

## PAPER

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# Tetrahedral DNA-directed core-satellite assembly as SERS sensor for mercury ions at the single-particle level†

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To monitor the deteriorating mercury emissions, it is imperative to propose methods for detecting mercury ions ( $\text{Hg}^{2+}$ ) with sensitivity and selectivity. The SERS spectral-resolved single-particle detection approach can be carried out using dark-field optical microscopy (DFM) combined with Raman spectroscopy. Herein, we have designed a novel yet convenient single-particle detection assay for quantifying  $\text{Hg}^{2+}$  using DFM-correlated Raman spectroscopy. In the assay, a tetrahedral DNA-directed core-satellite nanostructure is used as the SERS probe. Especially, one edge of the tetrahedron is made up of a single-stranded DNA containing a  $\text{Hg}^{2+}$  aptamer, which reconfigures upon the specific recognition of  $\text{Hg}^{2+}$ . As a result, the interparticle distance reduces from 4.5 to 1.2 nm, thus generating Raman signal enhancement. As a proof of concept,  $\text{Hg}^{2+}$  was detected in a linear range from 1 to 100 nM based on the variation in SERS intensity. Furthermore, the experimental results were supported by the finite difference time domain (FDTD) calculations. Owing to its high sensitivity and selectivity, this method was further employed to detect  $\text{Hg}^{2+}$  in practical tap water and lake water samples, revealing that the single-particle detection strategy holds great promise for  $\text{Hg}^{2+}$  analysis in real environment analysis.

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## Introduction

Mercury ions ( $\text{Hg}^{2+}$ ) can gradually accumulate in the human body through drinking water and food chains, which cause irreversible damage to the central nervous system, digestive system, kidneys, and other organs.<sup>1,2</sup> The damage caused by mercury is related to the amount of mercury accumulated in the body. Thus, this fact prompted us to look for a sensitive and selective method for  $\text{Hg}^{2+}$  detection. Until now, a series of methods for  $\text{Hg}^{2+}$  measurement have been developed, including fluorescence,<sup>3</sup> electrochemistry,<sup>4</sup> Raman scattering,<sup>5</sup> surface plasma resonance,<sup>6</sup> and colorimetric sensing.<sup>7</sup> Among these methods, surface-enhanced Raman scattering (SERS) is a powerful tool for  $\text{Hg}^{2+}$  detection with sensitivity and efficiency.<sup>8</sup> SERS techniques for  $\text{Hg}^{2+}$  detection are mainly based on indirect SERS since  $\text{Hg}^{2+}$  has no Raman activity,

which usually requires additional Raman reporters. The main assay strategy is tightly associated with the regulation of the “hotspot” structure. Hotspots serve as signal transducers to produce SERS signals. The Raman signal of the hotspot structure changes with the addition of the target molecule. However, it is hard to achieve a well-defined and controllable interparticle distance, which governs the SERS signal of hotspot structures. Besides, during the recognition process of  $\text{Hg}^{2+}$ , the auto-aggregation of nanoparticles is caused by external interferences, such as pH, temperature, and salt concentration, which usually lead to a false positive signal readout. Therefore, there is a need to develop a SERS-based biosensor with high reliability and precision.

Recently, the spectral-resolved single-particle detection strategy has received great attention for its advantageous capability to analyze the target object at the single-particle level by dark-field microscopy (DFM).<sup>9</sup> For example, Xiao and co-workers<sup>10</sup> designed a single-particle detection assay for the quantitative detection of alkaline phosphatase activity in human serum by using a single  $\text{MnO}_2$ -modified gold nanoparticle (AuNP) as the sensor. The SERS spectra of a single plasmonic nanoparticle can be collected by using DFM combined with Raman spectroscopy,<sup>11</sup> which opens up unprecedented opportunities for SERS biosensors in detecting target molecules at the single-particle level.<sup>12</sup> Compared with the

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traditional approaches, single-particle detection employs a single particle to generate an independent signal output, which effectively avoids the ensemble-averaged signal effect and greatly improves sensitivity and specificity.<sup>13</sup>

DNA nanotechnology has emerged as structural and functional building blocks in various plasmonic architectures owing to its excellent molecular recognition controllability and highly controllable length.<sup>14,15</sup> Especially, the tetrahedral DNA structure, with exceptional mechanical rigidity and structural stability, has greatly advanced the accurate fabrication of plasmonic architectures. Tetrahedral DNA-directed assembly is proven to be advantageous for the precise control of interparticle distance.<sup>16,17</sup> More importantly, the shape of the tetrahedron can be changed by the mechanical reconfiguration of the DNA strand at the arm of the tetrahedron using external stimuli.<sup>18</sup> Such reconfigurations may be exploited for the development of plasmonic probes based on the surface plasmon coupling effect. DNA tetrahedron-directed plasmonic architectures have displayed great potential as plasmonic probes in the biosensing field.<sup>19–21</sup>

