nuclear Reaction, Accelerators and Instrumentation for Nuclear Physics. E-mail: https://sonikag7@gmail.com.



Jonathan Tersur Orasugh

Dr Jonathan Tersur Orasugh earned his PhD in Nanoscience and Nanotechnology at the University of Calcutta, India. He is currently a Postdoctoral Fellow at the University of Johannesburg's Department of Chemical Sciences and a Senior Researcher at the Centre for Nanostructures and Advanced Materials, DSI-CSIR Nanotechnology Innovation Centre, Council for Scientific and Industrial Research, Pretoria, South Africa. Dr Orasugh's research focuses on the effect of various nanoparticles on the behavioral properties of polymeric matrices or their blends, with applications in drug delivery, edible/non-edible packaging, adsorption, catalysis, and so on. E-mail: https://JOrasugh@csir.co.za.



Sriparna De

Dr Sriparna De is currently working as an Assistant Professor in the Department of Allied Health Sciences, Brainware University. She also has post-doctoral experience in the DST-SERB project entitled "exploration of the role of biopolymers based nanohybrids in cancer therapeutic applications". Her PhD was in the field of biopolymer-based nanotechnological intervention towards sensor applications. Her research area focused on the implication and role of nanoparticles and biopolymer-based nanohybrids as drug delivery vehicles in cancer therapeutic applications. She has published 15 research publications and 2 book chapters. E-mail: https://sd.ah@brainwareuniversity.ac.in.



encourages the application of this technology in the field of materials design. In the medical sector, nanotechnology-driven biosensing arrays have been extensively adopted for the detection of viruses. Recently, biochemical research has opened a new avenue, wherein novel nanomaterials are fabricated with advanced biocompatibility using virions and virus-like templates. Currently, widespread outbreaks of viral respiratory infections have been reported worldwide. The scientific community is desperately seeking to optimize and design appropriate nano-vaccines and therapeutics, involving the latest nano-based approaches. This versatile nanotechnological paradigm is encouraged by virologists to continuously develop novel delivery devices, which will also be at the vanguard in fighting deadly viruses.

The ongoing pandemic has definitely ravaged the world and there will be many more in the future. Thus, it is necessary for the nano biomaterials research fraternity to come up with appropriate measures to combat COVID-19 and associated pandemic-causing agents in the near future. Nanotechnology and nanoscience-inspired materials such as non-woven disposable materials, antiviral coatings, PPE, multifunctional surfaces, air-conditioning filters, antibacterial textiles, and antiviral fabrics are among the many candidates attracting attention to provide solutions rapidly.⁸

Nanotechnology-based interventions should be put into full effect to counteract COVID-19 and subsequent outbreaks by various means, as follows: (i) development of contact tracing tools, (ii) fabrication of novel surfaces and surface coatings that aid in virus resistance, virus adhesion, and inactivation, (iii) production of fine mesh face masks and blood filters, (iv)

advanced tests for the rapid, sensitive and highly specific detection of infection and immunity, and (v) innovative drugs and vaccines encompassing nanomaterials capable of transferring broad range antiviral cargo or therapies to the lungs. The current crisis has also given us a stern reminder regarding the urgent need to critically analyse unforeseen circumstances stemming from the pandemic. Thus, a roadmap is mandatory to guide the systematic and rapid production of PPE and ventilators. Accordingly, nanotechnology may prove to be useful in aiding the manufacture of equipment by offering strategies for precursor synthesis together with improvement in durability and efficacy. In the following sections, our discussion focuses on the role of nanotechnology in dealing with and mitigating the ill effects of COVID-19 and similar pandemics the future.^{9,10}

1.1. History of outbreaks

The last report of an outbreak was the deadly ‘atypical pneumonia’, which appeared in November 2002, in the region of Guangdong Province, China. Subsequently, a similar occurrence was reported in March 2003, in Hong Kong. Similar types of respiratory disorders were successively reported worldwide including in Taiwan, China, Singapore, Vietnam, the USA, and Canada. This syndrome with new clinical symptoms has been equated with ‘severe acute respiratory syndrome (SARS)’.¹¹ SARS mainly originated from viruses associated with the *Coronaviridae* family, known as SARS-coronavirus (SARS-CoV).¹² However, sequence data indicates that SARS-CoV is not like previously known coronaviruses.¹³ On 22nd September 2012, the United Kingdom notified the WHO regarding a case study of a 49 year-old male from Qatar having a travel history to Saudi Arabia and Qatar and suffering from ‘acute respiratory syndrome’ and renal failure.¹⁴ The WHO termed the provisional case as “severe respiratory disease associated with novel coronavirus” dated September 25, 2012. On 29th September, this was revised to Severe Acute Respiratory Infections associated with novel coronavirus infection (SARI associated with nCoV). According to laboratory-confirmed reports from May 12, 2013, 34 cases were reported due to Middle East respiratory syndrome coronavirus (MERS-CoV). Also, there were 20 deaths with two cases from previous records of the Jordanian cluster of this class of disease confirmed by the Health Ministry of Jordan in April 2012.

Among the various CoV strains, the most infectious strains are alpha-coronaviruses and beta-coronaviruses, which affect mammals, whereas gamma-coronaviruses and delta-coronaviruses affect birds. Before 2019, only 6 CoVs were recognized, among which HCoV-229E, HCoV-OC43, HCoV-NL63, and HKU1 cause mild disease in the upper respiratory area together with fatal infection in infants, youth, and older patients. SARS-CoV and MERS-CoV can contaminate the lower respiratory tract and induce severe respiratory syndrome in people. Most importantly, the new coronavirus 2019-nCoV belongs to beta-coronaviruses, which can significantly affect the lower respiratory tract followed by the development of pneumonia. According to the WHO report on 31st December



Dipankar Chattopadhyay

Dr Dipankar Chattopadhyay is an eminent Professor currently working in the Department of Polymer Science and Technology, University of Calcutta, India, as well as a former HOD. He obtained his BTech in Plastics and Rubber Technology from the University of Calcutta, India, and MTech in Polymer Science and Engineering, IIT, New Delhi, with a PhD (Polymer Science Unit) from the IACS, University of Calcutta, India. He is an experienced research professional with expertise in polymer nanocomposites, biomaterials, conducting polymers, and nanomaterials. He has ~24 years of research experience and has completed more than 12 research projects and collaborative projects with industries. He is an active reviewer for various journals and supervised 12 scholars and five post-doctorate students. He has more than 127 publications and 3 patents. He is an Executive Member in the Society for Polymer Science, India; Material Research Society of India; Vice President, Indian Rubber Institute, Calcutta Chapter; and many more. E-mail: <https://dipankar.chattopadhyay@gmail.com>.

Dr Dipankar Chattopadhyay is an eminent Professor currently working in the Department of Polymer Science and Technology, University of Calcutta, India, as well as a former HOD. He obtained his BTech in Plastics and Rubber Technology from the University of Calcutta, India, and MTech in Polymer Science and Engineering, IIT, New Delhi, with a PhD (Polymer Science Unit) from the IACS, University of Calcutta, India.

He is an experienced research



2019, the Wuhan Municipal Health Commission of China indicated the existence of a cluster of cases of pneumonia in Wuhan, Hubei Province. Subsequently, a new coronavirus was detected. As of the 3rd of January 2020, about 44 patients having pneumonia of unknown etiology were identified, and the WHO was notified by the national authorities in China. On the 5th of January, the WHO announced that China was dealing with a significant new viral outbreak. At the end of January 2020, 9826 cases were reported globally with 9720 confirmed cases within China. Consulting existing data available on many websites about COVID-19 infections worldwide made it evident that the number of cases was increasing exponentially. As of June 10th, 2020, there were 7 323 918 confirmed cases including 413 733 deaths and 3 604 500 recovered cases worldwide.^{15,16}

The mode of transmission of a few CoVs is livestock, birds, bats, mice, whales, and many other wild animals. A report showed that swine acute diarrhea syndrome coronavirus (SADS-CoV) led to a major outbreak (in 2016) of a deadly disease in pigs in Southern China, which caused the death of 24000 piglets.¹⁷ This case was the first identified spillover of a bat coronavirus, which triggered deadly disease in livestock. 2019-nCoV and Beluga Whale CoV/SW1 belong to separate genera and diverse host spectra. Hence, the pathogenesis of CoVs needs further research to be identified to understand the specific action of these viruses.^{18,19}

1.2. Structure of COVID-19

According to the genomic and phylogenetic morphology of COVID-19, it is from the *Coronaviridae* family in the order *Nidovirales*, which is classified into alpha-coronavirus, beta-coronavirus, gamma-coronavirus, and delta-coronavirus. Among them, the beta-coronavirus genera can affect mammals, causing SARS-CoV.^{20,21} Considering its genomic structure, COVID-19 is composed of single-stranded RNA (+ssRNA) (~30 kb) with a 5'-cap structure and 3'poly-A tail. This is enveloped with a capsid comprising nucleoprotein and matrix protein, containing one of the longest genomes (26.4–31.7 kb) of all known RNA viruses. Also, it possesses various small open reading frames (ORFs), which exist among several genes such as ORF1ab, spike, envelope, membrane, and nucleocapsid. Polypeptides encoded by chymotrypsin-like protease (3CLpro) and one or two papain-like proteases are produced from these ORFs. Additionally, the 4 major structural proteins include spike (S), membrane (M), envelope (E), and nucleocapsid (N) proteins and various accessory proteins, such as the HE protein, 3a/b protein, and 4a/b protein, which are predominantly accountable for virus replication and genomic integrity.^{20,22} Based on the viral entry within the host cell, spike proteins, specifically, glycoprotein (M), play a pivotal role towards therapeutic targets, triggering the engulfment of the virus onto host cell membrane by releasing the NH₂ terminal moiety on the outer wall of the virus and long carboxylic cytoplasmic terminus in the virion (Fig. 1).²³

Meanwhile, the S protein is the prime facilitator of neutralizing antibody activities. Recognition and binding with the host cell and entry between the wall of the virus and the host

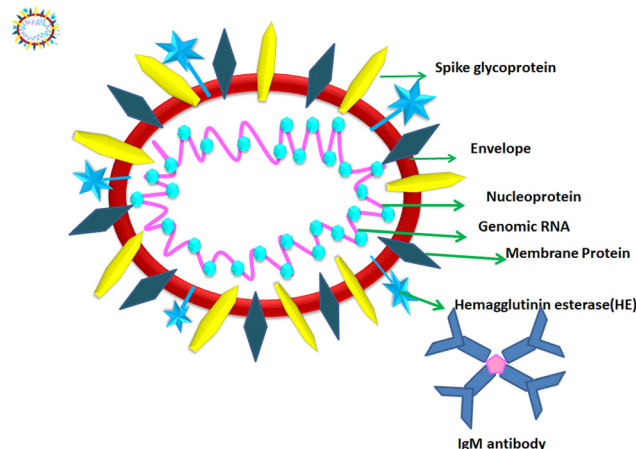


Fig. 1 Schematic structure of SARS-Cov-2 and its possible targets for diagnosis.

cell surface are governed by two subunits of the S protein, *i.e.*, S1, and S2. Interestingly, M plays a significant roles in the intracellular formation of virus particles through interaction with S proteins. The spike protein plays a dual role in virus pathogenicity. The S1 subunit consists of a receptor binding domain (RBD), an amino-terminal domain (NTD), and a C-terminal domain. RBD is responsible for binding the receptor and ACE2, which is present on the lung epithelial cells, for entry. Both RBD and NTD are the major contributors to the virus antigenicity, thus and neutralization antibodies are targeted to these regions of the S1 subunit of the spike proteins. Some neutralization antibodies also target CTD of S1. The S2 subunit forms a trimeric core of the spike protein and is mainly involved in virus fusion with the cell membrane.²⁴ COVID-19 disease is associated with hyperinflammation and increased levels of inflammatory cytokines. This is termed the 'cytokine storm syndrome (CSS)' and is the cause of severe disease, respiratory failure, and death. Studies showed that the S protein alone can trigger this cytokine storm and different pathways have been proposed. Increased levels of pro-inflammatory cytokines including IL-6, IL-2, IL-1 β , IL-8, IL-17, GM-CSF, MCP-1, and TNF- α were reported in COVID-infected individuals. Increased levels of cytokines lead to the recruitment of immune cells, which is the cause of CSS.^{25,26} Thus, vaccines were designed based on the spike proteins and found to be effective. However, COVID still continues to threaten individuals of all age groups and from all geographical regions even after three years since the pandemic began. India experienced and is still experiencing more than around 10 000 daily cases and 50–100 deaths. Although effective vaccines have been introduced and the majority of individuals completed two doses of the COVID-19 vaccine, significant virus activity is still being observed. The main reason for this is the emergence of mutant viruses that escape our immune system against the virus. The WHO categorized these COVID-19 variants into three categories, namely, VUI (variant under investigation), VOI (variant of interest), and VOC (variant of concern). All these variants have several mutations within the spike protein (S).



These mutations cause changes in the binding affinity of the virus to its receptor angiotensin-converting enzyme 2 (ACE2) and can also alter the levels of an immune response. VOCs are the major cause of serious disease including respiratory distress and deaths among COVID-19-infected individuals. The alpha variant or B.1.1.7 was isolated in the UK; the beta variant or B.1.351 first was isolated from South Africa; the gamma variant of P.1 was isolated from Brazil and the delta variant or B.1.617.2 was isolated from India, where the latter is the most deadly strain among them. The D614 mutation in S1 is the signature of this strain. Other common mutations are in the RBD domain of S1, which result in the stronger binding affinity of the virus to ACE2 and also cause hyperinflammation, leading to CSS.²⁷ Recently, the omicron variant B.1.1.529 was identified as the most rapidly spreading variant; however, the severity of the disease caused by this variant is much less compared to other VOCs. In this variant, 30 mutations were reported in the RBD region of S1.²⁸ These mutations caused increased transmissibility and immune evasion, even in vaccinated individuals. Because of the emergence of these variants, vaccine producers and policymakers require changes in existing strategies to control the global COVID-19 pandemic. Within these genera, the exploration and cultivation of various nanoparticles can inhibit the active spread of virions.²⁸ The utilization of nanoparticles can inactivate the infectivity and restrict the adherence property on abiotic surfaces and impact the intracellular environment.

1.3. Mechanism of entry of viruses into host cells

These viruses are sustained *via* multiplication in host cells. The process of infection includes attachment, penetration, uncoating, replication, assembly, and release. There are several specific receptors identified on the host cell membrane by which viruses enter cells utilizing the attachment proteins within the viral capsid or viral envelop-decorated glycoproteins. Based on the virus specificity, various infectivity schemes were found, wherein RNA viruses such as CoV put their genome to use to synthesize viral genomic RNA and mRNA, eventually resulting in the production of new viruses in the host cells. Bacteriophages gain entry into the host cell *via* nucleic acids, whereas their capsid remains outside the cell. Few animal and plant viruses gain entry to host cells *via* endocytosis. Upon entry in the host cell, CoVs use their genomics to synthesize viral genomic RNA and mRNA, and eventually the new virions into the host cells (Fig. 2).^{29–31}

A pivotal route of viral entry of the influenza virus, respiratory syncytial virus, and parainfluenza virus is identified as the human respiratory mucosa. The virulence nature and pathogenicity promote infection in the upper respiratory tract, leading to severe illness in the lower respiratory tract and morbidity and mortality. Majorly respiratory tract infections evolved due to SARS-CoV, MERS-CoV, and SARS-CoV-2.³² Due to its fascinating morphology, the entry mechanism in host cells involves the interaction between the host-receptor cells and the angiotensin-converting enzyme 2 (ACE2) protein site, which

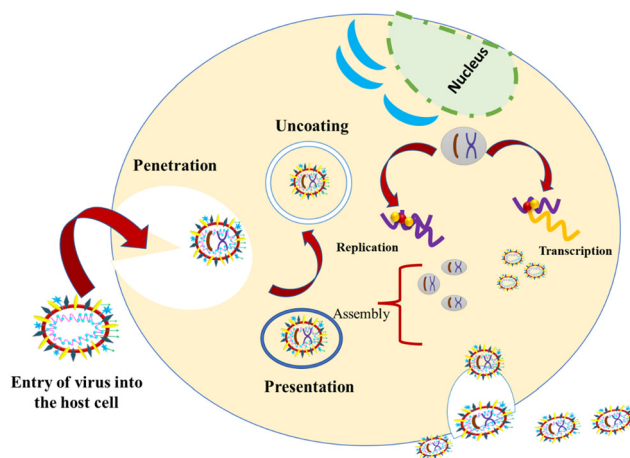


Fig. 2 Possible mechanism of viral activity within the host cell.

is associated with host-cellular membrane fusion followed by the release of genetic material into the host cytoplasm.

In the case of SARS-CoV-2, the spike S glycoprotein is also responsible for bonding and entrance into the cell. The unique morphological features of the S protein trigger the attachment, fusion, and entry of the virus in the host cells.^{33–35} Therefore, blocking the ACE2 receptor binding site, thereby hindering the viral endocytosis pathway, is a compelling route toward drug discovery and therapeutics.

2. Effectiveness of nanomaterials targeting spike proteins (SP) to prevent COVID-19 spread

The antiviral mechanistic approach of nanoparticles should target the viral endocytosis process including attachment, penetration, replication, and budding of viruses. Various morphological architectures possibly influence the blocking of viral replication.²⁹ Importantly, nanoparticles restrict the above-mentioned processes by varying the structural features of the capsid protein, thereby suppressing its virulent property, which may be ascribed to physicochemical methods of reducing the active viral levels (Fig. 3).

To facilitate their passage in the host cell, viruses use spike proteins triggered by certain enzymes including furin, trypsin, and cathepsin L9.⁴⁰ Among them, furin has the most accelerating effect on the spike protein located on the novel coronavirus cell membrane.

This enzyme reveals unique and fascinating properties given its ability to exist in human tissues including the lungs, liver, and small intestine, which facilitate the virus invading the host cell in a manner distinct from other SARS family viruses and modes of transmission. A recent investigation pin-pointed the chain of infection of the influenza family virus, wherein the haemagglutinin protein lies on the activation site, lucid from CoV SP, causing alteration in the contagious virus transmission channel. Also, scientific evidence demonstrates that furin and



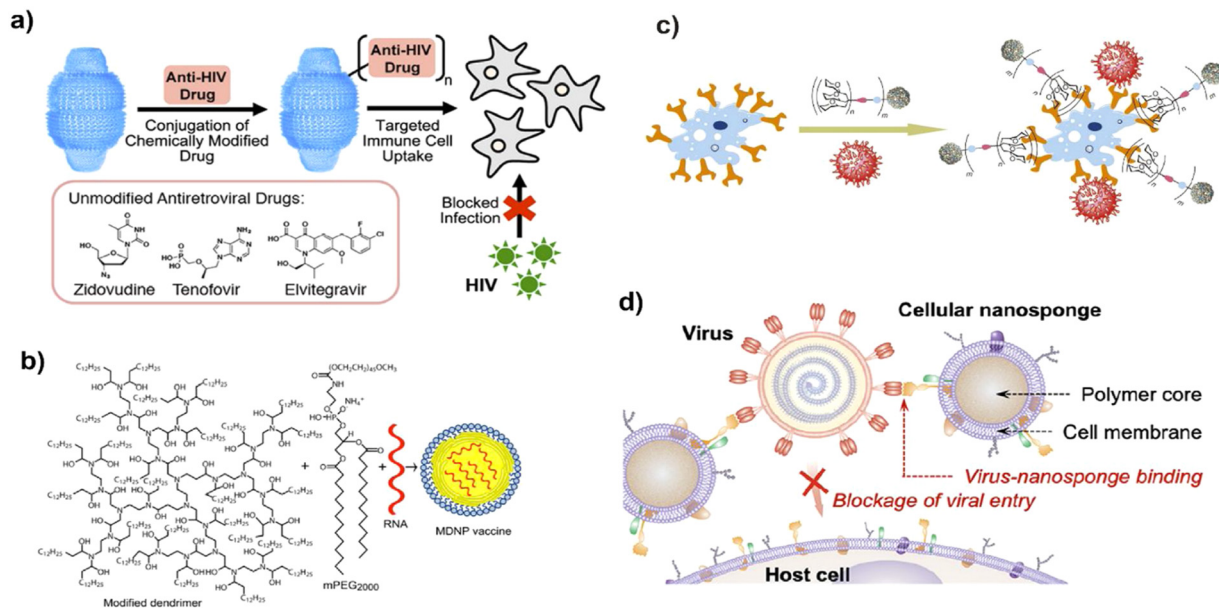


Fig. 3 Possible modes of the antiviral efficacy of nanotechnology. (a) Effect of antiviral drug delivery against HIV-1 infection, adapted from Fulcher *et al.*³⁶ Copyright 2019, American Chemical Society. (b) Schematic of vaccine delivery using lipid-derived dendrimer nanoparticles through m-RNA. Reproduced with permission from Chahal *et al.*³⁷ Copyright 2016, National Academy of Sciences, USA. (c) Blocking approach of virus-like glycodendrimer nanoparticles to the infection site, adapted from Ribeiro-Viana *et al.*³⁸ Copyright 2018, Nature Publishing Group. (d) Strategy of mimicking host cell membrane carrying nanodecoy host cell membrane for adsorbing Zika virus, adapted from Zhang *et al.*³⁹ Copyright 2020, American Chemical Society.

furin-like proteases such as fusogenic envelope glycoprotein of SARS CoV are the most susceptible sites for targeting treatment practice (Fig. 4).

