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# Highly emissive hybrid mesoporous organometallo-silica nanoparticles for bioimaging†

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Production of mesoporous silica nanoparticles (MSNs) with uniform textural characteristics and imaging properties on a large scale is still a challenge. Thus, the design of simple and scalable methods to obtain reproducible functionalized MSNs has become even more relevant. Herein, we describe an *in situ* strategy for the synthesis and surface functionalization of highly luminescent mesoporous organometallo-silica nanoparticles. Using the [Ir(dfppy)<sub>2</sub>(daspf)]PF<sub>6</sub> chromophore and TEOS as sol-gel precursors and different capping agents, such as DMDES or APTES, three different emissive MSNs were prepared (NP<sub>OH-IS</sub>, NP<sub>Me-IS</sub> and NP<sub>NH<sub>2</sub>-IS</sub>), each containing hydroxyl, methyl and amine groups on their surfaces, respectively. All three were tested on human tumor A549 (lung carcinoma) and HeLa (cervix carcinoma) cell lines, showing intense and stable yellow phosphorescence, biocompatibility and efficient internalization. Moreover, NP<sub>Me-IS</sub> nanoparticles showed excellent colloidal stability, both in water and biological media, and a BET area of 1120 m<sup>2</sup> g<sup>-1</sup>, making them not only luminescent biomarkers, but potentially also controlled delivery vectors.

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## Introduction

The development of nanostructured materials for biomedical applications has become a leading technology, yielding a wide variety of therapeutic and diagnostic agents over the last decade.<sup>1</sup> The ever-increasing demand for efficient monitoring

of specific biological processes has called for probes that exhibit many properties including biocompatibility, high stability, good solubility and appropriate emission features. In this context, different types of nanomaterials, including selenium- or cadmium-containing quantum dots (QDs),<sup>2</sup> carbon-based nanomaterials,<sup>3</sup> noble metal nanoparticles,<sup>4</sup> magnetic nanoparticles<sup>2a,5</sup> and metal-organic frameworks (MOFs),<sup>6</sup> have been used as probes for bioimaging. Among these nanomaterials, mesoporous silica nanoparticles (MSNs) have aroused great interest primarily due to their straightforward synthesis, the versatility of both their morphology and size, which can be appropriately adjusted to target purposes,<sup>7</sup> and their relatively low-toxicity in a biological environment.<sup>8</sup> Moreover, unlike other nanoparticles, MSNs offer advantages such as outstanding chemical modularity, inertness and biodegradability.<sup>9</sup> In this field, particle sizes play an important role in determining their cellular uptake behavior. It is well known that endocytosis is the main mechanism of cellular uptake for silica nanoparticles with sizes smaller than 200 nm.<sup>8,10</sup> This is one of the reasons why the synthesis of monodisperse MSNs with diameters of approximately 100 nm has recently gained much attention. Another relevant factor is their easy surface functionalization. Unmodified MSNs possess a negative zeta potential due to dissociation of superficial silanol groups at pH > 2–3. The cellular membrane is also mostly negatively charged, but

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silanol groups allow the cell to recognize these MSNs. Nevertheless, in order to enhance cellular uptake, there are many examples of surface functionalization of MSNs with positive charges.<sup>11</sup> The benefits of this are not completely clear, as positive charges on the surface can induce an immune response or cytotoxicity when compared with anionic or neutral materials.<sup>12</sup> Also, shell formation around nanoparticles using polymers or other biocompatible molecules to enhance biocompatibility can be highly desirable.<sup>10a,11a,13</sup>

