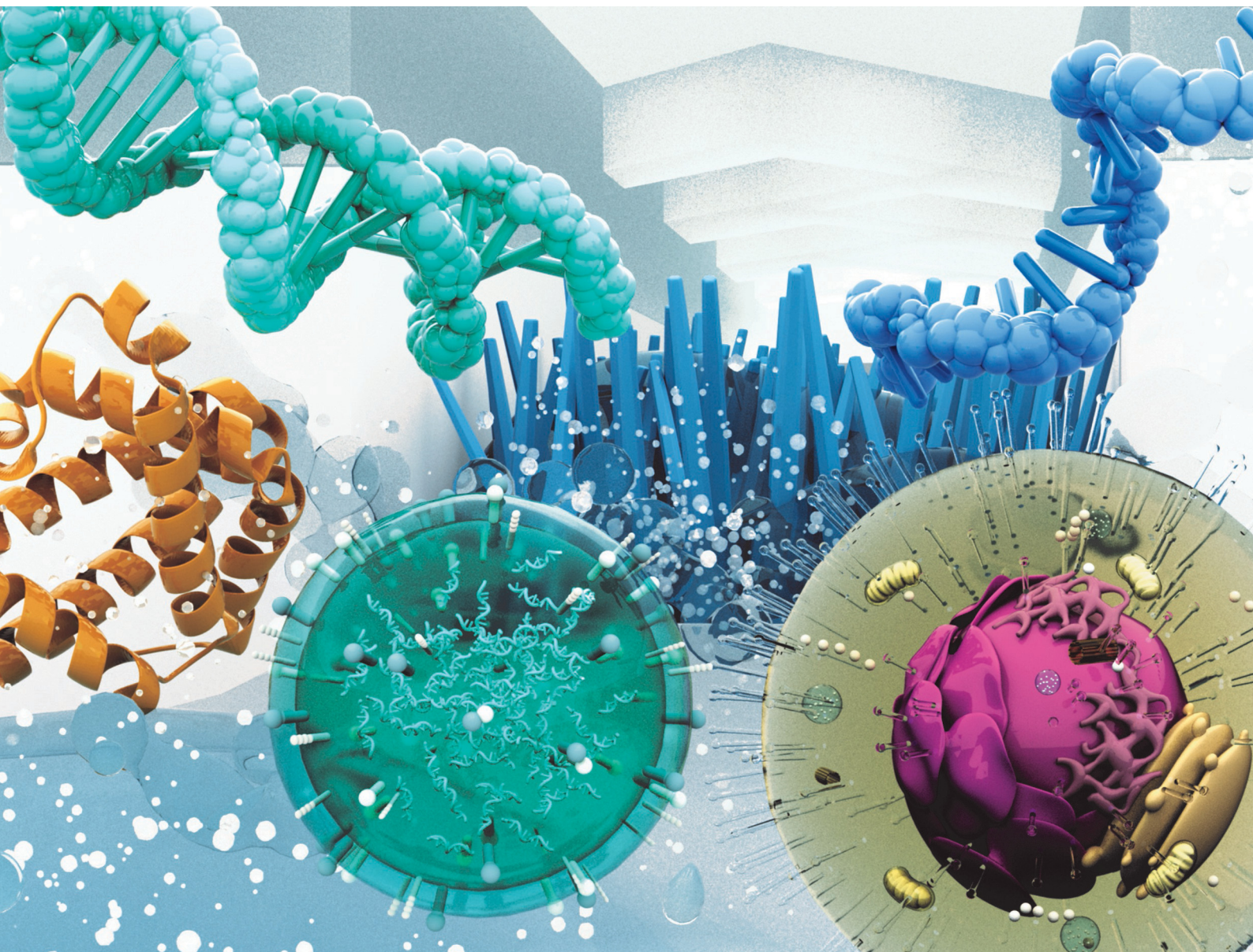


ChemComm

Chemical Communications

rsc.li/chemcomm



ISSN 1359-7345

FEATURE ARTICLE

Takao Yasui *et al.*

Oxide nanowire microfluidics addressing
previously-unattainable analytical methods
for biomolecules towards liquid biopsy


 Cite this: *Chem. Commun.*, 2021, 57, 13234

Oxide nanowire microfluidics addressing previously-unattainable analytical methods for biomolecules towards liquid biopsy

 Hiromi Takahashi,^a Yoshinobu Baba^{abc} and Takao Yasui^{ib}*^{abd}

Nanowire microfluidics using a combination of self-assembly and nanofabrication technologies is expected to be applied to various fields due to its unique properties. We have been working on the fabrication of nanowire microfluidic devices and the development of analytical methods for biomolecules using the unique phenomena generated by the devices. The results of our research are not just limited to the development of nanospace control with “targeted dimensions” in “targeted arrangements” with “targeted materials/surfaces” in “targeted spatial locations/structures” in microfluidic channels, but also cover a wide range of analytical methods for biomolecules (extraction, separation/isolation, and detection) that are impossible to achieve with conventional technologies. Specifically, we are working on the extraction technology “the cancer-related microRNA extraction method in urine,” the separation technology “the ultrafast and non-equilibrium separation method for biomolecules,” and the detection technology “the highly sensitive electrical measurement method.” These research studies are not just limited to the development of biomolecule analysis technology using nanotechnology, but are also opening up a new academic field in analytical chemistry that may lead to the discovery of new pretreatment, separation, and detection principles.

 Received 10th September 2021,
 Accepted 15th October 2021

DOI: 10.1039/d1cc05096f

rsc.li/chemcomm

1. Introduction

Biomolecule analysis has greatly impacted the understanding of molecular mechanisms underlying human health and disease. The ability to analyze biomolecules is expected to provide a powerful tool for disease diagnosis based on molecular signatures.¹ Because biomolecular analysis is largely dictated by the characteristics of biomolecules, an essential requirement for analysis is a sensitive method to overcome existing challenges and open new research fronts. Nanostructures fabricated by using self-assembly and nanofabrication technologies are expected to be applied to bioanalytical fields due to their unique properties and shapes.

Breakthrough research in nanotechnology over the past decade has led to significant progress in biomolecular analysis with the emergence of engineered nanomaterials. Several types of nanomaterials, including zero-dimensional (0D) nanoparticles,

one-dimensional (1D) nanowires, two-dimensional (2D) nanosheets, and three-dimensional (3D) nanoplates, were designed and developed to address challenges of materials and applications in traditional methods *via* their unique properties that lie


Takao Yasui

Takao Yasui is an Associate Professor of the Department of Biomolecular Engineering, Graduate School of Engineering, Nagoya University, a PRESTO Researcher at Japan Science and Technology Agency (JST), and a co-founder and a Nanodevice Director at Craif Inc. In 2011, he received his PhD from the Department of Applied Chemistry, Graduate School of Engineering, Nagoya University. He has received over 35 awards

for his contributions in the field of oxide nanowire microfluidics. His research interests are focused on designing, fabricating, and characterizing oxide nanowire microfluidics for application in healthcare, diagnosis, sensing biomolecules and engineering biology.

^a Department of Biomolecular Engineering, Graduate School of Engineering, Nagoya University, Furo-cho, Chikusa-ku, Nagoya 464-8603, Japan

^b Institute of Nano-Life-Systems, Institutes of Innovation for Future Society, Nagoya University, Furo-cho, Chikusa-ku, Nagoya 464-8603, Japan

^c Institute of Quantum Life Science, National Institutes for Quantum Science and Technology, Anagawa 4-9-1, Inage-ku, Chiba 263-8555, Japan

^d Japan Science and Technology Agency (JST), PRESTO, 4-1-8 Honcho, Kawaguchi, Saitama 332-0012, Japan. E-mail: yasui@chembio.nagoya-u.ac.jp



in their nanoscale size.^{2–4} Among them, much effort has been made to explore and utilize the attractive properties of nanowires in a wide range of fields, including electronics, photonics, energy conversion, and storage, as well as biomedical applications, ever since Morales and Lieber reported a method to synthesize nanowires.⁵ The widespread adoption of nanowires has been made possible by the advancement of the chemical synthesis of nanowires, whereby unprecedented characteristics and properties could be obtained, thereby enhancing the effectiveness of applications.

