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Recent advances in therapeutic engineered extracellular vesicles

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Extracellular vesicles (EVs) are natural particles secreted by living cells, which hold significant potential for various therapeutic applications. Native EVs have specific components and structures, allowing them to cross biological barriers, and circulate *in vivo* for a long time. Native EVs have also been bioengineered to enhance their therapeutic efficacy and targeting affinity. Recently, the therapeutic potential of surface-engineered EVs has been explored in the treatment of tumors, autoimmune diseases, infections and other diseases by ongoing research and clinical trials. In this review, we will introduce the modified methods of engineered EVs, summarize the application of engineered EVs in preclinical and clinical trials, and discuss the opportunities and challenges for the clinical translation of surface-engineered EVs.

1. Introduction

Extracellular vesicles (EVs), small particles derived from cells, were first discovered in the 1980s, when they were regarded as cell dust.¹ Subsequently, researchers investigated the structures and biological functions of EVs in intracellular communication and the transport of various biomolecules, including RNAs, pro-

teins, and lipids, to recipient cells or tissues.^{2,3} In the 2010s, scientists gained a better understanding of the preparation, isolation and functions of EVs, particularly in the fields of cancer treatment and immunology, revealing their critical roles in immune responses and tumor development.^{4,5} In recent years, scientists further developed EVs as cell-free therapeutics for drug delivery, immunomodulation, and therapy. EV-based therapies offer the potential for scalable production, improved storage and transport, reduced adverse effects, and overcoming the biological barriers due to their nanosize.^{6,7}

The surface engineering of extracellular vesicles could achieve many additional goals. One dominating purpose is to endow EVs with targeting affinity. Even though some EVs have been reported to intrinsically target specific cells, previous literature has revealed that it is insufficient to achieve accumulation *in vivo*.^{8,9} Another motivation for EV surface engineering is the introduction of therapeutic molecules. Compared with loading drugs, especially for large molecules, modification on the surface may be more accessible. To achieve the above purposes, researchers have utilized mainly genetic and chemical methods to modify the surface of extracellular vesicles and apply these extracellular vesicles in different disease therapies.

2. Source of EVs

Compared with parental cells, EVs are reported to lack certain structural proteins, such as actin, but can inherit surface proteins and some secreted proteins from the mother cells.^{10,11} This inherent property simplifies the development of EVs for potential applications, eliminating the need for additional procedures to introduce specific proteins of interest. Moreover, multiple proteins may collectively contribute to specific func-

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tions of EVs, enhancing their efficacy in these roles.¹² However, EVs secreted from mother cells exhibit heterogeneity, resulting in variations in the abundance of proteins of interest among individual EVs. Furthermore, the quality of EVs is greatly influenced by the conditions of the mother cells. EVs can be derived from various cell types and sources, each of which may have specific characteristics and functions.

2.1. Blood cell-derived EVs

Extracellular vesicles derived from blood cells, including Red Blood Cells (RBCs) and platelets could be produced in an easier protocol, because of the lack of nuclei and composite organelles.^{13–17} Additionally, as RBCs and platelets are the most two abundant cells in the blood, the output of EVs of RBCs and PEVs could be produced on a large scale.¹⁸ However, as these blood cells cannot reproduce *in vitro*, it is difficult to insert interested genes into these EVs.

RBC-derived EVs are released during various physiological and pathological conditions, reflecting the state of their parent cells. These vesicles carry a cargo rich in proteins, lipids, and microRNAs, including cytoskeletal proteins and antioxidant enzymes, which are also widely utilized for drug delivery.¹⁶ Platelet-derived EVs are key players in hemostasis, thrombosis, and inflammation. Laden with platelet-specific molecules like glycoprotein IIb/IIIa and P-selectin, as well as bioactive molecules such as growth factors and cytokines, these EVs orchestrate various physiological responses.^{19,20}

2.2. Immune cell-derived EVs

Extracellular vesicles from immune cells, including macrophages,^{21–23} dendritic cells,^{24,25} and T cells,^{26,27} are also utilized in disease therapy because of their immunomodulation capacity. For instance, T cell-derived EVs carry surface markers and cytokines characteristic of T cell subtypes, facilitating antigen presentation, immune activation, and regulation.²⁸ B cell-derived EVs may contain immunoglobulins and antigens, participating in humoral immune responses and antibody-mediated immunity.^{29,30} Similarly, NK cell-derived EVs modulate target cell recognition and immune responses through the transfer of cytotoxic molecules and regulatory proteins.^{31,32}

Macrophages and dendritic cells, as key antigen-presenting cells, release EVs with significant immunomodulatory functions. These EVs carry antigen-presenting molecules such as MHC molecules and co-stimulatory molecules, facilitating antigen presentation and T cell activation.^{21,33} Furthermore, macrophage-derived EVs may contain inflammatory mediators such as cytokines and chemokines, regulating local immune responses and inflammation.³⁴ Dendritic cell-derived EVs play crucial roles in immune tolerance and suppression by promoting regulatory T cell differentiation and suppressing effector T cell responses.³⁵

2.3. Tumor-derived EVs

Tumor-derived EVs (TEXs) play crucial roles in various stages of cancer progression, including tumor growth, angiogenesis,

metastasis, immune evasion, and drug resistance. They facilitate intercellular communication by transferring oncogenic molecules, promoting tumor–stroma interactions, and modulating the behavior of recipient cells within the tumor micro-environment.⁵ TEXs have inherited specific surface proteins from tumor cells, leading to the tumor-targeting ability.³⁶ Moreover, TEXs have emerged as promising biomarkers for cancer diagnosis, prognosis, and treatment response prediction, offering non-invasive avenues for monitoring disease progression and guiding therapeutic interventions.³⁷

2.4. Stem cell-derived EVs

Extracellular vesicles derived from stem cells are also strong candidates for the next generation of drugs.^{38,39} These EVs play crucial roles in intercellular communication, tissue repair, immune modulation, and regeneration. They exert their effects by transferring regulatory molecules to recipient cells, influencing cellular processes such as proliferation, differentiation, apoptosis, and inflammation.⁴⁰ Stem cell-derived EVs offer several advantages over stem cell-based therapies, including reduced risk of tumorigenicity, immunogenicity, and ethical concerns associated with cell transplantation. MSC EVs have been reported to play a vital role in tissue repair,⁴¹ and therapeutics of COVID-19.⁴² That may contribute to the large scale of MSC reproduction.

2.5. Bacteria-derived EVs

Outer membrane vesicles (OMVs) carry a variety of proteins from the parent bacterial cell surface, playing crucial roles in bacterial physiology, virulence, and host–pathogen interactions.⁴³ These proteins may include adhesins such as coagulase, adhesion factors, and lectins, facilitating bacterial attachment to host cell surfaces and establishment of infection.^{44,45} Additionally, OMVs may harbor virulence factors such as toxins, lytic enzymes, and lipopolysaccharides (LPSs), which, when released into host cells *via* OMVs, can induce cell damage and inflammation, and promote pathogen invasion and disease progression. OMVs, especially from *E. coli*, are utilized in tumor therapy, as LPSs on the surface of OMVs are immunomodulators to activate an immune response.^{46,47}

2.6. Plant-derived EVs

Plant EVs play crucial roles in regulating plant growth and development, responding to stress, and mediating intercellular communication. They are released from various cellular compartments such as chloroplasts, mitochondria, endoplasmic reticulum, and Golgi apparatus into the extracellular space, facilitating long-distance communication within and outside the plant organism and influencing the physiological and metabolic states of recipient cells.^{48,49} Moreover, plant EVs are strong candidates for the next generation of drug delivery systems because of the high output of nanovesicles.^{50,51}

2.7. Isolation methods of EVs

Various methods exist for isolating EVs from complex biological samples. These methods include ultracentrifugation, size

exclusion chromatography, ultrafiltration, immunoaffinity capture, precipitation, and microfluidic devices.^{52,53} Each method has its advantages and limitations, and the choice depends on factors such as sample type, desired purity, yield, and downstream applications. Integration of multiple isolation techniques often enhances the purity and yield of isolated EVs, facilitating their functional characterization and enabling their use in research and clinical settings.

3. Surface engineering strategies on EVs

Researchers are trying to introduce interesting peptides or other molecules on the surface of EVs to broaden the applications of EVs. Some molecules including aptamers, nanobodies, or specific cell-targeted peptides could endow EVs with targeted capacity, solving the off-target problem. Some molecules like maleimide can capture antigens after being modified on the surface of EVs, boosting the immune response through interactions with antigen-presenting cells. Other molecules such as SIRP- α and aPD-L1 could modulate the immune microenvironment of tumor sites, enhancing the therapeutic efficacy of EVs. To modify EVs with these molecules, the most two common strategies are genetic modification and chemical modification (Fig. 1).

3.1. Genetic modification on EVs

To fuse the interested proteins on the membranes of EVs, researchers introduce the target gene through plasmid or lentivirus into the parental cells, inverting the target gene into the gene of parental cells. Then, EVs secreted by these cells will carry these proteins. Typically, the interested protein is fused with specific membrane surface proteins of the parent cells, such as Lamp2b, CD63, and CD9. For example, Wang *et al.* ligated a cardiomyocyte specific peptide (CMP) to the extra-exo-

somal N-terminus of Lamp2b on cardiosphere-derived cells.⁵⁴ Additionally, Scott *et al.* fused CD63 of HEK293T cells with an anti-CoV-2 nanobody to neutralize SARS-CoV-2 *in vitro*.⁵⁵ Kim and colleagues also truncated CD9 to display SACE-2 variants on the surface of extracellular vesicles.⁵⁶ This fusion allows these proteins to effectively localize to the surface of EVs. The choice of fusion protein depends on specific application requirements.

Gene modification techniques offer robust tools for engineering EVs and can be used to achieve various purposes, including targeted delivery, imaging and therapeutics. In detail, by introducing specific targeting proteins, EVs can selectively deliver their cargo to specific cells or tissues, enabling efficient targeted therapy. For instance, IL-3 was introduced into EVs derived from HEK293 cells to enhance the binding affinity of EVs in Chronic Myeloid Leukemia (CML) blasts, where IL-3 receptors were overexpressed.⁵⁷ The fusion of fluorescent or other imaging-labeled proteins to the surface of EVs also allows real-time tracking of EV distribution and delivery *in vivo*.

