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Thermoresponsive block copolymers of increasing architecture complexity: a review on structure—property relationships

Controlling the transition temperature of thermoresponsive polymers can be critical for their applicability. It is well documented that factors like the polymer molar mass and composition affect this, but it is less so how the architecture affects this. This review summarises how the position of the monomer units within the polymer structure and the 3-D topology of the polymer affect the thermoresponsive properties of the polymers in aqueous solutions.
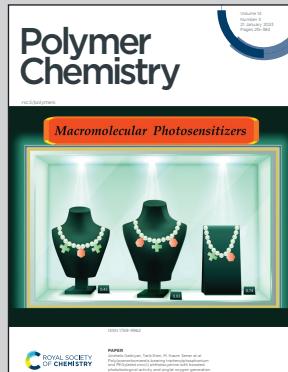
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Thermoresponsive block copolymers of increasing architecture complexity: a review on structure–property relationships

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Thermogels are an exciting class of stimuli responsive materials with many promising applications ranging from the medical field to additive manufacturing. This review focuses on the structure–property relationship of thermoresponsive block copolymers, with emphasis on the effect of architecture. Polymers based on Pluronic®, *N*-isopropylacrylamide, oligo(ethylene glycol) (meth)acrylate units, and 2-oxazoline units, which are amongst the most studied thermoresponsive units, are discussed. The effect of the polymer's architecture is crucial for controlling the thermoresponsive properties, such as cloud point and gelation temperature.

Introduction

Thermoresponsive polymers, also called temperature-responsive polymers, are polymers which exhibit a drastic change in their solubility as a response to temperature. When reduction in solubility at elevated temperatures is detected, this behaviour is

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2019). She has been working on well-defined polymers, specialising on thermoresponsive gels for biomedical applications. After her PhD studies, she was awarded an EPSRC Doctoral Prize fellowship (2018–2019) to work on in-depth physicochemical characterisation and drug delivery applicability of thermogels. She then worked as a Research Associate exploring the use of well-defined polymers in antibacterial and emulsion applications in Prof. Theoni K. Georgiou's group until April 2022. She is now a Research Associate for Professor Molly Stevens, working on polymers for biomedical applications.

Lezhi Wang

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characterised as a lower critical solution temperature (LCST) behaviour, while an upper critical solution temperature (UCST) is presented when the solubility is enhanced upon heating. This change in solubility can be manifested by means of (i) cloud point (CP), *i.e.*, the solution turns cloudy/opaque, (ii) precipitation, *i.e.*, complete phase separation to a solid (polymer) and a liquid (solvent), and (ii) gelation, *i.e.*, formation of a 3-D polymer network, Fig. 1, for LCST-type systems. The evolution of the CP with the concentration is depicted as a parabolic curve with the minimum corresponding to the LCST, Fig. 1(a), even though the terms CP and LCST are often used interchangeably in the literature. Similarly, a parabolic curve with a maximum is representative of the UCST-type behaviour. An appropriate combination of the polymer structure and the solvent triggers a reversible transition from solution to gel, which is favoured at higher concentrations, Fig. 1(b). These systems are widely known by the terms thermoresponsive gels, thermoreversible gels, thermogelators, and thermogels. Further heating of the gel might lead to destabilisation, such as gel syneresis, *i.e.*, exclusion of the solvent from the gel matrix due to internal stresses, and precipitation.

The LCST behaviour is attributed to the "hydrophobic effect".[1,2] Thermodynamically speaking, an increased change in the entropy of the system (ΔS) takes place upon heating, which contributes to lowering the Gibbs free energy (ΔG):

$\Delta G = \Delta H - T\Delta S$. In more detail, when the temperature of the thermoresponsive polymer solution increases, the interactions, such as hydrogen bonding (if any), between the polymer and the water molecules are weakened, and the entropic contribution of the water increases.[1,2] Therefore, driven by the change in the entropy of the system, a thermoresponse takes place, during which the separation between the polymer chains and the water molecules occurs, Fig. 2.

Thermoresponsive polymers have a wide range of applications, from biomedical applications, like drug delivery and tissue engineering,[3–6] to catalysis,[7–9] purification,[10,11] and additive manufacturing (3D printing) and fabrication of 3-D structures and objects,[12,13] Fig. 3. In the healthcare sector, the scientific interest has been focused on LCST-type systems, as the structural integrity of biologicals, such as proteins, genes, drugs, and cells, is preserved throughout the temperature window of the application. Tissue engineering and drug delivery are amongst the most popular applications of thermoresponsive gels with the LCST, which are used as depots for tissue regeneration or sustained and topical delivery, respectively.[5] Injectability is a key feature which makes thermoresponsive gels popular candidates in biomedical engineering as they offer a minimally invasive alternative to traditional implantation.[14] In addition to this, the high content of water and the soft tissue-resembling properties support their suitability in the tissue
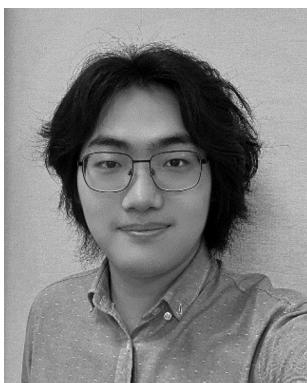
Mr Shaobai Wang obtained his BEng degree in Polymer Materials and Engineering from South China University of Technology in 2016, and an MSc degree in Advanced Materials Science and Engineering from Imperial College London in 2021. In 2022 he started his PhD studies under the supervision of Professor Theoni K. Georgiou. His PhD thesis focuses on stimuli responsive polymeric materials for biomedical applications.

Shaobai Wang

Professor Theoni K. Georgiou obtained a PhD in Polymer Chemistry under the supervision of Professor Costas Patrickios at the University of Cyprus in 2006. She then worked as a Postdoctoral Fellow under the supervision of Professor Antonios Mikos at Rice University, USA. In 2007 she moved to the University of Hull as a Research Councils of UK (RCUK) Academic Fellow. In 2014 she joined the Department of Materials at Imperial College

Theoni K. Georgiou

London as a Lecturer where she is now a Professor in Polymer Chemistry. She is an expert in the synthesis and characterisation of well-defined polymers of various architectures with a special focus in group transfer polymerisation (GTP). She has special interest in thermoresponsive polymers and specifically thermogels and how these can be tailored by varying the polymer chemistry, molar mass and polymer architecture. In 2017 she was awarded the 2016 Macro Group UK Young Researchers Medal for "contributions to polymer science which show outstanding promise for the future". She is an active member of the polymer community. Specifically, she has served as the Chair of Macrogroup UK (2019–2022), is a member of the editorial board for several polymer journals and is an Associate Editor for European Polymer Journal.
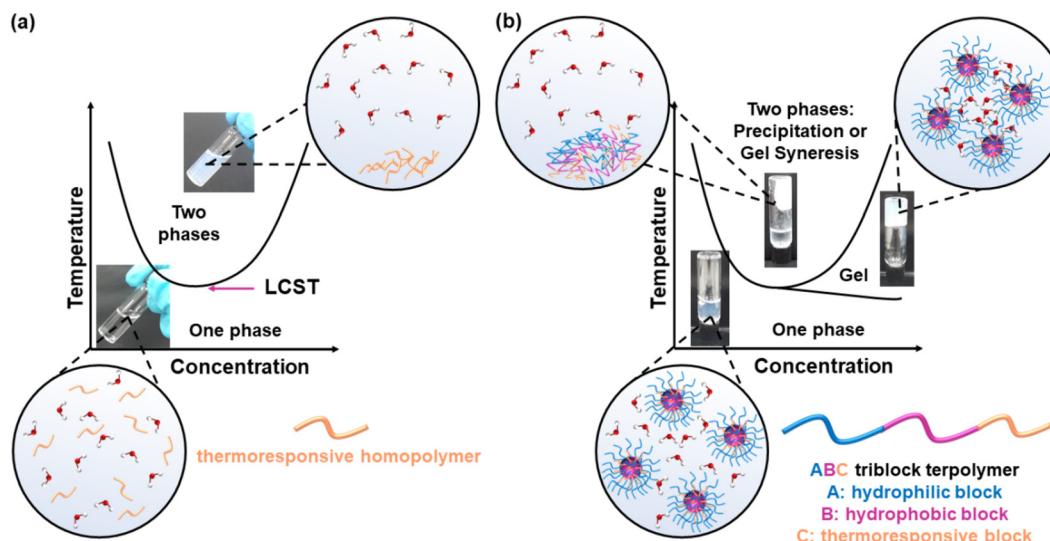
Fig. 1 Phase diagrams of (a) an aqueous solution of a thermoresponsive homopolymer presenting LCST behaviour and (b) an aqueous solution of a thermoresponsive ABC triblock terpolymer with LCST type thermogelling behaviour; A, B, and C blocks are shown in blue, purple, and orange, respectively.
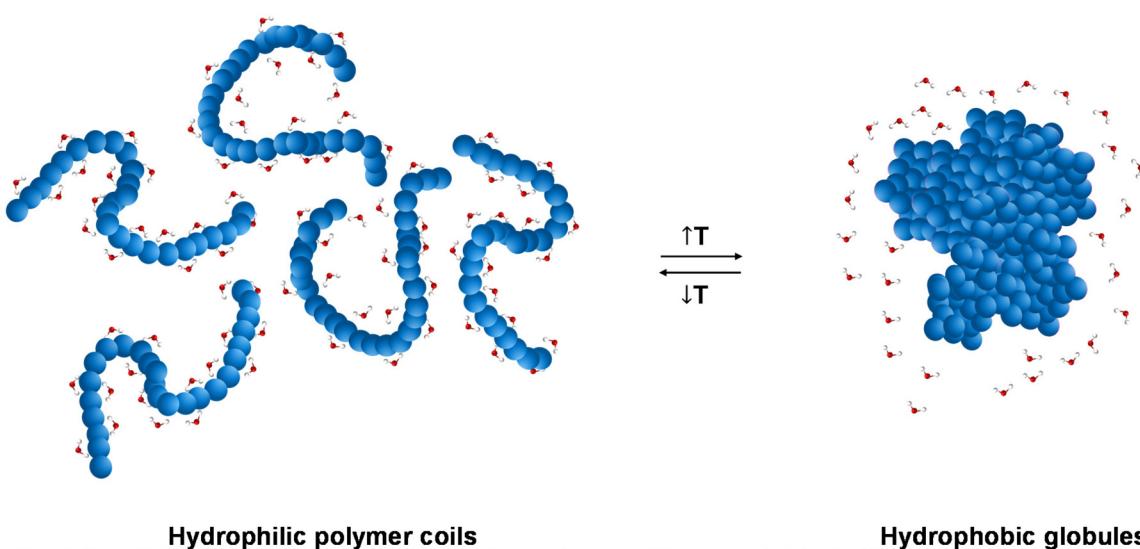
Fig. 2 Schematic illustration of the "hydrophobic effect", with a transition from hydrophilic polymer coils below the LCST to hydrophobic globules above the LCST.

engineering field.[15] Thus, this literature review focuses on summarising and discussing LCST-type polymers.

LCST-type thermoresponsive units

Several LCST-type thermoresponsive units, whose homo- or co-polymerisation produces thermoresponsive polymers have been well established in the literature. Amongst the most popular ones are *N*-isopropylacrylamide (NIPAAm) and ethylene glycol (EG), often combined with propylene glycol (PG), *e.g.*, Pluronic® polymers.[16] Other units presenting LCST-type

thermorespose are 2-(dimethylamino) ethyl methacrylate (DMAEMA),[17] EG-based (meth)acrylate units,[17,18] and *N*-vinylcaprolactam (VCL).[19] 2-Oxazoline-[20] and peptide-based thermoresponsive polymers have also been reported. The chemical structures, names and abbreviations of these units are shown in Fig. 4.

Block copolymers

It is widely accepted that block copolymers, defined as "polymers composed of block macromolecules",[21] have gained
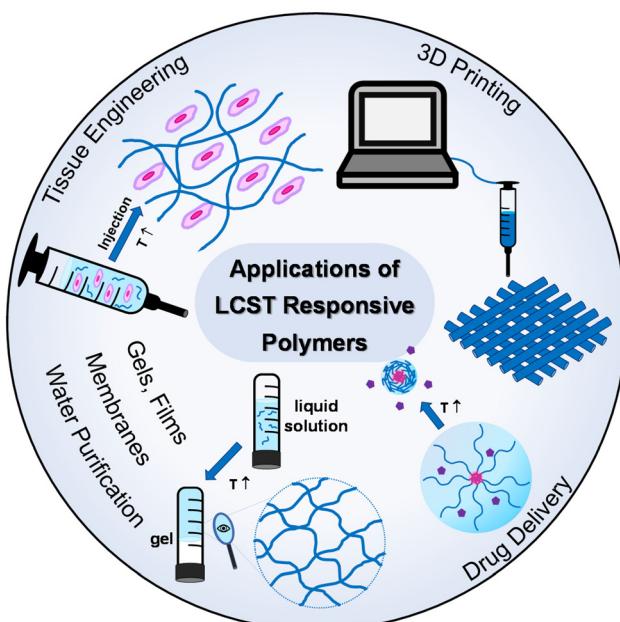
Fig. 3 Applications of thermoresponsive polymers with a lower critical solution temperature (LCST).

popularity over statistical copolymers, despite the ease in the synthesis of the latter. It is well known that the architecture governs the final properties, and several advantages of the block copolymers have been well established. Amphiphilic block copolymers, *i.e.*, polymers with both hydrophilic and hydrophobic blocks, self-assemble into well-ordered structures when dissolved in water, such as micelles of various shapes,

including spherical core–shell micelles, flower-like micelles, and polymersomes, Fig. 5. The size of the self-assembled structures depends on the polymer characteristics, such as molar mass and composition,[22] while the type and shape, such as spherical *versus* worm-like,[23] or micelles *versus* polymersomes/polymer vesicles,[24] can be controlled by varying the comonomer composition (hydrophilic/hydrophobic ratio) and the preparation method. Polymersome formation can also be temperature-driven, as previously reported for ABC triblock copolymers based on EG (A block), a random copolymer of EG and butylene glycol (B block), and isoprene (C block), respectively.[25] In these self-assembled structures, the hydrophobic blocks interact with each other, thus avoiding interactions with water, while the hydrophilic ones interact with water, either *via* hydrogen bonding, ion–dipole, or dipole–dipole interactions. Adopting such configurations enhances the water solubility, in contrast to the statistical copolymers, which do not self-assemble into well-ordered structures, due to the lack of distinct hydrophobic and hydrophilic blocks. In addition, hydrophobic drugs can be solubilised in the hydrophobic part of these self-assembled structures, thus enabling these structures to act as drug delivery vehicles. Block copolymers also favour the formation of physical gels *via* interconnection of the micelles, with their statistical counterparts being unable to form gels or the gels formed are less stable.[26,27] Physical gels have been extensively studied by researchers in the tissue engineering and drug delivery fields for curing numerous diseases, such as cancer and diabetes, thus highlighting the significance of studying block copolymers.

Block copolymers can be categorised by the number of blocks, with thermoresponsive diblock copolymers being the
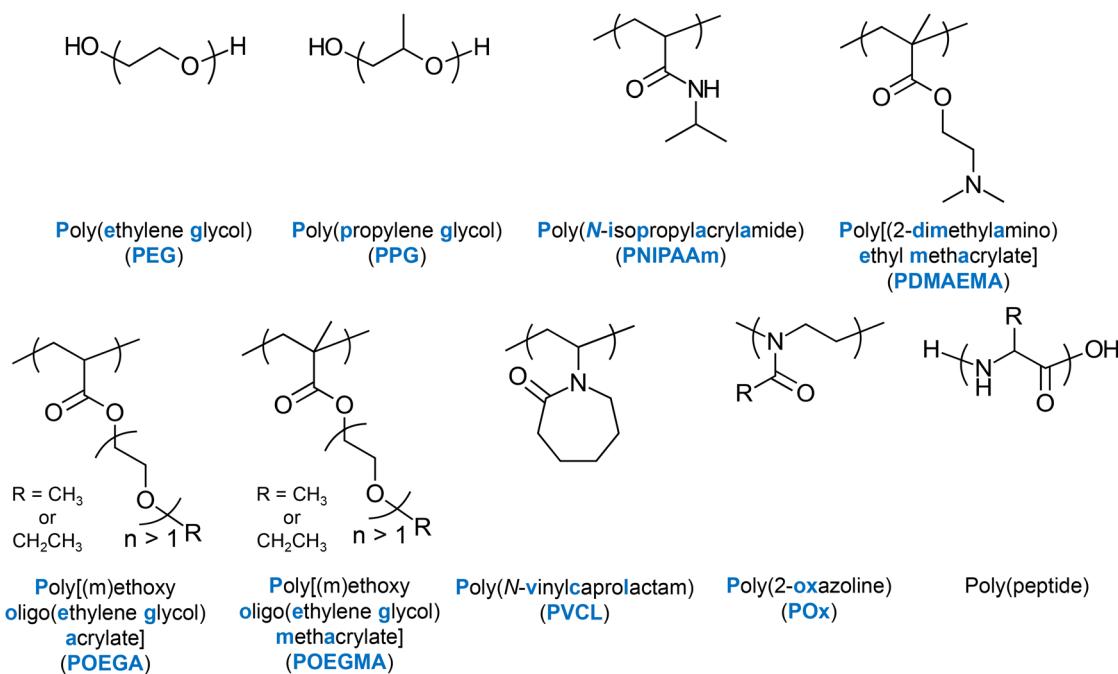
Fig. 4 Chemical structures, names, and abbreviations (if any) of the main thermoresponsive polymers reported in the literature.

