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# Spike trains in PANI-proteinoid nanomaterials with different light pulse rates

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Bio-inspired computing emulates the brain's information processing power in artificial architectures. We investigate the modification of emergent spike train dynamics in hybrid networks of polyaniline (PANI) nanomaterials hybridised with proteinoids under different optical stimulation frequencies. Hierarchical clustering of photoelectrochemical response data categorises activity patterns for 1 Hz, 5 Hz, and 20 Hz pulsed yellow light inputs. Importantly, the driving frequency controls nanofiber excitability and temporal coordination, with 1 Hz causing erratic spike bursts, 5 Hz rhythmic oscillations, and 20 Hz fast but unsustained responses. Raster plots and peristimulus time histograms show a development from stochastic to deterministic to complicated nonlinear dynamics like neuromorphic systems. Modelling the network as a forest-fire automaton quantifies spatiotemporal activity propagation, where illumination frequency modulates node ignition and recovery probability, shaping spike clusters and coherence. Photonic stimulation can modify information encoding regimes in these PANI-proteinoid composites, suggesting they can be synthetic neural networks. Our findings provide insights for constructing adaptive, brain-inspired computer systems by showing extrinsic control over the network's self-organized dynamics. The ability to delicately tune nanofiber excitation–relaxation cycles using optical pulse trains creates a prototype for biophysically-motivated perception, learning, and cognitive models in empirically accessible material frameworks.

## 1. Introduction

The remarkable ability of the human brain to process and adapt to complex, dynamic environment has led to the development of neuromorphic systems that try to replicate its computational principles.<sup>1,2</sup> Tanaka (2019)<sup>3</sup> and Kendall (2020)<sup>4</sup> propose brain-inspired techniques that overcome the limits of standard von Neumann designs by using the intrinsic dynamics and self-organisation of physical substrates. Conducting polymer nanomaterials based on polyaniline (PANI) are a potential material for realising neuromorphic capacities.<sup>5</sup>

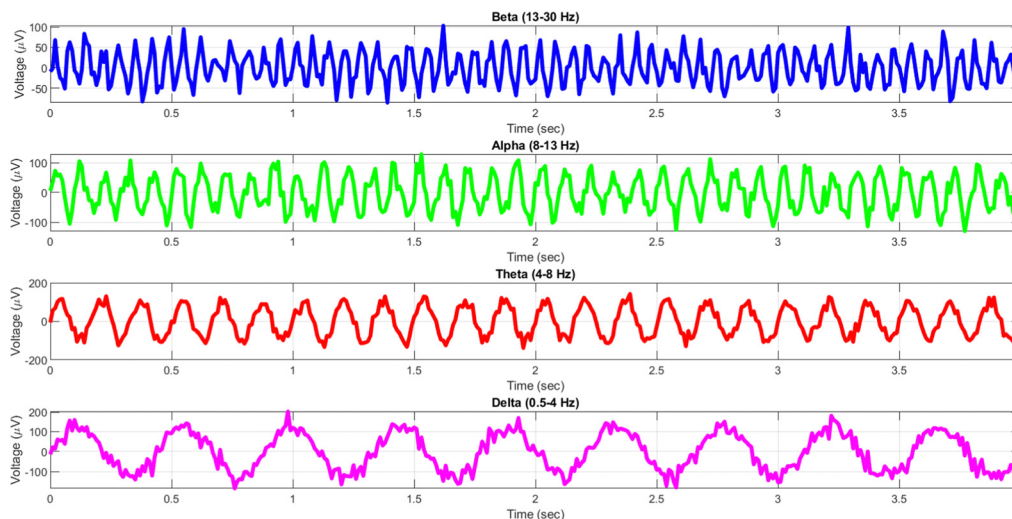
PANI nanomaterials have attracted interest due to their distinctive electrical and optical properties, which originate from their conjugated backbone and redox-active nature.<sup>6,7</sup> PANI nanomaterials enhance biocompatibility and self-assembly when coupled with biomolecules such as proteins or peptides.<sup>8–10</sup> Polyaniline (PANI) is a promising material for biosensing applications because of its distinctive characteristics, including high conductivity, biocompatibility, and ease of synthesis. Karimi and colleagues<sup>11</sup> developed a selective biosensor for detecting human cardiac troponin T (cTnT) by integrating molecularly imprinted polyaniline (MIP) with

reduced graphene oxide (rGO). In another study, Asmatulu and colleagues<sup>12</sup> developed an electrochemical nanobiosensor to detect cyclooxygenase-2 (COX-2) in human serum samples and phosphate-buffered saline (PBS) by using polyaniline nanomaterials. COX-2 is an enzyme that is essential in the process of inflammation and is frequently linked to different diseases, such as cancer. The biosensor was created by altering the electrode's surface with polyaniline nanomaterials, enhancing its surface area and conductivity to facilitate electron transport effectively.

Polyaniline (PANI) is used in tissue engineering and regenerative medicine, in addition to biosensing. An example of this is when developing conductive biomaterials to improve nerve regeneration. In the human body, barriers and cell membranes establish ionic barriers leading to the appearance of an electrical potential gradient across their surface. This gradient promotes nerve growth towards the outer regions, which is crucial for the normal functioning of the nervous system. Researchers have investigated the use of conductive biomaterials like polypyrrole (PPy) and polyaniline (PANI) to promote neurite extension with minimal electrical stimulation.<sup>13</sup> By integrating PANI into scaffolds or substrates, researchers have shown enhanced neurite outgrowth and alignment, which could lead to more efficient nerve regeneration techniques.<sup>14</sup>

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**Fig. 1** Examples of EEG rhythms and their corresponding frequency ranges. The subplots display simulated EEG waveforms for several frequency bands: (A) beta waves (13–30 Hz) exhibiting heightened randomness, (B) alpha waves (8–13 Hz) exhibiting heightened randomness, (C) theta waves (4–8 Hz), and (D) delta waves (0.5–4 Hz). The waveforms are produced using sinusoidal functions that have frequencies corresponding to each band. Additionally, random noise is used to mimic the variability exhibited in actual EEG recordings. The time range covers a period of 0 to 4 seconds, while the voltage range ranges from 0 to 200  $\mu\text{V}$ , representing normal amplitudes of EEG signals.

Unconventional computing applications of polyaniline (PANI) are substantially evidenced in prototypes of organic electronic materials<sup>15</sup> and functioning processors,<sup>16,17</sup> include perceptron,<sup>18,19</sup> memristors,<sup>20</sup> neuromorphic circuits.<sup>21–23</sup> These materials are attractive for future cybernetic systems because they are highly parallel processing devices with fault-tolerance and self-healing. Anisotropic colloidal suspensions of conductive polymer nanorods, especially PANI nanorods (NRs), are attractive for computer subsystems in these applications because they respond well to electrical fields. Recent research has investigated designing learning processes in PANI NR colloids for future cybernetic systems.<sup>24</sup> AC electrical stimulation can create programmed conductive paths to different states for learning. Due to AC field effects on hydrogen bonds stabilising dispersions in the fluid and charge orientation in polymeric chains, colloid resistance anisotropy can be repetitive coded in binary logic. Modifying PANI NRs' molecular structure changes their conductivity.<sup>24</sup>

Proteinoids, also known as thermal proteins, play a crucial role in the formation of complex structures in PANI-proteinoid nanomaterials. These proteinoids are synthesized through a simple thermal condensation reaction, where amino acids are heated to their melting point (160–200 °C) in an inert atmosphere, initiating polymerization and creating polymeric chains.<sup>25,26</sup> The resulting proteinoids can form hollow microspheres when swollen in an aqueous solution at moderate temperatures (around 50 °C).<sup>26</sup> These proteinoid microspheres exhibit electrical properties reminiscent of biological neurons, such as steady-state membrane potentials, oscillations, and action potentials.<sup>27,28</sup>

The integration of proteinoids with polyaniline (PANI) nanomaterials introduces a new level of complexity and functionality to the system. The proteinoid microspheres can act as

interconnected nodes within the PANI nanofiber network, facilitating the emergence of complex electrical dynamics and signal propagation. By harnessing the unique properties of proteinoids, such as their programmable size, stability, and long-lasting oscillatory behaviour,<sup>26,29,30</sup> PANI-proteinoid nanomaterials offer a promising platform for developing bio-inspired neuromorphic systems capable of processing and transmitting information in a manner analogous to biological neural networks.

The human brain displays a diverse array of rhythmic activity, commonly known as “brain waves,” that may be recorded using electroencephalography (EEG) recordings. These waves are a result of the coordination of several neurons and are linked to different functioning states of the brain.<sup>31</sup> Fig. 1 demonstrates that EEG rhythms cover many frequency ranges, such as delta (0.5–4 Hz), theta (4–8 Hz), alpha (8–13 Hz), beta (13–30 Hz), and gamma (30–100 Hz) waves.<sup>32</sup> Each frequency range has been associated with distinct cognitive functions, including as relaxation, drowsiness, attentiveness, and short-term memory.<sup>33</sup>

Remarkably, the spiking dynamics observed in PANI-proteinoid nanomaterials exhibit similarities to the oscillatory patterns reported in the brain. By varying the frequency of the optical pulses that are used to activate the nanomaterials, we can precisely control the patterns of electrical impulses created by these neuromorphic materials. The capacity to adjust the spiking behaviour of PANI-proteinoid nanomaterials presents intriguing prospects for simulating brain-like information processing and creating innovative neuromorphic computing platforms.<sup>34</sup>

In this paper, we investigate how different optical pulse frequencies affect the spiking dynamics of PANI-proteinoid nanomaterials. We show that specific temporal patterns of



light stimulation can entrain and control the electrical activity of these nanomaterials. Our findings demonstrate the potential of optically-stimulated PANI-proteinoid nanomaterials as programmable, neuromorphic components for brain-inspired computing. The capacity to alter spike trains with light opens up new opportunities in adaptive sensing, bioelectronic interfaces, and neuromorphic robotics. Furthermore, our findings contribute to a better understanding of emergent dynamics in complex, nanoscale systems, as well as its application to biological information processing.

The remaining part of the paper is structured as follows: Section 2 goes over the fabrication and characterization of PANI-proteinoid nanomaterials, as well as the experimental setup for optical stimulation. Section 3 summarises the findings of our experiments, emphasising the frequency-dependent regulation of spiking activity. In Section 4, we analyse the implications of our findings and present a theoretical model to explain the observed behaviours. Finally, Section 5 summarises the article and discusses future research directions.

## 2. Methods and materials

### 2.1. Materials

Sigma Aldrich supplied aniline ( $d = 1.022 \text{ g mol}^{-1}$ ,  $M = 93.13 \text{ g mol}^{-1}$ , CAS-No: 62-53-3, ACS reagent >99.5%), *p*-toluenesulfonic acid monohydrate (CAS-No 6192-52-5, ACS reagent >98.5%), and ammonium persulfate ( $d = 1.980 \text{ g cm}^{-3}$ ,  $M = 228.20 \text{ g mol}^{-1}$ , CAS: 7727-54-0, ACS reagent >98.0%). Merck KGaA supplied  $1 \text{ mol l}^{-1}$  of hydrochloric acid at 1 N. All compounds were utilised as obtained, without further purification. L-Phenylalanine, L-aspartic acid, and L-glutamic acid were purchased from Sigma Aldrich with a purity level exceeding 98%. These amino acids were used as the building blocks for the synthesis of proteinoids. 1-Methyl-2-pyrrolidinone, with a purity greater than 98%, was purchased from Sigma-Aldrich.

### 2.2. Synthesis of PANI nanotubes-nanospheres

PANI nanotubes-nanospheres have been made using the chemical oxidative polymerization of aniline using ammonium persulfate as the oxidant and *p*-toluenesulfonic acid monohydrate as the dopant. A standard procedure involved combining 5 ml of aniline with ammonium persulfate and *p*-toluenesulfonic acid monohydrate in a molar ratio of 1:1:0.5. The solution was agitated at ambient temperature for a duration of 60 minutes to ensure full dissolution and homogeneity. After stirring, the mixture was stored at  $-8^\circ\text{C}$  for three days to allow the polymerization reaction to proceed slowly and facilitate the formation of nanotubes and nanospheres. The low temperature helps to control the growth rate and morphology of the PANI nanostructures. After the polymerization process, the resulting dark green solid was obtained by filtering and then subjected to multiple washing with deionized water and ethanol to remove any remaining unreacted monomers and contaminants. The PANI nanotubes-nanospheres were subsequently subjected to a drying process in a vacuum oven at a temperature of  $30^\circ\text{C}$  for a duration of 24 hours.

### 2.3. Synthesis of proteinoids microspheres

Proteinoids were synthesized following the thermal polycondensation approach developed by Mougkogiannis *et al.*<sup>35</sup> The synthesis procedure involved the following steps:

- (1) A mixture consisting of 5 gr of L-phenylalanine, L-aspartic acid, and L-glutamic acid was prepared.
- (2) The amino acid mixtures were placed in a reaction vessel (100 ml) and subjected to heating at  $180^\circ\text{C}$  under reflux.
- (3) The thermal polycondensation reaction was allowed to proceed for 180 minutes.
- (4) The obtained proteinoids were then added to an aqueous solution and stirred for three hours at 80 degrees celsius.
- (5) The proteinoids were then lyophilized (freeze-dried) to remove any residual moisture and obtain a dry powder.
- (6) The lyophilized proteinoids were stored at room temperature for further characterization and use.

### 2.4. Synthesis of PANI-proteinoid suspension

In order to prepare the PANI-proteinoid suspension, the PANI that was synthesised was initially dissolved in 1-methyl-2-pyrrolidinone (NMP) to form a solution with a concentration of  $1 \text{ mg l}^{-1}$ . The selection of NMP as the solvent was based on its capacity to efficiently dissolve PANI and its compatibility with the proteinoid solution. The lyophilized proteinoids were dissolved in deionized water in a separate container, resulting in the formation of a proteinoid-water solution. The proteinoid solution's concentration was modified according to the required ratio of PANI to proteinoids in the resulting suspension. Subsequently, the PANI-NMP solution was gradually added into the proteinoid-water solution while maintaining a constant stirring rate. The mixing took place at ambient temperature to ensure a uniform dispersion of PANI throughout the proteinoid solution.

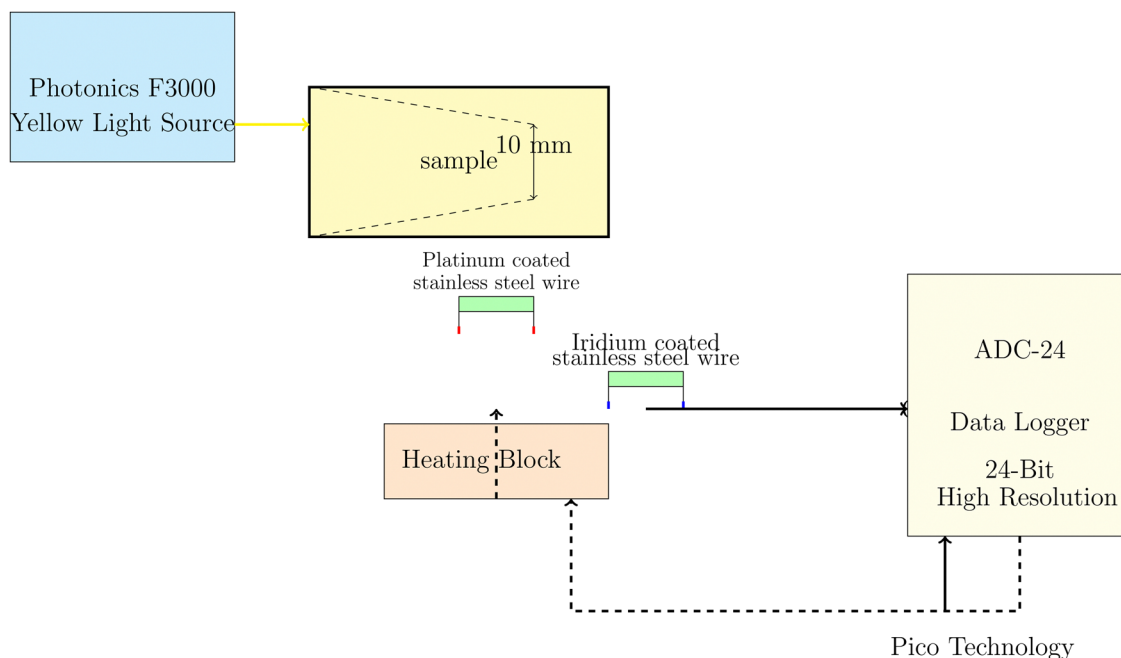
### 2.5. Characterisation techniques

The scanning electron microscopy (SEM) and Fourier-transform infrared spectroscopy (FT-IR) techniques were used to analyse the morphological and structural characteristics of the PANI nanotubes-nanospheres that were synthesised.

**2.5.1. Scanning electron microscopy (SEM).** We used a Quanta 650 microscope to image PANI nanotube-nanosphere morphology. A sputter coater encapsulated the samples with a small layer of gold before imaging to improve conductivity and imaging quality. Images from the SEM at various magnifications showed nanostructure morphology and surface characteristics.