Through the incorporation of therapeutic proteins or RNA, EVs can be engineered into effective drug carriers for the treatment of conditions such as cancer, infections, and various diseases. For example, EV overexpressed SIRP- α could increase cancer cell phagocytosis, boosting the immune response.⁵⁸

3.2. Chemical modification on the surface of EVs

Unlike genetic modifications which usually display proteins on EVs, modifications based on chemical methods could display peptides or other molecules on EVs.⁵⁹ Chemical modification strategies can be categorized into two distinct approaches based on the timing of the modifications: pre-isolation modifications and post-isolation modifications. Chemical modifications encompass several techniques, including electrostatic incorporation, click chemistry and covalent conjugation. As the membrane surface of the cells is negatively charged, the positively charged molecules could simply absorb on the surface by electrostatic incorporation. For instance, Qin and colleagues displayed positive tumor antigens on the surface of OMVs through electrostatic incorporation.⁶⁰

Additionally, click chemistry also plays a crucial role in the modification of extracellular vesicles (EVs). Click chemistry is typically an efficient method that allows for rapid surface modification of EVs.^{61,62} It could also be used to introduce a wide range of molecular modifications, such as drugs, targeting molecules, and fluorescent labels. Both fluorescent dyes and targeting peptides conjugated with azide groups could simply modify the NHS-engineered EV surface by click chemistry.⁶³

Moreover, covalent conjugation is another widely utilized technique for tailoring EVs' surface properties, offering several key advantages. This approach involves the attachment of various molecules to the EV surface through covalent bonds, resulting in a functionalized EV platform. For instance, DSPE-PEG, phospholipid-polyethylene glycol, could typically react with hydroxyl or amine groups on the surface of membranes,



Fig. 1 Schematic diagram of surface-engineered extracellular vesicles.

to form covalent bonds. Wang *et al.* functionalized targeting peptides with DSPE-PEG and modified them on the surface of donor cells.⁶⁴ The advantages of covalent conjugation include: (1) robust stability to the modified EVs, preventing the detachment of surface molecules and ensuring their persistence during storage and circulation in biological environments; (2) fine control over the degree and nature of modification, tailoring EVs to meet diverse research and clinical needs; and (3) minimizing non-specific protein adsorption to EV surfaces, maintaining their purity.

These chemical modification strategies can be utilized to endow EVs with specific functionalities, such as targeted drug delivery, real-time imaging, and therapeutic capabilities. For instance, cardiac homing peptides were conjugated on the surface of EVs, endowing EVs with affinity towards the infarcted hearts.⁶⁵ The insertion of fluorescent molecules labeled on the surface of EVs also helps to identify the location of the infarction.⁶⁶

3.3. Physical modification on the surface of EVs

Physical modification strategies offer versatile approaches for surface engineering of extracellular vesicles (EVs), enabling precise control over their surface properties and functionalities.^{67,68} These strategies involve the manipulation of EVs through physical means without directly altering their genetic or biochemical compositions.

One common physical modification strategy is membrane permeabilization, which involves techniques such as sonication, freeze-thaw cycles, or electroporation. These methods disrupt the integrity of the EV membrane, allowing for the insertion or attachment of exogenous molecules onto the EV surface.⁶⁹ This enables the introduction of targeting ligands, therapeutic agents, or imaging probes onto EVs, thereby enhancing their targeting specificity or therapeutic efficacy. Rayamajhi *et al.* hybridized macrophage-derived EVs with gadolinium-infused liposomes using sonication and membrane extrusion, achieving magnetic resonance imaging.⁷⁰

Another physical modification approach is membrane fusion, where EVs are fused with liposomes or synthetic nanoparticles carrying desired surface modifications.⁶⁷ This enables the transfer of surface proteins, lipids, or other molecules from the synthetic carriers to EVs, leading to the engineering of EVs with customized surface functionalities. Li *et al.* modified MSC EVs with platelet membranes based on extrusion, endowing EVs with the binding ability to monocytes.⁷¹ This strategy successfully targeted the infarcted heart and realized cardiac repair.

3.4. Metabolic engineering on the surface of EVs

Metabolic engineering strategies involve manipulating the cellular metabolism of EV-producing cells to modulate the biosynthesis and incorporation of specific molecules into EV membranes. One approach is to engineer donor cells to overexpress or knockdown genes involved in lipid metabolism, such as enzymes responsible for lipid synthesis or modification.⁷² This can lead to the production of EVs with altered lipid com-

positions, which in turn influence their surface properties and interactions with target cells or tissues.

Another metabolic engineering strategy involves the modulation of glycosylation pathways in donor cells to control the glycosylation patterns on EV surfaces.⁶⁷ Glycosylation plays crucial roles in EV biogenesis, cargo sorting, and intercellular communication, making it an attractive target for surface engineering.⁷³ By manipulating the expression of glycosyltransferases or glycosidases, researchers can engineer EVs with specific glycan structures on their surfaces, which can modulate their targeting, uptake, and immunogenicity profiles. For instance, Lim *et al.* modified EVs with an exogenous azide group based on metabolic glycoengineering to enhance the targeting affinity of EVs towards target tissues.⁷⁴

3.5. Lipid-based engineering on the surface of EVs

Lipid-based engineering strategies involve the manipulation of lipid composition and structure on the EV surface. One common approach is lipid insertion or incorporation, where lipids with desired functionalities, such as targeting ligands or therapeutic molecules, are inserted into the EV membrane.⁷⁵ This can be achieved through various techniques, including membrane fusion, incubation with lipid-modified molecules, and extrusion through lipid bilayers. For instance, Jhan *et al.* fused EVs with synthetic lipids to realize highly efficient gene delivery.⁶⁸ Lipid exchange is another strategy, where the native lipids of EVs are replaced with synthetic or modified lipids carrying specific functionalities.⁷⁶ This can be accomplished using methods such as solvent-based lipid exchange or membrane extrusion. Additionally, lipid conjugation involves the covalent attachment of molecules of interest, such as targeting ligands or imaging agents, to lipid molecules, which are then incorporated into the EV membrane.⁷⁵ The choice of different modification techniques depends on the specific goals of the study and the intended applications. Overall, chemical modifications of EVs provide a versatile toolkit for tailoring these vesicles to meet various research and clinical needs.

4. EVs for different disease therapy and clinical translation

4.1. Engineered EVs for cancer therapy

The therapeutic potential of EVs for tumors has been evaluated in recent years with encouraging outcomes. Drug delivery systems and tumor vaccines based on EVs could inhibit tumor growth in pre-clinical trials.^{77–81} Compared with their parent cells, EVs have lower immunogenicity and cytotoxicity. When loading drugs on EVs, these natural nanoscale carriers could enhance the targeting ability, and prolong the circulation time compared with free drugs. Researchers have also modified the surface of EVs derived from various cells and utilized engineered EVs for targeted therapy and immunotherapy (Table 1).

4.1.1. Surface-engineered EVs for targeted therapy. Even though extracellular vesicles have been utilized as drug delivery carriers in tumors, some EVs lack tumor-targeted capacity

Table 1 The summary of surface-engineered EVs for cancer therapy

Therapy	Parent cells	Surface engineering	Outcomes	Ref.
Targeted therapy	MPA-MB-231; HCT-116	PHA	Enhanced binding affinity of EVs	74
Targeted therapy	MSCs	Targeting peptides	Improved uptake of EVs	83
Targeted therapy	Neuro2A	Anti-EGFR nanobodies		88
Targeted therapy	HEK293T	IL-3	Enhanced targeting ability	57
Targeted therapy	HEK293T	CDH17nanobody	Targeted delivery of drugs	90
Targeted therapy	imDCs	iRGD	Enhanced binding ability	85
Targeted therapy	Grapefruits	Aptamers	Enhanced targeting ability	91
Immunotherapy	4T1; B16F10	SIRP- α and PD-1	Boosting multi-targeted ICB therapy	98
Immunotherapy	HEK293T	PD-1	Boosting anti-tumor immunity	99
Immunotherapy	HEK293T	SIRP- α	Increased cancer cell phagocytosis	58
Immunotherapy	HEK293T	CD64	Carrying aPD-L1; introducing ICB therapy	100
Immunotherapy	HEK293T	aPD-L1	Strengthen ICB therapy	131
Immunotherapy	Jurkat T	IL-2	Improving anti-cancer efficacy	132
Immunotherapy	CAR-T	Gene engineering	Potent antitumor effects and low toxicity	133
Immunotherapy	imDCs	aPD-L1	Introducing ICB therapy	103
Immunotherapy	DC2.4	Anti-CD19, PD-1	Targeting tumor cells; enhancing ICB therapy	104
Immunotherapy	<i>E. coli</i>	PD-1	Increasing anti-tumor efficacy	134
Immunotherapy	<i>E. coli</i>	TAAAs	Triggering potential antitumor immunity	60
Immunotherapy	<i>E. coli</i>	TAAAs	<i>In situ</i> controllable production of tumor antigens	107
Immunotherapy	<i>E. coli</i>	TAAAs	Display antigens	106
Immunotherapy	<i>E. coli</i>	Maleimide group	Capture of TAAAs	108
Immunotherapy	<i>E. coli</i>	Maleimide group	Capture of TAAAs after PTT	109

and the targeted capacity could partially be due to the surface characteristics. So, researchers modified the surface of EVs with targeted molecules, including PHA, targeting peptides, ScFv or aptamers to enhance the binding affinity of engineered EVs to the tumor site.

PEGylated hyaluronic acid (PHA) was reported to have strong affinity to CD44-overexpressing cells,⁸² which are usually utilized in the surface engineering of nanomaterials. Considering that the tumor site is also a CD44-abundant tissue, Lim *et al.* modified MDA-MB-231 cells and HCT-116 cells with PHA, based on biorthogonal copper-free click chemistry (BCC) and metabolic glycoengineering (MGE).⁷⁴ This strategy could successfully increase the tumor targeting of EVs derived from these two cell lines, as the fluorescence signal of PHA-EVs in the tumor site was about 2-fold higher than that of bare EVs.

Apart from targeted small molecules, targeted peptides are also utilized to enhance the targeting affinity of EVs. Sajeesh and colleagues have engineered adult human BM-MSCs with azide-modified cathepsin K-targeting peptide sequence based on copper-free click chemistry.⁸³ Cathepsin K is overexpressed in the wall of abdominal aortic aneurysm (AAA).⁸⁴ The cellular uptake of EVs increased sharply after the medication. The *ex vivo* binding of engineered EVs was about 10 times higher than that of bare EVs, indicating enhanced binding affinity of EVs towards the tumor site.⁸³ Tian *et al.* modified immature DCs with the iRGD targeting peptide and isolated EVs from engineered cells.⁸⁵ These EVs were loaded with doxorubicin *via* electroporation, which could enhance tumor binding affinity by about 3 times, compared with unmodified EVs. This strategy could inhibit MDA-MB-231 tumor growth and reduce cardiac damage compared with free DOX.