(a) Core–Shell Micelle　**(b) Flower-like Micelle**　**(c) Polymersome**

AB *or* ABA　ABC　BAB　AB

A: hydrophilic　B: hydrophobic　C: hydrophilic
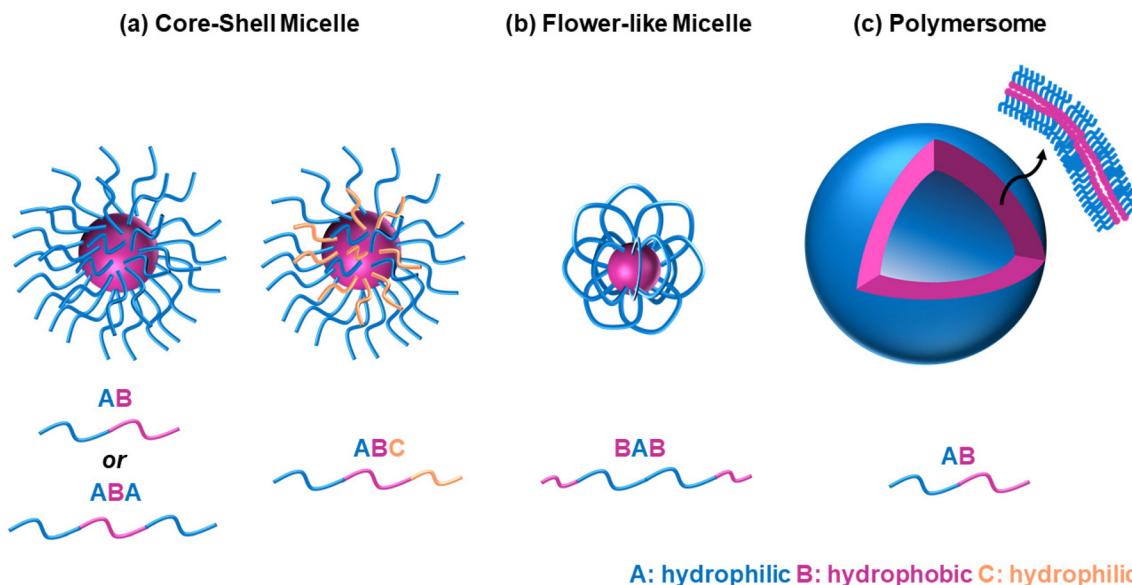
Fig. 5 Self-assembled structures adopted by amphiphilic block copolymers: (a) core−shell micelles by the AB, ABA, and ABC architectures, (b) flower-like micelles by the BAB architecture, and (c) polymersomes by the AB architecture. Blue and purple represent the hydrophilic and hydrophobic blocks, respectively, while when a second hydrophilic block is present, this is shown in orange. In the self-assembled structures, the compact hydrophobic part is represented by purple spheres.

most commonly reported because they are the easiest to make. Thermoresponsive triblock bipolymers, *i.e.*, polymers with three blocks and two different repeating units, namely ABA, have been extensively studied, with the thermoresponsive gels applied in clinical trials falling into this category. These are Pluronic® F127 (A = EG and B = PG) and ReGel® (A = poly (L-lactide-*co*-glycolide, PLGA, and B = EG). Thermoresponsive triblock terpolymers, *i.e.*, polymers with three blocks, each consisting of a different repeating unit, have also been studied, but fewer studies have been reported, due to their more difficult synthesis, as discussed in the following section. Increasing the complexity of the architecture to tetrablock (four blocks), pentablock (five blocks), hexablock (six blocks), heptablock (seven blocks), *etc.* opens new possibilities for developing novel thermoresponsive polymers with exciting self-assembling properties. Therefore, this review focuses on summarising and discussing studies on thermoresponsive multiblock copolymers, *i.e.*, block copolymers with more than two blocks, and the effect of temperature on their self-assembly and gelation properties. Each section summarises studies based on the same thermoresponsive unit, and the studies are discussed based on the increasing complexity of architecture, as can be seen in Table 1. The effect of architecture on the properties is identified and conclusions are drawn, whenever possible.

Da Silva *et al.* reported the synthesis and investigation of a library of ABA triblock copolymers consisting of PEG as the B central block and two thermoresponsive outer A blocks, varying from NIPAAm, to DMAEMA, to methoxy di(ethylene glycol) methacrylate (mDEGMA).[28] Extensive SANS measurements revealed that the self-assembly at the nanoscale driving

the thermogelling properties was highly depended on the MM of the blocks and the chemical nature of the thermoresponsive unit. Gels with a sharp sol–gel transition were formed by the mDEGMA- and NIPAAM-based analogues when the MM of the blocks was targeted to 10 kDa (B block) and either 10 or 20 kDa (A block). These copolymers adopted spherical or ellipsoid micellar structures, and the network formation was attributed to the bridging of the flower-like micelles by unimers.[28]

Synthetic approaches

The synthesis of block copolymers has been more challenging compared to statistical copolymers, as it requires multiple and controlled synthetic steps, and thus it has only been achieved with the discovery of living and controlled polymerisation techniques. These techniques include, but are not limited to, anionic polymerisation, ring opening polymerisation (ROP), group transfer polymerisation (GTP), reversible addition–fragmentation chain-transfer (RAFT) polymerisation, and atom transfer radical polymerisation (ATRP). The synthesis of block copolymers *via* these techniques is carried out in a controlled manner, with sequential addition of monomers leading to chain extension, which is possible due to the living/controlled nature of these polymerisation techniques. In 2016, Gody *et al.* published a report on the experimental requirements of chain growth polymerisation techniques that are needed to precisely control the polymer structure.[29] They reported that a minimum degree of polymerisation of 6 is required for producing icosablock copolymers with 95% fidelity, *i.e.*, to ensure

Table 1 The general category of thermoresponsive copolymers, the polymer architecture, and the comonomer(s) used

Main category of thermoresponsive polymers		Architecture	Comonomer(s)	Ref.
Pluronic® (EG/A and PG/B)		Triblock (ABA/BAB)	—	32–38
		Pentablock	DEAEMA, tBAEMA, DMAEMA, DiPAEMA, NIPAAm	39–49
		Multiblock	—	50
EG-containing degradable		Triblock (ABA/BAB)	LA, GA, CL & derivatives, depsipeptides	51–71
		Pentablock	CL, LA, L-lysine, L-histidine, γ-benzyl-L-glutamate	72–74
		Hyperbranched	PG, CL	75
		Multiblock	PG, 1,4-butylene adipate, betulin	76, 77
		Alternating block	Hydrophobic polyesters	78
Acrylamide	NIPAAm	Triblock (ABA/BAB)	St, tBuSt, BrBzA, EtHexA, OcDecA, AA & derivatives, DMAAm, Adac, ionic liquid, EG, VP, betaine ester, TEMPO, HTPB, HEMA, EtA	79–94
		Triblock (ABC)	CL, MA-POSS, mPEGV, St, MAGlc, HEMA, EG, LA, ethylene, propylene, BuA, NAM, NBOCAEMA, DEAEA, mOEGA480	95–107
		Tetrablock	DMAAm, EG, St, DMAEMA	108, 109
		Pentablock	DEAEMA, EG, DEAAm, PG, AA, tBA	110–114
		Multiblock	EG, DEAAm	115
		Star	EG, [R]-3-hydroxybutylate, PEGMA-co-PPGMA	116 and 117
	DEAAm	Triblock (ABA)	EG	118
		Triblock (ABC)	EG, DiBuAAm	119
Amine - DMAEMA		Triblock (ABA/BAB)	6-O-methacryloyl-D-galactopyranose, BuMA	120–122
		Triblock (ABC)	mDEGMA, TEGMA, mOEGMA300, mOEGMA500, MMA, EtMA, BuMA, HexMA	26 and 123–126
		Tetrablock	OEGMA300, BuMA	127
		Pentablock	BuMA	128
		Heptablock		
		Nonablock		
		Graft	VB, CL	129
EG-based (meth)acrylate	mDEGMA	Triblock (ABA/BAB)	mOEGA480, HEMA, MPC	130–132
		Triblock (ABC)	mPEG, HMAAm, DEAEMA, eDEGMA, MAEtMAm, RhoMA, BuMA, mOEGMA300	133–136
		Tetrablock	mOEGMA300, BuMA	137
		Star	mOEGA480, mOEGMA500, CL	130 and 138
	mTEGMA	Pentablock	EG, DMAEMA, BuMA	139
	mOEGMA300	Triblock (ABC)	BuMA, DEAEMA	140
	mOEGMA500	Triblock (ABA/BAB)	CL	141
	mMEGA	Triblock (ABA/BAB)	HEA	142
	mDEGA	Triblock (ABA/BAB) Star	St	143–145
	eDEGA	Triblock (ABA/BAB)	mOEGA480	146
Other	VCL	Triblock (ABA/BAB)	VP, tBA, AA	147–149
	Polypeptides	Tetrablock	Amino acids	150
	EtOx	Triblock (ABA/BAB)	LA, CL	151
	nProOx	Triblock (ABA/BAB)	EtOx, MeOx	152 and 153
	iProOx	Triblock (ABA/BAB)	MeOx, BuOx	154
	MeOx & iBuOx	Triblock (ABA/BAB)	—	155

Abbreviations (in the order they appear in the Table): EG, ethylene glycol; PG, propylene glycol, DEAEMA, 2-(diethylamino)ethyl methacrylate; tBAEMA, 2-(t-butylamino)ethyl methacrylate; DMAEMA, 2-(dimethylamino)ethyl methacrylate; DiPAEMA, 2-(diisopropylamino)ethyl methacrylate NIPAAm, N-isopropylacrylamide; LA, lactic acid; GA, glycolic acid; CL, ε-caprolactone; St, styrene; tBuSt, 4-t-butylstyrene; BrBzA, 3,5-dibromobenzyl acrylate; EtHexA, 2-ethylhexyl acrylate; OcDecA, octadecyl acrylate; AA, acrylic acid; Adac, adamantane acrylate; VP, N-vinylpyrrolidone; TEMPO, 2,2,6,6-tetramethylpiperidine-1-oxyl; HTPB, hydroxyterminated polybutadiene; HEMA, 2-hydroxyethyl methacrylate; EtA, ethyl acrylate; MA-POSS, 3-methacryloxypropylheptaphenyl polyhedral oligomeric silsesquioxanes; mPEGV, poly(ethylene glycol) methyl ether vinylphenyl; MAGlc, poly(3-O-methacryloyl-α,β-D-glucopyranose; BuA, n-butyl acrylate; NAM, 4-acryloylmorpholine; NBOCAEMA, 2-(((((2-nitrobenzyl)oxy)carbonyl)amino) ethyl methacrylate; DEAEA, 2-(dimethylamino)ethyl acrylate; mOEGA480, methoxy oligo(ethylene glycol) acrylate with an average M_n of 480 g mol⁻¹; DMAAm, N,N-dimethylacrylamide; DEAAm, N,N-diethylacrylamide; PEGMA-co-PPGMA, poly(ethylene glycol) methacrylate-co-poly(propylene glycol) methacrylate; DiBuAAm, N,N-dibutylacrylamide; BuMA, n-butyl methacrylate, mDEGMA, methoxy di(ethylene glycol) methacrylate; TEGMA, tri(ethylene glycol) methyl ether methacrylate; mOEGMA300, methoxy oligo(ethylene glycol) methacrylate with an average M_n of 300 g mol⁻¹; mOEGMA500, methoxy oligo(ethylene glycol) methacrylate with an average M_n of 500 g mol⁻¹; MMA, methyl methacrylate; EtMA, ethyl methacrylate; HexMA, n-hexyl methacrylate, VB, 4-vinyl benzyl; mTEGMA, methoxy tri(ethylene glycol) methacrylate; mMEGA, methoxy mono(ethylene glycol) acrylate; mDEGA, methoxy di(ethylene glycol) acrylate; eDEGA, ethoxy di(ethylene glycol) acrylate; MPC, 2-methacryloyloxyethyl phosphorylcholine; mPEG, monomethoxy poly(ethylene glycol); HMAAm, N-hydroxymethyl acrylamide; eDEGMA, ethoxy di(ethylene glycol) methacrylate; MAEtMAm, 2-(methacryloyloxy)ethyltrimethylammonium iodide; RhoMA, rhodamine-containing methacrylate; HEA, 2-hydroxyethyl acrylate; VCL, N-vinylcaprolactam; tBA, t-butyl acrylate; EtOx, 2-ethyl-2-oxazoline; nProOx, 2-n-propyl-2-oxazoline; iProOx, 2-isopropyl-2-oxazoline; MeOx, 2-methyl-2-oxazoline; BuOx, 2-butyl-2-oxazoline; iBuOx, 2-isobutyl-2-oxazoline.

that each polymer chain contains at least one repeating unit for the targeted block.[29]

The difficulty of the synthesis relies on several factors, such as the number of blocks and the symmetry of the structure. While diblock copolymers are easily synthesised *via* a two-step synthetic procedure, the synthesis of multiblock copolymers is more complicated, as has been highlighted by a recent review by Becer's group,[30] because the polymer chain should be extended without termination. In reality, termination might be detected, but this should be kept at minimum to ensure that the molar mass distribution of the final polymer is mono-modal, *i.e.*, polymer chains from different synthetic steps do not co-exist, thus ensuring reproducibility of the properties. The conventional way of synthesising block copolymers is sequential polymerisation by using a monofunctional initiator, thus resulting in unidirectional growth of the polymer chain. Triblock terpolymers (ABC), tetrablock ter- and quater-polymers, *etc.* are inevitably synthesised using a monofunctional initiator, thus increasing the complexity of their synthesis, evident from the limited studies published. On the other hand, a bifunctional initiator can be used for the synthesis of symmetric polymers, such as ABA triblock bipolymers and ABCBA pentablock terpolymers, to complete the synthesis in two and three steps, respectively, instead of the three and five

steps needed, respectively, when using a monofunctional initiator. Another approach that has been followed to synthesise ABCBA pentablock terpolymers is the conversion of a commercially available triblock bipolymer to a bifunctional initiator, followed by chain growth and consequent formation of a pentablock terpolymer in only one step. A combination of polymerisation techniques might be adopted to obtain the desired polymer structure. For example, for synthesising ABA triblock copolymers based on NIPAAm and poly(2-ethyl-2-oxazoline), Sahn *et al.* synthesised the middle oxazoline-based block *via* living cationic ring-opening polymerisation, while RAFT polymerisation facilitated the synthesis of the outer NIPAAm-based blocks.[31] These synthetic routes are illustrated schematically in Fig. 6.

Characterisation methods

Monitoring the polymer synthesis and characterising the polymer structure are necessary, with gel permeation chromatography (GPC) and nuclear magnetic resonance spectroscopy (NMR) being the most popular techniques amongst polymer chemists. Thus, GPC and NMR are normally used to monitor and confirm the molar mass and composition of the polymers,
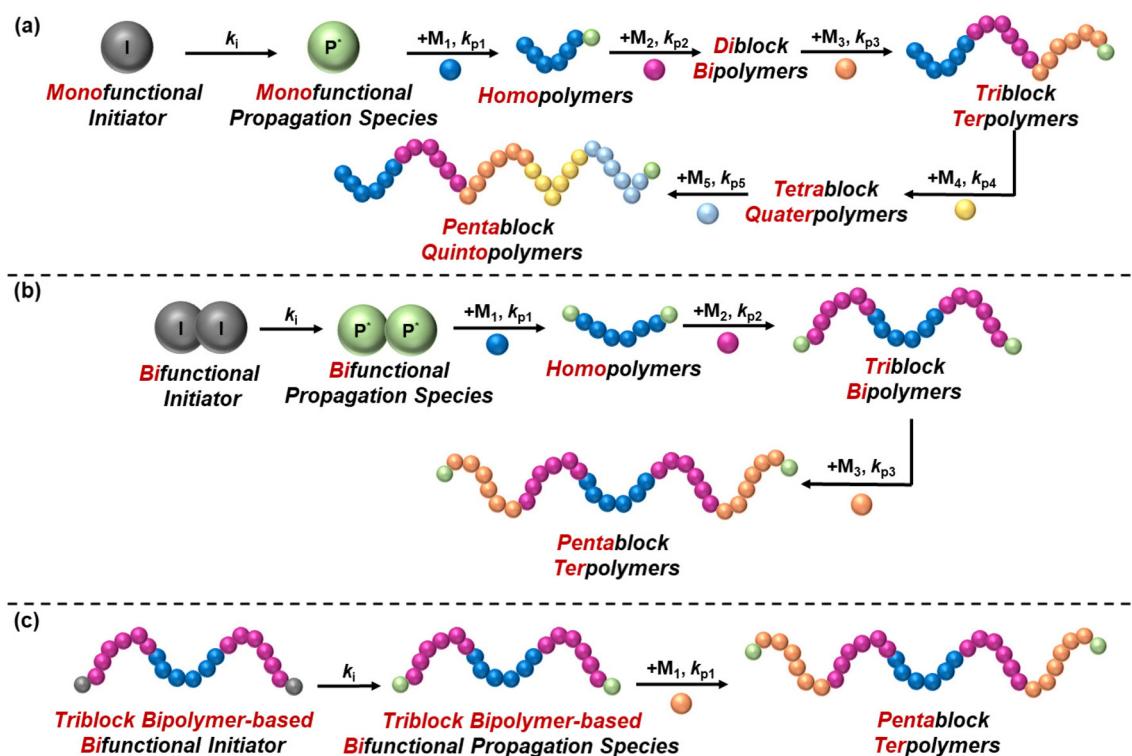

Fig. 6 Common synthetic approaches followed for the synthesis of thermoresponsive block copolymers: (a) synthesis of block copolymers using a monofunctional initiator, with unidirectional chain extension taking place upon addition of a different monomer. The chain growth from a homopolymer to a pentablock quintopolymer is given as an example. (b) Synthesis of block copolymers using a bifunctional initiator, with bidirectional chain growth taking place upon addition of a different monomer. The chain growth from a homopolymer to a symmetrical pentablock terpolymer is shown. (c) One-step synthesis of pentablock terpolymers using a triblock bipolymer–based bifunctional initiator, obtained by modification of a commercially available triblock bipolymer, with bidirectional chain growth.

