



Cite this: *Soft Matter*, 2025,
21, 9025

Curvature-dependent propulsion of elastic flagella†

Taylor E. Greenwood, ^{‡,ab} Luis Felipe Córdoba, ^{‡,ab} Jian Teng, ^a Saebom Lee,^a Genevieve Dare,^c Ebru Demir, ^c On Shun Pak ^d and Yong Lin Kong ^{*abe}

Soft robotic swimmers that can mimic the flagella-powered locomotion of micro-organisms are of significant interest in a broad range of applications. However, realising micro-organisms' dexterity in soft robots remains challenging without an effective mechanism to achieve bidirectional propulsion in low Reynolds numbers. Here, inspired by recent theoretical studies that suggest the possibility of intrinsically curved elastic flagella to achieve bidirectional propulsion, we experimentally investigate the propulsion behaviour of elastic artificial flagella with uniform intrinsic curvature, actuated by transverse oscillations at $Re < 0.1$. Our results reveal that the flagella's curvature influences the propulsion direction and magnitude, suggesting a transition between positive and negative propulsion when the flagella's central angle in the stress-free state (θ_0) is between 60° and 90° at $Sp = 1.5$ and 1.8 . We also investigate the relationship between the propulsion force and flagella oscillation with numerical simulations. These findings suggest the potential of on-demand curvature modulation during active oscillation to achieve bidirectional propulsion, enhancing the dexterity in flagella-driven artificial swimmers for a broad range of applications in microscale systems.

Received 31st December 2024,
Accepted 21st May 2025

DOI: 10.1039/d4sm01548g

rsc.li/soft-matter-journal

1. Introduction

Propulsion at the microscale often occurs at low Reynolds number (Re),¹ where $Re = \rho uL/\mu \ll 1$ (ρ is the fluid density, u is the translational velocity, L is the contour length, and μ is the dynamic viscosity). At low Re , the inertia effect is negligible, the viscous effect dominates, and the governing equations become Stokes equations under incompressible and Newtonian assumptions. Importantly, as the equations of motion are time-reversible, propulsion must incorporate non-reciprocal motion.² One method to generate propulsion at low Re is by oscillating a slender elastic body,^{2,3} as the body deformation is non-reciprocal, and the drag anisotropy on the slender body induces net propulsion.^{4–6} Using these principles, micro-organisms such as *Chlamydomonas* achieve propulsion at low Re by actively oscillating flexible appendages called flagella.^{5,7,8}

Inspired by biological flagella, prior works have investigated the propulsion characteristics of elastic artificial flagella.^{4,6,9–21} In contrast to the active internal torques that occur along the length of biological flagella during propulsion^{8,22–24} and which have been used in previous micro-scale swimmers,^{21,25,26} elastic artificial flagella are passive geometries that achieve propulsion due to interactions between fluid drag and flagella elasticity when actuated periodically at one end.⁴ Prior studies of elastic artificial flagella have largely focused on flagella with intrinsically straight profiles. For example, Wiggins and Goldstein studied the effect of flagella elasticity on locomotion with a focus on the deformations of the flagella during the motion;⁶ Yu *et al.* experimentally demonstrated propulsion by transverse periodic oscillation of a passive flexible filament;¹² and Peng *et al.* investigated the ability to increase propulsion by varying the flexibility along the filament.¹¹ However, straight flagella only exhibit positive propulsion (in the direction opposite to the wave propagation),³ which critically limits the functionalities that can be achieved. Bidirectional propulsion, or the ability to achieve both positive and negative propulsion, can enable advanced functionalities at the microscale by reversing flow in microfluidic devices, enhancing dexterity during micro-scale object manipulation^{16,17} and reversing locomotion.^{15,27,28}

Intriguingly, recent studies have reported that bidirectional propulsion can be achieved by designing elastic artificial flagella with intrinsically curved profiles in the stress-free state.^{14–16} For example, Namdeo *et al.* used a computational

^a Department of Mechanical Engineering, Rice University, Houston, TX, 77005, USA.
E-mail: kong@rice.edu

^b Department of Mechanical Engineering, University of Utah, Salt Lake City, UT, 84112, USA

^c Department of Mechanical Engineering & Mechanics, Lehigh University, Bethlehem, PA, 18015, USA

^d Department of Mechanical Engineering, Santa Clara University, Santa Clara, CA, 95053, USA

^e Rice Advanced Materials Institute, Rice University, Houston TX 77005, USA

† Electronic supplementary information (ESI) available. See DOI: <https://doi.org/10.1039/d4sm01548g>

‡ T. E. G. and L. F. C. contributed equally.



framework to demonstrate bidirectional propulsion with a 'Y'-shaped swimmer actuated with transverse oscillations,¹⁶ where the swimming direction could be reversed by curving the two free ends. More recently, Liu *et al.* combined asymptotic theory and simulations to demonstrate the bidirectional propulsion of a swimmer that consisted of a spherical body and two symmetrical circular-arc profile filaments actuated with harmonic angular oscillations,¹⁵ where the propulsion direction depended on the filament's curvature. In another study, Liu *et al.* combined theory and simulations to demonstrate the bidirectional propulsion of filaments with cosinusoidal profiles that were actuated with transverse oscillation,¹⁴ where the propulsion direction could be changed by adjusting the sperm number ($Sp = L(\xi_{\perp}\omega/A)^{1/4}$; L is the contour length, $\xi_{\perp}$ is the normal drag coefficient, ω is the oscillation frequency, and A is the filament's flexural rigidity). The authors noted that this relationship between Sp and propulsion direction could enable frequency-dependent bidirectional propulsion. Despite these impressive findings, the propulsion of elastic artificial flagella with intrinsic curvature that are periodically oscillated at one end has yet to be experimentally investigated.