The emergence of COVID-19 variants is a concern. Thus, in this regard, nanotechnology-based approaches are expected to be beneficial, providing better safeguards to tackle this COVID-19

pandemic. Recently, several nanoparticle-based strategies have been developed to prevent the spread of the mutant viruses. One approach is a lipid nanoparticle-based mRNA vaccine called mRNA-LNP, which is based on spike mRNA from new variants. Another effective approach is nanoparticle-based engineered neutralizing antibodies against variants of S proteins, where synthetic antibodies with antigen binding regions specific for new COVID-19 variants are designed.⁴¹ Given that all the variant stains of COVID-19 utilize ACE2 as a receptor and do not bind another molecule for entry, nanoparticle-based ACE2 decoys are expected to be more effective in preventing the virus spread. In this technology, the strong interaction of ACE2 receptors of decoy nanoparticles traps the virus of different variants and stops causing serious disease. Another nanotechnology-based method is the nonspecific physical inactivation of virus variants using polymer surfactants and pore-forming peptides. Nanoparticle-based anti-inflammatory drugs also show promise against COVID-19 variants of concern.⁴²

2.1. Implication of biosensors to screen SARS-CoV-2

It is considered that the factors of high transmissibility and the infectious nature of the COVID-19 virus are attributed to its heavy viral load in the upper respiratory area together with the inference that several patients do not show symptoms, thereby spreading the virus. Crucial nanotechnological interventions to fight pandemics include the inhibition of pathogen spreading, activation of suitable diagnostic tools, and proper immunization. For instance, the nanodiagnostic scheme relies on the specific interaction between nanoparticles and the target analyte to yield a quantifiable signal output, thereby catering to the identification of biomarkers or pathogens in their embryonic stages (Fig. 5).

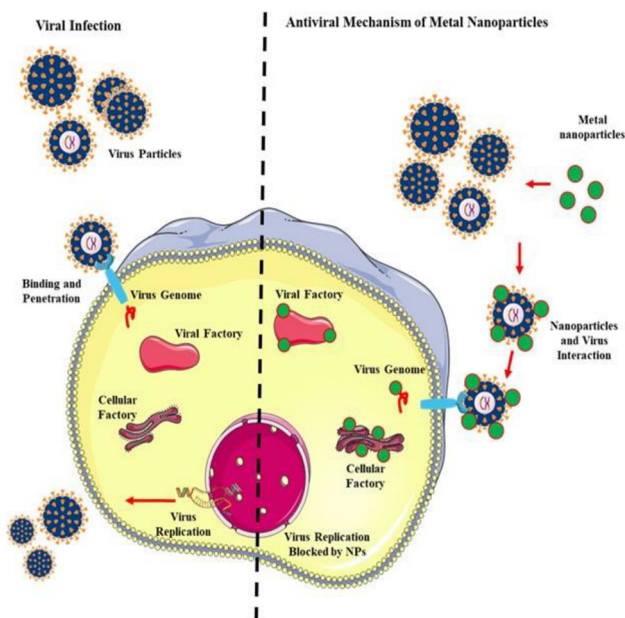


Fig. 4 Antiviral mechanism of nanoparticles (NPs). Reproduced with permission from Gurunathan *et al.*³² Copyright 2020, Multidisciplinary Digital Publishing Institute.



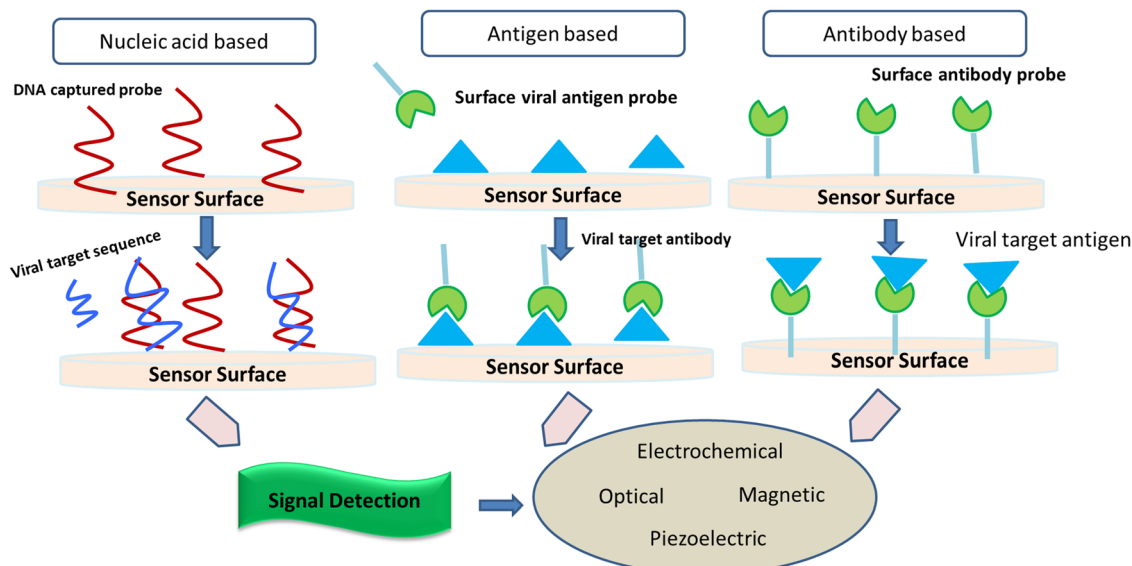


Fig. 5 Schematic illustration of various biosensors to detect SARS-CoV and MERS.

Nanobiosensors are a value-added substitute to regular diagnostic devices, which assess single molecules with great sensitivity, specificity, and precision characteristics for clinical and environmental analyses. Au-NP-based nano-carriers and a field-effect transistor (FET) sensor (altered *via* graphene sheets) that alters a given antibody for the SARS-CoV-2 spike protein were activated to identify SARS-CoV-2 in the culture mode. This sensor exhibited a comparable detection limit (LOD of 1.6×10^1 pfu mL⁻¹) to real pathological samples (LOD: 2.42×10^2 copies per mL).⁴³ Gold NP-studded DNA strands on the surface of electrodes were modified to identify in situ-amplified CTV (recombinase polymerase amplification (RPA) assay for amplification of the P20 gene) *via* electrochemical impedance spectroscopy (EIS) analysis. Here, the DNA sensor displayed a very low LOD of 1000 fg μL^{-1} .⁴⁴ Recently, paper/nanomaterial-customized detection techniques, especially, nanoparticle-based lateral-flow tools that may be seen by the bare eyes or administered using an android phone, are the latest known testing devices to filter COVID-19-related biomarkers.⁴⁵ Specialized research has also portrayed solid-phase isothermal recombinase polymerase amplification (RPA) routes for the detection of the *Citrus Tristeza* virus (CTV) in plant disease diagnostics.⁴⁶ This approach uses nanoparticle-engineered biosensors, which if modified appropriately for the detection of other viruses can be adopted, designed, and engineered for the diagnosis of COVID-19.

3. Nanotechnological approach to monitor SARS-CoV2

Different testing methods around the globe have aimed at focusing on parts of the coronavirus genetic profile. Clinical settings have utilized samples triggered by a patient's immune response such as DNA, RNA, antibodies, viral proteins, and

intact viral particles to recognize viruses. A host of established methodologies such as serological detection methods, western blot, virus culture, enzyme-linked immunosorbent assay (ELISA), and polymerase chain reaction (PCR) can be used to identify the analytes.⁴⁷ Generic methodologies are largely ineffective for fast real-time analysis due to complications related to the growth of cultured cells for cytopathological assay, problems associated with the transportation of expensive sophisticated tools at the point of interest, and the requirement of biocontainment and virus isolation. At the beginning of the pandemic, it was reported and globally circulated among health systems that some of the test kits provided results with less reliability and accuracy. Besides, another impending issue was the requirement of large amounts of testing reagents. Thus, this issue created a gap in the whole endeavour. In lieu of well-known diagnostic assays, viral biosensors can be used given that they offer scaled-down, fast, sensitive, cost-effective, and mobile foundations in contrast to standard laboratory methods. Among the various pathogens, viruses are the most important class to cause deadly airborne diseases. Influenza, a very commonplace and highly infectious virus, gets transmitted through small droplets as a result of sneezing, coughing, and talking.⁴⁸ Another fatally contagious viral infection, the avian influenza, has various subgroups, including H5N1, H5N2, H3N2, and H7N9. This virus mostly infects poultry and cattle, but it is possible for it to be transmitted to people and has incurred severe losses in federal economies globally.^{49–51}

SARS (severe acute respiratory syndrome) is a deadly virus-causing syndrome, which results in critical respiratory problems and even death. SARS belongs to the coronavirus family and was first recognized during a major outbreak in China in 2003. SARS was reported to be found in approximately 24 countries in 2003 with a case tally of 8000 and death tally of 774. The confirmatory test for the identification of respiratory virus disease is cell culture.⁵² In the late 1960s, distinguished



research groups carried out the first studies on coronavirus. Researchers independently differentiated a number of strains of a novel virus that expressed significant ether affinity properties. Electrochemical-based biosensors for the identification of influenza virus were one of the most remarkable ones according to the reports in the literature. 6 optical systems were ascertained to be the principal class of sensors for the detection of coronavirus, while a piezoelectric class of sensors was deemed for the identification of SARS-CoV-1. Besides, an electrochemical system was investigated for the detection of MERS and a different electrochemical detection for the identification of SARS-CoV-2. As an interesting alternative possessing greater sensitivity and rapidity compared to RT-qPCR and serological tests, Huang⁵¹ came up with a fibre-optic biosensor that could detect the SARS-CoV antigen, *i.e.*, the nucleocapsid (N) protein. Roh^{53,54} attained the same detection limit (0.1 pg mL^{-1}) using immobilized quantum dots conjugated with RNA aptamer on a chip to identify the N protein from SARS-CoV. Also, the extent of detection stated above was the lowest with the aid of biosensor devices. Park,⁵³ aiming to immobilize biomolecules, fabricated a surface plasmon-resonance (SPR) platform for the identification of SARS-CoV using the help of gold binding polypeptide (GBP). Park fused GBP with the SARS-CoV membrane envelope (SCVme), which possessed the capability to bond with anti-SCVme antibodies and a modified green fluorescent protein (GBP-E). Thus, this system developed by Park is an interesting system, where the specificity to the gold substrate is high, while keeping the biomolecular activity intact. As a radical effort for an optical sensor, Teengam⁵⁴ introduced a biosensor for the detection of MERS. The idea for the biosensor was to immobilize pyrrolidinyl peptide nucleic acid (PNA) on a paper-based analytical device (PAD) to recognize synthetic oligonucleotides having a sequence similar to MERS. The mechanism driving the results is the aggregation/de-aggregation of (–) silver nanoparticles with the introduction of (+) DNA followed by the subsequent addition of complementary DNA. The analysis of the results does not need to be done on the typical computing device given that they can be perceived by the naked eye.⁵⁵ Furthermore, a number of nanoscale devices has been evaluated. Immunocapture approaches amalgamated with antibody-coated chips have been utilized to image viruses⁵⁶ with the aid of atomic force microscopy (AFM). The limit of detection for coxsackievirus was 106–107 TCID₅₀ per mL (50% tissue culture infective dose). Within a very short time biosensors fabricated from nanowire/carbon nanotubes have transformed from theoretical concepts to practical devices capable of detecting DNA sequences and particular proteins with precision.

This concept of photo-induced nanomaterial possessing CNH for the specific eradication of viruses has been reported. In the mentioned discussion, the T7 bacteriophage was deemed to be the target virus recognizable by a T7 tag antibody. This virus bears a symmetrical structure with an approximate length of 100 nm and width of 55 nm together with long double-strand DNA (dsDNA; about 40 kbp) stationed on the head. This nanoparticle is constituted of a moiety of poly(ethylene glycol) (PEG) and functionalized CNH (CNH-COOH) with T7 tag Ab as

the identification site and phospholipid group linked at both ends to enhance its solubility. Briefly, researchers have successfully procured the T7 tag Ab-CN complex upon NIR laser irradiation T7 phage, which is a model virus successfully eliminated from the complex. Thus, these studies strongly suggest the production of CNH nanomaterials in the near future that exhibit potential for the photo-exothermic eradication of harmful viruses such as SARS, HIV, and avian influenza virus. It was unanimously by researchers that this research made a substantial contribution to antiviral biomedical applications. Ishikawa and co-workers (2009) were pioneers in developing an electrochemical biosensor for the identification of SARS-CoV.⁵⁷ They developed an FET-based immunosensor, which generated a measurable conductance variation as a result of antigen-antibody binding, producing the analyte amount. The virus antigen nucleocapsid N protein was used as a CoV biomarker.⁵⁸ Antibody mimic proteins, a viable alternative to conventional antibodies, have been already used as affinity binding agents.^{57,59} The first amperometric immunosensor for the detection of the MERS-CoV virus was reported by Layqah and Eissa in 2019.⁶⁰ In their endeavour, spike protein S1 was used as a MERS biomarker. The optimum conditions for this experiment were determined to be 10 g mL^{-1} for the concentration of antibody and 20 min for binding time, respectively. Square wave voltammetry (SWV) was used to measure the peak current of the ferro/ferri-cyanide redox probe, and as a result the current signal was obtained.⁵⁹

In the present scenario, there are two major papers focusing on affinity-based biosensors for the detection of COVID-19. A novel FET-based biosensor for the detection of SARS-CoV-2 was proposed by Seo and co-workers.⁶¹ The synthesized device could identify the SARS-CoV-2 antigen spike protein with small concentrations as low as 1 fg mL^{-1} in phosphate buffer. This device also exhibited no substantial degree of cross-reactivity with the MERS-CoV antigen.⁶¹ Qiu and co-workers suggested a dual biosensor by amalgamating LSPR sensing transduction and plasmonic photothermal (PPT) effect on a single chip. The philosophy guiding the sensor chip modification is the utilization of two-dimensional gold nanoislands (AuNIs), which are subsequently activated with complementary DNA (cDNA) receptors with the aid of Au-S bond formation between the thiol groups of cDNA and the AuNIs. This bifunctional biosensor traced a uniform linear range between 0.1 pM and 1 mM with a detection limit of 0.22 pM.⁶²

Recently, PathSensors Inc. reported the development of a “Canary” fast biosensor for the detection of the novel CoV-19. This biosensor uses a cell-based immunosensor, which captures the virus using signal amplification and gives a response in as little as 3–5 min. The primary application and use of the PathSensors device will be for testing environmental samples and keeping track of air in spaces prone to exposure, including hospitals, offices, and food services.⁶³ Graphene and graphene-based materials (GRMs) have been shown to exhibit extraordinary physicochemical, electrical, optical, antiviral, antimicrobial, and many more interesting characteristics, which qualify them as possible contenders for the design and progress of



strong-performing components and vehicles that will be needed for the COVID-19 virus and other futuristic disease outbreaks.⁶⁴ The requirement for rapid home testing kits that are user-friendly is urgent. The cardinal philosophy of POC is for the process to be comfortable and fast. It is desirable for a patient to get immediate medical reports after getting tested, enabling quick treatment from the luxury of their home, which alleviates the pain of traveling to access treatment.

3.1. Nanoparticle inhibition of viral infection

It is well-known that there are 2 classes of antiviral analytes, *i.e.*, virostatic and virucidal, based on their counteracting synergism against a particular virus, impeding viral replication and proliferation.⁶⁵ Nevertheless, many effective antiviral agents show toxic responses. Thus, to address this issue, research on the antiviral characteristics of nanomaterials has begun. The major question in these systems indeed involves their low toxicity and pure virus curbing routes (Fig. 6). Nanoscale composites are made by merging virostatic and virucidal inactivation processes.⁶⁶ In nanoscience, several nanomaterials have been explored, wherein non-pharmaceuticals denote a broad spectrum of nanomaterials having therapeutic efficacy, for example, dendrimers, liposomes, micelles, and nanocapsules.⁶⁷ Metal oxide nanoparticles (MONPs) possess an interesting inhibitory mechanism *via* the production of reactive oxygen species (ROS) and restricting the S spike protein of the viral reaction with cellular ACE2 receptor.

Metal nanoparticles have displayed potency as successful antiviral agents by thwarting viral particle entry in the exterior and restraining viral replication in the interior.⁶⁸ The efficiency and antiviral action of metal NPs depend on their physical structure and attached metal ions. It should be noted that capped metal NPs have a notably greater reaction with viruses and host cells compared to bare NPs.⁶⁹ Gold nanoparticles (AuNPs) have also sparked huge interest in the field and nanomedicine as a result of their outstanding electrical, optical, mechanical and biological properties. AuNPs possess outstanding mechanical, biological, electrical, and optical properties, which have attracted significant interest from the

industrial sector and nanomedicine.^{70,71} Gold NPs have attracted broad attention and provide efficient antiviral activity against viruses. Sialic acid-functionalized AuNPs exhibit activity against infections from influenza virus and are superior compared to conventional synthetic drugs such as zanamivir and oseltamivir.⁷²

AuNPs successfully enhance antiviral effects *via* polyvalent interactions with dendronized AuNPs, thus preventing HIV with more efficacy than solo dendrons. Functionalized AuNPs counteract the action of HIV, HSV, and influenza viruses.^{73,74} Di Gianvincenzo *et al.*⁷⁵ reported that an amphiphilic sulphate-ended ligand coated on gold nanoparticles binds with glycoprotein gp120 on the HIV envelope to restrain the extent of HIV infection *in vivo*.