**2.5.2. Fourier-transform infrared spectroscopy (FT-IR).** The chemical structure and functional groups of the PANI nanotubes-nanospheres were analysed using FT-IR spectroscopy. The FT-IR spectra were obtained using a Nicolet iS 5 FTIR Spectrometer (Thermo Scientific) within the wavenumber range of  $400$  to  $4000 \text{ cm}^{-1}$ , with a resolution of  $4 \text{ cm}^{-1}$ . The FT-IR spectra were analysed using the Omnic programme (OMNIC Series programme, Thermo Scientific) to determine the absorption bands that correspond to the functional groups and





**Fig. 2** Diagram illustrating the setup for electrochemical measurements of PANI-proteinoid samples under yellow light illumination. The Photonics F3000 system generates the yellow light source, which is directed onto the sample. Needle electrodes made from platinum-iridium coated stainless steel wires were placed 10 mm apart in the PANI-proteinoid composite to map spatiotemporal voltage responses. Signals were obtained using a high-precision 24-bit ADC data logger that was synchronized with a heating block for monitoring thermal and electrical parameters simultaneously. The system has high sensitivity to detect small voltage fluctuations in the  $\mu\text{V}$  range.

chemical bonds found in the PANI nanostructures. The detailed FT-IR spectra, peak assignments, and comparative analysis of PANI synthesized using different oxidizing agents (ammonium persulfate and ferrous nitrate) are provided in the appendix (Fig. 20a and b). The appendix includes the graphical representation of the FT-IR spectra, along with the peak lists and their corresponding intensities (Tables 5–7).

## 2.6. Electrical measurements

The electrochemical measurements of PANI-proteinoid samples under visible light illumination were performed using a Photonics F3000 system that had LED light sources from World Precision Instruments (Fig. 2). The specimens were subjected to yellow light with a wavelength of 590 nm, specifically identified as Part No: 593-30-003. The LEDs produce light with narrow band spectra, which have bandwidths that vary between 25 and 35 nm. The light intensity was varied from 20% to 100% of the maximum power density, which was fixed at  $30 \text{ mW cm}^{-2}$  for the unfiltered daylight LED. The choice of yellow light as the stimulation source for the PANI-proteinoid nanomaterials was based on several factors. Firstly, polyaniline (PANI) exhibits a strong absorbance peak in the yellow-green region of the visible spectrum, typically around 550–600 nm.<sup>36–38</sup> This absorption peak is attributed to the  $\pi\text{--}\pi^*$  transition of the quinoid rings in the emeraldine salt form of PANI.<sup>39</sup> By selecting yellow light, which falls within this absorption range, we aimed to maximize the optical response of PANI in the composite material. Furthermore, previous studies have demonstrated that PANI-based materials exhibit significant photoconductivity and

electrical responsiveness when exposed to yellow light.<sup>38,40</sup> The increased conductivity and charge carrier generation in PANI upon yellow light illumination have been attributed to the photoinduced electron transfer from the highest occupied molecular orbital (HOMO) to the lowest unoccupied molecular orbital (LUMO) of the polymer.<sup>40</sup> While PANI can respond to other wavelengths in the visible spectrum, such as blue and green light, the response is generally less pronounced compared to yellow light.<sup>37</sup> This is due to the lower absorption coefficients of PANI at shorter wavelengths and the less efficient photoinduced charge separation processes.<sup>38</sup>

The Photonics F3000 system was used to produce a yellow light source with a wavelength of 590 nm, as shown in Fig. 2. This light source was used to illuminate the PANI-proteinoid samples. Light was focused onto the sample, and needle electrodes composed of platinum-iridium coated stainless steel wires were positioned 10 mm apart within the PANI-proteinoid composite to record the voltage responses in space and time. The electrodes were linked to a high-precision 24-bit ADC data logger (Pico Technology) to capture the signals. The data logger was synchronised with a heating block to facilitate concurrent monitoring of thermal and electrical parameters. The system demonstrated a remarkable level of sensitivity, enabling it to detect even the smallest changes in voltage within the microvolt range.

The measurements yield significant information on the photosensitivity and optoelectronic characteristics of PANI-proteinoid composites. The capacity to regulate the electrical characteristics of these substances by means of precise light





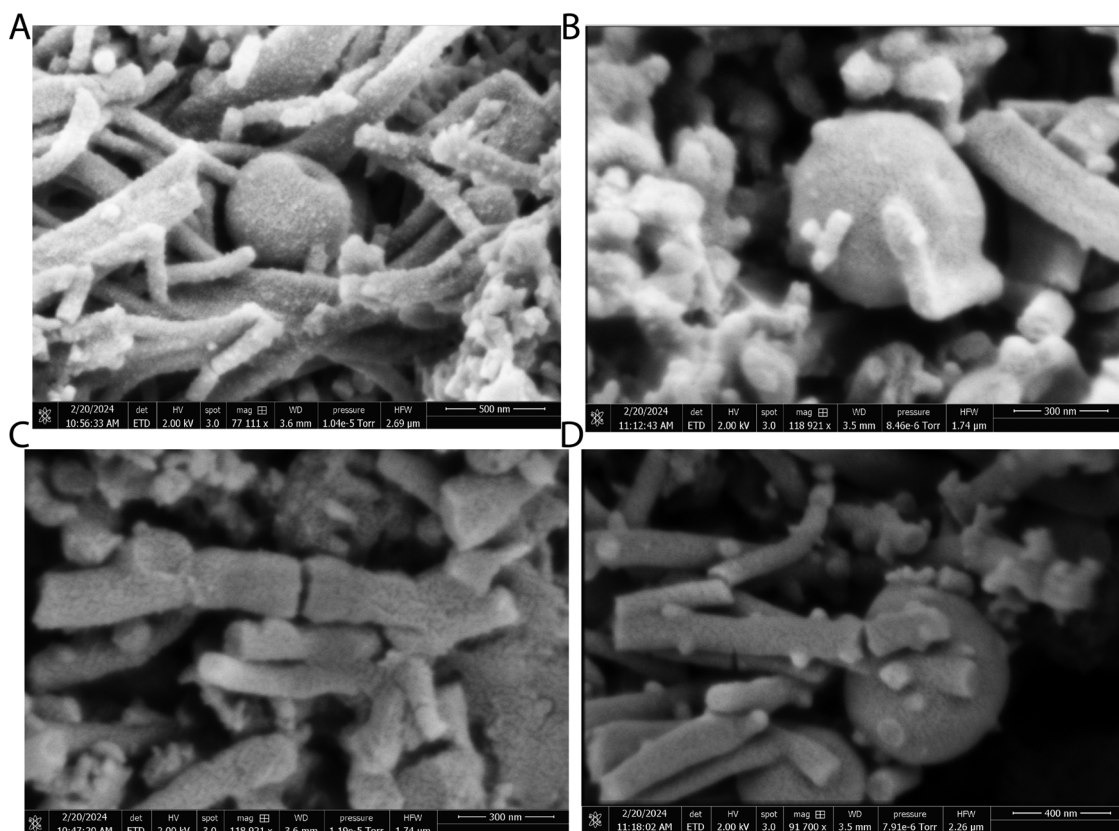
wavelengths and intensities presents opportunities for their usage in many domains, including photosensors, optoelectronic devices, and light-responsive systems.

### 3. Results

#### 3.1. Morphology of self-assembled polyaniline-proteinoids

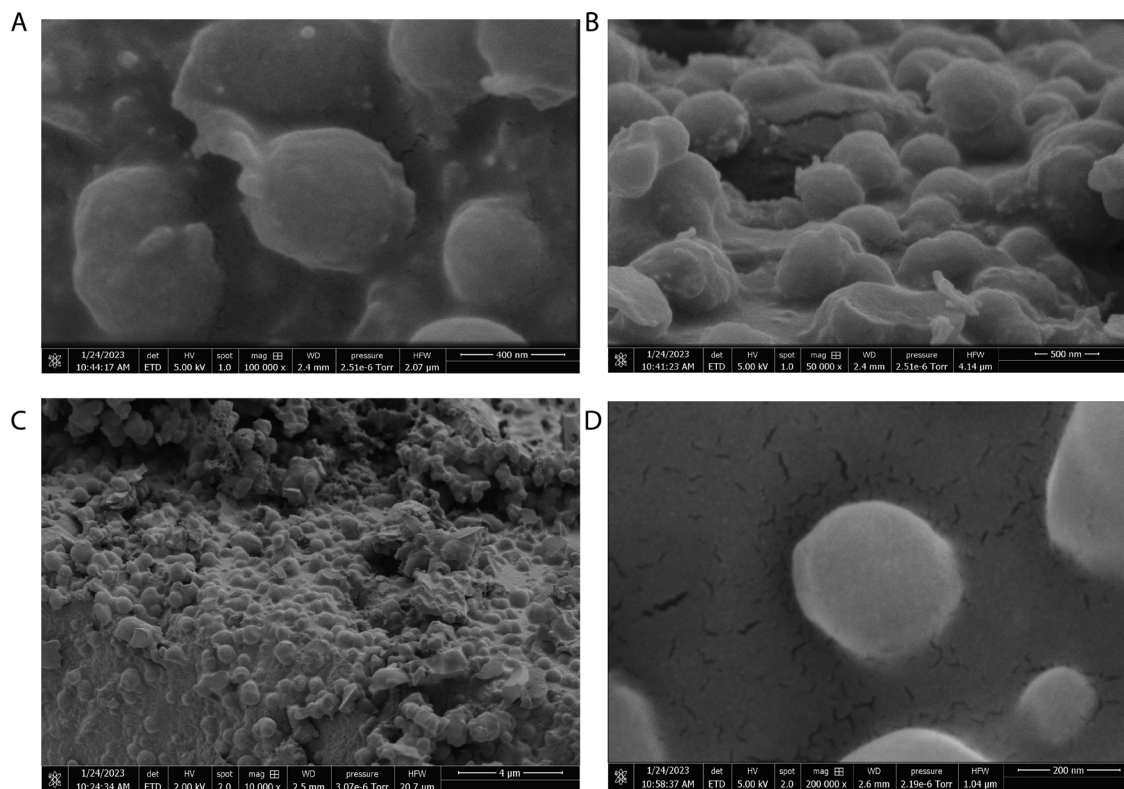
The scanning electron micrographs depicted in Fig. 3 and 4 illustrate the complex nanostructured morphology that is present in the proteinoid microspheres and polyaniline (PANI) fibres. Fig. 3A–D illustrates how the aniline polymerizes into aggregated granules and networks of interconnected nanofibrils, whereas Fig. 4A–D depict how the thermal condensation of amino acids produces nano-“islands” of proteinoid particles. Interestingly, the PANI assemblies have noticeable similarities with neuron cells, which extend intricate neuron-like structures known as dendrites. On the other hand, the proteinoid spheres can effectively simulate synapses and are capable of adapting due to their tailored surface patterns. By combining conductive polymeric fibrils with dynamically tunable peptide spheres, it is possible to replicate the structure and activity of neural tissue.

The structure of the polyaniline-proteinoid samples was examined using scanning electron microscopy (SEM). The samples were prepared by mixing equal volumes of proteinoid and polyaniline solutions (50/50 v/v) to ensure a homogeneous distribution of both components in the composite material. The resulting mixture was then allowed to dry, and the collected powder was used for SEM analysis. Fig. 5 displays a scanning electron microscope (SEM) image of the composite material, showcasing the complex structure of polyaniline nanomaterials and proteinoid ensembles. The elongated polyaniline nanomaterials, highlighted by orange arrows, display a clearly identifiable fibrous morphology. The image shows proteinoid ensembles, which are marked by circles, mixed with polyaniline nanomaterials. It seems that the proteinoid ensembles are coated with a layer of polyaniline, indicating a significant connection between the two components. The SEM imaging employed a high magnification of 13 000× and a modest accelerating voltage of 1.50 kV, enabling precise visualisation of the polyaniline-proteinoid composite without inducing notable sample damage. The use of a spot size of 1.9 enhanced the focus of the electron beam, resulting in the capacity to capture detailed images of the nanoscale



**Fig. 3** Scanning electron micrographs of polyaniline (PANI) nanostructures prepared *via* chemical oxidation of aniline using ammonium persulfate and sulfonic acid (1 : 1 : 0.5 molar ratio), followed by cooling nucleation at  $-8^{\circ}\text{C}$ . (A) PANI nanomaterials with 10 nm width and 500 nm length attached to a PANI nanosphere (400 nm diameter). Scale bar = 500 nm, mag = 77 111×. (B) High magnification image showing PANI nanomaterials surrounded by attached surface fibers on a central PANI nano-sphere. Scale bar = 300 nm, mag = 118 921×. (C) Branching PANI nanofibers resembling neural synapse morphology. Scale bar = 300 nm. (D) PANI nanofibers attached to nanospheres, with nucleation sites on the fibers resembling tree branches. Scale bar = 400 nm. Together, the images exhibit tunable PANI nanostructure morphology and integration of nanospheres and fibril units through oxidative polymerization.





**Fig. 4** Scanning electron micrographs of proteinoids self-assembled *via* thermal polycondensation of amino acids L-glutamic acid, L-phenylalanine, and L-aspartic acid (L-Glu:L-Phe:L-Asp). (A) Spherical proteinoid nanoparticles with 400 nm diameter, scale bar = 400 nm, mag = 100 000 $\times$ , HV = 5.30 kV. (B) An expansive view showing a “sea” of proteinoid nanospheres, scale bar = 500 nm. (C) Aggregated clusters of proteinoid particles, scale bar = 4 microns, mag = 10 000 $\times$ , HV = 2.30 kV. (D) Isolated proteinoid nanosphere with 400 nm diameter, scale bar = 400 nm, mag = 200 000 $\times$ , HV = 5.00 kV. Together the micrographs exhibit tunable, hierarchical self-assembly behaviours in tailorable peptide-based biomaterials.

characteristics with exceptional precision. The presence of elongated polyaniline nanomaterials and proteinoid ensembles coated with polyaniline indicates a unified and interconnected structure inside the composite material.

### 3.2. Spiking activity in polyaniline-proteinoid composites

Fig. 6 illustrates the spiking behaviour exhibited by the bioelectronic composite of polyaniline and proteinoid (PANI-P). The voltage tracings demonstrate swift oscillations, which are distinguished by the emergence of transient spike clusters atop baseline deviations that have been smoothed (Fig. 6A and B). The amplitude distribution parameters for the spikes reveal significant variability (mean  $\pm$  SD = 0.85  $\pm$  3.42 mV). However, time-resolved decoded signals exhibit semi-reproducible wave packet patterns. The “spike trains” depicted in Fig. 6C and D are representative instances of discrete bursts consisting of 2–5 back-to-back pulses with mixed polarity. Although the emergent bioelectronic transients retain stochastic characteristics in terms of intensity and patterning, the outcomes demonstrate a dependable ability to translate intricate conduction dynamics at the millisecond scale within the PANI-proteinoid networks.

After adjusting the voltage recordings to remove baseline drift, it becomes possible to accurately measure spike amplitude distributions without any underlying patterns. Displayed in the Fig. 6 are approximately 80 000 transient events recorded

with an average peak height of 1.75 mV above the threshold potential. The data shows a median of 1.15 mV and an inter-quartile range from 0.47 to 2.94 mV, indicating an asymmetric skew, with spikes exceeding 12 mV. Even with a standard deviation of 1.55 mV, noticeable patterns such as spike doublets and triplets influence the higher-level temporal organisation in these intricate biosynthetic matrices. Intense bursts occur at irregular intervals ranging from 0.55 to 6.05 minutes, indicating diverse dynamics in the landscape.