In bioanalytical and biomedical applications, nanowires have come under the spotlight by virtue of their regime size compared with that of biomolecules and high surface area-to-volume ratio; both are the critical factors in achieving high levels of sensitivity.^{2,6,7} Several studies on the interfaces between nanowire devices and biological systems, notably by the Lieber group, have extensively explored a variety of applications over the past two decades. For example, a nanowire-based sensor was developed by the Lieber group in 2001 to be applied to biological and chemical systems.⁸ In that work, they demonstrated the possibility to exploit nanowires as biosensors by configuring them in a field-effect transistor (FET) system. The nanowires were modified with a receptor selective to a specific biomolecule; the receptors and biomolecules were 3-aminopropyltriethoxysilane (APTES), biotin, and calmodulin, which responded to changes in pH, streptavidin, and calcium ions, respectively. Since then, nanowires have been widely explored in biosensing applications. In another report by the Lieber group in 2005, they demonstrated a nanowire FET as a real-time multiplexed device for early-stage detection of cancer⁹ by modifying the surfaces of the nanowires with antibodies to detect four different cancer protein markers in serum samples. In 2012, Huang *et al.*¹⁰ developed a biosensor based on the earlier nanowire FET system,^{8,9} in which the nanowires were functionalized with glutaraldehyde to immobilize prostate-specific antigen, as a demonstration device to detect PSA biomarkers at the femtogram level in desalted human serum samples. These early investigations opened opportunities in the field of nanosensors for bioanalytical and biomedical applications, and led to the dramatic growth of research on nanowire-based sensors that continues even now.^{6,11–15}

Besides nanowire-based sensors, there are several examples using nanowires as bioanalytical and biomedical tools that are due to the capabilities of nanowires to directly interface with biomolecules. For instance, the first cell-penetrating nanowire array for delivering genes was reported by the Yang group in 2007,¹⁶ and it showed that the nanowires could be used to deliver genes into living mammalian stem cells which were cultured on nanowires and survived up to a week. Later in 2009, Wang *et al.*¹⁷ demonstrated that 3D nanostructures coated with specific antibodies were able to capture circulating tumor cells (CTCs) with higher efficiency than a flat surface due to the high surface area-to-volume ratio of the nanowires. Based on a similar concept, previous studies have also reported nanowire arrays for isolating CD4⁺ T lymphocyte cells, a cancer biomarker, from heterogeneous cell mixtures by functionalizing nanowire

surfaces with a specific antibody.^{18,19} More recently, the Cho group has developed a conductive polymer nanowire platform that is effective for capture and release based on a simple electrochemical method for biomolecules, such as cells,²⁰ nucleic acids,²¹ and exosomes.²² Numerous studies on nanowires have been undertaken for interfacing with several biomolecules, including CTCs,^{23–32} nucleic acids,^{33–38} and exosomes,^{39–42} for a wide range of applications. These nanowire platforms showed improved biomolecule capture efficiency because of the nanowires, allowing for high sensitivity and specific recognition.

In the past decade there has been tremendous progress in the synthesis of nanowires, which results in new characteristics and properties, offering innovative applications. For example, Liu *et al.*⁴³ demonstrated bendable polycrystalline nanowires that enable capture of bacteria in the bloodstream with higher efficiency than traditional nanowires due to their increased anti-shearing force toward bacteria. Ren *et al.*⁴⁴ proposed a nanowire fabrication method based on a block copolymer-directed orthogonal assembly to construct arrays of 3D multilayer-crossed stacked metal oxide semiconducting nanowires, which can be subsequently doped with metal oxide, depending on a particular application. The nanowire arrays offer many target–receptor interfaces and improved molecule diffusion and good charge transport, which can benefit application in resistors, biosensors, and electrocatalysts (Table 1).

The advent of microfluidics⁴⁵ has brought about a paradigm shift in bioanalytical and biomedical applications of nanowires, and led to the emergence of the concept of microfluidic nanowire platforms. Integration of microfluidic systems and nanowires provides a variety of advantages over conventional methods. First, a microfluidic system coupled with nanoscale dimension wires offers several advantages, including enhanced sensitivity, reduced sample and reagent consumption, and shortened processing time. Second, the structural and physical properties of nanowires can be readily tailored to a particular application. Third, the surfaces of the nanowires can be modified with biomaterials, including enzymes, antibodies, and nucleic acids, which promises diverse applications with enhanced specificity.

In this feature article, we provide a comprehensive review on bioanalytical methods using nanowire microfluidic devices that are not feasible with conventional techniques (Fig. 1). We developed nanospace control with “targeted dimensions” in “targeted arrangements” with “targeted materials/surfaces” in “targeted spatial locations/structures” in microfluidic channels (Fig. 2) and deployed them for precise control of the nanospace to develop innovative bioanalysis. Specifically, we developed the following technologies: extraction technologies for biomolecules that have been difficult to extract with conventional techniques, separation technologies of biomolecules employing different separation principles from conventional technology, and detection technologies for biomolecules that enable highly sensitive electrical measurements. These studies are not just limited to the development of biomolecule analysis technologies using nanotechnology, but they are also opening



Table 1 Summary of types of nanowires and their applications

Materials	Applications	Diameter, length, and surface area-to-volume ratio ^a	Ref.	Note
ZnO	Extracellular vesicle separation	~100 nm, ~2 μm, ~40 μm ⁻¹	39, 86 and 87	Dissolve under alkaline conditions such as blood plasma ⁵¹
	Urinary miRNA extraction	~100 nm, ~2 μm, ~40 μm ⁻¹	55 and 56	
	Cell lysis and DNA extraction	~75 nm, ~1 μm, ~54 μm ⁻¹	38	
	Circulating tumor cell separation	~200 nm, ~1 μm, ~21 μm ⁻¹	23	
	Fluorescence-based DNA detection	~90 nm, ~1.4 μm, ~45 μm ⁻¹	97	
ZnO/ZnO	ssDNA extraction	~100 nm, ~1.7 μm, ~41 μm ⁻¹	49	Stable under alkaline conditions ⁵¹
ZnO/Al ₂ O ₃	ssDNA and RNA extraction	~100 nm, ~1.7 μm, ~41 μm ⁻¹	49 and 51	
	Extracellular vesicle extraction	~100 nm, ~2 μm, ~40 μm ⁻¹	55	
ZnO/SiO ₂	ssDNA extraction	~100 nm, ~1.7 μm, ~41 μm ⁻¹	49 and 50	
	Bacterial extraction	~70 nm, ~1.2 μm, ~58 μm ⁻¹	64	
ZnO/TiO ₂	Extracellular vesicle separation	~100 nm, ~2 μm, ~40 μm ⁻¹	86	
SnO ₂ /SiO ₂	DNA separation	~30 nm, ~2 μm, ~134 μm ⁻¹	78–80	
SiO ₂	DNA separation	~500 nm, ~4 μm, ~8 μm ⁻¹	69 and 70	
SnO ₂	Bacterial extraction	~10 nm, ~7 μm, ~400 μm ⁻¹	63	
ZnO/(Cu _{1-x} Zn _x)O	Electrical-based DNA detection	~100 nm, ~2 μm, ~40 μm ⁻¹	99	
WO ₃	Electrical DNA detection	~400 nm, ~5 μm, ~10 μm ⁻¹	98	
SiO ₂	Circulating tumor cell separation	~300 nm, ~4 μm, ~14 μm ⁻¹	27	
	Electrical-based DNA detection	~20 nm, ~4 μm, ~200 μm ⁻¹	8, 12 and 35	
Magnetic Polymer	Extracellular vesicle separation	~36 nm, ~2.3 μm, ~112 μm ⁻¹	40–42	
	Circulating tumor cell separation	~200 nm, ~14 μm, ~20 μm ⁻¹	22	

^a If the diameter or length was not given in the cited reference(s), these parameters were measured from the electron microscope images.

