



HIV detection from human serum with paper-based isotachophoretic RNA extraction and reverse transcription recombinase polymerase amplification

Journal:	<i>Analyst</i>
Manuscript ID	AN-ART-12-2020-002483.R1
Article Type:	Paper
Date Submitted by the Author:	18-Mar-2021
Complete List of Authors:	Bender, Andrew; University of Washington, Mechanical Engineering Sullivan, Benjamin; University of Washington, Mechanical Engineering Zhang, Jane; University of Washington, Mechanical Engineering Juergens, David; University of Washington, Chemical Engineering Lillis, Lorraine; PATH Boyle, David; PATH Posner, Jonathan; University of Washington, Mechanical Engineering

1
2
3
4
5 **HIV detection from human serum with paper-based**
6 **isotachophoretic RNA extraction and reverse transcription**
7 **recombinase polymerase amplification**
8
9
10
11

12 Andrew T. Bender¹, Benjamin P. Sullivan¹, Jane Y. Zhang¹, David C. Juergens², Lorraine
13 Lillis³, David S. Boyle³, and Jonathan D. Posner^{1,2,4}
14
15
16
17

18 ¹ Department of Mechanical Engineering, University of Washington, Seattle, USA
19

20 ² Department of Chemical Engineering, University of Washington, Seattle, USA
21

22 ³ PATH, Seattle, USA
23

24 ⁴ Family Medicine, School of Medicine, University of Washington, Seattle, USA
25
26
27
28
29

30 *Correspondence should be addressed to the following author(s):
31

32 Jonathan D. Posner (Professor)
33

34 Department of Mechanical Engineering
35

36 University of Washington
37

38 jposner@uw.edu
39
40
41

42 **Keywords:** point-of-care diagnostics, isotachophoresis, paper-based microfluidics,
43 nucleic acid testing
44
45
46
47
48
49
50
51
52
53
54
55
56
57
58
59
60

Abstract

The number of people living with HIV continues to increase with the current total near 38 million, of which about 26 million are receiving antiretroviral therapy (ART). These treatment regimens are highly effective when properly managed, requiring routine viral load monitoring to assess successful viral suppression. Efforts to expand access by decentralizing HIV nucleic acid testing in low- and middle-income countries (LMICs) has been hampered by the cost and complexity of current tests. Sample preparation of blood samples has traditionally relied on cumbersome RNA extraction methods, and it continues to be a key bottleneck for developing low-cost POC nucleic acid tests. We present a microfluidic paper-based analytical device (μ PAD) for extracting RNA and detecting HIV in serum, leveraging low-cost materials, simple buffers, and an electric field. We detect HIV virions and MS2 bacteriophage internal control in human serum using a novel lysis and RNase inactivation method, paper-based isotachopheresis (ITP) for RNA extraction, and duplexed reverse transcription recombinase polymerase amplification (RT-RPA) for nucleic acid amplification. We design a specialized ITP system to extract and concentrate RNA, while excluding harsh reagents used for lysis and RNase inactivation. We found the ITP μ PAD can extract and purify 5,000 HIV RNA copies per mL of serum. We then demonstrate detection of HIV virions and MS2 bacteriophage in human serum within 45-minutes.

1 Introduction

The number of people infected with HIV globally continues to steadily increase, with the current total over 36 million.¹ Since the advent of highly effective antiretroviral therapy (ART), almost 20 million HIV-positive people are on treatment, which requires routine viral load monitoring to assess successful viral suppression.² Additionally, early infant detection of HIV infections is not possible with typical lateral flow-based antibody tests, so highly sensitive nucleic acid amplification testing (NAATs) must be used to detect HIV nucleic acids.³ The majority of nucleic acid testing for HIV in low- and middle-income countries (LMICs) is carried out on dried blood spots shipped to central laboratories, where expensive automated tests quantitate viral titers.⁴ There have been increased efforts to scale-up decentralized HIV molecular testing in LMICs, and several point-of-care (POC) viral load tests have reached market to address this need.⁵ Yet effective scale-up efforts have been hampered by the platform and per-test costs, as well as the operational complexity of current viral load tests. For widespread use in LMICs, POC HIV viral load tests must be rapid, robust, low-cost, simple to use, and capable of sensitive detection of HIV virions in blood—the World Health Organization recommends a limit of detection (LOD) of 1,000 copies per mL of plasma.⁶

The majority of current commercial HIV POC tests have miniaturized and automated gold-standard approaches to molecular testing of RNA from blood samples.⁵ A primary roadblock for simplifying these tests for POC use is sample preparation due to the susceptibility of RNA to degradation and the complexity of blood, which contains immunoglobulins, cellular debris, and nucleases that inhibit downstream molecular assays.^{7,8} Endogenous blood RNases are particularly problematic because they are exceptionally stable enzymes and capable of rapidly degrading exogenous free RNA in blood in the order of seconds.^{9,10} Traditional sample preparation methods for bloodborne RNA targets use high concentrations of chaotropic salts, toxic disulfide reducing chemicals (e.g. β -mercaptoethanol), and harsh anionic detergents to lyse virions and inactivate blood RNases.^{11–13} Highly effective nucleic acid extraction and purification from the lysate is required to prevent chemicals from interfering with downstream amplification assays. Solid phase extraction is commonly used for purification, but this necessitates repeated buffer exchanges to separate, wash, and elute nucleic acids.¹⁴ For example, a

1
2
3 gold standard product for viral RNA extraction is the QIAamp Viral RNA Mini Kit (Qiagen),
4 and it requires 6 manual pipetting steps and 5 centrifugations, totaling 30 minutes to an
5 hour of hands-on time – according to the product handbook. Commercial POC tests
6 automate these steps using robotics, pumps, valves, and other methods for fluidic
7 exchanges.¹⁴ Automating extensive fluidic manipulation has required complicated
8 engineering designs. This approach faces a practical barrier to lowering the overall
9 platform costs of molecular testing in blood samples, which has prompted researchers to
10 find new sample preparation approaches for POC use.

11
12
13
14
15
16
17 Isotachopheresis (ITP) is an electrophoretic separation and concentration technique
18 that can extract and purify nucleic acids from complex biological samples.¹⁵ ITP is capable
19 of extracting nucleic acids from blood samples and removing contaminants, such as
20 hemoglobin and immunoglobulin G, that inhibit downstream amplification assays.^{8,16} This
21 separation process requires no physical manipulations, buffer exchanges, or other
22 intermediate user steps, but rather automates nucleic acid purification using an applied
23 electric field and simple buffers. ITP leverages a discontinuous buffer system with a
24 leading electrolyte (LE) and trailing electrolyte (TE) to develop an electric field gradient
25 that focuses charged species based on their electrophoretic mobilities.¹⁷ Analytes with
26 mobilities less than the LE and greater than the TE are focused into a concentrated plug
27 at the interface of the two electrolytes. Kondratova et al. were the first to use ITP in
28 agarose gels for DNA extraction from human blood samples, but their work was not well-
29 suited for POC diagnostics because it required lengthy deproteinization and dialysis
30 pretreatment steps.^{15,18} Microchannel-based ITP has since emerged as a promising
31 sample preparation approach for extracting DNA from blood specimens and amplifying
32 with off-chip quantitative polymerase chain reaction (qPCR).^{19–22} Notably, Eid et al.
33 detected DNA from *Listeria monocytogenes* cells in 2.5 μL of whole blood using alkaline
34 and proteinase K lysis, microchannel ITP purification, and recombinase polymerase
35 amplification for detection.²³

36
37
38
39
40
41
42
43
44
45
46
47
48
49
50 In moving towards molecular diagnostics that are appropriate for POC use in LMICs,
51 there are continuing efforts to implement ITP in microfluidic paper-based analytical
52 devices (μPADs). μPADs are well-suited for POC diagnostics due to their wicking
53 properties, ease of reagent deposition and storage, low material cost, and established
54
55
56
57
58
59
60

1
2
3 methods for high-volume manufacturing.²⁴ There are a number of ITP μ PADs that have
4 investigated extraction and concentration of analytes (e.g. fluorophores, DNA, indicator
5 dyes) from pure buffer systems.^{25–30} Our group has developed an ITP μ PAD with
6 integrated whole blood fractionation and DNA extraction.³¹ We have also demonstrated
7 simultaneous DNA extraction with ITP and on-chip DNA amplification using recombinase
8 polymerase amplification (RPA).³²
9

