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## A self-amplifying nanodrug to manipulate the Janus-faced nature of ferroptosis for tumor therapy†

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Ferroptosis, an unusual non-apoptotic cell death caused by the iron-dependent accumulation of lipid peroxide, enables the flexible design of an antitumor platform. Specifically, as a positive role, ferroptosis can induce an immune response accompanied with the interferon- $\gamma$  (IFN- $\gamma$ )-triggered disruption of the glutathione peroxidase 4 pathway for cascade enhancement of ferroptotic cell death and ferroptosis-induced immunotherapeutic efficacy. However, as a negative role, ferroptosis also triggers inflammation-associated immunosuppression by up-regulation of the cyclooxygenase-2/prostaglandin E<sub>2</sub> pathway and IFN- $\gamma$ -associated adaptive immune resistance by up-regulation of programmed death ligand-1 (PD-L1), impeding the antitumor efficacy of multiple immune cells by immune escape. Negative and positive roles endow ferroptosis with a Janus-faced nature. It is urgent to manipulate the Janus-faced nature of ferroptosis for eliciting the maximized ferroptotic therapeutic efficacy. Herein, a self-amplifying nanodrug (RCH NPs) was designed by co-assembling hemin (ferric porphyrin), celecoxib (anti-inflammatory drug) and roscovitine (cyclin-dependent kinase 5 inhibitor) with the assistance of human serum albumin for reprogramming the Janus-faced nature of ferroptosis. During hemin-triggered ferroptosis, celecoxib disrupted the inflammation-related immunosuppression while roscovitine destroyed the IFN- $\gamma$ -induced up-regulation of PD-L1 via the genetic blockade effect. The RCH NPs thus demonstrated superior therapeutic effects on tumors, thanks to self-amplifying ferroptotic immunotherapy. Our work offers a conceptually innovative strategy for harnessing ferroptosis against tumors.

### New concepts

Ferroptosis has recently been demonstrated to be a promising approach against tumors. However, ferroptosis has an inherent Janus-faced nature in cancer therapy, compromising its therapeutic efficacy. On the one hand, ferroptosis can inherently trigger the immune response accompanied with disruption of the glutathione peroxidase 4 pathway for realizing a cascade augment of ferroptotic cell death and ferroptotic immunotherapy. On the other hand, ferroptosis also intrinsically induces immune escape, where the triggered up-regulation of cyclooxygenase-2/prostaglandin E<sub>2</sub> and programmed death ligand-1 (PD-L1) significantly suppresses the antitumor efficacy of immune cells. It is of great interest, albeit challenging, to regulate the Janus-faced nature of ferroptosis for realizing an optimal ferroptotic therapy against tumors. Herein, a self-amplifying nanodrug was, for the first time, engineered for reshaping the Janus-faced nature of ferroptosis in cancer therapy. With the cooperation of hemin, celecoxib and roscovitine in the nanodrug, the Janus-faced nature of ferroptosis was powerfully manipulated, demonstrating a potent therapeutic efficacy against tumor progression and metastasis along with the long-lasting immunological memory response. The present nanodrug offers a conceptually innovative approach for manipulating the Janus-faced nature of ferroptosis to elicit the maximized therapeutic efficacy against tumors.

### Introduction

Ferroptosis, a newly discovered form of non-apoptotic cell death, has attracted increasing attention in tumor therapy due to its difference from apoptosis in cell morphology, genetics and biochemistry.<sup>1,2</sup> In the mechanism, ferroptosis is caused by the iron-dependent accumulation of lipid peroxide.<sup>3</sup> Therefore, the iron-based Fenton reaction is a potent approach to induce ferroptosis in tumor cells.<sup>4</sup> As cancer cells have an inherent resistance to apoptosis, ferroptosis provides a more efficient strategy for suppressing tumor progress *via* targeting the non-apoptosis pathway.

In particular, ferroptosis can induce immune response through ferroptotic tumor cells with the exposure of danger-associated molecular patterns (DAMPs) and the release of tumor-associated antigens (TAAs),<sup>5–9</sup> where the secretion of

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interferon- $\gamma$  (IFN- $\gamma$ ) by T cells is stimulated for immunotherapy. Based on the mechanism of T cell-mediated killing,<sup>10–13</sup> the triggered IFN- $\gamma$  makes tumor cells prone to ferroptosis by down-regulating the system  $x_c^-$  (consisting of SLC7A11 and SLC3A2) for glutathione (GSH) synthesis inhibition, wherein the detoxication of lipid peroxide against ferroptosis through the GSH-mediated glutathione peroxidase 4 (GPX4) pathway is disrupted. In a word, the ferroptosis-triggered immune response can boost the efficacy of ferroptosis, and the boosted ferroptosis augments the immune response in turn. Consequently, as a positive role, ferroptosis itself possesses a cascade enhancement of ferroptotic cell death and ferroptosis-induced immunotherapy once ferroptosis is triggered, thanks to the interplay of ferroptosis with the inherent induced IFN- $\gamma$ .

Despite the positive role of ferroptosis in tumor therapy, the intrinsically boosted immunotherapeutic efficacy is far from satisfactory as there also exists an inherent negative role in the ferroptosis-triggered immunotherapy. On the one hand, ferroptosis specifically induces inflammation-associated immunosuppression by up-regulating cyclooxygenase-2 (COX-2) along with the COX-2-derived up-regulation of prostaglandin E<sub>2</sub> (PGE<sub>2</sub>, a proinflammatory factor) in tumor cells.<sup>14–18</sup> As a result, ferroptosis inherently stimulates PGE<sub>2</sub>-based inflammation-associated immunosuppression, upon which ferroptotic tumor cells gain the privilege of immune escape and resistance to immunotherapy, impeding the immunotherapeutic efficacy. On the other hand, although the ferroptosis-induced T cell-secreted IFN- $\gamma$  could kill the tumor cells, it is also an accomplice of adaptive immune resistance, where IFN- $\gamma$  promotes T cell dysfunction through the IFN- $\gamma$ -induced up-regulation of tumoral programmed death ligand-1 (PD-L1) to rescue tumor cells from immune elimination.<sup>19–21</sup> Hence, as a negative role, ferroptosis also inherently elicits immune escape involving inflammation-associated immunosuppression by up-regulation of the COX-2/PGE<sub>2</sub> pathway and IFN- $\gamma$ -associated adaptive immune resistance by up-regulation of PD-L1, resulting in the major obstacle for ferroptotic immunotherapy.

Taken altogether, negative and positive roles endow ferroptosis with a Janus-faced nature, where ferroptosis-driven immune escape is regarded as “a limiting factor”, severely limiting the effectiveness of ferroptosis. Therefore, the design of a ferroptosis-based nanoplatform to manipulate the Janus-faced nature of ferroptosis for eliciting the maximized ferroptotic therapy is in urgent demand.

Herein, for the first time, we rationally designed a self-amplifying nanodrug to reprogram the Janus-faced nature of ferroptosis, which could harness the positive role of ferroptosis along with reversing its negative role to achieve the optimal ferroptotic tumor therapy. Our nanodrug (RCH NPs) is achieved by co-assembling hemin (Hemin, ferric porphyrin), celecoxib (Celeco, a non-steroidal anti-inflammatory drug), and roscovitine (Rosco, a cyclin-dependent kinase 5 (Cdk5) inhibitor) with human serum albumin (HSA). In RCH NPs, hemin acts as a ferroptosis inducer by converting endogenous hydrogen peroxide (H<sub>2</sub>O<sub>2</sub>) into cytotoxic hydroxyl radicals ( $\bullet$ OH) for lipid peroxidation through the Fenton reaction. Celecoxib selectively

inhibits the inflammatory COX-2/PGE<sub>2</sub> pathway that is up-regulated by ferroptosis to relieve inflammation-associated immunosuppression while roscovitine inhibits the Cdk5 pathway to suppress IFN- $\gamma$ -dependent PD-L1 gene transcription and abolish adaptive immune resistance through the genetic blockade effect (Scheme 1). Moreover, HSA not only facilitates the binding of hydrophobic drug molecules *via* hydrophobic pockets for efficacious drug delivery but also promotes accumulation at tumor tissues by albumin-binding proteins overexpressed in the tumor. Our RCH NPs demonstrated excellent therapeutic efficacy against tumor progression and metastasis, along with a long-lasting immunological memory response, thanks to the potent manipulation of the Janus-faced nature of ferroptosis. Our work thus offers a conceptually innovative approach for eliciting the maximized therapeutic efficacy of ferroptosis against tumors.