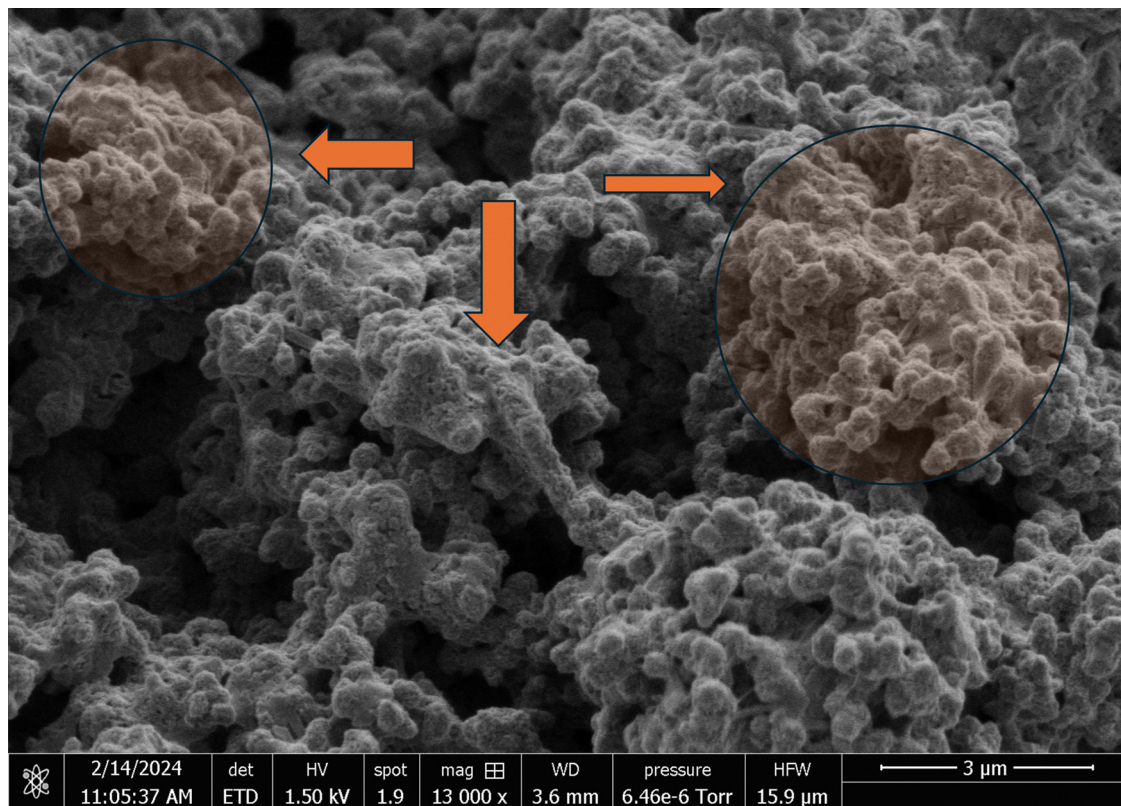
The proteinoid-PANI composites exhibit broad bandwidth behaviours as shown by the spectral distribution in Fig. 8A, spanning over 100 dB of signal intensities. Statistical analysis reveals the variance is centralized around a mean  $\mu$  = −68.95 dB with a standard deviation  $\sigma$  = 9.22 dB following a normal probability density function  $f(x) = \frac{1}{\sigma\sqrt{2\pi}}e^{-\frac{(x-\mu)^2}{2\sigma^2}}$  (Fig. 8B). While minimal signals become buried in sub-threshold noise < −104 dB, discernible bioelectronic activity emerges up to +12 dB, confirming richly heterogeneous conduction.

### 3.3. Modelling optically-triggered excitability using yellow light pulses in interfaced PANI-proteinoids

Analysing PANI-proteinoid composites using yellow light reveals changes in voltage patterns based on lighting frequency,







**Fig. 5** Scanning electron microscopy (SEM) image of polyaniline-proteinoid samples. The image was acquired with an accelerating voltage of 1.50 kV, a spot size of 1.9, and a magnification of 13 000 $\times$ . The scale bar represents 3  $\mu$ m. Orange arrows indicate elongated polyaniline nanomaterials, while highlighted circles show proteinoid ensembles covered with polyaniline. The scanning electron microscope (SEM) image displays the complex structure of the polyaniline-proteinoid composite, where polyaniline nanomaterials are tightly connected with proteinoid nanospheres.

as seen in Fig. 8. Yellow light at a frequency of 5 Hz stimulates naturally occurring repetitive spike patterns, which have recurrence periods centred around a specific resonance frequency.

This frequency is determined by the formula  $f(x) = \frac{1}{\sigma\sqrt{2\pi}} e^{-\frac{(x-\mu)^2}{2\sigma^2}}$  with parameters  $\mu = 554.83$  s and  $\sigma = 198.80$  s. Composite interactions enhance response amplitude sensitization, resulting in a 4-fold increase in means to  $0.118 \pm 0.109$  mV, as shown in distributions (Fig. 6D). The measurements confirm the ability to use programmable optical control to direct both the rhythm and strength of complex spike waveforms. Current research are concentrated on identifying differences in structure to better understand the information storage capabilities in complex intermittent pathways of these bioelectronic materials.

The coefficient of variation ( $C_V$ ) provides a quantitative basis for assessing spike train variability:

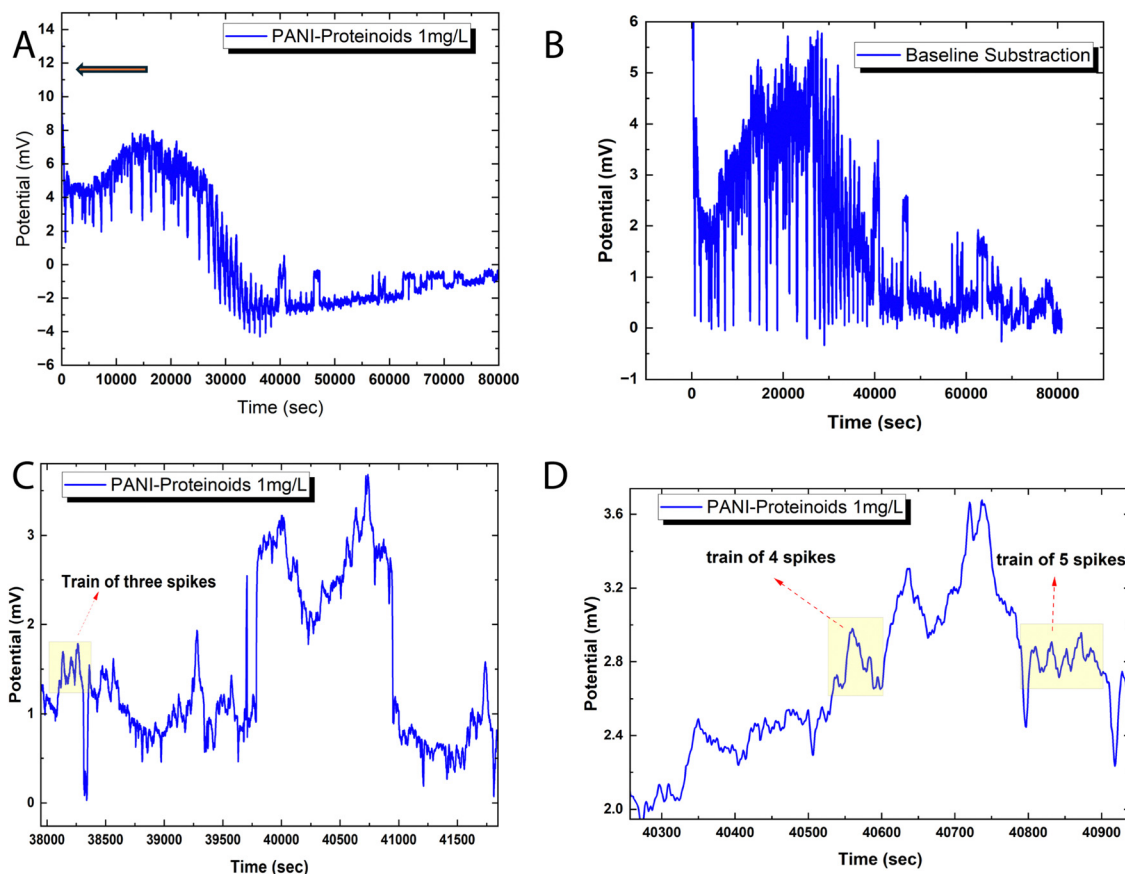
$$C_V = \frac{\sigma}{\mu} \quad (1)$$

where  $\sigma$  is the standard deviation and  $\mu$  is the mean of the inter-spike intervals. A higher  $C_V$  indicates more irregularity. The measured periods between oscillations for the PANI-proteinoid composite exhibit a  $C_V$  of 0.36, substantially exceeding the  $C_V =$

0 expectations for a periodic oscillator. The amplitude fluctuations demonstrate an even higher  $C_V$  of 0.93, nearing the  $C_V \approx 1$  typical of noisy biological neurons. The results demonstrate the unpredictable character of the bioelectronic bursting environment, which is influenced by an integrated network with shaping processes that randomly adjust times and intensities between occurrences. Identifying the origins of variability when recognising higher-order firing patterns might help understand the multiplex coding features that large synthetic systems have when they go through metastable states that are far from equilibrium. Studying sequence preferences, shape classifications, and transition probability goes beyond basic statistics to uncover mesoscale coordination principles and adjustable regime predictors despite ongoing uncertainties. The significant variation in the amplitudes and periods of the triggered voltages and periods across multiple recorded burst events is clear in the given values, which span a period of over 800 seconds and an amplitude of 210 millivolts (Table 4).

Fig. 7c, d and a, b compare the power spectral distributions of the absence ( $\mu = -68.95$  dB) and presence ( $\mu = -60.26$  dB) of pulsed yellow light (5 Hz) to illustrate that optical stimulation induces significant focusing of signal density across specific frequencies. In addition to achieving a 9 dB gain in mean baseline power to match increased coordination expectations, the concurrent decrease in standard deviation from 9.22 to 7.61





**Fig. 6** Spiking potential activity of composites composed of polyaniline and proteinoid (PANI-P). (A) Raw voltage trace spanning 80 858 measurements illustrating arbitrary oscillations. The amplitude distribution of spikes exhibits considerable dispersion (standard deviation = 3.42 mV), surpassing 12 mV (indicated by the orange arrow), and has a mean of 0.85 mV. This dispersion signifies the considerable variation in both intensity and temporal structure among evoked bursts. (B) The elimination of baseline trends exposes distinct, fleeting peaks that possess both positive and negative polarity, atop potential deviations that have been smoothed. (C), (D) Decoding a time-resolved signal differentiates discrete wave packets consisting of two, three, or five consecutive pulses. Although random, these high-resolution images validate the existence of semi-reproducible patterns within clusters of emergence spikes.

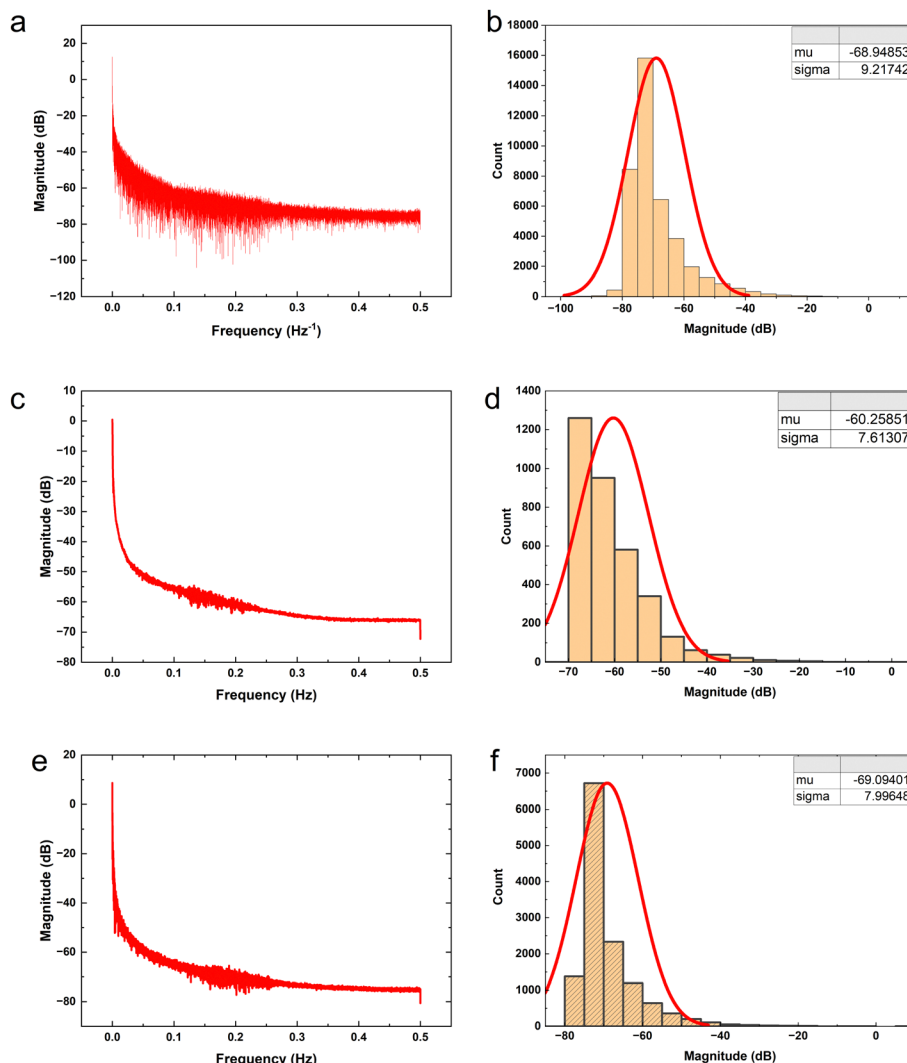
dB under optical forcing demonstrates that resonant synchronisation enables emergent selectivity. This deviation in variance trends from ambient background amplification demonstrates that light-activated accumulation is not simply stochastic magnification. While there is an apparent increase of approximately 9 dB in the mean signal intensity from Fig. 7b (−68.95 dB) to Fig. 7d (−60.26 dB), it is crucial to consider the standard deviations of both data sets. The standard deviation is around 10 dB for both Fig. 7b ( $\sigma = 9.22$  dB) and Fig. 7d ( $\sigma = 7.61$  dB), indicating a considerable spread in the signal intensities. The hypothesis test results indicate a statistically significant difference between the mean signal intensities of the power spectra in Fig. 7b and d. The test yielded an extremely low  $p$ -value ( $p = 0.000000000$ ), which is well below the commonly used significance threshold of 0.05. This suggests that the observed difference in mean signal intensities is highly unlikely to have occurred by chance alone. The confidence interval on the difference in means (ci) ranges from 8.419434 to 8.960599, indicating that the true difference in mean signal intensities between the two conditions is likely to fall within this range

with a high level of confidence. The test statistics provide further support for the significance of the difference. The  $t$ -statistic of 62.963792 with 4313.874658 degrees of freedom (df) indicates a large effect size and reinforces the statistical significance of the result. Additionally, the standard deviation (sd) of 7.613066 suggests a relatively consistent spread of signal intensities within each data set. These results strongly suggest that the increase of approximately 9 dB in the mean signal intensity from Fig. 7b (−68.95 dB) to Fig. 7d (−60.26 dB) represents a statistically significant difference between the electrical activity of the proteinoid-PANI composites in the default state and when driven at 5 Hz by yellow light. The statistical significance of this difference implies that the observed changes in electrical activity are unlikely to have occurred by chance and are likely to be biologically relevant.

Precisely modulated optical stimulation verifies external control over emergent bioelectronic dynamics in PANI-proteinoid networks. Pulsed 1 Hz illumination drives oscillatory voltage waveforms (Fig. 9) phase-locked to the rhythmic input. Statistical period distribution around  $1067 \pm 582$  s







**Fig. 7** Power spectra and statistical analysis of electrical activity in proteinoid-PANI composites driven by yellow light at different frequencies. (a) and (b) Power spectra of default activity plotting signal intensity (dB) against frequency (Hz) for 40 430 spectral data points. The table displays summary statistics indicating that the amplitude variance is centred around a mean of  $\mu = -68.95$  dB with a standard deviation of  $\sigma = 9.22$  dB. The cutoff range is from signals below  $-104$  dB to activity around  $+12$  dB, revealing various behaviours within noise interference. A normal distribution is created using the calculated mean and variance. Analysing the signal values reveals a wide bandwidth that is mostly dedicated to random sub-threshold fluctuations before reaching visible electrical events. (c) and (d) Quantification of the spectral patterns exhibited by PANI-proteinoid networks driven at 5 Hz by yellow light. The statistical analysis of signal power distribution across frequencies reveals a mean of  $-60.26$  dB and a standard deviation of  $7.61$  dB ( $N = 3420$ ). A fit of the signal intensities to an equivalent normal distribution emphasises the centralization of variance. At peaks, active energy surpasses noise floors and approaches 0 dB, indicating that particular conduction pathways are resonantly activated within the background. (e) and (f) Quantitative frequency domain analysis of 20 Hz-induced yellow light dynamics. The power spectrum is focused on the stimulation frequency and shows patterns across wider ranges. The statistical distribution of band-limited power around a mean of  $-69.094$  dB and a standard deviation of  $7.996$  dB indicates amplification compared to the default baseline activity. Other metrics indicate a total range from  $-80$  dB minimum to  $+8$  dB maximum.

(Table 3) proves reliable coordination, with concentrated amplitude measures showing consistent  $0.56$  mV events atop complex baselines. Higher input frequencies enhance periodicity and introduce amplitude variability similar to biological neurons with noise. Adjusting stimulus parameters promotes precise control of spike train information – in contrast to random uncertainty without tailored external influence.