Single-chain variable antibodies (scFv) have significant applications in achieving tumor-targeting of EVs as they could

bind with specific tumor-associated antigens. Human Epidermal Growth Factor Receptor 2 (HER2) is a membrane-bound receptor protein, which has become an important target in breast cancer.⁸⁶ Longatti and colleagues transfected HEK293 cells with the vector of anti-Her2-scFv and confirmed the high affinity of the engineered exosomes to HER2-positive cells.⁸⁷ The epidermal growth factor receptor (EGFR) is another target of some tumor cells, which is overexpressed on tumor cells. Kooijmans *et al.* modified Neuro2A cell lines with anti-EGFR nanobodies and collected EVs derived from these cells, evaluating their association with tumor cells.⁸⁸ This Cadherin 17 (CDH17) is reported as one of the most upregulated genes in gastric cancers (GC).⁸⁹ Hence Xia *et al.* developed a delivery platform based on EVs from HEK293 cells modified with CDH17 nanobodies to deliver imaging probes and other drugs.⁹⁰ This smart strategy was confirmed to accumulate more than three times in the tumor site compared with unmodified EVs, showing higher therapeutic efficacy in GC mouse models.

The above-mentioned EVs are derived from animal cells. Plant-derived extracellular vesicles, however, could be produced with mass production, and after simple modification, they could also be endowed with high affinity.⁵⁰ Moon *et al.* engineered EVs derived from grapefruits with a targeted aptamer.⁹¹ These engineered EVs could have 3 times higher affinity towards blood-brain barrier endothelial cells, compared with unmodified EVs, indicating their potential in targeting brain tumors.

4.1.2. Surface-engineered EVs for immunotherapy. In the tumor microenvironment, there are various tumor-infiltrating immune cells, including tumor-associated macrophages, T cells and dendritic cells.⁹² Enhancing the immune response towards cancer cells has become a revolutionary strategy to treat cancers.^{93,94} However, various mechanisms have been

reported to suppress this immune response toward cancer.^{95–97} Therefore, drugs to modulate immune cells have been investigated, such as immune checkpoint inhibitors or other activators/inhibitors towards specific immune cells. Considering the huge side effects of the above drugs, researchers began to modify extracellular vesicles, derived from various cells, such as tumor cells, HEK293 cells, and DCs with these molecules, boosting the immune response toward tumors.

Extracellular vesicles derived from tumor cells (TEXs) offer advantages in tumor immunotherapy, including their natural antigen presentation, immune stimulation, targeting capabilities, drug delivery potential, and immune monitoring ability. These attributes make TEXs a promising tool for enhancing immune therapy and improving immune responses. To further enhance the effectiveness of tumor treatment, SIRP α was edited on the surface of breast cancer cells and carried on the extracellular vesicles derived from these cancer cells.⁹⁸ SIRP α

EVs were fused with PD-1 EVs, boosting both the innate immune response and the adaptive immune response towards tumors (Fig. 2A). Consequently, these fused EVs could successfully inhibit tumor growth and protect the mice from tumor recurrence and metastasis.

HEK293 (Human Embryonic Kidney 293) cells are widely utilized EV-producers in tumor immunotherapy. For example, Koh *et al.* developed exosomes derived from HEK293 cells over-expressing SIRP α on the surface to intervene in the CD47–SIRP α axis.⁵⁸ These SIRP α -EVs could enhance the phagocytosis of bone marrow-derived macrophages *in vitro* two times compared with unmodified EVs. *In vivo* experiments, SIRP α EVs could selectively target tumor sites, further inhibiting the tumor growth significantly, even compared with CD47 antibody. Additionally, Li and colleagues modified HEK293 cells with the overexpression of PD-1 and utilized PD-1-EVs to treat cancers.⁹⁹ These PD-1-EVs could induce apoptosis of tumor

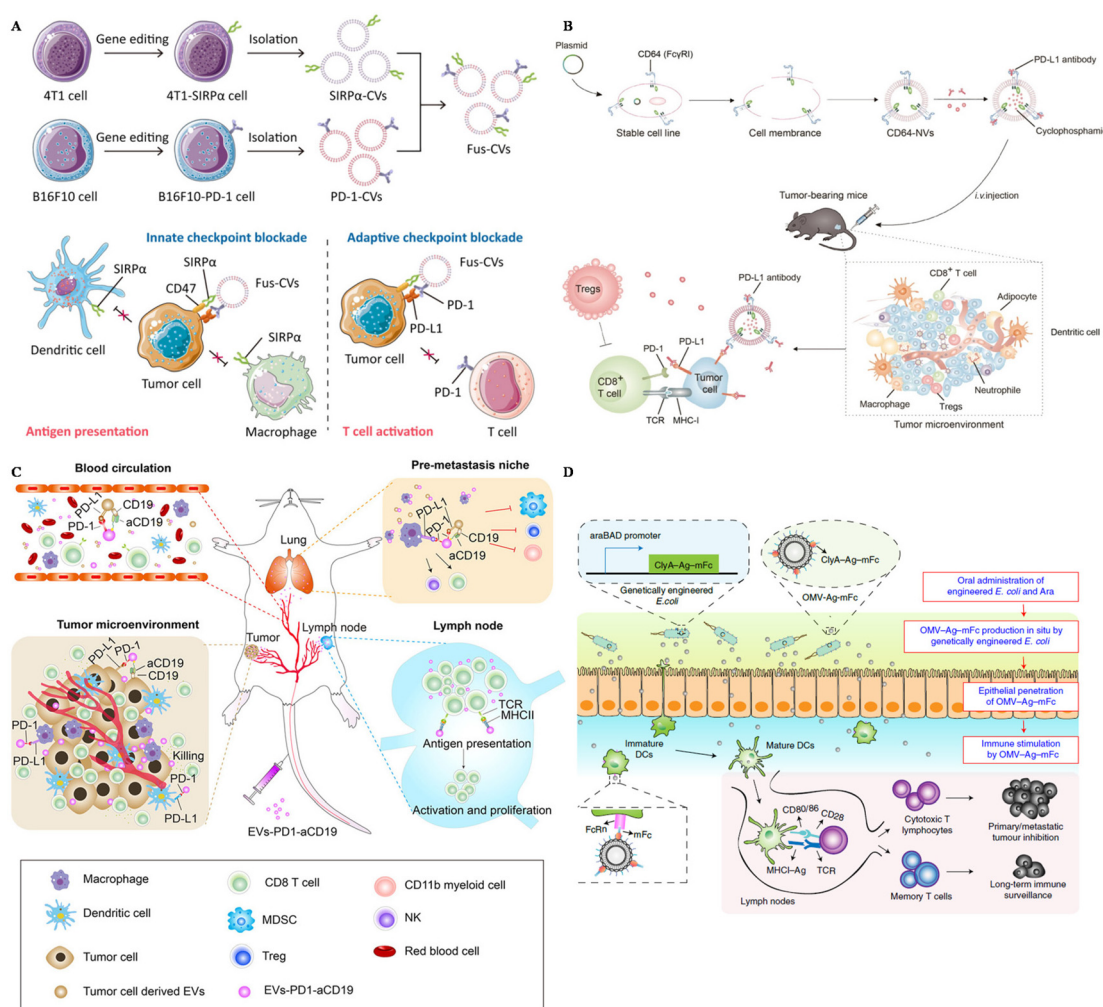


Fig. 2 The design of surface-engineered EVs for tumor therapy. (A) The preparation of multi-targeted extracellular vesicles.⁹⁸ Reproduced with permission. Copyright 2021, Wiley. (B) Scheme of the preparation of CD64-NVs-aPD-L1-CP and mechanisms.¹⁰⁰ Reproduced with permission. Copyright, 2021, Ivyspring International. (C) Scheme of the immune-boosting mechanism of EVs-PD-1-aCD19.¹⁰⁴ Reproduced with permission. Copyright, 2023, Elsevier. (D) Genetically engineered bacteria-derived-OMV-based oral tumor vaccine.¹⁰⁷ Reproduced with permission. Copyright, 2022, Springer.

cells *in vitro* via the expression of FasL and GramB. The antitumor efficacy of PD-1-EVs was even more significant compared with anti-PD-L1. To carry PD-L1 antibodies, Li *et al.* genetically engineered EVs from HEK293T cells with the display of CD64, working as a linker to catch antibodies (Fig. 2B).¹⁰⁰ This strategy could block PD-L1 of tumor cells *in vivo*, showing great therapeutic efficacy loaded with cyclophosphamide in the engineered EVs. Besides, Shi *et al.* transfected Expi 293 cells with α CD3 and α HER2 scFv, achieving dual targeting to T cells and breast cancer cells.¹⁰¹ These α CD3- α HER2-EVs could inhibit HER-2 expressing tumor growth and upregulate the percentage of T cells in the tumor site.

Apart from the primary investigation, HEK293 cells are also employed for the large-scale production of EVs. Their high proliferation rate and stability make them suitable for the mass production of EVs, meeting the quantity requirements for research and applications. Codiak Biosciences evaluated the therapeutic efficacy of intratumorally-administered HEK293-exosomes overexpressed PTGFRN on the surface to enhance the targeting delivery of the STING activator to antigen-presenting cells in solid tumors (NCT04592484). They also proposed to treat patients suffering from cutaneous T-cell lymphoma with HEK293-exosomes displayed IL-12 on the surface (NCT05156229). Moreover, Codiak Biosciences registered the use of HEK293-derived exosomes, the STAT6 anti-sense oligonucleotide (ASO) in tumor treatment. This strategy was proposed for the targeted delivery of drugs towards the myeloid, repolarizing macrophages from the immune suppressive M2 to the proinflammatory M1 phenotype (NCT05375604).

Dendritic cells (DCs) are professional antigen-presenting cells, originating mainly from bone marrow. They also play an important role in the anti-tumor immune response, as they can capture tumor-associated antigens, and process and present these antigens *via* MHC molecules, subsequently activating naïve T cells.¹⁰² Considering the complex interaction between DCs and other immune cells and the capacity to display antigens, EVs derived from DCs are also utilized in tumor immunotherapy. Dai *et al.* developed antigens including EVs derived from DCs and these EVs were also armed with aPD-L1, to prevent immune escape through the PD-1-PD-L1 axis.¹⁰³ This strategy could remarkably inhibit tumor growth and protect mice from tumor recurrence by boosting the immune response in the tumor site and lung tissues. To reprogram the immune microenvironment and enhance the tumor affinity, Xu and colleagues genetically engineered DC EVs with aCD19 and PD-1, loaded with TAAs and CPG (Fig. 2C).¹⁰⁴ This smart strategy could be used to interact with tumor cells, DCs, and macrophages because of the overexpression of PD-1, and modulate T cells due to MHCII and CD80 expressed on the surface of EVs. Engineered EVs were confirmed to accumulate more than four times compared with unmodified EVs. In general, these multifunctional EVs could reverse not only the immunosuppressive microenvironment *in situ*, but also the lung premetastatic niches in mouse models.