10
11
12
13
14 There are significant technical challenges that need to be overcome in order for ITP
15 μ PADs to be implemented for POC molecular testing of bloodborne pathogens, especially
16 RNA viruses. Sample preparation for nucleic acid testing of HIV and other bloodborne
17 RNA viruses requires lysis of the viral envelope, deactivation of blood RNases, and RNA
18 purification. Traditional lysis and RNase inactivation leverage high concentrations of
19 guanidine (4 to 6 M), which rapidly destroy viral envelopes and inactivate endogenous
20 blood RNases.¹¹ They are easily paired with silica-based columns or other substrates for
21 nucleic acid purification via solid phase extraction.¹⁴ However, guanidine is difficult to pair
22 with ITP systems for nucleic acid purification because high salt samples significantly
23 disrupt the electric field gradient, hindering rapid ITP separation.¹⁶ The only study we are
24 aware of that extracted RNA from blood samples was an assay targeting bacterial rRNA
25 using alkaline-based lysis and a glass microchannel for the ITP separation. The study
26 suffered LOD issues due to a low sample volume (~1 nL) and incomplete inactivation of
27 exogenous and endogenous RNases.²² There have been no reported ITP-based
28 extractions of viral RNA from blood or serum.
29
30
31
32
33
34
35
36
37
38
39

40 In this paper, we report a method for HIV detection from human serum with an MS2
41 bacteriophage internal process control using a novel lysis and RNase inactivation
42 method, paper-based ITP, and duplexed reverse transcription recombinase polymerase
43 amplification (RT-RPA). A previous study from our group examined varied enzymatic and
44 chemical approaches for immobilizing blood RNases.³³ We build on this work to develop
45 a novel 15-minute protocol for off-chip viral lysis, RNase inactivation, and serum protein
46 digestion. We design a specialized ITP system to focus RNA into a characteristic ITP
47 plug, while excluding proteinase K and anionic detergent present in the lysate. We
48 determine the LOD of the ITP μ PAD for RNA extraction by processing digested serum
49 spiked with known RNA concentrations and amplifying with off-chip RT-RPA. We then
50
51
52
53
54
55
56
57
58
59
60

1
2
3 demonstrate detection of HIV virions and MS2 bacteriophage in human serum within 45-
4 minutes. To our knowledge, this is the first example of an ITP-based assay for detecting
5 RNA viruses from blood samples. We propose that our assay may ultimately be
6 implemented in a fully integrated POC HIV viral load test with no intermediate user steps
7 using innovations that have previously been reported, such as integrated plasma
8 separation, in-membrane protein digestion, and simultaneous ITP and RPA.^{31,32}
9
10
11
12
13
14

15 **2 Materials and methods**

16 **2.1 Biological samples**

17
18
19 All experiments in this study were performed in a Biosafety Level (BSL) 2 with BSL-3
20 practices laboratory under a Biological Use Authorization approved by the Institutional
21 Biosafety Committee at the University of Washington. Human serum used in this study
22 was obtained from Sigma-Aldrich (St. Louis, MO, USA). According to the manufacturer's
23 specifications, pooled blood samples from males with blood type AB were centrifuged
24 and resulting plasma was clotted via calcium addition. We chose to perform all
25 experiments using this pooled serum rather than plasma for the sake of experimental
26 consistency and ease of use, as serum has no anticoagulants or risk of clotting. Pooled
27 serum is identical to plasma, except with clotting factors removed. Fluorescently labeled
28 DNA was a 70 base pair (bp) double stranded DNA sequence modified with a single Alexa
29 Fluor 488 molecule (Integrated DNA Technologies, Coralville, IA, USA).
30
31
32
33
34
35
36
37
38
39

40 Purified HIV RNA was prepared from HIV-1 supernatant as previously detailed by
41 Lillis et al.³⁴ HIV-1 supernatant (Group M, Subtype A, NCBI accession number:
42 JX140650) was obtained from the External Quality Assurance Program Oversight
43 Laboratory at Duke University.³⁵ Viral RNA was extracted and purified using the QIAamp
44 Viral RNA Mini Kit (Qiagen, Hilden, Germany) according to the manufacturer's standard
45 protocol. RNA was then quantified with quantitative real-time PCR based on the method
46 described by Rouet et al. using Superscript® III one-step RT-PCR system (Life
47 Technologies, Carlsbad, CA, USA).³⁶
48
49
50
51
52
53

54 Experimental work on HIV virion detection from human serum used a non-infectious
55 HIV strain to reduce laboratory safety risks. HIV detection work employed a cultured HIV-
56
57
58
59
60

1
2
3 1 subtype B (8E5) virus (SeraCare, Milford, MA, USA). The 8E5 HIV contains a single
4 base addition in its RNA genome at the pol gene, creating a reverse transcription-
5 defective virus with no infectivity. The 8E5 HIV was supplied in a concentrated
6 supernatant and then diluted with serum for experimental work. Bacteriophage MS2 was
7 the internal process control for the HIV assay. The phage was grown and isolated using
8 an established protocol.³⁷ MS2 stock solution was diluted with phosphate buffered saline
9 and stored at -80°C.
10
11
12
13
14
15

16 **2.2 Lysis, RNase inactivation, and protein digestion**

17
18 We employed a specialized chemistry for combined viral lysis, inactivation of blood
19 RNases, and digestion of serum proteins. This chemistry was based on a previous study
20 from our group investigating various methods for inactivating blood RNases.³³ We
21 incubated serum with a combination of 0.5% sodium dodecyl sulfate (Sigma-Aldrich), 1
22 mg/mL of proteinase K (Thermo Fisher Scientific, Waltham, MA, USA), and 10 mM
23 dithiothreitol (Sigma-Aldrich). Working stock reagent concentrations were high, such that
24 serum was only diluted 10% (i.e. a 40 μ L sample contained 36 μ L serum and 4 μ L lytic
25 reagents).
26
27
28
29
30
31

32 We conducted a series of experiments extracting HIV RNA from pre-digested
33 serum. For these RNA extraction experiments, we incubated serum with SDS and
34 proteinase K in a water bath for 1 hour at 50°C. Following this incubation, we spiked
35 known concentrations of purified HIV RNA into the digested serum. For experiments
36 detecting HIV virions in serum, we incubated serum spiked with 8E5 HIV for 15-minutes
37 at 65°C.
38
39
40
41
42
43

44 **2.3 ITP device construction and buffer composition**

45
46 ITP extractions were performed in single-use, disposable ITP μ PADs consisting of
47 a plastic petri dish (Thermo Fisher Scientific), acrylic reservoirs, and 22-gauge titanium
48 wire electrodes (McMaster Carr, Elmhurst, IL, USA). Reservoirs were cut with a CO₂ laser
49 cutter (Universal Laser Systems, Scottsdale, AZ, USA) and adhered to the petri dish
50 bases with double-sided tape (3M, Maplewood, MN, USA). The ITP strip spanned the two
51 reservoirs and was constructed from Fusion 5 membrane (GE Healthcare, Chicago, IL,
52
53
54
55
56
57
58
59
60

1
2
3 USA), which is made with a proprietary method to maximize porosity and minimize
4 adsorption of biomolecules. Membranes were cut into a teardrop shape (40 mm long with
5 maximum width of 8 mm and minimum width of 3 mm) with an electronic cutter machine
6 (Cameo 3, Silhouette, UT, USA). The membranes were not washed or blocked, and they
7 were stored at room temperature.
8
9

10
11
12 For the ITP system, the TE buffer consisted of 70 mM Tris, 70 mM serine, and 0.1%
13 w/v polyvinylpyrrolidone (PVP). The LE buffer in the ITP membrane was 135 mM Tris, 90
14 mM HCl, 50 mM KCl, 0.1% w/v PVP, and 100 ng/mL poly(A) carrier RNA. The LE buffer
15 in the anode reservoir contained 240 mM Tris, 160 mM HCl, 10 mM KCl, and 0.1% PVP.
16 Although the pH remained constant, the LE in the reservoir employed a higher
17 concentration of Tris to maximize its buffer capacity, which is common in ITP systems to
18 prevent pH changes from hydrolysis at the electrodes.³⁸ All chemicals were obtained from
19 Sigma-Aldrich. Buffers were prepared with molecular biology grade reagents, RNase-free
20 water (Thermo Fisher Scientific), and in PCR-grade microcentrifuge tubes (Eppendorf
21 AG, Hamburg, Germany) to limit introductions of exogenous RNases.
22
23
24
25
26
27
28
29