(a) Determination of the Cloud Point (CP)

(i) Visual tests

(ii) UV-Vis Spectroscopy

(iii) Dynamic Light Scattering (DLS)

(b) Determination of the Gelation Temperature (T_{gel})

(i) Visual tests

(ii) Rheology

Fig. 7 (a) Determination of the cloud point (CP) by (i) visual tests, as the temperature at which the solution turns cloudy, (ii) UV-Vis spectroscopy, as the temperature at which the transmittance drops to 50%, and (iii) dynamic light scattering (DLS), as the temperature at which 50% aggregation occurs. (b) Determination of the gelation temperature (T_{gel}) by (i) visual tests, as the temperature at which the sample does not flow upon tube inversion, and (ii) rheology, as the temperature at which the shear storage (shear elastic) modulus, G', overcomes the shear loss (shear viscous), G'', modulus. * The y axis indicated should be plotted in a logarithmic scale.

respectively. The following paragraphs will focus on how the thermoresponsiveness of the polymers is studied.

The thermoresponse of the polymers in solution can be monitored *via* a plethora of techniques, Fig. 7. Temperature-driven cloudiness/turbidity is detected visually or by ultraviolet-visible (UV-Vis) spectroscopy; the CP is determined by UV-Vis as the temperature at which the transmittance drops to 50%. A complementary technique for determining the CP is differential scanning calorimetry (DSC), including microDSC, with the phase separation presented as an endothermic peak on the DSC thermogram.[47,48,156,157] The effect of temperature on the self-assembly of thermoresponsive polymers has also received much attention, with dynamic light scattering (DLS) being used as an indication of the presence and size of the unimers (free polymer chains in solution), micelles or bigger aggregates, and static light scattering (SLS) being used to determine the aggregation number. DLS temperature ramps can also be performed to determine the CP as the temperature at which aggregation occurs at 50%. However, one should keep in mind that the theory of DLS assumes spheres; thus more powerful techniques, such as small-angle neutron scattering (SANS) and small-angle X-ray scattering (SAXS), could be used to determine more accurately the shape and size of the self-assembled structures. Gel formation as a response to tempera-

ture can be easily determined by the tube inversion method, as the temperature at which the sample does not flow when the vial is inverted, indicating a solid-like material. Rheological measurements can also detect the gelation temperature (T_{gel}), which is defined as the temperature at which the shear elastic modulus (also called the storage modulus, G') overcomes the shear viscous modulus (also called the loss modulus, G''), thus indicating a temperature-driven transition from a free-flowing solution to an elastic gel. In addition to the T_{gel}, rheology provides further insight into the rheological properties of the sample, such as the strength of the gel, gel destabilisation, and changes in the viscosity of the sample as a response to temperature when no gelation is detected. Both techniques determining the gelation are complementary and should be applied for a complete study.

Pluronic®-based polymers

Pluronic® polymers are commercially available thermoresponsive polymers with temperature driven micellisation, aggregation, and gelation. As previously mentioned, these polymers are ABA triblock copolymers with A and B being based on EG and PG, respectively. It has been previously

reported that the critical gelation concentration (CGC) and T_{gel} of these polymers decrease with the increase in MM,[32,33] as expected, since the viscosity of a polymer solution increases with its MM (Mark–Houwink's equation[21]). On the other hand, a decrease in the CP of Pluronic® solutions is observed with a decrease in MM.[34] When comparing Pluronic® polymers (ABA) with their reverse counterparts (BAB), known as reverse Pluronic® polymers, it is generally concluded that the CP of the ABA-type polymers increases with increasing polymer concentration, while the opposite trend is reported for the BAB-type polymer.[35] For example, while the CP of Pluronic® L44 (EG_{10}-b-PG_{23}-b-EG_{10}) increases from 62 °C (at 2 mM) to 73 °C (at 50 mM), the CP of reverse Pluronic® 10R5 (PG_8-b-EG_{22}-b-PG_8) decreases from 74 °C (at 2 mM) to 58 °C (at 50 mM).[35] Similar observations were made for Pluronic® L64 (EG_{13}-b-PG_{30}-b-EG_{13}), with the CP increasing from 52 °C (at 1 w/v%) to 58 °C (25 w/v%).[36] In a study by Zhou and Chu,[37] Pluronic® L64 was compared to reverse Pluronic® 17R4 (PG_{14}-b-EG_{24}-b-PG_{14}), and it was found that the ABA triblock bipolymer forms micelles in a wider range of temperatures and concentrations, while its BAB counterpart presents only a narrow window of micelle formation under the same conditions.[37] In addition to this, the CPs of the BAB are lower than the ones of the ABA polymer.[37] These observations indicate an architecture effect on the micellisation and CP, with the ABA triblock bipolymer forming more stable micelles in wider temperature and concentration ranges compared to the BAB one, presumably due to the entropically more favourable self-assembly into core–shell micelles (ABA), as opposed to the flower-like micelles (BAB).

Well-defined reverse Pluronic® polymers have been synthesised by Markus *et al. via* organocatalytic polymerisation; the *Đ* values varied from 1.02 to 1.07.[38] The MM of the middle hydrophilic block ranged from 4 to 20 kg mol^{-1}, while the DP of the outer hydrophobic blocks varied from 12 to 128. Copolymers with 20 kg mol^{-1} middle block and the DP of the outer blocks varying between 77 and 128 formed gels with an exceptionally high storage modulus, which is tenfold relative to Pluronic® F127. In addition, gel formation was detected at three times lower gelation concentration than Pluronic® F127.[38] Even though the authors have attributed these superior thermogelling properties to both the increased MM and BAB architecture, for clear trends to be established, a comparison should be made between copolymers differing in only one structural parameter.

Mallapragada and co-workers have previously reported the synthesis and investigation of thermoresponsive pentablock terpolymers with Pluronic® F127 (EG_{99}-b-PG_{66}-b-EG_{99}, MM ≈ 12 400 g mol^{-1}) as a central triblock terpolymer.[39–46] The synthesis of the pentablock terpolymer was carried out by bidirectional chain-extension of Pluronic® F127, *via* ATRP[39,40,42–46] or oxyanionic polymerisation,[41,44] with outer blocks consisting of an amine-containing methacrylate monomer, which provides pH-response. In most of the studies, 2-(diethylamino)ethyl methacrylate (DEAEMA) was used,[39,41–46] while in one of the studies the hydrophobicity of the amine-containing monomer

was varied from 2-(*t*-butylamino)ethyl methacrylate (*t*BAEMA), to DMAEMA, to DEAEMA, to 2-(diisopropylamino)ethyl methacrylate (DiPAEMA).[40] Copolymers with different MMs of the outer blocks were studied, thus simultaneously altering the total MM and composition of the copolymers. More specifically, pentablock terpolymers, with the total MM ranging from 12 800 to 22 000 g mol^{-1}, were reported, which preserved thermogelation. The T_{gel} could be tuned by changing the pH, with the lower pH increasing the T_{gel}.[40] Thus, these copolymers were studied as pH-responsive release depots, as gel dissolution, and thus release of the compound of interest, was promoted by decreasing the pH. Nile blue chloride,[41] lysozyme,[42] plasmid DNA,[44] and siRNA combined with gold nanoparticles[46] were tested, and it was found that the lower the pH, the faster the release.[41,42] The cytotoxic nature of these copolymers was highly associated with the content of DEAEMA, with the higher content increasing the cytotoxicity,[44] similarly to DMAEMA-based systems,[158–161] as the positive charges destabilise the negatively charged cellular membrane. Interestingly, the thermogelation could be tuned by changing the hydrophilicity of the amine-containing outer blocks.[40] While the *t*BAEMA-based polymers were too hydrophilic, thus preventing gelation, the DiPAEMA-based ones were too hydrophobic, thus making the polymers insoluble. Both DMAEMA- and DEAEMA-based polymers formed gels, with the latter lowering the T_{gel} and increasing the gel rigidity, presumably due to the increased hydrophobicity, thus enhancing the "hydrophobic effect". A comparison between a DEAEMA-containing pentablock terpolymer with Pluronic® F127 revealed the formation of more rigid gels by the latter, thus indicating a disturbance of the gelation by the addition of the outer blocks, attributed to the change in the micelle packing,[40] as revealed by SANS and nuclear magnetic resonance spectroscopy.[43] Interestingly, one of the DEAEMA-based pentablock copolymers has recently been used for membrane fabrication, and its pH- and thermoresponse were found to control the permeability of the membrane, which increased by increasing the pH and temperature.[39]

Pentablock terpolymers with outer NIPAAm-based blocks, instead of amino-containing methacrylate units, were also investigated.[47–49] In one of the studies, three different Pluronic® polymers were used, namely Pluronic® F108, F68, and F127.[48] By increasing the DP of the hydrophobic PG-based block, and by increasing the length of the NIPAAm-based outer blocks while keeping the Pluronic® constant, a decrease in the LCST and a higher aggregation number were recorded.[48] A similar pentablock terpolymer consisting of Pluronic® F127 was investigated *via* micro-differential scanning calorimetry (micro-DSC), SANS and NOESY experiments, which revealed two phase transitions corresponding to the thermoresponse of PG and NIPAAm, respectively.[47,48] It was confirmed that the thermoresponse of NIPAAm units triggered the change from classical core–shell micelles to flower-like micelles.[47,48]

In another study, Pluronic® F127 multiblock copolymers were produced by: (i) coupling of Pluronic® F127, *i.e.*, four times and (ii) random coupling of EG- and PG-based blocks, with the final copolymers having a similar content of EG but a

different MM of Pluronic® F127.[50] In both cases, the viscosity of the final product exceeded that of Pluronic® F127 by fifteen and six times, respectively. Prolonged anti-restenosis drug release was observed for the four-times coupled Pluronic® F127 (forty days) compared to Pluronic® F127 (seven days).[50] However, the favourable gelation characteristics of the synthesised polymers cannot be purely attributed to the multi-block architecture, as the increased MM does play a strong role in the viscosity of the solution, and consequently the gelation, as previously mentioned. Therefore, for clear architecture effects to be drawn, systematic studies need to be carried out, in which the feature of interest should be varied while keeping all the other parameters constant.

EG-containing degradable polymers

Thermoresponsive ABA and BAB triblock copolymers based on EG (A unit) and PLGA (B unit) have been reported in the literature, with the BAB counterparts of a specific MM and composition being trademarked as ReGel®.[51] Specifically, ReGel® polymers' MM varies from 3100 to 4500 g mol^{-1}, while the composition of the degradable component, i.e., PLGA, varies from 51 to 83 w/w%, in which the glycolate (GA) content varies from 15 to 35 w/w%.[51] Both structures have been patented by Macromed Inc.,[52–54] with the work to be strongly associated with Prof Sung Wan Kim (1940–2020, co-founder of Macromed Inc.).[162]

The composition and the MM of these copolymers strongly control their gelation properties. When the MM of the central EG-based block was kept constant (BAB-type), the gelation temperature was lower for polymers with a higher MM of the PLGA block and a higher content of D,L-lactate (D,L-LA).[55–58] The latter is expected as LA is more hydrophobic than GA, owing to the extra methyl group in its structure, thus enhancing the "hydrophobic effect", responsible for thermoresponse. Similarly, the longer the EG-based block, the higher the gelation temperature.[57,59] Similar observations were made for the ABA type polymers, as the lower the D,L-LA content, the higher the CGC.[60] On the other hand, when L-LA was used to fabricate BAB-type triblock copolymers, the T_{gel} decreased as the content in L-LA decreased, indicating that the effect of stereochemistry, i.e., the increase in crystallinity, overcomes the effect of hydrophobicity.[61]

The content and block length of these BAB triblock copolymers affect their properties at the nanoscale, as revealed by SANS. While an ellipsoid structure is adopted by the BAB copolymer with a shorter EG-based block in diluted solutions, core–shell spherical micelles are detected for the one with a longer EG-based block under the same conditions.[59] On the other hand, at higher concentrations, both copolymers adopt the core–shell spherical micelle configuration, and their thermally induced gelation is attributed to the packing of the micelles into cylinders.[59] When the ABA and BAB copolymers are compared, the critical gelation concentration (CGC) and the T_{gel} of the latter are

lower than the ones of the former, a feature attributed to the bridging of adjacent flower-like micelles by the PLGA blocks.[56,60,62] Monte-Carlo simulations in combination with experimental work revealed a lower CGC, T_{gel}, and precipitation temperature of the BAB-systems compared to those of the corresponding ABA and AB polymers.[63] The physical cross-linking of the core–shell micelles formed by the ABA and AB polymers was attributed to the formation of hydrophobic channels, throughout the gelation window. On the other hand, the thermogelation of the flower-like micelles adopted by the BAB polymer chains takes place in two steps: (i) gelation with a dominant crosslinking factor with the formation of hydrophilic bridges at lower temperatures, and (ii) gelation with a dominant crosslinking factor with the formation of hydrophobic channels at higher temperatures. These are shown schematically in Fig. 8.

ε-Caprolactone (CL) was also used as a repeating unit in combination with EG for the synthesis of degradable ABA and BAB triblock copolymers. It should be reminded that the hydrophobicity increases from GA to LA to CL, thus offering opportunities for modulating the gelation properties of the polymers and their degradability rate.