Mehranfar and Izadyar reported the properties of AuNPs attached with various moieties, such as 3-mercapto-ethyl sulfonate (MES), undecane sulfonic acid (Mus), octane thiol (OT), and a novel peptide, to hinder the CoV-19 virus using molecular dynamics simulations. Viewing the solid structure of angiotensin-converting enzyme 2 (ACE2), which can attach to the SARS-CoV-2 receptor-binding domain (RBD), about fifteen amino acids of ACE2 have substantial interplay with RBD. Hence, a novel peptide, using the above-mentioned amino acids has been considered and prepared as the functional moiety for AuNP. According to the results, the functionalized AuNPs show highly significant outcomes on the RBD and react quite strongly with this protein in SARS-CoV-2. Considering the above-mentioned nanoparticles, AuNPs were functionalized with a novel peptide coordinated with RBD, which has greater stability compared to ACE2 (human receptor for SARS-CoV-2). Various studies demonstrated strongly that these synthesized AuNPs can be fine contenders for antiviral agents against the COVID-19 virus.⁷⁶

It has been determined that therapeutically inactive organic molecules when conjugated to gold nanoparticles can become strongly active drugs.⁷⁴ AuNPs conjugated to peptide triazoles (AuNP-PT) showed a strong level of antiviral efficacy on HIV-1 compared to the parallel peptide triazoles. The stronger

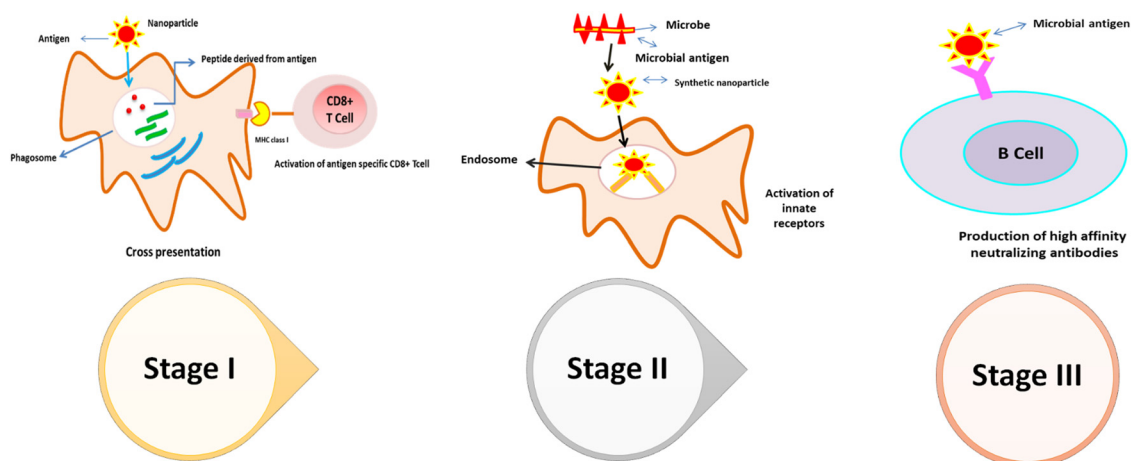


Fig. 6 Nanoparticle-mediated immune response infection.



virologic activity and parallel irreversible HIV-1 deactivation *via* AuNP-PT are because of the multi-valent interaction between the nanoparticles and metastable envelope spike (S) proteins on the HIV-1 virus.⁷⁷ Accordingly, the AuNPs enhanced the immune reaction by lowering the mRNA expression of interleukin (IL)-1 IL-6, the tumour necrosis factor (TNF)- α , IFN- γ , and the inducible nitric oxide synthase, which may be a notable alternative, mainly in antiviral therapeutics.⁷⁸ Furthermore, gold nanoclusters (AuNCs) restricted and blocked the viral entry site of the respiratory syndrome virus. Precisely, histidine-functionalized AuNCs were active in mitigating the proliferation of the pseudorabies virus (PRV).⁷⁹ Huang *et al.* produced a new gold nanorod-based HR1 peptide inhibitor (PIH-AuNRs) for MERS. This is a powerful HR1 inhibitor and functions on a selective basis for MERS-Cov S protein-mediated cell fusion with an IC₅₀ of 1.171 μ M. Specifically, PIH-AuNRs show a 10-fold higher inhibitory action than PIH and may present total cell fusion at 1.171 μ M. Also, PIH-AuNRs demonstrated noteworthy biostability and biocompatibility *in vitro* and *in vivo*, thereby suggesting their wide utilization possibilities for the cure of MERS. Hence, PIH-AuNRs are favourable antiviral devices and may soon have a major effect on the progress of therapeutics for clinical use.⁸⁰ Au@Ag nanorods (Au@AgNRs), which were made by coating AuNRs with silver, were seen to exhibit efficacy upon the multiplication of porcine epidemic diarrhea virus (PEDV).⁸¹ Viral titration analysis showed that Au@AgNRs could prevent PEDV occurrence by a magnitude of 4 orders after 12 h of infection, as confirmed *via* viral protein expression analysis. This portrayed that Au@AgNRs could suppress the entrance of PEDV and reduce mitochondrial membrane potential as well as caspase-3 activity. In addition, researchers portrayed that a huge rate of virus multiplication may result in the production of reactive oxygen species in cells. The released Ag⁺ and bare AuNRs by Au@AgNRs after the initiation by ROS have a remarkable antiviral action, which helps in providing large-scale suppression of the PEDV replication process. The results provided evidence that Au@AgNRs may be of use as a promising theranostic route to curb the multiplication of CoVs.

Focus should be placed on the stability of NPs, effective drug release in cells, decreased toxicity of medications after delivery, and targeting to certain tissues to make nanoparticle-based antiviral drug delivery successful. The entrapment of the mononuclear phagocytic system, which is found in tissues such as the liver and spleen, is another obstacle in the successful use of nanoparticles for medication delivery.⁸² It may be possible to overcome this obstacle by using biodegradable polymers such as PEG (polyethylene glycol) and PVP (polyvinylpyrrolidone). A change in the PEG modification distribution and a decrease in its *in vitro* toxicity can be achieved with the aid of gold nanorods. Besides, natural polymers such as dextran, chitosan, and pullulan, and surfactants such as sodium oleate and dodecylamine may aid in effective drug delivery.⁸³ Drug distribution to particular targets is a significant difficulty because failing to do so can result in hazardous side effects in other tissues and cells. Accordingly, the use of virosome-based medicine delivery may aid in resolving this problem. Without a nucleocapsid and

genetic materials, virosomes resemble enveloped viruses. Extracted glycoproteins have unique receptor binding and fusion capabilities, which enable them to bind to a cell surface receptor and deliver medicines to certain tissues and cells. Virosomes have recently been used to generate effective nanovaccines.⁸⁴

Current study discoveries are being applied to investigate improved engineering moieties to control virus replications to build broad-spectrum antiviral medicines against different viral mutations. The design will focus mostly on the downsizing of characteristics relevant to various viral presentations.

Although researchers have explored diverse nanoparticles for several viral inhibitions and COVID-19, we believe there is a large scope in this niche for the utilization of noncytotoxic, biocompatible, nanoparticles, which are effective in inhibiting diverse COVID-19 strains.

3.1.1. Silver nanoparticles. In addition, the interesting physicochemical and biological attributes of silver nanoparticles (AgNPs) are being utilized in antiviral, antibacterial, anti-inflammatory, anti-angiogenesis, antiplatelet, antifungal, and anticancer applications. The concoction of AgNPs is brought about by several physical, chemical, and biological methods. The biological methodology employed is apparently ecologically friendly, biocompatible, and safe in nature.⁸⁵ AgNPs are utilized as biomedical restorative agents for injury dressings, severe burn healing products, and anti-bacterial creams.⁸⁵ The synthesis of AgNPs by fungi-mediation significantly lowered the viral action for HSV-1/2 and HPV-3.⁸⁶ AgNPs could prevent contagious gastroenteritis virus-induced cell death by modifying the p38/mitochondria-caspase-3 signalling pathway in pig scrotum cells.⁸⁷ AgNPs have shown antiviral and defensive action towards the H3N2 influenza virus.⁸⁸ An Ag-nanocluster silica sputter-coated composite was used in an FFP3 face mask, which lowered the SARS-CoV-2 analyte to 0.⁸⁹ Huy *et al.* observed the antiviral action of AgNPs to influenza A, HBV, human parainfluenza, HSV, and HIV.⁹⁰ The antiviral action of AgNPs and chitosan composites also was investigated against the H1N1 influenza A virus. These complexes exhibited potential antiviral action in a structure-based route, but chitosan by itself did not. Alternatively, AgNPs alone exhibited antiviral action; however, the complexes exhibited outstanding antiviral action in comparison to AgNPs or chitosan by themselves.⁹¹ Biosynthesized silver NPs portrayed anti-dengue activity with the use of algae (*Centroceras clavulatum*), plant (*Bruguiera cylindrica*), and seed (*Moringa oleifera*) extract having concentrations of 12.5–50, 20, and 30 μ g mL⁻¹.⁹² Silver NPs aided in inhibiting the herpes virus from gaining entry inside the host cell.⁹³ Silver NPs (12–28 nm) containing leaf extracts of *Rhizophora lamarckii* also curbed HIV-1.⁹⁴ Silver nanoparticles (50 nm) have been shown to have 92% antiviral activity against hepatitis B.⁹⁵ Bio-synthesized AgNPs from plant extracts of *Lampranthus coccineus* and *Malephora lutea* demonstrated notable antiviral action on differing types of viruses including HSV-1, HAV-10, and CoxB4 virus.⁹⁶

Given that AgNPs are effective against diverse viral infections including COVID-19 according to the currently available literature, researchers can explore AgNPs in their pristine form,



composites, and hybrid form for the inhibition of diverse COVID-19 strains and other viruses.

3.1.2. Other metal nanoparticles. Selenium NPs bind to oseltamivir and inhibited the enterovirus action release of ROS in human astrocytoma tissues.⁹⁷ Cheng *et al.* discovered that SeNPs curbed the multiplication and cloning of the hepatitis B virus.⁹⁸ Subsequently, SeNPs were shown to be an effective treatment for the H1N1 influenza virus.⁹⁹ Alternatively, zinc nanoparticles curb the viral DNA polymerase activity of the herpes simplex virus.¹⁰⁰ Zinc oxide at a low concentration of 2.5 pg mL^{-1} acted as an antichikungunya agent by lowering the concentration of virus RNA transcripts within an infection period of 24 h *via* RT-PCR.¹⁰¹ Copper NPs yielded reactive oxygen species to deactivate the herpes simplex virus by oxidizing the viral proteins or breaking down the viral genome.¹⁰² CuNPs restricted the entry and inhibited the attachment stages of hepatitis infection.¹⁰³ Copper oxide NPs containing leaf extracts of *Tridax procumbens* portrayed larvicidal action on the chikungunya vector at a dosage of 4.209 mg L^{-1} .¹⁰⁴ Recently, the potential of copper was illustrated on the HuCoV-229E coronavirus, inhibiting several forms of CoVs, which suggests promising its effects against SARS-CoV-2.¹⁰⁵ Gallium NPs (bound with glucan) curbed HIV and subdued the infection of HIV and tuberculosis jointly.¹⁰⁶ Iron oxide NPs inhibited H1N1 influenza (50%) at a concentration of 1.1 pg .¹⁰⁷ Cui *et al.* found that titanium dioxide nanoparticles in the anatase phase inhibited the H9N2 avian influenza virus. Remarkably, UV-activated nanoparticles portrayed higher inhibitory action than that not exposed to UV light.¹⁰⁸ Tungsten carbide nanoparticles curbed norovirus causing a 4-log depreciation of murine norovirus within 15 min¹⁰⁹ and assisted in a decrease in poliovirus infection (3.5 log) within 15 min.¹¹⁰

4. Biosurfactants

Biosurfactants have a remarkable trait in which they can form micelles above their critical micelle concentration (CMC). This

justifies vigorous study looking at their embryonic applications in the prevention of viral spreading. The amphiphilic structure of biosurfactants suggests that their water-fearing layer can react with the lipid layer of the virus, while concomitantly reacting with hydrophobic substances such as H_2O . This unique amphiphilic nature is the cornerstone of the biosurfactant structure, which is very beneficial to disrupt the structure of viruses (Fig. 7).¹¹¹

Biosurfactants possess certain interesting physicochemical properties by which they can maintain their integrity while being delivered as an aerosol. This mode of delivery endows biosurfactants with a drug carrier-like feature considering the lungs as the main area of action. The solubility aspect of biosurfactants in aerosols offers the advantage of enhanced bioavailability post-delivery. Besides, biosurfactants are self-soluble, which augments the proportionality of the drug dosage at the site of action, thus producing better results.¹¹² Biosurfactant-mediated drug delivery offer benefits that are 2-fold in nature. This method of delivery not only provides a safe route for the drug to reach the target but also offers natural antiviral properties at the infection site. Biosurfactants also produce surfactant dysfunction at the alveoli, which is a probable scenario because of the ill effects of COVID-19 infection. Thus, biosurfactants offer healing by killing a host of viruses in the vicinity of a particular site, and consequently provides relief to patients. This aspect has attracted attention from the scientific community who are interested in the further investigation of biosurfactants as a probable treatment mechanism.

4.1. Liposomes

Liposomes are very attractive small spherical vesicles [15–1000 nm size] that originate from the presence of an aqueous core in phospholipids. Liposomes can entrap and produce both water-loving and water-fearing drugs. The liposomal lipid layer can shield the drug from degradation in the gastrointestinal

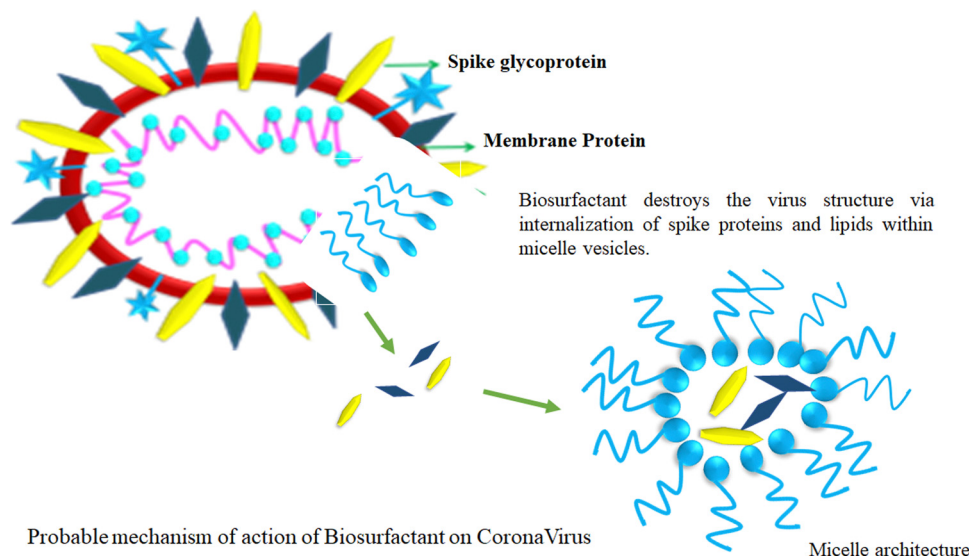


Fig. 7 Probable mechanism of action of biosurfactant on corona virus.



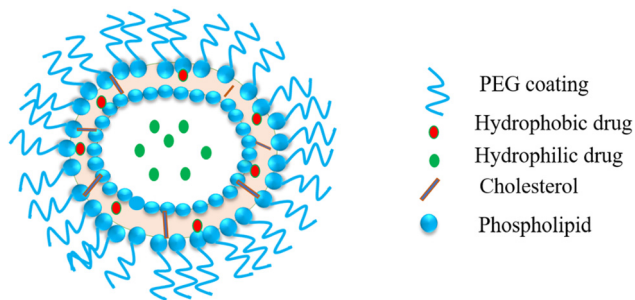


Fig. 8 Liposome: a spherical vesicle with an aqueous core formed by a phospholipid and cholesterol bilayer.

tract and assist in its slow and sustained release.¹¹³ Herein, we describe the embryonic use of liposomes as vehicles for the specific delivery of antiviral agents. These may also act as immunomodulators to monocytes and macrophages for prophylaxis and treating viral disease.¹¹⁴ Simico *et al.* investigated the antiherpetic activity effect *in vitro* upon the liposomal inclusion of *Artemisia arborescens* L. essential oil. They prepared multilamellar (MLV) and unilamellar (SUV) (+) liposomes to check the effect of vesicle anatomy and constitution of liposomes on the antiviral action of the vesicle-incorporated oil. They obtained liposomes from hydrogenated (P90H) and dehydrogenated (P90) soy phosphatidylcholine. The antiviral action was investigated for herpes simplex virus type 1 (HSV-1) *via* a quantitative tetrazolium-based colorimetric method. The observations exhibited that *Artemisia* essential oil may be included in a significant quantity in the prepared vesicular dispersions. Antiviral screening indicated that the liposomal assimilation of the essential oil increased the *in vitro* antiherpetic action, chiefly for P90H vesicles (Fig. 8).¹¹⁵

Nanocarbon fullerene liposomes exhibited activity against the H1N1 influenza virus *in vitro*.¹¹⁶ Acyclovir-loaded flexible membrane vesicles revealed remarkable antiviral properties in a murine model for HSV-1 infection.¹¹⁷ Stearylamine (SA)-loaded cationic liposomes impeded viral infectivity in the absence of preloaded active pharmaceutical components. The antiviral action of SA liposomes against herpes simplex virus type 1 in A549 cells demonstrated similar activity to the antiviral drug acyclovir.¹¹⁸

5. Carbon-based nanoparticles

Carbon dots (C-dots) obtained from benzoxazine monomer curbed the infectivity of the flavivirus.¹¹⁹ C-dots bond with an amine, curbing HSV-1 from entering the host cells.¹²⁰ Carbon quantum dots (CQDs) synthesized *via* the hydrothermal carbonization of citric acid restricted the entrance and multiplication of HCoV-229E.¹²¹ Graphene oxide and GQDs curbed the replication of HIV.¹²² GO-loaded hypericin worked well against the novel duck reovirus (NDRV).^{120,123} GO with curcumin restricted the respiratory syncytial virus posing as antiviral agents against hand, foot, and mouth disease.¹²⁴

Recent works in the literature have established the efficacy of carbon-based nanoparticles as well as quantum dots such as

graphene nanoparticles,¹²⁵ graphene quantum dots,¹²⁶ and carbon dots¹²⁷ for the inhibition of COVID-19. Even though progress has been made in this case, we believe that these findings are still in their infancy and there is more to be explored with these NPs in their pristine, chemically modified, composite, and hybrid forms.

5.1. Carbon nanotubes

Among the numerous nanomaterials, carbon nanotubes (CNTs) have achieved a paramount level of importance in antiviral therapy.¹²⁸ CNTs are superior to other nanomaterials given that they can traverse cellular walls, transport drugs and molecules, including small interfering RNA, DNA, and proteins within different types of cells, such as T and cancer cells.¹²⁹ Furthermore, CNTs possess multi-modular conjugation, which permits the inclusion of several functional groups on their exterior. This property gives rise to the supremacy of nanodrugs over the other streamlined agents.¹³⁰ CNTs have demonstrated their effectiveness as HIV inhibitors through their structure-based design.¹³¹

It has been reported that reactive oxygen species (ROS) generating compounds such as peroxides are deleterious to various viruses such as coronaviruses. For the fabrication of viral inactivation surfaces, metal-attached single-wall carbon nanotubes (SWCNTs) are very effective for the adsorption of H₂O₂. Aasi *et al.*¹³² investigated the capture of H₂O₂ molecules on metal-decorated SWCNTs using density functional theory (DFT). They observed that the metal-functionalized SWCNTs exhibited better adsorption capability than pristine SWCNTs. Finally, it was concluded that Ru-SWCNT and Rh-SWCNT composites illustrated excellent H₂O₂ adsorption. Moreover, they also revealed that Pt- and Cu-attached SWCNT-H₂O₂ composites have major potency as sieves for the eradication of viruses and their deactivation, and also have a large shelf-life (2.2×10^{12} and 1.9×10^8 years, respectively). This high adsorption of metal-attached SWCNTs and longevity of these nanoparticles imply that they are good contenders for synthesizing PPE kits against viruses.