30 **2.4 ITP extraction**

31
32 The ITP μ PAD processes a 40 μ L sample of serum pretreated with proteinase K,
33 SDS, and DTT. Experiments in this work used serum samples with either spiked RNA,
34 spiked HIV, or no analyte. The first step in ITP extraction is pipetting 40 μ L of sample onto
35 the porous membrane in the widened sample region proximal to the TE reservoir. 1 μ L of
36 fluorescently labeled DNA is also added to the sample region for monitoring the location
37 of the ITP during the separation. Then 40 μ L of LE buffer is added to wet the remainder
38 of the membrane. 250 μ L of LE and TE buffers are added to their respective reservoirs.
39 Initial locations of ITP buffers and sample are depicted in Figure 1.
40
41
42
43
44
45

46 ITP is initiated with a constant 110-volt bias across the ITP strip applied with a
47 source meter (model 2410, Keithley Instruments, OH, USA). The ITP plug location is
48 indicated by the fluorescently labeled DNA. We collected fluorescence images of the
49 separation membrane with a microscope (AZ-100, Nikon, USA) equipped with a 0.5X (NA
50 = 0.05) objective. Light supplied by a mercury lamp light source (X-Cite Exacte, Excelitas
51 Technologies Corp., Waltham, MA, USA) passed through an epifluorescence filter cube
52
53
54
55
56
57
58
59
60

1
2
3 set (Omega Optics, Austin, TX, USA) with peak excitation and emission wavelengths of
4 488 nm and 518 nm, respectively. A 16-bit cooled electron multiplying charge-coupled
5 device camera (Cascade II, Photometrics, Tucson, AZ, USA) collected grayscale images
6 of ITP extractions.
7
8
9

10 When the ITP plug reaches the center of the narrow extraction zone of the strip, the
11 voltage bias is removed, and this region of the strip is cut out. For RNA extraction
12 experiments, the extraction zone of the paper strip is placed in a 0.5 mL plastic tube with
13 a small hole at the bottom. The 0.5 mL plastic tube is placed inside a 1.5 mL plastic tube
14 and centrifuged, removing the contents of the ITP plug from the paper (~4 μ L of eluate).
15 This ITP eluate is pipetted directly into an RT-RPA reaction. For HIV detection
16 experiments from serum, we do not use a centrifuge, but instead add the extraction zone
17 of the paper strip directly to an off-chip RT-RPA reaction for duplexed detection of HIV
18 and MS2, as illustrated in Figure 1. We treated the benchtop, pipettes, forceps, and
19 scissors with 10% bleach solution between each experiment in order to prevent cross
20 contamination of nucleic acids.
21
22
23
24
25
26
27
28
29

30 **2.5 RT-RPA amplification and detection**

31
32 The RT-RPA primers and probe for HIV detection were developed by Lillis *et al.* and
33 can be used to amplify HIV-1 RNA across multiple subtypes.³⁴ The RT-RPA HIV detection
34 assay consists of a lyophilized pellet of RPA reagents from the TwistAmp exo kit (TwistDx,
35 UK), 29.5 μ L rehydration buffer, 14 mM magnesium acetate, 540 nM forward primer
36 (Integrated DNA Technologies), 540 nM reverse primer, 120 nM FAM-labeled probe (LGC
37 Biosearch Technologies, Hoddesdon, UK), 0.2 U/ μ L RNasin Plus Ribonuclease Inhibitor
38 (Thermo Fisher), 0.5 U/ μ L reverse transcriptase (AffinityScript, Agilent, Santa Clara, CA,
39 USA), and 1% w/v Triton X-100 (Sigma-Aldrich). The duplexed RT-RPA assay for HIV
40 and MS2 employed the reagents listed above as well as 216 nM MS2 forward primer, 216
41 nM MS2 reverse primer, and 48 nM Fluor Red 610-labeled probe.
42
43
44
45
46
47
48
49

50 Experiments examining ITP plug purity used 4 μ L of ITP extraction liquid and 2.5 μ L
51 of HIV RNA in the RT-RPA reactions. Experiments studying RNA extraction from digested
52 serum used 4 μ L of ITP extraction liquid in RT-RPA reactions. For HIV detection
53 experiments, we added the cutout paper ITP extraction zone (containing ~4 μ L of liquid)
54
55
56
57
58
59
60

1
2
3 directly to RT-RPA reaction tubes. We used RNase-free water to bring all RT-RPA
4 reactions to a total volume of 50 μL per tube. A standalone fluorometer specifically
5 designed for point-of-care testing applications (T16-ISO, Axxin, Australia) heated and
6 measured fluorescence of the RT-RPA reactions. Reaction tubes were removed after 5
7 minutes of incubation, briefly mixed, and returned to the fluorometer for another 10
8 minutes. The baseline fluorescence at 3 minutes was subtracted from fluorescence
9 values at all measurement time points for each respective reaction tube. For the HIV
10 assay, we used a threshold of 100 arbitrary fluorescence units in the FAM detection
11 channel to differentiate between successful and unsuccessful amplification. The MS2
12 assay fluorescence threshold was 50 arbitrary fluorescence units in the ROX detection
13 channel.
14
15
16
17
18
19
20
21
22

23 **2.6 RNase detection assay**

24
25 We employed the RNaseAlert Substrate Detection System (Integrated DNA
26 Technologies) for testing RNase activity in serum samples. We prepared the RNaseAlert
27 experiments in a lidded 96-well plate with black walls and clear bottom (Corning
28 Incorporated, Corning, NY, USA). The total assay volume for each well was 100 μL . Each
29 RNase detection assay contained 10 μL of RNaseAlert substrate, 10 μL of 10X
30 RNaseAlert buffer, 60 μL of RNase-free water, and 20 μL of sample. We used a 12-
31 channel pipette to concurrently add serum samples to each well. The plate was
32 immediately loaded into a plate reader (SpectraMax iD3, Molecular Devices, San Jose,
33 CA, USA). The excitation and emission wavelengths were 485 nm and 535 nm,
34 respectively. The gain was set to "low" with an exposure of 140 ms. The heating block in
35 the plate reader was set to 37°C. The instrument agitated the plate and measured the
36 fluorescence in the wells every 2 minutes over a 30-minute incubation time.
37
38
39
40
41
42
43
44
45
46
47
48
49
50
51
52
53
54
55
56
57
58
59
60

3 Results and discussion

3.1 Assay design and considerations

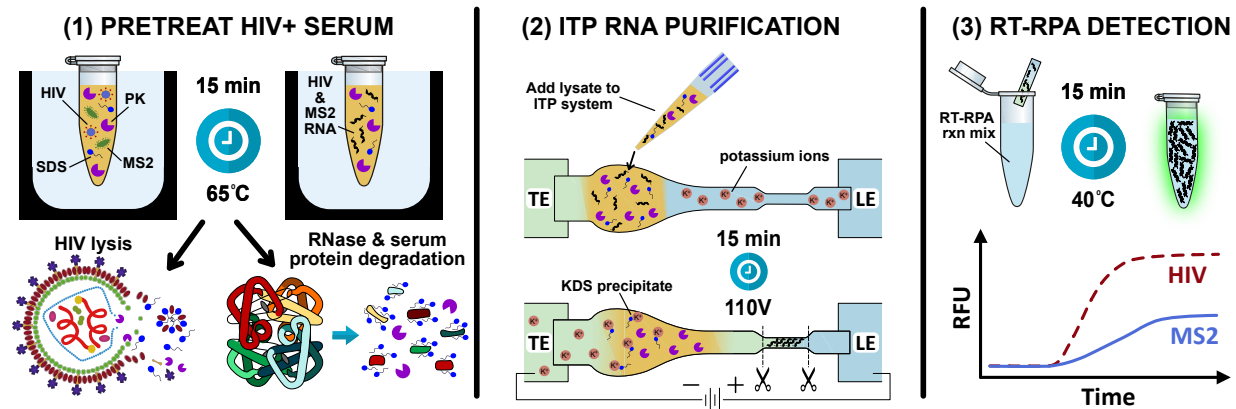


Figure 1. Schematic of the three-step process for detecting HIV and MS2 bacteriophage from human serum. (1) HIV+ serum spiked with MS2 phage is pretreated with proteinase K, SDS, and DTT at 65°C for 15 minutes. SDS and proteinase K simultaneously lyse HIV and degrade endogenous blood RNases. (2) Free HIV and MS2 RNA are extracted and purified with ITP from serum components, proteinase K, and SDS. Potassium ions in the leading electrolyte precipitate potassium dodecyl sulfate, preventing the anionic detergent from focusing in the ITP plug. (3) A duplexed RT-RPA reaction directly from the cut portion of the paper strip simultaneously amplifies HIV and MS2.