This study investigates the propulsion of elastic artificial flagella with uniform intrinsic curvature at low Re ($Re < 0.1$). Section 2 describes the methods used in the low Re experiments and simulations. In Sections 3.1 and 3.2, we evaluate the effect of curvature and Sp on propulsion using experimental and simulation results. In Sections 3.3 and 3.4, we then investigate the time-varying force and the time-varying curvature of the flagella. Lastly, we conclude in Section 4 by summarizing our observations and providing a discussion on the implications of the results.

2. Materials and methods

2.1 Experimental setup

To experimentally investigate the propulsion of elastic artificial flagella, we leverage 3D printing to fabricate flagella with uniform intrinsic curvature in the stress-free state and perform experiments in a macroscale setup at a low Re flow condition (Fig. 1). We build upon previous numerical and theoretical works that demonstrated bidirectional propulsion of elastic filaments with uniform intrinsic curvature that were angularly oscillated at one end,¹⁵ and elastic filaments with cosinusoidal intrinsic curvature that were transversely oscillated at one end.¹⁴ In this study, we design the flagella geometry with a uniform intrinsic curvature (Fig. 1(A) and (B)) that can, in principle, be modulated post-fabrication with an applied moment or internal strains (*e.g.*, due to asymmetric shrinkage) based on Euler-Bernoulli beam theory.²⁹ Additionally, in contrast to the numerical and theoretical works that utilized filaments with circular cross-sections and restricted the filaments to planar deformations, we design the flagella with a rectangular cross-section at an aspect ratio of 10 : 1 (height : width) to decrease potential out-of-plane bending during oscillation (Fig. S1, ESI†).

The macro-scale experiments were performed in a glass tank (1.2 m length, 0.33 m width, 0.35 m oil depth) filled with high-

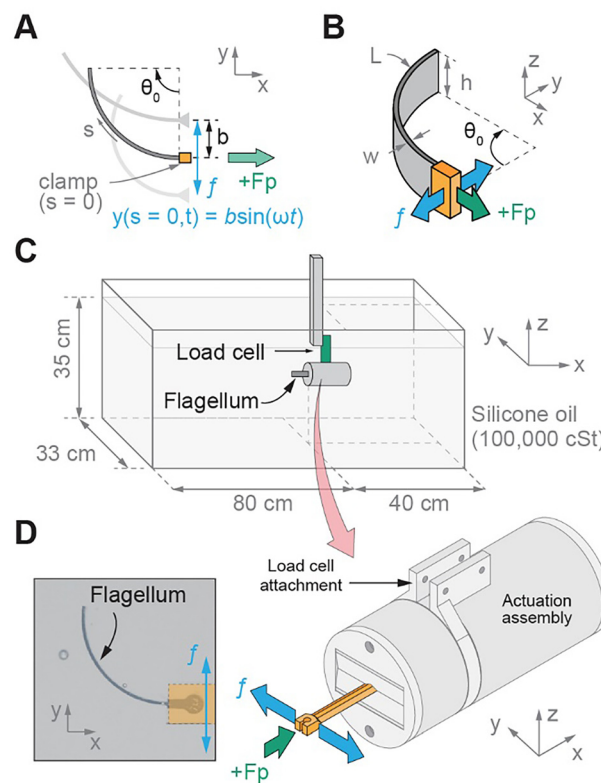


Fig. 1 Experimentally measuring the propulsion of flagella with uniform intrinsic curvature. (A) The flagellum curvature is defined by the central angle in the stress-free state, θ_0 . The clamped end is transversely oscillated at frequency f in the y -direction (b : amplitude), and the propulsive force F_p is measured in the x -direction (the direction of positive F_p is shown). (B) The flagellum is designed with a contour length $L = 22$ mm, width $w = 0.5$ mm, and height $h = 5$ mm. (C) Experiments are performed at the macroscale using an actuation assembly that is submerged in a tank of high-viscosity silicone oil. The F_p is measured with a load cell that connects the actuation assembly to a rigid frame. (D) The actuation assembly uses a Scotch Yoke mechanism to convert a motor's rotation to the transverse oscillation of the flagellum, where f is measured using the motor's encoder. In the schematics in (A)–(B), and in the image in (D), the flagellum has $\theta_0 = 90^\circ$.

viscosity silicone oil (PSF-100 000 cSt, Clearco) with a kinematic viscosity (ν) of 100 000 cSt and a density (ρ) of 977 kg m^{−3}. Experimental Reynolds numbers were in the range of 0.01 (at 1.5 Hz and $Sp = 1.5$ with $\beta = 0.25$) to 0.05 (at 6.0 Hz and $Sp = 2.1$ with $\beta = 0.25$), where the translational velocity $u = 2\pi\beta L$ (the dimensionless amplitude $\beta = b/L$, where b is the oscillation amplitude). The actuated end of the flagellum was attached to an actuation assembly and was oriented to be centered in width and depth, and approximately 40 cm from the front wall (Fig. 1(C) and (D)). The actuation assembly was designed to perform transverse actuation using a geared DC motor (4863, Pololu) and a Scotch Yoke mechanism similar to a previous study.¹² In the experiments, f was controlled using the motor input voltage, and b was controlled using the Scotch Yoke geometry. As shown in Fig. 1(A) and (B), the flagellum was clamped at one end and transversely oscillated in the y -direction at frequency f . The propulsive force F_p was measured in the