In this study, we designed a single-particle detection method based on tetrahedral DNA-directed core-satellite assemblies for  $\text{Hg}^{2+}$  detection. The core-satellite nanostructures were composed of satellite AuNPs tethered by tetrahedral DNA structures to a core AuNP. One edge of the tetrahedron consisted of single-stranded DNA containing a  $\text{Hg}^{2+}$  aptamer. The  $\text{Hg}^{2+}$  aptamer folded to form a hairpin structure in the presence of  $\text{Hg}^{2+}$ . As a consequence, the configuration of the tetrahedron changed from a relaxed state to a taut state (Scheme 1), leading to a decrease in the interparticle distance and thus producing Raman signal enhancement. A remarkable magnification in SERS intensity was observed with the increase in  $\text{Hg}^{2+}$  at the single-particle level. The lowest detection limit of  $\text{Hg}^{2+}$  was 0.36 nM. Besides, the finite difference time domain (FDTD) calculation verified the strong linear correlation between the variation in SERS intensity with  $\text{Hg}^{2+}$  concentration. Moreover, this SERS probe showed high specificity. Finally, this SERS probe successfully demonstrated  $\text{Hg}^{2+}$  detection in tap water and lake water. Taking advantage of its excel-

lent sensitivity and specificity, this proposed method can be useful for  $\text{Hg}^{2+}$  analysis in natural water.

### Experimental synthesis of AuNPs

Small satellite AuNPs were prepared by following a published protocol with slight modifications,<sup>22,23</sup> and core AuNPs were synthesized according to a previous report using the seed-growth method.<sup>21</sup> For more details, see ESI.†

### Preparation of the substrate

Briefly, indium tin oxide (ITO) glass slides were selected as the substrates. The surfaces of the substrates were cleaned by using a cleaning agent, acetone, ethanol, and ultrapure water. The substrates were cleaned in each solvent for 0.5 hours. After intense flushing with water, the cleaned substrates were modified with thiol by immersing them in 3-mercaptopropyltriethoxysilane (MPTES) (10:1 v/v) dissolved in anhydrous ethanol and incubating for 3 hours. Finally, the silanized substrates were washed with ethanol to remove excess MPTES.

### Fabrication of core-satellite nanostructures on the substrate

The silanized substrates were immersed in the 100 nm AuNPs solution for 10 min. The AuNP-functionalized substrates were washed with water and dried under nitrogen flow. Subsequently, a 100  $\mu\text{L}$  of tetrahedron-structured DNA solution (1 pM) was dropped onto the surface of the AuNP-modified substrate, followed by incubation in the shaker at room temperature for 3 hours. Then, the excess tetrahedron-structured DNA solution on the surface of the substrate was removed by thorough rinsing with ultrapure water and dried under a nitrogen flow. After that, 100  $\mu\text{L}$  of satellite AuNPs was dropped onto the substrate containing tetrahedral DNA and incubated for 4 h at room temperature with slow shaking. Finally, the core-satellite-nanostructure-decorated ITO substrates were washed with ultrapure water and dried with nitrogen.

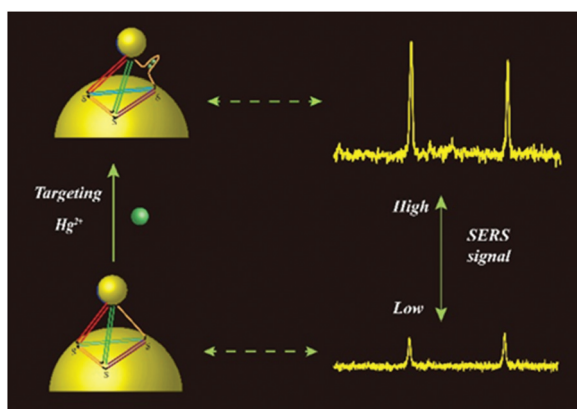
### SERS spectrum of the core-satellite nanostructure and $\text{Hg}^{2+}$ detection

To obtain the SERS scattering spectrum, the core-satellite-nanostructure-functionalized substrates were immobilized on an automatic stage. Then, the target  $\text{Hg}^{2+}$  solution was pipetted on the surface of the substrate. For the detection of  $\text{Hg}^{2+}$ , the SERS spectrum of a single core-satellite nanostructure was collected for 20 seconds before and after adding solutions containing various concentrations of  $\text{Hg}^{2+}$ .