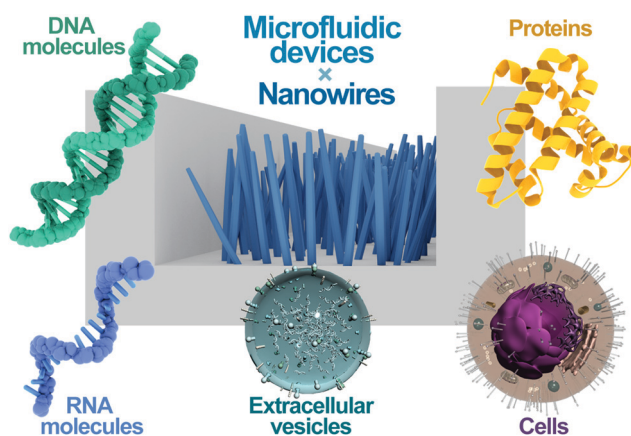


Fig. 1 An overview of bioanalytical methods using nanowire microfluidic devices. The combination of nanowires and microfluidic devices enables the analysis of DNA molecules, RNA molecules, proteins, extracellular vesicles, and cells.

up a new academic field in analytical chemistry that may lead to the discovery of new pretreatment, separation, and detection principles.

2. Nanowire-based extraction

The extraction of nucleic acids is the initial and essential step in preparing them for downstream processes, a step that provides insights into their molecular signatures, which is the key to developing strategies for molecular diagnostics. The total yield and quality of biomolecules have a significant impact on the overall analytical performance. However, the existing technologies to extract biomolecules suffer from low extraction efficiency due to the low sensitivity of their extraction platforms. Therefore, there is a need to develop strategies that

ensure the quality and maximum yield of nucleic acids, maximizing the effectiveness of analysis. Our work has focused on developing nanowire devices capable of extracting nucleic acids from different sources, including biological fluids, extracellular vesicles, and bacteria.

2.1. DNA and RNA extraction from biological fluids

Tremendous progress over the past decade has been made in unraveling the clinical significance of circulating nucleic acids, including cell-free DNA, mRNA, and miRNA, as biomarkers and their role in diseases, to accelerate the growing field of nucleic acids for molecular diagnostics.^{46–49} Accessing molecular biomarkers in biological fluids, such as blood and urine, has been hampered by a lack of sensitive devices to isolate low levels of biomolecules in the presence of high levels of contaminants in the fluids. To overcome this challenge, we demonstrated that ZnO/Al₂O₃ core/shell nanowires can capture single-stranded DNA (ssDNA) with high efficiency, presumably due to the attraction of the phosphate backbones and the nucleobases of nucleic acids to nanowire surfaces.⁵⁰ These findings suggest that ZnO/Al₂O₃ core/shell nanowires can be utilized as a nanostructure platform for capturing ssDNAs.

Since the biocompatibility of nanostructures with biological fluids is essential for biomedical applications, in our recent work, we enhanced this biocompatibility by developing annealed ZnO/Al₂O₃ core/shell nanowires as a platform for capturing RNA molecules (Fig. 3).⁵¹ We demonstrated that our devices are biocompatible with blood plasma samples and enable the capture of RNA molecules with high efficiency. This work represents a feasibility study to develop nanowire devices for capturing nucleic acids. More in-depth studies, such as those regarding the interaction mechanism between nucleic acids and nanowire surfaces, would promote the direct



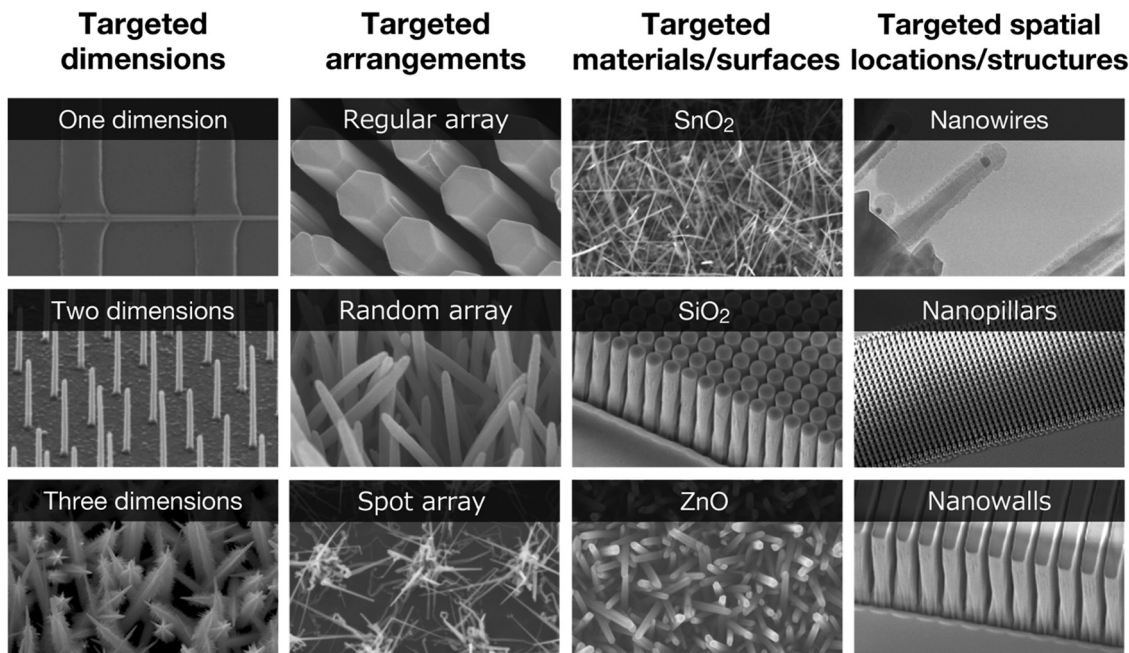


Fig. 2 A concept of nanostructures with “targeted dimensions” in “targeted arrangements” with “targeted materials/surfaces” in “targeted spatial locations/structures” in microfluidic channels.

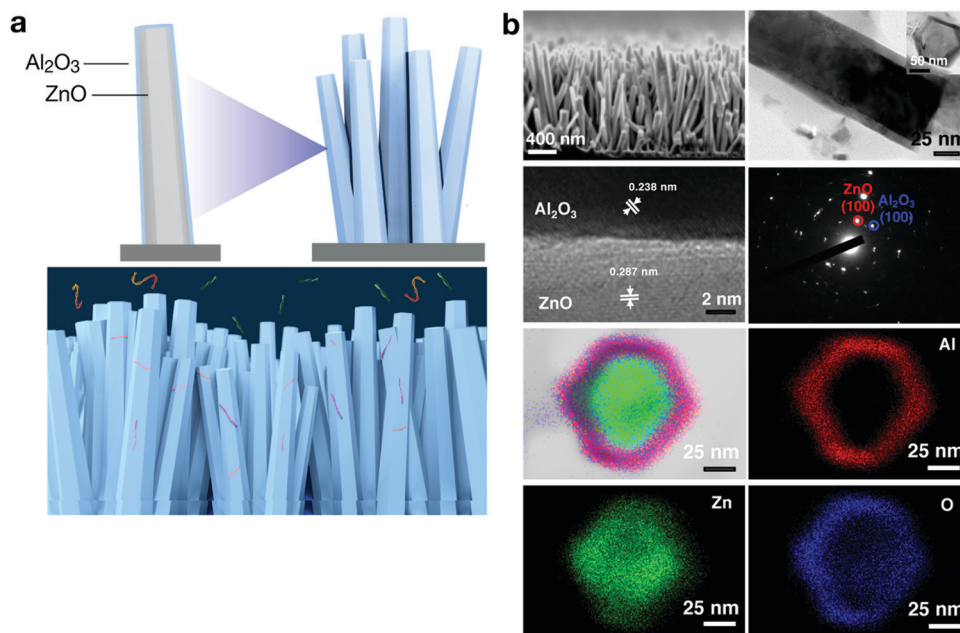


Fig. 3 (a) Annealed ZnO/Al₂O₃ core/shell nanowires were developed as a platform for capturing RNA molecules.⁵¹ (b) Characterization of the annealed ZnO/Al₂O₃ core/shell nanowires by scanning electron microscopy (SEM; first row left), transmission electron microscopy (TEM; first row right and second row left), X-ray diffraction (second row right), and TEM-energy dispersive X-ray spectroscopy (third and fourth rows).⁵¹

isolation of circulating nucleic acids or even sequence-specific nucleic acids from biological samples.