x -direction. The experiments were performed with $\beta = 0.25$. We focus on $f = 1.5, 3.0$, and 6.0 Hz due to simulation results for a flagellum with $\theta_0 = 90^\circ$ (Fig. S2, ESI†). Specifically, we chose $f = 3.0$ Hz, as it was near the minimum $\langle F_p \rangle$. We chose $f = 6.0$ Hz, as the $\langle F_p \rangle$ was positive at approximately the same magnitude as the $\langle F_p \rangle$ at 3.0 Hz (Fig. S2, ESI†). We chose the lower bound of $f = 1.5$ Hz due to hardware limitations, as the motor would stall at lower speeds, and the upper bound of $f = 6.0$ Hz was near the upper limit for the motor speed. The chosen frequencies ($1.5, 3.0$, and 6.0 Hz) correspond to Sp values within the Sp range of negative propulsion in previous studies.^{14,15}

2.2 Data acquisition and processing

During oscillation, the time-varying propulsion force F_p was measured using a load cell (ANYLOAD 108AA-100g, Tacuna Systems; load cell specifications shown in the ESI†) attached to the top of the actuation assembly. The frequency f was measured with an encoder on the actuation motor. The load cell and encoder were powered by a calibrated power supply (2231A-30-3 CAL DU, Keithley), and measurements were acquired using a data acquisition system (USB-6353 DAQ, NI) and LabVIEW. The experimental data were post-processed (MATLAB, MathWorks) to calculate F_p and f for each oscillation. During postprocessing, the steady-state $\langle F_p \rangle$ and $\langle f \rangle$ were calculated using the respective values between oscillations 40 and 50 (Fig. S3, ESI†). To compensate for the nonzero forces from the actuation assembly with no flagellum attached, the F_p data were corrected using a second-order polynomial fit to the no-flagellum data (Fig. S4 and S5, ESI†). A second-order fit was chosen, as it was the lowest-order fit that best approximated the data (linear fit $R = 0.9925$, second-order fit $R = 0.997$). A camera (EOS R6, Canon) was mounted above the experiment to capture flagellum deformation during experiments at 120 fps.

2.3 Flagella fabrication

The flagella were fabricated by SLA 3D printing (Form3 and Form3+, FormLabs) with clear resin (FormLabs). After printing, the parts were washed (Form Wash, FormLabs) in isopropyl alcohol for 20 min and post-cured for 60 min at 60°C (Form Cure, FormLabs) following procedures in the material data-sheet, which reports the material's Young's modulus as $E = 2.80$ GPa. The flagella material was chosen to target the desired range of Sp . While the modulus is relatively high compared to many elastomers, the flagella remain flexible during the motion as the viscous forces dominate when $Sp > 1$.

2.4 Simulations

Three-dimensional numerical simulations were used to solve for the zero-Reynolds-number flow field and the fluid-structure interaction between the deformable solid body (*i.e.*, flagellum) and the surrounding fluid flow. The simulations were performed using COMSOL Multiphysics 6.2. The incompressible, steady Stokes equations were solved using the finite-element method in COMSOL. In the simulation, the properties of the flagella and fluid remain consistent with the experimental setup, except that the flagella were positioned centrally within

a fluid volume of 0.5 m length, 0.25 m depth, and 0.25 m width, with the wall far away to eliminate any wall effects. The computational meshes were generated in COMSOL with a physics-based fine mesh setting. Sample simulation domains illustrating the mesh design (Fig. S6, ESI†) show a close-up of the flagella with surrounding fluid. We locally refined the mesh to ensure we captured the complete physics near the flagella.

In the simulation setup, we imposed no-slip boundary conditions on the walls. We implemented a fluid-structure interaction Multiphysics node on the flagellum body to provide coupling on a boundary between a fluid and solid structure. The initial condition is stationary, and then we imposed a sine wave on the clamped end of the flagellum to simulate the experimental setup with an amplitude of $b = \beta L$. Simulations were performed for a range of frequency parameters, where $f = 1.5, 3$, and 6 Hz for $\theta_0 = 0^\circ, 30^\circ, 60^\circ, 90^\circ, 120^\circ, 150^\circ$, and 180° . The $\langle F_p \rangle$ were calculated by taking the average of a spline fit to the x -component of the total traction on the flagellum exterior boundaries.

3. Results and discussion

3.1 Curvature-dependent propulsion

To investigate the effect of uniform intrinsic curvature on propulsion, we evaluate the propulsive force for designs with θ_0 between 0° and 180° at $\langle f \rangle \approx 1.5$ Hz, 3.0 Hz, and 6.0 Hz, which correspond to $Sp = 1.5, 1.8$, and 2.1 , respectively (Fig. 2). The propulsive force $\langle \overline{F_p} \rangle$ is normalized by $\langle F_p \rangle$ at $\theta_0 = 0^\circ$ to enable comparison across different $\langle f \rangle$. Based on numerical results in previous studies,^{14,15} we hypothesized that the intrinsic curvature would change the magnitude and direction of the propulsive force.