The optical transparency of silica in the visible region and chemical inertness make these MSNs exceptional substrates for the design of luminescent probes.<sup>14</sup> The design of fluorescent silica nanoparticles based on non-covalent inclusion or superficial grafting of conventional organic dyes, such as fluorescein or rhodamine, has attracted much research interest due to their remarkable properties.<sup>15</sup> However, these organic fluorescent molecules usually present aggregation-caused quenching (ACQ), and many of these inclusion approaches use reverse microemulsion or Stöber synthetic methods, leading, inevitably, to aggregation of the chromophores to produce MSNs with low emission efficiencies. To overcome this problem, several groups have doped MSNs with molecules featuring aggregation-induced emission (AIE) fluorescence or designed encapsulation methods to separate the chromophores.<sup>16</sup> Nevertheless, organic fluorophores still present several limitations such as photobleaching or small Stokes shifts and short lifetimes, which make the discrimination of their emissions from cell autofluorescence more difficult. In addition, non-covalently included or even superficially grafted chromophores can experience leaking in biological media, which causes an additional decrease of the emission and can induce biotoxicity.<sup>16c</sup>

In this context, chromophores that meet some important requirements, such as chemical- and photo-stability, large Stokes shifts or long lifetimes, would be desirable.<sup>17</sup> To meet this goal, phosphorescent transition metal complexes with a  $d^6$  ( $Ru^{II}$ ,  $Re^I$ , and  $Ir^{III}$ ) or  $d^8$  ( $Pt^{II}$ ) electronic configuration<sup>18</sup> and, predominantly, lanthanide derivatives ( $Eu^{III}$ ,  $Tb^{III}$ , and  $Yb^{III}$ )<sup>15b,19</sup> have been investigated for the preparation of emissive silica nanoparticles. Among them,  $Ir^{III}$  compounds can be considered an interesting alternative to organic fluorophores, as they display, in addition to all the above mentioned properties, high quantum yields ( $\phi$ ) and an easy adjustment of the emission wavelength by controlling the coordination ligands.<sup>20</sup> In fact, cyclometalated  $Ir^{III}$  complexes have already been extensively studied over the last few years in bioimaging and biosensing,<sup>21</sup> although many of them show considerable cytotoxicity.<sup>22</sup> This fact, very promising when using these complexes as therapeutic agents, is not desirable for their exclusive use as intracellular biomarkers. The design of MSNs for biomedical purposes by a combination of cyclometalated  $Ir^{III}$  complexes with silica nanoparticles is not very widespread<sup>23</sup> and, as far as we know, only two examples have been studied *in vivo*.<sup>23c,e</sup> Most of the reported studies involve incorporation of  $Ir^{III}$  complexes *via* encapsulation (non-covalent interactions) or through post-synthetic methods (grafting). Hence, it seems judicious to design a synthetic strategy to obtain highly

emissive MSNs with a better integration of the  $Ir^{III}$  complex in the silica matrix and, if possible, employ only small amounts of the expensive chromophore in a more effective way.

