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A molecular design strategy toward enzyme-activated probes with near-infrared I and II fluorescence for targeted cancer imaging†

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The advance of cancer imaging requires innovations to establish novel fluorescent scaffolds that are excitable and emit in the near-infrared region with favorable Stokes shifts. Nevertheless, the lack of probes with these optimized optical properties presents a major bottleneck in targeted cancer imaging. By coupling of boron dipyrromethene platforms to enzymic substrates *via* a self-immolative benzyl thioether linker, we here report a strategy toward enzyme-activated fluorescent probes to satisfy these requirements. This strategy is applicable to generate various BODIPY-based probes across the NIR spectrum *via* introducing diverse electron-withdrawing substituents at the 3-position of the BODIPY core through a vinylene unit. As expected, such designed probes show advantages of two-channel ratiometric fluorescence and light-up NIR (I and II) emission with large Stokes shifts upon enzyme activation, enabling targeted cancer cell imaging and accurate tumor location by real-time monitoring of enzyme activities. This strategy is promising in engineering activatable molecular probes suitable for precision medicine.

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Introduction

Scientists are in enthusiastic pursuit of novel assay techniques for targeted cancer imaging that could provide valuable insight into cancer diagnosis, treatment, and management.¹ Among the numerous analytical techniques, fluorescence imaging, due to its operational simplicity, high spatiotemporal resolution, and noninvasive capability, provides a powerful and popular tool for identification and enumeration of living cancers.² In this context, the past decades have witnessed the rapid development of versatile molecular fluorescent probes for detection of cancer-related biomarkers.³ Particularly, activatable molecular probes that generate fluorescence signals only in response to enzyme biomarkers of cancers have been reported for successful cancer imaging.⁴ However, most of the conventional fluorescent probes with emission in the visible light region encounter several challenges regarding strong autofluorescence and the scattering of short-wavelength light in living tissues

that significantly reduce the sensitivity of fluorescence imaging *in vivo*.⁵

An attractive approach for the detection of cancer biomarkers *in vitro* and *in vivo* is optical imaging in the near-infrared (NIR) range, offering a number of advantages, including less autofluorescence background, lower tissue absorption, better tissue penetration, and higher *in vivo* spatial resolution compared to visible imaging.⁶ Nevertheless, construction of small-molecule NIR fluorescent probes remains a significant challenge. Currently, several NIR probes to detect enzyme activities have been built based on cyanine and rhodamine scaffolds.⁷ However, these known NIR probes suffer from undesirable small Stokes shifts, which generally lead to severe cross-talk between the excitation and emission spectra that significantly compromises sensitive detection and accurate analysis.⁸ Thus, the advance of cancer-biomarker imaging requires innovations to establish novel fluorescent scaffolds that are excitable and emit in the NIR region with large Stokes shifts.

Here, we report a molecular design strategy that establishes a universal platform to access diverse enzyme-activated NIR fluorescent probes with desired optical properties. These activatable probes were engineered by coupling of BODIPY platforms to enzymic substrates *via* a self-immolative benzyl thioether linker (Fig. 1). The use of the benzyl thioether linker as a self-immolative spacer instead of the conventional benzyl ether can be ascribed to three reasons: (1) the ease of synthetic accessibility *via* the aromatic nucleophilic substitution (S_NAr)

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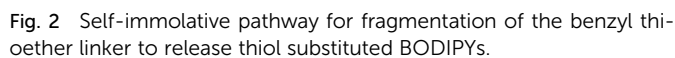
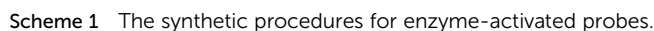
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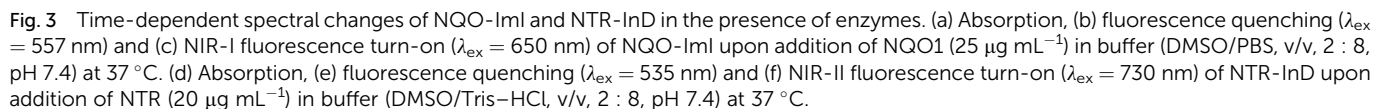
We then assessed the spectroscopic properties of probes NQO-ImI, NTR-ImI and ALP-ImI in the absence and presence of NQO1, NTR and ALP in aqueous solutions. For example, free NQO-ImI showed the typical features of BODIPY with absorption and emission at 557 nm and 635 nm ($\phi = 0.017$, Table S1†). Upon treatment with NQO1 (25 $\mu\text{g mL}^{-1}$) and the cofactor NADH (500 μM), a new absorption band around 675 nm emerged gradually (Fig. 3a), while the original absorption band of NQO-ImI at 557 nm was attenuated significantly, showing a remarkable red-shift of 118 nm. Interestingly, the fluorescence titration experiments demonstrated that NQO-ImI allowed the assay of NQO1 in both two-channel ratiometric and turn-on NIR fluorescence modes. Reaction of NQO-ImI and NQO1 elicited a time-dependent quenching of the fluorescence at 635 nm when the excitation wavelength was 557 nm (Fig. 3b). Fortunately, upon excitation at 650 nm or 675 nm, a new NIR emission at 725 nm ($\phi = 0.074$, Table S1†) with the Stokes shift of 50 nm was activated concomitantly (Fig. 3c), exhibiting a nearly 105-fold fluorescence intensity enhancement. In this context, the fluorescence intensity ratio at 635 and 725 nm (I_{725}/I_{635}) showed a 316-fold enhancement upon enzyme-catalyzed complete conversion (Fig. S2†). Of note, negligible fluorescence enhancement was found upon the pretreatment of NQO1