The experimental and simulation data in Fig. 2(A) demonstrate that the propulsion of the intrinsically curved flagella is curvature-dependent. To systematically discuss the results and compare the results with prior work, we will first discuss the general trends in the data, then focus on the transitions between positive and negative propulsion, and finally discuss the minimum $\langle \overline{F_p} \rangle$.

The results in Fig. 2(A) show general agreement between the experimental and simulation results, where increasing θ_0 tends to decrease $\langle \overline{F_p} \rangle$, with the highest rate of change between approximately $\theta_0 = 30^\circ$ and 90° . The general agreement of the simulation and experimental results demonstrates that the macroscale experimental setup was capable of capturing some of the curvature-dependent propulsion characteristics of the flagella with uniform intrinsic curvature in the stress-free state. The results also show differences between the experiments and simulations, including in the regions of negative $\langle \overline{F_p} \rangle$. The differences between the experiments and simulations can be partially attributed to imperfections in the experimental setup (*e.g.*, friction, clearance between parts, motor vibration) that lead to non-ideal actuation. The differences between the results are also influenced by differences in the geometrical setup (Fig. S7, ESI†).

Both the experimental and simulation results show that the $\langle \overline{F_p} \rangle$ transitions from positive to negative between $\theta_0 = 60^\circ$ and



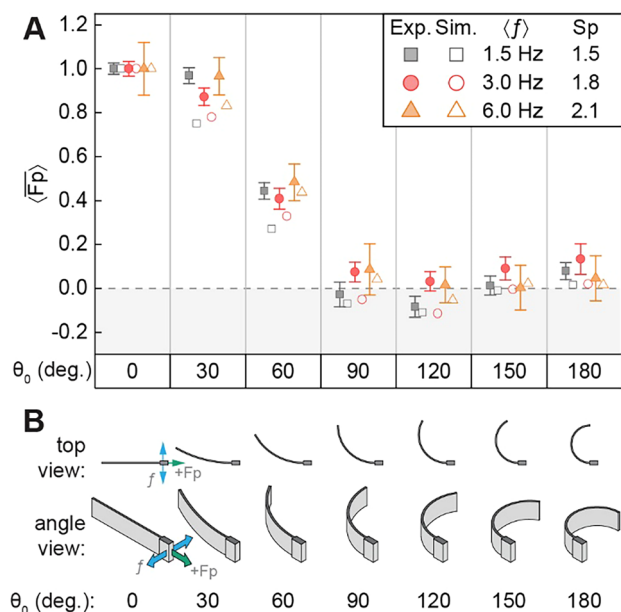


Fig. 2 Curvature-dependent propulsion. (A) The propulsive force $\langle F_p \rangle$ as a function of θ_0 and $\langle f \rangle$ for flagella with θ_0 between 0° and 180° , where $\langle F_p \rangle$ is normalized by $\langle F_p \rangle$ at $\theta_0 = 0^\circ$. All designs have the same dimensions ($L = 22$ mm, $h = 5$ mm, $w = 0.5$ mm) and were actuated at three frequencies ($\langle f \rangle = 1.52 \pm 0.03$, 3.03 ± 0.01 , and 6.00 ± 0.03 Hz corresponding to $Sp = 1.5$, 1.8 , and 2.1 , respectively; error represents standard deviation across all experimental trials at each frequency) with $\beta = 0.25$. Experimental (solid) and simulation (open) data were acquired at each $\langle f \rangle$ and θ_0 , where experimental error bars represent the standard deviation across 20 oscillations at steady state (10 oscillations each for two experiments at each frequency). (B) Illustrations show a top and three-dimensional view of each flagellum.

90° . Specifically, the experimental data transition between positive and negative $\langle F_p \rangle$ at $\langle f \rangle \approx 1.5$ Hz ($Sp = 1.5$), while the simulation data transition at $f = 1.5$ Hz ($Sp = 1.5$) and $f = 3.0$ Hz ($Sp = 1.8$). Additional simulation results show that the transition between positive and negative propulsion occurs near $\theta_0 = 80^\circ$ at 1.5 Hz and near $\theta_0 = 85^\circ$ at 3.0 Hz (Fig. S8, ESI†). In comparison, Liu *et al.* reported negative propulsion when $Sp < \sim 3$ for a flagellum with a cosine profile of one quarter wave under transverse oscillation, which qualitatively appears like a uniform intrinsic curvature profile with higher θ_0 .¹⁴ The transition between positive and negative propulsion near $\theta_0 = 90^\circ$ can be understood by using a reduced-order model in previous work¹⁴ that consisted of two rigid rods of equal length connected by a spring, with the second rod at an offset angle ϕ_1 when the spring was undeflected. The reduced-order model was shown to predict negative propulsion when $\phi_1 > 45^\circ$. In comparison, by modelling the present flagellum with uniform intrinsic curvature as a straight rod connecting the flagellum endpoints, the model would predict negative propulsion when $\theta_0 > 90^\circ$ ($\theta_0 = 90^\circ$ corresponds to $\phi_1 = 45^\circ$; details in ESI†), which is relatively close to the transition in the experimental and simulation results between $\theta_0 = 60^\circ$ and 90° . We anticipate that the transition point in the present results is lower than the $\theta_0 = 90^\circ$ prediction, as the curved flagellum will

exhibit more decrease in θ (*i.e.*, straightening) than increase in θ due to the increased length perpendicular to the transverse oscillation when traveling in the positive y -direction.