Studies on BAB triblock copolymers based on EG (A unit) and a random copolymer (B block) of CL with either LA[64,65] or GA[66] were reported. One of the studies on LA-containing polymers reported that the higher the MM of the middle block, the lower the gelation concentration.[65] On the other hand, the second study reported a lower T_{gel}, a wider gelation region, and a higher storage modulus, but a higher gelation concentration for the polymer with a longer EG-based middle block.[64] However, direct comparison should be avoided due to the difference in both MM and composition. SANS studies revealed the transition from core–shell micelles to rod-like objects for the polymer with a longer middle block, while the one with a shorter middle block existed as cylinders, regardless of the temperature. This was attributed to the shorter middle block being unable to form a loop, thus promoting intermicellar bridging.[64] As far as GA-containing copolymers are concerned, it was observed that the higher the CL/GA ratio, the lower the T_{gel}, despite the increase in the hydrophobicity of the structure, indicating that other factors, such as crystallisation, play an important role in the gelation properties.[66]

In some of the studies, BAB triblock copolymers based on EG (A unit) and CL's derivatives (B unit) were investigated.[67,68] In particular, the CL unit consisted of a benzyl carboxylate group at the α-position, which was hydrolysed to different extents to give carboxylic acid groups, which are pH-responsive. Increasing the content of the hydrophobic benzyl groups decreased the CP and the T_{gel} and increased the strength of the gels. As far as the carboxyl-containing copolymers are concerned, their micellisation was controlled by the pH, with the neutrally charged polymers self-assembling into micelles at lower concentrations.[67,68] However, depending on the polymerisation conditions, i.e., bulk versus solution, and polymerisation time, branching occurred, thus gelation or water-insolubility were promoted, depending on the level of branch-
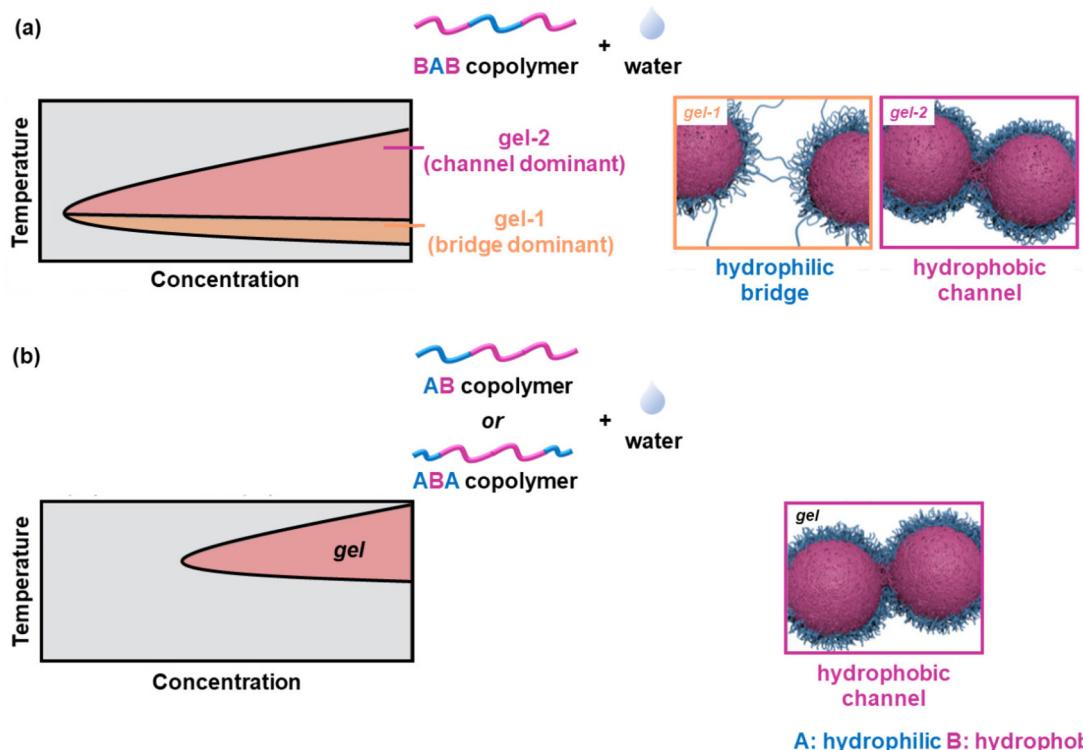
Fig. 8 (a) Schematic of the phase diagram of a PLGA-PEG-PLGA triblock copolymer (left) and the suggested gelation mechanism (right), and (b) schematic of the phase diagram of a PEG-PLGA diblock copolymer and a PEG-PLGA-PEG triblock copolymer (left) and the suggested gelation mechanism (right). A and B correspond to the hydrophilic PEG block (in blue) and the hydrophobic PLGA block (in purple), respectively. PEG and PLGA stand for poly(ethylene glycol) and poly(D,L-lactide-co-glycolide), respectively. Adapted with permission from S. Cui, L. Yu, and J. Ding, *Macromolecules*, 2019, **52**, 3697–3715. Copyright 2019 American Chemical Society.

ing.[163] This indicates the importance of synthesising well-defined polymers, thus ensuring reproducibility in the synthesis and the final properties.

Degradable BAB and ABA copolymers consisting of EG (A block) and either CL or depsipeptides (B block) were studied,[69,70] revealing that the architecture has an important role in the final properties. Concerning the study on CL-based copolymers, a lower T_{gel}, a wider gelation area and a higher storage modulus of the gels were obtained when the BAB-type copolymers were used, a feature attributed to the bridging of the flower-like micelles.[69] This is in agreement with the observations made on triblock copolymers based on PLGA instead of CL. In contrast, the ABA-type depsipeptide-containing polymers, which form classical core–shell micelles, showed temperature-driven gelation, while the BAB-type ones only presented a CP upon heating, which decreased by increasing the hydrophobicity of the depsipeptide.[70] However, it should be noted that in the latter study both the composition and the MM varied, thus illustrating the importance of performing systematic studies for clear conclusions to be drawn.

In an interesting study by Mohammadi *et al.*, several degradable triblock copolymers were studied.[71] In more detail, systems containing BAB-type copolymers with the A block consisting of EG and the B block consisting of GA/LA, LA and LA/CL were investigated. An injectable system which gels at body

temperature was formed by the LA-containing copolymer. On the other hand, GA/LA copolymers of different structures were mixed to achieve the same result, similarly to the LA/CL based copolymers. These thermogelling systems were studied as drug release depots, with the LA/CL containing systems prolonging the release,[71] presumably due to the increased hydrophobicity. This illustrates the potential of designing optimal thermogelling systems by blending of thermoresponsive polymers.

Degradable pentablock copolymers based on EG, CL and/or LA were also reported in the literature. In one of the studies, ABCBA pentablock terpolymers consisting of EG (A block), CL (B block) and LA (C block) of different hydrophobic contents showed that the higher the content of CL, the lower the T_{gel}, and the higher the rigidity of the gel.[72] In another study, ABCBA pentablock terpolymers with various ratios of D-LA (A block), L-LA (B block) and EG (C block) showed UCST-type gelation, attributed to the intermicellar aggregation and bridging, revealed by SAXS.[73] This observation indicates that slight variations in the position and chemical nature of the polymers can result in important differences in their thermogelling properties. Interestingly, copolymers with an equimolar content of enantiomers showed a wider gelation area and a higher storage modulus, as the gel destabilised at higher temperatures. When the pentablock copolymers were compared with their corresponding triblock copolymers, the gels destabilised

at lower temperatures from ABCBA, to the ACA/BCB enantiomeric mixture, to the isotactic BCB, to the atactic copolymer based on D,L-LA instead. This indicates that the position of the blocks and the degree of crystallinity are of great importance for the gelation.[73]

Hybrid ABCBA pentablock copolymers consisting of the hydrophilic peptide L-lysine (A unit), a hydrophobic statistical copolymer of poly(L-histidine)-co-poly(γ-benzyl-L-glutamate) as the B block, and hydrophilic and thermoresponsive EG (C unit) have been recently reported by Skoulas et al.; L-histidine is pH-responsive.[74] Physical hydrogels were formed at room temperature, which are temperature-insensitive when L-histidine is neutrally charged. However, when L-histidine is protonated by lowering the pH from 7.4 to 6.5, weaker gels with temperature-tuneable viscoelastic properties are observed.[74]

Degradable thermoresponsive copolymers with hyperbranched/multiblock architectures were also reported in the literature. In one of the studies, triblock and hyperbranched copolymers based on EG, PG and CL were compared with the hyperbranched architecture lowering the CP, the critical gelation temperature (CGT) and the critical gelation concentration.[75] Interestingly, the CGC values reported were as low as 4.3 wt%, depending on the composition. These superior gelation properties of the hyperbranched architecture were attributed to the enhanced chain interactions through hydrogen bonding between the branches.[75] Multiblock terpolymers based on 1,4-butylene adipate, EG and PG, and multiblock bipolymers based only on EG and PG were also reported, with the BA content enhancing the gelation characteristics.[76] A thermoresponsive multiblock bioconjugate was reported, namely (EG$_{23}$-b-betulin-b-EG$_{23}$)$_6$, which showed UCST-type behaviour with a transition from a turbid gel to a transparent solution to precipitation upon heating.[77]

An interesting study on thermoresponsive amphiphilic block copolymers with alternating hydrophilic and hydrophobic blocks has been recently published by Kostyurina et al.[78] This library of thermoresponsive polymers consisted of polyester hydrophobic blocks and PEG hydrophilic blocks of varying lengths. A linear relationship between the CP and the length of the hydrophobic block was revealed, while a logarithmic relationship between the CP and the length of the hydrophilic block was established instead. Amphiphilic alternating copolymers with short PEG blocks favour the formation of highly ordered polymer networks characterised by liquid crystalline cubic phases, as revealed by SAXS studies.[78]

Acrylamide thermoresponsive units

Several (meth)acrylamide homopolymers have been reported to present thermoresponse. In 1975, Taylor and Cerankowski reported the CP of several (meth)acrylamide homopolymer solutions at 1% in water, such as N-ethylacrylamide (CP = 74 °C), NIPAAm (CP = 32 °C),[164] N,N-diethylacrylamide (DEAAm, CP = 25 °C), and N-cyclopropylacrylamide (CP = 57 °C).[165] The structures and properties of these units are shown in Fig. 9. Amongst these, NIPAAm has been undoubtedly the most popular thermoresponsive unit, and it has been extensively studied for its thermoresponsive properties, including thermogelation. The relevant studies are discussed in the following paragraphs, with the major interest being focused on the effect of architecture on the thermoresponsive properties.

In several studies, NIPAAm (A unit) was combined with styrene (St, B unit) to form BAB triblock copolymers, which adopt flower-like configuration when dissolved in aqueous media.[79–82] SANS studies on copolymers containing deuterated St revealed the formation of a St-based hydrophobic core, and a NIPAAm-based hydrophilic corona below the CP. These micelles collapsed and formed clusters once the CP was reached. When a higher content of St was used, micelles, aggregates, and clusters formed both below and above the CP, as revealed by SANS and light scattering.[79–82] When varying the hydrophobic monomer from St to 4-t-butyl St (tBuSt), 3,5-dibromobenzyl acrylate (BrBzA), 2-ethylhexyl acrylate (EtHexA), to octadecyl acrylate (OcDecA), it was observed that the CGC decreases, and the gels were stronger, as the glass transition temperature of the hydrophobic monomer decreased.[83] On the other hand, no effect on the CP was observed, presumably due to the hydrophobic block being collapsed in the core of the micelle.[83]
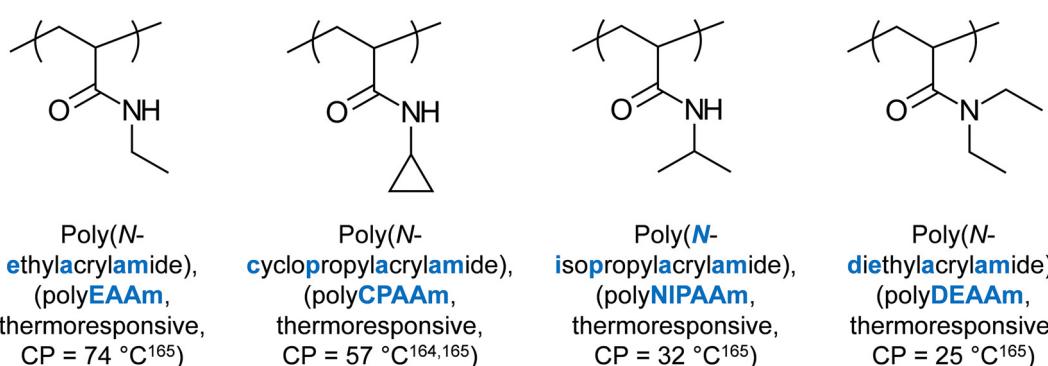
Fig. 9 Chemical structures and properties of thermoresponsive acrylamide units.

Poly(N-ethylacrylamide), (polyEAAm, thermoresponsive, CP = 74 °C[165])

Poly(N-cyclopropylacrylamide), (polyCPAAm, thermoresponsive, CP = 57 °C[164,165])

Poly(N-isopropylacrylamide), (polyNIPAAm, thermoresponsive, CP = 32 °C[165])

Poly(N-diethylacrylamide), (polyDEAAm, thermoresponsive, CP = 25 °C[165])

Several other units were used to form BAB triblock copolymers with NIPAAm forming the central hydrophilic and thermoresponsive block. Acrylic acid (AA) was incorporated into the structure to exhibit pH-responsive properties in addition to the thermoresponse; deprotonation of the carboxylic acid units disrupted thermoresponse, as expected.[84] Post-polymerisation modification of these copolymers with iron oxide introduced magnetic-responsive properties,[84] while phosphorylation of the AA units decreased the T_{gel}, with NIPAAm$_{117}$-b-AA(PEA)$_{303}$-b-NIPAAm$_{117}$ forming hydrogels under physiological conditions at only 2 wt%; PEA stands for O-phosphoethanolamine.[85] When the outer blocks consisted of a random copolymer of N,N-dimethylacrylamide (DMAAm) and adamantane acrylate (Adac), complexation with cyclodextrin was achieved, thus forming thermoresponsive supramolecular glycopolymers.[86] Incorporation of an ionic liquid, namely 3-methyl-1-(4-vinylbenzyl)-1-imidazolium chloride (A block) into the structure of BAB NIPAAm based triblock copolymers formed thermogels.[87]

ABA triblock copolymers, with NIPAAm forming the outer blocks, were also synthesised, and investigated by several groups. Increasing the length of the hydrophilic EG-based block resulted in an increase in the CP, as the "hydrophobic effect" was disrupted,[88] while increasing the length of the thermoresponsive NIPAAm block in copolymers containing N-vinylpyrrolidone (VP) decreased both the CGC and the T_{gel} of the system.[89] A positively charged betaine ester was incorporated into the central block to electrostatically attract the negatively charged antimicrobial drug, salicylate, thus forming biocompatible antimicrobial drug release depots based on thermogelling wound dressing.[90] Redox active polymers were also investigated by incorporating 2,2,6,6-tetramethylpiperidine-1-oxyl (TEMPO) units (B unit) into the structure, and the redox activity was affected by NIPAAm's thermoresponse.[91] In one of the studies, hydrophobic hydroxyterminated polybutadiene (HTPB) was used to form the central block, and its epoxidation increased the CP due to the introduction of more water molecules.[92]

Two studies have been reported in the literature in which ABA and BAB NIPAAm-based triblock copolymers were compared, and the effect of the architecture was discussed. In the first study, 2-hydroxyethyl methacrylate (HEMA) was used to fabricate the B block, and the ABA-type copolymers presented a lower T_{gel} than the BAB one.[93] In the second study, ethyl acrylate (EtA) was used as the hydrophobic B unit instead.[94] While the critical micellisation concentration (CMC) value of the ABA architecture was lower than its BAB counterpart, the CP of the former was higher than the latter.[94] These observations can be explained upon consideration of the self-assembled structures these copolymers adopt. The ABA architecture, with the hydrophobic block in the middle, forms traditional core–shell micelles, which are easier to form (lower CMC) and remain stable up to higher temperatures (higher CP). On the other hand, the BAB architecture forms flower-like micelles, whose formation requires folding of the polymer chain into a loop, thus their self-assembly is less favourable (higher CMC) and

these copolymers destabilise more easily upon heating (lower CP), due to the folding of the polymer chain.

Several studies reported the synthesis of triblock terpolymers based on NIPAAm and investigation of their thermoresponsive properties in terms of the CP. When PEG-PCL-PNIPAAM copolymers (ABC structure) were studied, the CP decreased upon increasing the DP of the hydrophobic and thermoresponsive blocks.[95] When their ACB counterparts were tested, the CP decreased as a function of the polymer concentration.[96] When the middle block in the ABC structure was changed to 3-methacryloxypropylheptaphenyl polyhedral oligomeric silsesquioxanes (MA-POSS), similar observations were recorded, i.e., the CP decreased when the DP of NIPAAm increased.[97] Double thermoresponsive ACB triblock terpolymers based on poly(ethylene glycol) methyl ether vinylphenyl (mPEGV, A block), NIPAAm (B block) and St (C block) presented two CP values, and the higher the DP of NIPAAm, the more pronounced the transmittance change.[98] When the change in the size as a function of temperature was monitored, collapse of the NIPAAm-based block on the hydrophobic core occurred upon NIPAAm's thermoresponse, leading to the shrinkage of the micelles above the CP.[95,96]

Two studies on triblock quaterpolymers, i.e., polymer with three different blocks, with one block consisting of repeating units with different chemical nature, were reported in the literature. In one of the studies, thermoresponsive glycopolymers were studied; these polymers were poly(3-O-methacryloyl-α,β-D-glucopyranose (MAGlc)-poly(HEMA-g-PCL))-PNIPAAm.[99] An increase in the CP was recorded as the DP of both the hydrophilic MAGlc and the thermoresponsive NIPAAm blocks increased, due to the increased hydrophilicity in their structure.[99] When PEG-poly(HEMA-g-LA)-PNIPAAm was studied, collapse of the NIPAAm block on the hydrophobic central block, and thus shrinkage of the micelles occurred above the CP, similarly to the previous observations.[100] It is worth noting that the highly hydrophilic PEG corona prevented aggregation above the CP.[100]

Lodge and co-workers have previously reported several studies on thermogels from ABC triblock terpolymers, with A, B, and C blocks being based on poly(ethylene-alt-propylene), EG, and NIPAAm, respectively.[101–103] In the first study on this subject, the ABC triblock terpolymers out-performed their CBC counterparts, by favouring gelation at lower concentrations. Detailed analysis on the ABC triblock terpolymers via cryogenic transmission electron microscopy, cryogenic scanning electron microscopy, and SANS revealed the formation of two-compartment polymer networks with distinct poly(ethylene-alt-propylene) and PNIPAAm cores, which are connected via hydrophilic PEG bridges. When dissolved in the ionic liquid 1-ethyl-3-methylimidazolium bis(trifluoromethylsulfonyl)imide, NIPAAm presents a UCST-behaviour instead, with two-compartment ion gels being formed above the UCST.[101–103]

In an intriguing study by Onoda et al., precise control of the sol–gel transition by blending two ABC triblock terpolymers was reported.[104] More specifically, the two ABC triblock terpolymers consisted of DMAAm as the central block and a

random copolymer of NIPAAm and *n*-butyl acrylate (BuA) as the A block, but they differed in the third block; this was based either on a random copolymer of NIPAAm and BuA, but with a different composition from the first block, or a NIPAAm homopolymer. The T_{gel} of the former was lower than that of the latter, due to the incorporation of more hydrophobic BuA units, as expected. Interestingly, the T_{gel} of the polymer blends varied linearly with the content in the two copolymers, while keeping the strength of the gel constant.[104]