2.2. MicroRNA extraction from extracellular vesicles (EVs) in biological fluids

A number of findings now point to the properties of EV-encapsulated miRNAs being involved in cell communication

and epigenetic regulation,^{52,53} leading them to emerge as a new potential source for liquid biopsy. Use of urine-based liquid biopsies serves as a truly non-invasive approach to access biomolecular information for molecular diagnostics. However, genomic analysis of miRNAs is restricted in sensitivity due to their limited abundance in urine.⁵⁴ To address this challenge, we proposed a nanowire-based methodology for collecting urine



miRNAs including EV-encapsulated miRNAs and EV-free miRNAs,⁵⁵ which facilitated the first direct extraction of miRNA from EVs in urine samples (Fig. 4). In this work, ZnO nanowires were grown from buried nanowires embedded in a PDMS substrate and bonded with the microchannel in which there was a PDMS herringbone-structure. We demonstrated that this device collected EVs at high efficiency and massively extracted various miRNAs that unveiled up to 1000 types of miRNA sequences. The effectiveness of the device is the result of the nanowire properties, the mechanical stability of the nanowires that are firmly anchored into the substrate and unaffected during buffer flow, and the electrostatic collection that enables negatively charged EVs to be collected with higher efficiency than by conventional methods. The results we obtained in this work have led us to employ this methodology further to extract miRNA from EVs in urine samples.

In one of our most recent papers, we developed a sterilizable and mass-producible nanowire-based device to help in meeting the long-term goal of achieving liquid biopsy using urinary miRNAs.⁵⁶ An assembly-type microfluidic nanowire device was fabricated by two processes: first, ZnO nanowire scaffolds were fabricated on a silicon substrate, and second, ZnO nanowire scaffolds were assembled in an assembly-type microfluidic device (Fig. 4). We showed the effectiveness of our device to extract miRNAs from 1 mL of urine samples, and it provided a significantly greater variety and quantity of miRNA sequences compared to conventional methods. In addition, by identifying the origin of urinary miRNAs in patients with central nervous system (CNS) tumors, we confirmed that many CNS tumor-derived miRNAs could be identified in urine. These findings will surely impact the development of a diagnostic model based on urinary miRNA expression.

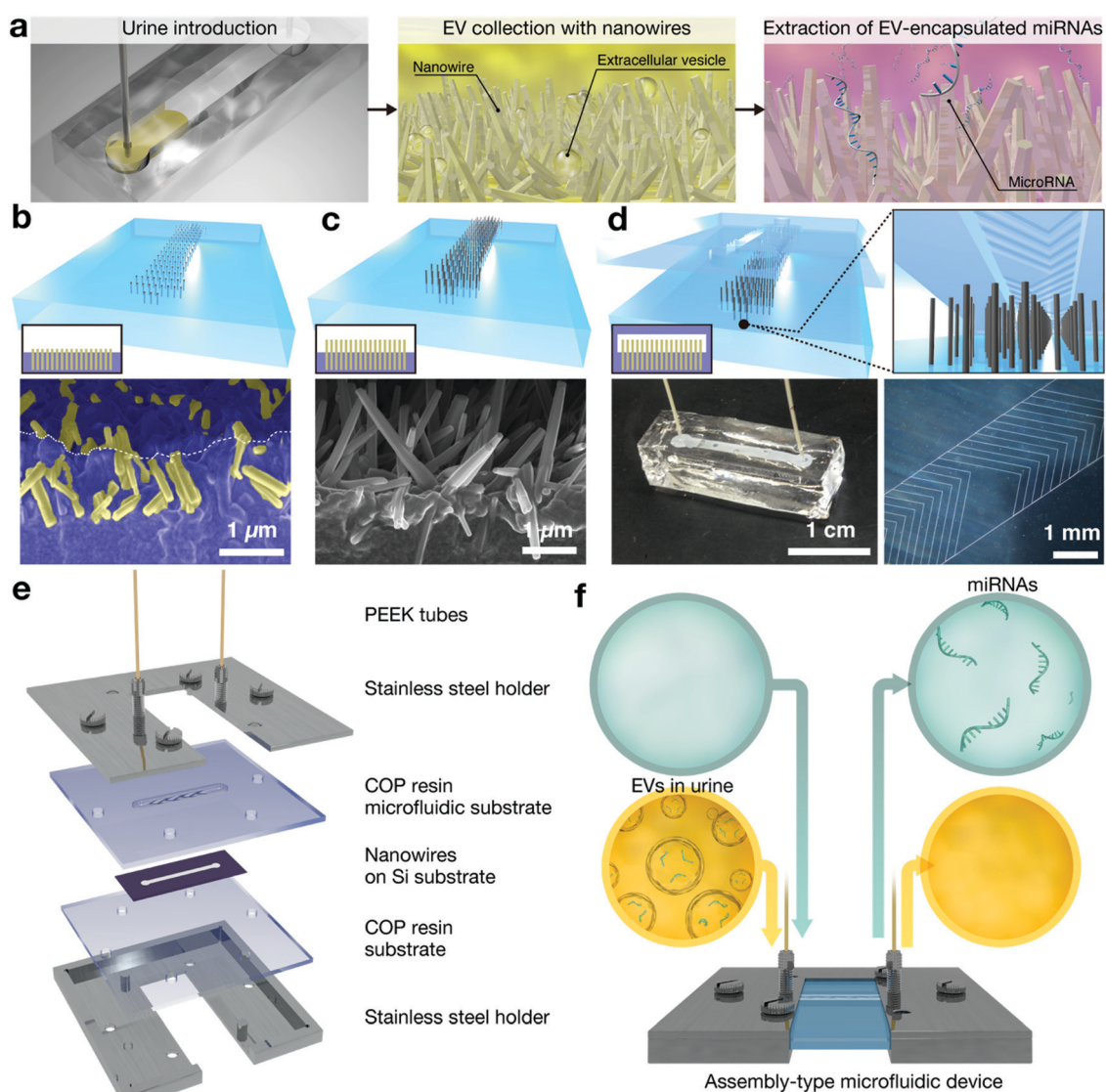


Fig. 4 (a) Schematic of miRNA extraction in urine.^{55,56} (b–d) Schematic and SEM images for nanowire microfluidics to extract miRNAs from urine.⁵⁵ (e) Exploded view of the assembly-type of nanowire microfluidics consisting of PEEK tubes, stainless steel holders, a COP resin microfluidic substrate, nanowires on a Si substrate, and a COP resin substrate.⁵⁶ (f) Schematic of miRNA extraction from urine using the assembly-type of nanowire microfluidics.⁵⁶



2.3. DNA extraction from bacteria

Bacteria are essential biomolecules that store genetic information both in single chromosomes, with the size of double-stranded DNA ranging from 600 kb to 9.5 Mb, and in plasmids, which play key roles in microorganisms.⁵⁷ Therefore, this has resulted in several studies whose purposes were investigating antibiotic resistance from bacterial plasmids,⁵⁸ molecular diagnostics of pathogens,⁵⁹ and microbial genome sequencing from single microbial cells.^{60,61} The genetic information contained inside bacteria must be isolated *via* the lysis method based on enzymatic, thermal, chemical, or mechanical treatment.⁶² However, these treatments have many disadvantages, including ineffective lysis caused by insufficient thermal diffusion or reagent diffusion, and high costs and complex setups. To solve these challenges, we previously reported our concept of nanowire-mediated microbial cell lysis, which enables extraction of DNAs from microbial cells (Fig. 5).^{63,64} This concept relies on the biocompatibility, thinness, and flexibility of SnO₂ nanowires, and on enhancing the adsorption of bacteria by entanglements. Its mechanism involves mechanical force that stretches the cell membrane, thereby rupturing cells. In addition, we showed the versatility of a device that allows its integration with nucleic acid amplification assay, as the loop-mediated isothermal amplification method, to amplify target genes isothermally. The device realizing our concept has the advantages of being simple and rapid, and using fewer samples, all of which are very important as a microfluidic analytical platform.