Outer membrane vesicles (OMVs) are secreted by most bacteria, containing a broad range of pathogen-associated mole-

cular patterns (PAMPs), regarded as ideal vaccine adjuvants as they could boost the innate immune response.¹⁰⁵ Because of this intrinsic characteristic, OMVs has become a candidate to display tumor-associated antigens (TAAs) to activate the immune response towards tumors. Qin *et al.* simply displayed TAAs on the surface of OMVs by electrostatic interactions.⁶⁰ This strategy could successfully elicit DC maturation and activation *in vitro* and further inhibit the metastasis of melanoma in mouse models with negligible toxicity. Moreover, Cheng and colleagues simplified the antigen display process with a plug-and-display system, and they modified the surface of OMVs with different antigen peptides.¹⁰⁶ Featuring different antigen peptides, these OMVs showed remarkable therapeutic efficacy in mouse melanoma and colorectal cancer models. They could also protect mice in the long term, with immune memory 80 days after the last vaccination, indicating the application potential of prophylactic vaccines. Apart from the preparation of OMVs *in vitro*, *in situ* produced OMVs could also boost the maturation of DCs. Yue *et al.* orally administered gene-engineered *E. coli* with TAAs (Fig. 2D).¹⁰⁷ This engineered *E. coli* could then produce OMVs with antigens in the intestine and OMVs could penetrate epithelial barriers, captured by DCs, followed by the rapid maturation of DCs. This strategy could also inhibit subcutaneous colorectal cancers, and elicit long-term immune memory in mouse models. Apart from directly displaying the antigens on the surface of OMVs, researchers also modified OMVs with the maleimide group to enhance the antigen capture capacity of DCs.^{108,109} Maleimide endows OMVs with high affinity to antigens, and after migration to the draining lymph nodes, OMV-Mal carried with TAAs could be taken up by immature DCs, boosting the maturation of DCs. OMVs modified with maleimide and loaded with 1-methyl-tryptophan (1-MT) could modulate both regulatory T cells and DCs after photothermal therapy.¹⁰⁹ 1-MT is an inhibitor of IDO, which could lead to a decrease of Treg, while the modification of the Mal group endows OMVs with carrying TAAs to DCs. This strategy could notably prolong the life span of tumor-bearing mice.

4.2. Engineered EVs for inflammatory disease therapy

Inflammatory diseases, including autoimmune diseases and infectious diseases, are disturbing people's health globally. Autoimmune diseases are usually related to uncontrollable immune responses, such as rheumatoid arthritis (RA), type I diabetes and ulcerative colitis.¹¹⁰ You *et al.* developed MSC EVs conjugated with dextran sulfate on the surface, achieving the targeted reprogramming macrophages in inflamed joints (Table 2).¹¹¹ An upregulated expression of PD-1 was confirmed in inflamed tissue in autoimmune patients.¹¹² To suppress the overwhelmed immune response and also increase the targeting affinity of EVs, the PD-1/L1 axis has been introduced into the treatment of autoimmune diseases. Becker modified a lymphoblast cell line, K562, with the expression of PD-L1 and utilized PD-L1 EVs to treat type I diabetes (Fig. 3A).¹¹³ This strategy could successfully suppress T cell activation *in vitro*, nearly

Table 2 The summary of surface-engineered EVs for autoimmune and infectious diseases

Diseases	Parent cells	Surface engineering	Outcomes	Ref.
I diabetes	K562	PD-L1	Suppressing T cell activation	113
Autoimmune diseases	MSCs	PD-L1	Reshaping the inflammatory ecosystem	114
RA	MSCs	Dextran sulfate	Reprogramming macrophages in inflammatory joints	111
COVID-19	HEK293	ACE-2 variants	Protecting K18-hACE-2 mice from infection	56
COVID-19	HEK293	ACE-2	Protecting mice from infection	115
COVID-19	HEK293	COVID-19 nanobody	Neutralizing SARS-CoV-2	55
COVID-19	MSCs	ACE-2	Inhibiting the infection of pseudovirus	116

the same level as healthy controls, further inducing the reduction of T cell cytotoxicity towards targeted cells *in vitro*.

Our group genetically engineered MSC EVs with the overexpression of PD-L1 and treat two autoimmune mouse models with MSC-EV-PD-L1 (Fig. 3B).¹¹⁴ *In vitro*, engineered EVs could bind with T cells, macrophages and dendritic cells, reverse the activation of T cells and BMDCs, and polarize macrophages towards M2 as well. In autoimmune mouse models, MSC-EV-PD-L1 could accumulate in the inflammatory colon and skin in ulcerative colitis and psoriasis, respectively. Furthermore, the excessive inflammation was relieved after the accumulation of engineered EVs, with a remarkable reduction of T cells and macrophages in the inflamed tissue, indicating the clinical potential of this strategy in the future.

Infectious diseases are usually caused by the infection of bacteria, fungi and viruses. SARS-CoV-2, a coronavirus that was first discovered in 2019, has led to millions of deaths all over the world. ACE-2, a protein that is expressed in some cells, has been regarded as a receptor for the spike protein of this virus, leading to further viral infection. Kim *et al.* engineered EVs to display ACE-2 variants on CD9 scaffolds (Fig. 3C).⁵⁶ ACE-2-EVs could inhibit the infection of wild-type viruses and delta variants in cell lines. Additionally, these EVs are also confirmed to protect mice expressing human ACE-2 from the viral infection, with a down-regulated proinflammatory response after treatment. Besides, Wu *et al.* developed ACE-2-engineered extracellular vesicles, protecting the infection of pseudovirus with the S protein in various cells *in vitro* and suppressing the entry of pseudovirus in the mouse model.¹¹⁵ Xie *et al.* also modified ACE-2 EVs, neutralizing the pseudovirus *in vitro* and block the infection of pseudovirus in the hACE2 mouse model.¹¹⁶ Moreover, Scott embedded an anti-CoV-2 nanobody in CD63, a widely expressed protein in EVs, to neutralize virus.⁵⁵ The results confirmed that EVs with the nanobody can successfully bind with the spike protein of SARS-CoV-2 and protect cells *in vitro*.

Surface-engineered extracellular vesicles derived from MSCs have been tested in clinical trials for the treatment of COVID-19 (Table 4). Tel-Aviv Sourasky Medical Center evaluated the biosafety of exosomes derived from MSCs and overexpressed CD24 in patients with either moderate or severe COVID-19 infection (NCT04747574). Eli Sprecher proposed to treat patients suffering from COVID-19 with exosomes overexpressed CD24 at a dose of 10^{10} daily for five days (NCT04969172). Other two medical societies also registered

the use of engineered MSC EVs with the overexpression of CD24 for phase II. Athens Medical Society proposed to treat SARS-CoV-2 positive patients with two doses of modified EVs, 10^9 and 10^{10} , respectively (NCT04902183). OBCTCD-24 Ltd registered to evaluate the safety and therapeutic efficacy of engineered MSC EVs (EUCTR2021-004259-17-GR).

4.3. Engineered EVs for the treatment of other diseases

Cardiovascular diseases are one of the leading causes of death in the world.¹¹⁷ Extracellular vesicles have been utilized in the therapy of cardiovascular diseases, due to the specific RNAs contained in EVs.¹¹⁸ However, the targeting ability of EVs has limited their further application. Therefore, to enhance the targeting capacity of MSC EVs, Li *et al.* modified EVs with platelet membranes (Table 3).⁷¹ With the expression of platelet specific proteins, like CD62P, EVs could bind with monocytes *in vitro* and target the infarcted hearts *in vivo*. Pei *et al.* also utilized a platelet membrane to improve the targeting ability of macrophage-derived EVs.¹¹⁹ Moreover, targeting peptides have been modified on the surface of blank EVs to improve their retention in specific tissues. For example, MSC EVs conjugated with the c(RGDyk) peptide, could cross the blood-brain barrier (BBB) and target the ischemic brain *via* intravenous injection.⁶³ MSC EVs could also target the ischemic heart after fusing with another targeting peptide. Besides, Wang *et al.* genetically modified MSCs with CD47 and developed their EVs for myocardial infarction reperfusion injury treatment.¹²⁰ With the expression of CD47, engineered EVs could accumulate 5 times in the heart, compared with unmodified EVs.

Apart from MSC EVs, cardiosphere-derived cells (CDCs) could also be utilized in the targeting treatment of cardiovascular diseases. Vandergriff *et al.* engineered CDC-EVs with a cardiac homing peptide, achieving increased retention of the exosomes (Fig. 4A).⁶⁵ Besides, Wang and colleagues engineered targeting EVs through a donor cell-assisted membrane modification, to increase the targeting affinity to blood cells.⁶⁴ Moreover, Mentkowski also modified CDCs with a cardiomyocyte-specific peptide (CMP) and isolated CMP-EVs for cardiomyocyte targeting (Fig. 4B).⁵⁴ CMP EVs could selectively bind with cardiomyocytes *in vitro*, with negligible binding affinity to cardiac fibroblasts and HUVECs *in vitro*. These EVs also showed enhanced uptake in the heart compared with blank EVs, indicating their therapeutic potential in the future.

Central nervous system (CNS) injuries including stroke, Parkinson's disease and Alzheimer's disease (AD) are disturbing



Fig. 3 The schematic of utilizing engineered EVs for inflammatory diseases. (A) The mechanism of EV-PD-L1 to induce cell killing of T cells. Reproduced with permission.¹¹³ Copyright 2023, the American Association for the Advancement of Science. (B) The schematic illustration of the preparation of PD-L1-MSC EVs and the immune boosting mechanism. Reproduced with permission.¹¹⁴ Copyright 2021, Wiley. (C) The schematic of utilizing engineered EVs for infection. Reproduced with permission.⁵⁶ Copyright 2022, Wiley.