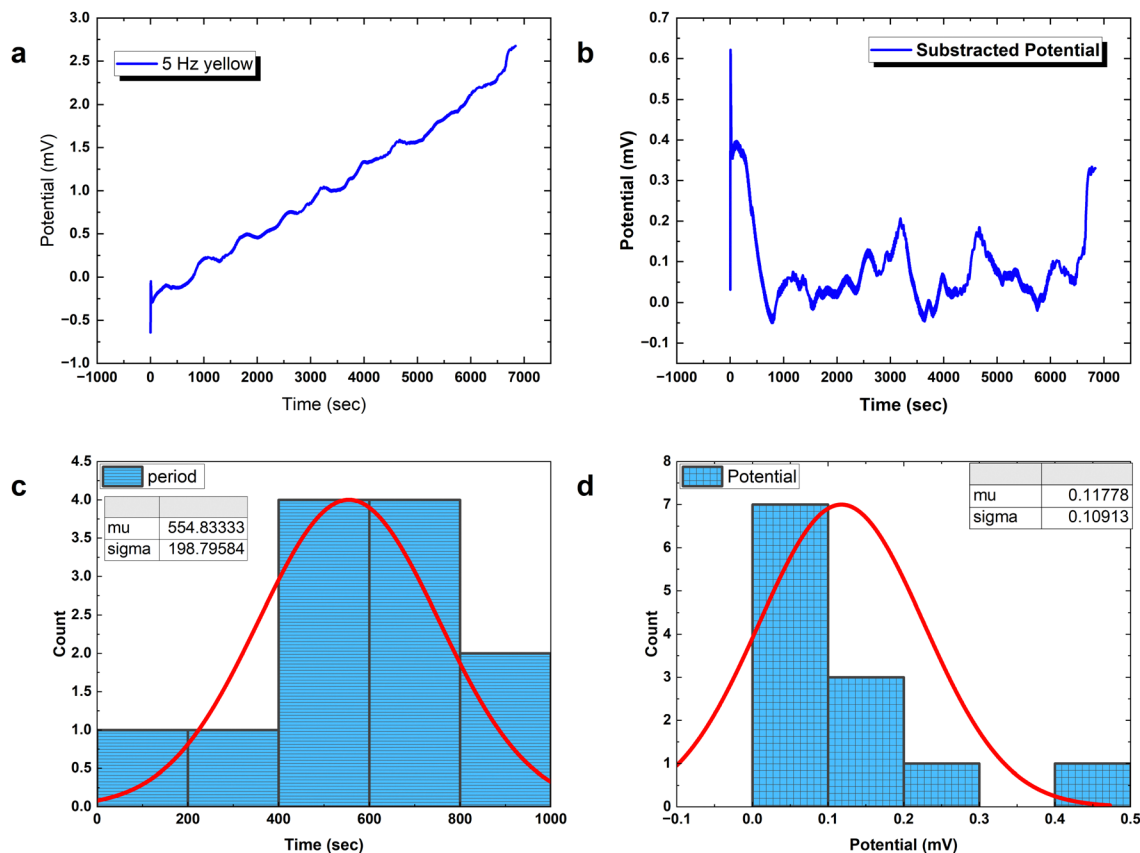
The amplitude distribution of the optically triggered electrical signals (1 Hz) in the PANI-proteinoid networks exhibits a bimodal character (Fig. 9d), suggesting the presence of two

distinct populations of electrical responses. To quantitatively analyse this bimodal distribution, we fitted the amplitude data with a bimodal distribution function, which is a sum of two Gaussian distributions. The equation of the bimodal distribution function is given by:

$$f(x) = A_1 \exp\left(-\frac{(x - \mu_1)^2}{2\sigma_1^2}\right) + A_2 \exp\left(-\frac{(x - \mu_2)^2}{2\sigma_2^2}\right) \quad (2)$$

where  $A_1$  and  $A_2$  are the amplitudes,  $\mu_1$  and  $\mu_2$  are the means,





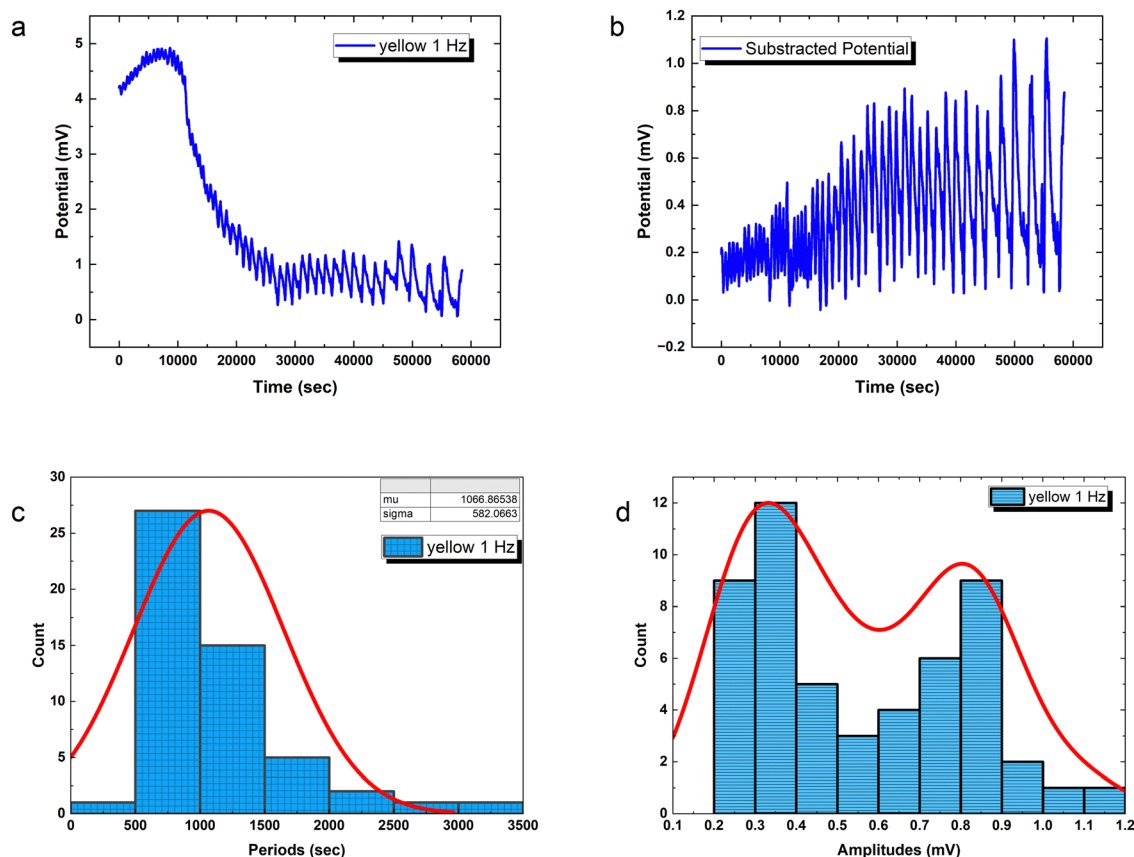
**Fig. 8** Analysis of how PANI-proteinoid networks react to 5 Hz yellow light stimulation. (a) Voltage recording displaying induced oscillatory bursting events superimposed on a baseline over time. (b) Removing low frequency trends reveals transient spike patterns, characterised by oscillations occurring at irregular intervals. (c) The distribution of measured times between evoked bursts peaks at  $554.83 \pm 198.80$  seconds, confirming the effectiveness of visual stimulation near to the 5 Hz target rhythm. (d) Amplitude variations of emergent voltage deflections are extracted at  $0.118 \pm 0.109$  mV, allowing for assessment of sensitivity enhancements resulting from synergistic photoresponse interactions across components. Studying the differences in shape of complicated spike waveforms can help identify the information encoding capabilities activated by programmable light passing via dynamic bioelectronic materials.

and  $\sigma_1$  and  $\sigma_2$  are the standard deviations of the two Gaussian components. The fitting of the bimodal distribution to the amplitude data was performed using the Levenberg–Marquardt algorithm, as the trust-region-reflective algorithm required at least as many equations as variables. The fitted parameters obtained from the bimodal distribution fitting are as follows:  $A_1$  (height1) = 1.094154,  $\mu_1$  (mean1) = 0.090  $\sigma_1$  (std1) = 0.2506,  $A_2$  (height2) = 1.7216  $\mu_2$  (mean2) = 0.3014,  $\sigma_2$  (std2) = -0.0457. The bimodal distribution fitting reveals that the amplitude data is characterized by two distinct peaks, with means located at approximately 0.90 mV and 0.30 mV. The presence of these two peaks indicates that the PANI-proteinoid networks exhibit two different types of electrical responses when optically stimulated.

PANI-proteinoid oscillation periods under sporadic illumination at 1 Hz have a coefficient of variation ( $C_V$ ) of 0.5455, which indicates that they vary by more than 50 percent relative to the mean periodicity. In contrast, spike amplitudes exhibit a  $C_V$  of 0.4639, which is close to fluctuations of 50%. On the contrary, raising the pulsation frequency to 5 Hz results in a  $C_V$  value of 0.36 for periods, which indicates a greater degree of

rhythmic consistency and approaches linear predictions in the presence of noise. Nonetheless, stimulation at a higher frequency also results in an increase in amplitude variability ( $C_V = 0.93$ ), which is close to the  $C_V \approx 1$  characteristic of abnormal biological neurons. In brief, although the use of optical forcing causes expected oscillations, accuracy decreases at 1 Hz. This implies that in order to induce emergent pathways into dependable coordination, the substrate must possess a sufficient excitation density.

20 Hz optical driving induces tight oscillation periodicity coordination with  $C_V = 0.4233$  (Fig. 10), contrasting greater irregularity at slower input rates. However, higher frequency stimulation fails to constrain amplitude heterogeneity ( $C_V = 0.4676$ ). This divergent tuning of activity features by input rate modulation occurs in biological neurons. In fact, at 20 Hz the PANI-proteinoid dynamics resemble matured neural networks through excelling regularity ( $C_V \approx 0.4$ ) over the  $C_V \approx 1$  extreme fluctuations in early developing brains. This suggests sufficient external energy infusion properly trains intrinsic processes into reliable communication regimes from disorder. Comparatively, 1 Hz stimulation shows poor  $C_V = 0.5455$  periodicity and



**Fig. 9** Optically regulated electrical dynamics in PANI-proteinoid networks. (a) Induced rhythmic spiking activity by pulsed yellow illumination at 1 Hz; this demonstrates light-directed neuromorphic excitation. (b) Complex oscillatory waveform morphology over minutes-long timescales after removing baseline drift. (c) By mapping oscillation periods to probability distributions, one can determine that  $1067 \pm 582$  s periods prevail in the structured coordination. (d) The histogram exhibits a bimodal distribution with two prominent peaks centered at approximately 0.30 mV and 0.90 mV. This bimodal character suggests the presence of two distinct populations of electrical responses within the composite material. The fitted curve (red line) represents a mixture of two Gaussian distributions, capturing the bimodal nature of the data. The precise optical triggerability and the measurable electrophysiological features demonstrated by the proteinoid-PANI composites highlight the potential for external optical control over emerging bioelectronic excitability. This proves that light, biocompatible materials can work together to activate photosensitive tissues. In addition to precise optical triggerability, electrophysiological features that can be measured allow external optical control over emerging bioelectronic excitability. This proves that light, biocompatible materials can work together to activate photosensitive substrates.

$C_V = 0.4639$  amplitude consistency. Increasing to 5 Hz recovers some periodicity ( $C_V = 0.36$  periods) at cost of noisier spikes ( $C_V = 0.93$  amplitudes) – recapitulating neural trajectories from irregularity to bursting synchronization.

Frequency domain quantification supports the claim that incremental optical stimulation leads to systematic spectral tuning by energising biomolecular ionic transport networks (Fig. 7a and b). When the signalling is at its basic level without any external adjustments, the average power level is  $-68.95$  dB with a standard deviation of  $9.21$  dB. With the addition of  $5$  Hz yellow pulsing, the reading shifts to  $-60.26$  dB ( $\sigma = 7.61$  dB), indicating a statistically significant increase of over  $8$  dB in coordinated amplification compared to spontaneous conduct. Increasing the input rate to  $20$  Hz results in a greater enhancement, with a mean of  $-69.095$  dB ( $\sigma = 7.996$  dB) in the spectra, showcasing more precise sub-band variability.

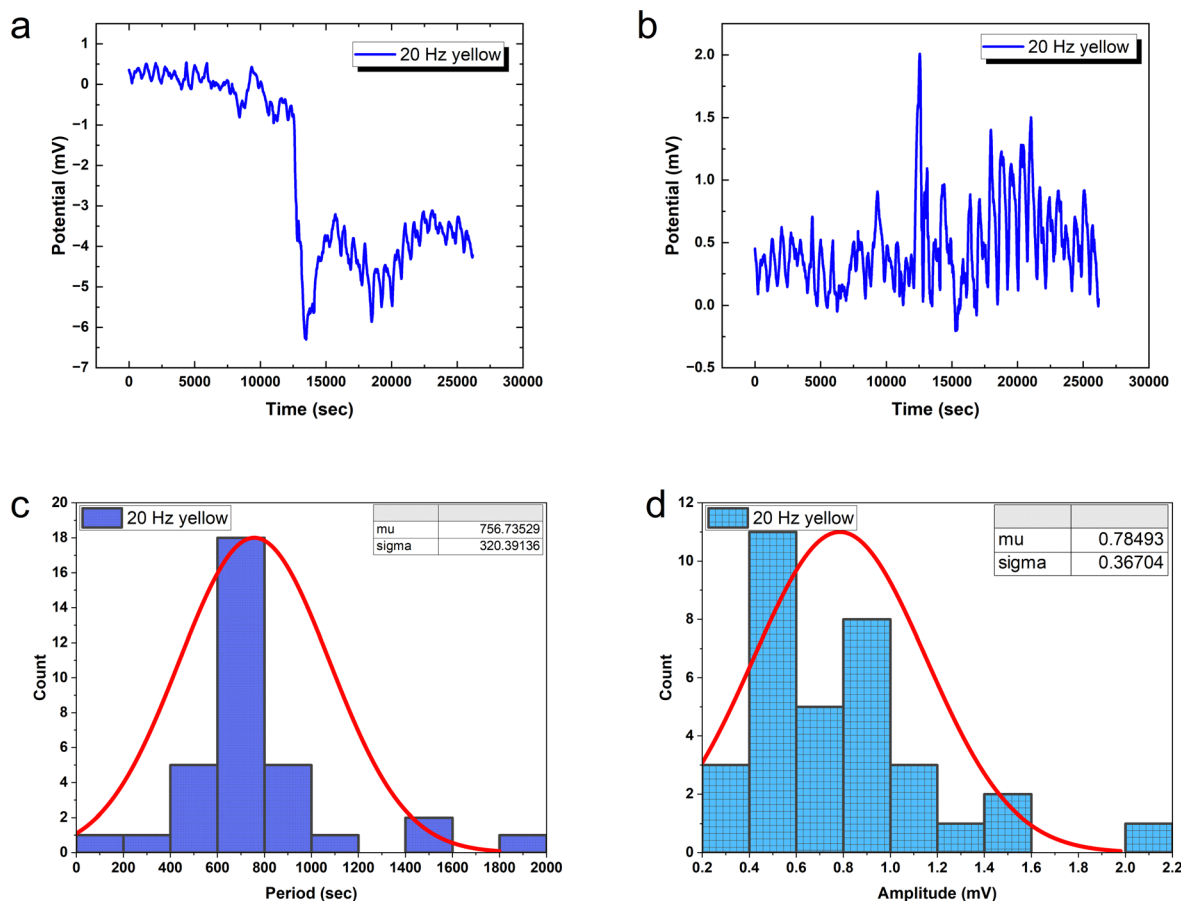
Analysing and comparing profiles confirms the advancement in focusing on specific wavelengths and increasing light

intensity through optical stimulation. This global reorganization reflects the neural plasticity processes triggered by stimuli, which are recalibrating communication through boosted pathways.

### 3.4. Exploring hierarchical maps and attentive vision: modulating spike trains in PANI-proteinoid nanofibers under varied optical pulse frequencies

Human beings demonstrate an exceptional capacity to consistently identify objects despite variations in illumination, scale, rotation, and other perceived factors. Hierarchical processing along the ventral visual stream, which results in view-invariant representations from ever-more-complex features, is believed to be the source of this refined object recognition. Therefore, by learning the complex nature of hierarchical processing, one can not only facilitate the development of computer vision systems but also uncover insights into the perceptual capabilities of the human brain. Our study investigates hierarchical





**Fig. 10** Proteinoid optical stimulation uncovers how environmental variables influence emergent reactivity. (a) At 20 Hz, yellow pulses cause rhythmic voltage oscillations that are synchronised with the input drive. (b) Removing baseline drift emphasises the intricate spike morphology. (c) The oscillation periods are centred around  $757 \pm 320$  seconds, indicating a more precise coordination compared to the 1 Hz excitation. (d) Increased amplitudes show more variability around a mean of  $0.78 \pm 0.37$  mV, similar to noisy biological spike statistics. Directed energy infusion when conductive composite transduction is combined, it could facilitate bioinspired optical logical functions.

representations for bio-hybrid systems that require invariant pattern recognition. In particular, we manipulate the spiking characteristics of proteinoid-PANI nanofibers by inputting patterns of varying optical pulse frequencies. Subsequently, the photoelectrochemical response data are subjected to hierarchical clustering in order to analyse the emergence of categories across different pulse rates. The purpose of this study is to find out how distinct response subgroups resulting from the nanofibers' complex biomolecular relaxation processes may serve as the foundation for invariant recognition. Our primary objective is to replicate the hierarchical feature learning that is thought to enable resilient perception in neural systems. Brain-mimetic computing and flexible biosensors may be significantly advanced as a result.