3. Nanowire-based separation

In biomolecular analysis, separating biomolecules from a complex mixture is a crucial step in understanding the underlying mechanism of the functions in specific biomolecules. In general, the most widely used biomolecule separation method is electrophoresis,⁶⁵ whereby biomolecules can be separated from each other under an electric field based on the charge-to-mass ratio. However, electrophoresis consumes time, labor, reagents, and sample resources. To overcome these limitations, nanostructure-based electrophoresis separation has been introduced due to its capability to manipulate fluid samples at the nanoscale, leading to reduced consumptions of time, labor, reagents, and sample resources. We have advanced the development of separation methods using nanostructures, such as nanopillars and nanowalls, for applications in combination with nanowires. Moreover, we have demonstrated the surface modification of nanowires with a specific peptide to separate biomolecules, including EVs and proteins, based on immunoaffinity, thereby promoting the separation efficiency.

3.1. DNA separation using nanopillars and nanowalls

Toward improved performance of DNA separation using nanostructures, we proposed that a nanopillar array and a nanowall array were good candidates that affect the transport of DNA molecules.^{66–74} Since nonequilibrium transport is considered to have the potential to overcome the intrinsic trade-off between the separation speed and resolution of DNA separations, we

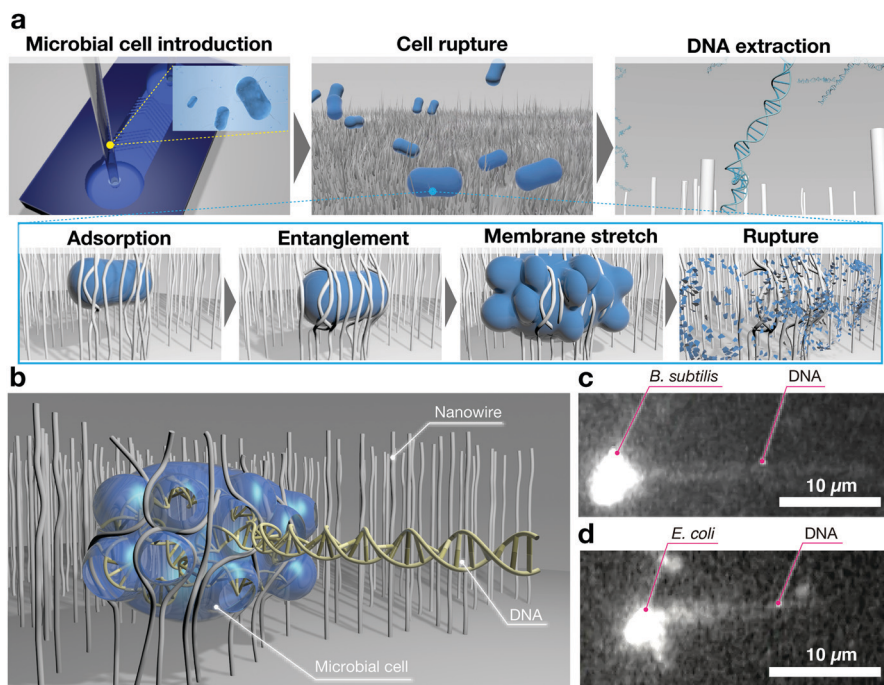


Fig. 5 (a) Schematic of DNA extraction in microbial cells. The adsorbed cells on nanowires are ruptured by nanowire-entanglement and membrane stretching.⁶³ (b–d) Schematic diagram of the moment of DNA extraction *via* nanowire-entanglement, and snapshots of fluorescence images of DNA extraction from *B. subtilis* and *E. coli*.⁶³



demonstrated that the nonequilibrium transport of DNA molecules could be achieved by arranging a nanopillar square array, and we achieved a faster separation without any loss of resolution (Fig. 6).⁶⁹ One major drawback of previous studies was the need for fluorescence labeling,⁷⁵ which can affect the biomolecular characteristics. In our recent work, we aimed at label-free monitoring of biomolecular separation using the intensity variation of a laser diffracted using a nanopillar array,⁷⁰ and we demonstrated that our proposed nanopillars yielded label-free monitoring and separating of DNA molecules in a nonequilibrium manner. In addition to the nanopillar array, we also proposed a nanowall array for DNA separations, methylation identification, and label-free detections (Fig. 6).^{71–74} We reported separation of a mixture of DNA fragments (48.5 kbp and 1 kbp fragments) within 30 s by applying an electric voltage, showing that larger DNA fragments migrate faster than shorter ones, and we confirmed that label-free detection based on the intensity variation of the laser diffracted by the nanowall array was achieved. These studies are not just limited to the development of DNA separation and detection technologies using nanotechnology, but are also opening up a new area of analytical chemistry that includes the discovery of new separation and detection principles.

In electrophoretic separation, it is necessary to consider not only the separation mechanism, but also the various factors involved in the separation, such as electroosmotic flow (EOF)

and preconcentration. We investigated the effect of electroosmotic flow and the possibility of preconcentration in arrays using nanopillars. We reported the first quantitative investigation and formulation of EOF mobility in microchannels with nanopillar array structures⁷⁶ and demonstrated that the charge density of the nanopillar region affected the suppression of EOF, while the arrangement of nanopillars had no effect on it. These findings contributed to the development of a nanopillar array chip for DNA manipulation and separation. Moreover, to overcome the challenges for detecting low concentrations of target biomolecules in samples, an on-line stacking technique was proposed.⁷⁷ The on-line stacking technique offers the capability to concentrate biomolecules into a smaller volume, and in this work, we developed a nanopillar array chip integrated with the on-line stacking for DNA separation, which allowed for faster separation, higher sensitivity and higher resolution compared to performance reported in previous studies. These results offer useful information for electrophoretic separation using not only nanopillars but also other nanostructures, such as nanowires.

3.2. DNA separation using nanowires

Despite the successful applications of nanopillar arrays and nanowall arrays for DNA separation, the fabrication process has remained technically challenging to obtain the desirable size range and form 3D designed spatial nanostructures. Nanowire arrays,

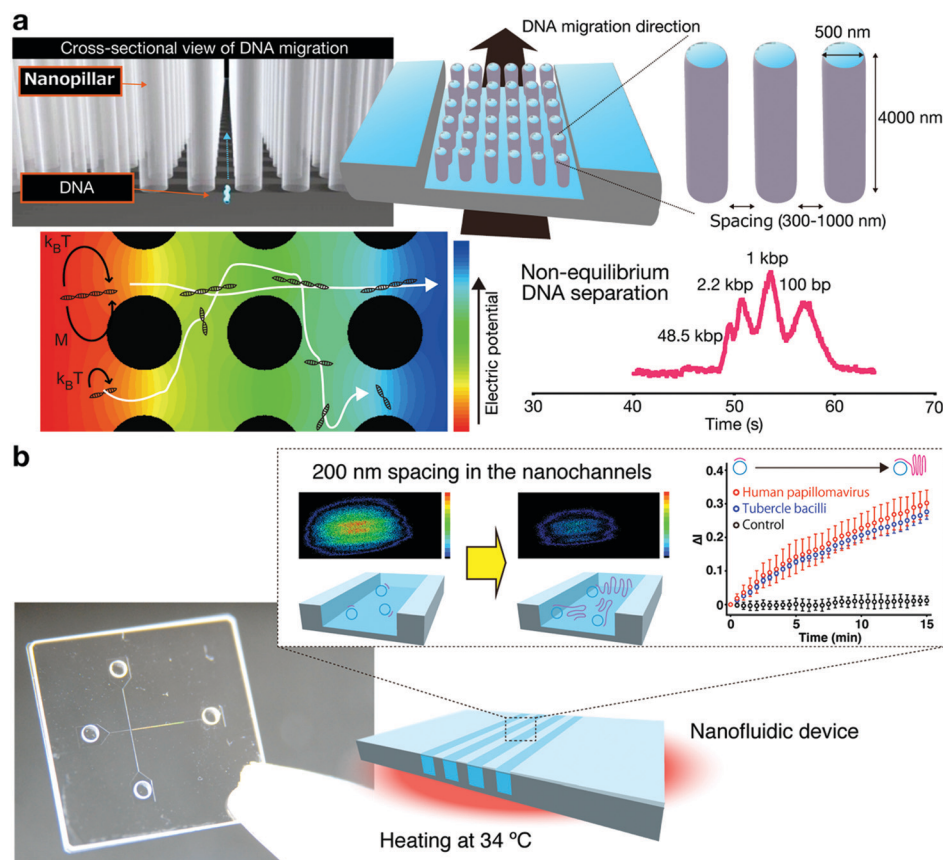


Fig. 6 (a) Non-equilibrium DNA separation using nanopillar arrays.⁶⁹ (b) Label-free detection of DNA amplification in a nanofluidic device.⁷³



therefore, have emerged as an alternative nanostructure due to the easy fabrication control for the desired size and spatial pattern. In addition, the thin structure of the nanowires offers a benefit for DNA separation, since it can elongate the DNA molecules effectively with minimal bending deformation. Among our early attempts to explore nanowire arrays, we developed a SnO₂ nanowire spot-array for DNA manipulation and separation.⁷⁸ This was the first time that a small structure with a diameter of about 10 nm had been fabricated at a targeted location inside a microchannel. We demonstrated that the nanowire spot-array could elongate long T4 DNA molecules *via* unique entanglement events. In addition, we found that the retardation of the electrophoretic mobility of DNA molecules caused DNA separation due to the frequent collisions and quick relaxation caused by the nanowire spot-array structure. The investigation presented in this work has provided the fundamentals for our development of nanowires for DNA manipulation and separation.