The experimental and simulation results in Fig. 2(A) show that the minimum $\langle F_p \rangle$ occurs at approximately $\theta_0 \approx 120^\circ$. In comparison, Liu *et al.* indicated that increasing curvature caused a reversal in the total propulsive force direction with a local minimum $\langle F_p \rangle$ at $\kappa_c \approx 2.62$, which corresponds to $\theta_0 = 150^\circ$ (the intrinsic curvature $\kappa_c = \theta_0$).¹⁵ The 30° difference in the local minimums of the previous report (which utilized angular oscillation at $Sp = 2$) and the present results (which utilized transverse oscillation at $Sp = 1.5$, 1.8 , and 2.1) suggests that similar phenomena may influence the directionality of propulsion for both angular and transverse oscillation. One possible explanation for the 30° difference could be the differences in the force distribution across the flagellum for transverse and angular oscillation, as angular oscillation will have a higher velocity and force near the end of the flagellum due to the rotational motion.

The results in Fig. 2(A) suggest that the propulsion of future intrinsically curved flagella could be modulated on-demand by changing θ_0 . For example, both the experimental and simulation results demonstrate that changing θ_0 between approximately 60° and 120° would cause a flagellum to transition between positive and negative $\langle F_p \rangle$ at 1.5 Hz (for more data showing the experimental results with negative F_p , see Fig. S9 and S10D, ESI†). Due to the constant curvature of a beam in pure bending,²⁹ the uniform intrinsic curvature of the flagella enables predictable curvature changes post-fabrication by inducing stress across the flagella's width. Building on this concept, future work could enable propulsion modulation by modulating the flagellum curvature with single-material constructs such as light-responsive polymers,¹⁶ or multi-layer constructs such as bimetallic strips³⁰ and anisotropic 3D printed materials.³¹

3.2 Sp-dependent propulsion

To investigate the effect of Sp on the propulsion of flagella with uniform intrinsic curvature, we performed experiments and simulations at 1.5 , 3.0 , and 6.0 Hz. The chosen frequencies correspond to $Sp = 1.5$, 1.8 , and 2.1 , respectively, which fall within the range of negative propulsion in previous studies. For instance, Liu *et al.* demonstrated negative propulsion below approximately $Sp = 3$ for a flagellum with a cosine profile of one quarter wave.¹⁴ In the same work, the authors predicted Sp -dependent negative propulsion below approximately $Sp = 1.8$ using a two-spring model.¹⁴ And, in a separate work, Liu *et al.* investigated negative propulsion at $Sp = 2$ using flagella with constant curvature profiles and circular cross-sections actuated by angular oscillation.¹⁵

The results in Fig. 2(A) and Fig. S11 (ESI†) demonstrate that the propulsion depends on Sp , where increasing Sp tends to increase $\langle F_p \rangle$. Specifically, the simulation data show that increasing Sp increases $\langle F_p \rangle$ for each design across the studied Sp range, except for the flagellum with $\theta_0 = 180^\circ$ (where $\langle F_p \rangle$ appears relatively constant across the studied Sp range). The



trend in the experimental results is less clear due to the relatively large error in the data. The simulation results agree with previous studies, which report that Sp tends to increase propulsion between $Sp = 1.5$ and 2.1 .^{14,15} We also note that a two-spring analytical model in previous work suggests that increasing Sp will ultimately cause the negative Fp to increase and become positive.¹⁴

The results in Fig. 2(A) and Fig. S11 (ESI[†]) suggest that the propulsion and the time-varying θ can be modulated by changing the oscillation frequency and the flagella's elastic modulus. Specifically, increasing f will increase Sp and thus tend to increase $\langle Fp \rangle$, while increasing E will decrease Sp and thus tend to decrease $\langle Fp \rangle$ (as the flexural rigidity $A = EI$, where E is the elastic modulus and I is the area moment of inertia). As Sp is the ratio of viscous to elastic forces, increasing Sp will also increase the variation in θ during the oscillation. This implies that increasing f will increase Sp and increase the variation in θ during the oscillation, while increasing E will decrease the variation in θ during the oscillation.

3.3 Time-varying propulsion

To further investigate the negative propulsion, we examine the time-varying Fp across a representative oscillation from simulations at 1.5 Hz ($Sp = 1.5$; Fig. 3). Here, we choose to focus on data collected at 1.5 Hz, as this f resulted in negative propulsion with $\theta_0 = 120^\circ$. We hypothesized that the negative $\langle Fp \rangle$ would be due to increased effectiveness in the negative stroke of the oscillation. A comparison between the data in Fig. 3(A), however, shows that the negative stroke of the flagellum with $\theta_0 = 60^\circ$ results in a lower minimum force ($Fp_{\min} \approx -55$ mN) than the flagellum with $\theta_0 = 120^\circ$ ($Fp_{\min} \approx -43$ mN). This finding is surprising considering that the $\langle Fp \rangle$ for the flagellum with $\theta_0 = 60^\circ$ is positive at 1.5 Hz (simulation: 3.53 mN, experiment: 2.01 ± 0.17 mN), while the $\langle Fp \rangle$ for the flagellum with $\theta_0 = 120^\circ$ is negative at 1.5 Hz (simulation: -1.43 mN, experiment: -0.38 ± 0.22 mN). By comparing Fp across the entire oscillation, we see that the flagellum with $\theta_0 = 120^\circ$ has a

negative $\langle Fp \rangle$ primarily due to a decreased magnitude in the positive stroke, rather than from an increased magnitude in the negative stroke as hypothesized. In other words, these results suggest that negative propulsion may be more easily achieved by decreasing the effectiveness of the positive stroke during the oscillation of flagella that exhibit both positive and negative propulsion during the oscillation.