Temperature- and photo-responsive hydrogels were fabricated using ABC triblock terpolymers, where A, B and C correspond to NIPAAm, 4-acryloylmorpholine (NAM), and 2-((((2-nitrobenzyl)oxy)carbonyl)amino) ethyl methacrylate (NBOCAEMA), respectively.[105] Self-assembly into core–shell micelles with the hydrophobic NBOCAEMA and the hydrophilic NIPAAm and NAM was recorded below the LCST of NIPAAm, and temperature-induced gelation occurred upon heating above the LCST. An increase in the T_{gel} upon UV-cross-linking of the micellar core was observed, thus offering a second trigger for the gel dissolution, in addition to temperature. These novel hydrogels were tested for co-delivery of the hydrophobic drug doxorubicin and the hydrophilic drug gemcitabine.[103]

Two studies reported the synthesis and investigation of thermoresponsive tetrablock terpolymers. In one of the studies, ABAB multiblock copolymers based on DMAAm and NIPAAm were investigated.[108] When comparing two tetrablock copolymers with similar compositions and different MMs, gelation was observed only for the higher MM copolymer, due to the hydrophilic blocks being long enough to act as bridges. When compared to the corresponding BAB triblock copolymer, the T_{gel} decreased and the strength of the gel increased, as the complexity of the architecture increased.[108] The self-assembly of EG-*b*-St-*b*-NIPAAm-*b*-DMAEMA tetrablock quaterpolymers was tuned by changing the temperature and the pH, thus employing the thermoresponsive properties of NIPAAm and the pH-responsive properties of DMAEMA.[109] In addition, by changing the pH of the solution from acidic to alkaline, the CP of the copolymers was decreased, due to the increase in the hydrophobicity of their structure.[109]

Two studies investigated ABCBA pentablock terpolymers based on the pH responsive DEAEMA (A block), the thermoresponsive NIPAAm (B block) and the hydrophilic EG (C block).[110,111] Both studies investigated the effect of DEAEMA's pH response on the self-assembly and the CP. In an acidic environment, the amine groups are protonated, thus temperature-driven micellisation due to NIPAAm's thermoresponse was observed. On the other hand, at alkaline pH, DEAEMA is hydrophobic, thus self-assembly at room temperature was observed. An increase in the pH lowers the CP, as expected, due to favouring the "hydrophobic effect".[110,111]

In a recent study by Lv *et al.*, double stimuli responsive ABCBA pentablock quaterpolymers have been shown to form different types of self-assembled structures depending on the pH and temperature.[114] More specifically, these copolymers consisted of thermosensitive NIPAAm (A unit), PG (C unit),

and a pH-responsive block based on a random copolymer of AA and *t*-butyl acrylate (*t*BA), but they differed in the length of the NIPAAm block and the ratio of AA : *t*BA. Interestingly, the degree of deprotonation of the AA units could determine the reversibility of the thermosensitive process, and tune the types of self-assembled nanostructures, with cylinders and spheres being identified.[114]

Degradable NIPAAm-containing pentablock terpolymers have also been reported in the literature. The ABCBA pentablock terpolymers were based on NIPAAm (A unit) and EG (C unit), while the B unit was based on a degradable hydrophobic monomer, either CL[112] or LA.[113] In both studies, longer outer NIPAAm chains favoured thermogelation. In the study by Abandansari *et al.*, the best-performing polymer (CL-based) presented the T_{gel} at 32 °C and the storage modulus (G') at 25 000 Pa, when the concentration was 20 wt%. Most importantly, the storage modulus drastically increased to 60 000 Pa when the concentration increased to 30 wt%.[112] Concerning the LA-containing pentablock terpolymer, gelation in a physiological medium was visually detected at 10 w/w% and 30 °C, which was not the case for its triblock ABC analogue, whose aqueous solutions were unable to form gels.[113]

Interestingly, a study on well-defined NIPAAm-based multiblock copolymers has been reported by Simula *et al.*[115] In this study, thermoresponsive triblock and pentablock copolymers were synthesised *via* aqueous Cu(0) mediated living radical polymerisation (SET-LRP), with excellent control over the molecular mass distribution ($Đ < 1.19$), quantitative conversions, and time-efficiency. Increasing the DP of NIPAAm (B unit) in BAB triblock copolymers with the PEG central block from 10 to 160 decreases the CP from 71.3 °C to 41.2 °C. Chain extension with a second thermoresponsive unit, namely DEAAm (C unit), to form a CBABC pentablock terpolymer reduced the CP from 71.3 °C to 52.5 °C. Substituting the thermoresponsive DEAAm unit with the hydrophilic DMAAm unit disrupted the thermo-response, as no CP was detected up to 90 °C.[115]

Two studies discussed the thermoresponse of NIPAAm-based star copolymers and their comparison with the corresponding linear analogues.[116,117] When A_2BA_2 copolymers (A: NIPAAm, B: EG) were compared with ABA triblock copolymers with the same MM and composition, a similar thermogelling behaviour was recorded. On the other hand, the gelation characteristics were favoured as the complexity of the architecture increased from ABC, ABCBA, and (ABC)$_4$ (A: [*R*]-3-hydroxy-butyrate, B: NIPAAm, C: poly(ethylene glycol) methacrylate-*co*-poly(propylene glycol) methacrylate), PEGMA-*co*-PPGMA. Specifically, the higher the complexity of the architecture the stronger the gels, and the lower the T_{gel}, with both ABCBA and (ABC)$_4$ forming gels at room temperature; the strength of the latter increased upon NIPAAm's thermoresponse.[116,117]

As previously mentioned, DEAAm is a less famous thermo-responsive unit, whose homopolymers have been reported to show a CP at 25 °C by Taylor and Cerankowski,[165] and 33 °C by Idziak *et al.*[166] The CP being close to the physiological temperature makes this unit a suitable candidate for designing

thermoresponsive polymers. In a study by Haddow et al., ABA triblock copolymers based on DEAAm (A unit) and EG (B unit) were synthesised, and the MM of the blocks was varied. Copolymers with a longer PEG middle block favoured gelation, due to the effective bridging of the micelles and the formation of spherical and elliptical aggregates upon heating, thus leading to gel formation.[118] Grubbs and co-workers reported the synthesis and investigation of two ABC triblock copolymers with A, B and C being based on EG, DEAAm, and N,N-dibutyl-acrylamide (DiBuAAm), respectively.[119] When the thermoresponsive middle block was short, gelation driven by a sphere to worm transition was recorded, while an increase in its length disrupted thermogelation due to difficulties in the re-arrangement of the self-assembled structures.[119]

Amine-based methacrylate thermoresponsive units

The DMAEMA unit has been extensively reported in the synthesis of polymers for various applications. Even though DMAEMA has been mostly incorporated into the polymer structure to exhibit pH-responsive properties, reports on its thermoresponse have also been published. The latter are discussed in the following paragraphs with an increased architecture complexity.

In one of the studies, AB diblock and ABA and BAB triblock copolymers consisting of hydrophilic 6-O-methacryloyl-D-galacto-topyranose (A unit) and pH- and temperature-responsive DMAEMA (B unit) were synthesised and investigated in terms of their thermoresponse.[120] At alkaline pH both units are water-soluble and thus they exist as unimers in solution below the LCST of DMAEMA. Upon heating, temperature-driven micellisation was induced, leading to the formation of traditional core–shell micelles by the AB and ABA copolymers, and flower-like micelles by the BAB ones, with their CP being detected between 35 and 55 °C, depending on their MM and composition.[120] Direct comparison between the different architectures cannot be made due to the variations in the MM and composition, which also affect the CP.

BAB triblock copolymers with DMAEMA units forming the A block and a random copolymer of DMAEMA and n-butyl methacrylate (BuMA) forming the B block were reported by Lauber et al.[121] These copolymers formed hydrogels at room temperature when the degree of ionisation of DMAEMA was kept at low values. However, the viscosity of the hydrogels decreased, and eventually homogeneous runny solutions were formed when protonating the DMAEMA units and thus increasing the hydrophilicity of the structure. Interestingly, upon heating of the solutions at high degrees of the protona-tion of DMAEMA, irreversible hydrogels were formed.[121]

A study on the same repeating units has been reported by our group, with symmetric and asymmetric BAB triblock copolymers being investigated.[122] While keeping both the MM and composition constant, within the same family, the T_{gel} of the copolymers increased by increasing the asymmetry from BAB

to B′AB′$_2$, to B″AB″$_4$. This trend was attributed to the insufficient bridging between the neighbouring flower-like micelles, thus interrupting the gelation.[122]

To the best of our knowledge, only our group has reported the synthesis and investigation of triblock terpolymers consisting of DMAEMA as the thermoresponsive unit (C unit).[26,123–126] In all the studies, the A block was based on a methoxy EG-based methacrylate unit, e.g., methoxy oligo(ethylene glycol) methacrylate with an average M_n of 300 g mol^{-1} (mOEGMA300), which is hydrophilic and thermoresponsive at a temperature higher than 70 °C.[17,167] Note that the thermoresponse of the OEGMA monomer depends on the number of EG groups and the chemistry of the terminal group, as will be discussed in more detail in the relevant section. The B block consisted of a hydrophobic unit with a linear alkyl side chain, e.g., BuMA. When investigating the MM and composition, it was observed that the gelation was favoured when the MM, the hydrophobic content, and the length of the hydrophobic side chain were increased, and when the length of the hydrophilic EG-based unit was decreased. The complexity of the architecture was varied by changing the position of the blocks in the structure, from ABC to ACB to BAC.[26,124,126] From our studies, it was concluded that the ABC architecture, i.e., the one with the hydrophobic block in the middle, shows the most favourable characteristics for injectable systems, as it favours self-assembly to smaller micelles and thus better dissolution at room temperature, while it presents a clear solution–gel transition upon heating.[26,124,126]

The only study on tetrablock terpolymers with DMAEMA as a thermoresponsive unit has been reported by our group in 2018.[127] In this study, the copolymers consisted of mOEGMA300, BuMA and DMAEMA as A, B, and C units respectively. The MM and composition were kept constant within the same family and the position of the blocks was varied as follows: ABCA, ABAC, ACAB, BACB, BABC, ABCB, CABC, CACB, and ACB. The position of the blocks strongly controlled the solubility, self-assembly and gelation properties of their aqueous solutions, with the BABC and ACBC architectures showing the widest gelation areas.[127]

Patrickios and co-workers have investigated multiblock bipolymers composed of DMAEMA and BuMA as the A and B blocks, respectively.[128] BAB, ABABA, BABABAB and ABABABABA copolymers with the DP$_A$ and DP$_B$ being kept the same in different copolymers, but simultaneously changing the total MM and composition, were investigated, and gelation was reported for the heptablock bipolymer. When the composition and total MM were kept constant in BAB, BABABAB and ABABABABA copolymers, only the triblock and heptablock copolymers formed gels. It was concluded that the gelation was favoured when the BuMA block is located at the end of the polymer chain, with the hydrophilic and thermoresponsive DMAEMA block being long enough to facilitate micelle bridging. When the DMAEMA block was incorporated at the end of the polymer chain, electrostatic repulsion between the positively charged amine groups interrupted gelation.[128]

DMAEMA-containing thermoresponsive multiblock brush type graft terpolymers were reported.[129] $CL_xCH_2CH_2[O(CL_y)]CH_2$-$b$-$VB_z$-$g$-$DMAEMA_w$ copolymers, with VB standing for 4-vinyl benzyl and x, y, z, and w denoting the DP of the corresponding units, showed a CP which was strongly controlled by the content of DMAEMA.[129]

EG-based (meth)acrylate thermoresponsive units

(Meth)acrylate units with EG on the side chain have received much scientific interest as alternative thermoresponsive units, due to the combination of their thermoresponsive ability and PEG's biocompatible nature.[168] It is well-documented that depending on the number of EG groups on the side chain, the hydrophobicity/hydrophilicity and thermoresponse of these (meth)acrylate polymers can be varied.[17,18,167] As an example, methoxy mono(ethylene glycol) methacrylate (MEGMA) homopolymers are water-insoluble, while methoxy oligo (ethylene glycol) methacrylate with an average M_n of 500 g mol^{-1} (mOEGMA500) shows no thermoresponse up to 95 °C.[17] In addition, changing the end group on the side chain from hydroxyl to methyl to ethyl, the CP decreases as the hydrophobicity increases.[17,18] The chemical nature of the backbone, *i.e.*, acrylate *versus* methacrylate, also affects the CP, with the thermoresponse of the acrylate units being affected by the length and the end group of the side chain, similarly to their methacrylate analogues.[18] The chemical structures and properties of EG-based (meth)acrylate units are summarised in Fig. 10.

Thermoresponsive ABA and BAB triblock copolymers consisting only of EG-based (meth)acrylate units were reported by Xiang *et al.*[130] In this study, the triblock copolymers were based on methoxy oligo(ethylene glycol) acrylate with an average M_n of 480 g mol^{-1} (mOEGA480) and mDEGMA and were compared with their corresponding diblock and star copolymers [both (AB)$_3$ and (BA)$_3$], with the attention being focused on the effect of matching the polarity of the end group (phenyl *versus* carboxyl) with the polarity of the adjacent block. Generally, mismatching the polarity disturbs the self-


(a) Acrylate Units:

Poly[methoxy mono(ethylene glycol) acrylate] (polymMEGA, hydrophobic, Water-insoluble[18])	Poly[methoxy di(ethylene glycol) acrylate] (polymDEGA, thermoresponsive, CP ≈ 40 °C[18])	Poly[methoxy oligo(ethylene glycol) acrylate with average M_n 480 g mol^{-1}] (polymOEGA480, thermoresponsive, CP ≈ 92 °C[18])	Poly[ethoxy di(ethylene glycol) acrylate] (polyeDEGA, thermoresponsive, CP ≈ 13 °C[18])

(b) Methacrylate Units:

Poly[methoxy di(ethylene glycol) methacrylate] (polymDEGMA, thermoresponsive, 27 ≤ CP ≤ 30 °C[17])	Poly[methoxy tri(ethylene glycol) methacrylate] (polymTEGMA, thermoresponsive, 49 ≤ CP ≤ 63 °C[17])	Poly[methoxy oligo(ethylene glycol) methacrylate with average M_n 300 g mol^{-1}] (polymOEGMA300, thermoresponsive, 71 ≤ CP ≤ 76 °C[17])	Poly[methoxy oligo(ethylene glycol) methacrylate with average M_n 500 g mol^{-1}] (polymOEGMA500, hydrophilic, no CP[17])

Fig. 10 Chemical structures and properties of (a) acrylate units and (b) methacrylate units discussed in this review.

assembly and sufficient hydration, thus leading to aggregation.[130]

Negru *et al.* reported a study on BAB triblock copolymers consisting of EG (A unit) and a random copolymer of ethoxy di(ethylene glycol) acrylate (eDEGA) and mOEGA480.[146] It was observed that increasing the DP of either block resulted in a decrease in the T_{gel}, while when the composition was systematically varied, the T_{gel} decreased as the hydrophilic mOEGA480 content decreased.[146]

In three of the studies, hydrophilic and thermoresponsive methoxy di(ethylene glycol) acrylate (mDEGA, A unit) was combined with hydrophobic styrene (St, B unit) to synthesise amphiphilic BAB triblock copolymers.[143–145] Miasnikova *et al.* investigated copolymers with a fixed DP of St, and a varied DP of the mDEGA block.[144] They observed that the copolymer with the shortest DEGA block was insoluble in water, while solubility was enhanced when longer mDEGA blocks were incorporated into the structure, which also increased the CP of these copolymers. While the composition effect dominated the thermoresponse in diluted solutions, the MM effect controlled the gelation in concentrated solutions, with the CGC decreasing with the increasing length of the mDEGA block, due to the easier bridging.[144] In another study by the same group, the BAB triblock copolymers were compared with their corresponding AB diblock copolymers and (BA)₃ star copolymers.[143] Interestingly, increasing the complexity of the architecture from diblock to triblock to star copolymers favours the thermoresponse by reducing the CP.[143] In addition to the reports on micellisation and gelation, thermoresponsive films based on these triblock copolymers were also investigated.[145] By increasing the temperature of the films, water was excluded from the structure and shrinkage was observed, driven by DEGA's thermoresponse.[145]

Studies in which triblock copolymers consisted of a hydrophilic and thermoresponsive EG-based (meth)acrylate unit and 2-hydroxyethyl (meth)acrylate were reported. In one of the studies, two ABA triblock copolymers based on mDEGMA (A block of constant length) and HEMA (B block of varied length) were compared, and it was revealed that the CP, the CGC and the T_{gel} decreased, while the strength of the formed gels increased by increasing the hydrophobic HEMA content.[131] BAB triblock copolymers with the B block being based on 2-hydroxyethyl acrylate (HEA) and the A block being based either only on methoxy mono(ethylene glycol) acrylate (mMEGA) or a gradient copolymer of HEA and mMEGA were reported.[142] It was observed that the BAB triblock copolymers presented lower CPs than their corresponding triblock-gradient copolymers, thus illustrating an architecture effect on the thermoresponse.[142]