To improve the resolution for DNA separation with the device, we have developed 3D nanowire arrays for ultra-fast separation of biomolecules.^{79–81} In our latest work, by advancing the self-assembling formation technology of nanowires, we fabricated branching nanowire structures and developed the world's first 3D nanowire arrays that can be spatially controlled to a level of a few nanometers at targeted locations in microchannels. The proposed methodology for controlling the pore size of the 3D nanowire arrays was varying the number of nanowire growth cycles (Fig. 7),⁸¹ which allows us to obtain nanowires sized as thin as the hydrodynamic radius of protein and RNA molecules.⁸⁰ Using this technique, we have achieved fast separation of not only DNA but also RNA and proteins with molecular weights smaller than DNA within a few seconds to a few tens of seconds.

3.3. EV separation using nanowires

To take advantage of the full potential of EVs as biomarkers, methodologies that not only separate special subsets of EVs but also profile encapsulated miRNAs and membrane proteins of EVs are required to identify the correlation between the captured EV subsets and profiled EV-encapsulated miRNAs and EV

membrane proteins. Current methodologies for EV separation are mainly divided into three groups:⁸² density-based separation using ultracentrifugation;⁸³ size-based separation using size exclusion chromatography; and immunoaffinity-based separation (for specific membrane proteins, *e.g.*, CD9, CD63, and CD81). As emerging alternatives, microfluidic-based platforms (density-, immunoaffinity-, and size-based separations)^{84,85} have been reported. The EV subsets obtained through density-, size-, and immunoaffinity-based separations have been extensively studied, but fewer efforts have been devoted to investigating the correlation between EV subsets obtained through surface charge-based separation and encapsulated miRNAs or expressed membrane proteins. We introduced a nanowire-based separation concept that could collect EVs based on nanowire surface potentials; the analysis targets were urinary microRNAs^{55,56} and expressed membrane proteins.⁸⁶

The feasibility of charge-based separation of EVs on nanowires was demonstrated by using different oxide materials⁸⁶ (Fig. 8). As different oxide materials, we deposited TiO₂ and SiO₂ on ZnO nanowires to form different surface potentials of the nanowires in the same pH range. Around pH = 7, the ZnO (bare) nanowires had a positively charged surface, and the ZnO/TiO₂ (core/shell) and ZnO/SiO₂ (core/shell) nanowires had a negatively charged one. All types of nanowires could separate EVs, and the ZnO (bare) nanowires showed the highest separation efficiency among the three types of nanowires. Although the positively charged surfaces of the nanowires showed the highest separation efficiency, the negatively charged surfaces of the nanowires could also separate EVs. The ZnO (bare) nanowires have become our first choice for charge-based separation of EVs from the standpoint of separation efficiency.⁸⁶

Charge-based separation combined with immunoaffinity-based separation is expected to be used for enhanced specific separation of EVs with specific biomarkers. We recently reported peptide-functionalized ZnO nanowires in which the nanowires were functionalized with the bifunctional peptide specific to CD9 cancer-related EVs.⁸⁷ Whereas the surface modification with antibodies could capture EVs, our methodology achieved functionalizing with the peptide without cross-linking in

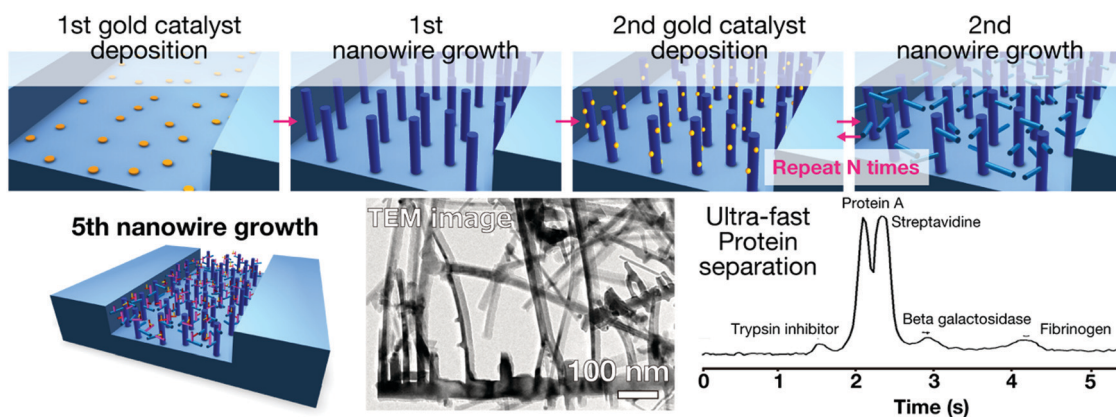


Fig. 7 The 3D nanowire array for ultra-fast separation of biomolecules.⁷⁹ The 3D nanowire array was fabricated by repeating catalyst deposition on the targeted special location and nanowire growth from the deposited catalyst.