3.4 Time-varying curvature

The simulation images in Fig. 3(B) and our observations during the experiments indicated that the flagella curvature varied during the oscillation. Changes in curvature during oscillation were anticipated, as the propulsion of elastic artificial flagella relies on interactions between the flagella's elasticity and the surrounding fluid. To quantify the time-varying curvature, we measured the instantaneous flagellum central angle (θ) in the macroscale experiments using image tracking on the experimental videos (Fig. 4). Here, we choose to focus on data collected at 1.5 Hz, as this f resulted in negative propulsion with $\theta_0 = 120^\circ$, and has the clearest images due to the lower translational velocity.

The results in Fig. 4 include three notable characteristics: the θ varies periodically over time in a roughly sinusoidal manner, the average θ is approximately equal to θ_0 (i.e., $\bar{\theta} \approx \theta_0$), and the amplitude of θ decreases with increasing θ_0 . First, the sinusoidal variation of θ was anticipated and can be attributed to the transverse oscillation of the clamped end of the flagella. Second, the observation of $\bar{\theta} \approx \theta_0$ was not unexpected, as a slender elastic body will intuitively bend in the direction opposite to the driven direction when in a viscous fluid. We suspect that slight deviations from $\bar{\theta} = \theta_0$ (e.g., the higher $\bar{\theta}$ for the flagellum designed with $\theta_0 = 90^\circ$) can be attributed to slight imperfections in the fabrication of the experimental flagella. Third, we attribute the decreasing amplitude of the time-varying θ with increasing θ_0 to a decreased deflection of curved cantilever beams under distributed loads and to changes in the fluid forces along the length of the flagella.

To compare the experimental results with simulations, we extract the profiles from the simulation and overlay the profiles onto the experimental images (Fig. S12, ESI[†]). A qualitative visual comparison between the experimental images and simulation profiles shows that the flagella deformations in the simulations agree closely with the flagella deformations in the experiments for flagella with $\theta_0 = 60^\circ$ and 120° . Notably, the comparison shows that the experimental flagellum with $\theta_0 = 90^\circ$ has more curvature (i.e., a higher θ) than in the simulation, which aligns with the data shown in Fig. 4(A), and suggests that the experimental flagellum with $\theta_0 = 90^\circ$ could have more curvature than the design due to imperfections in the fabrication.

The results in Fig. 4 and Fig. S12 (ESI[†]) suggest that the time-varying θ likely influences $\langle Fp \rangle$ by changing the relative magnitudes of the normal and tangential components of propulsion in the x -direction. For flagella with uniform intrinsic curvature ($\theta_0 > 0$), we suspect that the periodic variation in θ affects $\langle Fp \rangle$ by causing slight rotation of the drag-induced

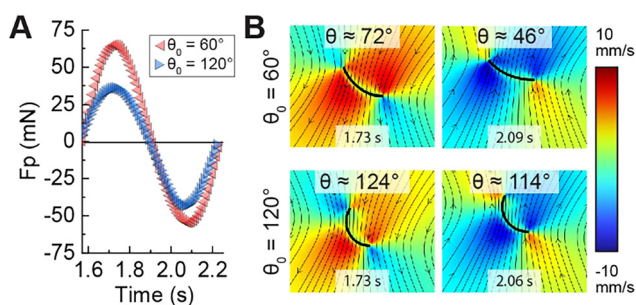


Fig. 3 Time-varying Fp from simulation data for flagella with $\theta_0 = 60^\circ$ and 120° oscillating at 1.5 Hz ($Sp = 1.5$). (A) Time-varying Fp over approximately one oscillation. (B) Simulation images at the peak and trough of the oscillation, with snapshot times indicated. In the images, the thick black lines represent the flagella profiles, the contours represent the horizontal velocity of the fluid (i.e., parallel to the direction in which Fp is measured), and the black arrows show the streamlines. Text on the images also indicates the instantaneous central angle θ of the flagella.