5.2. Fullerenes

Fullerenes are carbon cage moieties consisting of a fused ring system of pentagons and hexagons. They are superb electron acceptors in the ground state and can reversibly accept up to six electrons.¹³³ Fullerene nanoparticles have attracted substantial consideration by virtue of their distinctive physical and chemical characteristics. The possible reduction of viral activity using fullerenes has been postulated in various studies. Badir-eddy and team portrayed that under UV light, fullerol yielded singlet oxygen and superoxide. These two ROS deactivated the MS2 bacteriophage.¹³⁴ Hotze and team shed light on the toxicity route of fullerol upon exposure to viruses. Fullerol conglomerates connect with the viruses and allow the effective passage of 1 oxygen molecule to the capsids, which results in notable oxidative changes to the capsid proteins and small changes to DNA and phospholipids. These changes reduce the ability of the bacteriophage to attach to the receptors on the



body of their bacterial hosts.¹³⁵ The inactivation of the bacteriophage may result from the reduction in the structural integrity of its capsid (deformation or rupture of capsid locally) and reduction in the ejection ability of genomic RNA in the bacterium.¹³⁶ Fullerenes exhibit very low water solubility, which is the main drawback of their biological application. Hence, efforts should focus on making fullerenes water-soluble.¹³⁷ Kraevaya *et al.* reported the preparation of various water-soluble fullerenes having promising anti-HIV activity.¹³⁸ Du *et al.* synthesized a fullerene-liposome complex to investigate its antiviral activity against the influenza virus and performed an *in vivo* mouse model investigation.¹³⁹ Their conclusions indicated that this complex is a very effective antiviral agent against the influenza virus *in vitro* and *in vivo*. They also studied the antiviral activities of fullerene against a few enveloped viruses such as HIV, human cytomegalovirus, SFV, and VZV. Based on their observations, they concluded that the fullerene-liposome may potentially play a crucial role in inhibiting influenza virus infection through a wide array of antiviral activities with low toxicity in the nanomaterial field.¹³⁹

Shoji *et al.* investigated 12 fullerene derivatives to detect new efficient anti-influenza compounds using an *in vitro* PA endonuclease inhibition assay. Eight derivatives of fullerene were recognized to inhibit the endonuclease activity of the PA N-terminal domain or full-length PA protein *in vitro*. Silico docking simulation analysis of C₆₀ fullerene and PA endonuclease was performed, implying that fullerenes can be the active cavity of PA endonuclease.¹⁴⁰ Kraevaya *et al.* reported the design of a water-soluble C₆₀ fullerene derivative attached with 5 residues of phosphonic acid to investigate its antiviral activity.¹⁴¹ Muñoz synthesized a chain of amphiphilic glycodendro¹⁴² fullerene monoadduct to investigate the antiviral efficiency of Ebola virus glycoprotein (Ebo GP) pseudo-typed viral particles on Jurkat cells overexpressing DC-SIGN. They discerned an enhancement in the IC₅₀ value compared to various systems furnished with more carbohydrate groups.¹⁴³

5.3. Graphene

It has been well established in various reports that bacteria coming in contact with a graphene surface [a two-dimensional material] lose their integrity. However, although graphene-based virus-related research has focused on making suitable sensors, the effects of graphene on viruses have not been well-established. Stanford *et al.* reported a self-cleaning filter by counting laser-induced graphene (LIG), which was capable of capturing bacteria and particulates to reduce the transmission of nosocomial infections. The rapid growth of bacteria was stopped on the filter and by raising the temperature of the filter to above 300 °C, all the pathogens including bacteria, along with molecules were destroyed.¹⁴⁴

Gedanken *et al.* synthesized reduced graphene oxide (SMRGO) functionalized with sulfonated magnetic nanoparticles (MNPs) to entrap and demolish type 1 herpes simplex virus (HSV-1) photothermally.¹⁴⁵ They observed that SMRGO portrayed great (~99.99%) photothermal antiviral action by radiating the compound with near-IR light (NIR, 808 nm, 7 min). The distinctive planar structure, capturing efficiency, large surface area, and outstanding photothermal attributes of

graphene are responsible for this antiviral activity. In addition, the electrostatic interaction of MNPs with viral agents played a crucial play in significantly reducing infection. GO films enable the easy fabrication of breathable barrier layers in fabrics. Steinberg *et al.* reported GO membranes for preventive appliances designed to restrict the entry of chemical toxicants or biochemical agents from the environment except for outward perspiration.¹⁴⁶ Protective facemasks made of graphene could be recycled by the application of heat or photocatalysis method.¹⁴⁷ In addition, graphene-coated textiles and sieves that touch viruses can be sterilized by heat and electronic transduction. Furthermore, the denaturation process of viruses after adsorption on the surface of graphene and low thermal treatment at 56 °C for 30 min was demonstrated. Yang *et al.* designed a β -cyclodextrin (CD)-decorated graphene oxide (GO) composite, which demonstrated a very good level of antiviral action and could also load curcumin effectively. These researchers employed RSV, a negative-sense single-stranded enveloped RNA virus, as the control to investigate the antiviral properties of multifunctional GO. The results revealed that the composite, which possessed inhibitory and pathological effects on the virus, could avert RSV infection to the host cells by deactivating the virus and preventing viral attachment.¹²⁴

6. Polymer drug conjugates

A covalently bound therapeutic agent and a polymer constitute a polymer-drug conjugate, where the therapeutic agent can either be a large molecule such as a protein or a small molecule.¹⁴⁸ The philosophy behind conjugation is to attain greater efficiency *via* enlarged plasma stabilization and also safety *via* targeted delivery.¹⁴⁹

Many polymers have inbuilt antiviral potential and their complexation to antiviral drugs may work synergistically. Conjugation of interferon α 2A and α 2A with polyethylene glycol (PEG) worked on HCV.¹⁵⁰ Polymers having sialic acid attachment were synthesized and known to be outstanding inhibitors of viral entry *via* multivalent attachment to hyaluronic acid (HA) and NA on the wall of viruses.¹⁵¹ In 2018, Andersen *et al.* synthesized albumin-polymer-drug composites to guarantee an increased residential time and lymphatic accumulation, providing a suitable ratio of bare drugs of ART to primary human T cells, which portrayed high shielding from HIV infection compared to individual ART drugs. *N*-(2-Hydroxypropyl) methacrylamide (PHPMA) was the used polymer.¹⁵²

When added to the right drug delivery platforms, cell-penetrating peptides (CPPs) such as TAT-peptide have been reported to show promise as immune boosters.¹⁵³ In comparison to other translocation and delivery methods, CPPs have a lot of benefits, including being simple to create, affordable, and often having little cell toxicity with no immune reaction. To combat COVID-19, it is deemed important to develop drugs against SARS-CoV-2. Available works in literature have shown beyond doubt that polymeric-drug conjugate systems are an effective approach for combating COVID-19.¹⁵³ However, although these findings are interesting, there is a lot to be



investigated within this niche given that it is in its budding phase or development stage. Researchers can wisely adopt diverse CPPs and other polymeric macromolecules in this case towards containing COVID-19.

7. Quantum dots

“Quantum dots (QDs)” or “semiconductor nanomaterials” attached to major fluorescent probes are important for the identification and persistent fluorescence imaging of many cellular activities.¹⁵⁴ The major tactic related to suppressing SARS-CoV-2 infections with QDs may interest researchers substantially. The major reason for using QDs is because of their detectability at a specific wavelength of light. Also, QDs may be modified to the required size (1–10 nm) and shape to attack SARS-CoV-2 within a range of 60 and 140 nm in size. Now, the positive charge on the surface of carbon-based QDs is employed to curb the S protein of SARS-CoV-2.¹⁵⁵ In addition, the positive surface charges of QDs interplay with the (–) RNA chain of the virus, producing ROS in SARS-CoV-2.¹⁵⁶ Carbon dots (CDs) initiate interferon-activated genes, mainly interferon- α production, which are known to curb viral multiplication. Subsequently, the attachment of required moieties with QDs may interplay with entry receptors of CoV-2 and inhibit genomic multiplication.¹⁵⁷ The antiviral efficacy of CDs obtained from 4-aminophenyl boronic acid hydrochloride (4-AB/C-dots) portrayed inhibitory action against herpes simplex virus type 1, especially flaring in the initial stage of viral action.¹⁵⁸ To inspect the antiviral ability of less toxic QDs, Du *et al.* explored the viral inhibition effects of CDs minutely.¹⁵⁹ The virucidal ability of CDs was seen to be close to their carbon predecessor and formation methods, indicating the requirement of systematic probes of the antiviral action of various carbon dots. This team created a simple but low-cost route to produce stable CDs with antiviral attributes and explored their consequence on viral multiplication *via* PRV and PRRSV as model structures of DNA and RNA viruses, respectively. The obtained results indicated that CDs can remarkably suppress the replication of both PRV and PRRSV. Therapy using CDs could also drastically initiate the production of endogenous interferon and expression of interferon-stimulating genes (ISGs), which curb virus multiplication.¹⁵⁹ Recently, Loczechin *et al.* reported that various CDs made *via* hydrothermal carbonization and complexation with boronic acid (carbon quantum dots-3) show antiviral effects towards the extremely deadly COVID-19 virus in a dosage-dependent way.¹²¹ Also, CDs upscaled the expression of several ISGs, which are essential in the CD-based antiviral pathway.¹⁶⁰ In addition, Huang *et al.* developed benzoxazine monomer-obtained carbon dots (BZM-CDs), which exhibited virus-curling ability towards flaviviruses and other non-walled viruses, such as porcine parvovirus and adenovirus-associated virus.¹¹⁹ Earlier studies showed that the antiviral efficacy of functionalized CDs can be enhanced *via* suitable surface synthetic changes. For example, Szunerits *et al.* reported that carbon dots surface-modified with boronic acid or amine

groups can fight herpes simplex virus type 1 (HSV-1) by curbing its entry into host cells.¹²⁰ However, the *in vivo* toxicity of QDs is a noteworthy drawback of this antiviral agent.

Considering the above discussion, the modification of QDs and other experimental pathways using new functional groups against SARS-CoV-2 will give rise to nanotherapeutics for COVID-19 for the obliteration of this pandemic in the near future.¹⁶¹

8. Polymeric nanoformulations

Natural hydrophilic and synthetic hydrophobic polymers are mostly employed for the synthesis of nanoformulations. The use of surface-modified polymers helps to decrease the unspecific reaction with serum proteins and facilitates phagocytosis to manifest commendable changes in the pharmacokinetic profile of drugs. The design of polymer nanocarriers also plays a major part in deciding the manner of drug release with the aid of various sources of stimuli such as chemical, pH variation, magnetic field, outside heat source, and impingement of light. Thus, these methods have improved the bioavailability of drugs by reducing the effects of toxicity at non-specific sites and drug degradation prior to reaching the site of interest.¹⁶² Certain essential criteria that need to be considered prior to polymer selection are: (i) nanoparticle size; (ii) drug release profile from the polymer; (iii) physicochemical properties of the drug of interest; (iv) aspects of biodegradation ability, safety, and biocompatibility; (v) drug effectiveness and antigenicity; and (vi) surface morphology and functionalities.¹⁶³ The various types of polymer-based nanoformulations include nanocapsules, nanospheres, polymeric micelles, and solid polymeric nanoparticles.

8.1. Micelles

Micelles have a size in the range of 10 to 100 nm. They are composed of an inner hydrophobic core (holds water-insoluble drugs) that is enveloped in a hydrophilic polymer with an outer layer (such as PEG, which increases their circulation time, and subsequently improves their aggregation). A common example is polymeric micelles, which are well-known drug delivery agents, providing remarkable therapeutic efficacy. The encapsulation of drugs in polymeric micelles is important nanotechnology employed to develop water-soluble and stable drugs. Another reason to use micelles in drug formations is that they dissociate slowly, hence making way for higher drug retention, and also increased aggregation of the drug at the desired location.

8.1.1. Polymeric micelles. After surpassing the critical micellar concentration (CMC), the monomers assemble to form supramolecular nanoscale moieties known as micelles with a characteristic hydrophilic shell and hydrophobic core.^{164,165} Modifying the micellar surface *via* complexation with particular ligands or monoclonal antibodies shows advantageous aspects of targeted specific drug delivery with the aid of polymeric micelles.¹⁶⁶ Polymeric micelles proved to be advantageous by increasing the drug loading abilities and reducing loading steps. Studies suggested that a multifunctional block



copolymer of poly(L-lactic acid)-*b*-poly(ethylene glycol) (PLLA-*b*-PEG) decorated with sialic acid derivative (methyl-*b*-neuraminic acid, mNA) can be employed to formulate micelles. Amantadine drug was coordinated to these micelles and sialic acid possessed the capability to bond with hemagglutinin viruses to prevent infection and hemagglutination mediated by the virus.¹⁶⁷

9. Implication of nanotechnology to mitigate the cytokine storm

Cytokines are a class of signalling molecules that moderate and control the human immunological system. Viruses such as COVID-19 trigger a cytokine storm in the human system called cytokine release syndrome (CRS), which emanates due to unrestricted immune reactions. The inflammatory cytokine storm is the main reason for acute respiratory distress syndrome (ARDS), resulting in a multiple-organ failure, which is one of the primary reasons of death in critical patients. It is noble that extensive current research on drug trials on interleukin (IL)-6, which block its receptor site (Tocilizumab, an anti-IL-6 receptor antibody, and Sarilumab) or IL-6 itself (Siltuximab), are being conducted. On account of the primary nature of macrophages in COVID-19, ACE2-expressing CD68⁺CD169⁺ macrophages comprised of the SARS-CoV-2 nucleoprotein antigen portray a higher discharge of IL-6 in the affected lymphatic system.¹⁶⁷ The cells and tissues affected by SARS-CoV-2 also exhibit the upregulated expression of Fas, denoting the role of CD169⁺ macrophages in the significant pathogenesis of viral replication, anomalous inflammation, and lymphocyte apoptosis. Enlarged alveolar exudate caused by the elongated neutrophils and monocytes passing into the lung arterioles containing fibrin deposits was been studied in biopsy slides of affected patients. The state-of-the-art of Nanomedicine may be highly promising in this extensive area by inducing the specificity/efficiency of immunosuppressant delivery-targeting immune cells, followed by minimization of drug overdosage and subsequent possible side effects.¹⁶⁸ The distinct architecture of Nanotool design can substantially circumvent the immune system, thereby tuning the surface charge and providing favourable room for drug encapsulation or loading. Carbon-based porous nanostructured materials, mainly graphene, has excellent potential to rummage the CRS from the serum *via* an extracorporeal perfusion method. In addition, hierarchically porous carbon nanomaterials showed efficacious adsorption of several cytokines, such as IL-6 and TNF- α . Through the impressive application of nanotechnology and nanomedicine, we can envision therapeutic modalities and target specific immune subpopulations by utilizing a fascinating immunomodulatory platform.¹⁶⁹

10. Reusable and recyclable masks

One-time-use surgical masks or respirators can prevent oral droplets containing viruses from entering the lungs, aiding in

the reduction of the chance of being infected, together with the maintenance of proper hygiene practices.¹⁷⁰ Nevertheless, conventional masks have a few limitations including surface hydrophobicity, reusability, and recyclability. Thus, to overcome these limitations, the latest nanostructured materials and polymeric fibres, fluorinated polymers, metal nanowires, and graphene have been explored as superhydrophobic coatings (Fig. 9).

Super-hydrophobic surface coatings on N95 masks can be made possible *via* laser-induced graphene materials, which are adaptable, scalable, and cost-effective in comparison to the market predecessors, such as polyimide, SPEEK, and Bakelite. Zhong *et al.* formulated a double-mode laser-induced forward transfer process for accumulating graphene in a commercial surgical mask.¹⁷² The decontamination stratagem is improved *via* the usage of nanostructured and layered graphene layers, having a static contact angle of more than 140°, wherein the enhanced superhydrophobicity facilitates low adherence of the virus droplets on the mask surface. In addition, solar illumination induces surface sterilization by the prompt increase in the surface temperature to about 80 °C.¹⁷¹ Meanwhile, plasmonic photothermal and superhydrophobic coatings on N95 respirators provide profound protection compared to existing PPE. The coating of silver nanoparticles results in extra shielding through the decontamination effect of the silver ions on microbes. The synergistic landscape of nanostructured composite coatings can encourage the scientific community to miniaturize advanced personal protection equipment (PPE) in the future to fight the COVID-19 pandemic.

11. Exploration of nanovaccines

Nanotechnology has embraced both prophylactic and various therapeutic approaches to combat the outbreaks of fatal diseases and respiratory infectious illnesses. In general, nanovaccines are a novel troop of vaccines, wherein nanoparticles (NPs) are used as functional vehicles. Conventional vaccines exhibit various constraints regarding weak immunogenicity, inherent *in vivo* instability, toxicity, and require various multiple administration profiles. Nanotechnology enabled the design of vaccines favouring the cellular immune response, which can assist the advanced phagocytosis process associated with lymphoid tissue. Now, this ultimately leads to enhanced antigen detection to the receptor site and virus penetration.¹⁷³ The current onset of respiratory contagious diseases is inspiring the development of novel antigen formulations and a new blueprint for viral vaccination based on an emerging nanotechnology-driven approach. Likewise, to upgrade the route of vaccine administration and their delivery to smaller and remote villages in countries around the world, it is necessary to boost the frequency of vaccinations and storage capability of vaccines, which is in the early stages of implementation. Typical vaccines have been fashioned to exploit compromised or live-attenuated organisms (1st generation), but subunit and RNA/DNA vaccines (2nd and 3rd generations, respectively) are pragmatically oriented



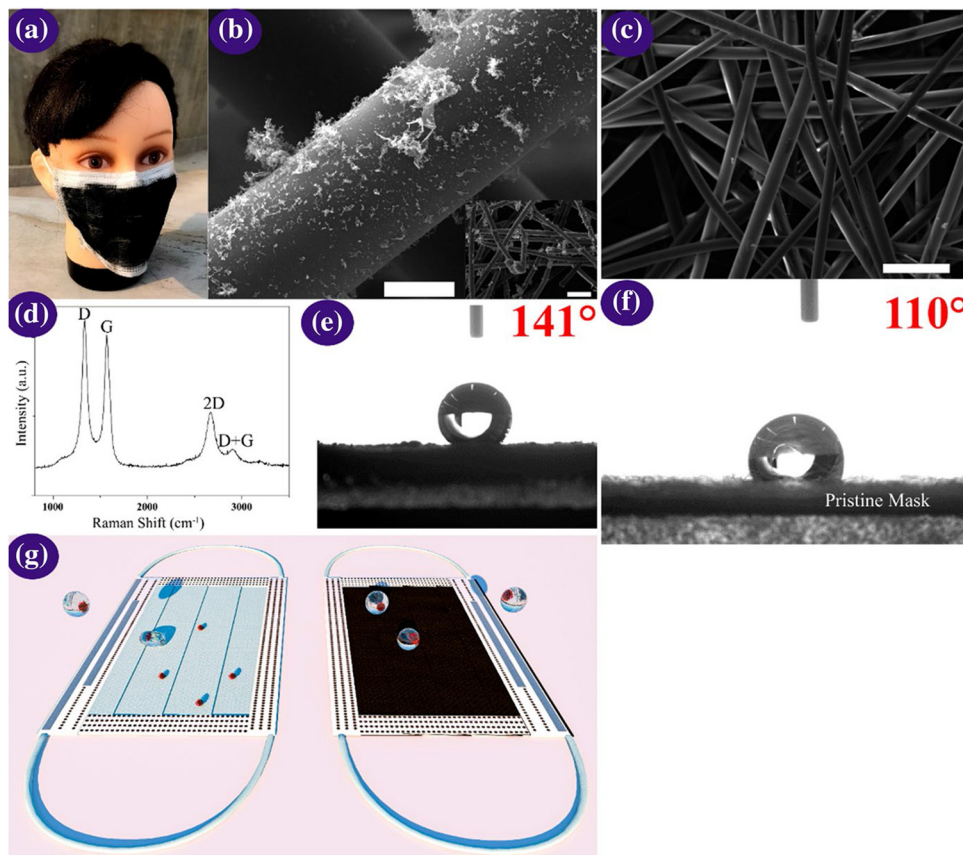


Fig. 9 (a) Optical micrographs of the laser-modified graphene mask. (b) Scanning micrographs of the graphene layer nonwoven fibre matrix on a surgical mask; scale bar is 10 μM . The inset is a zoomed-out image, with the scale bar of 100 μM . (c) Scanning micrographs of the nonwoven fibre matrix derived from a surgical mask; the scale bar is 100 μM . (d) Raman spectrum of the graphene layered mask. (e and f) Measurement of contact angle on the graphene layered and bare mask and (g) self-cleaning property analysis of the black graphene-coated mask compared to a pristine surgical mask. Illustration of the self-cleaning properties of the black graphene-coated mask (right) compared to the pristine blue mask (left). Reproduced with permission from Zhong *et al.*¹⁷¹ Copyright 2020, American Chemical Society.

to advocate preventive immunity from infectious diseases. Surface tailoring with nanocarriers with targeting moieties offers opportunities and facilitates specificity and selectivity in the immune responses by attacking specific surface receptors of various immune cells.^{174–176}

The exploration of nano-vaccines minimizes the adversity arising due to cold chain transportation and storage stability given that nanoformulations can be easily lyophilized, leading to an increased shelf-life. Furthermore, the unique size of nanoparticles, which is comparable to that of viruses and bacteria, aids in the prompt recognition of immune systems. Versatile nanostructured carriers, including non-metal NPs, QDs, carbon nanomaterials, polymeric NPs (chitosan, poly(lactide-co-glycolides) (PLGA), poly(glutamic acid) (PGA), metal/metal oxide NPs, silica NPs, carbon black NPs, liposomes, dendrimers, solid lipid nanocarriers, and virus-like particles (VLPs)) have been extensively synthesized and scrutinized to transport various compounds, *e.g.*, drugs, proteins/peptides, DNA/RNA, antibodies, and vaccines, due to their usefulness in antigen therapeutics. Considering the fascinating structural architecture of nanoparticles, they have been widely admired as vaccine adjuvants and utilized in vaccine delivery.