Table 3 The summary of surface-engineered EVs for other diseases

Diseases	Parent cells	Surface engineering	Outcomes	Ref.
Cardiac repair	MSCs	Platelet membrane	Accumulating in the infarcted hearts	71
Viral myocarditis	Macrophages	Platelet membrane	Increasing the targeting capacity of EVs	119
Cerebral ischemia	MSCs	Targeting peptide	Crossing the BBB	63
Myocardial infarction	CDCs	Targeting peptide	Increasing retention of the infarcted heart	65
Myocardial infarction	MSCs	Targeting peptide	Increasing retention	120
Heart injury	CDCs	Targeting peptide	Targeting affinity to cardiomyocytes	54
Angiogenesis	K562	RGD targeting peptide	Increasing targeting of blood vessels	64
Myocardial infarction reperfusion injury	MSCs	CD47	Improving biodistribution in the heart	135
Central nervous system injuries	M2 microglia	DA7R; SDF-1	Enhancing accumulation in the ischemic area	122
White matter injury	MSCs	SIRP- α	Attenuating neuroinflammation	123
Alzheimer's disease	MSCs	SHP2	Restoring mitophagy in AD mice	127
Alzheimer's disease	MSCs	Hypoxic condition	Regulating immune responses in AD mice	128
Alzheimer's disease	MSCs	AD condition	Prolonging lift-time of AD mice	129
Alzheimer's disease	MSCs	RVG peptide	Enhancing the accumulation of EVs	130

Table 4 List of clinical trials on the use of surface-engineered EVs

Title	Sponsor	Status	Registered time	Reference
A phase I feasibility study to evaluate the safety of CD24-exosomes in patients with moderate/severe COVID-19 infection	Tel-Aviv Sourasky Medical Center	Phase I	2020.9.25	NCT04747574
A phase II randomized, double-blind, placebo-controlled study to evaluate the safety and efficacy of exosomes overexpressing CD24 to prevent clinical deterioration in patients with moderate or severe COVID-19 infection	Eli Sprecher	Phase II	2021.7.11	NCT04969172
A phase II randomized, single-blind dose study to evaluate the safety and efficacy of exosomes overexpressing CD24 in 10^9 dose <i>versus</i> 10^{10} dose, for the prevention of clinical deterioration in patients with moderate or severe COVID-19	Athens Medical Society	Phase II	2021.6.21	NCT04902183
A clinical trial for the safety and efficacy of exosomes that overexpress CD24 for preventing the deterioration of moderate or severe COVID-19	OBCTCD-24	Phase II	2022.1.28	EUCTR2021-004259-17-GR
Phase II trial of a vaccination with tumor antigen-loaded dendritic cell-derived exosomes on patients with unresectable non-small cell lung cancer responding to induction chemotherapy	Gustave Roussy, Cancer Campus, Grand Paris	Phase II	2010.7.8	NCT01159288
A first-in-human study of CDK-002 (exoSTING) in subjects with advanced/metastatic, recurrent, injectable solid tumors	Codiak BioSciences	Phase I/II	2020.10.18	NCT04592484
A phase 1/2a study of CDK-003 in patients with cutaneous T-cell lymphoma (CTCL)	Codiak BioSciences	Phase I/IIa	2021.12.14	NCT05156229
A study of exoASO-STAT6 (CDK-004) in patients with advanced hepatocellular carcinoma (HCC) and patients with liver metastases from either primary gastric cancer or colorectal cancer (CRC)	Codiak BioSciences	Phase I	2022.5.16	NCT05375604
iExosomes in treating participants with metastatic pancreatic cancer with KrasG12D mutation	M.D. Anderson Cancer Center	Phase I	2021.1.27	NCT03608631

human health.¹²¹ As free drugs are difficult to accumulate in the CNS due to the blood–brain barrier (BBB), EVs seem to be a potential platform to carry drugs across the BBB, alleviating CNS injury. Ruan *et al.* modified EVs derived from M2 microglia with the targeting peptide and the stem cell recruiting factor to enhance the accumulation of EVs in the ischemic area of the stroke mouse model and increase neurogenesis (Fig. 4C).¹²² Besides, Gao engineered MSCs with SIRP- α and isolated EV–SIRP- α to calm down neuroinflammation.¹²³ These engineered EVs could not only alleviate white matter injury, but also induce M2 polarization due to the recruitment of Treg.

AD is reported as a progressive neurodegenerative disorder with a huge prevalence globally, which could be alleviated by mitophagy.¹²⁴ Tyrosine phosphatase-2 (SHP-2) is a phosphatase whose expression is upregulated during mitophagy.¹²⁵

SHP-2 is a potential drug to induce mitophagy but its application is hindered by its poor BBB penetration and poor stability.¹²⁶ Considering this, our group displayed SHP-2 on the surface of MSC EVs to solve this problem.¹²⁷ EVs–SHP-2 had high BBB penetration ability in AD mice, because of the existence of A β 1–42. The higher accumulation of SHP-2 led to a remarkable reduction of A β 1–42, and improvement of cognitive decline, indicating therapeutic potential in AD treatment. Besides, researchers also engineered EVs by exposing parental MSCs within different conditions and collecting these EVs to treat AD. For instance, Cui *et al.* utilized EVs from hypoxia-conditioned MSCs to regulate immune responses in the brains and alleviate A β accumulation.¹²⁸ Santamaria *et al.* developed EVs from MSCs exposed to AD mouse brain homogenates *in vitro* and these EVs could recover memory function and

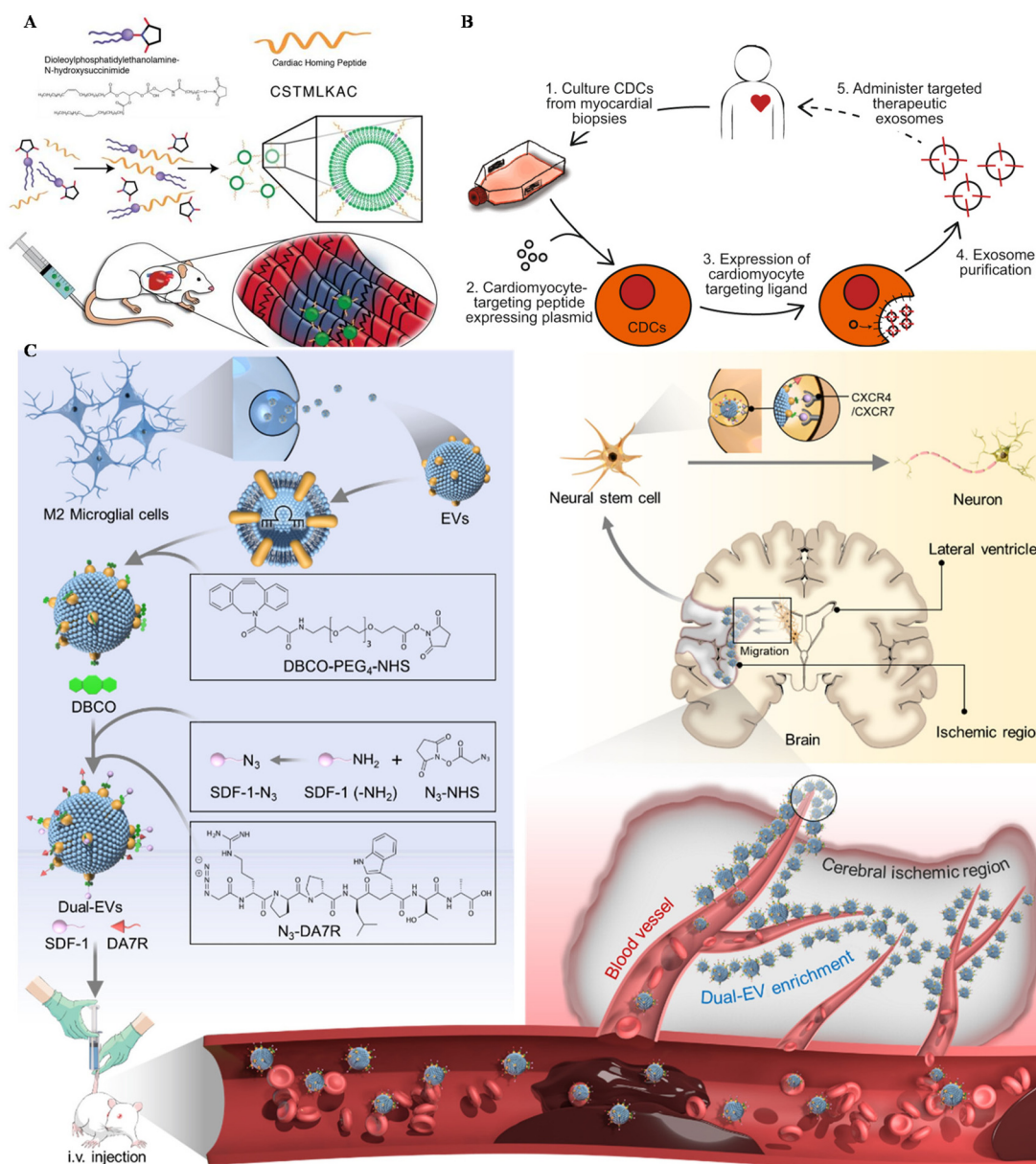


Fig. 4 Utilizing surface-engineered EVs in other diseases. (A) The preparation of myocardium-targeting exosomes. Reproduced with permission.⁶⁵ Copyright 2018, Ivyspring International. (B) Schematic diagram for the construction of CDC-derived targeted exosomes. Reproduced with permission.⁵⁴ Copyright 2019, Springer Nature. (C) The schematic of utilizing engineered EVs for neurological diseases. Reproduced with permission.¹²² Copyright 2022, Elsevier.

prolong the lifespan of AD mice.¹²⁹ Additionally, Cui *et al.* modified EVs with the RVG peptide, to enhance the target capacity of MSC EVs. This strategy successfully increases the delivery efficacy of EVs in AD treatment and improves the memory capacity of AD mice.¹³⁰

5. Conclusion and perspectives

Engineered extracellular vesicles, working as drug delivery systems, are currently a subject of extensive research and devel-

opment. Their present status involves successful laboratory demonstrations of using surface-engineered EVs in the treatment of various diseases, including tumors, autoimmune diseases, infections and other diseases shown above. Early-stage clinical trials are also exploring their potential, particularly in COVID-19. Furthermore, there is growing commercial interest in the applications of EVs, leading to increased investment and collaboration in this field.

Surface engineering of extracellular vesicles (EVs) encompasses various techniques aimed at enhancing their stability, targeting specificity, and therapeutic efficacy. These techniques include

chemical conjugation, where molecules like lipids, peptides, antibodies, or aptamers are covalently attached to EV surfaces, ensuring stable attachment and imparting specific functionalities. Besides, genetic engineering modifies the EV surface composition during biogenesis within donor cells, allowing for precise control over surface properties. Click chemistry offers selective and efficient conjugation of bioactive molecules, enabling rapid and specific modification of EV surfaces. Moreover, comprehensive characterization ensures biological compatibility and evaluates changes in EV size, morphology, and surface properties post-modification. These techniques enable precise customization of EV surface properties, facilitating the development of tailored EV-based therapeutics and diagnostics with enhanced efficacy and specificity.

Five different modification methods are utilized in the surface engineering of EVs, namely chemical engineering, genetic engineering, physical modification, metabolic engineering and lipid-based modification, each of them having distinct advantages and disadvantages. Chemical modification is mostly preferred for its high speed and flexibility, as it allows quick engineering within a short time using various molecules, including peptides and aptamers across different cells or their extracellular vesicles. However, it lacks the precision and control of genetic engineering and may introduce unintended effects on the stability and biological activity of EVs. Moreover, certain chemicals utilized in chemical engineering may be toxic to extracellular vesicles.

On the other hand, genetic modification provides a high degree of specificity and control, allowing precise adjustments to EV composition without affecting their biological activity. Genetically engineered EVs tend to exhibit long-term stability enabling target gene overexpression. Nevertheless, genetic engineering is more time-consuming and labor-intensive, requiring specialized skills and equipment and is not universally applicable to all cell types.