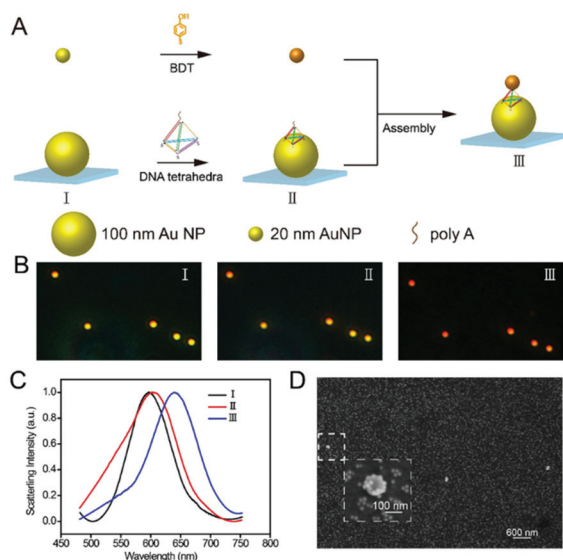
## Results and discussion

### Fabrication and characterization of the DNA-mediated core-satellite nanostructure

The synthesized SERS probes were made of core-satellite nanostructures. The core-satellite nanostructure was fabricated with several 20 nm-sized AuNPs connected by a tetrahedral DNA structure to 100 nm-sized AuNPs, as shown schematically in



**Scheme 1** Schematic of the mechanism of  $\text{Hg}^{2+}$  detection.



**Fig. 1** Fabrication of DNA-mediated core-satellite nanostructures. (A) Synthetic scheme of the core-satellite nanostructure. (B) Typical DFM images and the corresponding scattering spectra (C) of (I) core AuNPs, (II) tetrahedral DNA structure-decorated core AuNPs, and (III) core-satellite nanostructures. (D) Typical SEM image of the core-satellite nanostructures (Inset: the enlarged SEM image).

Fig. 1A. The tetrahedral DNA structure was constructed from a single DNA strand and three thiol-modified single DNA strands (listed in Table S1†). Each thread of the tetrahedral DNA structure contained 26 base pairs. The tetrahedron-structured DNA carried a polyA sequence at one vertex and three thiol groups at the other three vertices. It is worth noting that one edge of the tetrahedron-structured DNA contained a single-stranded DNA that could specifically recognize  $\text{Hg}^{2+}$ . To confirm the successful assembly of the tetrahedron-structured DNA, polyacrylamide gel electrophoresis (PAGE) was performed. As displayed in Fig. S1†, the tetrahedron moved more slowly than both the single-strand DNA and other combinations of two or three DNA strands, demonstrating the successful formation of a tetrahedral DNA structure.<sup>24</sup> To prove that the  $\text{Hg}^{2+}$  aptamer does not hybridize with polyA, PAGE was performed. Tetra 3 and tetra 4 strands contained the  $\text{Hg}^{2+}$  aptamer and polyA, respectively (Table S1†). As expected, in Fig. S1†, there are two bands in column 15. The result proved that tetra 3 could not hybridize with tetra 4, indicating that polyA could not hybridize with the  $\text{Hg}^{2+}$  aptamer. The AuNPs were characterized by transmission electron microscopy (TEM) and extinction spectra. As displayed in their TEM images (Fig. S2B and D†), the acquired 20 nm- and 100 nm-sized AuNPs were both spherical and presented high monodispersity. The as-prepared 20 nm- and 100 nm-sized AuNPs showed the main absorbance peaks at 520 and 568 nm, respectively (Fig. S2A and D†). The core-satellite nanostructure was fabricated by following our protocol previously reported.<sup>21</sup> The tetrahedral DNA structures were immobilized onto the surface of core AuNP *via* the strong gold–thiol bonds, and the residual

polyA section that served as an effective anchoring block was introduced for connecting the 20 nm-sized AuNPs.<sup>25,26</sup>