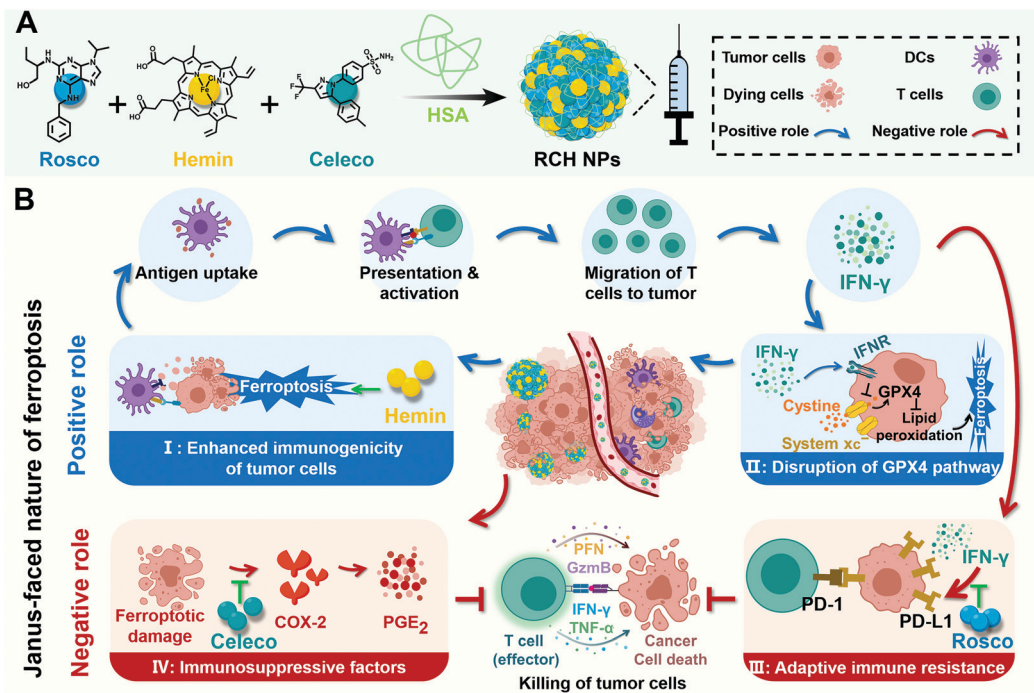
## Results and discussion

### Preparation and characterization of RCH NPs

The RCH NPs nanodrug was achieved through the co-assembly of hemin, celecoxib and roscovitine with the help of HSA. The brown-colored solution of as-prepared RCH NPs displayed a remarkable Tyndall effect upon laser irradiation (the inset in Fig. 1A). As shown in Fig. 1A, the typical UV-Vis absorbance peaks demonstrated the successful co-assembly of hemin, celecoxib and roscovitine for achieving the RCH NPs. The encapsulation efficiency of hemin, celecoxib and roscovitine in RCH NPs was measured to be 71.20%, 56.96%, 33.47%, respectively. The transmission electron microscopy (TEM) image demonstrated that RCH NPs showed a spherical morphology (the inset in Fig. 1B). Dynamic light scattering (DLS; Fig. 1B) indicated that the size of the RCH NPs was  $143.6 \pm 1.4$  nm (PDI:  $0.154 \pm 0.007$ ). As illustrated in Fig. S1 (ESI<sup>†</sup>), the particle-size results for RCH NPs at different times in water or phosphate buffered saline (PBS, pH 7.4) verified the excellent stability of the RCH NPs. The RCH NPs possessed a negative surface charge with a zeta potential of  $-19.03 \pm 0.47$  mV (Fig. S2, ESI<sup>†</sup>).

### *In vitro* release behavior of RCH NPs

The release property of roscovitine at different pH values (7.4, 6.5 and 5.0) was evaluated. As displayed in Fig. S3 (ESI<sup>†</sup>), nearly 72% of roscovitine was released in the acidic pH (5.0) of the lysosome, while only 35% was released at physiological pH (7.4) within 36 h. Roscovitine exhibited pH-responsive release properties. This result suggested that the acidic environment in tumor cells could effectively trigger drug release after the RCH NPs were internalized. Furthermore, after incubation for 2, 4, 6 and 9 h, the medium was collected for characterization using DLS. The DLS result exhibited an evolutionary disassembly behavior of RCH NPs along with time (Fig. S4, ESI<sup>†</sup>). In contrast to the initial nanoparticles, the particle size of the RCH NPs decreased significantly after 2 h of incubation; then the nanoparticles progressively dissociated into smaller particles



**Scheme 1** (A) Illustration of the fabrication of RCH NPs and (B) schematic diagram of ferroptotic immunotherapy *via* RCH NPs reprogramming the Janus-faced nature of ferroptosis to abolish inherent ferroptosis-driven immune escape.

after incubation for another 2, 4, and 7 h, identifying the disassembly of RCH NPs over time. Changes in the particle size of the RCH NPs further confirmed the release behavior of drugs from the nanodrug in the acidic tumor environment.

#### Evaluation of RCH NPs-mediated antitumor effect *in vitro*

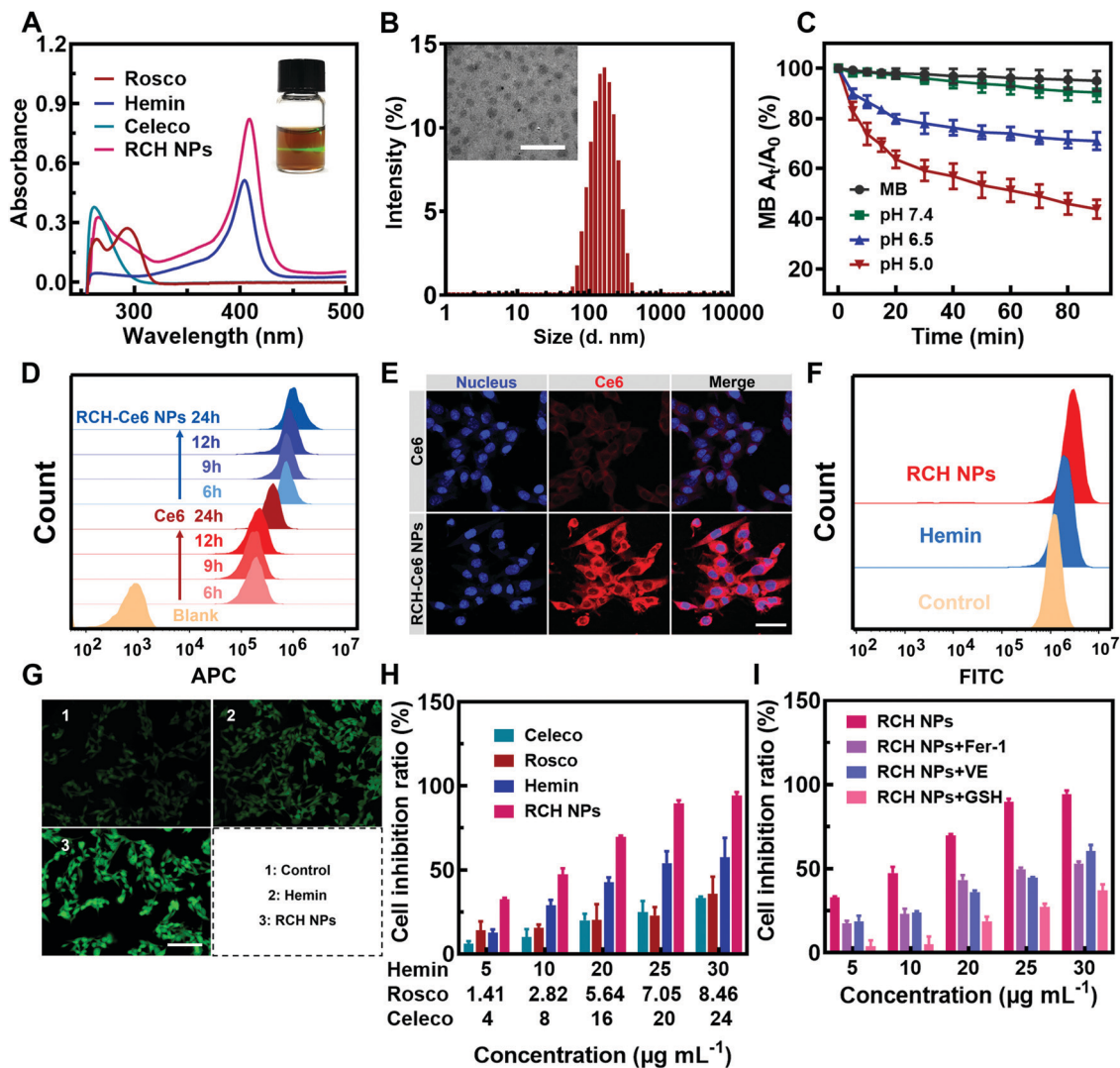
The Fenton activity of RCH NPs was evaluated using ultraviolet spectrophotometry based on the  $\bullet\text{OH}$  detection probe methylene blue (MB).<sup>22</sup> The decrease in the typical UV-Vis absorbance peak of MB at 660 nm reflected the performance of producing  $\bullet\text{OH}$ . As shown in Fig. 1C, determination of the Fenton activity of RCH NPs at various pH values was conducted. The RCH NPs showed negligible Fenton activity at pH 7.4. By contrast, the Fenton activity of RCH NPs increased immensely as the pH was reduced to 5.0. Benefiting from this unique feature, the Fenton reaction induced by the RCH NPs enabled the response to the acidic tumor microenvironment and avoided damage to normal tissues at the same time. To further prove the Fenton activity of RCH NPs, the typical oxidation reaction of TMB (3,3',5,5'-tetramethylbenzidine) was utilized to detect the generation of  $\bullet\text{OH}$  in pH 5.0 media. Compared with the mixture of TMB and  $\text{H}_2\text{O}_2$ , there was an obvious absorbance peak at 655 nm after adding the RCH NPs (Fig. S5, ESI<sup>†</sup>), which is the typical UV-Vis absorbance peak of oxidized TMB (oxTMB). As shown in Fig. S6 (ESI<sup>†</sup>), the oxidation reaction of TMB became stronger along with time. The results confirmed that the RCH NPs could act as a Fenton catalyst to generate  $\bullet\text{OH}$  for ferroptosis.