In this context, VLPs deliver repetitive immune viral epitopes to initiate a specific, strong immune reaction consisting of humoral or cellular immunities.^{177,178} Interestingly, the first VLP nano-vaccine licensed for individual convenience was HBsAg (hepatitis B surface antigen). Epaxal[®], an FDA-approved liposomal vaccine, is used to prevent HAV and is pragmatic together with immune potentiating reconstituted influenza virus (IRIV).

Liposomes (virosomes) were used to make aluminium-free vaccines made from formalin-deactivated HAV (strain RG-SB). The liposome-based vaccine HepaXen was designed initially with the target to counter hepatitis A, C, and E with a focus on antiviral action. An immune response of 20-fold greater than a popular prophylactic vaccine was attained by a combination of reconnected hepatitis B and plasmid DNA encoding. Another vaccine, Inflexal V, is an approved virosomal adjuvanted vaccine for influenza that possesses good biocompatibility and has the capability to mimic natural infection.

In current trends of vaccination, mainly live-attenuated vaccines exhibit relapse jeopardy to their pathogenic virulence in specific immunocompromised conditions. To combat COVID-19, avant-garde vaccination aims to target the transmembrane spike



(S) glycoprotein, which is responsible for host cell penetration. This prompt coupling of human ACE2 with SARS-CoV receptors triggers the chain of transmission in large human populations. Vaccination of mice with CoV S NPs resulted in the production of significant yields of neutralizing antibodies contrary to the homologous virus.¹⁷⁹ An adjuvant can play a prime protagonist to instigate the production of neutral antibodies to the COVID-19 S protein. Thus, a nanotechnology-driven innovative approach can open a new avenue of vaccination, which can restrict the CoV pathway and multiplication in *in vivo* systems. Amongst the wide spectrum of nanoparticles, silver and gold NPs are employed as adjuvants to accelerate the IgA/IgG specific antigen.^{180,181} Furthermore, the nonvascular architecture of spike proteins (S proteins) can also be explored together with research focused on the development of NP-based vaccination systems against CoV diagnostic theranostic schemes. Considering the published report of the genomic analysis of SARS-CoV-2 on January 11, 2020, extensive investigation has been carried to design vaccines against COVID-19. The first vaccine Phase I human clinical trial was initiated on March 16, 2020,¹⁸² and subsequently, 59 novel patients entered the trial quickly as of May 22, 2020.¹⁸³

Immune-targeted nanotherapeutics can be explored by designing nanomaterials at the nanoscale, which are proficient in magnifying the host's immune reaction, including adjuvants in the milieu of vaccination. Progress of these vaccines will be based on the interactive pattern of viral antigens and immunogenic spike protein (S1), targeted *via* antibodies of restorative patients who have recovered from the virus.^{184,185} Successful vaccination requires a suitable type of polymeric conjugate relevant to the target antigen. In this context, lipid and lipid-based NPs can be adopted as a delivery platform for mRNAs or siRNAs to facilitate the design of major viral proteins for vaccines or for disabling viral antigenic target genes.^{184,185} Several different companies are conducting developmental research on mRNA-based vaccines by entrapping SARS-CoV-2 proteins such as the spike protein encoded in nanoliposomes having particular physical and chemical attributes, which are possibly lower than that known for vaccination from some tumour antigens. On March 16, 2020, Moderna and the Vaccine Research Center at the US National Institutes of Health (NIH), in partnership, began with early volunteers in a Phase I clinical trial, testing and evaluating an mRNA vaccine (mRNA-1273) encapsulated in lipid NPs. This was completed within a given time of only 63 days after sequence selection (NCT04283461). The enrolment of the first group of volunteers (18 to 55 year-old healthy subjects) was completed on April 16, 2020.

Another study inferred the exploration of SARS-CoV-2 nanodrugs by vaccinating camelids (llama or alpaca) with target antigens such as RBD, S1, or S2 of the SARS-CoV-2S protein. Afterward, the vaccinated nanodrug reserves can be entrenched and filtered. The attachment of nanodrugs to the RBD can prevent its receptor from attaching ACE2, thereby restricting viral attachment and entrance. The attachment of nanodrugs to S1 or S2 may prevent the S protein from transforming to its post-fusion conformation, thus restricting membrane fusion and viral entrance.¹⁸⁶

Tao *et al.* aimed at vaccine development against influenza viruses including H1N1, H3N2, and H5N1, utilizing gold nanoparticles coupled with matrix protein 2 (M2e).¹⁸⁷ Additionally Novavax, an adjuvant, entered a Phase III clinical trial, showing 89% efficacy to recombinant SARS-CoV-2 glycoprotein-mediated NVX-CoV2373.¹⁸⁸ The Novavax COVID-19 vaccine demonstrated 89.3% efficacy in a UK Phase 3 Trial.¹⁸⁹ The virus-like protein (VLP) instigates the self-assembly of different genetically engineered viral structural proteins, specifically amplifying the humoral and cell-mediated immunity (AMI and CMI). Currently, extensive research work is underway to develop monodispersed VLP-based vaccine formulations based on commercialized prophylactic against both the hepatitis B virus (HBV) and human papillomavirus (HPV). For instance, *Nicotiana benthamiana* has been explored for the development of genetic VLP architecture vaccines, modulating the spike proteins of SARS-CoV-2. A trial run has been initiated with vaccine candidates by Medicago and SpyBiotech (Serum Institute of India) for commercialization,¹⁹⁰ and SpyBiotech and Serum Institute of India, announced that the first subjects have been dosed in phase I/II trials of a novel virus-like particle vaccine targeting COVID-19.¹⁹¹

Owing to the scalability, sustainability, and prolonged expression of antibodies, nucleic acid-based vaccines and encoded antigenic peptides boost the immune response against viral proteins. However, their major drawbacks include the lack of stability and low cellular internalizations under several physiological conditions. Thus, to address this issue, researchers have focused on the development of DNA vaccines and clinical trial runs were carried out under the active guidance of Inovio Pharmaceuticals/International Vaccine Institute, USA,¹⁹² Phase II/III Study of COVID-19 DNA Vaccine (AG0302-COVID19),¹⁹³ Study of COVID-19 DNA Vaccine (AG0301-COVID-19),¹⁹³ Cadila Healthcare Limited (India),¹⁹⁴ which was predicted to hit the market on June 13 May, 2021,¹⁹⁵ Genexine Consortium (South Korea),¹⁹⁶ Entos Pharmaceuticals Inc. (Canada),¹⁹⁷ GeneOne Life Science, Inc. (South Korea),¹⁹⁸ University of Sydney, Bionet Co., Ltd. Technovalia (Australia),¹⁹⁹ and Takis/Rottapharm Biotech (Italy).²⁰⁰

Importantly, to bifurcate the insertional mutagenesis, Shim *et al.* and Zhao *et al.* prepared polyethyleneimine and polyethyleneimine-stearic acid (PSA) cationic nanomicelles, respectively, for the delivery of mRNA encoding HIV-1 gag to dendritic cells.²⁰¹ Another vaccine candidate, ARCoV-based on a lipid-nanoparticle, targeted the receptor-binding domain (RBD)-encoded site of SARS-CoV-2, leading to the successive release of antibodies for neutralizations.²⁰²

Another prime consequence in the phylogenetic tree map of SARS-CoV-2 is that many variants have emerged, including delta (B.1.617.2), alpha (B.1.1.7), beta (B.1.351), omicron (B.1.1.529) and gamma (P.1). Instead of the variant positions in the S gene, the low immunogenic E sequence may be considered as a prominent targeting site for vaccine development. Current trends imply that the continuous mutation of SARS-CoV2 is quite alarming wherein variants can subsequently infect the vaccinated community, thereby leading to a collapse in herd immunity. Consequently, the NCBI omicron variant with altered genetic mutations showed significant effects and mild breakthrough infections in vaccinated people.²⁰³



Table 1 Update of COVID-19 vaccine candidates including those in the clinical trial phase

Developer	Commercial name	Vaccine	Efficacy towards variants	Ref.
Pfizer-BioNTech COVID-19 Vaccine + Fosun Pharma	Comirnaty	Lipid nanoparticle mRNA vaccines (BNT162b2)	IV NCT04844489; 91% protection against symptomatic; 50% drop after booster for omicron variant	205
Moderna Therapeutics Inc. and the National Institute of Allergy and Infectious Diseases (NIAID)	Spikevax	Prefusion stabilized S protein mRNA-1273 vaccine	IV NCT04900467 94% against any type of COVID-19, being 98% effective in preventing severe disease and 63% effective	206
AstraZeneca and University of Oxford	Vaxzevria	ChAdOx1-S Chimpanzee Adenovirus encoding the SARS-CoV-2 spike glycoprotein	IV NCT04760132 76% against symptomatic COVID-19; 40% against delta variant	207
Janssen Pharmaceuticals, Companies of Johnson Johnson	COVID-19 Vaccine Janssen	Ad26.COVS.S Adenovirus type 26 encoding the SARS-CoV-2 spike glycoprotein	77% after 28 days from single intramuscular immunization and 100% after two doses	208
Novavax	Nuvaxvoid	SARS-CoV-2 recombinant spike protein	III NCT04583995; vaccine efficacy of 90%; in severe moderate people 100%	209
Russian Gamaleya Institute's	Sputnik V	Noviral vector-based vaccine	80% effective	210
Bharat Biotech	BBV152	BBV152 Inactivated vaccine	70% effective	190
Sinovac	CoronaVac	CoronaVac Inactivated vaccine	NA	211
Johnson & Johnson		JNJ-78436735 nonreplicating viral vector	NA	212

Alternatively, nasal vaccination is a promising method for stimulating mucosal immunity in a significant manner. Nasopharynx-associated lymphoid tissue (NALT) tactically disseminated in the nasopharynx and oropharyngeal regions and antigens accumulate NALT through dendritic cells and APC (antigen-presenting cells), inhibiting the spike protein and thereby neutralizing SARS-CoV in Dc cells (Table 1).²⁰⁴

Another pivotal aspect regarding the significant effect of a booster dose is illustrated herewith. Various types of COVID-19 vaccines including mRNA, viral vector, inactivated, and protein-based vaccines are effectively practiced and highlighted as boosters in the community. Boosters can facilitate the neutralizing antibody levels (nAb) and their surrogate markers (anti-spike IgG).⁴¹ In the case of an immunocompromised individual, a booster dose modulates the cross-reactivity, which further enhances the T cell responses. In summary, the findings signify that the amalgamation between vaccine-induced immunity with the emergence of SARS-CoV-2 variants has ultimately piloted breakthrough COVID-19 infections, especially among elderly and immunocompromised individuals having co-morbidities.^{41,213}

12. Gene editing using CRISPR/Cas technology: cutting-edge technology towards targeting SARS-CoV2

CRISPR/Cas9 technology originated based on a bacterial defence mechanism against invading viruses. This has now cast off to inhibit persistent viral infections by integrating their genome into the human genome of the host cells.^{214,215} However, genetic remodelling of viruses can evolve to the emergence of new variants highly resistant to CRISPR/Cas9 or other therapeutic agents, thereby boosting the pathogenic index of the virus. Henceforth, variable genomic site-targeting using carrier-free CRISPR/Cas9 schemes can be predominantly in demand for *in vivo* therapeutic applications (Fig. 10).

In 2018, *Streptococcus pyogenes* Cas9 (SpCas9) mRNA and modified single-guide RNA (sgRNA) were grafted onto lipid-based NPs (LNP-INT01). Afterward, testing was carried out in mouse models, wherein this effective biodegradable nanosystem edited the transthyretin (Ttr) gene in the mouse liver with a reduced 97% efficacy rate in the TTR serum protein levels.²¹⁶ A similar study revealed the significant contribution of TT3 lipid-like nanomaterial (LLNs)-induced CRISPR/Cas9 to knock down the subtilisin/kexin type 9 (Pcsk9) gene and reduce the developmental expression of HBV DNA in a mouse model. Besides, TT3 lipid-like nanomaterials (LLNs) were also explored and found to instigate the CRISPR/Cas9-mediated knockdown of the proprotein convertase subtilisin/kexin type 9 (Pcsk9) gene, thereby reducing the expression and genetic deletion of targeted HBV DNA in mice. Upon mutation, *Leptotrichia wadei* (LwaCas13a)-derived Cas13a and *Prevotella* sp. (PspCas13b)-derived Cas13b can be employed to target endogenous transcripts in human embryonic kidney HEK293 cells and mammalian cells, respectively. RNA viral genome obliteration is associated with Cas13d, a type VI RNA-guided nuclease, which could cleave the RNA genome of the virus without damaging the human transcriptome.²¹⁷

Various studies have exploited CRISPR/Cas13d gene-editing technology based on gRNA containing spacer sequences that are complementary to the S gene, ORF1ab, and Cas13d protein, whereas the pCX539 backbone cloned sequences transfected into cultured HEK293T and N2A cells mediated by the Cas13e gene-editing system.^{218,219} Another avant-garde approach was concocted based on the CRISPR/Cas13d system, wherein the PAC-MAN strategy relies on the 22 CRISPR RNAs (crRNAs) to target all the different RNA-dependent RNA polymerase (RdRP) genes as well as the nucleocapsid gene sequence in the lung epithelial cell line (A549) to treat Covid-19. Further CRISPR/Cas systems for Covid-19 gene editing can be transfected by either AAVs or lipofectamine.²²⁰ To tune the immunogenicity and efficiency of AAV in *in vivo* systems, CRISPR/Cas systems in NPs may lead to the introduction of safer and highly-efficient gene-editing platforms for modulating the spatio-temporal release of therapeutic agents.^{219,221}



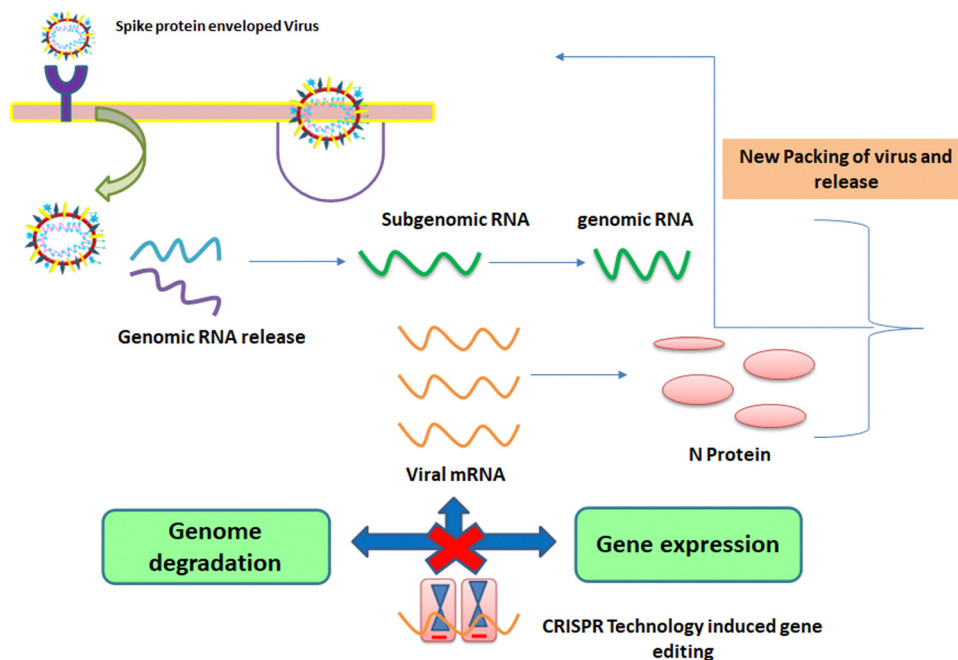


Fig. 10 Advanced technology (CRISPR) toolkit for targeting SARS-CoV *via* genomic editing.

13. Nanotechnology approaches for antiretroviral drugs delivery

To date, the present antiviral treatment has still not framed the epitome and adaptability given that ambiguity arises due to the penetrating efficiency in intricate biological barriers. Nanotechnology can be critically scrutinized in this regard. Nanotechnology has promoted remarkable possible opportunities in healthcare settings and in various diagnostics fields. The various fascinating features of NPs include their nanometric size²²² and huge surface area to volume ratios to achieve a large drug loading.²²³ Surface functionalization that enables cellular membrane passage serves to promote NPs as a good candidate as drug delivery vehicles. Also, the versatile properties of NPs, including bioavailability,²²⁴ virucidal activity, enhanced biomimetic properties,²²⁵ and improved specificity, favour antiviral delivery and sustained drug release to the target site and decrease the emergence of drug resistance, enhance the personalized therapeutic prospect, and reduce adverse drug side effects. To formulate wide-spectrum antiviral agents against various viral mutations, current research findings are being employed to explore advanced engineered moieties to subdue virus replication. The design will be mainly dedicated to the miniaturization of features pertinent to various presentations of the virus.

14. Conclusion and future perspective

To mitigate the COVID-19 catastrophe worldwide, which poses an unprecedented threat and has had major negative impacts on the global arenas including healthcare systems, nanotechnological intervention is intrinsically furnishing advanced

devices and schematic pathways for the unprecedented search for a full understanding of the pathophysiology of various viruses. The one-of-a-kind architecture of nano-tailored sensing platforms and various nanocarrier systems such as nanotraps, nanorobots, nanobubbles, nanoribbons, and nanodiamonds is making the way in the diagnosis, prevention, and therapeutics of viral infections. Nanotraps are potentially fashioned to rummage the targeted infectious virion and viral proteins *via* water-insoluble and coulombic interactions. Astonishingly, miniaturized nanorobots consisting of polymeric/biopolymeric materials including biomimetic substances that prompt pathogen detection, genome editing, and act as a therapeutics delivery vehicle can be noteworthy for the early detection and eradication of pathogens. Future endeavours can be triggered to design nanofibers, nanodiamonds, and nanobubbles as nanotraps for the specific delivery of numerous drugs, giving us a wide range of theranostic tools for disease diagnosis and related comorbidities in a heterogeneous population. Further research on an upscale immune reaction and the use of nanoparticles as an adjuvant to antiviral vaccines provide remarkable solutions to prevent and control viral infections.