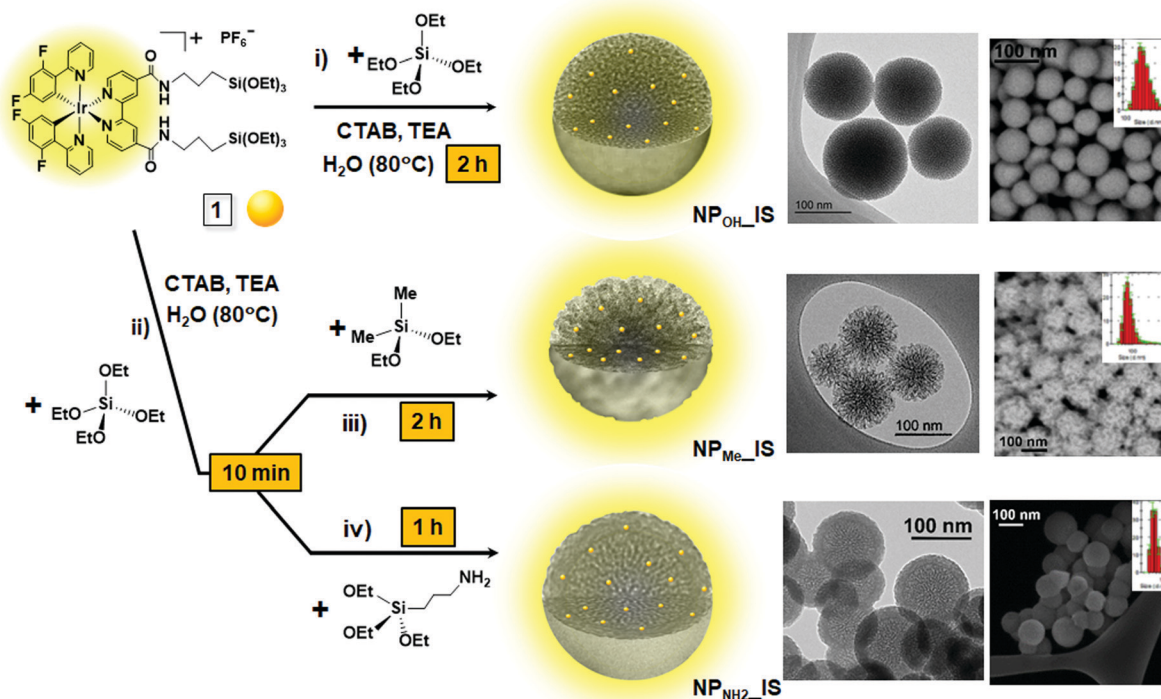
In the last few years, our group has studied the “sol-gel coordination chemistry” approach based on the *in situ* co-condensation of a silica source with small amounts of organometallic complexes bearing terminal alkoxy-silane groups.<sup>24</sup> Following this method, we have recently prepared white-light emitting discrete MSNs containing three different emissive cyclometalated  $Ir^{III}$  derivatives,<sup>25</sup> which have been used in lighting applications. Herein, we report a modification of this synthetic approach to fabricate stable, monodisperse, precisely size-controllable and brightly phosphorescent MSNs, in which the amount of dyes has been extremely reduced (less than 1 wt% of the MSN). We chose the bis(cyclometalated) complex  $[Ir(dfppy)_2(dasipy)]PF_6$  (**1**;  $dfppy$  = 2-(2,4)-difluorophenyl-pyridinyl;  $dasipy$  = *N,N'*-dipropyltriethoxysilane-2,2'-bipyridine-4,4'-dicarboxamide), which is highly emissive in solution. In an attempt to control the aggregation tendency of the nanoparticles, as well as their morphology and surface charge, *in situ* functionalization was carried out using two different capping agents, diethoxydimethylsilane (DMDES), which should make the particles more hydrophobic, and 3-aminopropyltriethoxysilane (APTES), with hydrophilic amine groups, which should give a positive charge to the nanoparticle surface. For comparison purposes, related MSNs with the chromophore grafted on their surface were also prepared. All of the *in situ* hybrid MSNs showed internalization into cells with excellent biocompatibility and high photoluminescence efficiency. Moreover, these MSNs also exhibit excellent textural properties with high surface areas (up to  $1000\text{ m}^2\text{ g}^{-1}$ ), paving the way for their future use not only as phosphorescent biomarkers, but also in controlled intramolecular delivery.