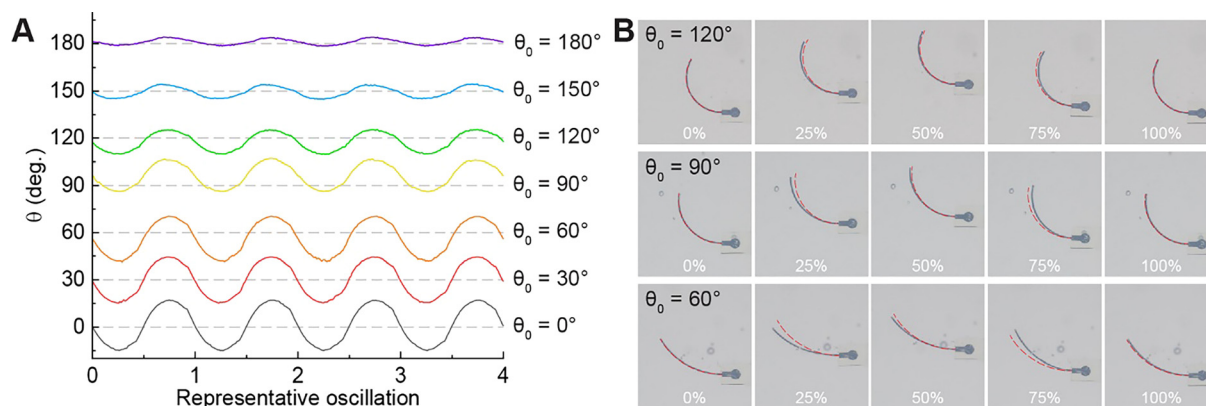


Fig. 4 Experimental data demonstrating the time-varying θ at 1.5 Hz ($Sp = 1.5$). (A) Time-varying θ across four representative oscillations at steady state for one flagellum at each θ_0 . The θ was measured using image tracking on each frame in the experimental videos. (B) Experimental images at approximately 0%, 25%, 50%, 75%, and 100% of an oscillation for flagella with $\theta_0 = 120^\circ$ (top row), 90° (middle row), and 60° (bottom row). To enable comparison between images, a red dashed line is overlaid on each image that shows the instantaneous profile at 0% of the oscillation.

force vectors depending on the actuation direction. When the flagellum is actuated in the positive y -direction, θ decreases, which would cause the force vectors to rotate in the positive z -direction, causing a decrease in the magnitude of F_p in the x -direction (as $\xi_\perp > \xi_\parallel$, where $\xi_\perp$ and $\xi_\parallel$ are the resistive force coefficients^{5,32} in the perpendicular and parallel directions, respectively). On the other hand, when the flagellum is moving in the negative y -direction, θ increases, which would cause the force vectors to rotate in the negative z -direction, causing an increase in the magnitude of F_p . Future studies could investigate this hypothesis by building upon existing reduced-order models¹⁴ to account for the observed periodic variation in θ for flagella with uniform intrinsic curvature.

4. Conclusion

In this work, we studied the low Re ($Re < 0.1$) propulsion of elastic artificial flagella with uniform intrinsic curvature. First, we used macroscale experiments and three-dimensional numerical simulations to demonstrate that the time-averaged propulsion $\langle F_p \rangle$ is curvature dependent, with a transition between positive and negative propulsion when the central angle θ_0 is between 60° and 90° at $\langle f \rangle \approx 1.5$ Hz. Next, we demonstrated that F_p also depends on Sp . We then used simulation data of the time-varying F_p to observe that negative $\langle F_p \rangle$ at $\theta_0 = 120^\circ$ is primarily due to a decrease in the effectiveness of the positive portion of the oscillation. Lastly, we investigated the time-varying curvature, which was shown to vary sinusoidally with $\bar{\theta} \approx \theta_0$.

We envision that future studies could leverage the curvature-dependent and Sp -dependent propulsion of intrinsically curved flagella shown in this work to achieve a variety of objectives, such as enhancing propulsion efficiency. These future developments could include methods to formally optimize designs for single or multiple objectives by incorporating FE simulations into numerical optimization algorithms.

The findings presented in this work suggest that flagella with uniform intrinsic curvature could achieve propulsion

modulation, including bidirectional propulsion, by on-demand curvature modulation during active oscillation. Building on this concept, we envision that propulsion could be modulated in response to local environmental factors such as salinity, pH, temperature, and light, even without the need for external feedback or changes in externally controlled parameters (*e.g.*, oscillation direction or frequency). For example, the stimuli-responsive curvature modulation could be achieved using a multi-layered construct of responsive materials with differing expansion coefficients, similar to a bimetallic strip. Autonomous propulsion modulation in response to environmental conditions is desirable to reduce the complexity of low Re flow control devices and artificial microscale swimmers. Moreover, such behaviour, which loosely resembles the biological locomotion of *Chlamydomonas* cells that have adapted to swim toward light,⁷ could be particularly advantageous where sensing and localization are challenging due to size or access constraints (*e.g.*, within the human body).

This work considers a flagellum clamped at its driven end, consistent with prior work.¹⁴ The clamped end could be replicated in practice by using an actuation method that applies a counteracting torque at the driven end (*e.g.*, using a uniform magnetic field) to maintain the driven end perpendicular to the transverse motion. Future work could extend the present results by investigating the propulsive force and motion of an unconstrained swimmer that more closely resembles biological organism locomotion^{23,24} by accounting for the differences in the boundary conditions (*e.g.*, force and torque-free at every instant). We suspect that an unconstrained swimmer would exhibit in-plane rotation due to the geometric asymmetry. One potential method to reduce this rotation could be to mirror the geometry across a plane perpendicular to the actuation direction.

Author contributions

Y. L. K., O. S. P., and T. E. G. conceived and planned the research. T. E. G., L. F. C., and S. L. performed experiments and collected data. J. T., S. L., E. D., and G. D. performed



simulations and collected data. All authors analysed the data. T. E. G., J. T., and Y. L. K. prepared the manuscript with input from all authors.

Data availability

The data supporting this article have been included as part of the ESI.†

Conflicts of interest

Y. L. K. is an inventor on multiple active patents describing 3D printing technologies, including active electronic materials and devices, and multifunctional hybrid devices and structures. Y. L. K. is also an inventor of gastric-resident systems, including gastric-resident electronics. All other authors declare no conflict of interest.

Acknowledgements

Y. L. K. acknowledges the support from the National Institutes of Health (NIH) NIBIB Trailblazer Award (grant no. R21-EB029563); NIH NIBIB R01 Award (grant no. R01-EB032959); Office of Naval Research Young Investigator Program Award (ONR YIP, N00014-23-1-2391), 3M Non-Tenured Faculty Award; CDMRP Discovery Award (HT9425-23-1-0041). O. S. P. acknowledges partial support from NSF under grant no. CBET-2323046 and CBET-2419945. Y. L. K. and O. S. P. acknowledge the National Science Foundation (NSF) under the Emerging Frontiers in Research and Innovation (EFRI) Program (grant no. EFRI 1830958).