14.1. Future traits

COVID-19 has brought the world to its knees, where viruses such as COVID are known to mutate with time. The progression of this pandemic has not been significantly impacted by various SARS-CoV-2 strains, but it can in the future. David Montefiori questioned whether COVID-19, the fatal virus that caused the epidemic this year, would be evolving as it travelled from person to person. Montefiori is a virologist who has devoted most of his career to understanding how HIV can



avoid the immune system due to unintentional mutations. He reasoned that SARS-CoV-2 may have a similar outcome.

Montefiori, who oversees the Duke University AIDS vaccine research lab in Durham, North Carolina, contacted Bette Korber, a recognized authority on HIV evolution and a long-time collaborator, in March. As coronavirus spread around the world, Korber, a computational biologist at the Los Alamos National Laboratory (LANL) in New Mexico, had already begun searching thousands of coronavirus genetic sequences for mutations that may have altered the characteristics of this virus.

SARS-CoV-2 is evolving much more slowly than HIV as it spreads. However, for Korber, one mutation jumped out. Korber found that in the gene that codes for the spike protein, which facilitates viral particle cellular entry, a mutation repeatedly showed up in samples from COVID-19 patients. The amino acid aspartate (D, in biochemical shorthand) was routinely being substituted by glycine (G) due to a copying error, which changed a single nucleotide in the 29 903-letter RNA coding of the virus. This substitution occurs at the 614th amino-acid position of the spike protein, which is known as the D614G mutation by virologists. In a preprint uploaded to the bioRxiv server in April, Korber, Montefiori, and others issued a warning that “D614G is increasing in frequency at an alarming rate”. It quickly took over as the main SARS-CoV-2 lineage in Europe before spreading to the US, Canada, and Australia. The research stated that D614G indicated a “more transmissible variant of SARS-CoV-2” that had evolved as a result of natural selection.

The creation of “variants of concern” is the result of novel sets of mutations, where mutations that affect the properties of a virus, such as its transmissibility and antigenicity, may happen as a result of changes in the immunological profiles of the human hosts. Since many of the most recent SARS-CoV-2 variants are linked to increased transmission, concerns have been raised about the types and rates of viral changes.²²⁶ The virus has fewer opportunities to mutate the less it distributes.²²⁷ SARS-CoV-2 may continue to change in ways that both hasten viral transmission and lessen the effectiveness of vaccines. Infected individuals may also spread the infection even before showing any symptoms. Additionally, many persons who receive a vaccination but subsequently contract an infection may not exhibit any symptoms and will inadvertently continue to spread the virus to others,²²⁸ making it difficult to stop its transmission. We will probably be dealing with this pandemic for years to come if we give up on methods to stop the spread and allow the virus to spread unchecked.

It is not strange to see new versions of viruses develop because viruses constantly mutate. Since the start of the pandemic, the mutations-Y145H and A222V-have been identified in numerous coronavirus lineages. The formation of a novel variant is characterized by an accumulation of mutations that dramatically change the characteristics of the virus lineage. Five SARS-CoV-2 variants have been identified as of December 2021, including the alpha variant (previously known as the UK Variant and referred to as B.1.1.7), the beta variant (previously known as the South Africa variant and referred to as B.1.351), the gamma variant (previously known as the Brazil variant and

referred to as P.1), the delta variant (previously known as the India variant and referred to as B) (formerly called the South Africa variant and referred to as B.1.1.529). All are said to have transmission rates that are noticeably higher than lineages from prior times.

According to reports, the prevalent delta variant can replicate roughly 1000 times more than its ancestors and exhibits immune-evasive characteristics.²²⁹ According to current research, coronavirus antibodies made for the original strain (Wuhan strain) may only be half as potent as those made for the delta variation.²³⁰ Even worse is that those who have the delta strain of the virus are shedding a lot more virus. The host's immunity to the virus may be impacted when the viral dosage received is higher.²³¹ Recent research suggests that the effectiveness of the existing vaccinations, which were created to target the spike protein of the original virus, varies depending on the variation.²³² The spike protein seems to be reasonably stable even for the delta version, despite the possibility of some slight alterations. Another variation, known as AY.4.2 and dubbed “delta plus” by some, has been discovered in the UK and has the potential to spread more rapidly than the standard delta.²³³ Although most covid infections in the UK are still caused by the standard delta, “delta plus” infections are on the rise. Although there is currently no proof that it results in worsening of the sickness, the most recent official data indicate that 6% of covid cases are of this type. Also, the effectiveness of current vaccinations against the delta plus sub-variant is not yet known.

Omicron was found in South Africa,^{234,235} which exhibits a large number of spike protein mutations and is regarded by the WHO as a “variant of concern.” The spike protein, which the virus uses as a point of entry into our cells and is the target of current vaccinations, has 32 mutations in this version. The receptor-binding domain (RBD) alterations in the omicron variant total 10 compared to just 2 in the widely spread delta variant. Additionally, according to early studies from the University of Hong Kong, the omicron variation infects and replicates in the human bronchus 70 times quicker than its forerunners, yet the infection in the lung is noticeably lower.²³⁶ This data confirms the findings that although this variant is more contagious, it results in less severe disease. It is currently undergoing peer review for publication. The spread of this variation around the globe has already been reported by the governments and media of numerous nations. Both the effectiveness of the available vaccinations against this variation and its potential level of hazard is unknown to scientists at this time. In the upcoming weeks, we anticipate some succinct responses.

Uncertainty exists on how vaccination affects virus transmission.²³⁷ According to recent research, those who received the delta-type vaccine can contain just as much virus in their noses as those who were not immunized.²³⁸ Contrarily, compared to those who are unprotected and infected with the delta form, those who have had vaccinations may have a shorter duration during which they are contagious. For the first week of illness, delta virus loads were comparable between the two groups, but after day 7, in those who had received vaccinations, they rapidly decreased.²³⁹



SARS-CoV-2 transmission is not yet seasonal. It has been observed that greater infection not always happens during winter outbreaks in a number of warmer nations, including Iran and India. However, research suggests that the stability and spread of respiratory viruses are enhanced by dry winter air and that breathing dry air during colder weather may weaken the respiratory-tract immune system.²⁴⁰ In addition, people are more prone to stay inside during the winter, which increases the chance of virus transmission by droplets. Accordingly, the containment efforts in the Northern Hemisphere may be hampered by these elements this winter.

Many nations may overlook the discovery of new SARS-CoV-2 variants because they lack the facilities and trained staff necessary to conduct thorough virus genome analyses. Unknown to us, there may be many more varieties circulating worldwide, which will affect the pace of transmission in various regions of the world. Primo or breakthrough infections require careful COVID-19 detection assays, especially considering the constant appearance of novel viral strains. In samples, the PCR test looks for signs of the genetic material of the virus. The PCR test typically looks for a three-part sequence on the spike protein of the virus to confirm the existence of an infection. One of these PCR targets was observed to be increasingly tested negative in samples from England regions with rapidly increasing case numbers, despite the fact that the other two targets in the tests were still functioning. It is rare to have two test sequences function, while the third does not. Investigations revealed that the virus in these samples had changed, where a deletion at the H69 and V70 locations was identified to be the root of the test failures.²⁴¹

Considering the present challenges posed by COVID-19 with respect to its various variants, it is important to develop vaccines for specific variants and test kits for the diverse variants, given that the many variants may mutate into forms that require specified test approaches to detect and treat them.

Conflicts of interest

There are no conflicts to declare.

Acknowledgements

The authors wish to appreciate DST West Bengal, the Centre for Research in Nanoscience and Nanotechnology, and the Department of Polymer Science and Technology University of Calcutta for their financial and technical support.

References

- 1 C. Weiss, M. Carriere, L. Fusco, I. Capua, J. A. Regla-Nava, M. Pasquali, J. A. Scott, F. Vitale, M. A. Unal and C. Mattevi, *ACS Nano*, 2020, **14**, 6383–6406.
- 2 L. Zhang, D. Lin, X. Sun, U. Curth, C. Drosten, L. Sauerhering, S. Becker, K. Rox and R. Hilgenfeld, *Science*, 2020, **368**, 409–412.
- 3 M. Gandhi, D. S. Yokoe and D. V. Havlir, *N. Engl. J. Med.*, 2020, **382**, 2158–2160.
- 4 P. Hassanzadeh, *J. Controlled Release*, 2020, **328**, 112–126.
- 5 WHO Coronavirus (COVID-19) Dashboard, <http://covid.who.int> (accessed 2021-03-13).
- 6 R. Medhi, P. Srinoi, N. Ngo, H.-V. Tran and T. R. Lee, *ACS Appl. Nano Mater.*, 2020, **3**, 8557–8580.
- 7 J. Sharma, K. Shepardson, L. L. Johns, J. Wellham, J. Avera, B. Schwarz, A. Rynda-Apple and T. Douglas, *ACS Appl. Mater. Interfaces*, 2020, **12**, 18211–18224.
- 8 S. Fukushi, A. Fukuma, T. Kurosu, S. Watanabe, M. Shimojima, K. Shirato, N. Iwata-Yoshikawa, N. Nagata, K. Ohnishi and M. Ato, *J. Virol. Methods*, 2018, **251**, 22–29.
- 9 R. Yan, Y. Zhang, Y. Li, L. Xia, Y. Guo and Q. Zhou, *Science*, 2020, **367**, 1444–1448.
- 10 J. F.-W. Chan, S. Yuan, K.-H. Kok, K. K.-W. To, H. Chu, J. Yang, F. Xing, J. Liu, C. C.-Y. Yip and R. W.-S. Poon, *Lancet*, 2020, **395**, 514–523.
- 11 H. L. Chan, S. K. Tsui and J. J. Sung, *Trends Mol. Med.*, 2003, **9**, 323–325.
- 12 H. F. Rabenau, J. Cinatl, B. Morgenstern, G. Bauer, W. Preiser and H. W. Doerr, *Med. Microbiol. Immunol.*, 2005, **194**, 1–6.
- 13 P. A. Rota, M. S. Oberste, S. S. Monroe, W. A. Nix, R. Campagnoli, J. P. Icenogle, S. Peñaranda, B. Bankamp, K. Maher, M.-H. Chen, S. Tong, A. Tamin, L. Lowe, M. Frace, J. L. DeRisi, Q. Chen, D. Wang, D. D. Erdman, T. C. T. Peret, C. Burns, T. G. Ksiazek, P. E. Rollin, A. Sanchez, S. Liffick, B. Holloway, J. Limor, K. McCaustland, M. Olsen-Rasmussen, R. Fouchier, S. Günther, A. D. M. E. Osterhaus, C. Drosten, M. A. Pallansch, L. J. Anderson and W. J. Bellini, *Science*, 2003, **300**, 1394–1399.
- 14 K. L. Hon, *Travel Med. Infect. Dis.*, 2013, **11**, 285–287.
- 15 T. Liu, J. Hu, M. Kang, L. Lin, H. Zhong, J. Xiao, G. He, T. Song, Q. Huang and Z. Rong, Time-varying transmission dynamics of Novel Coronavirus Pneumonia in China, *bioRxiv*, 2020, preprint, DOI: [10.1101/2020.01.25.919787](https://doi.org/10.1101/2020.01.25.919787).
- 16 Y. Zhu, L. Chen, H. Ji, M. Xi, Y. Fang and Y. Li, *Neurosci. Bull.*, 2020, **36**, 299–302.
- 17 P. Zhou, H. Fan, T. Lan, X.-L. Yang, W.-F. Shi, W. Zhang, Y. Zhu, Y.-W. Zhang, Q.-M. Xie, S. Mani, X.-S. Zheng, B. Li, J.-M. Li, H. Guo, G.-Q. Pei, X.-P. An, J.-W. Chen, L. Zhou, K.-J. Mai, Z.-X. Wu, D. Li, D. E. Anderson, L.-B. Zhang, S.-Y. Li, Z.-Q. Mi, T.-T. He, F. Cong, P.-J. Guo, R. Huang, Y. Luo, X.-L. Liu, J. Chen, Y. Huang, Q. Sun, X.-L.-L. Zhang, Y.-Y. Wang, S.-Z. Xing, Y.-S. Chen, Y. Sun, J. Li, P. Daszak, L.-F. Wang, Z.-L. Shi, Y.-G. Tong and J.-Y. Ma, *Nature*, 2018, **556**, 255–258.
- 18 P. V. M. Simas, A. C. de Souza Barnabé, R. Durães-Carvalho, D. F. de Lima Neto, L. C. Caserta, L. Artacho, F. A. F. Jacomassa, M. C. Martini, M. M. A. B. Dos Santos and P. A. N. Felippe, *Emerging Infect. Dis.*, 2015, **21**, 729.
- 19 J. Cui, F. Li and Z.-L. Shi, *Nat. Rev. Microbiol.*, 2019, **17**, 181–192.
- 20 S. Van Boheemen, M. De Graaf, C. Lauber, T. M. Bestebroer, V. S. Raj, A. M. Zaki, A. D. Osterhaus, B. L. Haagmans, A. E. Gorbalenya and E. J. Snijder, *mBio*, 2012, **3**, e00473.
- 21 Y. Chen, Q. Liu and D. Guo, *J. Med. Virol.*, 2020, **92**, 418–423.



- 22 M. Czub, H. Weingartl, S. Czub, R. He and J. Cao, *Vaccine*, 2005, **23**, 2273–2279.
- 23 C. A. De Haan, L. Kuo, P. S. Masters, H. Vennema and P. J. Rottier, *J. Virol.*, 1998, **72**, 6838–6850.
- 24 Y. Huang, C. Yang, X. Xu, W. Xu and S. Liu, *Acta Pharmacol. Grzech.*, 2020, **41**, 1141–1149.
- 25 P. Song, W. Li, J. Xie, Y. Hou and C. You, *Clin. Chim. Acta*, 2020, **509**, 280–287.
- 26 T. Gu, S. Zhao, G. Jin, M. Song, Y. Zhi, R. Zhao, F. Ma, Y. Zheng, K. Wang and H. Liu, *Front. Immunol.*, 2021, **11**, 621441.
- 27 N. Magazine, T. Zhang, Y. Wu, M. C. McGee, G. Veggiani and W. Huang, *Viruses*, 2022, **14**, 640.
- 28 Y. Araf, F. Akter, Y. D. Tang, R. Fatemi, M. S. A. Parvez, C. Zheng and M. G. Hossain, *J. Med. Virol.*, 2022, **94**, 1825–1832.
- 29 L. Chen and J. Liang, *Mater. Sci. Eng., C*, 2020, **112**, 110924.
- 30 M. Yang, K. Sunderland and C. Mao, *Chem. Rev.*, 2017, **117**, 10377–10402.
- 31 M. Oswald, S. Geissler and A. Goepferich, *Mol. Pharmaceutics*, 2017, **14**, 2177–2196.
- 32 S. Gurunathan, M. Qasim, Y. Choi, J. T. Do, C. Park, K. Hong, J.-H. Kim and H. Song, *Nanomaterials*, 2020, **10**, 1645.
- 33 M. Hoffmann, H. Kleine-Weber, S. Schroeder, N. Krüger, T. Herrler, S. Erichsen, T. S. Schiergens, G. Herrler, N.-H. Wu, A. Nitsche, M. A. Müller, C. Drosten and S. Pöhlmann, *Cell*, 2020, **181**, 271–280.e278.
- 34 X. Ou, Y. Liu, X. Lei, P. Li, D. Mi, L. Ren, L. Guo, R. Guo, T. Chen and J. Hu, *Nat. Commun.*, 2020, **11**, 1–12.
- 35 Q. Wang, Y. Zhang, L. Wu, S. Niu, C. Song, Z. Zhang, G. Lu, C. Qiao, Y. Hu and K.-Y. Yuen, *Cell*, 2020, **181**, 894–904.e899.
- 36 J. A. Fulcher, K. Tamshen, A. L. Wollenberg, V. A. Kickhoefer, J. Mrazek, J. Elliott, F. J. Ibarrodo, P. A. Anton, L. H. Rome, H. D. Maynard, T. Deming and O. O. Yang, *Bioconjugate Chem.*, 2019, **30**, 2216–2227.
- 37 J. S. Chahal, O. F. Khan, C. L. Cooper, J. S. McPartlan, J. K. Tsosie, L. D. Tilley, S. M. Sidik, S. Lourido, R. Langer and S. Bavari, *Proc. Natl. Acad. Sci. U. S. A.*, 2016, **113**, E4133–E4142.
- 38 R. Ribeiro-Viana, M. Sánchez-Navarro, J. Luczkowiak, J. R. Koeppe, R. Delgado, J. Rojo and B. G. Davis, *Nat. Commun.*, 2012, **3**, 1–9.
- 39 Q. Zhang, A. Honko, J. Zhou, H. Gong, S. N. Downs, J. H. Vasquez, R. H. Fang, W. Gao, A. Griffiths and L. Zhang, *Nano Lett.*, 2020, **20**, 5570–5574.
- 40 T. Tang, M. Bidon, J. A. Jaimes, G. R. Whittaker and S. Daniel, *Antiviral Res.*, 2020, **178**, 104792.
- 41 U. S. Kumar, R. Afjei, K. Ferrara, T. F. Massoud and R. Paulmurugan, *ACS Nano*, 2021, **15**, 17582–17601.
- 42 G. Muthiah, A. Sarkar, S. Roy, P. Singh, P. Kumar, K. Bhardwaj and A. Jaiswal, *ChemNanoMat*, 2022, **8**, e202100505.
- 43 G. Seo, G. Lee, M. J. Kim, S.-H. Baek, M. Choi, K. B. Ku, C.-S. Lee, S. Jun, D. Park, H. G. Kim, S.-J. Kim, J.-O. Lee, B. T. Kim, E. C. Park and S. I. Kim, *ACS Nano*, 2020, **14**, 5135–5142.
- 44 M. Khater, A. D. L. Escosura-Muñiz, L. Altet and A. Merkoçi, *Anal. Chem.*, 2019, **91**, 4790–4796.
- 45 F. Biotech, FDA greenlights first smartphone-based home COVID-19 test, <https://www.fiercebiotech.com/medtech/fda-greenlights-first-smartphone-based-home-covid-19-test>, (accessed 03.09.2022, 2022).
- 46 G. Palestino, I. García-Silva, O. González-Ortega and S. Rosales-Mendoza, *Expert Rev. Anti-Infect. Ther.*, 2020, **18**, 849–864.
- 47 B. Udugama, P. Kadhiresan, H. N. Kozłowski, A. Malekjahani, M. Osborne, V. Y. Li, H. Chen, S. Mubareka, J. B. Gubbay and W. C. Chan, *ACS Nano*, 2020, **14**, 3822–3835.
- 48 J. M. Ferdinands, L. E. W. Olsho, A. A. Agan, N. Bhat, R. M. Sullivan, M. Hall, P. M. Mourani, M. Thompson and A. G. Randolph, *J. Infect. Dis.*, 2014, **210**, 674–683.
- 49 W. Chantong and J. B. Kaneene, *Southeast Asian J. Trop. Med. Public Health*, 2011, **42**, 596.
- 50 R. J. Coker, B. M. Hunter, J. W. Rudge, M. Liverani and P. Hanvoravongchai, *Lancet*, 2011, **377**, 599–609.
- 51 M. Jonduo, S.-S. Wong, N. Kapo, P. Ominipi, M. Abdad, P. Siba, P. McKenzie, R. Webby and P. Horwood, *West. Pac. Surveill. Response J.*, 2013, **4**, 11.
- 52 S. Das, S. Dunbar and Y.-W. Tang, *Front. Microbiol.*, 2018, **9**, 2478.
- 53 J. C. Huang, Y.-F. Chang, K.-H. Chen, L.-C. Su, C.-W. Lee, C.-C. Chen, Y.-M. A. Chen and C. Chou, *Biosens. Bioelectron.*, 2009, **25**, 320–325.
- 54 C. Roh and S. K. Jo, *J. Chem. Technol. Biotechnol.*, 2011, **86**, 1475–1479.
- 55 M. Park, J. Won, B. Y. Choi and C. J. Lee, *Exp. Mol. Med.*, 2020, **52**, 963–977.
- 56 P. Teengam, W. Siangproh, A. Tuantranont, T. Vilaivan, O. Chailapakul and C. S. Henry, *Anal. Chim. Acta*, 2018, **1044**, 102–109.
- 57 F. N. Ishikawa, H.-K. Chang, M. Curreli, H.-I. Liao, C. A. Olson, P.-C. Chen, R. Zhang, R. W. Roberts, R. Sun and R. J. Cote, *ACS Nano*, 2009, **3**, 1219–1224.
- 58 Y. Chen, K.-H. Chan, Y. Kang, H. Chen, H. K. Luk, R. W. Poon, J. F. Chan, K.-Y. Yuen, N. Xia and S. K. Lau, *Emerging Microbes Infect.*, 2015, **4**, 1–5.
- 59 R. Funari, K.-Y. Chu and A. Q. Shen, *Biosens. Bioelectron.*, 2020, **169**, 112578.
- 60 L. A. Layqah and S. Eissa, *Microchim. Acta*, 2019, **186**, 224.
- 61 G. Seo, G. Lee, M. J. Kim, S.-H. Baek, M. Choi, K. B. Ku, C.-S. Lee, S. Jun, D. Park and H. G. Kim, *ACS Nano*, 2020, **14**, 5135–5142.
- 62 G. Qiu, Z. Gai, Y. Tao, J. Schmitt, G. A. Kullak-Ublick and J. Wang, *ACS Nano*, 2020, **14**, 5268–5277.
- 63 I. PathSensors, Announced the Development of a SARS-CoV-2 Biosensor, PathSensors Inc., 2022, <https://markets.businessinsider.com/news/stocks/pathensors-inc-announced-the-development-of-a-sars-cov-2-biosensor-1029025341>.
- 64 A. Srivastava, N. Dwivedi, C. Dhand, R. Khan, N. Sathish, M. Gupta, R. Kumar and S. Kumar, *Mater. Today Chem.*, 2020, **18**, 100385.
- 65 Y. Abo-zeid and G. R. Williams, *Wiley Interdiscip. Rev.: Nanomed. Nanobiotechnol.*, 2020, **12**, e1592.
- 66 R. Parboosing, G. E. Maguire, P. Govender and H. G. Kruger, *Viruses*, 2012, **4**, 488–520.