In two of the studies, ATRP facilitated the synthesis of ABA triblock copolymers consisting of an EG-based methacrylate unit and either PCL[141] or 2-methacryloyloxyethyl phosphorylcholine (MPC).[132] When increasing the length of the mOEGA500 block in mOEGA500-*b*-PCL-*b*-mOEGA500 polymers, the CMC and the CP decreased, thus indicating that the MM effect governs the composition effect.[141]

Biocompatible mDEGMA₁₁₃-*b*-MPC₂₄₃-*b*-mDEGMA₁₁₃ copolymers formed physical gels, with the T_{gel} decreasing from 32 to 19 when the concentration increased from 5 to 25 wt%.[132]

Synthesising triblock terpolymers offers the possibility of incorporating different units into the structure, which may provide additional properties, *e.g.*, pH-response. To the best of our knowledge, no study has investigated the effect of architecture of EG-based (meth)acrylate triblock terpolymers, *i.e.*, the position of the blocks, and how it affects the thermoresponsive properties. Thus, this paragraph discusses studies in which the architecture was kept constant. In one of the studies, Liu *et al.* investigated thermo- and pH-responsive ABC triblock copolymers based on monomethoxy poly(ethylene glycol) (mPEG, A block), mDEGMA-*co*-N-hydroxymethyl acrylamide (mDEGMA-*co*-HMAAm, B block) and DEAEMA (C unit).[133] These copolymers presented temperature-driven micellisation at acidic pH, due to the thermoresponse of mDEGMA, and their CP decreased by increasing the content of HMAAm.[133] Double thermoresponsive ABC triblock copolymers were reported by Hu *et al.*[134] These polymers consisted of ethoxy di(ethylene glycol) methacrylate (eDEGMA, A block) and 2-(methacryloyloxy)ethyltrimethylammonium iodide (MAEtMAm, B block), while the C block was based on a random copolymer of mDEGMA with rhodamine-B containing methacrylate (RhoMA). Heating the samples above the CP of eDEGMA resulted in micellisation, while in concentrated solutions, physical hydrogels were formed when the system was heated above the CP of mDEGMA. Interestingly, incorporation of thermoresponsive silica nanoparticles resulted in the formation of a hybrid gel with improved mechanical strength, due to the enhanced intermicellar bridging.[134] Our group has previously reported a study on mOEGMA300-*b*-BuMA-*b*-DEAEMA copolymers, where BuMA stands for *n*-butyl methacrylate, and the aqueous solutions were investigated at an initial pH value, at which the DEAEMA copolymers are not protonated, and thus they are hydrophobic.[140] It was found that gelation was promoted when BuMA and DEAEMA contents increased due to the enhanced hydrophobicity.[140] When replacing the DEAEMA block with the thermoresponsive mDEGMA, and when the composition is targeted appropriately, a promising biocompatible thermogelling system is fabricated, which has a low gelation concentration (2 w/w%) and shows great potential in injectable gel applications.[135,136]

Only our group has previously published a study on EG-based (meth)acrylate tetrablock terpolymers.[137] The composition and MM of the copolymers were kept constant, while the architecture was varied from ABCA, ABAC, ACAB, BACB, BABC, BABC, ABCB, CABC, CACB and ACBC; A, B, and C blocks consisted of mOEGMA300, BuMA, and mDEGMA, respectively. When comparing these architectures, it was concluded that higher CPs are detected for copolymers with the hydrophobic BuMA block being adjacent to the thermoresponsive mDEGMA one, as upon thermoresponse of mDEGMA, self-assembled structures with a BuMA- and mDEGMA-based core and a hydrated OEGMA300 corona may be formed. Similarly, self-assembled structures which can pre-

serve a hydrophilic OEGMA300 corona upon the thermoresponse of mDEGMA favour gelation, with the ABCA architecture forming physical gels at 5 w/w% at physiological temperature.[137]

A study on an (A-co-B)-b-C-b-D-b-C-b-(A-co-B) pentablock quaterpolymer has been published by Papadakis and co-workers.[139] The central D block consisted of EG, while the C block was based on DMAEMA. The outer blocks consisted of a random copolymer of BuMA and methoxy tri(ethylene glycol) methacrylate (mTEGMA). It should be noted that this study was performed in a pH range at which DMAEMA is positively charged, thus the thermoresponse is provided only by mTEGMA. A thorough physicochemical investigation has been performed using a combination of DLS, SLS, SANS and SAXS, which revealed significant hydration of the hydrophobic core and the highly swollen hydrophilic corona, with the number of loops and tangling chains being highly dependent on the temperature and pH.[139]

Thermoresponsive four-arm star copolymers with the arms being formed by a triblock terpolymer have been reported in the literature.[138] The architecture of the arms varied from ABC to ACB, where A, B, and C correspond to CL, mOEGMA500, and mDEGMA, respectively. In either case, the length of the outer block was varied, which resulted in two opposite trends: (i) the longer the mDEGMA block in (ABC)$_4$ star copolymers, the more favoured the thermoresponse was (both CP and gelation), and (ii) the longer the mOEGMA500 block in (ACB)$_4$ star copolymers, the more interrupted the gelation was, due to the increase in hydrophilicity. A 10 wt% solution of an (ABC)$_4$ copolymer formed gels at a physiologically applicable temperature.[138] This study indicates an architecture effect, according to which the position of the block is crucial for promoting gelation.

Polymers based on other thermoresponsive units

Several studies have investigated the thermoresponsive properties of polymers based on VCL, peptides, and oxazolines. Due to the limited number of studies in which the effect of architecture has been investigated, the following paragraphs discuss studies in which generally the effects of the polymer structure, i.e., architecture, composition, and MM, on the thermoresponse have been reported.

Three studies on VCL-based copolymers have been published and the effect of composition and MM on the thermoresponsive properties has been discussed.[147–149] Two of the studies have been carried out by Debuigne's group, in which BAB double thermoresponsive copolymers were studied; the B block consisted of VCL, while the A block was a random copolymer of VCL and N-vinylpyrrolidone (VP).[147,148] It should be pointed out that VP, which consists of a five-membered ring, is more hydrophilic when compared to VCL (seven-membered ring). Two CP values were detected, which correspond to the thermoresponse of VCL and VP. It was observed that the

longer the VCL-based outer blocks, the lower the CP and T_{gel} and the higher the strength of the gels. Addition of salts lowered the thermoresponsive point, due to the ionic strength effect.[147,148] The third study investigated the CP of BAB triblock copolymers based on VCL (A block) and a random copolymer of tBA and AA (B block).[149] In this study, the Turbiscan Lab instrument was used for the first time to determine the CP of these copolymers, with the CP increasing with the content of AA.[149]

To the best of our knowledge, only one study reported thermoresponsive LCST type polypeptides.[150] An elastin-like (AB)$_2$ "tetrablock" copolymer with MESLLP{[(VPGVG)$_2$-(VPGEG)-(VPGVG)$_2$]$_{10}$-b-[VGIPG]$_{60}$}$_2$V was biosynthesised by Martín et al.; the amino acids used are methionine (M), glutamic acid (E), serine (S), leucine (L), proline (P), valine (V), glycine (G), and isoleucine (I). This polypeptide was double-responsive, with the first block being pH-responsive and the second block showing thermoresponse. Temperature-triggered gelation was observed in concentrated samples (5 to 15 wt%), with the storage modulus increasing with the concentration. Interestingly, patterns with different shapes, such as hexagonal, circular, square pits, grooves, and cylindrical pillars, were created via replica molding, thus indicating the potential applicability of these polypeptides in the bioengineering field.[150]

Poly(2-oxazoline)s are a special class of polymers with the tertiary amide bond participating in the backbone of the polymers, Fig. 3.[20] By substituting the side chain with hydrophobic moieties, the hydrophilicity of the structure changes. For example, polymers consisting of 2-methyl-2-oxazoline (MeOx) are very hydrophilic, thus showing no thermoresponse, while polymers based on 2-butyl-2-oxazoline (BuOx) are very hydrophobic, and are thus water-insoluble. Poly(2-oxazoline)s bearing alkyl chains with intermediate lengths are thermoresponsive, with the transition temperature being controlled by the chemical nature of the side chain.[20] For example, high MM polymers of 2-ethyl-2-oxazoline (EtOx) present a CP at around 61 to 69 °C,[169] and polymers of 2-isopropyl-2-oxazoline (iProOx) present a CP at around 26 to 34 °C,[170,171] while their analogues with linear side chains, namely 2-n-propyl-2-oxazoline (nProOx), show a CP at 25 °C.[172] The structure of poly(2-oxazoline)s and their respective LCST values (if any) reported in the literature are summarised in Fig. 11.

A few studies have been reported on the effect of the polymer structure of poly(2-oxazoline)s on their properties. In one of the studies, ABA copolymers based on hydrophilic MeOx (A block) and iProOx-co-BuOx (B block, thermoresponsive) were investigated, and it was found that the higher the content of hydrophobic BuOx, the lower the CP,[154] as expected. Luxenhofer's group reported several studies on oxazoline-based thermogelling triblock copolymers.[152,155,173,174] In three of the studies, the ABA triblock copolymers consisted of hydrophilic MeOx (A unit) and a hydrophobic block based on either 2-isobutyl-2-oxazoline (iBuOx), 2-phenethyl-2-oxazoline (PhEtOx) or 2-benzhydryl oxazine (BzHOx) as the B unit.[155,173,174] While none of these units are thermoresponsive,

Poly(2-methyl-2-oxazoline)
(polyMeOx, hydrophilic,
No CP[20])

Poly(2-ethyl-2-oxazoline)
(polyEtOx, thermoresponsive,
61 °C ≤ CP ≤ 69 °C[169])

Poly(2-n-propyl-2-oxazoline)
(polynProOx, thermoresponsive,
CP ≈ 25 °C[172])

Poly(2-isopropyl-2-oxazoline)
(polyiProOx, thermoresponsive,
26 ≤ CP ≤ 34 °C[170, 171])

Poly(2-n-butyl-2-oxazoline)
(polynBuOx, hydrophobic,
Water-insoluble[20])
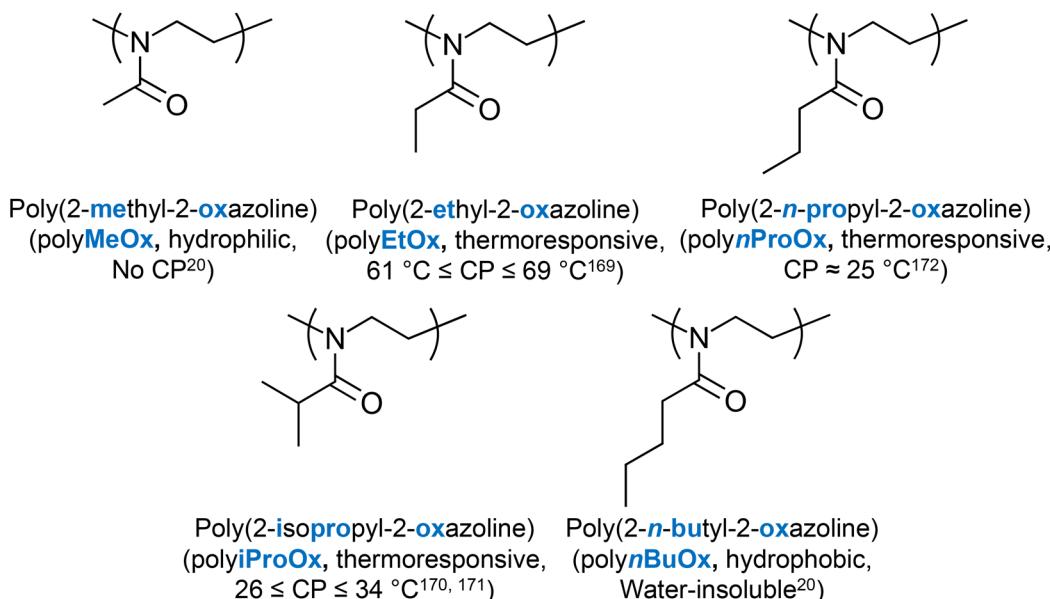
Fig. 11 Chemical structures and properties of poly(2-oxazoline)s.

the combination resulted in the formation of thermo-responsive gels, and by changing the B block from alkyl to aromatic, the thermogelling behaviour changed from the LCST to UCST, when concentrated solutions (20 wt%) were tested.[155,173,174] Intriguingly, the UCST-type thermogel based on PhEtOx was used to fabricate bioink for printing.[173] Interestingly, the same group has investigated the effect of the block position on the thermoresponsive properties of triblock bipolymers, *i.e.*, ABA *versus* BAB.[152] These copolymers consisted of MeOx (A unit) and 2-n-propyl-2-oxazoline (nProOx, B unit, thermoresponsive), and they presented temperature-driven self-assembly, but no gelation. While the BAB architecture showed aggregation, presumably due to the flower-like structure, the ABA one formed smaller self-assembled structures.[152] In a similar study on flower-like micelles adopted by the BAB architecture, where the A and B units are EtOx and nProOx, respectively, it was observed that the content and length of the hydrophilic middle block were crucial in gel formation, with the aqueous solution of a copolymer with 78 wt% of EtOx forming a hydrogel at 20 wt% at physiological temperature.[153]

EtOx (A unit) was combined with either L-LA[175] or CL[151] (B unit) to form degradable BAB triblock copolymers. It was found that the CP of the L-LA-based copolymers increased with the MM,[175] similarly to what has been previously observed for Pluronic® polymers, while the gelation was favoured by increasing the content of the hydrophobic CL,[151] as expected.

Effect of architecture – synopsis

In summary, the architecture has a key role in the thermo-responsive properties of the polymers. However, the effect of architecture depends on the chemical nature of the thermo-responsive units and the repeating units they are copolymerised with. The trends reported in the literature are summarised in the following paragraphs and the general trends identified are listed in Table 2.

The effect of the position of the blocks within the polymer chain on the thermoresponse is highlighted by the triblock bipolymers, *i.e.*, ABA- and BAB-type architecture, Table 2. For example, Pluronic® polymers (ABA) present a CP which increases with the polymer concentration, while their reverse counterparts (BAB) show the opposite trend at the specific concentrations tested that ranged from 5 to 50 mM.[35] The micellisation of these copolymers is also affected by the architecture,[37] with the micellisation of the ABA architecture being favoured compared to the BAB one, presumably due to its self-assembled structure, *i.e.*, core–shell micelles (ABA) *versus* flower-like micelles (BAB); the latter show a lower CP.[37] As far as ABA and BAB triblock copolymers based on PEG (A block) and PLGA (B block) are concerned, the CGC and T_{gel} of the BAB architecture are lower than those of the ABA one, due to the two PLGA outer blocks joining two different adjacent micelles, thus resulting in bridging.[56,60,62,63] Similar trends were observed when substituting the PLGA block with PCL, with the BAB counterpart showing a lower T_{gel}, a wider gelation area and a higher storage modulus[69] In NIPAAm-based polymers, when HEMA was used as a comonomer, the ABA-type copolymers presented a lower T_{gel} than the BAB ones,[93] but when EtA was used instead, the CMC value of the ABA architecture was lower, and the CP was higher than the BAB one.[94] In poly(2-oxazoline)s, aggregation was observed for the BAB copolymers based on MeOx (A unit) and nProOx (B unit), with better-defined self-assembled structures being adopted by the ABA one.[152] Generally, it can be concluded that the for-

Table 2 Effect of architecture on the thermoresponsive properties – synopsis

Architecture	Effect
Triblock Bipolymers ABA vs BAB (A: thermoresponsive, B: hydrophobic)	$CP_{BAB} < CP_{ABA}$ [37,94] $CMC_{ABA} < CMC_{BAB}$ [94] $CGC_{BAB} < CGC_{ABA}$ [56,60,62,63] $T_{gel, BAB} < T_{gel, ABA}$ [56,60,62,63,69] $G'_{BAB} > G'_{ABA}$ [69] ABC: clear sol–gel transition [26,124,126]
Triblock Terpolymers ABC vs ACB vs BAC (A: hydrophilic, B: hydrophobic, C: thermoresponsive)	When C is next to B → $\uparrow$CP & $\downarrow T_{gel}$ & $\downarrow$CGC [127,137]
Tetrablock Terpolymers ABCA vs ABAC vs ACAB vs BACB vs BABC vs ABCB vs CABC vs CACB vs ACBC (A: hydrophilic, B: hydrophobic, C: thermoresponsive) **Two A blocks** **Two B blocks** **Two C blocks**	When B is an outer block → Gelation [128]
Multiblock Bipolymers BAB vs BABABAB vs ABABABABA (A: thermoresponsive, B: hydrophobic)	
Linear Block vs Star Copolymers Case 1: vs Case 2: vs	$CP_{star} < CP_{linear}$ [143] $T_{gel, star} < T_{gel, linear}$ [116]

Abbreviations: CP, cloud point; CMC, critical micellisation concentration; CGC, critical gelation concentration; T_{gel}, gelation temperature; G', storage modulus. Hydrophilic, hydrophobic, and thermoresponsive blocks are shown in blue, purple, and orange, respectively. In the case of Pluronic® polymers and their reverse counterparts, the B block, namely PPG, is also thermoresponsive at lower temperatures, and its thermoresponse promotes the self-assembly.

mation of well-defined micelles by the ABA architecture is favoured due to the formation of traditional core–shell micelles, as the adaptation of flower-like micelles might be less favourable entropically. As far as gelation is concerned, the BAB architecture with the B unit being hydrophobic favours the formation of the network by bridging of adjacent flower-like micelles.