References

- 1 E. Lauga and T. R. Powers, *Rep. Prog. Phys.*, 2009, **72**, 096601.
- 2 E. M. Purcell, *Am. J. Phys.*, 1977, **45**, 3–11.
- 3 G. I. Taylor, *Proc. R. Soc. London, Ser. A*, 1951, **209**, 447–461.
- 4 E. Lauga, *Phys. Rev. E: Stat., Nonlinear, Soft Matter Phys.*, 2007, **75**, 041916.
- 5 J. Gray and G. J. Hancock, *J. Exp. Biol.*, 1955, **32**, 802–814.
- 6 C. H. Wiggins and R. E. Goldstein, *Phys. Rev. Lett.*, 1997, **80**, 3879–3882.
- 7 E. F. Smith, *Mol. Biol. Cell*, 2002, **13**, 3303–3313.
- 8 I. H. Riedel-Kruse, A. Hilfinger, J. Howard and F. Jülicher, *HFSP J.*, 2007, **1**, 192–208.
- 9 I. S. M. Khalil, H. C. Dijkslag, L. Abelmann and S. Misra, *Appl. Phys. Lett.*, 2014, **104**, 223701.
- 10 Y. Xiao, J. Zhang, X. Zhao, B. Fang, L. Ma and N. Hao, *Sens. Actuators, A*, 2023, **361**, 114592.
- 11 Z. Peng, G. J. Elfring and O. S. Pak, *Soft Matter*, 2017, **13**, 2339–2347.
- 12 T. S. Yu, E. Lauga and A. E. Hosoi, *Phys. Fluids*, 2006, **18**, 091701.
- 13 T. S. Singh, P. Singh and R. D. S. Yadava, *Soft Matter*, 2018, **14**, 7748–7758.
- 14 Z. Liu, F. Qin and L. Zhu, *Phys. Rev. Fluids*, 2020, **5**, 124101.
- 15 Z. Liu, F. Qin, L. Zhu, R. Yang and X. Luo, *Phys. Fluids*, 2020, **32**, 041902.
- 16 S. Namdeo, S. N. Khaderi and P. R. Onck, *Phys. Rev. E: Stat., Nonlinear, Soft Matter Phys.*, 2013, **88**, 043013.
- 17 S. Namdeo, S. N. Khaderi, J. M. J. den Toonder and P. R. Onck, *Biomechanics*, 2011, **5**, 034108.
- 18 S. Sudo, S. Segawa and T. Honda, *J. Intell. Mater. Syst. Struct.*, 2006, **17**, 729–736.
- 19 I. S. M. Khalil, A. F. Tabak, Y. Hamed, M. Tawakol, A. Klingner, N. E. Gohary, B. Mizaikoff and M. Sitti, *IEEE Robot. Autom. Lett.*, 2018, **3**, 1703–1710.
- 20 A. A. Evans and E. Lauga, *Phys. Rev. E: Stat., Nonlinear, Soft Matter Phys.*, 2010, **82**, 041915.
- 21 V. Magdanz, I. S. M. Khalil, J. Simmchen, G. P. Furtado, S. Mohanty, J. Gebauer, H. Xu, A. Klingner, A. Aziz, M. Medina-Sánchez, O. G. Schmidt and S. Misra, *Sci. Adv.*, 2020, **6**, eaba5855.
- 22 I. R. Gibbons, *J. Cell Biol.*, 1981, **91**, 107s–124s.
- 23 C. Li, B. Chakrabarti, P. Castilla, A. Mahajan and D. Saintillan, *Phys. Rev. Fluids*, 2023, **8**, 113102.
- 24 K. Y. Wan and R. E. Goldstein, *Phys. Rev. Lett.*, 2018, **121**, 058103.
- 25 R. Dreyfus, J. Baudry, M. L. Roper, M. Fermigier, H. A. Stone and J. Bibette, *Nature*, 2005, **437**, 862–865.
- 26 B. J. Williams, S. V. Anand, J. Rajagopalan and M. T. A. Saif, *Nat. Commun.*, 2014, **5**, 3081.
- 27 S. Mohanty, Q. Jin, G. P. Furtado, A. Ghosh, G. Pahapale, I. S. M. Khalil, D. H. Gracias and S. Misra, *Adv. Intell. Syst.*, 2020, **2**, 2000064.
- 28 A. Gürbüz, K. Qin, J. J. Abbott and O. S. Pak, *Soft Matter*, 2023, **19**, 7100–7108.
- 29 O. A. Bauchau and J. I. Craig, in *Structural analysis. Solid mechanics and its applications*, ed. O. A. Bauchau and J. I. Craig, Springer, Dordrecht, 2009, vol. 163, pp. 173–221.
- 30 S. Timoshenko, *J. Opt. Soc. Am.*, 1925, 233–255.
- 31 A. S. Gladman, E. A. Matsumoto, R. G. Nuzzo, L. Mahadevan and J. A. Lewis, *Nat. Mater.*, 2016, **15**, 413–418.
- 32 O. S. Pak and E. Lauga, in *Fluid-Structure Interactions in Low-Reynolds-Number Flows*, ed. C. Duprat and H. Stone, 2015, pp. 100–167.