## Results and discussion

### Synthesis and characterization of the organometallic precursor and organometallo-silica nanoparticles

Highly emissive complex **1** was prepared by reacting the solvate precursor  $[Ir(dfppy)_2(NCMe)_2]PF_6$ <sup>26</sup> and a stoichiometric amount of the *dasipy* ligand,<sup>27</sup> using dichloromethane as a solvent (Scheme S1, ESI†). The complex was fully characterized by elemental analysis, mass spectrometry and the usual spectroscopic means (IR, absorption, multinuclear NMR; see the Experimental section in the ESI†). The NMR data of complex **1** show the presence of two equivalent cyclometalated groups and one symmetric *dasipy* ligand, thus confirming the proposed structure, with both cyclometalated nitrogen atoms in a mutually *trans* disposition. The FTIR spectrum of complex **1** exhibits characteristic vibration bands of the N–H and C=O units of the amide groups at *ca.*  $3327$  and  $1670\text{ cm}^{-1}$ , respectively. The strong intensity features in the high energy region correspond to the  $\nu(C-H)$  of the aromatic systems ( $>3000\text{ cm}^{-1}$ ) and aliphatic groups ( $<3000\text{ cm}^{-1}$ ),<sup>28</sup> while the absorption observed between  $1600$  and  $1400\text{ cm}^{-1}$  is characteristic of stretching vibrations within aromatic rings.<sup>29</sup>





**Scheme 1** Schematic representation of the synthesis of *in situ* hybrid mesoporous organometallo-silica nanoparticles (NP<sub>OH-IS</sub>, NP<sub>Me-IS</sub> and NP<sub>NH<sub>2</sub>-IS</sub>), including TEM and SEM images of each, showing their textural differences, as well as their DLS size distributions.

The spectrum also features intense peaks at 1163 and 1074 cm<sup>-1</sup> corresponding to  $\nu(\text{Si-O-C})$  stretching, which is commonly assigned to terminal trialkoxysilyl groups.<sup>24a</sup>

Complex 1 was used as a precursor for preparing three series of pale-yellow hybrid mesoporous organometallo-silica nanoparticles (NP<sub>Me-IS</sub>, NP<sub>OH-IS</sub> and NP<sub>NH<sub>2</sub>-IS</sub>) with three different surface functionalities. The synthetic one-pot route of all these nanoparticles is illustrated in Scheme 1 (see also the Experimental section), while their metal content and textural properties are shown in Table 1. In all cases, the amount of each reactant was calculated to achieve a nominal metal content of

*ca.* 0.2 wt%. In detail, NP<sub>OH-IS</sub> was synthesized by direct co-condensation of complex 1 and TEOS, by mixing a solution containing both reactants in ethanol with a basic aqueous solution of CTAB and triethanolamine (TEA) at 80 °C. After two hours of stirring at this temperature, spherical discrete emissive nanoparticles with an average diameter of *ca.* 180 nm were obtained (Scheme 1, i). NP<sub>Me-IS</sub> and NP<sub>NH<sub>2</sub>-IS</sub> nanoparticles, containing methyl or propylamine superficial groups, respectively, were prepared following a similar procedure, but adding the corresponding capping agent (DMDES for NP<sub>Me-IS</sub> and APTES for NP<sub>NH<sub>2</sub>-IS</sub>) after the first 10 minutes of reaction

**Table 1** Metal content and textural properties of the different organometallo-silica nanoparticles synthesized, both IS and G, in comparison with related complex-free silica nanoparticles

Sample	Ir <sup>a</sup> (wt%)	A <sub>BET</sub> <sup>b</sup> (m <sup>2</sup> g <sup>-1</sup> )	V <sub>p</sub> <sup>0.99c</sup> (cm <sup>3</sup> g <sup>-1</sup> )	d <sub>p</sub> <sup>d</sup> (nm)	ZP <sup>e</sup> (mV)	DLS size <sup>f</sup> (nm)
NP <sub>OH</sub>	—	760	1.2	3.0	n.d. <sup>g</sup>	n.d. <sup>g</sup>
NP <sub>OH-IS</sub>	0.1 (0.2)	780	1.0	3.1	-13.1 ± 0.4	180
NP <sub>OH-G</sub>	0.2 (0.2)	390	1.2	4.3	-19.0 ± 0.6	40–200
NP <sub>Me</sub>	—	980	1.6	4.8	n.d. <sup>g</sup>	n.d. <sup>g</sup>
NP <sub>Me-IS</sub>	0.1 (0.2)	1120	2.2	5.0	-22.6 ± 1.7	80
NP <sub>Me-G</sub>	0.2 (0.2)	950	1.5	5.1	-21.6 ± 0.8	40–200
NP <sub>NH<sub>2</sub></sub>	—	230	1.2	4.0	n.d. <sup>g</sup>	n.d. <sup>g</sup>
NP <sub>NH<sub>2</sub>-IS</sub>	0.2 (0.2)	100	0.4	5.2	26.3 ± 1.0	60
NP <sub>NH<sub>2</sub>-G</sub>	0.1 (0.2)	100	0.9	5.5	35.6 ± 2.5	60