The HIV detection assay with an MS2 bacteriophage internal control requires serum pretreatment, RNA purification with our ITP μ PAD, followed by duplexed RT-RPA. This diagnostic scheme is illustrated in Figure 1. Serum pretreatment via SDS and proteinase K is necessary for viral lysis, RNase inactivation, and serum protein degradation. SDS is a powerful protein denaturant that has long been used in lysis chemistries while proteinase K is a broad spectrum protease that degrades proteins into a corresponding assortment of polypeptides.¹⁰ Proteolytic digestion is a crucial serum pretreatment step in ITP-based extractions. It has been widely reported that extraction of nucleic acids with ITP is inhibited by nonspecific binding with blood proteins.^{20,23,32,39} Extensive protein degradation reduces nucleoprotein complex formation and allows for electromigration of nucleic acids.

1
2
3 We designed our ITP system to separate RNA from inhibitors of downstream RT-
4 RPA and achieve high analyte accumulation in the ITP plug. Blood contains a variety of
5 inhibitors of nucleic acid amplification assays, including undesirable salts and interfering
6 proteins (e.g. hemoglobin, immunoglobulin, lactoferrin).^{8,40} Both SDS and proteinase K
7 are potent inhibitors of RT-RPA because they inactivate the enzymes and proteins
8 required in the amplification mechanism. SDS is an anionic detergent, so dodecyl sulfate
9 carries the same negative charge as nucleic acids in most buffer conditions. Therefore, it
10 is challenging to electrophoretically separate dodecyl sulfate from nucleic acids using ITP.
11 To address this we instead removed dodecyl sulfate from the lysate with precipitation
12 mediated by a potassium salt, leveraging the very low solubility of potassium dodecyl
13 sulfate (KDS) in water.^{41,42} We employed potassium chloride in the leading electrolyte in
14 the ITP strip and in the reservoir. Upon application of the electric field, potassium cations
15 migrated from the LE buffer toward the cathode in the TE reservoir. Potassium cations
16 therefore encountered dodecyl sulfate in this migration path forming KDS precipitate, as
17 illustrated in Figure 1.
18
19
20
21
22
23
24
25
26
27
28

29 Proteinase K in the serum lysate can be purified away from viral RNA with ITP based
30 on its charge. Proteinase K has an isoelectric point of 8.9 and therefore has a net positive
31 charge in buffers less than pH 8.9.¹⁰ In electrokinetic systems that maintain pH less than
32 8.9, proteinase K electromigrates in the opposite direction of nucleic acids due to their
33 contrasting charges. ITP systems must be carefully designed because there can be sharp
34 pH gradients, depending on the selection of TE, LE, and buffering counterion. We used
35 numerical simulations to guide our design of the ITP system and select proper electrolytes
36 for purifying and extracting RNA from serum. We used an open-source electrophoretic
37 modeling tool, the Stanford Public Release Electrophoretic Separation Solver
38 (SPRESSO), to approximate concentration and pH profiles resulting from various ITP
39 buffers and plot the simulation outputs in Figure 2. We do not go into depth on the
40 equations and assumptions of the simulations here, but details can be found in the original
41 SPRESSO report.⁴³
42
43
44
45
46
47
48
49
50
51

52 In Figure 2A, we show simulated concentration profiles of distinct ionic species for
53 an ITP system with a leading electrolyte comprised of 160 mM HCl and 240 mM tris paired
54 with a trailing electrolyte of 70 mM tris and 70 mM serine. As ITP progresses with an
55
56
57
58
59
60

1
2
3 applied electric field, three distinct zones are formed: the original TE zone, the adjusted
4 TE (ATE) zone, and the LE zone. The ATE zone is a region with TE ions which was
5 previously occupied by the LE. As seen in Figure 2A, the ATE has increased
6 concentrations of serine and tris compared with the original TE, elevating its pH. We found
7 that using serine as the TE and an LE comprised of HCl with tris as the counterion
8 maintained a pH less than 8.9 in all regions (see Figure 2B). Therefore, our ITP system
9 was designed for proteinase K to be positively charged and electrophoretically separated
10 from RNA.
11

12 We found that serine ($pK_a = 9.33$, fully ionized electrophoretic mobility of 34.3×10^{-9}
13 $m^2 V^{-1} s^{-1}$) was a highly effective TE for its suitability for proteinase K removal and
14 obtaining sufficient nucleic acid extraction. It has been reported in the literature that
15 lowering the TE conductivity is a key mechanism for increasing analyte accumulation in
16 the ITP plug.⁴⁴ Low conductivity creates high electric fields in the TE region of the ITP
17 system, resulting in faster electromigration of analytes in this zone and enhanced
18 accumulation in the ITP plug. We found that under a pH of 9.0, serine has a very low
19 electrophoretic mobility, resulting in low conductivities in the TE and ATE zones. A
20 majority of the ITP studies on nucleic acid extraction from blood use HEPES ($pK_a = 7.66$,
21 mobility of $21.8 \times 10^{-9} m^2 V^{-1} s^{-1}$) as the TE.¹⁶ As shown in Figure 2B, HEPES maintains
22 relatively low pH in the system and is well-suited for removing proteinase K. However,
23 HEPES has a higher electrophoretic mobility than serine at pH less than 9, so simulations
24 showed that HEPES could not generate as high of electric field strength in the ATE zone
25 as serine ($\sim 0.5 \times$ lower). In experimentation, we found that we could not achieve efficient
26 nucleic acid extraction from serum using HEPES as TE. The lower electrophoretic
27 mobility of serine is useful in focusing HIV RNA that may have reduced mobility in our ITP
28 system due to the tortuosity of the porous membrane and polypeptides that may bind or
29 interact with RNA.⁴⁵ There have been reports of ITP nucleic acid extractions from blood
30 samples using β -alanine ($pK_a = 10.24$, mobility of $30.8 \times 10^{-9} m^2 V^{-1} s^{-1}$) as the TE which
31 offers very high electric field strength in the ATE zone and extraction efficiencies up to
32 93%.^{15,39} However, we found that the high pK_a of β -alanine resulted in a higher alkaline
33 ATE than serine, making it ineffective for proteinase K removal (see Figure 2B). We
34 experimented with different counterions, which can be used for pH control, but we found
35
36
37
38
39
40
41
42
43
44
45
46
47
48
49
50
51
52
53
54
55
56
57
58
59
60

that using tris as the counterion resulted in ITP plugs near pH 8 that were highly compatible with RT-RPA reaction conditions which are also tris-buffered (~pH 8). We also performed experimental validations of pH profiles generated in SPRESSO using pH paper (Figure S1).

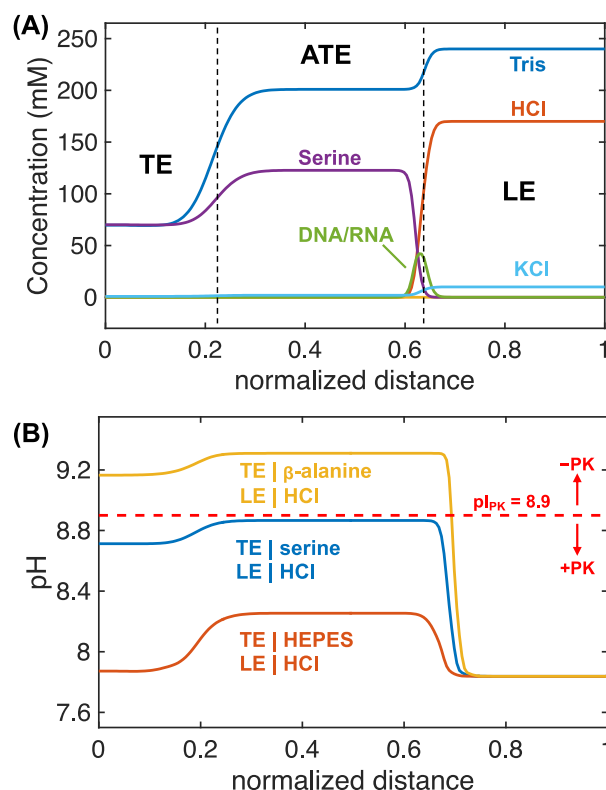


Figure 2. Simulations describing the ion concentration and pH profiles of ITP systems. (A) SPRESSO simulation results of concentration profiles with a TE buffer comprised of 70 mM Tris and 70 mM serine and a LE buffer of 240 mM Tris, 160 mM HCl, and 10 mM KCl. As the ITP plug migrates into the region previously containing LE, an adjusted trailing electrolyte (ATE) zone develops directly adjacent to the ITP plug. (B) Simulation results of pH profiles of three different TE selections: HEPES, serine, and β -alanine. All TE, LE, and counterion concentrations are the same as in (A). The pH of the ATE differs from 8.26 to 9.31 depending on the TE selection. When the pH of the ATE zone is less than 8.9, proteinase K is positively charged and will not electromigrate with negatively charged RNA.