The examination and hierarchical clustering of the photoelectrochemical data demonstrate discernible patterns in the PANI-proteinoid system's response to various frequencies of illumination (Table 1 and Fig. 11). The clustering identifies between groups with a rapid response (period 0.05–0.31 s) and a moderate amplitude (496–816 mV) when illuminated with yellow light pulses at 1 Hz (Fig. 11A). As the frequency

increases to 5 Hz (Fig. 11B), the amplitude rises (632–3060 mV) while the period shortens (0.34–1.05 s), indicating a faster

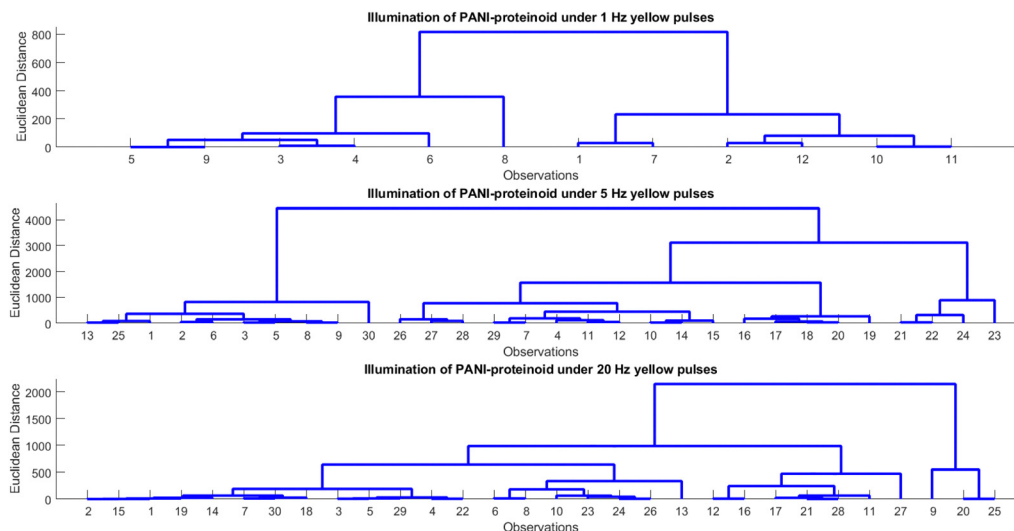
**Table 1** Cluster means for amplitude and period under varied pulse frequencies

1 Hz pulse		5 Hz pulse		20 Hz pulse	
Cluster	Amplitude (mV)	Cluster	Amplitude (mV)	Cluster	Amplitude (mV)
1	496.0	1	3060.0	1	1911.0
2	419.0	2	2332.3	2	1435.0
3	816.5	3	1753.0	3	684.1
4	674.0	4	1189.5	4	887.1
5	157.0	5	632.1	5	444.1

1 Hz pulse		5 Hz pulse		20 Hz pulse	
Cluster	Period (s)	Cluster	Period (s)	Cluster	Period (s)
1	0.130470	1	0.945400	1	0.572700
2	0.054265	2	1.048033	2	0.774250
3	0.308265	3	0.840874	3	0.662915
4	0.110772	4	0.713168	4	0.896857
5	0.006260	5	0.339883	5	1.002700





**Fig. 11** Analysis and hierarchical clustering of photoelectrochemical data relating to the PANI-proteinoid in the presence of pulsed yellow light illumination. Yellow light pulses at 1 Hz, 5 Hz, and 20 Hz, dendrograms illustrate the outcomes of clustering. The analysis of cluster means for amplitude and period provides insights into the patterns that govern the photoelectrochemical response as the pulse frequency varies. Key observations include: higher frequency pulses exhibit increased amplitude and decreased period, both of which indicate a quicker response time of up to 5 Hz; divergence into discrete response groups at 20 Hz implies the presence of intricate relaxation mechanisms.

response time. Nevertheless, the response initiates branching into clusters with contrasting amplitudes (444–1911 mV) and periods (0.57–1.00 s) at 20 Hz (Fig. 11C). This indicates the initiation of intricate relaxation mechanisms within the PANI-proteinoid. In general, an increase in pulsed illumination frequency enhances the photoelectrochemical response time until 5 Hz, at which point non-linear effects become more prevalent.

Capable of processing a wide range of input patterns and reacting appropriately, the integrated PANI-proteinoid complex demonstrates essential attributes of a perceptron, thus further advancing PANI-based perceptron prototypes developed by Erokhin and colleagues.<sup>18,19,41,42</sup> When considering the excitability of the nanofiber network, the applied optical pulse frequencies operate in a manner similar to adjusting the probabilities of neuron spikes and refractory dynamics. Encoded in the hierarchical clustering of amplitude and period data, the resultant photoelectrochemical response classifies the inputs as a nonlinear decision boundary. Although the present study solely investigates three distinct illumination frequencies, the ability to differentiate between the induced dynamics is an essential proof-of-concept.

### 3.5. Nearest neighbour classification analysis of PANI-proteinoid response to yellow light stimulation

The nearest neighbour (NN) classification method was used to examine the distinctiveness and grouping of PANI-proteinoid responses, taking into account their amplitude and period characteristics at various frequency of yellow light pulses (Fig. 12). NN classification allocates an input to the class of its closest neighbour, defined by a metric such as the

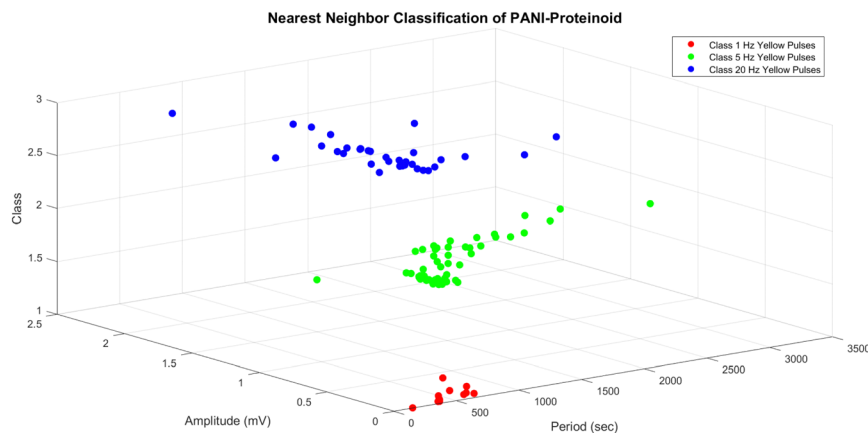
Euclidean distance between vectors **x** and **y**:

$$d(\mathbf{x}, \mathbf{y}) = \sqrt{\sum_{n=1}^M (x_n - y_n)^2} \quad (3)$$

where *M* is the dimensionality of the feature space.

The three-dimensional scatter plot (Fig. 12) illustrates the arrangement of the data points and their corresponding classes. The y-axis represents the amplitude, the x-axis represents the period, and the z-axis represents the class. The dataset has three distinct classes: class 1 (represented by red circles) corresponds to yellow pulses with a frequency of 1 Hz, class 2 (represented by green circles) corresponds to yellow pulses with a frequency of 5 Hz, and class 3 (represented by blue circles) corresponds to yellow pulses with a frequency of 20 Hz. The NN classifier establishes a decision boundary that is composed of linear segments, where each segment represents the perpendicular bisector between two data points from distinct classes. The input space is divided into discrete regions that correspond to different classes, as evidenced by the separate clusters in the plot. The findings of the NN classification, as shown in Fig. 12, offer valuable information about the distinguishability and grouping of the PANI-proteinoid responses at various stimulation frequencies. The separate groupings associated with each category indicate that the amplitude and time features of the reactions differ considerably depending on the frequency of the yellow light pulse applied. This discovery emphasises the potential of utilising PANI-proteinoid systems as biosensors or signal processors that are sensitive to different frequencies. By varying the stimulation frequency, it is possible to encode and distinguish between various states or categories of responses.





**Fig. 12** Nearest neighbor (NN) classification of a three-dimensional dataset representing the amplitude and period of PANI-proteinoid responses under different yellow light pulse frequencies. The dataset has three classes: class 1 (red circles) corresponds to 1 Hz yellow pulses, class 2 (green circles) corresponds to 5 Hz yellow pulses, and class 3 (blue circles) corresponds to 20 Hz yellow pulses. The NN classifier assigns each data point to the class of its closest neighbour in the feature space. The three-dimensional scatter plot depicts the distribution of data points and their corresponding classes, with amplitude on the y-axis, period on the x-axis, and class on the z-axis. The NN classification sheds light on the separability and clustering of PANI-proteinoid responses based on their amplitude and period properties across multiple stimulation frequencies.

The period values for the 1 Hz yellow pulses group (class 1) range from 157.00 to 831.00 seconds, while the amplitude values cover from 0.01 to 0.41 mV. These findings suggest that the PANI-proteinoid responses to 1 Hz stimulation have longer duration and smaller magnitude compared to the other groups.

The 5 Hz yellow pulses group (class 2) has a broader range of period values, ranging from 63.00 to 3060.00 seconds, with amplitude values ranging from 0.20 to 1.11 mV. These findings indicate that the PANI-proteinoid responses to 5 Hz stimulation exhibit greater variability in terms of their timing and signal intensity compared to the group stimulated at 1 Hz.

The 20 Hz yellow pulses group, classified as class 3, has period values that range from 134.00 to 1911.00 seconds and amplitude values that span from 0.37 to 2.01 mV. The amplitude values in the higher range show that the PANI-proteinoid responses to 20 Hz stimulation have stronger signal intensity compared to the groups with lower frequencies.

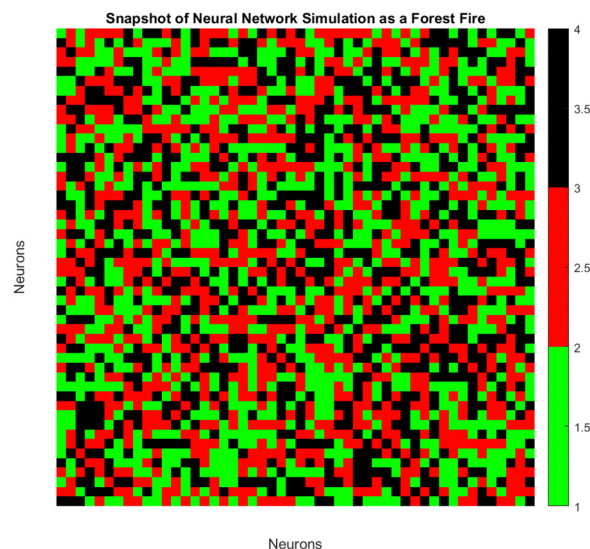
The borders serve as a numerical indicator of the disparities in the PANI-proteinoid reactions when exposed to different frequencies of stimulation. The separate ranges of period and amplitude values for each group indicate that the frequency of the yellow light pulses applied has a notable influence on the temporal and signal properties of the PANI-proteinoid system.

From the viewpoint of neuromorphic engineering, these discoveries emphasise the possibility of utilising PANI-proteinoid systems as signal processors or pattern recognizers that are dependent on frequency. The capacity to distinguish between various stimulation frequencies based on the response characteristics presents opportunities for encoding and decoding information in these bio-inspired devices.

### 3.6. Modeling neural network dynamics: forest fire simulation with neuronal states influenced by PANI-proteinoid amplitude under yellow light stimulation

The spatiotemporal patterns of spiking dynamics exhibited by neurons in large-scale networks are comparable in complexity

to the propagation of forest fires (Fig. 13). Individual neurons cycle through active (firing), refractory (recovering), and quiescent states, visualised here as burning, burnt, and green trees respectively. Previous computational models have demonstrated that in such networks, simple growth and ignition principles can give rise to emergent critical dynamics characterised by activity cycles that extend across all scales. By modulating PANI-proteinoid films photoelectrochemically, our bio-hybrid system is capable of simulating these multifaceted neural interactions. The applied optical pulse frequencies (1 Hz, 5 Hz, 20 Hz) tune the excitability of the underlying



**Fig. 13** A snapshot of a neural network simulation as a forest fire represents the spatiotemporal dynamics of neurons. Each pixel denotes a single neuron coloured based on its state: green for quiescent, red for active, and black for refractory. The visualisation may be influenced by amplitude data from 1 Hz, 5 Hz, and 20 Hz yellow light pulse stimulation onto the PANI-proteinoid complex, potentially impacting the activity states depicted.



nanofiber network, regulating the readiness of quiescent nodes to fire, as well as recovery timescales, and spontaneous activation rates. As illustrated through the analogy of a forest fire, this results in the formation of clusters, oscillations, and surges of spiking activity. The spatiotemporal dynamics of the neural network are visualized using an analogy to a forest fire model on a discrete lattice (Fig. 13). Each lattice site represents the state of a neuron, categorized as:

$$s_{r,t} = \begin{cases} 1 & \text{active (firing)} \\ 0 & \text{quiescent (polarized)} \\ 100 & \text{refractory (hyperpolarized)} \end{cases} \quad (4)$$

The state  $s_{r,t}$  at position  $\mathbf{r}$  and time  $t$  evolves according to a set of probabilistic update rules:

$$p(s_{r,t} = 100 | s_{r,t-1} = 1) = 1 \quad (5)$$

$$p(s_{r,t} = 0 | s_{r,t-1} = 100) = p \quad (6)$$

$$p(s_{r,t} = 1 | s_{r,t-1} = 0) = \begin{cases} 1 & \text{if } \sum_{\Delta\mathbf{r}} W_{\Delta\mathbf{r}} s_{\mathbf{r}+\Delta\mathbf{r},t-1} > \theta \\ f & \text{otherwise} \end{cases} \quad (7)$$

Here,  $W_{\Delta\mathbf{r}}$  gives the connection weight from a neighbor displaced by  $\Delta\mathbf{r}$ , and  $\theta$  is a firing threshold. The evolution captures the cycle of firing, recovery, and resting phases. The model visualizes how cascades of activity emerge across the network.

To model the gradual recovery from the refractory state, an additional state transition rule is introduced (eqn (8)):

$$s_{r,t} = \begin{cases} s_{r,t-1} - 1 & \text{if } s_{r,t-1} > 1 \\ s_{r,t-1} & \text{otherwise} \end{cases} \quad (8)$$

By reducing the state value of neurons in the refractory state (represented by values greater than 1) by 1 in each time step until they reach the quiescent or active state, this rule ensures that they gradually recover.

### 3.7. Neuronal spike timing analysis in PANI-proteinoid sample under varying yellow light pulse frequencies

The integrated PANI-proteinoid structure is similar to a biological perceptron in its capacity to interpret different input spike patterns and respond accordingly. Specifically, the applied optical pulse frequencies modulate the excitability dynamics of the nanofiber network in a manner similar to adapting neuron firing rates and recovery time periods. The measured photoelectrochemical response, stored in the hierarchical clustering of amplitude and period characteristics, serves as a nonlinear decision boundary for categorising stimulation methods. Thus, the synergistic interactions of the complex biomolecular components enable integrative capabilities similar to neural processing.

While the current study uses three discrete illumination frequencies as inputs, the system properly differentiates between the resulting dynamics, showing its pattern integration potential. Additional research using gradually changing pulse cycles would help to map out more complex partition

boundaries. In essence, the bio-hybrid material acting as a perceptron “neuron” receives spatiotemporal light inputs at its “dendrites” and integrates and translates them into differential “firing” responses. The displayed input–output signal processing offers insight into emergent cognition-mimetic properties.

PANI-proteinoid structures show potential for developing increasingly brain-like functions, ranging from low-level feature extraction to high-level invariant pattern recognition. At its root, the ability to organise this biosynthetic soft material into customisable computational networks suggests adaptability in accordance with the demands of vision and other cognitive functions.

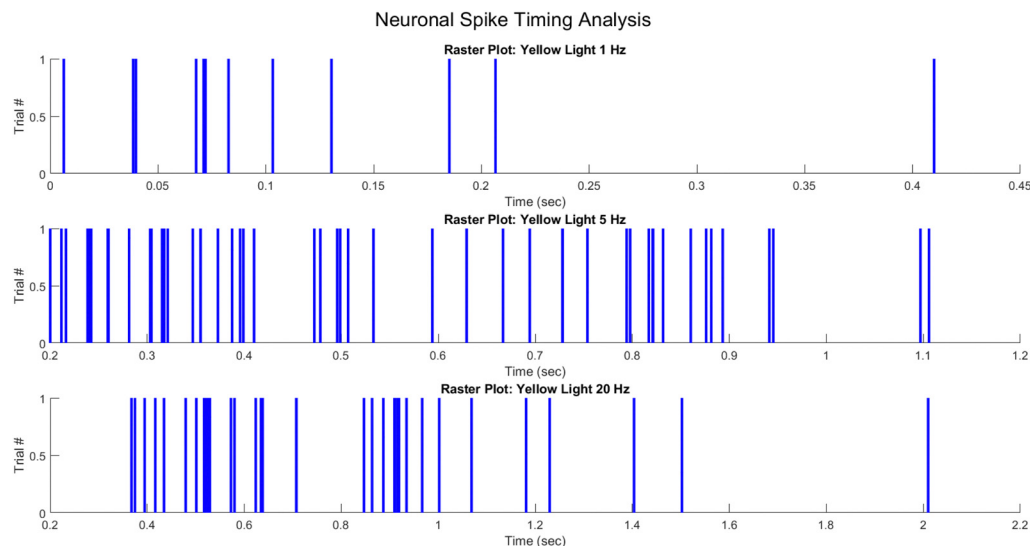
For visualising the spike timing activity of neurons, raster diagrams are an important technique. In the same way that action potentials are characterised by their timing as stereotypical electrical impulses that communicate information mainly through their visual characteristics, raster plots offer an intuitive depiction by representing spikes as distinct checkboxes on a timeline. Assigning spike events to specific trials, each pulse indicates the moment when a recorded voltage trace surpasses a predetermined threshold. The capacity to plot repeated experiments along a shared axis provides valuable information regarding the dynamic code that temporal spike patterns carry.