The advantages of physical modification include simplicity, lower costs, and minimal impact on cells. However, its drawbacks include potential unpredictable effects on vesicle stability and function, as well as challenges in achieving precise control. In contrast, metabolic engineering could have precise control over vesicle composition and yield, thus enhancing their potential for drug delivery or therapeutic efficacy. However, metabolic engineering requires a deep understanding of cellular metabolic pathways and may involve complex genetic engineering techniques, resulting in higher costs and technical hurdles. Lastly, lipid-based surface engineering utilizes the properties of lipids to modulate the surface characteristics of vesicles. Advantages include the ability to modify the external surface properties of vesicles without affecting their internal contents, thus enhancing their potential applications in drug delivery and biological imaging. However, this method requires in-depth research into lipid chemistry and biology and may face challenges related to lipid stability and vesicle structure. Researchers should select the approach that best aligns with their needs based on specific research objectives, available resources, and experimental conditions.

However, achieving the clinical use of surface-engineered extracellular vesicles is full of challenges. As extracellular vesicles are heterogeneous, it is urgent to employ various quality control (QC) measurements to ensure the stability and biosafety of engineered EVs. Moreover, the loading ratio of displayed peptides should be measured to ensure lot-to-lot consistency. Additionally, the yield of extracellular vesicles from cultured cells should also be increased with some physical methods to guarantee large scale EV production.

Looking forward, future development of surface-engineered EVs should focus on standardization and quality control, advanced large-scale production techniques, and the initiation of more clinical trials to validate the efficacy and safety of surface-engineered EVs in various disease treatments. Furthermore, exploring their application in multimodal delivery systems could open new avenues for innovative medical treatments. In summary, surface-engineered EVs working as drug delivery systems have significant potential in improving the diagnosis and treatment of various diseases.

Author contributions

Chenlu Yao: writing – original draft (lead). Hong Zhang: writing – review & editing. Chao Wang: writing – review & editing (lead).

Conflicts of interest

There are no conflicts of interest to be declared.

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References

- 1 C. Harding, J. Heuser and P. Stahl, *J. Cell Biol.*, 1983, **97**, 329–339.
- 2 J. Skog, T. Würdinger, S. van Rijn, D. H. Meijer, L. Gainche, W. T. Curry, B. S. Carter, A. M. Krichevsky and X. O. Breakefield, *Nat. Cell Biol.*, 2008, **10**, 1470–1476.
- 3 H. Valadi, K. Ekström, A. Bossios, M. Sjöstrand, J. J. Lee and J. O. Lötvall, *Nat. Cell Biol.*, 2007, **9**, 654–659.
- 4 P. D. Robbins and A. E. Morelli, *Nat. Rev. Immunol.*, 2014, **14**, 195–208.
- 5 E. D'Asti, D. Garnier, T. H. Lee, L. Montermini, B. Meehan and J. Rak, *Front. Physiol.*, 2012, **3**, 294.

- 6 L. Cheng and A. F. Hill, *Nat. Rev. Drug Discovery*, 2022, **21**, 379–399.
- 7 X. Zhang, H. Zhang, J. Gu, J. Zhang, H. Shi, H. Qian, D. Wang, W. Xu, J. Pan and H. A. Santos, *Adv. Mater.*, 2021, **33**, 2005709.
- 8 F. N. Faruqu, J. T.-W. Wang, L. Xu, L. McNickle, E. M.-Y. Chong, A. Walters, M. Gurney, A. Clayton, L. A. Smyth, R. Hider, J. Sosabowski and K. T. Al-Jamal, *Theranostics*, 2019, **9**, 1666–1682.
- 9 T. Smyth, M. Kullberg, N. Malik, P. Smith-Jones, M. W. Graner and T. J. Anchordoquy, *J. Controlled Release*, 2015, **199**, 145–155.
- 10 M. P. Zaborowski, L. Balaj, X. O. Breakefield and C. P. Lai, *BioScience*, 2015, **65**, 783–797.
- 11 F. Tian, S. Zhang, C. Liu, Z. Han, Y. Liu, J. Deng, Y. Li, X. Wu, L. Cai, L. Qin, Q. Chen, Y. Yuan, Y. Liu, Y. Cong, B. Ding, Z. Jiang and J. Sun, *Nat. Commun.*, 2021, **12**, 2536.
- 12 G. Qiu, G. Zheng, M. Ge, J. Wang, R. Huang, Q. Shu and J. Xu, *Stem Cell Res. Ther.*, 2019, **10**, 359.
- 13 Q. Ma, J. Bai, J. Xu, H. Dai, Q. Fan, Z. Fei, J. Chu, C. Yao, H. Shi, X. Zhou, L. Bo and C. Wang, *Adv. NanoBiomed Res.*, 2021, **1**, 2100071.
- 14 Q. Ma, Q. Fan, X. Han, Z. Dong, J. Xu, J. Bai, W. Tao, D. Sun and C. Wang, *J. Controlled Release*, 2021, **329**, 445–453.
- 15 Q. Ma, Q. Fan, J. Xu, J. Bai, X. Han, Z. Dong, X. Zhou, Z. Liu, Z. Gu and C. Wang, *Matter*, 2020, **3**, 287–301.
- 16 W. Chiangjong, P. Netsirisawan, S. Hongeng and S. Chutipongtanate, *Front. Med.*, 2021, **8**, 761362.
- 17 W. M. Usman, T. C. Pham, Y. Y. Kwok, L. T. Vu, V. Ma, B. Peng, Y. S. Chan, L. Wei, S. M. Chin, A. Azad, A. B.-L. He, A. Y. H. Leung, M. Yang, N. Shyh-Chang, W. C. Cho, J. Shi and M. T. N. Le, *Nat. Commun.*, 2018, **9**, 2359.
- 18 Y. Ito, S. Nakamura, N. Sugimoto, T. Shigemori, Y. Kato, M. Ohno, S. Sakuma, K. Ito, H. Kumon, H. Hirose, H. Okamoto, M. Nogawa, M. Iwasaki, S. Kihara, K. Fujio, T. Matsumoto, N. Higashi, K. Hashimoto, A. Sawaguchi, K.-I. Harimoto, M. Nakagawa, T. Yamamoto, M. Handa, N. Watanabe, E. Nishi, F. Arai, S. Nishimura and K. Eto, *Cell*, 2018, **174**, 636–648.
- 19 S.-C. Tao, S.-C. Guo and C.-Q. Zhang, *Int. J. Biol. Sci.*, 2017, **13**, 828–834.
- 20 F. Puhm, E. Boilard and K. R. Machlus, *Arterioscler., Thromb., Vasc. Biol.*, 2020, **41**, 87–96.
- 21 Y. Wang, M. Zhao, S. Liu, J. Guo, Y. Lu, J. Cheng and J. Liu, *Cell Death Dis.*, 2020, **11**, 924.
- 22 C. Cianciaruso, T. Beltraminelli, F. Duval, S. Nassiri, R. Hamelin, A. Mozes, H. Gallart-Ayala, G. Ceada Torres, B. Torchia, C. H. Ries, J. Ivanisevic and M. De Palma, *Cell Rep.*, 2019, **27**, 3062–3080.
- 23 Y. Zhao, Y. Zheng, Y. Zhu, H. Li, H. Zhu and T. Liu, *J. Nanobiotechnol.*, 2022, **20**, 359.
- 24 A. Matsumoto, M. Asuka, Y. Takahashi and Y. Takakura, *Biomaterials*, 2020, **252**, 120112.
- 25 O. Markov, A. Oshchepkova and N. Mironova, *Front. Pharmacol.*, 2019, **10**, 1152.
- 26 J. Chen, F. Huang, Y. Hou, X. Lin, R. Liang, X. Hu, J. Zhao, J. Wang, N. Olsen and S. G. Zheng, *Cell. Mol. Immunol.*, 2021, **18**, 2516–2529.
- 27 S. Shin, I. Jung, D. Jung, C. S. Kim, S.-M. Kang, S. Ryu, S.-J. Choi, S. Noh, J. Jeong, B. Y. Lee, J.-K. Park, J. Shin, H. Cho, J.-I. Heo, Y. Jeong, S. H. Choi, S. Y. Lee, M.-C. Baek and K. Yea, *Biomaterials*, 2022, **289**, 121765.
- 28 I. S. Okoye, S. M. Coomes, V. S. Pelly, S. Czesio, V. Papayannopoulos, T. Tolmachova, M. C. Seabra and M. S. Wilson, *Immunity*, 2014, **41**, 89–103.
- 29 M. F. Gutknecht, N. E. Holodick and T. L. Rothstein, *iScience*, 2023, **26**, 107526.
- 30 F. Zhang, R. Li, Y. Yang, C. Shi, Y. Shen, C. Lu, Y. Chen, W. Zhou, A. Lin, L. Yu, W. Zhang, Z. Xue, J. Wang and Z. Cai, *Immunity*, 2019, **50**, 738–750.
- 31 F. Wu, M. Xie, M. Hun, Z. She, C. Li, S. Luo, X. Chen, W. Wan, C. Wen and J. Tian, *Front. Immunol.*, 2021, **12**, 658698.
- 32 C. H. Wu, J. Li, L. Li, J. Sun, M. Fabbri, A. S. Wayne, R. C. Seeger and A. Y. Jong, *J. Extracell. Vesicles*, 2019, **8**, 1588538.
- 33 J. Kowal and M. Tkach, in *International Review of Cell and Molecular Biology*, ed. C. Lhuillier and L. Galluzzi, Academic Press, 2019, vol. 349, pp. 213–249.
- 34 A. Barone, N. d'Avanzo, M. C. Cristiano, D. Paolino and M. Fresta, *Biomedicines*, 2022, **10**, 252.
- 35 F. Lyu, K. Wu, S.-Y. Wu, R. P. Deshpande, A. Tyagi, I. Ruiz, S. Yalavarthi and K. Watabe, *Oncogene*, 2024, **43**, 319–327.
- 36 Y. Jiao, Y. Tang, Y. Li, C. Liu, J. He, L.-K. Zhang and Y.-Q. Guan, *J. Controlled Release*, 2022, **349**, 606–616.
- 37 C. Marar, B. Starich and D. Wirtz, *Nat. Immunol.*, 2021, **22**, 560–570.
- 38 S. Keshtkar, N. Azarpira and M. H. Ghahremani, *Stem Cell Res. Ther.*, 2018, **9**, 63.
- 39 S. Rani, A. E. Ryan, M. D. Griffin and T. Ritter, *Mol. Ther.*, 2015, **23**, 812–823.
- 40 M. Riazifar, E. J. Pone, J. Lötvall and W. Zhao, *Annu. Rev. Pharmacol. Toxicol.*, 2017, **57**, 125–154.
- 41 S. Varderidou-Minasian and M. J. Lorenowicz, *Theranostics*, 2020, **10**, 5979–5997.
- 42 A. Krishnan, S. Muthusamy, F. B. Fernandez and N. Kasoju, *Tissue Eng. Regener. Med.*, 2022, **19**, 659–673.
- 43 M. G. Sartorio, E. J. Pardue, M. F. Feldman and M. F. Haurat, *Annu. Rev. Microbiol.*, 2021, **75**, 609–630.
- 44 M. Kaparakis-Liaskos and R. L. Ferrero, *Nat. Rev. Immunol.*, 2015, **15**, 375–387.
- 45 K. E. Bonnington and M. J. Kuehn, *Biochim. Biophys. Acta, Mol. Cell Res.*, 2014, **1843**, 1612–1619.
- 46 S. Qing, C. Lyu, L. Zhu, C. Pan, S. Wang, F. Li, J. Wang, H. Yue, X. Gao, R. Jia, W. Wei and G. Ma, *Adv. Mater.*, 2020, **32**, 2002085.
- 47 S. Wang, J. Guo, Y. Bai, C. Sun, Y. Wu, Z. Liu, X. Liu, Y. Wang, Z. Wang, Y. Zhang and H. Hao, *Front. Immunol.*, 2022, **13**, 987419.