3.2 Nucleic acid extraction visualization

We examined the nucleic acid extraction performance of our ITP μ PAD using fluorescence imaging of labeled DNA. We found that labeled DNA was a convenient analyte for optimizing experimental conditions and studying ITP dynamics. Our ITP device employs a uniquely shaped porous membrane with a wide sample region that holds a 40 μ L volume, as shown in Figure 3A. Over a 15-minute period, nucleic acids electromigrate into an extraction region containing approximately 4 μ L volume, which can be cut out and directly added to an RT-RPA reaction. This concentration step from a large sample volume to a 10-fold smaller extraction volume is advantageous for detecting HIV which may contain less than hundreds of RNA copies in 40 μ L of serum.

In Figure 3B, we present experimental images of an ITP extraction of DNA labeled with Alexa Fluor at a concentration of 100 nM in 40 μ L of digested serum. We show images of the early electromigration and focusing into a concentrated plug over the first 10 minutes of ITP. We plot the y -averaged intensity as a function of strip length at 0, 5, and 10 minutes. Before the electric field is applied ($t=0$) the DNA is diffusely distributed over the sample zone with a low average fluorescent intensity. Labeled DNA electromigrate out of the sample zone into the straight region of the strip, forming a concentrated plug between the LE and ATE. After 10 minutes, the DNA has electromigrated across the majority of the strip length, reaching a distance approximately 23 mm from the middle of the sample zone. An additional 5 minutes of migration centers the ITP plug in the extraction region of the strip. We measured the extraction efficiency of the ITP system using fluorescence quantification of labeled DNA (see Figure S2). We observed extraction efficiencies ranging from 70 to 81% with a 40 μ L digested serum sample. We observed improved extraction efficiencies, up to greater than 90%, when processing diluted serum samples. For reference, Qiagen's laboratory-based QIAamp Viral RNA Mini Kit self-reports RNA extraction yields greater than 90% from clinical specimens. We calculated the extraction efficiency of the ITP system using 70 bp labeled DNA, and we expect this yield is similar for HIV RNA which is \sim 10 kilobase pairs in length. Previous studies have shown that DNA and RNA have a similar electrophoretic mobility, and nucleic acid length does not significantly change its free solution mobility.^{46,47} Therefore, both short DNA and longer viral RNA should focus into the ITP plug of our

1
2
3 system. It is possible that the mobility of the HIV RNA may be reduced by the porous
4 media due to its greater length, but we do not expect this to significantly affect the yield.
5
6

7 We observe several interesting phenomena in extraction experiments with our ITP
8 μ PAD. The data suggest DNA concentration profiles are Gaussian, as predicted by peak-
9 mode ITP literature.⁴⁴ We observe electroosmotic flow of the system causes slight
10 dispersion of the plug, widening the DNA distribution and reducing the maximum peak
11 intensity. Electroosmotic dispersion is common in electrokinetic systems and has been
12 extensively studied in isotachopheresis.^{48,49} A region of low-level fluorescence is evident
13 trailing the ITP plug. We hypothesize this fluorescence is from DNA that has formed
14 complexes with polypeptides in the proteolyzed serum proteins, reducing its
15 electrophoretic mobility and preventing stacking. This phenomenon has been previously
16 observed in ITP studies and is supported by the propensity of nucleic acids to
17 nonspecifically interact with proteins in biological samples.^{20,50} It is also possible that KDS
18 precipitate may accumulate within the pore structure and impede the electromigration of
19 nucleic acids. We also see a small amount of residual fluorescence remain in the sample
20 region of the ITP strip during extraction. We believe this is due to a trace amount of target
21 DNA adsorbing to the porous membrane. We screened various membranes to identify
22 the optimal substrate for the ITP μ PAD, and we found that Fusion 5 resulted in the least
23 DNA adsorption or entanglement (Figure S3). In experiments using pure buffer systems,
24 we did not encounter any issues with analyte loss during the ITP extraction (Figure S4,
25 S5). We found that we were able to successfully electromigrate 10 copies of synthetic
26 DNA and 50 copies of HIV RNA across a 30 mm Fusion 5 strip using RPA for detection.
27
28
29
30
31
32
33
34
35
36
37
38
39
40
41
42
43
44
45
46
47
48
49
50
51
52
53
54
55
56
57
58
59
60

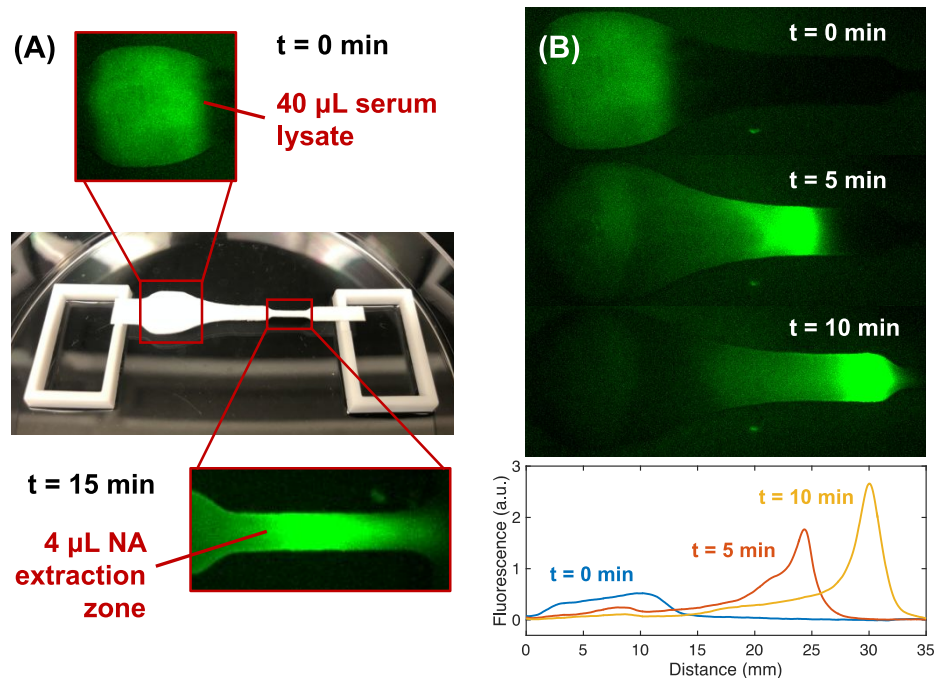


Figure 3. Experimental fluorescence images of ITP extraction of labeled DNA from proteolyzed serum. (A) The ITP system consists of a paper strip spanning two acrylic reservoirs within a plastic petri dish. Nucleic acids are extracted from a 40 μL serum lysate into a 4 μL extraction zone. (B) DNA labeled with Alexa Fluor 488 is mixed with digested human serum and is initially located in the wide sample zone of the Fusion 5 membrane. DNA focuses into a concentrated plug in the straight portion of the strip ($t=10$ min) before entering the extraction zone ($\sim t=15$ min). Pixel intensities of the images are y-averaged, creating normalized fluorescence distribution with respect to distance along the membrane for each time point (0, 5, and 10 minutes).

3.3 HIV RNA extraction

Our initial experimental efforts to extract HIV RNA spiked into serum were challenged by rapid RNA degradation in serum samples with no RNase control measures, which is consistent with previous reports of extensive RNA degradation in serum on the order of seconds.⁹ To mitigate issues with RNases, we leveraged previous work that developed an RNase inactivation method for human serum via incubation with 0.5% SDS, 1 mg/mL proteinase K, and 10 mM DTT for 1 hour at 50°C³³. Our ITP system was designed to remove SDS and proteinase K in the resulting lysate from focusing in the plug. We performed a set of experiments to assess the purity of the ITP plug by observing its effect on RT-RPA reactions. For these experiments, we processed a 40 μL serum