The self-assembly process was monitored by the DFM images and scattering spectra (Fig. 1B and C). The scattering peak of the individual bare 100 nm-sized AuNPs was found at 560 nm. The corresponding scattered light showed yellow color. When the tetrahedral DNA structure was attached to a 100 nm-sized AuNP, the scattering spectra shifted from 560 to 570 nm. Simultaneously, the color of the scattered spot evolved from yellow to yellow-red due to the change in the reflective index of the gold surface microenvironment.<sup>27</sup> After adding the satellite AuNP solution, the decoration of the satellite AuNPs on the core AuNP led to an extraordinary red-shift in the scattering spectra, accompanied by the variation of the scattering light from yellow-red to red. We attribute this phenomenon to the plasmon coupling effect.<sup>28</sup> Moreover, the successful formation of the core-satellite nanostructure was confirmed by the scanning electron microscopic (SEM) image showing that the surface of the core AuNP was decorated with the satellite AuNPs. (Fig. 1D). Besides, we noted that the satellite AuNPs were also deposited on the ITO glass substrate due to nonspecific adsorption (Fig. 1D). Because of the limit of CCD sensitivity, the image resolution of DFM was limited. The scattered light from AuNPs with a size of at least 40 nm could not be detected by DFM microscopy (Fig. 1B).<sup>29</sup>

With respect to the SERS test, the SERS spectrum of a single particle was recorded by using DFM combined with the Raman spectroscopy setup (Fig. S3†). The results are depicted in Fig. S4†, which shows the DFM image of the core-satellite nanostructure (Fig. S4B†) and the corresponding SERS spectrum (Fig. S4†). A sufficiently intense Raman signal from a single particle could be observed, confirming the single-particle test. The most prominent bands at 1072 and 1583  $\text{cm}^{-1}$  were assigned to the  $\nu_{8a}$  and  $\nu_{12}$  aromatic ring vibrations, respectively.<sup>30</sup> After the optical measurement, we characterized the morphology of individual nanoparticles *via in situ* SEM. The results are displayed in Fig. S4C†, which shows the surface topography of the core-satellite nanostructure and demonstrates that the SERS spectrum was captured from a single particle. Besides, to rule out the influence of small AuNPs nonspecifically adsorbed on the substrates, SERS tests were performed at 10 random blank positions near or far from the scattering light spot, and almost no SERS signal could be obtained (Fig. S5†). This is because the small AuNPs offer a relatively low electromagnetic field within these regions. Therefore, the small AuNPs nonspecifically adsorbed on the substrates would have a negligible effect in the following experiments.

### The principle of $\text{Hg}^{2+}$ detection

For the construction of the SERS sensor, the core-satellite nanostructures used as SERS probes were prepared with several satellite AuNPs connected by the tetrahedral DNA structure to core AuNPs. The sequence for  $\text{Hg}^{2+}$  recognition was designed at one edge of the tetrahedron. According to previous reports, it is well-known that  $\text{Hg}^{2+}$  ions induce the conjunction of the thymine–thymine (T–T) base pair.<sup>31,32</sup> The thorough

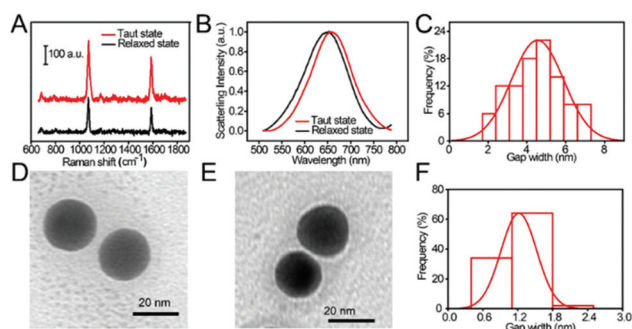
principle for  $\text{Hg}^{2+}$  detection is described in Scheme 1. Upon binding the target  $\text{Hg}^{2+}$ , the  $\text{Hg}^{2+}$  aptamer is converted to a hairpin structure owing to the formation of the T- $\text{Hg}^{2+}$ -T bond, which induces the transformation of the tetrahedra from a relaxed state to a taut state.<sup>18</sup> Consequently, the transformation of the tetrahedra draws the satellite AuNP closer to the core AuNP, producing strong SERS intensity due to the surface plasmon coupling effect. Benefiting from the specific coordination between the  $\text{Hg}^{2+}$  aptamer and  $\text{Hg}^{2+}$  ions, this can be an ideal SERS probe for  $\text{Hg}^{2+}$  detection with high sensitivity and specificity. To verify the working principle of  $\text{Hg}^{2+}$  detection at the single-particle level, the core-satellite nanostructures immobilized on a substrate were exposed to 100 nM  $\text{Hg}^{2+}$  and incubated for 10 min. The variation in the SERS spectra in the absence and presence of  $\text{Hg}^{2+}$  was tested. As shown in Fig. 2A, the SERS intensity enhanced remarkably, illustrating that the detection platform can be used for the qualitative analysis of  $\text{Hg}^{2+}$  based on the SERS spectral changes. The above principle was further verified by using scattering spectra. Upon adding  $\text{Hg}^{2+}$ , the  $\text{Hg}^{2+}$  aptamer combined with  $\text{Hg}^{2+}$  to form a hairpin structure, resulting in a remarkable red-shift of the scattering spectra (Fig. 2B). This result indicated that the addition of  $\text{Hg}^{2+}$  could decrease the interparticle distance, leading to an obvious increase in the plasmon coupling effect. Thus, it can be concluded that the qualitative detection of  $\text{Hg}^{2+}$  is feasible with our proposed principle. To further demonstrate the  $\text{Hg}^{2+}$  stimulus-responsive enhancement in the SERS signal of the SERS sensor,  $\text{I}^-$  ions were used as the inhibitor of the SERS sensor after  $\text{Hg}^{2+}$  ion stimulation. When  $\text{I}^-$  ions are introduced, the complex of  $\text{HgI}_2$  is preferably formed because it is an energetically stabilized product, which would lead to the structural separation of T- $\text{Hg}^{2+}$ -T, recovering to the initial level.<sup>33</sup> Therefore,  $\text{I}^-$  ions can work as the inhibitor for surface recycling. As expected, the SERS signal observably increased on adding 100 nM  $\text{Hg}^{2+}$  ions; comparatively, the intensity of the Raman scattering peaks significantly decreased, with the structure being restored