In general, trials are arranged vertically in the raster structure, where each row corresponds to the activity sequence of a single trial. The neural activity patterns that correspond to particular stimuli or patterns are evident in the resultant matrix of ticks. As an illustration, a neuron might exhibit consistent firing at specific intervals preceding the go-cue of each trial, or it might fire at a rising rate as a decision threshold approaches. Rough spike timelines generated from raw voltage readings enable raster plots to facilitate the rapid derivation of encoding messages. They are ubiquitous in the study of neural computation, spanning from early sensory processing to higher cognition, due to their practicality.

To generate a raster plot, it is necessary to depict lines or checkboxes at the times of the extracted spikes along a common time axis that spans all trials. MATLAB enables the construction of programmatic pixels by employing functions such as “histc()” and “line()” to transform vectors representing spike times onto a timebase array. Visualising the complete raster plot matrix can be performed through the use of graphics functions such as “image()” and the vertical layering of these spike mappings. A simple mapping between spike occurrences and timesteps is necessary to transform raw data into insightful rasters.

In order to represent the spiking activity of the PANI-proteinoid system in response to different optical stimulation protocols, the measured photoelectrochemical pulse response times were utilised to generate raster diagrams (Fig. 14). Spike events were visually depicted as vertical lines that were recorded at the time of occurrence of the pulse peak for each trial. Under yellow light pulsing at 1 Hz (Fig. 14A), 5 Hz (Fig. 14B), and 20 Hz (Fig. 14C), raster diagrams represented the emergent rhythmicity and synchronicity across trials.





**Fig. 14** Raster plots illustrating the spike timing of neuronal responses to yellow light pulses at varying frequencies. Subplot 1 depicts spike events in response to 1 Hz pulses, subplot 2 shows responses to 5 Hz pulses, and subplot 3 displays the neuronal activity under 20 Hz pulses. Each tick mark along the y-axis represents a separate trial, while the x-axis denotes the time in seconds. The tick marks indicate individual spike events, providing insight into the temporal firing patterns of the neurons under different stimulation conditions.

Spikes clustered into intermittent bursts separated by lengthy inter-pulse intervals when illuminated at 1 Hz. This observed pattern suggests a decreased excitation-recovery cycle that limits reliable response to individual pulses. At 5 Hz, reliable spiking activity occurs with each optical pulse, confirming appropriate tuning to the faster stimulation frequency. However, at 20 Hz the temporal precision deteriorates with variable spike timing and intermittent dropped pulses that disrupt the rhythmic structure.

The capacity to entrain to mid-range frequencies indicates a resonant activation of underlying processes, whereas divergence at higher rates suggests that the relaxation kinetics impose a limit. In general, the raster graphs offer a visual representation of the non-linear mechanisms that control transient phenomena in the neuro-mimetic biosystems under consideration. Reconstructing the intricate modulation of excitability mechanisms in response to diverse input stimulation is the objective of computational modelling.

To reveal fine-grained dynamic structure in the spiking activity of the PANI-proteinoid system, peri-event time histograms (PETHs) were constructed around light pulse onset events (Fig. 15). By mapping average spike counts across trials into discrete time bins spanning stimuli, PETHs allowed inference on input-driven response profiles.

PETHs centered on light pulse initiation showcase the mean activity modulation under 1 Hz (Fig. 15A), 5 Hz (Fig. 15B), and 20 Hz (Fig. 15C) protocols. At 1 Hz, the response features low baseline activity with intermittent bursts lacking temporal precision. This progresses into rhythmic, entrained firing at 5 Hz, before deteriorating into sporadic activity unable to track the elevated 20 Hz frequency.

The differential PETH profiles illustrate the system's tendency for tuning to mid-level frequencies, whereas divergence

at extremely high pulse rates implies the potential emergence of complicated non-linear effects that resemble stochastic resonance phenomena in neurons. Systematically elucidating the mechanisms corresponding to neural excitation, inhibition, and refractoriness in these synthetic networks is possible by employing PETHs to decode input-activated dynamics.

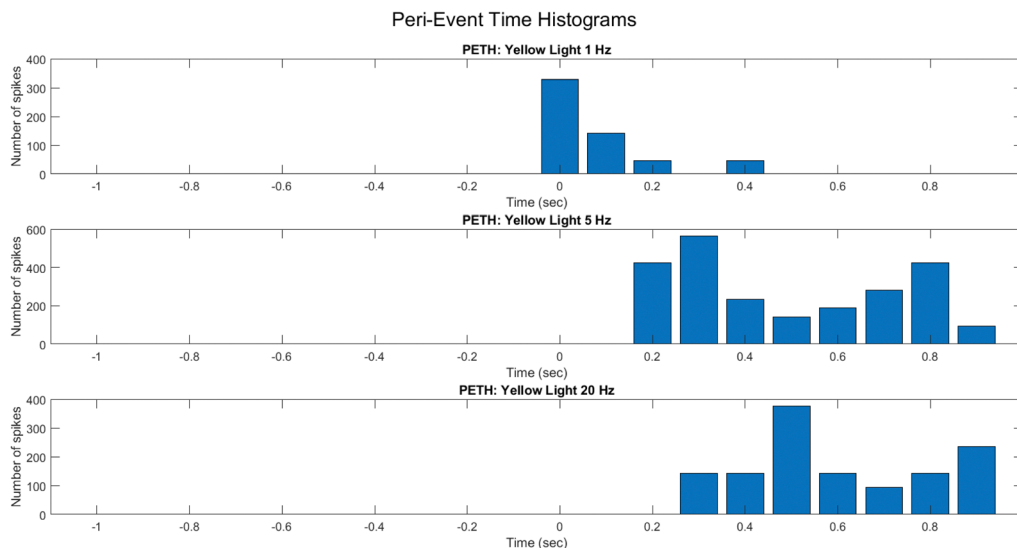
### 3.8. Effect of yellow light pulses in PANI-proteinoid on EEG waves across different frequency bands

We conducted a comparison between the electrical activity of PANI-proteinoid samples and EEG brain waves in order to examine the similarity between them. We examined the similarities in temporal structure and synchronisation patterns between PANI-proteinoid signals and simulated EEG waveforms across several frequency bands. EEG recordings commonly display four distinct frequency bands: delta (0.5–4 Hz), theta (4–8 Hz), alpha (8–13 Hz), and beta (13–30 Hz). We employed cross-correlation analysis to compare the electrical activity of PANI-proteinoid with each simulated brain wave. Signals that are more similar have higher cross-correlation coefficients, which quantify the degree of linear dependence between them. In addition, we determined the lag at which the highest correlation occurred, indicating the temporal alignment of the signal. We discovered intriguing parallels between the electrical dynamics of PANI-proteinoid and brain wave oscillations. These findings suggest that self-assembled nano-fibers can exhibit emergent neural synchronisation and coordination characteristics. Understanding this resemblance has the potential to pave the way for neuromorphic computer architectures and bio-inspired information processing systems.

In order to explore the potential similarity between the spontaneous electrical activity of PANI-proteinoids and brain waves, we conducted a cross-correlation analysis by comparing





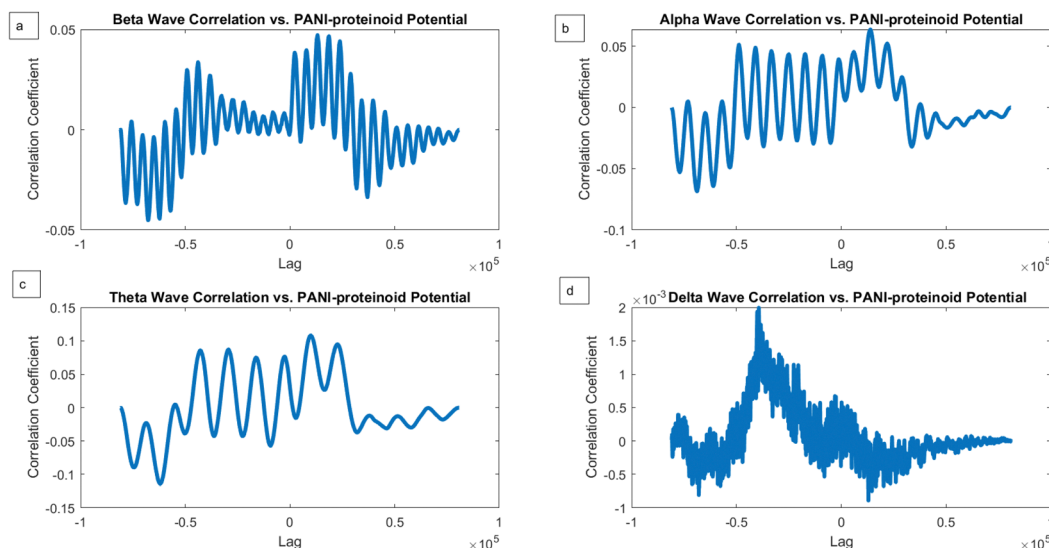


**Fig. 15** A comparison of peri-event time histograms (PETHs) that illustrate the mean neural activity around significant events in the three datasets. Each histogram illustrates the temporal distribution of spike occurrences in the PANI-proteinoid sample with respect to the initiation of movement, as the yellow light pulse frequencies varied. By comparing the neural activity dynamics under various experimental conditions through the examination of neural firing patterns preceding and following the onset of the stimulus using PETHs.

the PANI-proteinoid data with simulated waveforms representing various frequency bands of EEG (Fig. 16). The cross-correlation coefficients measure the degree of linear correlation between the PANI-proteinoid activity and each brain wave, where larger values indicate a greater level of similarity.

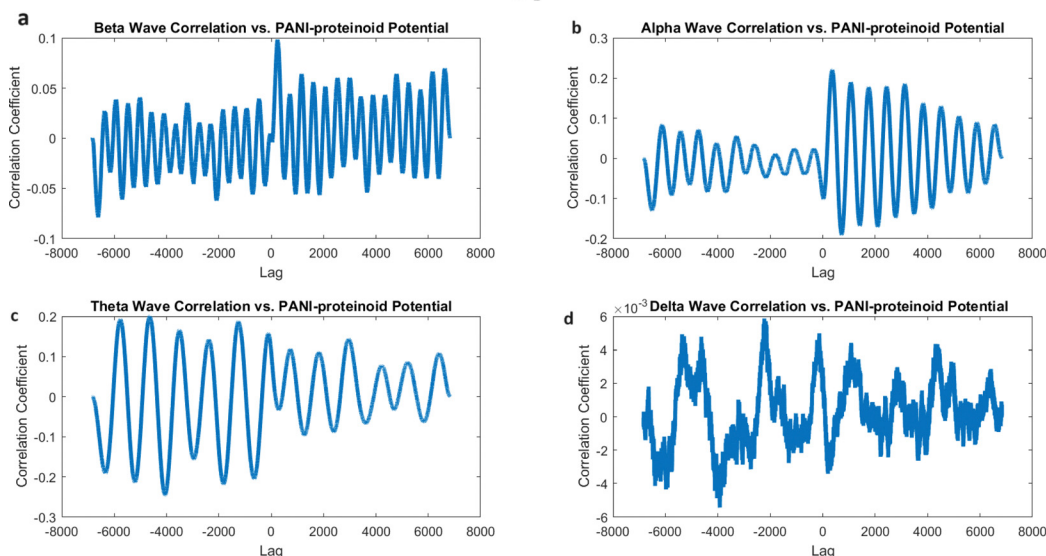
The findings of our study demonstrate varying degrees of connection strengths within different frequency bands. The

theta waves (4–8 Hz) showed the strongest association, with a value of 0.1080 (Fig. 16c). This discovery implies a possible similarity in the timing and coordination patterns between the electrical activity of PANI-proteinoid and the rhythmic behaviour linked to cognitive processes in the brain. Alpha waves, which have a frequency range of 8–13 Hz, showed the second-highest correlation with a coefficient of 0.0637 (Fig. 16b). Beta



**Fig. 16** Analysis of the cross-correlation between the electrical activity of PANI-proteinoids and simulated brain waves. (a) Accumulated correlation coefficient of 0.0472 between PANI-proteinoid data and beta waves (13–30 Hz) via cross-correlation. (b) Alpha waves (8–13 Hz) cross-correlate PANI-proteinoid data, yielding a correlation coefficient of 0.0637. (c) PANI-proteinoid data cross-correlation with theta waves (4–8 Hz), with the maximum correlation coefficient of 0.1080. (d) PANI-proteinoid data cross-correlation with delta waves (0.5–4 Hz), with the least significant correlation coefficient of 0.0020. Different correlation strengths indicate that the PANI-proteinoid dynamics and particular brain wave patterns share distinct similarities. The prominent correlation with theta waves indicates a potential parallel in the temporal structure and synchronization of PANI-proteinoid electrical activity and the oscillatory behavior associated with cognitive processes in the brain.

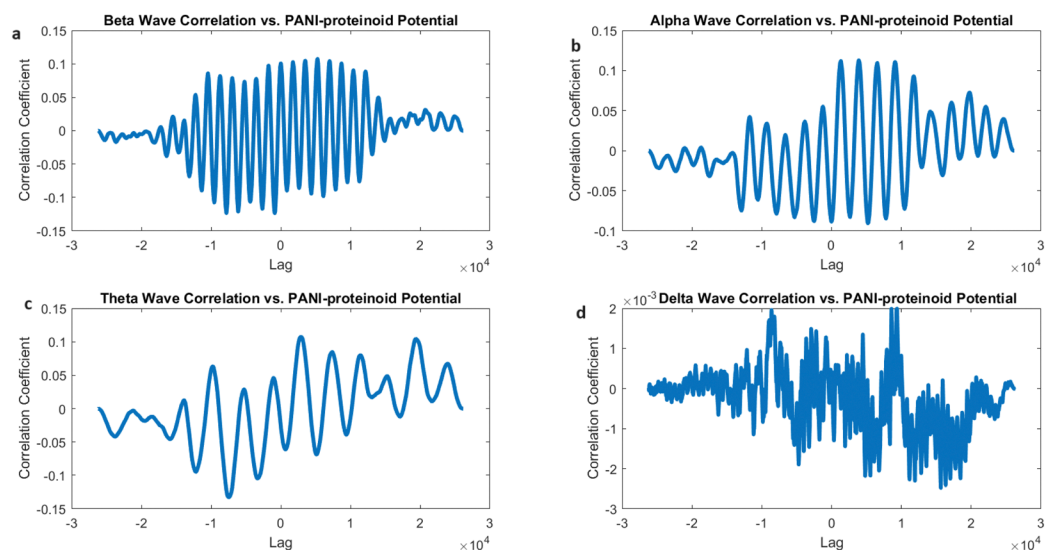




**Fig. 17** Analysis of the cross-correlation between the electrical activity of PANI-proteinoids and simulated brain waves under 5 Hz yellow light illumination. (a) The observed correlation coefficient between PANI-proteinoid data and beta waves (13–30 Hz) is 0.0984. (b) Cross-correlation with alpha waves (8–13 Hz) yields the highest correlation coefficient of 0.2207, indicating that PANI-proteinoid activity and alpha oscillations share a more pronounced similarity in temporal patterns. (c) The correlation coefficient of 0.1995 between the cross-correlation and theta waves (4–8 Hz) indicates a moderate alignment with the dynamics of the theta band. (d) Cross-correlation with delta waves (0.5–4 Hz) demonstrates the least significant correlation coefficient of 0.0059, suggesting that there is little resemblance to sluggish delta oscillations. The observation that the optically stimulated PANI-proteinoid nanofibers correlate more strongly with alpha waves when illuminated at 5 Hz indicates that these nanofibers might demonstrate emergent dynamics comparable to the oscillatory patterns observed in the brain during the early phases of sleep and relaxed consciousness.

waves, which have a frequency range of 13–30 Hz, had a coefficient of 0.0472 (Fig. 16a). The delta waves (0.5–4 Hz) exhibited the lowest correlation, with a value of 0.0020 (Fig. 16d).