1
2
3 lysate with no added HIV RNA with our ITP system. The extraction zone of the strip was
4 centrifuged to dewater the membrane. The resulting ITP plug eluate (~4 μL) was added
5 to an RT-RPA reaction with 500 copies of HIV RNA to determine if the eluate inhibited
6 the amplification reaction. Figure 4A shows fluorescence amplification curves detecting
7 HIV RNA which indicate the compatibility of ITP plugs with RT-RPA. Positive control
8 reactions with only HIV RNA are provided for comparison. We found that the contents of
9 ITP plugs in extractions including KCl in the LE did not significantly impact RT-RPA
10 performance. In ITP extractions with no KCl, the contents of the ITP plug inhibited RT-
11 RPA such that no amplification was detected. This indicates that the potassium-mediated
12 SDS precipitation removed enough of the anionic detergent to enable RT-RPA. Our
13 results also indicate that our ITP system was successful in preventing proteinase K from
14 focusing in the ITP plug. This supports the simulations of pH conditions in Figure 2B that
15 found the ITP system pH was less than the isoelectric point of proteinase K (8.9). We
16 tested an alternate ITP system that was not designed for proteinase K removal (β -alanine
17 as TE) and found that the resulting ITP plugs contained proteinase K and completely
18 inhibited RT-RPA (Figure S6).
19
20
21
22
23
24
25
26
27
28
29
30

31 We analyzed the performance of the ITP μPAD for RNA extraction using pre-
32 digested serum spiked with known concentrations of HIV-1 RNA. Figure 4B presents
33 amplification curves for extracted HIV-1 RNA at different input concentrations in serum.
34 This assay successfully detects 5,000 copies of HIV RNA per mL of serum, corresponding
35 to 200 RNA copies per 40 μL of processed serum. As expected, we found that
36 amplification is much more robust when extracting and detecting higher concentrations
37 of HIV in serum. We found that our sample pretreatment protocol for digesting serum
38 proteins and inactivating endogenous RNases was crucial for ITP RNA extractions. We
39 also tested the ITP μPAD performance with a robust, synthetic DNA target (200 bp in
40 length) and found an order of magnitude improved sensitivity of 500 cp/ml (20 copies per
41 40 μL sample) compared with HIV RNA (Figure S7). One primary consideration is that
42 the RPA assay used for DNA detection (nearly single copy sensitivity) was approximately
43 10-fold more sensitive than the RT-RPA assay for HIV RNA (~25 copy sensitivity). There
44 may be multiple reasons why lower detection limits were observed with DNA, but we
45 hypothesize that direct amplification from DNA targets is significantly more efficient than
46
47
48
49
50
51
52
53
54
55
56
57
58
59
60

first synthesizing complementary DNA templates from the viral RNA via reverse transcription before RPA can begin.

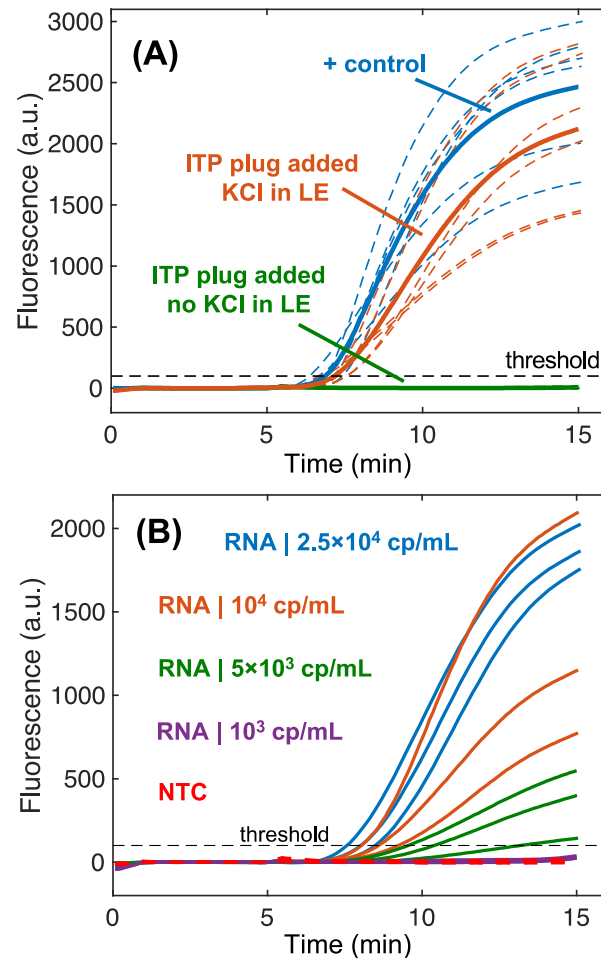


Figure 4. Purification and extraction of nucleic acids from serum samples via paper-based ITP. (A) Fluorescence measurements of RPA assays assessing the level of inhibitors present in ITP plugs. Experiments evaluating ITP purification have 500 copies of HIV-1 RNA with 4 μ L of ITP plug eluate added into them. Positive control reactions contain only 500 copies of RNA. We plot the replicate amplification curves (N=6 for each) with a dashed line and respective averages with a solid line. Two different ITP systems were evaluated: one containing potassium chloride in the leading electrolyte to precipitate dodecyl sulfate and the other with no potassium chloride. Positive control experiments (N=3) simply include nuclease free water. (B) 5,000 HIV-1 RNA copies per mL of digested serum (200 copies in 40 μ L of serum) were consistently extracted and amplified

1
2
3 over the threshold fluorescence value with RT-RPA (N=3). No template control (NTC)
4 experiments (N=3 for each assay) did not increase in fluorescence.
5
6
7

8 9 **3.4 Detection of HIV-positive serum**

10
11 We employed our RNase inactivation chemistry for viral lysis and serum protein
12 digestion, followed by isotachophoretic extraction on our μ PAD to detect HIV virions in
13 human serum. We built upon previous work to identify a protocol for rapid RNase
14 inactivation that is better suited for POC testing applications. We used a commercial
15 RNase detection assay to evaluate the serum pretreatment conditions for rapid and
16 complete RNase inactivation and plotted the results in Figure 5A. Incubations of serum
17 with proteinase K alone did not remove RNase activity. Serum treatment with 0.5% SDS
18 alone temporarily inactivated RNases, but activity was restored when the sample was
19 diluted into the detection assay. The combination of 0.5% SDS, 1 mg/mL proteinase K,
20 and 10 mM DTT was able to permanently reduce serum RNase activity to negligible levels
21 when incubated at 50°C for 1 hour (Figure 5A). A significantly reduced incubation time of
22 15 minutes also achieved nearly complete RNase inactivation when heated to a higher
23 temperature of 65°C.
24
25
26
27
28
29
30
31
32
33

34 The SDS and proteinase K leveraged in the 15-minute RNase inactivation protocol
35 are both commonly used reagents in lysis protocols,⁵¹ so we hypothesized that this
36 chemistry would be effective for HIV viral lysis. SDS is a powerful anionic detergent that
37 is effective for protein denaturation and lipid membrane disruption.^{52,53} Proteinase K is a
38 broad-spectrum protease that lyses cells and pathogens via degradation of structural
39 proteins.^{10,54} We pretreated HIV+ serum with our specialized protocol and then extracted
40 RNA from the lysate with our ITP μ PAD. Off-chip duplexed RT-RPA detected HIV and
41 MS2 internal control RNA. Similar to HIV, MS2 bacteriophage is a single-stranded RNA
42 virus and consequently acts as an internal process control for viral lysis, RNase
43 inactivation, RNA extraction, reverse transcription, and RPA. We were able to detect HIV
44 in serum at 5×10^4 cp/mL using our assay. Tests with HIV-negative serum did not amplify
45 although the MS2 internal control was still detected. Our assay protocol requires 15
46
47
48
49
50
51
52
53
54
55
56
57
58
59
60

minutes for serum pretreatment, 15 minutes for ITP, and 15 minutes for RT-RPA, which totals a 45-minute test runtime.