to its initial state upon the addition of  $\text{I}^-$  ions (Fig. S7†). This result indicates that the changes in the SERS signal were derived in response to the  $\text{Hg}^{2+}$  stimulus.

The TEM images demonstrated the  $\text{Hg}^{2+}$  stimuli-responsive variation in the interparticle distance. However, the core-satellite nanostructures in the TEM images appeared as two-dimensional structures owing to the capillary forces and drying effect during sample preparation. This fact led to difficulty in measuring the interparticle distance from the TEM images.<sup>34,35</sup> To precisely characterize the interparticle distance, a dimer of two 20 nm-sized AuNPs was synthesized by using the same tetrahedral DNA structure to replace the core-satellite nanostructure. Because the two AuNPs of the dimer were located on the same plane of the TEM grid during sample preparation, the spacing between the dimers should be close to the real situation in the experiment. The interparticle distance between the dimer in the absence and presence of excess  $\text{Hg}^{2+}$  was characterized by TEM (Fig. 2D and E). Statistical analysis showed that the average distance between the dimers decreased from 4.5 to 1.2 nm upon exposure to the  $\text{Hg}^{2+}$  solution (Fig. 2C and F). Additionally, in the presence of excess  $\text{Hg}^{2+}$ , the intensity of the Raman scattering peaks significantly increased (Fig. S8†). This result is in good agreement with the foregoing SERS spectra in Fig. 2A.