The internalization of the drug into cells is the prerequisite for RCH NPs to exert their therapeutic effect. The uptake behavior of RCH NPs in B16F10 cells was investigated using

flow cytometry and laser scanning confocal microscopy (LSCM). Chlorin e6 (Ce6) was chosen as a fluorescent indicator because RCH NPs had no effective fluorescent property. In contrast to tumor cells treated with free Ce6, cells of the RCH-Ce6 NPs group exhibited a significantly stronger red fluorescence intensity (Fig. 1D and E), indicating the higher uptake efficiency of RCH NPs, which was ascribed to the HSA-governed binding effect. The better internalization of the HSA-based nanodrug results from the albumin-binding protein that is overexpressed by B16F10 cells.<sup>23–25</sup> In addition, the cellular fluorescence signal, which represents the uptake efficiency, became stronger with time, exhibiting a time-dependent manner.

Using 2',7'-dichlorofluorescein diacetate (DCFH-DA) as the probe, the *in vitro* Fenton-reaction-triggered production of  $\bullet\text{OH}$  was investigated using flow cytometry and fluorescence microscopy. As illustrated in Fig. 1F, the RCH NPs group exhibited a much stronger fluorescence than the other groups, revealing its excellent capability for  $\bullet\text{OH}$  generation. Qualitative analysis *via* fluorescence microscopy indicated results that were consistent with flow cytometry (Fig. 1G), demonstrating that our designed RCH NPs were an efficient iron-based nanoplatform for ferroptosis due to their outstanding  $\bullet\text{OH}$  generation.

The *in vitro* cytotoxicity of RCH NPs was investigated using the MTT assay. As can be seen from Fig. 1H, the RCH NPs markedly induced a higher level of cell inhibition against B16F10 cells in comparison with free celecoxib, roscovitine and hemin. The contribution of ferroptosis to the RCH NPs-induced cytotoxicity in B16F10 cells was further investigated. Compared with the group of RCH NPs, the addition of ferroptosis inhibitors such as ferrostatin-1 (Fer-1), vitamin E (VE), and



**Fig. 1** (A) UV-Vis spectra of roscovitine, hemin, celecoxib and RCH NPs as well as the image displaying the Tyndall effect of RCH NPs (inset). (B) Size distribution and the TEM image (inset) of RCH NPs. Scale bar: 400 nm. (C) MB degradation induced by the Fenton reaction of RCH NPs at different pH (7.4, 6.5 and 5.0). (D) Flow cytometry results and (E) fluorescent images of cell uptake for the free Ce6 and RCH-Ce6 NPs. Scale bar: 40  $\mu\text{m}$ . (F) Flow cytometry results and (G) fluorescent images of intracellular  $\cdot\text{OH}$  generation in PBS, hemin and RCH NPs. Scale bar: 200  $\mu\text{m}$ . (H) Cytotoxicity test of celecoxib, roscovitine, hemin and RCH NPs on B16F10 cells after 24 h of incubation. (I) Ferroptosis in RCH NPs-mediated cytotoxicity: cellular inhibition ratios under the treatment of RCH NPs co-incubating with various ferroptosis inhibitors such as Fer-1, VE, and GSH.

GSH, which have properties of radical-trapping or antioxidation in RCH NPs groups, saved cells from ferroptosis, confirming that ferroptosis played an essential role in RCH NPs-mediated cytotoxicity (Fig. 1I). These results demonstrated that RCH NPs could kill tumor cells effectively and were adopted as a brilliant ferroptosis inducer.

#### *In vitro* antitumor immune response of RCH NPs

The immunogenic cell death (ICD)-inducing ability of RCH NPs based on ferroptosis was examined *via* release of the high mobility group box 1 (HMGB1) from the nucleus, the exposure of calreticulin (CRT) on the cell surface and the secretion of adenosine triphosphate (ATP). Compared with other groups, the cells of the RCH NPs group were observed to enhance HMGB1 release from the nucleus (Fig. 2A) and a larger amount

of CRT exposure on the surface (Fig. 2B). The ATP content secreted by tumor cells was further examined using a microplate reader. As displayed in Fig. S7 (ESI<sup>†</sup>), the highest ATP secretion was observed in the cells treated with RCH NPs, which is 2.6-fold higher than that of the control group. The above results thus confirmed that RCH NPs could generate potent ICD for eliciting antitumor immunotherapy.

As the immunogenicity triggered by RCH NPs was expected to arouse a significant antitumor immune response, dendritic cell (DC) activation and maturation triggered by ICD were assessed to understand the immune response, which was regarded as further evidence of the positive role of ferroptosis in antitumor immunity as detailed above. Bone-marrow-derived dendritic cells (BMDCs) from C57BL/6 mice were incubated with different groups of tumor cells. Flow cytometry