<sup>a</sup> Iridium content calculated from high resolution ICP mass spectroscopy analyses after treatment of the samples with diluted HF. Values in brackets represent the nominal metal content. <sup>b</sup> BET surface area estimated by the multipoint BET method using adsorption data in the relative pressure (*P/P*<sub>0</sub>) range of 0.05–0.3. <sup>c</sup> Total pore volume read directly from the adsorption branch of the isotherm at 0.99. <sup>d</sup> Average mesopore diameter determined from the isotherm using the NLDFT equilibrium model. Samples were centrifuged and air dried before gas adsorption measurements. <sup>e</sup> ZP is zeta potential measured from Milli-Q H<sub>2</sub>O colloidal suspensions. <sup>f</sup> Dynamic light scattering (DLS) sizes were determined based on the intensity distribution. <sup>g</sup> Not determined.



at 80 °C (Scheme 1, ii). Discrete emissive nanoparticles of *ca.* 80 (NP<sub>Me-IS</sub>) or 60 nm (NP<sub>NH<sub>2</sub>-IS</sub>) were obtained after a total reaction time of two hours or one hour, respectively (Scheme 1, iii, iv). Besides their different textural properties, the three hybrid *in situ* NPs contain the chromophore homogeneously dispersed within the silica matrix and show the mesoporosity characteristic of the surfactant (CTAB) employed, which was removed by ionic exchange with a saturated ammonium nitrate solution in all cases. The molar ratio of the synthesis gel was 1.00 TEOS:6.6 × 10<sup>-4</sup> complex 1:0.060 CTAB:0.026 TEA:80.0 H<sub>2</sub>O (0.135 DMDDES or 0.023 APTES, when appropriate).

For comparative purposes, three types of related pale-yellow grafted MSNs (NP<sub>Me-G</sub>, NP<sub>OH-G</sub> and NP<sub>NH<sub>2</sub>-G</sub>) were obtained, with the chromophore conventionally attached to the surface of the NPs. To this end, the corresponding white complex-free silica nanoparticles (NP<sub>Me</sub>, NP<sub>OH</sub> and NP<sub>NH<sub>2</sub></sub>) were prepared, following the same procedures described for each of the *in situ* materials, but without the addition of the precursor complex 1 (Scheme S2, i–iv, ESI†). These complex-free nanoparticles were reacted in ethanol with an appropriate amount of complex 1 to yield a material with the same nominal silica/complex molar ratio as that obtained for hybrid *in situ* materials. These reactions were carried out using NaF as the catalyst to ensure hydrolysis and condensation of most of the alkoxy silane groups of complex 1 (Scheme S2, v and see the Experimental section, ESI†).