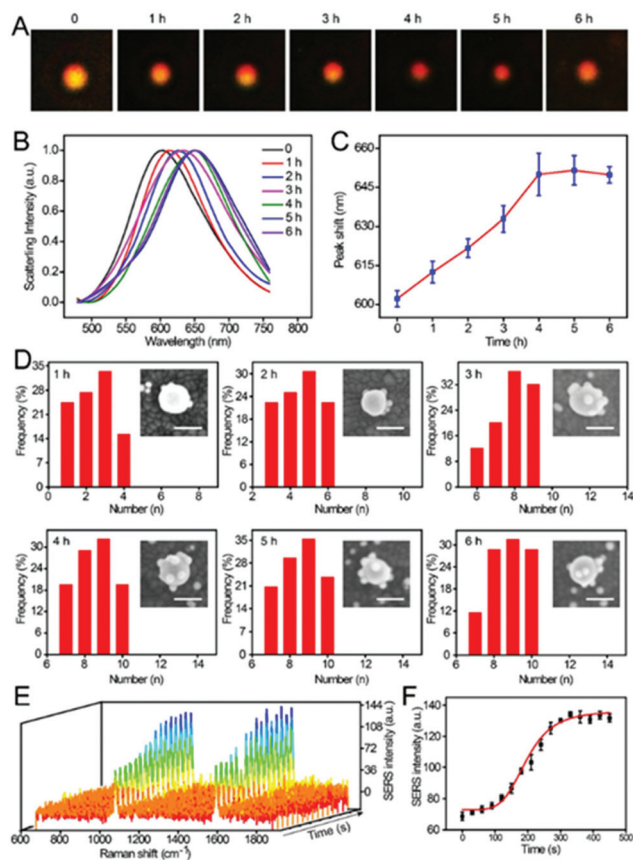
### Optimization of conditions

To achieve the best detection effect, we investigated the optimized conditions, such as the number of satellite AuNPs around the core AuNP and reaction time. Firstly, the effect of the satellite AuNPs number on the core AuNP was investigated. The number of satellite AuNPs attached to the core AuNP surface was controlled by tuning the immersion time in the satellite AuNP solution. As we all know, the localized surface plasmon resonance (LSPR) property heavily depends on the number of satellite AuNPs per core AuNP.<sup>31</sup> Therefore, the DFM and scattering spectra techniques were applied to monitor the assembly process. As the immersion time increased, the color of the scattering spot gradually changed from yellow-red to red under the dark-field microscope (Fig. 3A). Simultaneously, the scattering peak increased gradually along with the increase in immersion time (Fig. 3B and C). This result is mainly due to the strong plasmon coupling effect. The red-shift of scattering spectral peak achieved the max value and then remained constant after 4 h, implying that the surface coverage reached saturation. To understand the assembly process in-depth, the surface coverage of the core AuNP was characterized by using SEM at different time points. The typical SEM images of a single isolated core-satellite nanostructure at different immersion times were observed (Fig. 3D, inset). Moreover, a statistical analysis of the satellite AuNP number was performed. As the immersion time increased, an increasing number of satellite AuNPs were adsorbed to the surface of the core AuNPs (Fig. 3D). When the immersion time was more than 4 h, the surface coverage of the core AuNP had reached saturation. This result is in excellent agreement with the behavior observed in the scattering spectra. When the



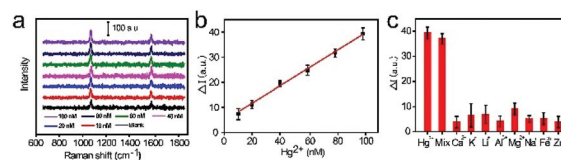
**Fig. 2** Detection mechanism. (A) Raman spectra and (B) the corresponding scattering spectra of the individual core-satellite assembly in the absence and presence of 100 nM  $\text{Hg}^{2+}$ . Typical TEM image of the isolated gold dimer (D) before and (E) after treatment with excess  $\text{Hg}^{2+}$ . Statistical analysis of gap width in the (C) absence and (F) presence of excess  $\text{Hg}^{2+}$ .





**Fig. 3** Optimization of the assay conditions. (A) DFM images and (B) scattering spectra of the core-satellite nanostructures at various incubation times. (C) Plot of the SPR wavelength shift with incubation time. (D) Statistical distribution of the satellite AuNP number attached per core AuNP. Inset: typical SEM images of the core-satellite nanostructures treated for various immersion times (scale bars, 100 nm). (E) Time-resolved Raman spectra of an individual core-satellite assembly in the presence of 100 nM  $\text{Hg}^{2+}$ . (F) Time-resolved SERS intensity of a single core-satellite nanostructure exposed to 100 nM  $\text{Hg}^{2+}$ .

incubation time exceeded 4 h, the number of satellite AuNPs remained almost constant. In contrast, more satellite AuNPs were nonspecifically adsorbed on the surface of the substrate, making it difficult to distinguish the scattering light spot of the individual particles in the DFM image. Therefore, 4 h was considered the optimum immersion time for the surface coverage to reach saturation. Subsequently, the influence of reaction time was also studied. Reaction time is a critical factor influencing the affinity between  $\text{Hg}^{2+}$  and the  $\text{Hg}^{2+}$  aptamer, which determines the analytical performance. To monitor this reaction in real-time, the time-dependent SERS spectra of a single core-satellite assembly were recorded over 10 min at a certain time interval upon treatment with 100 nM  $\text{Hg}^{2+}$  (Fig. 3E and F). With the increase in reaction time, the Raman intensity ascended. The reaction achieved equilibrium in 5 min, showing the maximum intensity. To ensure the accuracy of data, 7 min was taken as the optimal reaction time.