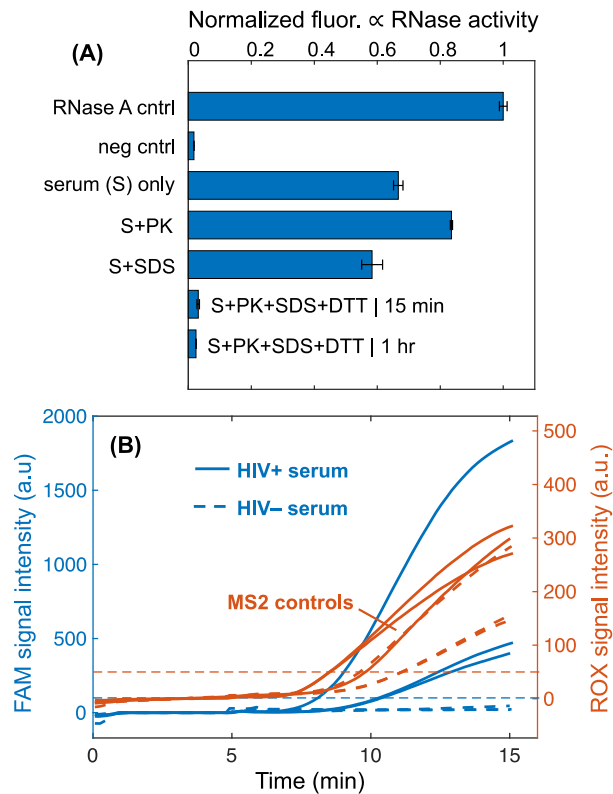


Figure 5. (A) RNase activity of serum samples pretreated with proteinase K and/or SDS. A commercial RNase detection assay, RNaseAlert, measures RNase activity by means of fluorescence intensity increase. High fluorescence denotes high RNase activity. We found that incubation of serum with 0.5% SDS, 1 mg/mL proteinase K at 65°C for 15 minutes resulted in negligible RNase activity in the lysate. Experiments were run in triplicate and one standard deviation around the mean is plotted for each. RNase A (1.5 U/L) is the positive control, and the negative control is RNase-free water add to the RNaseAlert assay. (B) Detection of HIV-1 virions and MS2 phage from human serum. Fluorescence intensities of the two different emission spectra used to simultaneously detect HIV and MS2 amplification. FAM signal intensity indicates successful amplification of target HIV-1, while ROX signal reports amplification of an MS2 region. Experiments with HIV-positive serum amplify while those with HIV-negative serum do not. All MS2 controls amplify for each respective experiment.

4 Concluding remarks

We report on a diagnostic assay for HIV detection from human serum within 45-minutes using a novel sample pretreatment chemistry, an ITP μ PAD, and RT-RPA. We demonstrate several advancements in the use of ITP for POC nucleic acid-based tests. We identified a protocol for viral lysis, RNase inactivation, and serum protein digestion using a short incubation with proteinase K, SDS, and DTT. This chemistry is unique from previous sample pretreatments in ITP studies which did not adequately address serum RNases. Our pretreatment method is also distinct from typical solid phase extraction lysis buffers which rely on high concentrations of guanidinium salts. We designed a specialized ITP μ PAD that can directly process 40 μ L of serum lysate. This is the largest volume of serum that has been used in ITP nucleic acid extractions, to our knowledge. We controlled the pH of our system to remove proteinase K and leveraged potassium chloride to precipitate SDS in the lysate. We confirmed that the resulting ITP plug was free of inhibitors of RT-RPA and found the ITP μ PAD could extract 5,000 copies of HIV RNA per mL of proteolyzed serum. We then demonstrated that our assay detects HIV in human serum within 45-minutes. Our assay features an MS2 bacteriophage for an internal process control of lysis, RNA extraction, reverse transcription, and amplification. This work is the first example of an ITP-based detection assay for RNA viruses in human serum.

Our work describes a potential sample preparation method leveraging paper-based ITP that may be used in POC molecular testing for HIV. While our primary focus was detecting bloodborne viruses, the ITP μ PAD may also be an effective for sample preparation tool for viral pathogens in other complex samples, such as SARS-CoV-2 in saliva or respiratory specimens. We seek to eliminate the need for numerous buffer exchanges, highly concentrated chaotropic agents, and toxic chemicals found in typical viral RNA sample preparation methods. For example, solid-phase extraction employs high-molarity guanidine thiocyanate which forms harmful cyanide gas when combined with bleach, complicating safe disposal of test materials.⁵⁵ Lysis buffers with SDS, proteinase K, and DTT are relatively safe for handling by untrained users and feature easy disposal in resource-limited health care settings. Future work is needed to ensure

1
2
3 that our lysis protocol results in sample lysate that is safe to handle and free of culturable
4 virus.
5

6
7 We demonstrate HIV detection from serum at a viral load of 5×10^4 cp/mL, which is
8 within the clinically relevant range for HIV. Among people living with HIV, there is a
9 significant population who are either not on ART or who have not achieved viral
10 suppression due to adherence issues or a strain of HIV that is resistant to a particular
11 drug regimen. People with unsuppressed HIV infections may have viral loads as high as
12 10^7 cp/mL.⁵⁶ The WHO has recommended that POC tests for viral load monitoring of HIV-
13 positive patients on drug therapies have an LOD of 1,000 cp/mL in order to maximize
14 treatment failure detection.⁶ While RT-RPA is not as effective as RT-PCR for viral load
15 quantification, there is an established approach for a semi-quantitative test that indicates
16 whether a sample has exceeded the recommended 1,000 cp/mL threshold.^{57,58} This
17 approach is leveraged by a commercial product, the SAMBA II, which qualitatively
18 indicates whether an HIV viral load is above or below the test's LOD of 1,000 cp/mL.⁵⁸
19 Ongoing efforts in our lab are focused on improving our device's LOD to this
20 recommended value by increasing the sample volume, minimizing RNA degradation, and
21 improving the ITP extraction efficiency.
22
23
24
25
26
27
28
29
30
31
32

33 The ITP μ PAD features convenient sample addition, low-cost materials, and rapid
34 results, yet there are several aspects of an effective POC test that we do not address,
35 such as plasma separation and on-chip integration of assay steps. Our research group
36 and others have previously demonstrated that plasma can be generated from whole blood
37 samples with asymmetric polymer membranes that are readily integrated with paper-
38 based receiving membranes.^{31,59,60} We have also reported a method for integrating
39 paper-based ITP and RPA for simultaneous extraction and amplification of nucleic
40 acids.³² Future work is focused on advancing our ITP μ PAD to integrate all assay
41 operations on-chip, as we move towards a fully integrated point-of-care HIV viral load
42 monitoring test that is well suited for LMICs.
43
44
45
46
47
48
49
50
51
52
53
54
55
56
57
58
59
60

Conflict of interest

The authors have declared no conflict of interest.

Supporting information

Supporting information file: The supporting information file contains experimental validation of simulated ITP systems, extraction efficiency calculation, description of membrane selection process, demonstration of extraction of DNA from pure buffer, importance of TE selection for proteinase K removal, ITP μ PAD for the extraction of DNA from human serum with off-chip detection, and effects of non-proteolyzed serum on ITP performance.

Acknowledgements

We thank the funding and support from the National Institute of Biomedical Imaging and Bioengineering (R01EB022630) of the National Institutes of Health (NIH) and a National Science Foundation (NSF) Graduate Research Fellowship (A.T.B.). The content is solely the responsibility of the authors and does not necessarily represent the official views of the NIH or NSF.

5 References

- 1 WHO | Data and statistics, <http://www.who.int/hiv/data/en/>, (accessed March 11, 2020).
- 2 World Health Organization (WHO), Guideline on when to start antiretroviral therapy and on pre-exposure prophylaxis for HIV, http://apps.who.int/iris/bitstream/10665/186275/1/9789241509565_eng.pdf.
- 3 World Health Organization, World Health Organization, and Department of HIV/AIDS, *WHO recommendations on the diagnosis of HIV infection in infants and children.*, 2010.
- 4 T. Roberts, J. Cohn, K. Bonner and S. Hargreaves, *Clin Infect Dis*, 2016, **62**, 1043–1048.
- 5 P. K. Drain, J. Dorward, A. Bender, L. Lillis, F. Marinucci, J. Sacks, A. Bershteyn, D. S. Boyle, J. D. Posner and N. Garrett, *Clinical Microbiology Reviews*, 2019, **32**, 25.