- 48 Y. Cui, J. Gao, Y. He and L. Jiang, *Protoplasma*, 2020, **257**, 3–12.
- 49 S. Rome, *Food Funct.*, 2019, **10**, 529–538.
- 50 L. Yu, Z. Deng, L. Liu, W. Zhang and C. Wang, *Front. Bioeng. Biotechnol.*, 2020, **8**, 584391.
- 51 N. P. Ly, H. S. Han, M. Kim, J. H. Park and K. Y. Choi, *Bioact. Mater.*, 2023, **22**, 365–383.
- 52 M. Y. Konoshenko, E. A. Lekchnov, A. V. Vlassov and P. P. Laktionov, *BioMed Res. Int.*, 2018, **2018**, 8545347.
- 53 Q. Zhang, D. K. Jeppesen, J. N. Higginbotham, J. L. Franklin and R. J. Coffey, *Nat. Protoc.*, 2023, **18**, 1462–1487.
- 54 X. Wang, Y. Chen, Z. Zhao, Q. Meng, Y. Yu, J. Sun, Z. Yang, Y. Chen, J. Li, T. Ma, H. Liu, Z. Li, J. Yang and Z. Shen, *J. Am. Heart Assoc.*, 2018, **7**, e008737.
- 55 T. A. Scott, A. Supramaniam, A. Idris, A. A. Cardoso, S. Shrivastava, G. Kelly, N. A. Grepo, C. Soemardy, R. M. Ray, N. A. J. McMillan and K. V. Morris, *Mol. Ther. – Methods Clin. Dev.*, 2022, **24**, 355–366.
- 56 H. K. Kim, J. Cho, E. Kim, J. Kim, J. S. Yang, K. C. Kim, J. Y. Lee, Y. Shin, L. F. Palomera, J. Park, S. H. Baek, H. G. Bae, Y. Cho, J. Han, J. H. Sul, J. Lee, J. H. Park, Y. W. Cho, W. Lee and D. G. Jo, *J. Extracell. Vesicles*, 2022, **11**, e12179.
- 57 D. Bellavia, S. Raimondo, G. Calabrese, S. Forte, M. Cristaldi, A. Patinella, L. Memeo, M. Manno, S. Raccosta, P. Diana, G. Cirrincione, G. Giavaresi, F. Monteleone, S. Fontana, G. De Leo and R. Alessandro, *Theranostics*, 2017, **7**, 1333–1345.
- 58 E. Koh, E. J. Lee, G.-H. Nam, Y. Hong, E. Cho, Y. Yang and I.-S. Kim, *Biomaterials*, 2017, **121**, 121–129.
- 59 M. Piffoux, J. Volatron, K. Cherukula, K. Aubertin, C. Wilhelm, A. K. A. Silva and F. Gazeau, *Adv. Drug Delivery Rev.*, 2021, **178**, 113972.
- 60 H. Qin, H. Li, J. Zhu, Y. Qin, N. Li, J. Shi, G. Nie and R. Zhao, *Small*, 2023, 2303225.
- 61 W. Xi, T. F. Scott, C. J. Kloxin and C. N. Bowman, *Adv. Funct. Mater.*, 2014, **24**, 2572–2590.
- 62 C. D. Hein, X.-M. Liu and D. Wang, *Pharm. Res.*, 2008, **25**, 2216–2230.
- 63 T. Tian, H.-X. Zhang, C.-P. He, S. Fan, Y.-L. Zhu, C. Qi, N.-P. Huang, Z.-D. Xiao, Z.-H. Lu, B. A. Tannous and J. Gao, *Biomaterials*, 2018, **150**, 137–149.
- 64 J. Wang, W. Li, Z. Lu, L. Zhang, Y. Hu, Q. Li, W. Du, X. Feng, H. Jia and B.-F. Liu, *Nanoscale*, 2017, **9**, 15598–15605.
- 65 A. Vandergriff, K. Huang, D. Shen, S. Hu, M. T. Hensley, T. G. Caranasos, L. Qian and K. Cheng, *Theranostics*, 2018, **8**, 1869–1878.
- 66 T. J. Antes, R. C. Middleton, K. M. Luther, T. Ijichi, K. A. Peck, W. J. Liu, J. Valle, A. K. Echavez and E. Marbán, *J. Nanobiotechnol.*, 2018, **16**, 61.
- 67 S. Rayamajhi and S. Aryal, *J. Mater. Chem. B*, 2020, **8**, 4552–4569.
- 68 Y.-Y. Jhan, D. Prasca-Chamorro, G. Palou Zuniga, D. M. Moore, S. Arun Kumar, A. K. Gaharwar and C. J. Bishop, *Int. J. Pharm.*, 2020, **573**, 118802.
- 69 M. Richter, P. Vader and G. Fuhrmann, *Adv. Drug Delivery Rev.*, 2021, **173**, 416–426.
- 70 S. Rayamajhi, R. Marasini, T. D. T. Nguyen, B. L. Plattner, D. Biller and S. Aryal, *Biomater. Sci.*, 2020, **8**, 2887–2904.
- 71 Q. Li, Z. Huang, Q. Wang, J. Gao, J. Chen, H. Tan, S. Li, Z. Wang, X. Weng, H. Yang, Z. Pang, Y. Song, J. Qian and J. Ge, *Biomaterials*, 2022, **284**, 121529.
- 72 J. P. K. Armstrong, M. N. Holme and M. M. Stevens, *ACS Nano*, 2017, **11**, 69–83.
- 73 C. Williams, F. Royo, O. Aizpurua-Olaizola, R. Pazos, G.-J. Boons, N.-C. Reichardt and J. M. Falcon-Perez, *J. Extracell. Vesicles*, 2018, **7**, 1442985.
- 74 G. T. Lim, D. G. You, H. S. Han, H. Lee, S. Shin, B. H. Oh, E. K. P. Kumar, W. Um, C. H. Kim, S. Han, S. Lee, S. Lim, H. Y. Yoon, K. Kim, I. C. Kwon, D. G. Jo, Y. W. Cho and J. H. Park, *J. Extracell. Vesicles*, 2021, **10**, e1207.
- 75 A. H. Mohammadi, Z. Ghazvinian, F. Bagheri, M. Harada and K. Baghaei, *BioDrugs*, 2023, **37**, 353–374.
- 76 T. Limongi, F. Susa, M. Marini, M. Allione, B. Torre, R. Pisano and E. di Fabrizio, *Nanomaterials*, 2021, **11**, 3391.
- 77 W. Lin, Y. Xu, X. Chen, J. Liu, Y. Weng, Q. Zhuang, F. Lin, Z. Huang, S. Wu, J. Ding, L. Chen, X. Qiu, L. Zhang, J. Wu, D. Lin and S. Qiu, *Theranostics*, 2020, **10**, 4871–4884.
- 78 S. K. Horrevorts, D. A. Stolk, R. van de Ven, B. v. H. Hof, S. Duinkerken, M. Hulst, M. H. Heineke, W. Ma, S. A. Dusoswa, R. Nieuwland, J. J. Garcia-Vallejo, A. A. van de Loosdrecht, T. D. de Gruijl, S. J. van Vliet and Y. van Kooyk, *Cancers*, 2019, **11**, 1266–1284.
- 79 T. Yong, Z. Wei, L. Gan and X. Yang, *Adv. Mater.*, 2022, **34**, 2201054.
- 80 S. Walker, S. Busatto, A. Pham, M. Tian, A. Suh, K. Carson, A. Quintero, M. Lafrence, H. Malik, M. X. Santana and J. Wolfram, *Theranostics*, 2019, **9**, 8001–8017.
- 81 A. Taghikhani, F. Farzaneh, F. Sharifzad, S. Mardpour, M. Ebrahimi and Z. M. Hassan, *Front. Immunol.*, 2020, **11**, 221.
- 82 K. Y. Choi, H. Y. Yoon, J.-H. Kim, S. M. Bae, R.-W. Park, Y. M. Kang, I.-S. Kim, I. C. Kwon, K. Choi, S. Y. Jeong, K. Kim and J. H. Park, *ACS Nano*, 2011, **5**, 8591–8599.
- 83 S. Sajeesh, A. Camardo, S. Dahal and A. Ramamurthi, *Mol. Pharm.*, 2023, **20**, 2801–2813.
- 84 C.-L. Liu, J. Guo, X. Zhang, G. K. Sukhova, P. Libby and G.-P. Shi, *Nat. Rev. Cardiol.*, 2018, **15**, 351–370.
- 85 Y. Tian, S. Li, J. Song, T. Ji, M. Zhu, G. J. Anderson, J. Wei and G. Nie, *Biomaterials*, 2014, **35**, 2383–2390.
- 86 S. Loibl and L. Gianni, *Lancet*, 2017, **389**, 2415–2429.
- 87 A. Longatti, C. Schindler, A. Collinson, L. Jenkinson, C. Matthews, L. Fitzpatrick, M. Blundy, R. Minter, T. Vaughan, M. Shaw and N. Tigue, *Nanoscale*, 2018, **10**, 14230–14244.
- 88 S. A. A. Kooijmans, C. G. Aleza, S. R. Roffler, W. W. van Solinge, P. Vader and R. M. Schiffelers, *J. Extracell. Vesicles*, 2016, **5**, 31053.