Incorporation of complex 1 into all types of MSNs and preservation of its molecular structure were clearly verified by absorption and emission studies (see the Photophysical properties section), ICP mass spectroscopy analyses and FTIR analysis. ICP analyses of these solids (see Table 1) gave incorporation yields between 50% and 100%, depending on the type of the NP. Thus, incorporation yields of the NP<sub>OH</sub> and NP<sub>Me</sub> samples were 50% and 100% for the *in situ* (IS) and grafted (G) materials, respectively. Nevertheless, capping with the APTES amine seems to favor the incorporation of the cationic complex 1 into the *in situ* material and to hinder grafting of the complex on the surface of the previously synthesized NP<sub>NH<sub>2</sub></sub>, thus leading to the opposite trend (100% incorporation yield for NP<sub>NH<sub>2</sub>-IS</sub> and 50% for NP<sub>NH<sub>2</sub>-G</sub>). Also, the FTIR spectra of all hybrid NPs, both *in situ* and grafted, show, in addition to the bands corresponding to the Si–O and Si–O–Si bonds (see Fig. S1, ESI†), the weak absorptions characteristic of complex 1 at *ca.* 2900 cm<sup>-1</sup> and 1500–1400 cm<sup>-1</sup>, which are due to the ν(C–H) of aliphatic groups and the ν(ring) of aromatic groups, respectively. Moreover, the FTIR spectra of the NP<sub>Me</sub> and NP<sub>NH<sub>2</sub></sub> samples (IS and G) also feature characteristic bands due to the ν(Si–CH<sub>3</sub>) (1267 cm<sup>-1</sup> and 850 cm<sup>-1</sup>) and ν(N–H) (3285 cm<sup>-1</sup> and 1390 cm<sup>-1</sup>) vibration modes, respectively, which correspond to the presence of their respective capping agents (NP<sub>Me</sub>, DMDDES; NP<sub>NH<sub>2</sub></sub>, APTES). The absence of intense peaks in the area between 1470 and 1390 cm<sup>-1</sup>, related to the C–H vibrations of CTAB, confirms the complete removal of the surfactant, which ensures a high biocompatibility when exposing the NPs to biological media.

As commented previously, all the materials are formed of well-defined spherical nanoparticles, although with clear distinctive textural properties given by the differential surface functionalization (Table 1 and Fig. S2–S4, ESI†). Regarding the hybrid *in situ* NPs (Scheme 1), those obtained in the absence of capping agent (NP<sub>OH-IS</sub>) displayed the characteristic morphology and mesoporosity of discrete MSNs prepared using CTAB as the surfactant. Through DLS analyses (Table 1 and Fig. S5, ESI†), it was found that NP<sub>OH-IS</sub> is the largest one with an average diameter of 180 nm, although inspection by electronic microscopy (TEM and FESEM, Fig. S2a, b and S4a, ESI†) seems to point to a lower average diameter of between 100 and 120 nm. NP<sub>Me-IS</sub>, capped with DMDDES, displayed an average diameter of 80 nm and a stellate morphology with an open mesoporosity (Fig. S2c, d and S4b, ESI†), while NP<sub>NH<sub>2</sub>-IS</sub>, which is the smallest one with an average diameter of 60 nm, clearly shows a core–shell morphology formed by a mesoporous core and a disordered organosilica shell of *ca.* 16 nm in diameter (Fig. S2e, f and S4c, ESI†). This fact, due to surface functionalization with APTES, would explain the blocking of their mesoporosity detected by gas adsorption measurements in these materials as described below.

The three types of complex-free control MSNs (NP<sub>Me</sub>, NP<sub>OH</sub> and NP<sub>NH<sub>2</sub></sub>; Fig. S3, ESI†) show similar sizes to those described for their related hybrid *in situ* materials (Fig. S2, ESI†). Nevertheless, as observed in the TEM and DLS results (Fig. S3 and S5, ESI†), the procedure for the synthesis of the grafted nanoparticles produces a wide dispersion of sizes for NP<sub>OH-G</sub> and NP<sub>Me-G</sub> (from 40 to 200 nm) with respect to the complex-free starting materials (NP). This fact can be associated with the presence of NaF in the reaction media, which could modify both the size and morphology of the silica nanoparticles. It is well known that the fluoride anion has been revealed as a versatile catalyst for sol–gel processes, indeed at nearly neutral pH and moderate temperatures,<sup>30</sup> although the kinetics of the reactions are still under study.<sup>31</sup> In contrast, NP<sub>NH<sub>2</sub>-G</sub> maintains a similar size distribution to that shown for NP<sub>NH<sub>2</sub>-IS</sub>, perhaps due to the presence of their organosilica shell.