Moving to triblock terpolymers, to the best of our knowledge, only our group has reported the effect of architecture within the triblock terpolymer structure.[26,124,126] It has been concluded that the ABC architecture outperforms the ACB and BAC architectures by presenting a clear sol–gel transition, i.e., a transition from a solution to gel without solubility issues, upon heating; the A, B and C blocks were based on an EG-based methacrylate unit, an alkyl methacrylate unit, and DMAEMA, respectively.[26,124,126]

Concerning tetrablock copolymers, our group has systematically investigated the effect of the block position within the tetrablock terpolymer architecture in both DMAEMA-[127] and DEGMA-containing[137] thermoresponsive polymers. In both studies the hydrophilic and hydrophobic blocks were based on mOEGMA300 (A block) and BuMA (B block), respectively, while DMAEMA or DEGMA were the C block. It has been generally observed that architectures with the thermoresponsive block being adjacent to the hydrophobic one show a higher CP, presumably due to the re-arrangement of the core–shell micelles upon heating, with the thermoresponsive block collapsing in the hydrophobic block upon thermoresponse. Interestingly, these structures favour thermogelation, as this re-arrangement might lead to the formation of well-hydrated mOEGMA300 bridges, thus leading to network formation. Due to the different chemical nature of these two families, i.e., ionic versus non-ionic, the best architectures were ACBC and ABCA for the DMAEMA- and DEGMA-containing polymers, respectively.[127,137]

When multiblock bipolymers consisting of DMAEMA (A unit) and BuMA (B unit) were systematically compared, only the BAB triblock and BABABAB heptablock copolymers showed gelation, while the corresponding ABABABABA nonablock copolymer did not.[128] This was attributed to the hydrophobic outer blocks facilitating bridging, in contrast to the positively charged DMAEMA outer blocks preventing gelation.[128]

Increasing the transition to a more complex topology, specifically from a linear block to a star structure generally favours thermoresponse. For example, in NIPAAm-containing polymers, lower T_{gel} and stronger gels were formed by the $(ABC)_4$ architecture compared to the corresponding ABC one.[116] Similar findings were reported when the ABCBA pentablock terpolymer and the ABC triblock terpolymer were compared.[116] Changing the architecture from AB to BAB to $(BA)_3$, in mDEGA-containing polymers, reduced the CP.[143]

Conclusions

Thermoresponsive polymers are polymers whose solubility changes as a response to temperature. Amongst them, LCST-type polymers are of major importance in biomedical applications. In this review, we summarised the studies in which thermoresponsive block copolymers of increasing architecture complexity have been reported. We have identified four main categories of polymers, depending on the general chemical structures, such as Pluronic®-, EG-containing degradable, acrylamide-, and EG (meth)acrylate-based polymers. Other thermoresponsive families, such as poly(2-oxazoline)s, are also discussed. The number of blocks and the position of the blocks within the polymer chain are of major importance, with BAB triblock bipolymers favouring gelation over their ABA counterparts, due to efficient micelle bridging; A and B are thermoresponsive and hydrophobic, respectively. In triblock and tetrablock terpolymers, architectures with (i) the hydrophilic and/or thermoresponsive blocks at the end of the polymer chain, surrounding the hydrophobic one, and (ii) the thermoresponsive block being next to the hydrophobic block (in tetrablock terpolymers), favour thermogelation. This may be attributed to the easier rearrangement of the micelles upon thermoresponse, while preserving well-hydrated bridges. Moving from linear to star architectures, thermoresponse is favoured as the complexity of architecture increases. It should be kept in mind that although in this review we aimed to compare how the repeating unit/block position affects the thermoresponse, accurate comparisons can only be made when the composition and the overall MM are kept constant, as both parameters affect the thermoresponsive properties.

Conflicts of interest

There are no conflicts to declare.

Acknowledgements

References

1 N. T. Southall, K. A. Dill and A. D. J. Haymet, *J. Phys. Chem. B*, 2002, **106**, 521–533.
2 J. C. Foster, I. Akar, M. C. Grocott, A. K. Pearce, R. T. Mathers and R. K. O'Reilly, *ACS Macro Lett.*, 2020, 1700–1707.
3 V. Nele, J. P. Wojciechowski, J. P. K. Armstrong and M. M. Stevens, *Adv. Funct. Mater.*, 2020, **30**, 2002759.
4 M. T. Cook, P. Haddow, S. B. Kirton and W. J. McAuley, *Adv. Funct. Mater.*, 2021, **31**, 2008123.
5 A. P. Constantinou and T. K. Georgiou, *Polym. Int.*, 2021, **70**, 1433–1448.
6 C. De Las Heras Alarcón, S. Pennadam and C. Alexander, *Chem. Soc. Rev.*, 2005, **34**, 276–285.
7 S. Ikegami and H. Hamamoto, *Chem. Rev.*, 2009, **109**, 583–593.

8 H. Hamamoto, Y. Suzuki, Y. M. A. Yamada, H. Tabata, H. Takahashi and S. Ikegami, *Angew. Chem., Int. Ed.*, 2005, **44**, 4536–4538.

9 D. E. Bergbreiter, B. L. Case, Y. Liu and J. W. Caraway, *Macromolecules*, 1998, **31**, 6053–6062.

10 I. Lokuge, X. Wang and P. W. Bohn, *Langmuir*, 2007, **23**, 305–311.

11 K. Nishimori, M. Maruyama, Y. Shimazaki, M. Ouchi and H. Yoshida, *ACS Appl. Polym. Mater.*, 2019, **1**, 1925–1929.

12 M. Zhang, A. Vora, W. Han, R. J. Wojtecki, H. Maune, A. B. A. Le, L. E. Thompson, G. M. McClelland, F. Ribet, A. C. Engler and A. Nelson, *Macromolecules*, 2015, **48**, 6482–6488.

13 V. G. Rocha, E. García-Tuñón, C. Botas, F. Markoulidis, E. Feilden, E. D'Elia, N. Ni, M. Shaffer and E. Saiz, *ACS Appl. Mater. Interfaces*, 2017, **9**, 37136–37145.

14 V. Pertici, T. Trimaille and D. Gigmes, *Macromolecules*, 2020, **53**, 682–692.

15 B. V. K. J. Schmidt, *Macromol. Rapid Commun.*, 2022, 2100895.

16 S. Lanzalaco and E. Armelin, *Gels*, 2017, **3**, 36.

17 Q. Li, A. P. Constantinou and T. K. Georgiou, *J. Polym. Sci.*, 2021, **59**, 230–239.

18 G. Vancoillie, D. Frank and R. Hoogenboom, *Prog. Polym. Sci.*, 2014, **39**, 1074–1095.

19 J. Liu, A. Debuigne, C. Detrembleur and C. Jérôme, *Adv. Healthcare Mater.*, 2014, **3**, 1941–1968.

20 R. Hoogenboom and H. Schlaad, *Polym. Chem.*, 2017, **8**, 24–40.

21 A. D. McNaught and A. Wilkinson, **https://goldbook.iupac.org/terms/view/B00685**, (accessed 2020).

22 A. P. Constantinou, G. Patias, B. Somuncuoğlu, T. Brock, D. W. Lester, D. M. Haddleton and T. K. Georgiou, *Polym. Chem.*, 2021, **12**, 3522–3532.

23 N. Ghasdian, D. M. A. Buzza, P. D. I. Fletcher and T. K. Georgiou, *Macromol. Rapid Commun.*, 2015, **36**, 528–532.

24 X. Zhang, C. Contini, A. P. Constantinou, J. J. Doutch and T. K. Georgiou, *J. Polym. Sci.*, 2021, **59**, 1724–1731.

25 Y. Cai, K. B. Aubrecht and R. B. Grubbs, *J. Am. Chem. Soc.*, 2011, **133**, 1058–1065.

26 M. A. Ward and T. K. Georgiou, *Polym. Chem.*, 2013, **4**, 1893–1902.

27 S. Sugihara, K. Hashimoto, S. Okabe, M. Shibayama, S. Kanaoka and S. Aoshima, *Macromolecules*, 2004, **37**, 336–343.

28 M. A. da Silva, P. Haddow, S. B. Kirton, W. J. McAuley, L. Porcar, C. A. Dreiss and M. T. Cook, *Adv. Funct. Mater.*, 2021, 2109010.

29 G. Gody, P. B. Zetterlund, S. Perrier and S. Harrisson, *Nat. Commun.*, 2016, **7**, 10514.

30 V. P. Beyer, J. Kim and C. R. Becer, *Polym. Chem.*, 2020, **11**, 1271–1291.

31 M. Sahn, T. Yildirim, M. Dirauf, C. Weber, P. Sungur, S. Hoeppener and U. S. Schubert, *Macromolecules*, 2016, **49**, 7257–7267.

32 M. Vadnere, G. Amidon, S. Lindenbaum and J. L. Haslam, *Int. J. Pharm.*, 1984, **22**, 207–218.

33 K. H. Sun, Y. S. Sohn and B. Jeong, *Biomacromolecules*, 2006, **7**, 2871–2877.

34 M. Almeida, M. Magalhães, F. Veiga and A. Figueiras, *J. Polym. Res.*, 2017, **25**, 31.

35 B. Naskar, S. Ghosh and S. P. Moulik, *Langmuir*, 2012, **28**, 7134–7146.

36 J. P. Mata, P. R. Majhi, C. Guo, H. Z. Liu and P. Bahadur, *J. Colloid Interface Sci.*, 2005, **292**, 548–556.

37 Z. Zhou and B. Chu, *Macromolecules*, 1994, **27**, 2025–2033.

38 F. Markus, J. R. Bruckner and S. Naumann, *Macromol. Chem. Phys.*, 2020, **221**, 1900437.

39 C. Bar, N. Çağlar, M. Uz, S. K. Mallapragada and S. A. Altinkaya, *ACS Appl. Mater. Interfaces*, 2019, **11**, 31367–31377.

40 M. D. Determan, J. P. Cox, S. Seifert, P. Thiyagarajan and S. K. Mallapragada, *Polymer*, 2005, **46**, 6933–6946.

41 B. C. Anderson, S. M. Cox, P. D. Bloom, V. V. Sheares and S. K. Mallapragada, *Macromolecules*, 2003, **36**, 1670–1676.

42 M. D. Determan, J. P. Cox and S. K. Mallapragada, *J. Biomed. Mater. Res.*, 2007, **81A**, 326–333.

43 M. D. Determan, L. Guo, C. Lo, P. Thiyagarajan and S. K. Mallapragada, *Phys. Rev. E: Stat., Nonlinear, Soft Matter Phys.*, 2008, **78**, 021802.

44 A. Agarwal, R. Unfer and S. K. Mallapragada, *J. Controlled Release*, 2005, **103**, 245–258.

45 S. Peleshanko, K. D. Anderson, M. Goodman, M. D. Determan, S. K. Mallapragada and V. V. Tsukruk, *Langmuir*, 2007, **23**, 25–30.

46 M. Uz, S. K. Mallapragada and S. A. Altinkaya, *RSC Adv.*, 2015, **5**, 43515–43527.

47 A. Mei, X. Guo, Y. Ding, X. Zhang, J. Xu, Z. Fan and B. Du, *Macromolecules*, 2010, **43**, 7312–7320.

48 P. Parekh, S. Ohno, S. Yusa, C. Lv, B. Du, D. Ray, V. K. Aswal and P. Bahadur, *Polym. Int.*, 2020, **69**, 1113–1121.

49 Y. Wu, X. Liu, Y. Wang, Z. Guo and Y. Feng, *Macromol. Chem. Phys.*, 2012, **213**, 1489–1498.

50 D. Cohn, A. Sosnik and A. Levy, *Biomaterials*, 2003, **24**, 3707–3714.

51 G. M. Zentner, R. Rathi, C. Shih, J. C. McRea, M. Seo, H. Oh, B. G. Rhee, J. Mestecky, Z. Moldoveanu, M. Morgan and S. Weitman, *J. Controlled Release*, 2001, **72**, 203–215.

52 R. C. Rathi, G. M. Zentner and B. Jeong, MacoMed Inc. US6201072B1, 2001.

53 R. C. Rathi, G. M. Zentner and B. Jeong, MacroMed Inc. US6117947, 2000.

54 R. C. Rathi and G. M. Zentner, MacroMed Inc. US6004573, 1999.

55 D. Lee, M. Shim, S. Kim, H. Lee, I. Park and T. Chang, *Macromol. Rapid Commun.*, 2001, **22**, 587–592.

56 M. S. Shim, H. T. Lee, W. S. Shim, I. Park, H. Lee, T. Chang, S. W. Kim and D. S. Lee, *J. Biomed. Mater. Res.*, 2002, **61**, 188–196.

57 N. Y. Steinman, M. Haim-Zada, I. A. Goldstein, A. H. Goldberg, T. Haber, J. M. Berlin and A. J. Domb, *J. Polym. Sci., Part A: Polym. Chem.*, 2019, **57**, 35–39.

58 L. L. Osorno, D. E. Maldonado, R. J. Whitener, A. N. Brandley, A. Yiantsos, J. D. R. Medina and M. E. Byrne, *J. Appl. Polym. Sci.*, 2020, **137**, 48678.

59 N. K. Khorshid, K. Zhu, K. D. Knudsen, S. Bekhradnia, S. A. Sande and B. Nyström, *Macromol. Biosci.*, 2016, **16**, 1838–1852.

60 B. Jeong, Y. H. Bae and S. W. Kim, *Macromolecules*, 1999, **32**, 7064–7069.

61 C. Chen, L. Chen, L. Cao, W. Shen, L. Yu and J. Ding, *RSC Adv.*, 2014, **4**, 8789–8798.

62 Y. J. Kim and S. W. Kim, *Controlled Drug Delivery from Injectable Biodegradable Triblock Copolymer*, Polymer Gels, ACS symposium series, 2002, ch. 20, pp. 300–311.

63 S. Cui, L. Yu and J. Ding, *Macromolecules*, 2019, **52**, 3697–3715.

64 J. E. Nielsen, K. Zhu, S. A. Sande, L. Kováčik, D. Cmarko, K. D. Knudsen and B. Nyström, *J. Phys. Chem. B*, 2017, **121**, 4885–4899.

65 D. A. Prince, I. J. Villamagna, C. C. Hopkins, J. R. de Bruyn and E. R. Gillies, *Polym. Int.*, 2019, **68**, 1074–1083.

66 L. Yu, W. Sheng, D. Yang and J. Ding, *Macromol. Res.*, 2013, **21**, 207–215.

67 N. Safaei Nikouei and A. Lavasanifar, *Acta Biomater.*, 2011, **7**, 3708–3718.

68 N. S. Nikouei, M. R. Vakili, M. S. Bahniuk, L. Unsworth, A. Akbari, J. Wu and A. Lavasanifar, *Acta Biomater.*, 2015, **12**, 81–92.

69 S. J. Bae, J. M. Suh, Y. S. Sohn, Y. H. Bae, S. W. Kim and B. Jeong, *Macromolecules*, 2005, **38**, 5260–5265.

70 Y. Ohya, H. Yamamoto, K. Nagahama and T. Ouchi, *J. Polym. Sci., Part A: Polym. Chem.*, 2009, **47**, 3892–3903.

71 M. Mohammadi, K. Patel, S. P. Alaie, R. B. Shmueli, C. G. Besirli, R. G. Larson and J. J. Green, *Acta Biomater.*, 2018, **73**, 90–102.

72 S. Bobbala, V. Tamboli, A. McDowell, A. K. Mitra and S. Hook, *AAPS J.*, 2016, **18**, 261–269.

73 H. Mao, G. Shan, Y. Bao, Z. L. Wu and P. Pan, *Soft Matter*, 2016, **12**, 4628–4637.

74 D. Skoulas, G. Mangiapia, D. Parisi, M. Kasimatis, E. Glynos, E. Stratikos, D. Vlassopoulos, H. Frielinghaus and H. Iatrou, *Macromolecules*, 2021, **54**, 10786–10800.

75 Z. Li, Z. Zhang, K. L. Liu, X. Ni and J. Li, *Biomacromolecules*, 2012, **13**, 3977–3989.

76 C. Liu, Z. Zhang, K. L. Liu, X. Ni and J. Li, *Soft Matter*, 2013, **9**, 787–794.

77 J. Zhao, J. Jeromenok, J. Weber and H. Schlaad, *Macromol. Biosci.*, 2012, **12**, 1272–1278.

78 E. Kostyurina, J. U. De Mel, A. Vasilyeva, M. Kruteva, H. Frielinghaus, M. Dulle, L. Barnsley, S. Förster, G. J. Schneider, R. Biehl and J. Allgaier, *Macromolecules*, 2022, **55**(5), 1552–1565.