- 89 R. Ito, N. Oue, K. Yoshida, K. Kunimitsu, H. Nakayama, K. Nakachi and W. Yasui, *Virchows Arch.*, 2005, **447**, 717–722.
- 90 P. Xia, H. Yuan, M. Tian, T. Zhong, R. Hou, X. Xu, J. Ma, H. Wang, Z. Li, D. Huang, C. Qu, L. Dai, C. Xu, C. Yang, H. Jiang, Y. He, F. Rückert, Z. Li, Y. Yuan and J. Wang, *Adv. Funct. Mater.*, 2022, **33**, 2209393.
- 91 K. Moon, J. Hur, K. P. Kim, K. Lee and J. Y. Kang, *Adv. Mater. Interfaces*, 2023, **10**, 2300220.
- 92 M. Binnewies, E. W. Roberts, K. Kersten, V. Chan, D. F. Fearon, M. Merad, L. M. Coussens, D. I. Gabrilovich, S. Ostrand-Rosenberg, C. C. Hedrick, R. H. Vonderheide, M. J. Pittet, R. K. Jain, W. Zou, T. K. Howcroft, E. C. Woodhouse, R. A. Weinberg and M. F. Krummel, *Nat. Med.*, 2018, **24**, 541–550.
- 93 B. Lv, Y. Wang, D. Ma, W. Cheng, J. Liu, T. Yong, H. Chen and C. Wang, *Front. Immunol.*, 2022, **13**, 844142.
- 94 L. Xu, C. Zou, S. Zhang, T. S. M. Chu, Y. Zhang, W. Chen, C. Zhao, L. Yang, Z. Xu, S. Dong, H. Yu, B. Li, X. Guan, Y. Hou and F.-M. Kong, *J. Hematol. Oncol.*, 2022, **15**, 87–117.
- 95 H. Phuengkham, L. Ren, I. W. Shin and Y. T. Lim, *Adv. Mater.*, 2019, **31**, 1803322.
- 96 Y. Tie, F. Tang, Y.-Q. Wei and X.-W. Wei, *J. Hematol. Oncol.*, 2022, **15**, 61–94.
- 97 S. G. Kalathil and Y. Thanavala, *Cancer Immunol. Immunother.*, 2016, **65**, 813–819.
- 98 Q. F. Meng, Y. Zhao, C. Dong, L. Liu, Y. Pan, J. Lai, Z. Liu, G. T. Yu, X. Chen and L. Rao, *Angew. Chem., Int. Ed.*, 2021, **60**, 26320–26326.
- 99 B. Li, T. Fang, Y. Li, T. Xue, Z. Zhang, L. Li, F. Meng, J. Wang, L. Hou, X. Liang, X. Zhang and Z. Gu, *Nano Today*, 2022, **46**, 101606.
- 100 L. Li, Q. Miao, F. Meng, B. Li, T. Xue, T. Fang, Z. Zhang, J. Zhang, X. Ye, Y. Kang, X. Zhang, Q. Chen, X. Liang, H. Chen and X. Zhang, *Theranostics*, 2021, **11**, 6033–6043.
- 101 X. Shi, Q. Cheng, T. Hou, M. Han, G. Smbatyan, J. E. Lang, A. L. Epstein, H. J. Lenz and Y. Zhang, *Mol. Ther.*, 2020, **28**, 536–547.
- 102 P. Guernonprez, J. Valladeau, L. Zitvogel, C. Théry and S. Amigorena, *Annu. Rev. Immunol.*, 2002, **20**, 621–667.
- 103 X. Dai, Z. Wang, M. Fan, H. Liu, X. Yang, X. Wang, X. Zhou, Y. Dai, J. Zhang and Z. Li, *Extracell. Vesicles*, 2022, **1**, 100012.
- 104 F. Xu, D. Jiang, J. Xu, H. Dai, Q. Fan, Z. Fei, B. Wang, Y. Zhang, Q. Ma, Q. Yang, Y. Chen, E. A. Ogunnaike, J. Chu and C. Wang, *Cell Rep.*, 2023, **42**, 113138.
- 105 M. Li, H. Zhou, C. Yang, Y. Wu, X. Zhou, H. Liu and Y. Wang, *J. Controlled Release*, 2020, **323**, 253–268.
- 106 K. Cheng, R. Zhao, Y. Li, Y. Qi, Y. Wang, Y. Zhang, H. Qin, Y. Qin, L. Chen, C. Li, J. Liang, Y. Li, J. Xu, X. Han, G. J. Anderson, J. Shi, L. Ren, X. Zhao and G. Nie, *Nat. Commun.*, 2021, **12**, 2041.
- 107 Y. Yue, J. Xu, Y. Li, K. Cheng, Q. Feng, X. Ma, N. Ma, T. Zhang, X. Wang, X. Zhao and G. Nie, *Nat. Biomed. Eng.*, 2022, **6**, 898–909.
- 108 W.-R. Zhuang, Y. Wang, W. Nie, Y. Lei, C. Liang, J. He, L. Zuo, L.-L. Huang and H.-Y. Xie, *Nat. Commun.*, 2023, **14**, 1675–1690.
- 109 Y. Li, K. Zhang, Y. Wu, Y. Yue, K. Cheng, Q. Feng, X. Ma, J. Liang, N. Ma, G. Liu, G. Nie, L. Ren and X. Zhao, *Small*, 2022, **18**, 2107461.
- 110 P. Marrack, J. Kappler and B. L. Kotzin, *Nat. Med.*, 2001, **7**, 899–905.
- 111 D. G. You, G. T. Lim, S. Kwon, W. Um, B. H. Oh, S. H. Song, J. Lee, D.-G. Jo, Y. W. Cho and J. H. Park, *Sci. Adv.*, 2021, **7**, eabe0083.
- 112 L. M. Francisco, P. T. Sage and A. H. J. I. R. Sharpe, *Immunol. Rev.*, 2010, **236**, 219–242.
- 113 M. W. Becker, L. D. Peters, T. Myint, D. Smurlick, A. Powell, T. M. Brusko and E. A. Phelps, *Sci. Adv.*, 2023, **9**, eadg1082.
- 114 F. Xu, Z. Fei, H. Dai, J. Xu, Q. Fan, S. Shen, Y. Zhang, Q. Ma, J. Chu, F. Peng, F. Zhou, Z. Liu and C. Wang, *Adv. Mater.*, 2021, **34**, 2106265.
- 115 C. Wu, Q. Xu, H. Wang, B. Tu, J. Zeng, P. Zhao, M. Shi, H. Qiu and Y. Huang, *Acta Pharm. Sin. B*, 2022, **12**, 1523–1533.
- 116 F. Xie, P. Su, T. Pan, X. Zhou, H. Li, H. Huang, A. Wang, F. Wang, J. Huang, H. Yan, L. Zeng, L. Zhang and F. Zhou, *Adv. Mater.*, 2021, **33**, 2103471.
- 117 K. Mc Namara, H. Alzubaidi and J. K. Jackson, *Integr. Pharm. Res. Pract.*, 2019, **8**, 1–11.
- 118 C. M. Boulanger, X. Loyer, P.-E. Rautou and N. Amabile, *Nat. Rev. Cardiol.*, 2017, **14**, 259–272.
- 119 W. Pei, Y. Zhang, X. Zhu, C. Zhao, X. Li, H. Lu and K. Lv, *ACS Nano*, 2024, **18**, 2782–2799.
- 120 X. Wang, Y. Chen, Z. Zhao, Q. Meng, Y. Yu, J. Sun, Z. Yang, Y. Chen, J. Li, T. Ma, H. Liu, Z. Li, J. Yang and Z. Shen, *J. Am. Heart Assoc.*, 2018, **7**, e008737.
- 121 C. Meisel, J. M. Schwab, K. Prass, A. Meisel and U. Dirnagl, *Nat. Rev. Neurosci.*, 2005, **6**, 775–786.
- 122 H. Ruan, Y. Li, C. Wang, Y. Jiang, Y. Han, Y. Li, D. Zheng, J. Ye, G. Chen, G.-Y. Yang, L. Deng, M. Guo, X. Zhang, Y. Tang and W. Cui, *Acta Pharm. Sin. B*, 2023, **13**, 2202–2218.
- 123 X. Gao, H. Yang, W. Xiao, J. Su, Y. Zhang, H. Wang, W. Ni and Y. Gu, *Biomater. Res.*, 2022, **26**, 67–91.
- 124 D. Mantle and I. P. Hargreaves, *Int. J. Mol. Sci.*, 2022, **23**, 12603.
- 125 W.-Q. Qiu, W. Ai, F.-D. Zhu, Y. Zhang, M.-S. Guo, B. Y.-K. Law, J.-M. Wu, V. K.-W. Wong, Y. Tang, L. Yu, Q. Chen, C.-L. Yu, J. Liu, D.-L. Qin, X.-G. Zhou and A.-G. Wu, *Free Radicals Biol. Med.*, 2022, **179**, 76–94.
- 126 L. Lu, S. Zhang, C. Li, C. Zhou, D. Li, P. Liu, M. Huang and X. Shen, *Cell Death Dis.*, 2017, **8**, e2767–e2767.
- 127 F. Xu, Y. Wu, Q. Yang, Y. Cheng, J. Xu, Y. Zhang, H. Dai, B. Wang, Q. Ma, Y. Chen, F. Lin and C. Wang, *Adv. Mater.*, 2022, **34**, 2207107.
- 128 G. H. Cui, J. Wu, F. F. Mou, W. H. Xie, F. B. Wang, Q. L. Wang, J. Fang, Y. W. Xu, Y. R. Dong, J. R. Liu and H. D. Guo, *FASEB J.*, 2018, **32**, 654–668.

- 129 G. Santamaria, E. Brandi, P. L. Vitola, F. Grandi, G. Ferrara, F. Pischutta, G. Vegliante, E. R. Zanier, F. Re, A. Uccelli, G. Forloni, N. K. de Rosbo and C. Balducci, *Cell Death Differ.*, 2021, **28**, 203–218.
- 130 G.-H. Cui, H.-D. Guo, H. Li, Y. Zhai, Z.-B. Gong, J. Wu, J.-S. Liu, Y.-R. Dong, S.-X. Hou and J.-R. Liu, *Immun. Ageing*, 2019, **16**, 10.
- 131 X. Li, T. Zhu, R. Wang, J. Chen, L. Tang, W. Huo, X. Huang and Q. Cao, *Adv. Mater.*, 2023, **35**, 2211138.
- 132 D. Jung, S. Shin, S. M. Kang, I. Jung, S. Ryu, S. Noh, S. J. Choi, J. Jeong, B. Y. Lee, K. S. Kim, C. S. Kim, J. H. Yoon, C. H. Lee, F. Bucher, Y. N. Kim, S. H. Im, B. J. Song, K. Yea and M. C. Baek, *J. Extracell. Vesicles*, 2022, **11**, 12287.
- 133 W. Fu, C. Lei, S. Liu, Y. Cui, C. Wang, K. Qian, T. Li, Y. Shen, X. Fan, F. Lin, M. Ding, M. Pan, X. Ye, Y. Yang and S. Hu, *Nat. Commun.*, 2019, **10**, 4355.
- 134 Y. Li, R. Zhao, K. Cheng, K. Zhang, Y. Wang, Y. Zhang, Y. Li, G. Liu, J. Xu, J. Xu, G. J. Anderson, J. Shi, L. Ren, X. Zhao and G. Nie, *ACS Nano*, 2020, **14**, 16698–16711.
- 135 Z. Wei, Z. Chen, Y. Zhao, F. Fan, W. Xiong, S. Song, Y. Yin, J. Hu, K. Yang, L. Yang, B. Xu and J. Ge, *Biomaterials*, 2021, **275**, 121000.