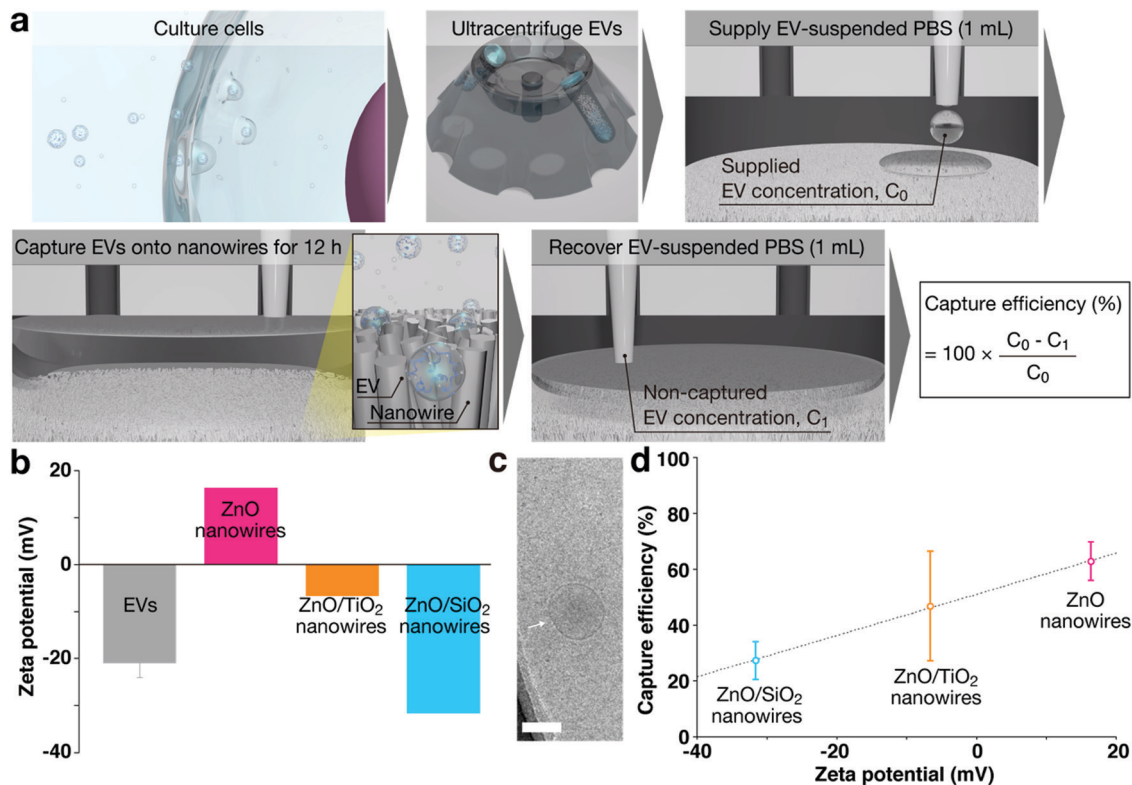


Fig. 8 (a) Schematic showing steps for surface charge-based separation of EVs.⁸⁶ (b) Zeta potentials of the EVs in PBS, and ZnO (bare), ZnO/TiO₂ (core/shell) and ZnO/SiO₂ (core/shell) nanowires in water.⁸⁶ (c) A cryo-TEM image of the EVs; scale bar, 100 nm. The white arrow indicates the EVs.⁸⁶ (d) Capture efficiency of EVs using different material nanowires (pink, ZnO (bare); orange, ZnO/TiO₂ (core/shell); cyan, ZnO/SiO₂ (core/shell)).⁸⁶

the immobilization step, and it provided simple, bio-friendly, and surface-specific functionalization strategies. This peptide-functionalized ZnO nanowire device provided capture and release of EVs under neutral salt conditions with higher efficiency than conventional methods.

3.4. Protein separation using nanowires

As alternatives to electrophoresis-based separation and charge-based separation, strategies based on molecular recognition have received attention as they may target specific molecules, enhancing the specificity and sensitivity of the device. As such, we proposed surface-modified nanowires for biomolecular recognition that would allow the separation of target biomolecules.⁸⁸ In this work, we modified nanowires with thiolated 2-methacryloyloxyethyl phosphorylcholine (MPC-SH) to capture the target protein, by allowing for the reduction of nonspecific absorption. The surface-modified nanowires developed here recognize biomolecules on the surfaces of the nanowires, which can be used in nanowire-embedded biosensors for label-free detection (described in Section 4).

4. Nanowire-based detection

The detection of biomolecules is a critical capability for the effective diagnosis and management of cancers and infectious diseases. Molecular biomarkers are unique disease indicators

that have long been recognized for their effectiveness in providing genetic information from the very early stage until the terminal stage of a disease and in leading a move toward personalized treatment and medicine. Nevertheless, the detection of biomolecules is largely dictated by their characteristics that are rarely present in biological samples. Thus, an essential requirement is a highly sensitive method that can detect low levels of biomolecular analytes. Through the convergence of engineering and life science, the past decades have been witnessing significant progress in advanced biological sensors,^{89–96} in a wide range of areas, including genomics, proteomics, biomedical diagnostics, and drug discovery. The regime of molecular sizes mostly lies in the nanometer scale, necessitating that their detection capability be nanoscale. In this regard, nanowire-based sensors have been long recognized as suitable biosensors due to their comparable dimensions with respect to Debye length and due to their good sensitivity and short response time.

4.1. Fluorescence detection on nanowires

For fluorescence detection, we proposed the idea of *in situ* detection of DNAs and RNAs captured on nanowires. Previous success had led us to further develop a nanowire device integrated with a microheater that was capable of *in situ* heating.⁹⁷ We utilized the device for *in situ* annealing ssDNA to serinol nucleic acid with a molecular beacon (SNA-MB)



Acknowledgements

This review was supported by PRESTO (JPMJPR19H9), Japan Science and Technology Agency (JST), the Strategic International Research Cooperative Program (eASIA, JPMJSC19E3), JST, the JSPS Grant-in-Aid for Scientific Research (B) 21H01960, the JSPS Grant-in-Aid for Scientific Research (S) 18H05243, the JSPS Grant-in-Aid for Exploratory Research 20K21124, and the JSPS Grant-in-Aid for Scientific Research on Innovative Areas "Chemistry for Multimolecular Crowding Biosystems".