Although cross-correlation analysis offers insights on the similarity between PANI-proteinoid activity and brain waves, it is crucial to take into account the statistical significance of



**Fig. 18** Analysed the cross-correlation between the electrical activity of PANI-proteinoid during 20 Hz yellow light stimulation and simulated brain waves. (a) The cross-correlation between PANI-proteinoid data and beta waves (13–30 Hz) results in a correlation coefficient of 0.1073. (b) The cross-correlation analysis with alpha waves (8–13 Hz) shows a correlation coefficient of 0.1128, demonstrating a minor preference for synchronisation with alpha-band oscillations. (c) The cross-correlation analysis using theta waves (4–8 Hz) reveals a correlation coefficient of 0.1074, which is comparable to the correlation observed in the beta-band. (d) The cross-correlation analysis with delta waves (0.5–4 Hz) reveals a correlation coefficient of 0.0020, indicating a limited level of alignment with the slow delta oscillations. The correlation coefficients between beta, alpha, and theta bands, when stimulated under 20 Hz, suggest that the synchronisation of PANI-proteinoid activity is spread out and aligned with higher-frequency brain wave patterns. This discovery implies that the use of high-frequency optical stimulation can potentially trigger a state of increased alertness and cognitive functioning in the PANI-proteinoid system, similar to the mental states linked to beta and alpha brain oscillations.



these correlations. The correlation coefficients obtained, which range from 0.0020 to 0.1080, are relatively low and do not suggest a significant linear link between the signals. In order to ascertain the statistical significance of these connections, more analysis, such as hypothesis testing and careful consideration of the sample size, would be required.

However, when PANI-proteinoids are exposed to yellow light with a frequency of 5 Hz (Fig. 17), the cross-correlation analysis produces clear and separate outcomes. The correlation coefficients demonstrate a significant rise in all frequency bands as compared to the spontaneous activity. Remarkably, the strongest link is currently reported with alpha waves (0.2207), followed by theta waves (0.1995) and beta waves (0.0984). The correlation coefficient with delta waves is relatively low, with a value of 0.0059.

The increased correlation seen between alpha waves and the lighting of PANI-proteinoid nanofibers with frequencies below 5 Hz suggests that these nanofibers activated by light may display emergent dynamics that closely match the rhythmic patterns observed during relaxed alertness and early sleep stages in the brain. The change in correlation strengths suggests that the external visual stimulation influences the timing and coordination of PANI-proteinoid electrical activity, potentially leading to a closer resemblance to alpha-band oscillations.

The cross-correlation examination of the electrical activity of PANI-proteinoids under 20 Hz yellow light stimulation and simulated brain waves revealed interesting patterns of synchronisation (Fig. 18). The correlation coefficients for beta waves (0.1073), alpha waves (0.1128), and theta waves (0.1074) demonstrate a fairly even distribution, indicating that PANI-proteinoid activity is dispersedly aligned with higher-frequency brain wave patterns (Fig. 18a–c). Significantly, the slightly elevated connection with alpha waves suggests a little inclination towards synchronisation with oscillations linked to a state of relaxed wakefulness and the initial phases of sleep.

On the other hand, the correlation with delta waves (0.0020) is still very low (Fig. 18d), indicating that there is only a little degree of similarity with the slow oscillations that are usually seen during deep sleep. This discovery indicates that the use of high-frequency optical stimulation at 20 Hz can potentially trigger a state of increased alertness and cognitive processing in the PANI-proteinoid system, similar to the cognitive states linked to beta and alpha oscillations in the brain.

The correlation coefficients between beta, alpha, and theta bands, when stimulated below 20 Hz (Fig. 18), show a generally balanced relationship. This is in contrast to the observed correlation mostly with alpha waves when stimulated at 5 Hz (Fig. 17). This comparison demonstrates how optical stimulation modulates the dynamics of PANI-proteinoid in a frequency-dependent manner. When the brain is stimulated at a frequency of 5 Hz, it becomes more comparable to alpha-band oscillations, which can help promote a state of relaxation. On the other hand, when the brain is stimulated at a frequency of 20 Hz, it becomes more synchronised throughout higher-frequency bands, indicating increased cognitive processing.

## 4. Discussion

This study shows the complex dynamics and tunable spiking behaviour of PANI-proteinoid nanofiber networks when exposed to different optical stimulation frequencies. The results have significant implications for understanding the emergence of complex functionalities in neuromorphic materials as well as developing adaptable, brain-inspired computing systems.

Different driving frequencies induced different kinds of photoelectrochemical responses, as shown in Table 2 by the hierarchical clustering analysis. Significantly, the shift from irregular bursting at 1 Hz to unsustained bursting at 20 Hz, followed by rhythmic synchronisation at 5 Hz, mimics the frequency-dependent adaptations that have been observed in biological neurons.<sup>43,44</sup> This indicates that the PANI-proteinoid networks exhibit intrinsic plasticity in which the temporal patterns of the input stimuli influence the excitability and refractory dynamics.

The amplitudes and coefficient of variation ( $C_V$ ) of the inter-spike intervals were used as a quantitative indicator of the spiking temporal regularity and consistency. Furthermore, the  $C_V$  values showed non-monotonic variation in relation to the driving frequency, suggesting the presence of a complex relationship between the time scales of stimulation and the inherent relaxation dynamics of the nanofibers.

Previous research in the field of neuroscience have established that the  $C_V$  of neural spiking is based upon the adaptation currents,<sup>45</sup> the relative contributions of excitatory and inhibitory inputs,<sup>46</sup> and the membrane time constant.<sup>47</sup> An examination of these variables within the framework of PANI-proteinoid networks may provide significant knowledge regarding the sources of stochastic variability and its operational function in encoding information. The forest-fire cellular automata model effectively represented the propagation of spatio-temporal activity within the nanofiber networks. Through the manipulation of ignition and recovery probabilities for individual nodes in response to variations in illumination frequency, we successfully replicated the synchronisation patterns and emergent spike clusters. This finding provides further evidence in favour of the concept that optical stimulation can adjust internal dynamics and network connectivity, thereby enabling the manipulation of self-organised activity. Further research may utilise this potential to manipulate neuromorphic computations in a way that facilitates pattern recognition, decision making, and memory formation.<sup>48</sup>

**Table 2** Summary of frequency-dependent spiking dynamics in PANI-proteinoid networks

Frequency (Hz)	Spiking regime	Inter-spike interval $C_V$	Amplitude $C_V$
1	Irregular bursting	0.55	0.46
5	Rhythmic entrainment	0.36	0.93
20	Unsustained spiking	0.42	0.47



**Table 3** Oscillation metrics under optical stimulation (yellow light 1 Hz). Structured variation of spike amplitude envelopes around 0.56 mV and a concentrated periodicity distribution around a 1067 s rhythm imply strong coordination of signalling dynamics

Period (s)	Amplitude (mV)
725	0.20
679	0.24
573	0.24
749	0.24
591	0.22
657	0.30
688	0.32
618	0.26
626	0.32
601	0.32
733	0.30
647	0.26
803	0.35
629	0.40
650	0.41
618	0.39
632	0.50
613	0.21
627	0.35
593	0.36
620	0.37
667	0.40
608	0.28

Being able to manipulate the spiking dynamics of PANI-proteinoid networks optically presents promising prospects for the advancement of neuromorphic computing and sensing platforms. One potential application of frequency-dependent entrainment is the implementation of selective attention mechanisms, which involve amplifying relevant stimuli at particular frequencies while suppressing others.<sup>49</sup> Furthermore, the materials' capacity to support complex dynamics and high-dimensional parameter spaces may facilitate the development of reservoir computing methods for time-series classification and prediction tasks.<sup>3</sup>

In addition, because of their biocompatibility and ability to self-assemble, PANI-proteinoid nanofibers are highly promising for biomedical applications and bioelectronic interfaces. The integration of neuromorphic materials with flexible electronics and wearable devices has the potential to enable the development of brain-inspired, adaptive sensors and actuators

**Table 4** Sample recorded oscillation periods and amplitudes for PANI-proteinoid complexes under 5 Hz yellow light driving

Period (s)	Amplitude (mV)
831	0.41
717	0.072
406	0.03849
396	0.03977
437	0.06767
496	0.13047
802	0.20653
157	0.00626
437	0.07113
644	0.18515
647	0.0827
688	0.10324

**Table 5** Periods in seconds and amplitudes in mV for PANI-proteinoid under yellow light illumination at 20 Hz

Period (s)	Amplitude (mV)
658	0.3945
656	0.5292
713	0.6238
719	0.5799
708	0.5222
918	0.7075
631	0.5229
932	0.5171
1911	0.5727
774	0.4165
708	0.9097
400	0.4793
1107	0.5013
678	0.3746
654	0.4345
393	2.01
572	1.0686
612	0.5254
665	0.9668
1437	0.3675
551	0.8866
723	0.8469
851	1.4036
817	1.2298
1433	1.181
811	1.5022
134	1.002
554	0.9346
724	0.8634
720	0.9152
505	0.6378
698	0.7072
721	0.91896
641	0.6344

capable of seamless interaction with biological systems.<sup>50</sup> The formation of memories, decision-making, and pattern recognition are examples of desired neuromorphic computations.<sup>48</sup> Neuromorphic engineering, which mimics the brain's computational principles in artificial systems, presents exciting new possibilities because to PANI-proteinoid nanofibers. These nanofibers are excellent for many applications due to their

**Table 6** FT-IR peak positions and intensities of PANI synthesized using ferrous nitrate as an oxidant

Peak position-wavenumber (cm <sup>-1</sup> )	Intensity
402.60	0.171
409.04	0.178
424.37	0.167
442.44	0.172
469.64	0.161
511.96	0.159
527.30	0.159
1052.28	0.103
1216.93	0.158
1228.87	0.149
1365.58	0.149
1510.42	0.0978
1581.13	0.0968
1738.53	0.173
2921.68	0.136
2970.00	0.135





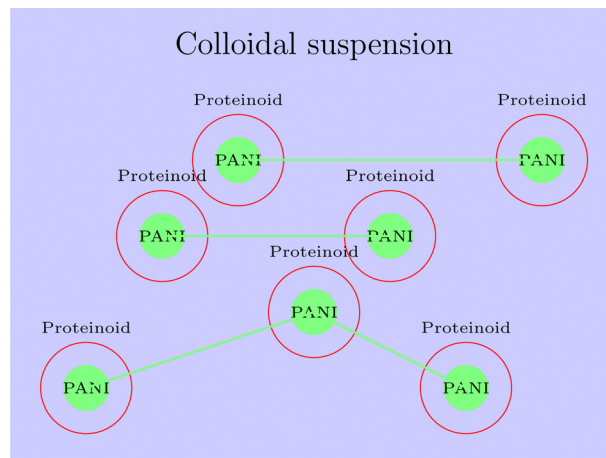
**Table 7** FT-IR peak positions and intensities of PANI synthesized using ammonium persulfate as an oxidant

Peak position (cm <sup>-1</sup> )	Intensity
409.32	0.339
420.63	0.331
510.74	0.349
565.95	0.348
681.41	0.344
740.87	0.312
813.71	0.307
1007.94	0.317
1031.97	0.317
1119.87	0.337
1150.09	0.340
1216.94	0.361
1228.42	0.348
1288.03	0.299
1365.38	0.309
1443.96	0.318
1488.90	0.339
1566.02	0.279
1738.29	0.289
2970.03	0.252

frequency-dependent entrainment and complicated dynamics when optically stimulated.

- **Adaptive sensing:** in machine olfaction, tactile sensing, and event-based vision, adaptive sensors can process and classify complex spatiotemporal patterns in real time using optically-stimulated PANI-proteinoid nanofibers' frequency-dependent entrainment and complex dynamics.
- **Bioelectronic interfaces:** PANI-proteinoid nanofibers are attractive biological system interfaces due to their biocompatibility and self-assembly. They create adaptive, brain-inspired interfaces for neural prosthetics, biosensors, and closed-loop neuromodulation when combined with flexible electronics and wearable devices.
- **Neuromorphic robotics:** robots can learn, adapt, and analyse sensory data using PANI-proteinoid networks as neuromorphic controllers. This could lead to autonomous robots for exploration, search and rescue, and human-robot interaction in dynamic and unstructured environments.

The PANI-proteinoid composite, depicted in Fig. 19, demonstrates a distinctive mechanism that integrates the conductive characteristics of PANI nanoparticles with the encapsulation and stabilisation characteristics of proteinoids. This combination of components results in improved electrical characteristics and creates opportunities for a wide range of potential uses. An essential feature of the PANI-proteinoid mechanism is the creation of a conductive network within the composite. The figure shows the interconnected PANI nanoparticles, represented in green, which facilitate efficient electron transfer and enhance electrical conductivity. The interconnections among the PANI nanoparticles facilitate the formation of conductive channels, hence enhancing the movement of electric charges across the composite material. Another vital component of the method involves the containment of the PANI nanoparticles within the proteinoid microspheres, which are seen in red. The proteinoids encapsulate and stabilise the PANI



**Fig. 19** The diagram shows colloidal suspensions of PANI nanoparticles and proteinoid microspheres. PANI nanoparticles are green, proteinoid proteinoids are red. Blue indicates colloidal suspension. The composite's PANI nanoparticle connections form a conductive network. This diagram shows how to efficiently create colloidal suspensions of PANI nanoparticles encapsulated and interconnected by proteinoid microspheres, which improves electrical characteristics and has several applications.

nanoparticles, inhibiting their aggregation and ensuring a uniform dispersion within the colloidal suspension. Enclosing the composite material not only increases its stability but also creates a protective barrier that boosts the adaptability and effectiveness of the PANI nanoparticles in different surroundings.

## 5. Conclusion

We examined the emergent electrical signalling of PANI-proteinoid nanofiber networks under diverse optical stimulation conditions. We used pulsed yellow light at 1, 5, and 20 Hz to alter excitation-relaxation dynamics and spike train patterns in these neuromorphic composites. Hierarchical clustering of photoelectrochemical reaction data revealed driving frequency-induced activity patterns. Nanofibers displayed irregular spike bursts with long inter-pulse intervals at 1 Hz, indicating a delayed recovery cycle that couldn't track input. Increasing stimulation to 5 Hz gave the network rhythmic oscillations with optical pulse train-locked spiking. Refractory dynamics decreased firing rates at 20 Hz, generating stochastic spiking and temporal coordination problems. Raster plots and perievent time histograms showed irregular, rhythmic, and complex nonlinear dynamics like biological neural networks. To model spatiotemporal activity propagation, we treated the PANI-proteinoid system as a forest-fire cellular automata with illumination frequency influencing node ignition and recovery probability. These findings show that PANI-proteinoid nanofibers could be hardware equivalents of biological brain networks, with photonic stimulation enabling flexible information encoding. We found optical control over self-organized neuromorphic dynamics in PANI-proteinoid nanofibers, which is a big step towards unconventional, life-like computers and brain-interface materials.



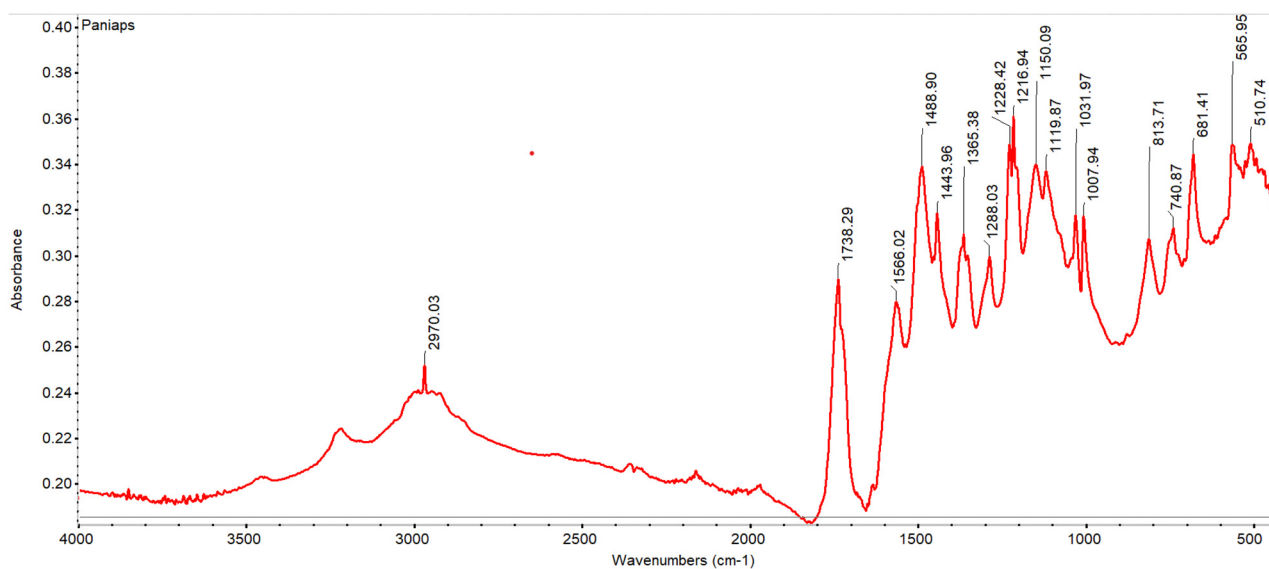
## Conflicts of interest

There are no conflicts to declare.