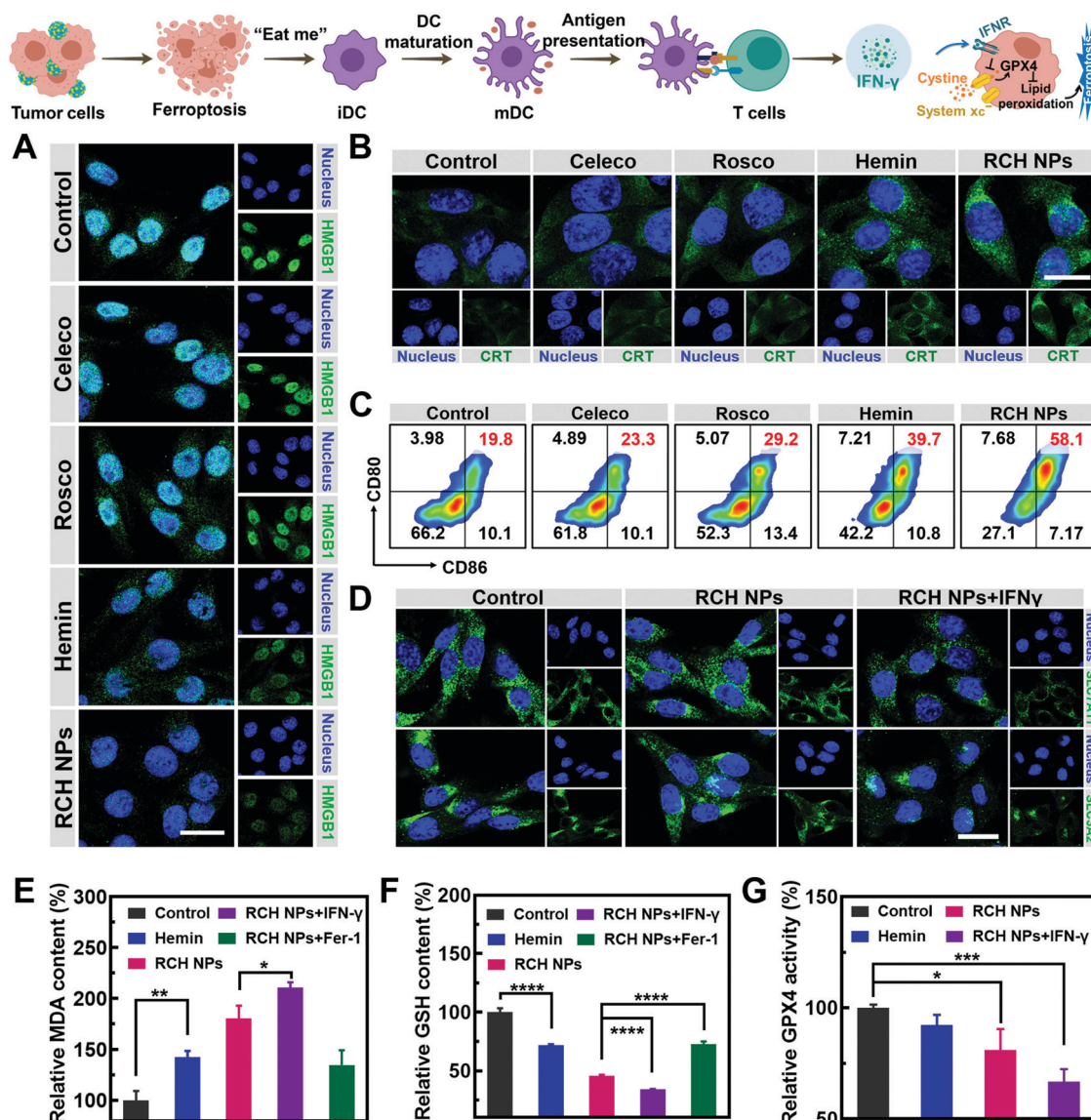


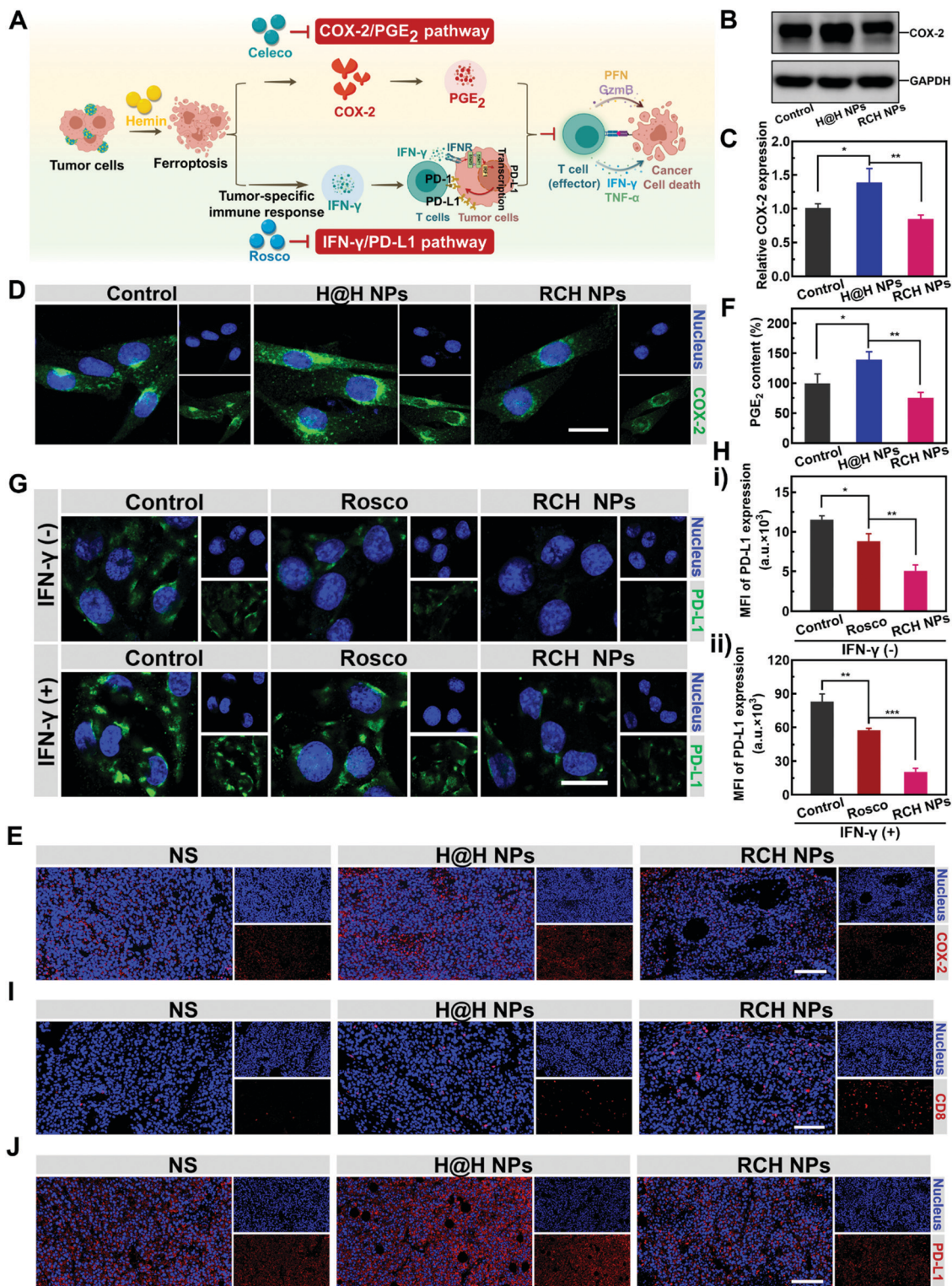
Fig. 2 Fluorescent images of (A) HMGB1 release from the cell nucleus and (B) CRT exposure on the B16F10 cell membrane after different treatments. Scale bar: 20  $\mu$ m. (C) Flow cytometry results of DC maturation of different groups. (D) Fluorescent images of SLC7A11 and SLC3A2 expression under different treatments. Scale bar: 20  $\mu$ m. (E) MDA content, (F) GSH content, and (G) activity of the GPX4 in B16F10 cells during incubation with different formulations.

was utilized to analyze the proportion of the matured DCs (CD11c<sup>+</sup>CD80<sup>+</sup>CD86<sup>+</sup>). The RCH NPs group induced considerable DC maturation, demonstrating 2.93-fold greater efficiency than that of the control group (Fig. 2C). These results indicated that RCH NPs could successfully activate the immune response for efficient immunotherapy wherein the enhanced immunogenicity of tumor cells and DC maturation were demonstrated.

As an aspect of the Janus-faced nature of ferroptosis, the positive role of ferroptosis in antitumor therapy was considered to participate in T cell-mediated immunotherapy by IFN- $\gamma$ . IFN- $\gamma$  derived from cytotoxic T cells can be significantly up-regulated by the ferroptosis-activated immune response. As a killing mechanism of T cell-mediated immunotherapy, IFN- $\gamma$  could in turn sensitize tumor cells to ferroptosis by

reducing the expression of SLC7A11 and SLC3A2 to enhance ferroptosis-specific lipid peroxidation, as reported.<sup>10,11</sup> From *in vitro* cellular experiments, IFN- $\gamma$  was added directly to incubate tumor cells. As shown in Fig. 2D, LSCM was utilized to assess the expression level of SLC7A11 and SLC3A2. The fluorescence of the two proteins of tumor cells showed negligible changes after treatment with RCH NPs. By contrast, the cell fluorescence decreased significantly after co-incubation with IFN- $\gamma$ . The above results revealed that IFN- $\gamma$  derived from the activated immune system could down-regulate SLC7A11 and SLC3A2, resulting in a cascade enhancement of ferroptotic cell death and ferroptosis-induced immunotherapy.

As the vital biomarker of ferroptosis, the accumulation of lipid peroxide inside tumor cells determines the lethality of



**Fig. 3** (A) Illustration showing that the RCH NPs abrogate ferroptosis-driven immune escape. (B) Western blot results, (C) corresponding quantitative determination and (D) fluorescent images of the COX-2 expression of different groups (scale bar: 20 μm). (E) Immunofluorescence-stained images of tumor sections for COX-2 expression analysis. Scale bar: 200 μm. (F) ELISA results of PGE<sub>2</sub> secretion with different treatments. (G) Fluorescent images (scale bar: 20 μm) and (H) flow cytometry results of PD-L1 expression on B16F10 cells after different treatments. (I) Immunofluorescence-stained images of tumor sections for CD8<sup>+</sup> T cell infiltration analysis. Scale bar: 200 μm. (J) Immunofluorescence-stained images of the tumor sections for PD-L1 expression analysis. Scale bar: 200 μm.

ferroptosis, wherein malondialdehyde (MDA), working as a lipid oxidation end-product, shows increased levels during ferroptosis.<sup>26,27</sup> By contrast, GSH, a major nutrient involved in multiple aspects of oxidation–reduction in tumor cells,

would be consumed by cytotoxic  $\bullet\text{OH}$  generated from the Fenton reaction in ferroptosis.<sup>28</sup> With both as biomarkers of ferroptosis, the extent of MDA production (Fig. 2E) and GSH depletion (Fig. 2F) induced by RCH NPs was further investigated in B16F10 cells to confirm the intrinsic characteristics of ferroptosis. RCH NPs exhibited more efficient MDA production and GSH depletion than free hemin, thanks to the enriched accumulation of RCH NPs through nanosize-amplified cellular uptake. The more efficient MDA production and GSH depletion demonstrated the more effective intracellular lipid peroxidation for ferroptosis. As a control, the RCH NPs group with ferroptosis inhibitor Fer-1 exhibited less efficient MDA production and GSH depletion. In addition, an enhanced extent of MDA production and GSH depletion by RCH NPs with  $\text{IFN-}\gamma$  co-incubation was also observed, revealing that the immune response could augment ferroptosis-specific lipid peroxidation by  $\text{IFN-}\gamma$  secretion for facilitating ferroptosis. Taken altogether, the ferroptosis-induced immune response could in turn enhance ferroptosis *via* the secreted  $\text{IFN-}\gamma$ , realizing self-amplification between ferroptosis and immunotherapy in a cascade manner.

Ferroptosis can be promoted *via* the deactivation of GPX4.<sup>29</sup> GPX4-catalyzed detoxication of the lipid peroxide to non-toxic lipid alcohols needs GSH to act as the cofactor. Inspired by the excellent results in the GSH depletion assay with RCH NPs, the activity of GPX4 was further examined. According to Fig. 2G, hemin displayed a slight inhibition of GPX4 activity in contrast to the control group. However, the GPX4 activity decreased markedly in tumor cells of the RCH NPs group, and this trend became more obvious with the addition of  $\text{IFN-}\gamma$ , further indicating that  $\text{IFN-}\gamma$  was helpful in making the tumor cells more efficient to ferroptosis. This could be ascribed to the blockage of GSH synthesis *via* the inhibition of SLC7A11 and SLC3A2 governed by  $\text{IFN-}\gamma$ , as mentioned above.

### Disruption of inherent ferroptosis-driven immune escape by RCH NPs

Ferroptotic tumor cells are biologically characterized by the up-regulated COX-2 along with the COX-2-derived up-regulation of  $\text{PGE}_2$ .<sup>14–16</sup> However,  $\text{PGE}_2$  is a major inflammation-associated immunosuppressive factor that endows ferroptotic tumor cells with immune escape for suppressing the antitumor immunity.<sup>17,18</sup> Thus, as a negative role, ferroptosis inherently stimulates inflammation-associated immunosuppression (Fig. 3A). Our RCH NPs are composed of celecoxib, a non-steroidal anti-inflammatory drug, which enables the tailoring of the COX-2 activity. To uncover the regulation of COX-2 by our RCH NPs during ferroptosis, the *in vitro* and *in vivo* COX-2 expression levels were investigated with the control experiments. Considering the uptake efficiency and water solubility between the free hydrophobic hemin drug and hemin-based nanoparticles, the assembly of hemin and HSA (defined as H@H NPs) was utilized as a control for comparison with the reprogramming role of the RCH NPs. For western blot analysis at the cellular level (Fig. 3B and C), a higher level of COX-2 for the H@H NPs group was observed over that of the NS (normal saline) group, indicating that the up-regulated COX-2 level was

triggered by hemin-mediated ferroptosis. Notably, the level of COX-2 for the RCH NPs group significantly decreased compared with that of the H@H NPs group, thanks to the inhibition of COX-2 by celecoxib within the RCH NPs. The results of cellular fluorescence images were in agreement with that of western blot analysis (Fig. 3D). Moreover, for the immunofluorescence-stained images of tumor sections (Fig. 3E), the stronger COX-2 expression of the H@H NPs group over the NS group and the weaker COX-2 expression of RCH NPs compared with the H@H NPs group were observed, consistent with the results at the cellular level. The above results thus demonstrated that the RCH NPs could powerfully suppress the COX-2 activity. The secretion of  $\text{PGE}_2$  was further assessed using an ELISA kit to verify the proinflammatory role triggered by ferroptosis and the anti-inflammatory role mediated by the RCH NPs. As shown in Fig. 3F, the H@H NPs promoted the secretion of  $\text{PGE}_2$  in tumor cells compared with the control group, indicating that ferroptosis inherently triggered  $\text{PGE}_2$ -based inflammation-associated immunosuppression. However, the  $\text{PGE}_2$  content of the RCH NPs group was significantly lower than that of the H@H NPs group due to the unique role of celecoxib, further demonstrating that RCH NPs could potentially inhibit the inflammatory COX-2/ $\text{PGE}_2$  pathway up-regulated by ferroptosis to relieve inflammation-associated immunosuppression.