With respect to physisorption studies (Table 1 and Fig. 1), all materials yielded type IV isotherms, typical of mesoporous materials. Capping of the nanoparticles with APTES provokes a partial blocking of the mesoporosity in NP<sub>NH<sub>2</sub></sub>, which shows the smallest surface area compared to those in NP<sub>OH</sub> and NP<sub>Me</sub> (230 m<sup>2</sup> g<sup>-1</sup> vs. 760 m<sup>2</sup> g<sup>-1</sup> and 980 m<sup>2</sup> g<sup>-1</sup>, respectively). The hybrid organometallo-silica nanoparticles NP<sub>OH-IS</sub> and NP<sub>Me-IS</sub> show very similar textural parameters to those observed for their control complex-free related MSNs (Table 1), which is consistent with the homogeneous integration of the organometallic complex in the silica matrix.<sup>24a</sup> Regarding their mesoporosity, NP<sub>Me-G</sub> also presents excellent textural parameters, whereas NP<sub>OH-G</sub> has half the BET surface area compared with the related NP<sub>OH-IS</sub> sample. A marked decrease in the mesopore volume is observed after incorporation of the chromophore into both the *in situ* and grafted amine functionalized MSNs (*A*<sub>BET</sub>, 230 m<sup>2</sup> g<sup>-1</sup> NP<sub>NH<sub>2</sub></sub> vs. 100 m<sup>2</sup> g<sup>-1</sup> NP<sub>NH<sub>2</sub>-IS,G</sub>).



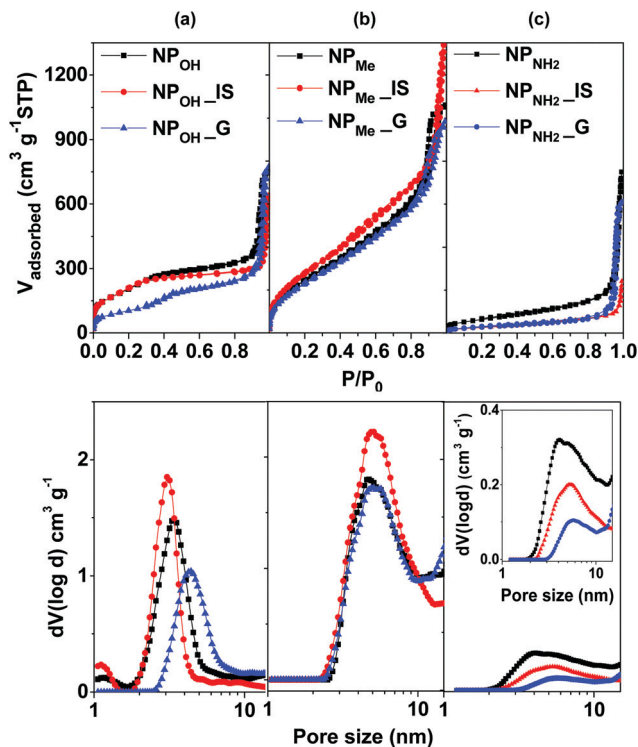


Fig. 1  $N_2$  adsorption/desorption isotherms at 77 K (above) and the corresponding pore size distribution calculated using the NLDFT method (below) of the hybrid MSNs, both *IS* and *G*, in comparison to the related complex-free silica nanoparticles (NP): (a)  $NP_{OH}$ , (b)  $NP_{Me}$ , and (c)  $NP_{NH_2}$ .