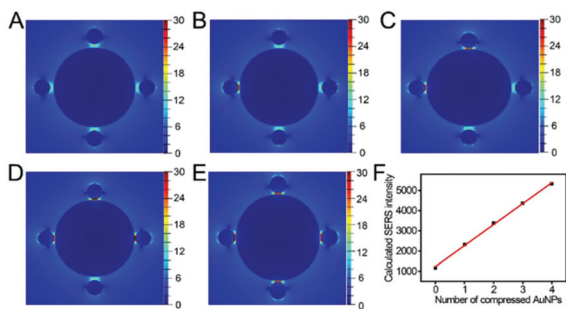


**Fig. 4** Detection of  $\text{Hg}^{2+}$ . (A) The  $\text{Hg}^{2+}$  concentration-dependent SERS spectra ranging from 100 to 1 nM and the blank control. (B) The linear relationship between the variation in the SERS intensity of 4-MBA at 1072  $\text{cm}^{-1}$  and  $\text{Hg}^{2+}$  concentration. (C) Selectivity of the method for  $\text{Hg}^{2+}$ .

### Detection of $\text{Hg}^{2+}$

Under the optimized conditions, the sensitivity of this sensor was evaluated based on SERS signals after introducing different concentrations of  $\text{Hg}^{2+}$  (1 to 100 nM). Fig. 4A presents the representative SERS spectra under different  $\text{Hg}^{2+}$  concentrations. According to the literature,<sup>21</sup> the Raman scattering peak at 1583  $\text{cm}^{-1}$ , which belongs to the aromatic ring breathing mode, suffers from relevant interference due to the attachment of  $\text{Hg}^{2+}$  to the carboxyl group of 4-mercaptobenzoic acid (4-MBA). The reason might be the redistribution of charges between the ring breathing vibrational band upon the adsorption of  $\text{Hg}^{2+}$  on the carboxyl group of 4-MBA.<sup>36,37</sup> On the contrary, the Raman scattering peak at 1073  $\text{cm}^{-1}$  exhibited no frequency shift, indicating that it did not suffer from any interference upon the coordination of  $\text{Hg}^{2+}$  to the carboxyl group. Therefore, for the accuracy of quantitative  $\text{Hg}^{2+}$  detection, the characteristic SERS peak of 4-MBA at 1072  $\text{cm}^{-1}$  was employed. To demonstrate the stability of the SERS probe for  $\text{Hg}^{2+}$  detection at the single-particle level, lots of SERS spectral experiments were repeated at the same  $\text{Hg}^{2+}$  concentration for statistical analyses. The thirty SERS intensity variations at 1072  $\text{cm}^{-1}$  ( $\Delta I$ ) were distributed as a Gaussian curve (Fig. S9†). The SERS intensity increased linearly with the  $\text{Hg}^{2+}$  concentration in the range of 10 to 100 nM. Moreover, the linear regression equation ( $\Delta I = 0.3494C(\text{Hg}^{2+}) + 4.4314$ ) for  $\text{Hg}^{2+}$  detection was obtained for the SERS signals at 1072  $\text{cm}^{-1}$  (Fig. 4B). The corresponding correlation  $R^2$  was 0.9953. The detection limit (LOD) for  $\text{Hg}^{2+}$  was 0.36 nM at a signal-to-noise ratio of 3. The lowest concentration for quantitative detection of  $\text{Hg}^{2+}$  by this method corresponded to 1 nM, which is lower than the allowable maximum residue limit of  $\text{Hg}^{2+}$  (10 nM) in drinkable water as per the United States Environmental Protection Agency (USEPA).<sup>33,38</sup> Compared with the previously reported methods for  $\text{Hg}^{2+}$  measurement,<sup>39–43</sup> the proposed strategy for  $\text{Hg}^{2+}$  shows much higher detection sensitivity (Table S2†).

To further demonstrate the sensing mechanism based on the SERS intensity variation with the concentration of  $\text{Hg}^{2+}$ , FDTD simulation was carried out to investigate the variation in the electromagnetic intensity of the core-satellite nanostructures during the compression of the particles. The SERS intensity was dominated by the enhancement in the local electromagnetic field, which is directly proportional to the second power of the electromagnetic field. Five structural models with



**Fig. 5** FDTD simulations of the core-satellite nanostructure as a function of the increasing number of satellites. (A–E) The local electric field distribution of core AuNPs assembled with different numbers of compressed satellite AuNPs: 0–4, respectively. The labels 0–4 correspond to the number of compressed satellite AuNPs. (F) The linear range between the calculated SERS intensity and the compressed satellite AuNP number.

a core AuNP of size 100 nm and four satellite AuNPs of size 20 nm were used in the simulation (Fig. S6†). The interparticle distance between the core AuNP and the satellite AuNPs varied from 4.5 to 1.2 nm. For simplicity, the contributions of the DNA strands, 4-MBA and glass slides were ignored.<sup>44</sup> Fig. 5A–E vividly displays the electric-field distribution of the different models with four satellite AuNPs distributed around the surface of a core AuNP. The electromagnetic enhancement is highly localized in the gap regions. The intensity of the electromagnetic field in the gap is enhanced as the interparticle distance between the satellite and core AuNP decreases from 4.5 to 1.2 nm. As shown in Fig. 5F, with the increase in the compressed satellite AuNP number, a linear rise in SERS intensity happens. These calculated results are in accordance with the experimental results, which demonstrate that the increase in SERS intensity observed in our experiments is due to the increase in the compressed satellite AuNP number.