The effective immune response elicited by ferroptosis could enhance the production of  $\text{IFN-}\gamma$  *via* the recruitment of cytotoxic T cells. However, as another negative role, ferroptosis-stimulated  $\text{IFN-}\gamma$  production could act as an accomplice of adaptive immune resistance to promote the expression of PD-L1 on tumor cells by inducing interferon regulatory factors 1 (IRF1), thus impairing the antitumor immunotherapy effect (Fig. 3A). Recent literature reports have identified that Cdk5 inhibition could lead to the persistent expression of PD-L1 transcriptional repressors, interferon regulatory factors 2 (IRF2), and interferon regulatory factor 2 binding protein 2 (IRF2BP2), which not only directly down-regulated the tumoral PD-L1 expression by virtue of genetic blockage, but also blunted the cascade reaction between PD-L1 up-regulation and  $\text{IFN-}\gamma$  stimulation *via* the competition between IRF1 and IRF2.<sup>30–32</sup> Thus the roscovitine-based nanodrug can reverse the adaptive immune resistance by disrupting the  $\text{IFN-}\gamma$ -governed PD-L1 up-regulation. To understand the efficacy of roscovitine in RCH NPs for regulation of the expression of PD-L1 in cellular experiments, we assessed the PD-L1 expression level on the surface of B16F10 cells after treatment *via*  $\text{IFN-}\gamma$  alone (the control group), free roscovitine +  $\text{IFN-}\gamma$  and RCH NPs +  $\text{IFN-}\gamma$  for 24 h. As elucidated in Fig. 3G and H, for the group of  $\text{IFN-}\gamma$  alone,  $\text{IFN-}\gamma$  stimulation significantly up-regulated the PD-L1 expression level on the B16F10 cells, indicating severe adaptive immune resistance induced by the  $\text{IFN-}\gamma$ . However, the groups of both free roscovitine +  $\text{IFN-}\gamma$  and RCH NPs +  $\text{IFN-}\gamma$  exhibited the effective inhibition of PD-L1 expression, where RCH NPs +  $\text{IFN-}\gamma$  demonstrated a greater efficiency than free roscovitine +  $\text{IFN-}\gamma$ . Therefore, even under  $\text{IFN-}\gamma$  stimulation, the RCH NPs possessed an excellent ability for the persistent suppression of PD-L1 expression, indicating that the RCH NPs-induced attenuation of PD-L1 expression was irreversible for subsequent  $\text{IFN-}\gamma$  stimulation,

thanks to the roscovitine in the RCH NPs. As a result, the RCH NPs could precisely reverse adaptive immune resistance in ferroptosis. To further understand the efficacy of the RCH NPs in regulating the IFN- $\gamma$ -induced PD-L1 expression in ferroptosis, we conducted an *in vivo* study within tumors. We investigated the quantity of intratumoral cytotoxic T cells (CD8<sup>+</sup> T cells) after different treatments. As depicted in Fig. 3I, the effective immune response elicited by ferroptosis significantly promoted the recruitment of cytotoxic T cells in the RCH NPs group, which in turn enabled the stimulation of IFN- $\gamma$  secretion. For the immunofluorescence-stained images of tumor sections in determining the PD-L1 expression (Fig. 3J), the stronger PD-L1 expression of the H@H NPs group over the NS group and the weaker PD-L1 expression of the RCH NPs group compared with the H@H NPs group were observed, which was consistent with the above results at the cellular level. From the results either at the cellular level or *in vivo*, our RCH NPs could potentially blunt the cascade reaction between IFN- $\gamma$  stimulation and PD-L1 up-regulation for reversing the adaptive immune resistance induced by IFN- $\gamma$  in ferroptosis, enabling efficient ferroptotic immunotherapy.

Taken together, the inherent negative roles of ferroptosis in immunotherapy can be potentially solved by our RCH NPs, either *via* eliminating inflammation-associated immunosuppression or *via* reversing the adaptive immune resistance for maximizing the therapeutic efficacy of ferroptosis (Fig. 3A).

#### *In vivo* antitumor performance of RCH NPs

The feasibility of the RCH NPs as an intravenous injection preparation was evaluated. According to Fig. S8 (ESI<sup>†</sup>), the hemolysis ratio of the RCH NPs was below 5% at each concentration, indicating that intravenous administration was feasible for our biocompatible RCH NPs. Due to the lack of effective fluorescent properties for the RCH NPs, RCH-Ce6 NPs were utilized as a substitute for the RCH NPs in the fluorescence imaging study, where the RCH-Ce6 NPs were prepared in a similar way to that of the RCH NPs. The fluorescence imaging results, to understand the *in vivo* distribution and intratumoral accumulation of Ce6-loaded RCH NPs after intravenous administration, are shown in Fig. 4A. The total fluorescence intensity (TFI) of the RCH-Ce6 NPs group in the tumor tissue was markedly stronger than that of the free Ce6 group, demonstrating the superior tumor accumulation, thanks to the enhanced permeability and retention (EPR) effect along with the HSA-governed interaction with albumin-binding proteins overexpressed in tumors.<sup>33–35</sup> In addition, the fluorescence signal results of normal organs and tumors (Fig. 4A and Fig. S9, ESI<sup>†</sup>) revealed the tissue-distribution characteristics of the nanodrug. The strong fluorescence signal of tumors in *ex vivo* imaging further confirmed the superior accumulation of RCH-Ce6 NPs at the tumor site. Notably, a weak fluorescence intensity was detected in the spleen, heart and lungs of both groups, indicating the low accumulation and distribution in all three of these organs, which could result in modest toxic effects. The strong fluorescence intensity of the RCH-Ce6 NPs in the liver and kidneys might be attributed to its metabolic and excretory pathways.

The antitumor performance was investigated in B16F10 tumor-bearing mice, which were treated with NS, free celecoxib, roscovitine, hemin, and RCH NPs *via* intravenous administration every 2 days (Fig. 4B). The tumor volume was monitored during the treatment period (Fig. 4C). The celecoxib group showed the smallest inhibition of tumor growth, while the groups of roscovitine and hemin showed moderate tumor-growth suppression. However, the RCH NPs displayed the highest inhibition efficacy for tumors, where the tumor growth was significantly suppressed during the course of treatment. Moreover, the tumor weight and inhibition ratio further confirmed the superiority of the RCH NPs in tumor therapy (Fig. 4D). Photographs of the excised tumors after different treatments were shown in Fig. 4E. The results of hematoxylin-eosin (H&E) staining revealed there was no visible pathological damage in the main organs along with massive cell death and tissue damage in the tumor sites (Fig. S10, ESI<sup>†</sup>), demonstrating the good biocompatibility and outstanding antitumor effect of the RCH NPs. Moreover, the body-weight differences of the mice in all groups were negligible during the treatment (Fig. 4F). As two common blood biochemical markers, alanine amino transferase (ALT) and aspartate aminotransferase (AST) were detected to evaluate the safety issues. As displayed in Fig. S11 and S12 (ESI<sup>†</sup>), compared with the NS group, the content of ALT and AST in the RCH NPs group showed negligible changes. The results of blood chemistry further revealed that the RCH NPs had good biological safety. These results thus confirmed that our RCH NPs exhibited a powerful antitumor therapeutic performance with good biocompatibility.

#### *In vivo* immune response of RCH NPs

The efficient antitumor performance of the RCH NPs benefited not only from the ferroptosis-triggered direct killing effect but also the antitumor immunotherapeutic capability activated by reprogramming the Janus-faced nature of ferroptosis. To understand the immune response caused by our RCH NPs, flow cytometry analysis was employed to examine the ferroptosis-triggered immune response. As the typical sentinels of the immune system, DCs in tumor draining lymph nodes (TDLNs) were assayed *via* staining with the markers of CD80 and CD86 to quantitatively determine the proportion of matured DCs (CD11c<sup>+</sup>CD86<sup>+</sup>CD80<sup>+</sup>). Compared with the NS group, the RCH NPs group demonstrated a 2.9-fold higher ratio of the matured DCs (Fig. 5A and B), indicating its powerful capability of RCH NPs in promoting DC maturation with effective initiation of the immune response, thanks to the enhanced immunogenicity by ferroptosis.