Chem. Sci., 2019, 10, 7222–7227 | 7223



rate (V_{\max}) of $64.10 \mu\text{M min}^{-1}$ (Fig. S4†). Similar optical responsiveness was observed for probes NTR-ImI and ALP-ImI with the exception of activation by NTR and ALP, respectively (Fig. S5–S10†). It should be noted that the maximal excitation and emission changed slightly upon varying the testing conditions. In addition, these designed probes exhibited good optical responsiveness to enzymes within a physiological pH range (pH 8 to approximately 6; Fig. S11†).

To further red-shift the absorption and emission and enlarge the Stokes shift, a stronger electron-withdrawing unit 3-ethyl-1,1,2-trimethyl-1*H*-benz[*e*]indolium instead of 1,2-dimethyl-1*H*-imidazol-5(4*H*)-one was appended to the BODIPY core through a vinylene unit, and probes NTR-InD, NQO-InD and ALP-InD were thus obtained. As predicted, enzymes initiated self-immolation in these probes and eventually led to formation of



InD-BOD-S that was excitable (730 nm) and emitted (900 nm) in the NIR region with a large Stokes shift of 170 nm (Fig. 3 and S12–S16†). Upon reaction with enzyme NTR (20 $\mu\text{g mL}^{-1}$), generation of NIR absorption at 730 nm was noted with a concomitant decrease of the band at 535 nm (Fig. 3d). Such treatment with enzymes made the emission at 612 nm (excitation at 535 nm) completely quenched within 5 min (Fig. 3e). Gratifyingly, a robust increase in the fluorescence intensity at 900 nm was observed when the excitation wavelength was 730 nm, producing a 12-fold increase (Fig. 3f). Importantly, these probes could exhibit enzyme-activated emission with a fluorescence tail in the region (1000–1300 nm) of NIR-II, which is preferable for *in vivo* cancer imaging as NIR-II imaging enables high-resolution bioimaging with deep-tissue penetration.¹² In addition, these probes and the NIR products ImI-BOD-S and InD-BOD-S showed good stability under testing conditions (Fig. S17 and S18†), indicative of the suitability for *in vivo* imaging. Collectively, all these optical advantages of such designed probes, including light-up NIR-II emissions with a large Stokes shift of 170 nm, make them a superior platform for *in vivo* cancer imaging.

After demonstrating the low cytotoxicity of our designed probes toward living cells (Fig. S19†), we then testified their capability for selectively identifying cancer cells by real-time tracking of enzyme activities. For evaluation of NTR activity, A549 cells were exposed to the probe NTR-ImI because such cells are known to overexpress NTR under hypoxic conditions.¹³ The treatment of A549 cells with NTR-ImI under normoxic conditions (20% O_2) led to bright fluorescence signals in the green channel and relatively moderate fluorescence signals in the red channel (Fig. 4). The fluorescence ratio of the red channel to green channel was found to be 0.8. In contrast, this fluorescence ratio ($I_{\text{red}}/I_{\text{green}}$) showed a time-dependent enhancement when A549 cells were incubated with NTR-ImI under hypoxia (1% O_2), for example, $I_{\text{red}}/I_{\text{green}}$ was markedly

increased to 1.6 when the incubation time was 1 h, suggesting significant activation of NTR-ImI by NTR to produce ImI-BOD-S in hypoxic cancer cells. These imaging experiments demonstrated that NTR-ImI is capable of monitoring NTR activity in dual-color imaging modality.

To explore the feasibility of visualization of cancer cells based on NQO1 activity, imaging experiments with HT-29 cells were performed. As shown in Fig. 4, HT-29 cells (high NQO1 activity)¹³ exhibited relatively faint fluorescence in the green channel and strong fluorescence in the red channel, resulting in a significant red-to-green signal ratio of 1.8. In contrast, addition of dicoumarol, an enzyme inhibitor, led to bright fluorescence in green and moderate emission in red channels. Such treatment with dicoumarol induced the red-to-green signal ratio to be significantly lowered, indicative of the fluorescence imaging signal indeed initiated by NQO1 activity. All these results implied that the designed probes can serve as a promising tool for targeted cancer cell imaging by real-time monitoring of enzyme activities in living cells.