- 67 R. Bawa, *Eur. J. Nanomed.*, 2010, **3**, 34–40.
- 68 S. Galdiero, A. Falanga, M. Vitiello, M. Cantisani, V. Marra and M. Galdiero, *Molecules*, 2011, **16**, 8894–8918.
- 69 R. A. Schwendener, *Ther. Adv. Vaccines*, 2014, **2**, 159–182.
- 70 A. Gupta, D. F. Moyano, A. Parnsubsakul, A. Papadopoulos, L.-S. Wang, R. F. Landis, R. Das and V. M. Rotello, *ACS Appl. Mater. Interfaces*, 2016, **8**, 14096–14101.
- 71 D. Bartczak, O. L. Muskens, T. Sanchez-Elsner, A. G. Kanaras and T. M. Millar, *ACS Nano*, 2013, **7**, 5628–5636.
- 72 W.-H. Wen, M. Lin, C.-Y. Su, S.-Y. Wang, Y.-S. E. Cheng, J.-M. Fang and C.-H. Wong, *J. Med. Chem.*, 2009, **52**, 4903–4910.
- 73 H. Andresen, M. Mager, M. Griefsner, P. Charchar, N. Todorova, N. Bell, G. Theocharidis, S. Bertazzo, I. Yarovsky and M. M. Stevens, *Chem. Mater.*, 2014, **26**, 4696–4704.
- 74 M.-C. Bowman, T. E. Ballard, C. J. Ackerson, D. L. Feldheim, D. M. Margolis and C. Melander, *J. Am. Chem. Soc.*, 2008, **130**, 6896–6897.
- 75 P. Di Gianvincenzo, M. Marradi, O. M. Martínez-Ávila, L. M. Bedoya, J. Alcamí and S. Penadés, *Bioorg. Med. Chem. Lett.*, 2010, **20**, 2718–2721.
- 76 A. Mehranfar and M. Izadyar, *J. Phys. Chem. Lett.*, 2020, **11**, 10284–10289.
- 77 A. R. Bastian, A. Nangarlia, L. D. Bailey, A. Holmes, R. V. K. Sundaram, C. Ang, D. R. Moreira, K. Freedman, C. Duffy and M. Contarino, *J. Biol. Chem.*, 2015, **290**, 529–543.
- 78 M. A. Dkhill, A. A. Bauomy, M. S. Diab and S. Al-Quraishy, *Int. J. Nanomed.*, 2015, **10**, 7467.
- 79 Y. Bai, Y. Zhou, H. Liu, L. Fang, J. Liang and S. Xiao, *ACS Appl. Nano Mater.*, 2018, **1**, 969–976.
- 80 X. Huang, M. Li, Y. Xu, J. Zhang, X. Meng, X. An, L. Sun, L. Guo, X. Shan and J. Ge, *ACS Appl. Mater. Interfaces*, 2019, **11**, 19799–19807.
- 81 T. Du, J. Zhang, C. Li, T. Song, P. Li, J. Liu, X. Du and S. Wang, *Bioconjugate Chem.*, 2020, **31**, 2553–2563.
- 82 S. M. Moghimi, A. C. Hunter and J. C. Murray, *Pharmacol. Rev.*, 2001, **53**, 283–318.
- 83 W. H. De Jong, *Int. J. Nanomed.*, 2008, **3**, 133–149.
- 84 K. Asadi and A. Gholami, *Int. J. Biol. Macromol.*, 2021, **182**, 648–658.
- 85 R. M. Rosa, J. C. Silva, I. S. Sanches and C. Henriques, *Mater. Lett.*, 2017, **207**, 145–148.
- 86 S. Gaikwad, A. Ingle, A. Gade, M. Rai, A. Falanga, N. Incoronato, L. Russo, S. Galdiero and M. Galdiero, *Int. J. Nanomed.*, 2013, **8**, 4303.
- 87 X. Lv, P. Wang, R. Bai, Y. Cong, S. Suo, X. Ren and C. Chen, *Biomaterials*, 2014, **35**, 4195–4203.
- 88 D. Xiang, Y. Zheng, W. Duan, X. Li, J. Yin, S. Shigdar, M. L. O'Connor, M. Marappan, X. Zhao and Y. Miao, *Int. J. Nanomed.*, 2013, **8**, 4103.
- 89 C. Balagna, S. Perero, E. Percivalle, E. V. Nepita and M. Ferraris, *Open Ceram.*, 2020, **1**, 100006.
- 90 T. Q. Huy, N. T. H. Thanh, N. T. Thuy, P. Van Chung, P. N. Hung, A.-T. Le and N. T. H. Hanh, *J. Virol. Methods*, 2017, **241**, 52–57.
- 91 Y. Mori, T. Ono, Y. Miyahira, V. Q. Nguyen, T. Matsui and M. Ishihara, *Nanoscale Res. Lett.*, 2013, **8**, 1–6.
- 92 T. Prasad and E. Elumalai, *Asian Pac. J. Trop. Biomed.*, 2011, **1**, 439–442.
- 93 C. Wan, J. Tai, J. Zhang, Y. Guo, Q. Zhu, D. Ling, F. Gu, J. Gan, C. Zhu and Y. Wang, *Cell Death Dis.*, 2019, **10**, 1–16.
- 94 S. D. Kumar, G. Singaravelu, S. Ajithkumar, K. Murugan, M. Nicoletti and G. Benelli, *J. Cluster Sci.*, 2017, **28**, 359–367.
- 95 R. Govender, A. Phulukdaree, R. M. Gengan, K. Anand and A. A. Chuturgoon, *J. Nanobiotechnol.*, 2013, **11**, 1–9.
- 96 E. G. Haggag, A. M. Elshamy, M. A. Rabeh, N. M. Gabr, M. Salem, K. A. Youssif, A. Samir, A. B. Muhsinah, A. Alsayari and U. R. Abdelmohsen, *Int. J. Nanomed.*, 2019, **14**, 6217.
- 97 J. Zhong, Y. Xia, L. Hua, X. Liu, M. Xiao, T. Xu, B. Zhu and H. Cao, *Artif. Cells, Nanomed., Biotechnol.*, 2019, **47**, 3485–3491.
- 98 Z. Cheng, X. Zhi, G. Sun, W. Guo, Y. Huang, W. Sun, X. Tian, F. Zhao and K. Hu, *J. Med. Virol.*, 2016, **88**, 653–663.
- 99 Z. Lin, Y. Li, M. Guo, M. Xiao, C. Wang, M. Zhao, T. Xu, Y. Xia and B. Zhu, *RSC Adv.*, 2017, **7**, 35290–35296.
- 100 M. M. Melk, S. S. El-Hawary, F. R. Melek, D. O. Saleh, O. M. Ali, M. A. El Raey and N. M. Selim, *Int. J. Nanomed.*, 2021, **16**, 8221.
- 101 R. Kumar, G. Sahoo, K. Pandey, M. Nayak, R. Topno, V. Rabidas and P. Das, *Int. J. Infect. Dis.*, 2018, **73**, 368.
- 102 N. Shionoiri, T. Sato, Y. Fujimori, T. Nakayama, M. Nemoto, T. Matsunaga and T. Tanaka, *J. Biosci. Bioeng.*, 2012, **113**, 580–586.
- 103 X. Hang, H. Peng, H. Song, Z. Qi, X. Miao and W. Xu, *J. Virol. Methods*, 2015, **222**, 150–157.
- 104 S. Muthamil Selvan, K. Vijai Anand, K. Govindaraju, S. Tamilselvan, V. G. Kumar, K. S. Subramanian, M. Kannan and K. Raja, *IET Nanobiotechnol.*, 2018, **12**, 1042–1046.
- 105 S. L. Warnes, Z. R. Little and C. W. Keevil, *mBio*, 2015, **6**, e01697.
- 106 S.-r Choi, B. E. Britigan and P. Narayanasamy, *Antimicrob. Agents Chemother.*, 2017, **61**, e02505.
- 107 R. Kumar, M. Nayak, G. C. Sahoo, K. Pandey, M. C. Sarkar, Y. Ansari, V. Das, R. Topno, M. Madhukar and P. Das, *J. Infect. Chemother.*, 2019, **25**, 325–329.
- 108 H. Cui, J. Jiang, W. Gu, C. Sun, D. Wu, T. Yang and G. Yang, *Photochem. Photobiol.*, 2010, **86**, 1135–1139.
- 109 F. Pfaff, B. Glück, T. Hoyer, D. Rohländer, A. Sauerbrei and R. Zell, *Letts. Appl. Microbiol.*, 2019, **69**, 302–309.
- 110 A. H. M. O.-R. Kaaden, *General Virology. Measurement of infectivity, Medical microbiology, infection and epidemic theory for veterinarians, biologists, agricultural scientists and interested parties from related fields*, 6th edn, 1993.
- 111 L. Sandeep and S. Rajasree, *J. Anal. Pharm. Res.*, 2017, **4**, 10.15406.
- 112 M. L. Smith, S. Gandolfi, P. M. Coshall and P. K. Rahman, *Front. Microbiol.*, 2020, **11**, 1341.
- 113 T. Li, D. Cipolla, T. Rades and B. J. Boyd, *J. Controlled Release*, 2018, **288**, 96–110.
- 114 S. C. Mogenssen, *Microbiol. Rev.*, 1979, **43**, 1–26.



- 115 C. Sinico, A. De Logu, F. Lai, D. Valenti, M. Manconi, G. Loy, L. Bonsignore and A. M. Fadda, *Eur. J. Pharm. Biopharm.*, 2005, **59**, 161–168.
- 116 H. Ji, Z. Yang, W. Jiang, C. Geng, M. Gong, H. Xiao, Z. Wang and L. Cheng, *J. Huazhong Univ. Sci. Technol., Med. Sci.*, 2008, **28**, 243–246.
- 117 G. Sharma, K. Thakur, A. Setia, B. Amarji, M. P. Singh, K. Raza and O. P. Katare, *Drug Delivery Transl. Res.*, 2017, **7**, 683–694.
- 118 K. Tahara, M. Kobayashi, S. Yoshida, R. Onodera, N. Inoue and H. Takeuchi, *Int. J. Pharm.*, 2018, **543**, 311–317.
- 119 S. Huang, J. Gu, J. Ye, B. Fang, S. Wan, C. Wang, U. Ashraf, Q. Li, X. Wang and L. Shao, *J. Colloid Interface Sci.*, 2019, **542**, 198–206.
- 120 A. Barras, Q. Pagneux, F. Sane, Q. Wang, R. Boukherroub, D. Hober and S. Szunerits, *ACS Appl. Mater. Interfaces*, 2016, **8**, 9004–9013.
- 121 A. Loczechin, K. Séron, A. Barras, E. Giovanelli, S. Belouzard, Y.-T. Chen, N. Metzler-Nolte, R. Boukherroub, J. Dubuisson and S. Szunerits, *ACS Appl. Mater. Interfaces*, 2019, **11**, 42964–42974.
- 122 D. Iannazzo, A. Pistone, M. Salamò, S. Galvagno, R. Romeo, S. V. Giofrè, C. Branca, G. Visalli and A. Di Pietro, *Int. J. Pharm.*, 2017, **518**, 185–192.
- 123 X. Du, R. Xiao, H. Fu, Z. Yuan, W. Zhang, L. Yin, C. He, C. Li, J. Zhou and G. Liu, *Mater. Sci. Eng., C*, 2019, **105**, 110052.
- 124 X. X. Yang, C. M. Li, Y. F. Li, J. Wang and C. Z. Huang, *Nanoscale*, 2017, **9**, 16086–16092.
- 125 F. De Maio, V. Palmieri, G. Babini, A. Augello, I. Palucci, G. Perini, A. Salustri, P. Spilman, M. De Spirito, M. Sanguinetti, G. Delogu, L. G. Rizzi, G. Cesareo, P. Soon-Shiong, M. Sali and M. Papi, *iScience*, 2021, **24**, 102788.
- 126 T. Seifi and A. R. Kamali, *Med. Drug Discovery*, 2021, **11**, 100099.
- 127 A. Kalkal, P. Allawadhi, R. Pradhan, A. Khurana, K. K. Bharani and G. Packirisamy, *Sens. Int.*, 2021, **2**, 100102.
- 128 I. Banerjee, M. P. Douaisi, D. Mondal and R. S. Kane, *Nanotechnology*, 2012, **23**, 105101.
- 129 Z. Liu, M. Winters, M. Holodniy and H. Dai, *Angew. Chem., Int. Ed.*, 2007, **46**, 2023–2027.
- 130 A. Bianco, *Expert Opin. Drug Delivery*, 2004, **1**, 57–65.
- 131 D. Iannazzo, A. Pistone, S. Galvagno, S. Ferro, L. De Luca, A. M. Monforte, T. Da Ros, C. Hadad, M. Prato and C. Pannecouque, *Carbon*, 2015, **82**, 548–561.
- 132 A. Aasi, S. M. Aghaei, M. D. Moore and B. Panchapakesan, *Int. J. Mol. Sci.*, 2020, **21**, 5211.
- 133 M. Mohan Gokhale and R. Ravindra Somani, *Mini-Rev. Org. Chem.*, 2015, **12**, 355–366.
- 134 A. R. Badireddy, E. M. Hotze, S. Chellam, P. Alvarez and M. R. Wiesner, *Environ. Sci. Technol.*, 2007, **41**, 6627–6632.
- 135 E. M. Hotze, T. Phenrat and G. V. Lowry, *J. Environ. Qual.*, 2010, **39**, 1909–1924.
- 136 M. A. Gacem, H. Gacem and A. Ould-El-Hadj-Khelil, *Carbon Nanomaterials for Agri-Food and Environmental Applications*, Elsevier, 2020, pp. 505–533.
- 137 P. Innocenzi and L. Stagi, *Chem. Sci.*, 2020, **11**, 6606–6622.
- 138 O. A. Kraevaya, A. S. Peregodov, I. A. Godovikov, E. V. Shchurik, V. M. Martynenko, A. F. Shestakov, J. Balzarini, D. Schols and P. A. Troshin, *Chem. Commun.*, 2020, **56**, 1179–1182.
- 139 D. Chun-Xian, X. Hai-Rong, J. Hong, L. Qiang, X. Hong and Y. Zhan-Qiu, *Sci. Res. Essays*, 2012, **7**, 705–711.
- 140 M. Shoji, E. Takahashi, D. Hatakeyama, Y. Iwai, Y. Morita, R. Shirayama, N. Echigo, H. Kido, S. Nakamura and T. Mashino, *PLoS One*, 2013, **8**, e66337.
- 141 O. A. Kraevaya, A. V. Novikov, A. F. Shestakov, E. S. Ershova, E. A. Savinova, L. V. Kameneva, N. N. Veiko, D. Schols, J. Balzarini and S. V. Kostyuk, *Chem. Commun.*, 2020, **56**, 10203–10206.
- 142 A. Muñoz, B. M. Illescas, J. Luczkowiak, F. Lasala, R. Ribeiro-Viana, J. Rojo, R. Delgado and N. Martín, *J. Mater. Chem. B*, 2017, **5**, 6566–6571.
- 143 A. Muñoz, D. Sigwalt, B. M. Illescas, J. Luczkowiak, L. Rodriguez-Perez, I. Nierengarten, M. Holler, J.-S. Remy, K. Buffet and S. P. Vincent, *Nat. Chem.*, 2016, **8**, 50–57.
- 144 M. G. Stanford, J. T. Li, Y. Chen, E. A. McHugh, A. Liopo, H. Xiao and J. M. Tour, *ACS Nano*, 2019, **13**, 11912–11920.
- 145 A. R. Deokar, A. P. Nagvenkar, I. Kalt, L. Shani, Y. Yeshurun, A. Gedanken and R. Sarid, *Bioconjugate Chem.*, 2017, **28**, 1115–1122.
- 146 R. Spitz Steinberg, M. Cruz, N. G. Mahfouz, Y. Qiu and R. H. Hurt, *ACS Nano*, 2017, **11**, 5670–5679.
- 147 V. Palmieri and M. Papi, *Nano Today*, 2020, **33**, 100883.
- 148 I. Ekladios, Y. L. Colson and M. W. Grinstaff, *Nat. Rev. Drug Discovery*, 2019, **18**, 273–294.
- 149 N. Larson and H. Ghandehari, *Chem. Mater.*, 2012, **24**, 840–853.
- 150 X. Chen, X. Chen, W. Chen, X. Ma, J. Huang and R. Chen, *J. Med. Virol.*, 2014, **86**, 1705–1713.
- 151 J. Li, F. Yu, Y. Chen and D. Oupický, *J. Controlled Release*, 2015, **219**, 369–382.
- 152 A. H. Andersen, C. F. Riber, K. Zuwala, M. Tolstrup, F. Dagnæs-Hansen, P. W. Denton and A. N. Zelikin, *ACS Macro Lett.*, 2018, **7**, 587–591.
- 153 M. A. Ansari, Q. M. S. Jamal, S. Rehman, A. Almatroudi, M. A. Alzohairy, M. N. Alomary, T. Tripathi, A. H. Alharbi, S. F. Adil, M. Khan and M. Shaheer Malik, *Arabian J. Chem.*, 2020, **13**, 8069–8079.
- 154 M. A. Boles, D. Ling, T. Hyeon and D. V. Talapin, *Nat. Mater.*, 2016, **15**, 141–153.
- 155 D. Ting, N. Dong, L. Fang, J. Lu, J. Bi, S. Xiao and H. Han, *ACS Appl. Nano Mater.*, 2018, **1**, 5451–5459.
- 156 X. Dong, M. M. Moyer, F. Yang, Y.-P. Sun and L. Yang, *Sci. Rep.*, 2017, **7**, 1–10.
- 157 D. Iannazzo, A. Pistone, S. Ferro, L. De Luca, A. M. Monforte, R. Romeo, M. R. Buemi and C. Pannecouque, *Bioconjugate Chem.*, 2018, **29**, 3084–3093.
- 158 S. Basak and G. Packirisamy, *Nano-Struct. Nano-Objects*, 2020, **24**, 100620.
- 159 T. Du, J. Liang, N. Dong, L. Liu, L. Fang, S. Xiao and H. Han, *Carbon*, 2016, **110**, 278–285.
- 160 H. Liu, Y. Bai, Y. Zhou, C. Feng, L. Liu, L. Fang, J. Liang and S. Xiao, *RSC Adv.*, 2017, **7**, 28016–28023.
- 161 S. Manivannan and K. Ponnuchamy, *Appl. Organomet. Chem.*, 2020, **34**, e5887.