The antitumor immune effect is primarily governed by CD8<sup>+</sup> cytotoxic T lymphocytes (CTLs, CD3<sup>+</sup>CD8<sup>+</sup>), which release cytotoxins to kill tumor cells directly.<sup>36,37</sup> As shown in Fig. 5C and D, the tumor infiltration of CD8<sup>+</sup> T cells in the hemin group was significantly increased to 2.1-fold compared with the NS group, indicating that ferroptosis could elicit an effective local immune response for immunotherapy. In particular, the tumor infiltration of CD8<sup>+</sup> T cells of the RCH NPs-treated group was further elevated up to 2.8-fold compared with the NS group. These results clearly indicated that the RCH NPs could induce a



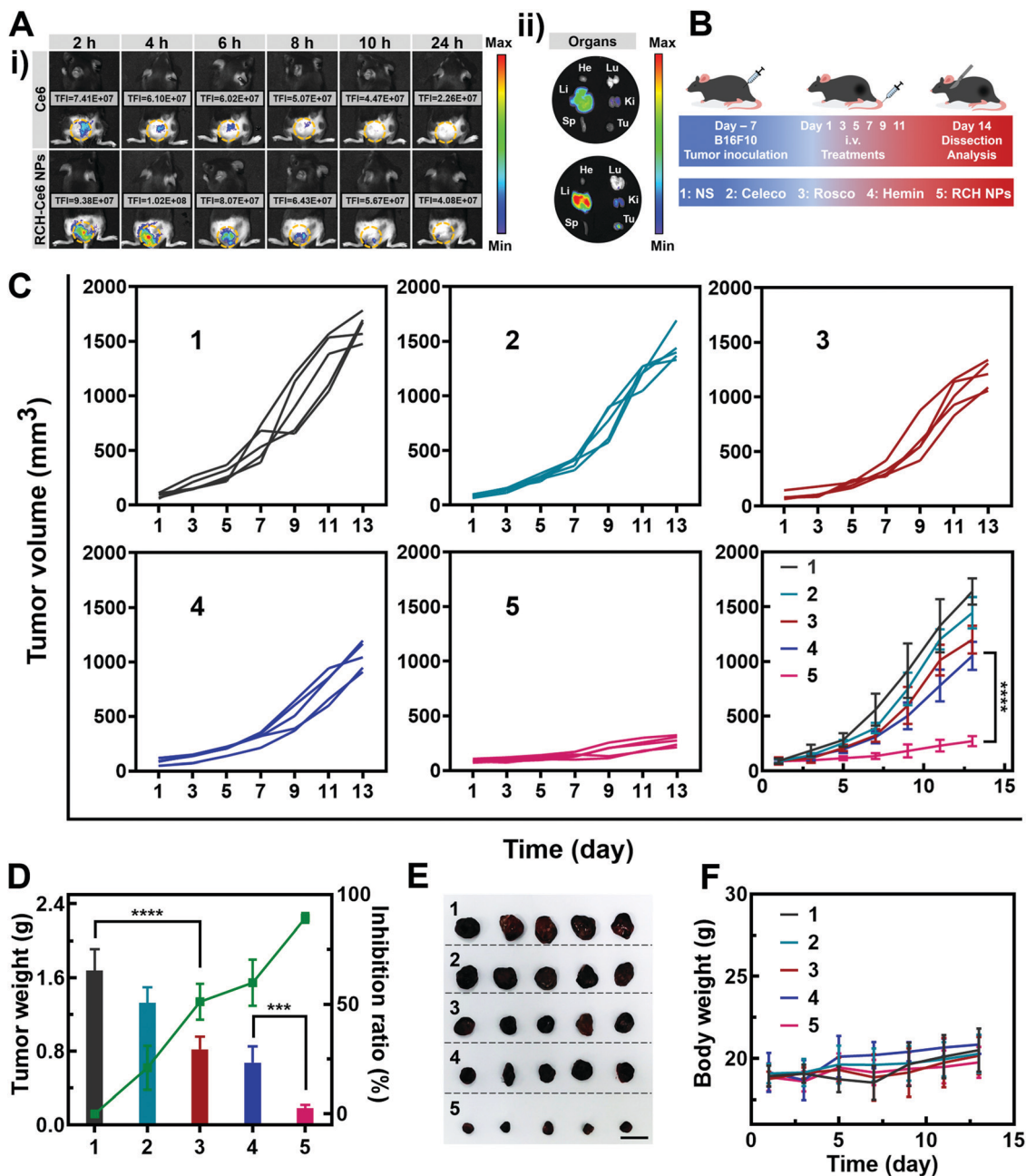


Fig. 4 (A) Fluorescence photographs of (i) the mice after injection of free Ce6 and RCH–Ce6 NPs and (ii) the main organs and tumors (He, heart; Sp, spleen; Ki, kidney; Li, liver; Lu, lung; and Tu, tumor) excised 24 h after injection. (B) Schematic illustration for the experiment with RCH NPs to inhibit tumor growth. (C) Average tumor-growth curves and individual tumor-growth kinetics of different treated mice. (D) Change in tumor weight, and tumor inhibition ratio of different groups ( $n = 5$ ). (E) Photographs of excised tumors of different groups ( $n = 5$ ). Scale bar: 2 cm. (F) Body weight of different groups ( $n = 5$ ). The groups include 1, NS; 2, Celeco; 3, Rosco; 4, Hemin; and 5, RCH NPs.

more potent local immune response at the tumor tissue site *via* reprogramming the Janus-faced nature of ferroptosis.

Furthermore, T lymphocytes in the spleen were analyzed to validate the systemic immune response triggered by the RCH NPs. The proportion of splenic CD8<sup>+</sup> T lymphocytes was greatly elevated in the RCH NPs group, revealing that systemic immunity had been induced (Fig. 5E and F). The secretion of cytokines including interleukin-2 (IL-2), tumor necrosis factor- $\alpha$  (TNF- $\alpha$ ) and IFN- $\gamma$  were further analyzed *via* ELISA. As presented in

Fig. S14 (ESI<sup>†</sup>), the RCH NPs efficiently up-regulated the levels of these three T-helper 1 (Th1)-type cytokines, further revealing that the remarkable systemic immune response had been triggered by treatment with the RCH NPs. As a result, apart from the direct killing effect caused by ferroptosis, the excellent antitumor effect of our RCH NPs was also attributed to their ability to facilitate the maturation of DCs, activating the immune effector cells, and elevating the levels of crucial immune cytokines, which accordingly led to a powerful antitumor immunotherapeutic efficacy.

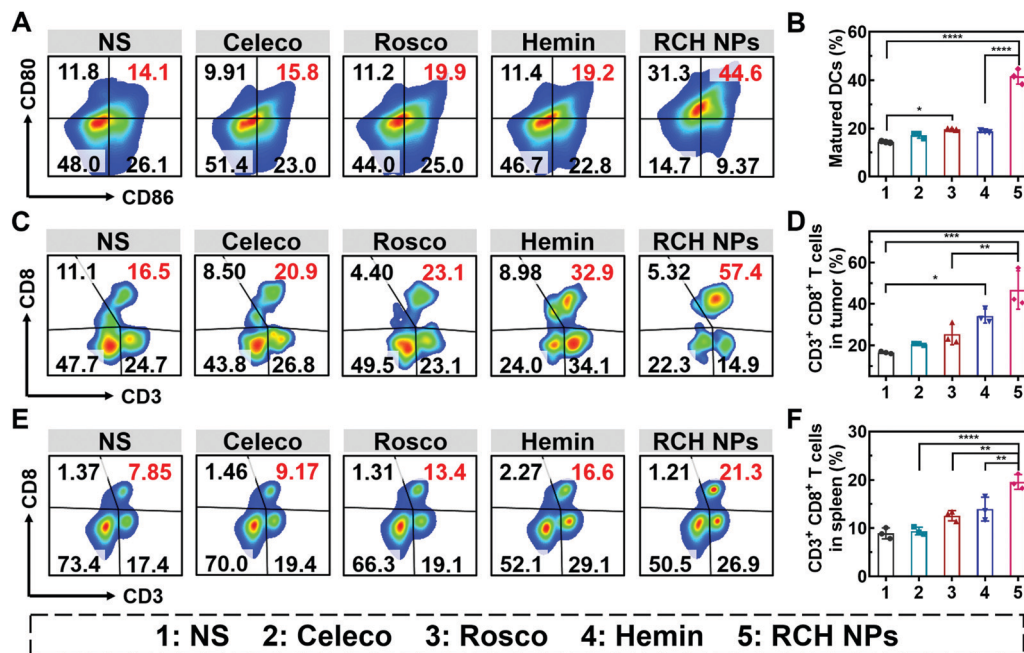


Fig. 5 (A) Flow analysis and (B) quantitative result of the percentages of maturated DCs in the TDLNs under different treatments ( $n = 3$ ). (C) Flow analysis and (D) quantitative result of the percentages of tumor infiltrating CD8<sup>+</sup> T lymphocytes of various treated mice ( $n = 3$ ). (E) Flow analysis and (F) quantitative result of CD8<sup>+</sup> T lymphocytes in splenic lymphocytes of various treated mice ( $n = 3$ ). The groups include 1, NS; 2, Celeco; 3, Rosco; 4, Hemin; and 5, RCH NPs.