79 A. Papagiannopoulos, J. Zhao, G. Zhang, S. Pispas and A. Radulescu, *Eur. Polym. J.*, 2014, **56**, 59–68.

80 J. Adelsberger, A. Kulkami, A. Jain, W. Wang, A. M. Bivigou-Koumba, P. Busch, V. Pipich, O. Holderer, T. Hellweg, A. Laschewsky, P. Müller-Buschbaum and C. M. Papadakis, *Macromolecules*, 2010, **43**, 2490–2501.

81 J. Adelsberger, E. Metwalli, A. Diethert, I. Grillo, A. M. Bivigou-Koumba, A. Laschewsky, P. Müller-Buschbaum and C. M. Papadakis, *Macromol. Rapid Commun.*, 2012, **33**, 254–259.

82 J. Adelsberger, I. Grillo, A. Kulkarni, M. Sharp, A. M. Bivigou-Koumba, A. Laschewsky, P. Müller-Buschbaum and C. M. Papadakis, *Soft Matter*, 2013, **9**, 1685–1699.

83 A. M. Bivigou-Koumba, E. Görnitz, A. Laschewsky, P. Müller-Buschbaum and C. M. Papadakis, *Colloid Polym. Sci.*, 2010, **288**, 499–517.

84 C. Kuo, T. Liu, A. Hardiansyah, C. Lee, M. Wang and W. Chiu, *Nanoscale Res. Lett.*, 2014, **9**, 520.

85 Z. Lin, S. Cao, X. Chen, W. Wu and J. Li, *Biomacromolecules*, 2013, **14**, 2206–2214.

86 N. Cakir, G. Hizal and C. R. Becer, *Polym. Chem.*, 2015, **6**, 6623–6631.

87 E. Karjalainen, V. Khlebnikov, A. Korpi, S. Hirvonen, S. Hietala, V. Aseyev and H. Tenhu, *Polymer*, 2015, **58**, 180–188.

88 A. Maleki, K. Zhu, R. Pamies, R. R. Schmidt, A. Kjøniksen, G. Karlsson, J. G. Hernández Cifre, J. García De La Torre and B. Nyström, *Soft Matter*, 2011, **7**, 8111–8119.

89 H. Cong, J. Li, L. Li and S. Zheng, *Eur. Polym. J.*, 2014, **61**, 23–32.

90 L. Mi, H. Xue, Y. Li and S. Jiang, *Adv. Funct. Mater.*, 2011, **21**, 4028–4034.

91 T. Uemukai, T. Hioki and M. Ishifune, *Int. J. Polym. Sci.*, 2013, **2013**, 196145.

92 Y. Luo, J. Zhang, F. Han, F. Xu, Y. Chen and R. Liu, *J. Appl. Polym. Sci.*, 2015, **132**, 41877.

93 X. Zhao, W. Liu, D. Chen, X. Lin and W. W. Lu, *Macromol. Chem. Phys.*, 2007, **208**, 1773–1781.

94 Y. Yu, D. Hong, Z. Liu, F. Jia, Y. Zhou and C. Leng, *J. Polym. Res.*, 2013, **20**, 235.

95 X. Cao, Y. Chen, W. Chai, W. Zhang, Y. Wang and P. Fu, *J. Appl. Polym. Sci.*, 2015, **132**, 41361.

96 J. Chen, M. Liu, H. Gong, Y. Huang and C. Chen, *J. Phys. Chem. B*, 2011, **115**, 14947–14955.

97 Y. Zheng, L. Wang, R. Yu and S. Zheng, *Macromol. Chem. Phys.*, 2012, **213**, 458–469.

98 Q. Li, F. Huo, Y. Cui, C. Gao, S. Li and W. Zhang, *J. Polym. Sci., Part A: Polym. Chem.*, 2014, **52**, 2266–2278.

99 Y. Luo, L. Liu, X. Wang, H. Shi, W. Lv and J. Li, *Soft Matter*, 2012, **8**, 1634–1642.

100 C. Wu, A. Ying and S. Ren, *Colloid Polym. Sci.*, 2013, **291**, 827–834.

101 C. Zhou, M. A. Hillmyer and T. P. Lodge, *J. Am. Chem. Soc.*, 2012, **134**, 10365–10368.

102 C. C. Hall, C. Zhou, S. P. O. Danielsen and T. P. Lodge, *Macromolecules*, 2016, **49**, 2298–2306.

103 C. Zhou, G. E. S. Toombes, M. J. Wasbrough, M. A. Hillmyer and T. P. Lodge, *Macromolecules*, 2015, **48**, 5934–5943.

104 M. Onoda, T. Ueki, R. Tamate, A. M. Akimoto, C. C. Hall, T. P. Lodge and R. Yoshida, *ACS Macro Lett.*, 2018, **7**, 950–955.

105 C. Wang, G. Zhang, G. Liu, J. Hu and S. Liu, *J. Controlled Release*, 2017, **259**, 149–159.

106 A. Skandalis and S. Pispas, *Polymer*, 2018, **157**, 9–18.

107 D. Giaouzi and S. Pispas, *Polymers*, 2020, **12**, 1382.

108 Z. Ge, Y. Zhou, Z. Tong and S. Liu, *Langmuir*, 2011, **27**, 1143–1151.

109 J. Chen, M. Liu, H. Gong, G. Cui, S. Lü, C. Gao, F. Huang, T. Chen, X. Zhang and Z. Liu, *Polym. Chem.*, 2013, **4**, 1815–1825.

110 X. Li, R. Fan, Y. Wang, M. Wu, A. Tong, J. Shi, M. Xiang, L. Zhou and G. Guo, *RSC Adv.*, 2015, **5**, 101494–101506.

111 G. Isapour, R. Lund, K. Zhu, Z. Quan, K. D. Knudsen and B. Nyström, *Eur. Polym. J.*, 2015, **70**, 79–93.

112 H. S. Abandansari, E. Aghaghafari, M. R. Nabid and H. Niknejad, *Polymer*, 2013, **54**, 1329–1340.

113 V. Pertici, C. Pin-Barre, C. Rivera, C. Pellegrino, J. Laurin, D. Gigmes and T. Trimaille, *Biomacromolecules*, 2019, **20**, 149–163.

114 C. Lv, J. Gao, K. An, J. Nie, J. Xu and B. Du, *Macromolecules*, 2021, **54**, 6489–6501.

115 A. Simula, V. Nikolaou, A. Anastasaki, F. Alsubaie, G. Nurumbetov, P. Wilson, K. Kempe and D. M. Haddleton, *Polym. Chem.*, 2015, **6**, 2226–2233.

116 G. Barouti, S. S. Liow, Q. Dou, H. Ye, C. Orione, S. M. Guillaume and X. J. Loh, *Chem. – Eur. J.*, 2016, **22**, 10501–10512.

117 M. Teodorescu, I. Negru, P. O. Stanescu, C. Draghici, A. Lungu and A. Sârbu, *J. Macromol. Sci., Pure Appl. Chem.*, 2011, **48**, 177–185.

118 P. J. Haddow, M. A. da Silva, D. B. Kaldybekov, C. A. Dreiss, E. Hoffman, V. Hutter, V. V. Khutoryanskiy, S. B. Kirton, N. Mahmoudi, W. J. McAuley and M. T. Cook, *Macromol. Biosci.*, 2021, 2100432.

119 Z. Sun, Y. Tian, W. L. Hom, O. Gang, S. R. Bhatia and R. B. Grubbs, *Angew. Chem., Int. Ed.*, 2017, **56**, 1491–1494.

120 H. Arslan, O. Zırtıl and V. Bütün, *Eur. Polym. J.*, 2013, **49**, 4118–4129.

121 L. Lauber, J. Santarelli, O. Boyron, C. Chassenieux, O. Colombani and T. Nicolai, *Macromolecules*, 2017, **50**, 416–423.

122 M. A. Ward and T. K. Georgiou, *J. Polym. Sci., Part A: Polym. Chem.*, 2013, **51**, 2850–2859.

123 M. A. Ward and T. K. Georgiou, *Soft Matter*, 2012, **8**, 2737–2745.

124 M. A. Ward and T. K. Georgiou, *J. Polym. Sci., Part A: Polym. Chem.*, 2010, **48**, 775–783.

125 A. P. Constantinou and T. K. Georgiou, *Polym. Chem.*, 2016, **7**, 2045–2056.

126 A. P. Constantinou, H. Zhao, C. M. McGilvery, A. E. Porter and T. K. Georgiou, *Polymers*, 2017, **9**, 31.

127 A. P. Constantinou, N. Sam-Soon, D. R. Carroll and T. K. Georgiou, *Macromolecules*, 2018, **51**, 7019–7031.

128 M. Popescu, I. Athanasoulias, C. Tsitsilianis, N. A. Hadjiantoniou and C. S. Patrickios, *Soft Matter*, 2010, **6**, 5417–5424.

129 T. Sanal, O. Oruç, T. Öztürk and B. Hazer, *J. Polym. Res.*, 2015, **22**, 3.

130 X. Xiang, X. Ding, N. Chen, B. Zhang and P. A. Heiden, *J. Polym. Sci., Part A: Polym. Chem.*, 2015, **53**, 2838–2848.

131 Y. Zhang and W. Zhao, *Iran. Polym. J.*, 2015, **24**, 481–490.

132 M. Nagao, J. Sengupta, D. Diaz-Dussan, M. Adam, M. Wu, J. Acker, R. Ben, K. Ishihara, H. Zeng, Y. Miura and R. Narain, *ACS Appl. Bio Mater.*, 2018, **1**, 356–366.

133 S. Liu, L. Tian, H. Mao, W. Ning, P. Shang, J. Wu and X. Shi, *J. Polym. Res.*, 2018, **25**, 264.

134 B. Hu, W. Fu and B. Zhao, *Macromolecules*, 2016, **49**, 5502–5513.

135 A. P. Constantinou, B. Zhan and T. K. Georgiou, *Macromolecules*, 2021, **54**, 1943–1960.

136 A. P. Constantinou, V. Nele, J. J. Doutch, J. S. Correia, R. V. Moiseev, M. Cihova, D. C. A. Gaboriau, J. Krell, V. V. Khutoryanskiy, M. M. Stevens and T. K. Georgiou, *Macromolecules*, 2022, **55**(5), 1783–1799.

137 A. P. Constantinou, K. Zhang, B. Somuncuoğlu, B. Feng and T. K. Georgiou, *Macromolecules*, 2021, **54**(13), 6511–6524.

138 W. Zhu, A. Nese and K. Matyjaszewski, *J. Polym. Sci., Part A: Polym. Chem.*, 2011, **49**, 1942–1952.

139 F. A. Jung, P. A. Panteli, C. Ko, J. Kang, L. C. Barnsley, C. Tsitsilianis, C. S. Patrickios and C. M. Papadakis, *Macromolecules*, 2019, **52**, 9746–9758.

140 A. P. Constantinou, T. Lan, D. R. Carroll and T. K. Georgiou, *Eur. Polym. J.*, 2020, **130**, 109655.

141 M. Luzón, T. Corrales, F. Catalina, V. San Miguel, C. Ballesteros and C. Peinado, *J. Polym. Sci., Part A: Polym. Chem.*, 2010, **48**, 4909–4921.

142 W. Steinhauer, R. Hoogenboom, H. Keul and M. Moeller, *Macromolecules*, 2013, **46**, 1447–1460.

143 A. Miasnikova and A. Laschewsky, *J. Polym. Sci., Part A: Polym. Chem.*, 2012, **50**, 3313–3323.

144 A. Miasnikova, A. Laschewsky, G. De Paoli, C. M. Papadakis, P. Müller-Buschbaum and S. S. Funari, *Langmuir*, 2012, **28**, 4479–4490.

145 Q. Zhong, E. Metwalli, M. Rawolle, G. Kaune, A. M. Bivigou-Koumba, A. Laschewsky, C. M. Papadakis, R. Cubitt and P. Müller-Buschbaum, *Macromolecules*, 2013, **46**, 4069–4080.

146 I. Negru, M. Teodorescu, P. O. Stanescu, C. Draghici, A. Lungu and A. Sârbu, *Soft Mater.*, 2013, **11**, 149–156.

147 A. Kermagoret, K. Mathieu, J. Thomassin, C. Fustin, R. Duchêne, C. Jérôme, C. Detrembleur and A. Debuigne, *Polym. Chem.*, 2014, **5**, 6534–6544.

148 J. Thomassin, K. Mathieu, A. Kermagoret, C. Fustin, C. Jérôme and A. Debuigne, *Polym. Chem.*, 2015, **6**, 1856–1864.

149 M. L. Tebaldi, L. A. Fiel, A. M. Santos, S. S. Guterres and A. R. Pohlmann, *J. Macromol. Sci., Part A: Pure Appl. Chem.*, 2013, **50**, 581–587.

150 L. Martín, F. J. Arias, M. Alonso, C. García-Arévalo and J. C. Rodríguez-Cabello, *Soft Matter*, 2010, **6**, 1121–1124.

151 C. Kim, S. C. Lee, S. W. Kang, I. C. Kwon and S. Y. Jeong, *J. Polym. Sci., Part B: Polym. Phys.*, 2000, **38**, 2400–2408.

152 A. Zahoranová, M. Mrlík, K. Tomanová, J. Kronek and R. Luxenhofer, *Macromol. Chem. Phys.*, 2017, **218**, 1700031.

153 B. D. Monnery and R. Hoogenboom, *Polym. Chem.*, 2019, **10**, 3480–3487.

154 M. Hruby, S. K. Filippov, J. Panek, M. Novakova, H. Mackova, J. Kucka, D. Vetvicka and K. Ulbrich, *Macromol. Biosci.*, 2010, **10**, 916–924.

155 M. M. Lübtow, M. Mrlik, L. Hahn, A. Altmann, M. Beudert, T. Lühmann and R. Luxenhofer, *J. Funct. Biomater.*, 2019, **10**, 36.

156 M. Wagner, C. Pietsch, A. Kerth, A. Traeger and U. S. Schubert, *J. Polym. Sci., Part A: Polym. Chem.*, 2015, **53**, 924–935.

157 P. Alexandridis and J. F. Holzwarth, *Langmuir*, 1997, **13**, 6074–6082.

158 T. K. Georgiou, M. Vamvakaki, C. S. Patrickios, E. N. Yamasaki and L. A. Phylactou, *Biomacromolecules*, 2004, **5**, 2221–2229.

159 P. van de Wetering, J. Cherng, H. Talsma and W. E. Hennink, *J. Controlled Release*, 1997, **49**, 59–69.

160 P. van de Wetering, E. E. Moret, N. Schuurmans-Nieuwenbroek, M. J. van Steenbergen and W. E. Hennink, *Bioconjugate Chem.*, 1999, **10**, 589–597.

161 C. V. Synatschke, A. Schallon, V. Jérôme, R. Freitag and A. H. E. Müller, *Biomacromolecules*, 2011, **12**, 4247–4255.

162 T. Okano and K. Kim, *Regener. Ther.*, 2020, **14**, 330–331.

163 N. Ghasemi, M. R. Vakili and A. Lavasanifar, *ACS Appl. Polym. Mater.*, 2021, **3**, 2608–2617.

164 A. Narumi, S. Sato, X. Shen and T. Kakuchi, *Polym. Chem.*, 2022, **13**, 1293–1319.

165 L. D. Taylor and L. D. Cerankowski, *J. Polym. Sci., Polym. Chem. Ed.*, 1975, **13**, 2551–2570.

166 I. Idziak, D. Avoce, D. Lessard, D. Gravel and X. X. Zhu, *Macromolecules*, 1999, **32**, 1260–1263.

167 J. Lutz, A. Hoth and K. Schade, *Des. Monomers Polym.*, 2009, **12**, 343–353.

168 J. Lutz, *Adv. Mater.*, 2011, **23**, 2237–2243.

169 P. Lin, C. Clash, E. M. Pearce, T. K. Kwei and M. A. Aponte, *J. Polym. Sci., Part B: Polym. Phys.*, 1988, **26**, 603–619.

170 J. Zhao, R. Hoogenboom, G. Van Assche and B. Van Mele, *Macromolecules*, 2010, **43**, 6853–6860.

171 U. Hiroshi and K. Shiro, *Chem. Lett.*, 1992, **21**, 1643–1646.

172 J. Park and K. Kataoka, *Macromolecules*, 2007, **40**, 3599–3609.

173 L. Hahn, E. Karakaya, T. Zorn, B. Sochor, M. Maier, P. Stahlhut, S. Forster, K. Fischer, S. Seiffert, A. Pöppler, R. Detsch and R. Luxenhofer, *Biomacromolecules*, 2021, **22**, 3017–3027.

174 L. Hahn, L. Keßler, L. Polzin, L. Fritze, S. Forster, H. Helten and R. Luxenhofer, *Macromol. Chem. Phys.*, 2021, **222**, 2100114.

175 C. Wang and G. Hsiue, *Biomacromolecules*, 2003, **4**, 1487–1490.