- 1
2
3 6 World Health Organization, *Consolidated guidelines on the use of antiretroviral drugs*
4 *for treating and preventing HIV infection: recommendations for a public health*
5 *approach.*, 2016.
6
7 7 A. Niemz, T. M. Ferguson and D. S. Boyle, *Trends in Biotechnology*, 2011, **29**, 240–
8 250.
9
10 8 M. Sidstedt, J. Hedman, E. L. Romsos, L. Waitara, L. Wadsö, C. R. Steffen, P. M.
11 Vallone and P. Rådström, *Analytical and Bioanalytical Chemistry*, 2018, **410**, 2569–
12 2583.
13
14 9 N. B. Y. Tsui, E. K. O. Ng and Y. M. D. Lo, *Clin. Chem.*, 2002, **48**, 1647–1653.
15
16 10 M. M. Burrell, Ed., *Enzymes of molecular biology*, Humana Press, Totowa, N.J, 1993.
17
18 11 R. Boom, C. J. Sol, M. M. Salimans, C. L. Jansen, P. M. Wertheim-van Dillen and J.
19 van der Noordaa, *J. Clin. Microbiol.*, 1990, **28**, 495–503.
20
21 12 P. Chomczynski and N. Sacchi, *Anal. Biochem.*, 1987, **162**, 156–159.
22
23 13 E. J. Wood, *Biochemical Education*, 1983, **11**, 82–82.
24
25 14 N. Ali, R. de C. P. Rampazzo, A. D. T. Costa and M. A. Krieger, *Biomed Res Int*,
26 2017, **2017**, 9306564.
27
28 15 V. Kondratova, O. Serd'uk, V. Shelepov and A. Lichtenstein, *BioTechniques*, 2005,
29 **39**, 695–699.
30
31 16 A. Rogacs, L. A. Marshall and J. G. Santiago, *Journal of Chromatography A*, 2014,
32 **1335**, 105–120.
33
34 17 L. G. Longsworth, *J. Am. Chem. Soc.*, 1953, **75**, 5705–5709.
35
36 18 V. N. Kondratova, I. V. Botezatu, V. P. Shelepov and A. V. Lichtenstein, *Biochemistry*
37 *(Moscow)*, 2009, **74**, 1285–1288.
38
39 19 L. A. Marshall, A. Rogacs, C. D. Meinhart and J. G. Santiago, *Journal of*
40 *Chromatography A*, 2014, **1331**, 139–142.
41
42 20 A. Persat, L. A. Marshall and J. G. Santiago, *Anal. Chem.*, 2009, **81**, 9507–9511.
43
44 21 Y. Qu, L. A. Marshall and J. G. Santiago, *Anal. Chem.*, 2014, **86**, 7264–7268.
45
46 22 A. Rogacs, Y. Qu and J. G. Santiago, *Anal. Chem.*, 2012, **84**, 5858–5863.
47
48 23 C. Eid and J. G. Santiago, *Analyst*, 2017, **142**, 48–54.
49
50 24 M. M. Gong and D. Sinton, *Chem. Rev.*, 2017, **117**, 8447–8480.
51
52 25 B. Y. Moghadam, K. T. Connelly and J. D. Posner, *Anal. Chem.*, 2014, **86**, 5829–
53 5837.
54
55 26 X. Li, L. Luo and R. M. Crooks, *Lab Chip*, 2015, **15**, 4090–4098.
56
57 27 F. Schaumburg, P. A. Kler, C. S. Carrell, C. L. A. Berli and C. S. Henry,
58 *Electrophoresis*, , DOI:10.1002/elps.201900273.
59
60 28 T. Rosenfeld and M. Bercovici, *Lab on a Chip*, 2018, **18**, 861–868.

- 1
2
3 29 B. Y. Moghadam, K. T. Connelly and J. D. Posner, *Anal. Chem.*, 2015, **87**, 1009–
4 1017.
5
6 30 T. Rosenfeld and M. Bercovici, *Lab Chip*, , DOI:10.1039/C4LC00734D.
7
8 31 B. P. Sullivan, A. T. Bender, D. N. Ngyuen, J. Yuqian Zhang and J. D. Posner,
9 *Journal of Chromatography B*, 2020, 122494.
10
11 32 A. T. Bender, M. D. Borysiak, A. M. Levenson, L. Lillis, D. S. Boyle and J. D. Posner,
12 *Analytical Chemistry*, 2018, **90**, 7221–7229.
13
14 33 A. T. Bender, B. P. Sullivan, L. Lillis and J. D. Posner, *The Journal of Molecular*
15 *Diagnostics*, , DOI:10.1016/j.jmoldx.2020.04.211.
16
17 34 L. Lillis, D. A. Lehman, J. B. Siverson, J. Weis, J. Cantera, M. Parker, O. Piepenburg,
18 J. Overbaugh and D. S. Boyle, *Journal of Virological Methods*, 2016, **230**, 28–35.
19
20 35 A. M. Sanchez, C. T. DeMarco, B. Hora, S. Keinonen, Y. Chen, C. Brinkley, M. Stone,
21 L. Tobler, S. Keating, M. Schito, M. P. Busch, F. Gao and T. N. Denny, *J. Immunol.*
22 *Methods*, 2014, **409**, 117–130.
23
24 36 F. Rouet, M.-L. Chaix, E. Nerrienet, N. Ngo-Giang-Huong, J.-C. Plantier, M. Burgard,
25 M. Peeters, F. Damond, D. K. Ekouevi, P. Msellati, L. Ferradini, S. Rukobo, V.
26 Maréchal, N. Schvachsa, L. Wakrim, C. Rafalimanana, B. Rakotoambinina, J.-P. Viard,
27 J.-M. Seigneurin, C. Rouzioux and for the A. N. de R. sur le S. A. W. Groups, *JAIDS*
28 *Journal of Acquired Immune Deficiency Syndromes*, 2007, **45**, 380–388.
29
30 37 J. Dreier, M. Störmer and K. Kleesiek, *Journal of Clinical Microbiology*, 2005, **43**,
31 4551–4557.
32
33 38 A. Persat, M. E. Suss and J. G. Santiago, *Lab Chip*, 2009, **9**, 2454–2469.
34
35 39 V. N. Kondratova, I. V. Botezatu, V. P. Shelepov and A. V. Lichtenstein, *Analytical*
36 *Biochemistry*, 2011, **408**, 304–308.
37
38 40 W. A. Al-Soud and P. Rådström, *J. Clin. Microbiol.*, 2001, **39**, 485–493.
39
40 41 H. Suzuki and T. Terada, *Analytical Biochemistry*, 1988, **172**, 259–263.
41
42 42 L. Boiso and J. Hedman, *Forensic Science International: Genetics*, 2017, **29**, e16–
43 e18.
44
45 43 M. Bercovici, S. K. Lele and J. G. Santiago, *Journal of Chromatography A*, 2009,
46 **1216**, 1008–1018.
47
48 44 T. K. Khurana and J. G. Santiago, *Analytical Chemistry*, 2008, **80**, 6300–6307.
49
50 45 N. C. Stellwagen and E. Stellwagen, *J Chromatogr A*, 2009, **1216**, 1917–1929.
51
52 46 N. C. Stellwagen, C. Gelfi and P. G. Righetti, *Biopolymers*, 1997, **42**, 687–703.
53
54 47 *Biophysical Journal*, 2004, **86**, 681–689.
55
56 48 S. Bhattacharyya, P. P. Gopmandal, T. Baier and S. Hardt, *Physics of Fluids*, 2013,
57 **25**, 022001.
58
59 49 G. Garcia-Schwarz, M. Bercovici, L. A. Marshall and J. G. Santiago, *Journal of Fluid*
60 *Mechanics*, 2011, **679**, 455–475.

- 1
2
3 50 E. Jankowsky and M. E. Harris, *Nat Rev Mol Cell Biol*, 2015, **16**, 533–544.
4
5 51 D. Goldenberger, I. Perschil, M. Ritzler and M. Altwegg, *PCR methods and*
6 *applications*, 1995, **4**, 368–370.
7
8 52 M. Johnson, *Materials and Methods*.
9
10 53 Brown Robert B and Audet Julie, *Journal of The Royal Society Interface*, 2008, **5**,
11 S131–S138.
12
13 54 R. McGookin, *Methods Mol. Biol.*, 1985, **2**, 109–112.
14
15 55 S. Paik and X. Wu, *Chem. Health Saf.*, 2005, **12**, 33–38.
16
17 56 C. D. Pilcher, G. Joaki, I. F. Hoffman, F. E. Martinson, C. Mapanje, P. W. Stewart,
18 K. A. Powers, S. Galvin, D. Chilongozi, S. Gama, M. A. Price, S. A. Fiscus, M. S. Cohen
19 and M. for the UNC Project, *AIDS*, 2007, **21**, 1723–1730.
20
21 57 L. M. Luft, M. J. Gill and D. L. Church, *International Journal of Infectious Diseases*,
22 2011, **15**, e661–e670.
23
24 58 A. V. Ritchie, I. Ushiro-Lumb, D. Edemaga, H. A. Joshi, A. De Ruiter, E. Szumilin, I.
25 Jendrulek, M. McGuire, N. Goel, P. I. Sharma, J.-P. Allain and H. H. Lee, *Journal of*
26 *Clinical Microbiology*, 2014, **52**, 3377–3383.
27
28 59 A. Nabatiyan, Z. A. Parpia, R. Elghanian and D. M. Kelso, *J. Virol. Methods*, 2011,
29 **173**, 37–42.
30
31 60 S. Hin, M. Loskyll, V. Klein, M. Keller, O. Strohmeier, F. von Stetten, R. Zengerle and
32 K. Mitsakakis, *Microelectronic Engineering*, 2018, **187–188**, 78–83.
33
34
35
36
37
38
39
40
41
42
43
44
45
46
47
48
49
50
51
52
53
54
55
56
57
58
59
60