### The abscopal effect of RCH NPs for bilateral model

Inspired by the excellent results of the *in vivo* immune response triggered by the RCH NPs on B16F10 tumor-bearing mice, the abscopal effect of RCH NPs was further investigated in bilateral tumor-bearing mice, which were treated with NS and RCH NPs *via* intratumoral (primary tumor) administration every 4 days for a total of 3 times. The volume of the primary and abscopal tumors was monitored during the treatment period. Compared with the NS group, the primary tumor growth of the RCH NPs-treated mice was significantly inhibited, as shown in Fig. S15 (ESI<sup>†</sup>). For the abscopal tumors, the RCH NPs indicated a potent inhibition effect on the tumor growth, superior to the NS group (Fig. S16, ESI<sup>†</sup>). The results of the tumor weight and inhibition ratio further confirmed the excellent abscopal effect of the RCH NPs in antitumor therapy (Fig. S17 and S18, ESI<sup>†</sup>), which was mainly attributed to the triggered immunotherapy in untreated abscopal tumors. In addition, the body-weight differences of the mice in two groups were negligible during the treatment (Fig. S19, ESI<sup>†</sup>). Moreover, CTLs in abscopal tumors were analyzed using flow cytometry to systematically reveal the immunotherapeutic effect of RCH NPs. After treatment with RCH NPs, the tumor infiltration of CD8<sup>+</sup> T cells in abscopal tumors was improved, and was 2.3-fold higher than that of the NS group (Fig. S20, ESI<sup>†</sup>). These results suggested that our RCH NPs are an effective antitumor nanodrug to fight against both primary tumors and abscopal tumors *via* an enhanced immune response.

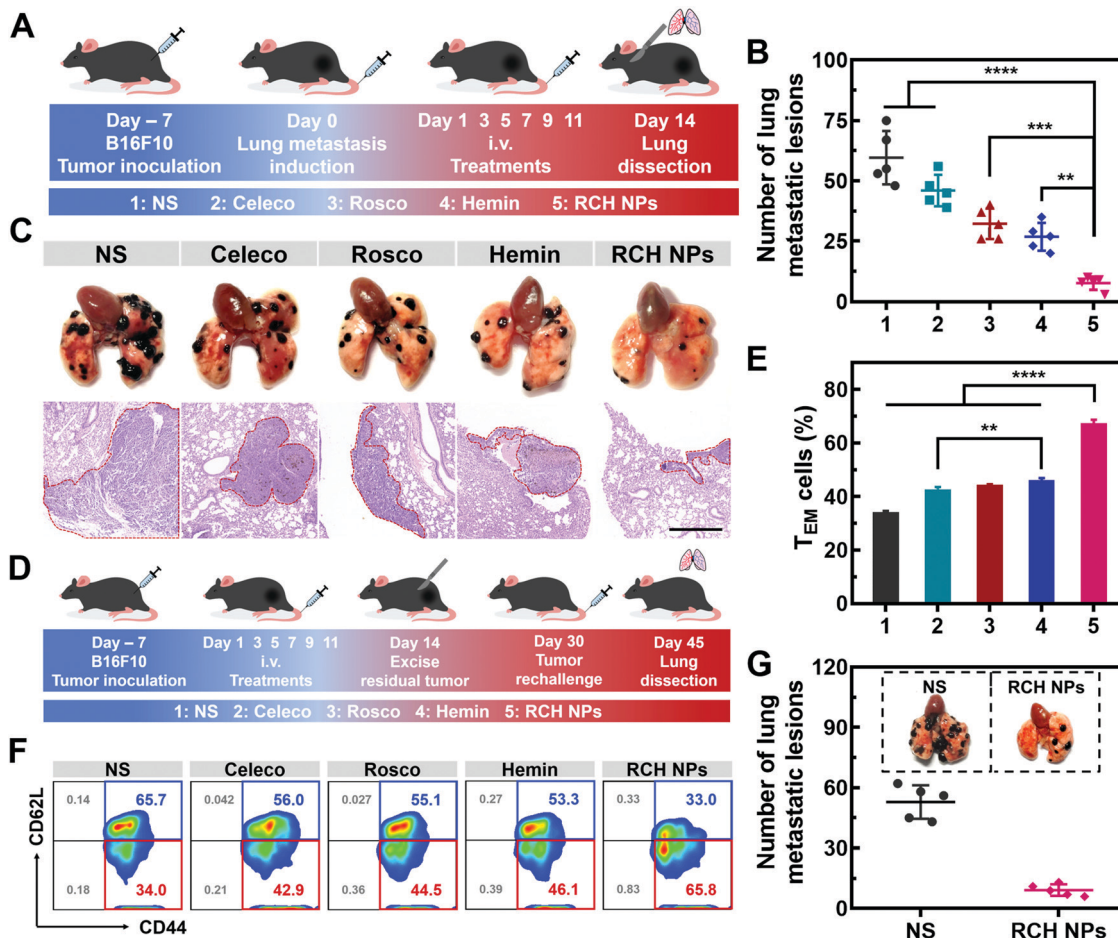
### *In vivo* anti-metastasis evaluation of RCH NPs

Tumor metastasis is the main factor dominating the survival of cancer patients.<sup>38</sup> The anti-metastasis capability of our

designed RCH NPs was further examined using an established lung metastatic model based on the intravenous injection of B16F10 cells into tumor-bearing mice (Fig. 6A). After treatment with various formulations, the lungs of the mice were recovered to examine the metastatic lesions. As presented in Fig. 6B, metastatic nodules of the NS group appeared on the lung surface in large quantities, the number of which was approximately 60. However, the number of lung metastasis nodules in the other groups were decreased by different degrees. In particular, the number of lung metastasis nodules in the RCH NPs group decreased by 87.2% compared with the NS group. H&E images of the lungs further confirmed that the RCH NPs group displayed the minimal extent of cancerization (Fig. 6C). The potent ability of inhibiting lung metastasis by the RCH NPs benefited from the powerful self-activated systemic immune response. Therefore, our RCH NPs could act as a pre-eminent nanodrug for suppressing tumor metastasis.

### *In vivo* long-term immune response evaluation of RCH NPs

Memory T cells play a crucial role in the long-term antitumor effect with the hallmarks of long-lasting self-renewal, replication and survival in body.<sup>39,40</sup> Hence, inspired by the results of the excellent systemic immunological response, the percentages of memory T cells were further tested to explore the capability of the immune memory caused by the RCH NPs. As illustrated in Fig. 6D for 16 days after the surgical resection, the spleens were separated from the mice of all groups to quantitatively analyze the percentages of central memory T cells ( $T_{CM}$ , CD3<sup>+</sup>CD8<sup>+</sup>CD62L<sup>+</sup>CD44<sup>+</sup>) and effector memory T cells ( $T_{EM}$ , CD3<sup>+</sup>CD8<sup>+</sup>CD62L<sup>-</sup>CD44<sup>+</sup>). Compared with the NS group, the percentage of  $T_{EM}$  in the RCH NPs group of mice was



**Fig. 6** (A) Schematic illustration of the experimental approach for RCH NPs inhibiting lung metastasis. (B) Numbers of the lung metastatic lesions in different treated mice ( $n = 5$ ). (C) Camera images (above) and H&E staining images (below) of lung metastasis in B16F10 tumor-bearing mice. Scale bar: 500  $\mu\text{m}$ . (D) Schematic illustration of the immunological memory evaluation. (E) The proportion of effector memory T cells in the spleens from different treated mice ( $n = 3$ ). (F) Flow cytometry results of the ratio of memory T cells in spleens. (G) Camera images of lung metastasis ( $n = 5$ ). The groups include 1, NS; 2, Celeco; 3, Rosco; 4, Hemin; and 5, RCH NPs.

clearly elevated from  $34.3 \pm 0.4\%$  to  $67.3 \pm 1.3\%$  (Fig. 6E and F), while the percentage of  $T_{CM}$  was reduced from  $65.3 \pm 0.4\%$  to  $31.9 \pm 1.0\%$  (Fig. S21, ESI<sup>†</sup>). These results confirmed that the powerful immunological memory had been elicited by the RCH NPs. We further explored the performance of RCH NPs for long-term tumor inhibition *via* rechallenging the mice with B16F10 cells at 16 days post-tumor excision. From Fig. 6G, the lungs of the mice treated with NS exhibited many metastatic lesions, while the lung metastasis of the mice treated with the RCH NPs was significantly reduced. As a result, our RCH NPs enabled a potent immunological memory with the capacity for long-term tumor-growth suppression.

## Conclusion

In summary, a self-amplifying nanodrug was precisely designed to reprogram the Janus-faced nature of ferroptosis *via* harnessing the positive role of ferroptosis along with reversing its inherent negative role to achieve optimal ferroptotic tumor therapy. As a

positive role, the RCH NPs demonstrated powerful ferroptotic damage along with inducing an immune response, where the generated  $\text{IFN-}\gamma$  triggered disruption of the GPX4 pathway for cascade enhancement of ferroptotic cell death and ferroptosis-induced immunotherapeutic efficacy. In particular, the inherent negative roles of ferroptosis in immunotherapy were potently solved by our RCH NPs *via* both eliminating inflammation-associated immunosuppression and reversing  $\text{IFN-}\gamma$ -related adaptive immune resistance for maximizing the immunotherapeutic efficacy, thanks to the cooperation of celecoxib and roscovitine in the nanodrug. Our designed nanodrug (RCH NPs), which consists of hemin, celecoxib and roscovitine, is a promising multifunctional drug-delivery system for biomedical applications, and demonstrates powerful therapeutic efficacy against tumor progression and metastasis along with a long-lasting immunological memory response. Compared with traditional ferroptosis-based inorganic nanoplateforms (such as iron-based metal-organic frameworks), the RCH NPs demonstrate excellent biological safety and a more efficient immunotherapy effect, with great potential for further clinical development. The present work offers a

conceptually innovative approach for manipulating the Janus-faced nature of ferroptosis to elicit maximized therapeutic efficacy against tumors.