The ability of the probes for *in vivo* targeted cancer visualization was subsequently evaluated. Fig. 5 illustrates the NIR imaging results of A549 subcutaneous xenograft nude mice treated with NTR-ImI and NTR-InD *via* intratumoral injection, respectively. Immediately after *in situ* probe administration, remarkable NIR fluorescence was collected specifically in the tumor region (Fig. 5a and b), while barely detectable fluorescence lighted up in the normal injection site, indicative of the rapid and specific activation of probes by tumor-derived enzymes. The fact that dicoumarol, an inhibitor of NTR, effectively attenuated the fluorescence signals in the tumor also demonstrated the vital role of NTR in tumors for selective activation of probes for targeted cancer imaging. The fluorescence signals in the tumor site gradually increased overtime



Fig. 4 Visualization of cancer cells by confocal microscopy imaging. A549 cells cultured with NTR-ImI (10 μM) under various oxygen concentration conditions. HT-29 cells or HT-29 cells pretreated with dicoumarol (0.5 mM) for 2 h were incubated with NQO-ImI (20 μM) for 2 h. Green channel at 600–670 nm with $\lambda_{\text{ex}} = 514$ nm excitation, red channel at 700–755 nm using $\lambda_{\text{ex}} = 633$ nm; ratio image was $F_{\text{red}}/F_{\text{green}}$. Scale bar = 50 μm .



Fig. 5 Targeted cancer visualization in the A549 tumor-bearing mouse model. (a) Time-dependent NIR-I imaging of mice injected with NTR-ImI (30 nmol) or NTR-ImI + dicoumarol (0.3 mmol). (b) Time-dependent NIR-II imaging of mice injected with NTR-InD (30 nmol) or NTR-InD + dicoumarol (0.3 mmol). (c) The fluorescence intensity of the tumor over the normal injection site in (a) and (b) *via* region of interest analysis. (d) Validation of the superiority of NIR-II over NIR-I imaging using NTR-InD and NTR-ImI in a simulated deep-tissue setting.



and eventually reached a plateau after 60 min post-injection. Interestingly, the fluorescence intensity of the tumor over the normal site (T/N) in NTR-InD treated mice was much higher than that of NTR-ImI treated ones at each post-injection time point (Fig. 5c), presumably due to greatly reduced auto-fluorescence and photon scattering in the NIR-II region.¹² It was clear that the T/N of NIR-II from NTR-InD injected mice was 10.6 (60 min), while that of NIR-I in NTR-ImI treated ones was only 1.5 (60 min). Furthermore, the advantage of NIR-II imaging with intrinsically deeper penetration over NIR-I imaging was also tested in a simulated deep-tissue setting (Fig. 5d and S20†). The results showed that the bright NIR-II signal from NTR-InD could be used to sensitively visualize A549 tumors even at a depth of 7 mm. In contrast, the tumor NIR-I fluorescence signal from NTR-ImI was undetectable above 3 mm. These results suggest that NIR-II imaging is reliable to provide precise location of tumors within deep tissues, which is difficult to achieve by visible and traditional NIR-I fluorescence imaging. It should be noted that cancers can also be rapidly visualized and differentiated by real-time and *in vivo* tracking of NQO1 activity with probes NQO-ImI and NQO-InD as a proof-of-concept (Fig. S21†). Taken together, these cancer biomarker-activated molecular probes could provide a powerful and popular tool for accurate identification of living cancers.

Live subject statement

Animal experiments were carried out in compliance with Chinese legislation on the Use and Care of Research Animals, and guidelines established by Fudan University Animal Studies Committee for the Care and Use of laboratory animals. All experimental procedures were approved by this committee.

Conclusions

In summary, we have established a universal platform to access diverse enzyme-activated NIR fluorescent probes for targeted cancer imaging. These activatable probes were constructed by coupling of BODIPY platforms to enzymic substrates *via* a self-immolative benzyl thioether linker. As proof-of-concept examples, enzymes (NTR, NQO1, and ALP) initiated the formation of the *p*-amino/hydroxybenzyl thioether linker and spontaneous 1,6-elimination reactions to release thiol-substituted BODIPYs that can be facilely derivatized *via* tuning the electron-withdrawing power of the substituents appended at the 3-position of the BODIPY core. In this way, the design strategy allows access to novel fluorescent scaffolds that are excitable and emit in the NIR (I and II) region with favorable Stokes shifts. Interestingly, such designed probes were capable of targeted cancer cell imaging and differentiation by real-time monitoring of enzyme activities. More importantly, *in vivo* targeted cancer imaging implied that these biomarker-activated molecular probes could provide a powerful tool for accurate identification. In light of the promising features, further study toward the optimization of the molecular structure to endow probes with good water solubility by appending hydrophilic units or utilizing the supramolecular assembly approach is

currently underway. To our knowledge, enzyme-activated probes with the aforementioned favorable responsiveness are highly limited. It is anticipated that our design approach can be generalizable for customization of a wide range of activatable probes with optimized optical properties, thus facilitating targeted cancer diagnostics.

Conflicts of interest

The authors declare no competing financial interest.

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