References

- R. Mayeux, *NeuroRx*, 2004, **1**, 182–188.
- Y. N. Xia, P. D. Yang, Y. G. Sun, Y. Y. Wu, B. Mayers, B. Gates, Y. D. Yin, F. Kim and Y. Q. Yan, *Adv. Mater.*, 2003, **15**, 353–389.
- A. Zhang and C. M. Lieber, *Chem. Rev.*, 2016, **116**, 215–257.
- J. Hu, T. W. Odom and C. M. Lieber, *Acc. Chem. Res.*, 1999, **32**, 435–445.
- A. M. Morales and C. M. Lieber, *Science*, 1998, **279**, 208–211.
- B. Tian and C. M. Lieber, *Chem. Rev.*, 2019, **119**, 9136–9152.
- G. Zhou, L. Wang, X. Wang, Y. Yu and A. Mutzke, *Vacuum*, 2019, **166**, 88–96.
- Y. Cui, Q. Q. Wei, H. K. Park and C. M. Lieber, *Science*, 2001, **293**, 1289–1292.
- G. F. Zheng, F. Patolsky, Y. Cui, W. U. Wang and C. M. Lieber, *Nat. Biotechnol.*, 2005, **23**, 1294–1301.
- Y.-W. Huang, C.-S. Wu, C.-K. Chuang, S.-T. Pang, T.-M. Pan, Y.-S. Yang and F.-H. Ko, *Anal. Chem.*, 2013, **85**, 7912–7918.
- K. Dawson and A. O'Riordan, *J. Phys.: Conf. Ser.*, 2011, **307**, 012004.
- R. Smith, S. M. Geary and A. K. Salem, *ACS Appl. Nano Mater.*, 2020, **3**, 8522–8536.
- E. Garnett, L. Mai and P. Yang, *Chem. Rev.*, 2019, **119**, 8955–8957.
- S. Rahong, T. Yasui, N. Kaji and Y. Baba, *Lab Chip*, 2016, **16**, 1126–1138.
- H. Zeng, G. Zhang, K. Nagashima, T. Takahashi, T. Hosomi and T. Yanagida, *Chemosensors*, 2021, **9**, 41.
- W. Kim, J. K. Ng, M. E. Kunitake, B. R. Conklin and P. D. Yang, *J. Am. Chem. Soc.*, 2007, **129**, 7228–7229.
- S. Wang, H. Wang, J. Jiao, K. J. Chen, G. E. Owens, K. Kamei, J. Sun, D. J. Sherman, C. P. Behrenbruch, H. Wu and H. R. Tseng, *Angew. Chem., Int. Ed.*, 2009, **48**, 8970–8973.
- D.-J. Kim, J.-K. Seol, M.-R. Lee, J.-H. Hyung, G.-S. Kim, T. Ohgai and S.-K. Lee, *Appl. Phys. Lett.*, 2012, **100**, 163703.
- S. T. Kim, D.-J. Kim, T.-J. Kim, D.-W. Seo, T.-H. Kim, S.-Y. Lee, K. Kim, K.-M. Lee and S.-K. Lee, *Nano Lett.*, 2010, **10**, 2877–2883.
- W. Y. Hong, S. H. Jeon, E. S. Lee and Y. Cho, *Biomaterials*, 2014, **35**, 9573–9580.
- S. Jeon, H. Lee, K. Bae, K. A. Yoon, E. S. Lee and Y. Cho, *Theranostics*, 2016, **6**, 828–836.
- J. Lim, M. Choi, H. Lee, J.-Y. Han and Y. Cho, *Front. Chem.*, 2019, **6**, 664.
- H. Cui, Q. Liu, R. Li, X. Wei, Y. Sun, Z. Wang, L. Zhang, X.-Z. Zhao, B. Hua and S.-S. Guo, *Nanoscale*, 2020, **12**, 1455–1463.
- M. A. Doucey and S. Carrara, *Trends Biotechnol.*, 2019, **37**, 86–99.
- Y. D. Ivanov, T. S. Romanova, K. A. Malsagova, T. O. Pleshakova and A. I. Archakov, *Molecules*, 2021, **26**, 3734.
- H. J. Yoon, M. Kozminsky and S. Nagraath, *ACS Nano*, 2014, **8**, 1995–2017.
- C. Wang, M. Ye, L. Cheng, R. Li, W. Zhu, Z. Shi, C. Fan, J. He, J. Liu and Z. Liu, *Biomaterials*, 2015, **54**, 55–62.
- S.-K. Lee, G.-S. Kim, Y. Wu, D.-J. Kim, Y. Lu, M. Kwak, L. Han, J.-H. Hyung, J.-K. Seol and C. Sander, *Nano Lett.*, 2012, **12**, 2697–2704.
- M. Kwak, L. Han, J. J. Chen and R. Fan, *Small*, 2015, **11**, 5600–5610.
- W. Hong, S. Lee, H. J. Chang, E. S. Lee and Y. Cho, *Biomaterials*, 2016, **106**, 78–86.
- Q. Shen, H. Yang, C. Peng, H. Zhu, J. Mei, S. Huang, B. Chen, J. Liu, W. Wu and S. Cao, *Int. J. Nanomed.*, 2019, **14**, 205.
- H. Lee, M. Choi, J. Lim, M. Jo, J.-Y. Han, T. M. Kim and Y. Cho, *Theranostics*, 2018, **8**, 505.
- R. Niepelt, U. C. Schröder, J. Sommerfeld, I. Slowik, B. Rudolph, R. Möller, B. Seise, A. Csaki, W. Fritzsche and C. Ronning, *Nanoscale Res. Lett.*, 2011, **6**, 1–7.
- W. C. Maki, N. N. Mishra, E. G. Cameron, B. Filanoski, S. K. Rastogi and G. K. Maki, *Biosens. Bioelectron.*, 2008, **23**, 780–787.
- Z. Gao, A. Agarwal, A. D. Trigg, N. Singh, C. Fang, C.-H. Tung, Y. Fan, K. D. Buddharaju and J. Kong, *Anal. Chem.*, 2007, **79**, 3291–3297.
- H. Lee, N. R. Hwang, S.-H. Hwang and Y. Cho, *Biosens. Bioelectron.*, 2016, **86**, 864–870.
- Y. He, S. Su, T. Xu, Y. Zhong, J. A. Zapien, J. Li, C. Fan and S.-T. Lee, *Nano Today*, 2011, **6**, 122–130.
- H. Y. So, K. Lee, N. Murthy and A. P. Pisano, *ACS Appl. Mater. Interfaces*, 2014, **6**, 20693–20699.
- Z. Chen, S.-B. Cheng, P. Cao, Q.-F. Qiu, Y. Chen, M. Xie, Y. Xu and W.-H. Huang, *Biosens. Bioelectron.*, 2018, **122**, 211–216.
- J. Lim, M. Choi, H. Lee, Y.-H. Kim, J.-Y. Han, E. S. Lee and Y. Cho, *J. Nanobiotechnol.*, 2019, **17**, 1–12.
- Z. Nemati, M. R. Zamani Kouhpanji, F. Zhou, R. Das, K. Makielski, J. Um, M.-H. Phan, A. Muela, M. Fdez-Gubieda and R. R. Franklin, *Nanomaterials*, 2020, **10**, 1662.
- Z. Nemati, J. Um, M. R. Zamani Kouhpanji, F. Zhou, T. Gage, D. Shore, K. Makielski, A. Donnelly and J. Alonso, *ACS Appl. Nano Mater.*, 2020, **3**, 2058–2069.
- L. Liu, S. Chen, Z. Xue, Z. Zhang, X. Qiao, Z. Nie, D. Han, J. Wang and T. Wang, *Nat. Commun.*, 2018, **9**, 444.
- Y. Ren, Y. Zou, Y. Liu, X. Zhou, J. Ma, D. Zhao, G. Wei, Y. Ai, S. Xi and Y. Deng, *Nat. Mater.*, 2020, **19**, 203–211.
- E. K. Sackmann, A. L. Fulton and D. J. Beebe, *Nature*, 2014, **507**, 181–189.
- J. C. M. Wan, C. Massie, J. Garcia-Corbacho, F. Mouliere, J. D. Brenton, C. Caldas, S. Pacey, R. Baird and N. Rosenfeld, *Nat. Rev. Cancer*, 2017, **17**, 223–238.
- I. Amelio, R. Bertolo, P. Bove, O. C. Buonomo, E. Candi, M. Chioocchi, C. Cipriani, N. Di Daniele, C. Ganini, H. Juhl, A. Mauriello, C. Marani, J. Marshall, M. Montanaro, G. Palmieri, M. Piacentini, G. Sica, M. Tesaro, V. Rovella, G. Tisone, Y. Shi, Y. Wang and G. Melino, *Cell Death Discovery*, 2020, **6**, 131.
- H. Takahashi, T. Yasui and Y. Baba, *Chem. Lett.*, 2021, **50**, 1244–1253.
- M. Musa, T. Yasui, K. Nagashima, M. Horiuchi, Z. T. Zhu, Q. L. Liu, T. Shimada, A. Arima, T. Yanagida and Y. Baba, *Anal. Methods*, 2021, **13**, 337–344.
- M. Musa, T. Yasui, Z. Zhu, K. Nagashima, M. Ono, Q. Liu, H. Takahashi, T. Shimada, A. Arima, T. Yanagida and Y. Baba, *Anal. Sci.*, 2021, **37**, 1139–1145.
- H. Takahashi, T. Yasui, A. Klamchuen, N. Khemasiri, T. Wuthikhun, P. Paisrisarn, K. Shinjo, Y. Kitano, K. Aoki, A. Natsume, S. Rahong and Y. Baba, *Nanomaterials*, 2021, **11**, 1768.
- A. M. Rusek, M. Abba, A. Eljaszewicz, M. Moniuszko, J. Niklinski and H. Allgayer, *Mol. Cancer*, 2015, **14**, 1–10.
- Z. Qian, Q. Shen, X. Yang, Y. Qiu and W. Zhang, *BioMed Res. Int.*, 2015, **2015**, 649161.
- P. Paisrisarn, T. Yasui and Y. Baba, *Anal. Sci.*, 2020, **36**, 791–798.
- T. Yasui, T. Yanagida, S. Ito, Y. Konakade, D. Takeshita, T. Naganawa, K. Nagashima, T. Shimada, N. Kaji, Y. Nakamura, I. A. Thiodorus, Y. He, S. Rahong, M. Kanai, H. Yukawa, T. Ochiya, T. Kawai and Y. Baba, *Sci. Adv.*, 2017, **3**, e1701133.
- Y. Kitano, K. Aoki, F. Ohka, S. Yamazaki, K. Motomura, K. Tanahashi, M. Hirano, T. Naganawa, M. Iida, Y. Shiraki, T. Nishikawa, H. Shimizu, J. Yamaguchi, S. Maeda, H. Suzuki, T. Wakabayashi, Y. Baba, T. Yasui and A. Natsume, *ACS Appl. Mater. Interfaces*, 2021, **13**, 17316–17329.
- A. Griswold, *Nat. Education*, 2008, **1**, 57.
- P. M. Bennett, *Br. J. Pharmacol.*, 2008, (153 Suppl 1), S347–S357.
- L. Váradi, J. L. Luo, D. E. Hibbs, J. D. Perry, R. J. Anderson, S. Orenge and P. W. Groundwater, *Chem. Soc. Rev.*, 2017, **46**, 4818–4832.
- M. C. Wilson, T. Mori, C. Ruckert, A. R. Uria, M. J. Helf, K. Takada, C. Gernert, U. A. E. Steffens, N. Heycke, S. Schmitt, C. Rinke, E. J. N. Helfrich, A. O. Brachmann, C. Gurgui, T. Wakimoto, M. Kracht, M. Crusemann, U. Hentschel, I. Abe, S. Matsunaga, J. Kalinowski, H. Takeyama and J. Piel, *Nature*, 2014, **506**, 58–62.
- C. Rinke, P. Schwientek, A. Sczyrba, N. N. Ivanova, I. J. Anderson, J. F. Cheng, A. Darling, S. Malfatti, B. K. Swan, E. A. Gies,