## Conflicts of interest

The authors declare no conflict of interest.

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## References

- 1 S. J. Dixon, K. M. Lemberg, M. R. Lamprecht, R. Skouta, E. M. Zaitsev, C. E. Gleason, D. N. Patel, A. J. Bauer, A. M. Cantley, W. S. Yang, B. Morrison, 3rd and B. R. Stockwell, *Cell*, 2012, **149**, 1060–1072.
- 2 B. R. Stockwell, J. P. Friedmann Angeli, H. Bayir, A. I. Bush, M. Conrad, S. J. Dixon, S. Fulda, S. Gascón, S. K. Hatzios, V. E. Kagan, K. Noel, X. Jiang, A. Linkermann, M. E. Murphy, M. Overholtzer, A. Oyagi, G. C. Pagnussat, J. Park, Q. Ran, C. S. Rosenfeld, K. Salnikow, D. Tang, F. M. Torti, S. V. Torti, S. Toyokuni, K. A. Woerpel and D. D. Zhang, *Cell*, 2017, **171**, 273–285.
- 3 B. Hassannia, P. Vandenabeele and T. Vanden Berghe, *Cancer Cell*, 2019, **35**, 830–849.
- 4 C. Liang, X. Zhang, M. Yang and X. Dong, *Adv. Mater.*, 2019, **31**, e1904197.
- 5 F. Zhang, F. Li, G. H. Lu, W. Nie, L. Zhang, Y. Lv, W. Bao, X. Gao, W. Wei, K. Pu and H. Y. Xie, *ACS Nano*, 2019, **13**, 5662–5673.
- 6 Q. Wen, J. Liu, R. Kang, B. Zhou and D. Tang, *Biochem. Biophys. Res. Commun.*, 2019, **510**, 278–283.
- 7 B. Ding, P. Zheng, F. Jiang, Y. Zhao, M. Wang, M. Chang, P. Ma and J. Lin, *Angew. Chem., Int. Ed.*, 2020, **59**, 16381–16384.
- 8 Q. Jiang, K. Wang, X. Zhang, B. Ouyang, H. Liu, Z. Pang and W. Yang, *Small*, 2020, **16**, e2001704.
- 9 D. Tang, R. Kang, T. V. Berghe, P. Vandenabeele and G. Kroemer, *Cell Res.*, 2019, **29**, 347–364.
- 10 W. Wang, M. Green, J. E. Choi, M. Gijón, P. D. Kennedy, J. K. Johnson, P. Liao, X. Lang, I. Kryczek, A. Sell, H. Xia, J. Zhou, G. Li, J. Li, W. Li, S. Wei, L. Vatan, H. Zhang, W. Szeliga, W. Gu, R. Liu, T. S. Lawrence, C. Lamb, Y. Tanno, M. Cieslik, E. Stone, G. Georgiou, T. A. Chan, A. Chinnaiyan and W. Zou, *Nature*, 2019, **569**, 270–274.
- 11 X. Lang, M. D. Green, W. Wang, J. Yu, J. E. Choi, L. Jiang, P. Liao, J. Zhou, Q. Zhang, A. Dow, A. L. Saripalli, I. Kryczek, S. Wei, W. Szeliga, L. Vatan, E. M. Stone, G. Georgiou, M. Cieslik, D. R. Wahl, M. A. Morgan, A. M. Chinnaiyan, T. S. Lawrence and W. Zou, *Cancer Discovery*, 2019, **9**, 1673–1685.
- 12 Y. Su, B. Zhao, L. Zhou, Z. Zhang, Y. Shen, H. Lv, L. H. H. AlQudsy and P. Shang, *Cancer Lett.*, 2020, **483**, 127–136.
- 13 M. A. Badgley, D. M. Kremer, H. C. Maurer, K. E. Delgiorno, H. J. Lee, V. Purohit, I. R. Sagalovskiy, A. Ma, J. Kapilian, C. E. M. Firl, A. R. Decker, S. A. Sastra, C. F. Palermo, L. R. Andrade, P. Sajjakulnukit, L. Zhang, Z. P. Tolstyka, T. Hirschhorn, C. Lamb, T. Liu, W. Gu, E. S. Seeley, E. Stone, G. Georgiou, U. Manor, A. Iuga, G. M. Wahl, B. R. Stockwell, C. A. Lyssiotis and K. P. Olive, *Science*, 2020, **368**, 85–89.
- 14 W. S. Yang, R. SriRamaratnam, M. E. Welsch, K. Shimada, R. Skouta, V. S. Viswanathan, J. H. Cheah, P. A. Clemons, A. F. Shamji, C. B. Clish, L. M. Brown, A. W. Girotti, V. W. Cornish, S. L. Schreiber and B. R. Stockwell, *Cell*, 2014, **156**, 317–331.
- 15 D. Tang, X. Chen, R. Kang and G. Kroemer, *Cell Res.*, 2021, **31**, 107–125.
- 16 D. Li and Y. Li, *Signal Transduction Targeted Ther.*, 2020, **5**, 108.
- 17 P. Kalinski, *J. Immunol.*, 2012, **188**, 21–28.
- 18 D. Wang and R. N. DuBois, *Carcinogenesis*, 2015, **36**, 1085–1093.
- 19 J. L. Benci, L. R. Johnson, R. Choa, Y. Xu, J. Qiu, Z. Zhou, B. Xu, D. Ye, K. L. Nathanson, C. H. June, E. J. Wherry, N. R. Zhang, H. Ishwaran, M. D. Hellmann, J. D. Wolchok, T. Kambayashi and A. J. Minn, *Cell*, 2019, **178**, 933–948.e914.
- 20 S. Spranger, R. M. Spaapen, Y. Zha, J. Williams, Y. Meng, T. T. Ha and T. F. Gajewski, *Sci. Transl. Med.*, 2013, **5**, 200ra116.
- 21 P. Sharma and J. P. Allison, *Science*, 2015, **348**, 56–61.
- 22 H. Tian, M. Zhang, G. Jin, Y. Jiang and Y. Luan, *J. Colloid Interface Sci.*, 2021, **587**, 358–366.
- 23 J. Park, B. Sun and Y. Yeo, *J. Controlled Release*, 2017, **263**, 90–101.
- 24 B. Hoang, M. J. Ernsting, A. Roy, M. Murakami, E. Undzys and S. D. Li, *Biomaterials*, 2015, **59**, 66–76.
- 25 C. Neuzillet, A. Tijeras-Raballand, J. Cros, S. Faivre, P. Hammel and E. Raymond, *Cancer Metastasis Rev.*, 2013, **32**, 585–602.
- 26 T. Liu, W. Liu, M. Zhang, W. Yu, F. Gao, C. Li, S. B. Wang, J. Feng and X. Z. Zhang, *ACS Nano*, 2018, **12**, 12181–12192.
- 27 B. Yu, B. Choi, W. Li and D. H. Kim, *Nat. Commun.*, 2020, **11**, 3637.
- 28 M. Gao, J. Deng, F. Liu, A. Fan, Y. Wang, H. Wu, D. Ding, D. Kong, Z. Wang, D. Peer and Y. Zhao, *Biomaterials*, 2019, **223**, 119486.
- 29 L. Chen, Z. Lin, L. Liu, X. Zhang, W. Shi, D. Ge and Y. Sun, *ACS Biomater. Sci. Eng.*, 2019, **5**, 4861–4869.
- 30 R. D. Dorand, J. Nthale, J. T. Myers, D. S. Barkauskas, S. Avril, S. M. Chirieleison, T. K. Pareek, D. W. Abbott, D. S. Stearns, J. J. Letterio, A. Y. Huang and A. Petrosiute, *Science*, 2016, **353**, 399–403.
- 31 Q. Li, Z. P. Zhao, X. H. Qin, M. Z. Zhang, Q. Du, Z. H. Li and Y. X. Luan, *Adv. Funct. Mater.*, 2021, **31**, 2104630.

- 32 Q. Li, Y. Zhou, W. He, X. Ren, M. Zhang, Y. Jiang, Z. Zhou and Y. Luan, *J. Controlled Release*, 2021, **338**, 33–45.
- 33 C. Zhou, X. Song, C. Guo, Y. Tan, J. Zhao, Q. Yang, D. Chen, T. Tan, X. Sun, T. Gong and Z. Zhang, *ACS Appl. Mater. Interfaces*, 2019, **11**, 42534–42548.
- 34 H. Kobayashi, R. Watanabe and P. L. Choyke, *Theranostics*, 2013, **4**, 81–89.
- 35 M. Zhang, T. W. Herion, C. Timke, N. Han, K. Hauser, K. J. Weber, P. Peschke, U. Wirkner, M. Lahn and P. E. Huber, *Neoplasia*, 2011, **13**, 537–549.
- 36 Q. Chen, L. Xu, C. Liang, C. Wang, R. Peng and Z. Liu, *Nat. Commun.*, 2016, **7**, 13193.
- 37 B. Farhood, M. Najafi and K. Mortezaee, *J. Cell. Physiol.*, 2019, **234**, 8509–8521.
- 38 S. Zhou, Q. Shang, N. Wang, Q. Li, A. Song and Y. Luan, *J. Controlled Release*, 2020, **328**, 617–630.
- 39 T. Walzer, C. Arpin, L. Beloeil and J. Marvel, *J. Immunol.*, 2002, **168**, 2704–2711.
- 40 M. Yu, X. Duan, Y. Cai, F. Zhang, S. Jiang, S. Han, J. Shen and X. Shuai, *Adv. Sci.*, 2019, **6**, 1900037.