To prove the selectivity of detection by this SERS biosensor, several similar metal ions, such as  $\text{Hg}^{2+}$ ,  $\text{Ca}^{2+}$ ,  $\text{K}^+$ ,  $\text{Li}^+$ ,  $\text{Al}^{3+}$ ,  $\text{Mg}^{2+}$ ,  $\text{Na}^+$ ,  $\text{Fe}^{3+}$ ,  $\text{Zn}^{2+}$  and the mixture containing all the above metal ions, were further employed under optimized conditions. The SERS signal of the individual core-satellite assembly in solutions containing 100 nM  $\text{Hg}^{2+}$  and 100-fold other metal ions, respectively, are described in Fig. 4C. The SERS intensity remained unchanged after treatment with the other metal ions except for  $\text{Hg}^{2+}$  and the mixture of metal ions. The high selectivity of this detection is due to the specific coordination between the  $\text{Hg}^{2+}$  aptamer and  $\text{Hg}^{2+}$  ions. This comparison demonstrated that the proposed SERS sensor possesses excellent selectivity, making it suitable for working in a complex ecological system.

To prove the ability of the method in the measurement of  $\text{Hg}^{2+}$  ions in practical applications, tap water and lake water collected from our laboratory and a lake in our university were tested. Before analysis, samples with three different  $\text{Hg}^{2+}$  concentrations (10, 50 and 100 nM) were prepared with diluted tap water and lake water. Fig. S10† depicts the SERS spectra of

**Table 1** Determination for  $\text{Hg}^{2+}$  in tap water and lake water

Water sample	Spilled $\text{Hg}^{2+}$ (nM)	Measured $\text{Hg}^{2+}$ (nM)	RSD (%)
Tap water	10	9.59	1.82
	50	49.8	2.01
	100	101.6	1.68
Lake water	10	10.9	1.29
	50	48.1	2.07
	100	102.3	1.84

the  $\text{Hg}^{2+}$  detection in tap water and lake water. To prove the accuracy and reliability of this method, the spiked recovery was calculated and is summarized in Table 1. It was found that the relative standard deviation (RSD) ranged from 1.29% to 2.07%. We attribute this to the favorable affinity of the  $\text{Hg}^{2+}$  aptamer and  $\text{Hg}^{2+}$ . The results indicate that our SERS sensor can be used for detecting  $\text{Hg}^{2+}$  ions in complex biological samples.

## Conclusions

In summary, we designed a novel single-particle detection assay for the sensitive and selective quantitative analysis of  $\text{Hg}^{2+}$  by using DFM-correlated Raman spectroscopy. After the addition of  $\text{Hg}^{2+}$ , the  $\text{Hg}^{2+}$  aptamer folded up and formed a hairpin structure, which led to a variation in the tetrahedral DNA configuration. Consequently, the interparticle distance reduced from 4.5 to 1.2 nm, which tremendously increased the SERS signal. Based on this principle, a detection range from 1 to 100 nM, with a low LOD of 0.36 nM, was obtained. Furthermore, the FDTD simulation results revealed that the variation in SERS intensity had a linear response to the concentration of  $\text{Hg}^{2+}$ . In addition, the proposed  $\text{Hg}^{2+}$  detection process presented highly favorable specificity in the presence of a series of similar metal ions. Thus, the SERS probe was applied for the detection of  $\text{Hg}^{2+}$  ions in real water samples. The proposed SERS probe exhibits great potential in  $\text{Hg}^{2+}$  detection in real water samples.

## Author contributions

N. Feng performed all the experiments. N. Feng, J. J. Shen, C. Li, Q. Q. Zhao, E. K. Fodjo, L. Zhang, S. F. Chen, Q. L. Fan and L. H. Wang analyzed the data. N. Feng, L. Zhang, and L. H. Wang wrote the manuscript.

## Conflicts of interest

There are no conflicts to declare.

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