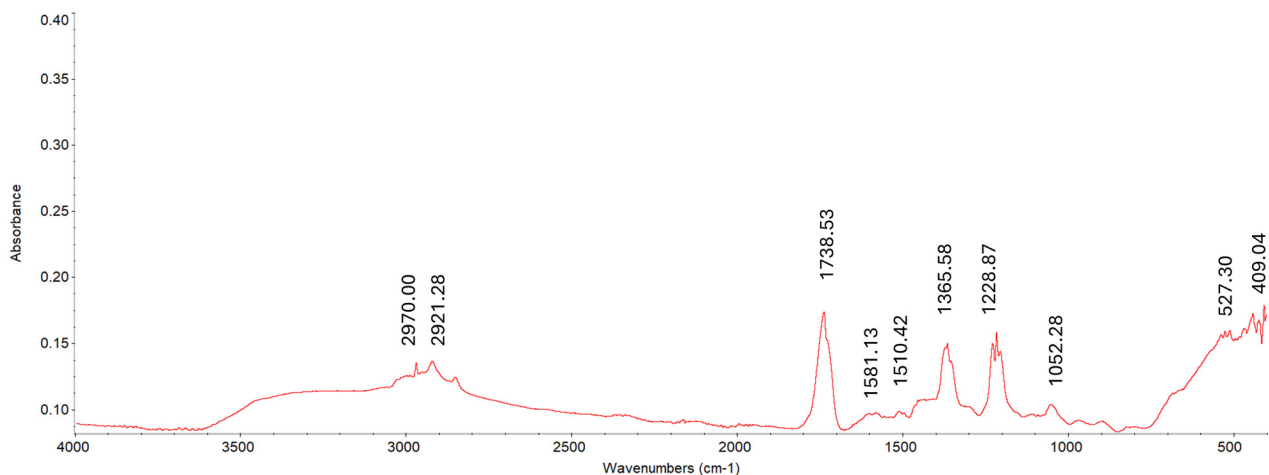
## Appendices

The FT-IR spectrum of PANIAPS (Fig. 20a) exhibits characteristic absorption bands associated with PANI. The peaks at  $1566.02\text{ cm}^{-1}$  and  $1488.90\text{ cm}^{-1}$  correspond to the C=C stretching vibrations of the quinoid and benzenoid rings, respectively. The peak at  $1365.38\text{ cm}^{-1}$  is attributed to the C–N stretching vibration in the quinoid imine units. The absorption bands at  $1216.94\text{ cm}^{-1}$  and  $1150.09\text{ cm}^{-1}$  are assigned to the C–H in-plane bending vibrations of the quinoid and benzenoid rings, respectively. The peaks at  $1031.97\text{ cm}^{-1}$

and  $813.71\text{ cm}^{-1}$  are associated with the out-of-plane bending vibrations of C–H in the substituted benzenoid rings. On the other hand, the FT-IR spectrum of PANInitrate (Fig. 20b) shows some similarities to PANIAPS but with notable differences. The absorption bands at  $1581.13\text{ cm}^{-1}$  and  $1510.42\text{ cm}^{-1}$  correspond to the C=C stretching vibrations of the quinoid and benzenoid rings, respectively. However, the relative intensities of these peaks are different compared to PANIAPS, suggesting a variation in the proportion of quinoid and benzenoid units in the polymer chain. The peak at  $1365.58\text{ cm}^{-1}$  is attributed to the C–N stretching vibration in the quinoid imine units, similar to PANIAPS. The absorption bands at  $1228.87\text{ cm}^{-1}$  and  $1216.93\text{ cm}^{-1}$  are assigned to the C–H in-plane bending vibrations of the quinoid and benzenoid rings, respectively. A notable difference between the two spectra is the presence of



(a) PANIAPS



(b) PANInitrate

**Fig. 20** FT-IR spectra of PANI synthesized using (a) ammonium persulfate (PANIAPS) and (b) ferrous nitrate (PANInitrate) as oxidizing agents.



a strong absorption band at  $1738.53\text{ cm}^{-1}$  in PANIntrate, which is absent in PANIAPS. This peak is typically associated with the C=O stretching vibration of carbonyl groups, indicating the presence of oxidized structures or impurities in PANIntrate. However, upon closer inspection, both PANIAPS and PANIntrate clearly display an absorption band at approximately  $1738\text{ cm}^{-1}$ , although with varying intensities. The absorbance of the peak at  $1738.53\text{ cm}^{-1}$  is around 0.28 in PANIAPS and roughly 0.17 in PANIntrate. The presence of oxidised structures or impurities in both PANI samples is indicated by the absorption band, which is normally linked with the C=O stretching vibration of carbonyl groups. However, the extent of this presence differs between the two samples. There are also differences in the absorption bands below  $1000\text{ cm}^{-1}$  between PANIAPS and PANIntrate. The PANIAPS sample exhibits strong peaks at  $565.95\text{ cm}^{-1}$  and  $510.74\text{ cm}^{-1}$ , whereas the PANIntrate sample shows observed peaks at  $527.30\text{ cm}^{-1}$  and  $511.96\text{ cm}^{-1}$ . The observed differences indicate changes in the patterns of substitution and the presence of different functional groups in the two PANI samples.

## Data availability

The data for the paper has been uploaded to the Zenodo database. You can access the data through the following link: [\[https://zenodo.org/records/10808307\]](https://zenodo.org/records/10808307).

## References

- 1 G. Indiveri and T. K. Horiuchi, Frontiers in neuromorphic engineering, *Front. Neurosci.*, 2011, **5**, 13375.
- 2 D. Marković, A. Mizrahi, D. Querlioz and J. Grollier, Physics for neuromorphic computing, *Nat. Rev. Phys.*, 2020, **2**(9), 499–510.
- 3 G. Tanaka, T. Yamane, J. B. Héroux, R. Nakane, N. Kanazawa, S. Takeda, H. Numata, D. Nakano and A. Hirose, Recent advances in physical reservoir computing: A review, *Neural Networks*, 2019, **115**, 100–123.
- 4 J. D. Kendall and S. Kumar, The building blocks of a brain-inspired computer, *Appl. Phys. Rev.*, 2020, **7**(1), 011305.
- 5 S. Stafström, J. Bredas, A. Epstein, H. Woo, D. Tanner, W. Huang and A. MacDiarmid, Polaron lattice in highly conducting polyaniline: Theoretical and optical studies, *Phys. Rev. Lett.*, 1987, **59**(13), 1464.
- 6 J. Huang, Syntheses and applications of conducting polymer polyaniline nanofibers, *Pure Appl. Chem.*, 2006, **78**(1), 15–27.
- 7 D. Li, J. Huang and R. B. Kaner, Polyaniline nanofibers: a unique polymer nanostructure for versatile applications, *Acc. Chem. Res.*, 2009, **42**(1), 135–145.
- 8 B. Ertekin, Z. Cimen, H. Yilmaz and U. Yilmaz, Synthesis and characterization of polyaniline/ignimbrite nanocomposite material, *J. Mater. Sci. Eng.*, 2016, **5**, 1000237.
- 9 M. J. Antony and M. Jayakannan, Polyaniline nanoscaffolds for colorimetric sensing of biomolecules *via* electron transfer process, *Langmuir*, 2011, **27**(10), 6268–6278.
- 10 S. Er, U. Laraib, R. Arshad, S. Sargazi, A. Rahdar, S. Pandey, V. K. Thakur and A. M. Díez-Pascual, Amino acids, peptides, and proteins: implications for nanotechnological applications in biosensing and drug/gene delivery, *Nanomaterials*, 2021, **11**(11), 3002.
- 11 M. Karimi, M. Rabiee, M. Tahriri, R. Salarian and L. Tayebi, A graphene based-biomimetic molecularly imprinted polyaniline sensor for ultrasensitive detection of human cardiac troponin t (ctnt), *Synth. Met.*, 2019, **256**, 116136.
- 12 R. Asmatulu, Z. Veisi, M. N. Uddin and A. Mahapatro, Highly sensitive and reliable electrospun polyaniline nanofiber based biosensor as a robust platform for COX-2 enzyme detections, *Fibers Polym.*, 2019, **20**, 966–974.
- 13 L. Tian, M. P. Prabhakaran and S. Ramakrishna, Strategies for regeneration of components of nervous system: scaffolds, cells and biomolecules, *Regener. Biomater.*, 2015, **2**(1), 31–45, DOI: [10.1093/rb/rbu017](https://doi.org/10.1093/rb/rbu017).
- 14 S. H. Bhang, S. I. Jeong, T.-J. Lee, I. Jun, Y. B. Lee, B.-S. Kim and H. Shin, Electroactive electrospun polyaniline/poly [(l-lactide)-co-(ε-caprolactone)] fibers for control of neural cell function, *Macromol. Biosci.*, 2012, **12**(3), 402–411.
- 15 V. Erokhin, T. Berzina and M. P. Fontana, Hybrid electronic device based on polyaniline-polyethyleneoxide junction, *J. Appl. Phys.*, 2005, **97**(6), 064501.
- 16 V. Erokhin, T. Berzina, K. Gorshkov, P. Camorani, A. Pucci, L. Ricci, G. Ruggeri, R. Sigala and A. Schüz, Stochastic hybrid 3d matrix: learning and adaptation of electrical properties, *J. Mater. Chem.*, 2012, **22**(43), 22881–22887.
- 17 G. Baldi, S. Battistoni, G. Attolini, M. Bosi, C. Collini, S. Iannotta, L. Lorenzelli, R. Mosca, J. Ponraj and R. Verucchi, *et al.*, Logic with memory: and gates made of organic and inorganic memristive devices, *Semicond. Sci. Technol.*, 2014, **29**(10), 104009.
- 18 V. Demin, V. Erokhin, A. Emelyanov, S. Battistoni, G. Baldi, S. Iannotta, P. Kashkarov and M. Kovalchuk, Hardware elementary perceptron based on polyaniline memristive devices, *Org. Electron.*, 2015, **25**, 16–20.
- 19 A. Emelyanov, D. Lapkin, V. Demin, V. Erokhin, S. Battistoni, G. Baldi, A. Dimonte, A. Korovin, S. Iannotta and P. Kashkarov, *et al.*, First steps towards the realization of a double layer perceptron based on organic memristive devices, *AIP Adv.*, 2016, **6**(11), 111301.
- 20 D. Lapkin, A. Emelyanov, V. Demin, T. Berzina and V. Erokhin, Spike-timing-dependent plasticity of polyaniline-based memristive element, *Microelectron. Eng.*, 2018, **185**, 43–47.
- 21 V. Erokhin, T. Berzina, A. Smerieri, P. Camorani, S. Erokhina and M. P. Fontana, Bio-inspired adaptive networks based on organic memristors, *Nano Commun. Networks*, 2010, **1**(2), 108–117.
- 22 N. V. Prudnikov, D. A. Lapkin, A. V. Emelyanov, A. A. Minnekhanov, Y. N. Malakhova, S. N. Chvalun, V. A. Demin and V. V. Erokhin, Associative stdp-like learning of



- neuromorphic circuits based on polyaniline memristive microdevices, *J. Phys. D: Appl. Phys.*, 2020, **53**(41), 414001.
- 23 E. Juzekaeva, A. Nasretudinov, S. Battistoni, T. Berzina, S. Iannotta, R. Khazipov, V. Erokhin and M. Mukhtarov, Coupling cortical neurons through electronic memristive synapse, *Adv. Mater. Technol.*, 2019, **4**(1), 1800350.
  - 24 A. Chiolerio, E. Garofalo, N. Phillips, E. Falletta, R. de Oliveira and A. Adamatzky, Learning in colloidal polyaniline nanorods, *Results Phys.*, 2024, **58**, 107501, DOI: [10.1016/j.rinp.2024.107501](https://doi.org/10.1016/j.rinp.2024.107501).
  - 25 K. Harada and S. W. Fox, The thermal condensation of glutamic acid and glycine to linear peptides<sup>1</sup>, *J. Am. Chem. Soc.*, 1958, **80**(11), 2694–2697.
  - 26 S. W. Fox, Thermal proteins in the first life and in the “mind-body” problem, *Evolution of Information Processing Systems*, Springer, 1992, pp. 203–228.
  - 27 A. T. Przybylski, Excitable cell made of thermal proteinoids, *BioSystems*, 1985, **17**(4), 281–288.
  - 28 Y. Ishima, A. T. Przybylski and S. W. Fox, Electrical membrane phenomena in spherules from proteinoid and lecithin, *BioSystems*, 1981, **13**(4), 243–251.
  - 29 A. T. Przybylski, W. P. Stratten, R. M. Syren and S. W. Fox, Membrane, action, and oscillatory potentials in simulated protocells, *Naturwissenschaften*, 1982, **69**(12), 561–563.
  - 30 Y. Bi, A. Pappelis, C. S. Sikes and S. W. Fox, Evidence that the protocell was also a protoneuron, *Orig. Life Evol. Biosph.*, 1994, **24**(2–4).
  - 31 E. Niedermeyer, Ultrafast eeg activities and their significance, *Clin. EEG Neurosci.*, 2005, **36**(4), 257.
  - 32 L. Spyrou, S. Sanei and C. C. Took, *Estimation and location tracking of the p300 subcomponents from single-trial eeg*, in: 2007 IEEE International Conference on Acoustics, Speech and Signal Processing-ICASSP'07, IEEE, 2007, vol. 2, pp. II-1149.
  - 33 M. Teplan, *et al.*, Fundamentals of eeg measurement, *Meas. Sci. Rev.*, 2002, **2**(2), 1–11.
  - 34 Z. Wang, X. Wang and Z. Zeng, Memristive circuit design of brain-like emotional learning and generation, *IEEE Trans. Cybern.*, 2021, **53**(1), 222–235.
  - 35 P. Mougkogiannis, N. Phillips and A. Adamatzky, Transfer functions of proteinoid microspheres, *BioSystems*, 2023, **227**, 104892.
  - 36 S. Xiong, J. Lan, S. Yin, Y. Wang, Z. Kong, M. Gong, B. Wu, J. Chu, X. Wang and R. Zhang, *et al.*, Enhancing the electrochromic properties of polyaniline via coordinate bond tethering the polyaniline with gold colloids, *Sol. Energy Mater. Sol. Cells*, 2018, **177**, 134–141.
  - 37 E. Kang, K. Neoh and K. Tan, Polyaniline: a polymer with many interesting intrinsic redox states, *Prog. Polym. Sci.*, 1998, **23**(2), 277–324.
  - 38 L. Chen, L.-J. Sun, F. Luan, Y. Liang, Y. Li and X.-X. Liu, Synthesis and pseudocapacitive studies of composite films of polyaniline and manganese oxide nanoparticles, *J. Power Sources*, 2010, **195**(11), 3742–3747.
  - 39 J. Masters, Y. Sun, A. MacDiarmid and A. Epstein, Polyaniline: allowed oxidation states, *Synth. Met.*, 1991, **41**(1–2), 715–718.
  - 40 S. Bhadra, D. Khastgir, N. K. Singha and J. H. Lee, Progress in preparation, processing and applications of polyaniline, *Prog. Polym. Sci.*, 2009, **34**(8), 783–810.
  - 41 V. Erokhin, Polymer-based adaptive networks, *The New Frontiers of Organic and Composite Nanotechnology*, Elsevier, 2008, pp. 287–353.
  - 42 S. Battistoni, V. Erokhin and S. Iannotta, Organic memristive devices for perceptron applications, *J. Phys. D: Appl. Phys.*, 2018, **51**(28), 284002.
  - 43 E. M. Izhikevich, Which model to use for cortical spiking neurons?, *IEEE Trans. Neural Networks*, 2004, **15**(5), 1063–1070.
  - 44 W. Senn and S. Fusi, Learning only when necessary: better memories of correlated patterns in networks with bounded synapses, *Neural Comput.*, 2005, **17**(10), 2106–2138.
  - 45 Y.-H. Liu and X.-J. Wang, Spike-frequency adaptation of a generalized leaky integrate-and-fire model neuron, *J. Comput. Neurosci.*, 2001, **10**, 25–45.
  - 46 M. N. Shadlen and W. T. Newsome, The variable discharge of cortical neurons: implications for connectivity, computation, and information coding, *J. Neurosci.*, 1998, **18**(10), 3870–3896.
  - 47 T. W. Troyer and K. D. Miller, Physiological gain leads to high isi variability in a simple model of a cortical regular spiking cell, *Neural Comput.*, 1997, **9**(5), 971–983.
  - 48 D. V. Christensen, R. Dittmann, B. Linares-Barranco, A. Sebastian, M. Le Gallo, A. Redaelli, S. Slesazek, T. Mikolajick, S. Spiga and S. Menzel, *et al.*, 2022 roadmap on neuromorphic computing and engineering, *Neuromorphic Comput. Eng.*, 2022, **2**(2), 022501.
  - 49 F. Walter, F. Röhrbein and A. Knoll, Neuromorphic implementations of neurobiological learning algorithms for spiking neural networks, *Neural Networks*, 2015, **72**, 152–167.
  - 50 A. Armgarth, S. Pantzare, P. Arven, R. Lassnig, H. Jinno, E. O. Gabrielsson, Y. Kifle, D. Cherian, T. Arbring Sjöström and G. Berthou, *et al.*, A digital nervous system aiming toward personalized iot healthcare, *Sci. Rep.*, 2021, **11**(1), 7757.