- 162 E. Ratemi, *Stimuli Responsive Polymeric Nanocarriers for Drug Delivery Applications*, 2018, vol. 1, pp. 121–141.
- 163 S. Kumar, N. Dilbaghi, R. Saharan and G. Bhanjana, *Bionanoscience*, 2012, **2**, 227–250.
- 164 H. Cabral, K. Miyata, K. Osada and K. Kataoka, *Chem. Rev.*, 2018, **118**, 6844–6892.
- 165 K. Miyata, R. J. Christie and K. Kataoka, *React. Funct. Polym.*, 2011, **71**, 227–234.
- 166 Y. S. Ahn, H. J. Baik, B. R. Lee, E. S. Lee, K. T. Oh, D. H. Lee and Y. S. Youn, *Macromol. Res.*, 2010, **18**, 747–752.
- 167 H. Al-Lawati, H. M. Aliabadi, B. S. Makhmalzadeh and A. Lavasanifar, *Expert Opin. Drug Delivery*, 2018, **15**, 397–418.
- 168 Y. Yang, M. Yang, J. Yuan, F. Wang, Z. Wang, J. Li, M. Zhang, L. Xing, J. Wei, L. Peng, G. Wong, H. Zheng, W. Wu, C. Shen, M. Liao, K. Feng, J. Li, Q. Yang, J. Zhao, L. Liu and Y. Liu, *Innovation*, 2020, **1**, 100061.
- 169 Z. Feng, B. Diao, R. Wang, G. Wang, C. Wang, Y. Tan, L. Liu, C. Wang, Y. Liu and Y. Liu, *medRxiv*, 2020, preprint, DOI: [10.1101/2020.03.27.20045427](https://doi.org/10.1101/2020.03.27.20045427).
- 170 C. C. Leung, T. H. Lam and K. K. Cheng, *Lancet*, 2020, **395**, 945.
- 171 H. Zhong, Z. Zhu, J. Lin, C. F. Cheung, V. L. Lu, F. Yan, C.-Y. Chan and G. Li, *ACS Nano*, 2020, **14**, 6213–6221.
- 172 H. Zhong, Z. Zhu, P. You, J. Lin, C. F. Cheung, V. L. Lu, F. Yan, C.-Y. Chan and G. Li, *ACS Nano*, 2020, **14**, 8846–8854.
- 173 M.-G. Kim, J. Y. Park, Y. Shon, G. Kim, G. Shim and Y.-K. Oh, *Asian J. Pharm. Sci.*, 2014, **9**, 227–235.
- 174 S. Misumi, M. Masuyama, N. Takamune, D. Nakayama, R. Mitsumata, H. Matsumoto, N. Urata, Y. Takahashi, A. Muneoka and T. Sukamoto, *J. Immunol.*, 2009, **182**, 6061–6070.
- 175 D. Raghuvanshi, V. Mishra, M. R. Suresh and K. Kaur, *Vaccine*, 2012, **30**, 7292–7299.
- 176 B. Lepenies, J. Lee and S. Sonkaria, *Adv. Drug Delivery Rev.*, 2013, **65**, 1271–1281.
- 177 J. M. Ball, D. Y. Graham, A. R. Opekun, M. A. Gilger, R. A. Guerrero and M. K. Estes, *Gastroenterology*, 1999, **117**, 40–48.
- 178 A. Geldmacher, D. Skrastina, G. Borisova, I. Petrovskis, D. H. Krüger, P. Pumpens and R. Ulrich, *Vaccine*, 2005, **23**, 3973–3983.
- 179 C. M. Coleman, Y. V. Liu, H. Mu, J. K. Taylor, M. Massare, D. C. Flyer, G. M. Glenn, G. E. Smith and M. B. Frieman, *Vaccine*, 2014, **32**, 3169–3174.
- 180 D. Sanchez-Guzman, P. Le Guen, B. Villeret, N. Sola, R. Le Borgne, A. Guyard, A. Kemmel, B. Crestani, J.-M. Sallenave and I. Garcia-Verdugo, *Biomaterials*, 2019, **217**, 119308.
- 181 H. Sekimukai, N. Iwata-Yoshikawa, S. Fukushi, H. Tani, M. Kataoka, T. Suzuki, H. Hasegawa, K. Niikura, K. Arai and N. Nagata, *Microbiol. Immunol.*, 2020, **64**, 33–51.
- 182 W. H. Organisation, NIH Clinical Trial of Investigational Vaccine for COVID-19 Begins., <https://www.niaid.nih.gov/news-events/nih-clinical-trial-investigational-vaccine-covid-19-begins> (accessed 2020-05-05).
- 183 W. H. Organisation, Draft Landscape of COVID-19 Candidate Vaccines, <https://www.who.int/who-documents-detail/draft-landscape-of-covid-19-candidate-vaccines>, (accessed 2020-05-22, 2020).
- 184 L. Du, Y. Yang, X. Zhang and F. Li, *Nanoscale*, 2022, **14**, 1054–1074.
- 185 F. Amanat and F. Krammer, *Immunity*, 2020, **52**, 583–589.
- 186 B. Li, X. Zhang and Y. Dong, *Wiley Interdiscip. Rev.: Nanomed. Nanobiotechnol.*, 2019, **11**, e1530.
- 187 W. Tao, B. L. Hurst, A. K. Shakya, M. J. Uddin, R. S. Ingrole, M. Hernandez-Sanabria, R. P. Arya, L. Bimler, S. Paust and E. B. Tarbet, *Antiviral Res.*, 2017, **141**, 62–72.
- 188 C. Keech, G. Albert, I. Cho, A. Robertson, P. Reed, S. Neal, J. S. Plested, M. Zhu, S. Cloney-Clark and H. Zhou, *N. Engl. J. Med.*, 2020, **383**, 2320–2332.
- 189 Novavax, Novavax COVID-19 Vaccine Demonstrates 89.3% Efficacy in UK Phase 3 Trial, [https://ir.novavax.com/2021-01-28-Novavax-COVID-19-Vaccine-Demonstrates-89-3-Efficacy-in-UK-Phase-3-Trial#:~:text=\(Nasdaq%3A%20NVAX\)%2C%20a,the%20United%20Kingdom%20\(%20UK%20\)](https://ir.novavax.com/2021-01-28-Novavax-COVID-19-Vaccine-Demonstrates-89-3-Efficacy-in-UK-Phase-3-Trial#:~:text=(Nasdaq%3A%20NVAX)%2C%20a,the%20United%20Kingdom%20(%20UK%20)). (accessed 08.09.2022, 2022).
- 190 Y. Li, R. Tenchov, J. Smoot, C. Liu, S. Watkins and Q. Zhou, *ACS Cent. Sci.*, 2021, **7**, 512–533.
- 191 SpyBiotech, SpyBiotech and Serum Institute of India announce that the first subjects have been dosed in a Phase I/II trial of a novel virus-like particle vaccine targeting COVID-19, <https://www.globenewswire.com/news-release/2020/09/08/2089755/0/en/SpyBiotech-and-Serum-Institute-of-India-announce-that-the-first-subjects-have-been-dosed-in-a-Phase-I-II-trial-of-a-novel-virus-like-particle-vaccine-targeting-COVID-19.html>, (accessed 08.09.2022, 2022).
- 192 INO-4800, INO-4800 COVID-19 Vaccine, <https://www.precisionvaccinations.com/vaccines/ino-4800-covid-19-vaccine>, (accessed 08.09.2022, 2022).
- 193 I. AnGes, Phase II/III Study of COVID-19 DNA Vaccine (AG0302-COVID19), <https://clinicaltrials.gov/ct2/show/NCT04655625>.
- 194 ZyCoV-D, ZyCoV-D COVID-19 Vaccine, <https://www.precisionvaccinations.com/vaccines/ino-4800-covid-19-vaccine>, (accessed 08.09.2022, 2022).
- 195 D. S. Patel, ZyCoV-D, the made-in-India Covid vaccine by Zydus Cadila, likely to hit markets in June, <https://theprint.in/health/zycov-d-the-made-in-india-covid-vaccine-by-zydus-cadila-likely-to-hit-markets-in-june/657272/>, (accessed 08.09.2022, 2022).
- 196 J. Y. Ahn, J. Lee, Y. S. Suh, Y. G. Song, Y.-J. Choi, K. H. Lee, S. H. Seo, M. Song, J.-W. Oh and M. Kim, *medRxiv*, 2021, preprint, DOI: [10.1101/2021.05.26.21257700](https://doi.org/10.1101/2021.05.26.21257700).
- 197 M. M. Silveira, G. M. S. G. Moreira and M. Mendonça, *Life Sci.*, 2021, **267**, 118919.
- 198 J. Y. Noh, H. W. Jeong, J. H. Kim and E.-C. Shin, *Nat. Rev. Immunol.*, 2021, **21**, 687–688.
- 199 ClinicalTrials.gov., The Safety and Immunogenicity of a DNA-based Vaccine (COVIGEN) in Healthy Volunteers (COVALIA), <https://clinicaltrials.gov/ct2/show/NCT04742842>.
- 200 Takis and Rottapharm Biotech announce favourable preliminary results from the phase I clinical trial of COVID-eVax, a DNA-based vaccine candidate against COVID-19, <https://www.rottopharmbiotech.com/07-september-2021-press-release/> (accessed 2022-09-09).



- 201 B.-S. Shim, S.-M. Park, J.-S. Quan, D. Jere, H. Chu, M. K. Song, D. W. Kim, Y.-S. Jang, M.-S. Yang and S. H. Han, *BMC Immunol.*, 2010, **11**, 1–9.
- 202 N.-N. Zhang, X.-F. Li, Y.-Q. Deng, H. Zhao, Y.-J. Huang, G. Yang, W.-J. Huang, P. Gao, C. Zhou and R.-R. Zhang, *Cell*, 2020, **182**, 1271–1283.e1216.
- 203 C. B. Jackson, M. Farzan, B. Chen and H. Choe, *Nat. Rev. Mol. Cell Biol.*, 2022, **23**, 3–20.
- 204 R. W. Chan, S. Liu, J. Y. Cheung, J. G. Tsun, K. C. Chan, K. Y. Chan, G. P. Fung, A. M. Li and H. S. Lam, *Front. Immunol.*, 2021, 4169.
- 205 W. H. Organization, Interim recommendations for use of the Pfizer–BioNTech COVID-19 vaccine, BNT162b2, under emergency use listing: interim guidance, first issued 8 January 2021, updated 15 June 2021, updated 19 November 2021, World Health Organization, 2021.
- 206 W. H. Organization, Interim recommendations for use of the Moderna mRNA-1273 vaccine against COVID-19: interim guidance, first issued 25 January 2021, updated 15 June 2021, updated 19 November 2021, updated 23 February 2022, World Health Organization, 2022.
- 207 P. SARS-CoV, Variants_of_Concern_VOC_Technical_Briefing_12_England. pdf.
- 208 W. H. Organization, *Background document on the Janssen Ad26. COV2. S (COVID-19) vaccine: background document to the WHO Interim recommendations for use of Ad26. COV2. S (COVID-19) vaccine, 17 March 2021*, World Health Organization, 2021.
- 209 E. Yasinski, COVID-19 Vaccine Side Effect Tracker, <https://medshadow.org/covid19-vaccine-side-effects-2/#gameleya>.
- 210 D. Y. Logunov, I. V. Dolzhikova, D. V. Shcheblyakov, A. I. Tukhvatulin, O. V. Zubkova, A. S. Dzharullaeva, A. V. Kovyrshina, N. L. Lubenets, D. M. Grousova and A. S. Erokhova, *Lancet*, 2021, **397**, 671–681.
- 211 A. Hasanzadeh, M. Alamdaran, S. Ahmadi, H. Nourizadeh, M. A. Bagherzadeh, M. A. M. Jahromi, P. Simon, M. Karimi and M. R. Hamblin, *J. Controlled Release*, 2021, **336**, 354–374.
- 212 D. Vasireddy, P. Atluri, S. V. Malayala, R. Vanaparthy and G. Mohan, *J. Clin. Med. Res.*, 2021, **13**, 204.
- 213 R. M. Burckhardt, J. J. Dennehy, L. L. Poon, L. J. Saif and L. W. Enquist, *J. Virol.*, 2022, **96**, e01973.
- 214 M. Doerflinger, W. Forsyth, G. Ebert, M. Pellegrini and M. Herold, *Cell. Microbiol.*, 2017, **19**, e12693.
- 215 C. Lee, *Molecules*, 2019, **24**, 1349.
- 216 J. D. Finn, A. R. Smith, M. C. Patel, L. Shaw, M. R. Youniss, J. van Heteren, T. Dirstine, C. Ciullo, R. Lescarbeau and J. Seitzer, *Cell Rep.*, 2018, **22**, 2227–2235.
- 217 O. O. Abudayeh, J. S. Gootenberg, P. Essletzbichler, S. Han, J. Joung, J. J. Belanto, V. Verdine, D. B. Cox, M. J. Kellner and A. Regev, *Nature*, 2017, **550**, 280–284.
- 218 T. M. Nguyen, Y. Zhang and P. P. Pandolfi, *Cell Res.*, 2020, **30**, 189–190.
- 219 C. Xu, Y. Zhou, Q. Xiao, B. He, G. Geng, Z. Wang, B. Cao, X. Wang, D. Zhou and T. Yuan, *Research Square*, 2020, DOI: [10.21203/rs.3.rs-30924/v1](https://doi.org/10.21203/rs.3.rs-30924/v1).
- 220 I. Kraja, R. Bing, N. Hiwatashi, B. Rousseau, D. Nalband, K. Kirshenbaum and R. C. Branski, *Laryngoscope*, 2017, **127**, E231–E237.
- 221 M. Burmistrz, K. Krakowski and A. Krawczyk-Balska, *Int. J. Mol. Sci.*, 2020, **21**, 1122.
- 222 R. Romeo, C. Carnovale, S. V. Giofrè, M. A. Chiacchio, A. Garozzo, E. Amata, G. Romeo and U. Chiacchio, *Beilstein J. Org. Chem.*, 2015, **11**, 328–334.
- 223 D. D. Richman, D. M. Margolis, M. Delaney, W. C. Greene, D. Hazuda and R. J. Pomerantz, *Science*, 2009, **323**, 1304–1307.
- 224 J. Szebeni, S. M. Wahl, G. V. Betageri, L. M. Wahl, S. Gartner, M. Popovic, R. J. Parker, C. D. Black and J. N. Weinstein, *AIDS Res. Hum. Retroviruses*, 1990, **6**, 691–702.
- 225 T. Dutta, M. Garg and N. K. Jain, *Eur. J. Pharm. Sci.*, 2008, **34**, 181–189.
- 226 A. Haque and A. B. Pant, *J. Autoimmun.*, 2022, **127**, 102792.
- 227 T. G. Flower, C. Z. Buffalo, R. M. Hooy, M. Allaire, X. Ren and J. H. Hurley, *Proc. Natl. Acad. Sci. U. S. A.*, 2021, **118**, e2021785118.
- 228 J. Shastri, S. Parikh, V. Aggarwal, S. Agrawal, N. Chatterjee, R. Shah, P. Devi, P. Mehta and R. Pandey, *Front. Med.*, 2021, 1379.
- 229 K. K. Riemersma, L. A. Haddock III, N. A. Wilson, N. Minor, J. Eickhoff, B. E. Grogan, A. Kita-Yarbro, P. J. Halfmann, H. E. Segaloff, A. Kocharian, K. R. Florek, R. Westergaard, A. Bateman, G. E. Jeppson, Y. Kawaoka, D. H. O'Connor, T. C. Friedrich and K. M. Grande, *PLoS Pathog.*, 2022, **18**(9), e1010876.
- 230 J. P. Moore and P. A. Offit, *Jama*, 2021, **325**, 821–822.
- 231 H. Kawasuji, Y. Takegoshi, M. Kaneda, A. Ueno, Y. Miyajima, K. Kawago, Y. Fukui, Y. Yoshida, M. Kimura and H. Yamada, *PLoS One*, 2020, **15**, e0243597.
- 232 K. Sharma, A. Koirala, K. Nicolopoulos, C. Chiu, N. Wood and P. N. Britton, *Paediatr. Respir. Rev.*, 2021, **39**, 22–31.
- 233 S. R. Kannan, A. N. Spratt, A. R. Cohen, S. H. Naqvi, H. S. Chand, T. P. Quinn, C. L. Lorson, S. N. Byrareddy and K. Singh, *J. Autoimmun.*, 2021, **124**, 102715.
- 234 W. H. Organization, World Health Organization, <https://www.who.int/news/item/28-11-2021-update-on-omicron>, 2021.
- 235 O. J. Wouters, K. C. Shadlen, M. Salcher-Konrad, A. J. Pollard, H. J. Larson, Y. Teerawattananon and M. Jit, *Lancet*, 2021, **397**, 1023–1034.
- 236 M. Chan, *Braz. J. Implantol. Health Sci.*, 2022, **4**, 50–54.
- 237 N. Subbaraman, *Nature*, 2021, **596**, 327–328.
- 238 P. A. Christensen, R. J. Olsen, S. W. Long, S. Subedi, J. J. Davis, P. Hodjat, D. R. Walley, J. C. Kinskey, M. O. Saavedra and L. Pruitt, *Am. J. Pathol.*, 2022, **192**, 320–331.
- 239 P. Y. Chia, S. W. X. Ong, C. J. Chiew, L. W. Ang, J.-M. Chavatte, T.-M. Mak, L. Cui, S. Kalimuddin, W. N. Chia and C. W. Tan, *Clin. Microbiol. Infect.*, 2022, **28**, 612.e611–612.e617.
- 240 S. Yuan, S.-C. Jiang and Z.-L. Li, *Front. Public Health*, 2020, **8**, 240.
- 241 A. Bal, G. Destras, A. Gaymard, K. Stefic, J. Marlet, S. Eymieux, H. Regue, Q. Semanas, C. d'Aubarede and G. Billaud, *Euro-surveillance*, 2021, **26**, 2100008.