Zeta potentials of the six types of hybrid nanoparticles were measured from Milli-Q  $H_2O$  colloidal suspensions (Table 1). As expected, in these media, both unmodified  $NP_{OH}$  and methyl capped  $NP_{Me}$  show negative zeta potentials, while amine functionalized  $NP_{NH_2}$  features positive values; nevertheless, a clear trend between the values of the *in situ* and related grafted materials cannot be established. Finally, all the materials can be easily resuspended in water or biological media (see biological activity), showing good ( $NP_{OH\_IS,G}$ ) to excellent ( $NP_{Me\_IS,G}$ ) colloidal stability, except for  $NP_{NH_2\_IS,G}$ , which forms large aggregates of up to 4  $\mu m$  in water within a few hours.

To further study the stability of MSNs in the physiological medium used for the cell culture, hybrid organometallo-silica MSNs, both *in situ* and grafted, were suspended in a complete medium for six months (RPMI 1640 medium supplemented with 10% fetal bovine serum (FBS) and 2.0 mM *L*-glutamine, penicillin (100 U  $mL^{-1}$ ) and streptomycin (100  $\mu g mL^{-1}$ )). After this time, nanoparticles were centrifuged and redispersed in EtOH, still displaying their yellow emission under UV illumination. Inspection by microscopy (see Fig. S4 for FESEM and S6, ESI<sup>†</sup> for TEM) shows that all the nanoparticles were highly stable in this biological media and only the organosilica shells of  $NP_{NH_2\_IS}$  and  $NP_{NH_2\_G}$  were partially damaged. Moreover, the centrifuged mother liquors were analyzed by high resolution ICP-MS, showing an iridium metal concentration ranging from 1 to 10 ppb in all the cases, which indicates that there was

a negligible transference of the chromophore from the nanoparticles to the biological media in this period.

### Photophysical properties and theoretical calculations

The absorption and emission data of complex **1** and those of the different organometallo-silica nanoparticles (NPs) in several media are collected in Tables S1 and S2 (ESI<sup>†</sup>). Selected spectra are shown in Fig. 2, 3 and Fig. S7–S10 (ESI<sup>†</sup>). Also, TD-DFT calculations based on the optimized cation model  $1^+$  in THF have been carried out (see Fig. 2b and 4 and Fig. S11–S14 and Tables S3–S5 in the ESI<sup>†</sup>). The experimental UV-vis spectrum in tetrahydrofuran solution of complex **1** (Fig. 2a and Table S1, ESI<sup>†</sup>) is in good qualitative agreement with the calculated allowed absorptions (Fig. S13 and Table S5, ESI<sup>†</sup>). According to calculations, the intense high-energy band below 300 nm is ascribed to spin allowed  $\pi-\pi^*$  transitions located on the C<sup>^N</sup> and N<sup>^N</sup> aromatic ligands with minor metal-to-ligand contributions. The shoulder at 305 nm might be related to the transition calculated at 308 nm ( $S_{19}$ ), which corresponds to a combination of intraligand and ligand-to-ligand charge transfer transitions ( $^1IL/LL'CT$ ) (L: C<sup>^N</sup>, L': N<sup>^N</sup>), with a certain metal-to-ligand charge transfer ( $^1ML'CT$ ) character. The low energy band at 360 nm agrees with the calculated transitions at 367 ( $S_7$ ) and 369 ( $S_6$ ) nm, which are mainly associated with HOMO  $\rightarrow$  L+1 and H-4  $\rightarrow$  LUMO transitions (Fig. 2b and Table S4, ESI<sup>†</sup>). The HOMO and H-4 are located at the iridium center (ca. 40%) and the phenyl groups of both phenylpyridine ligands (ca. 60%), whereas the LUMO and L+1 are centered on the bipyridine ligand (96%). Therefore, this low energy transition is attributed to a mixture of  $^1ML'CT/LL'CT$  transitions. On the other hand, due to the strong spin-orbit coupling (SOC) associated with iridium, complex **1** also shows additional weak absorptions ( $>400$  nm) ascribed to spin-forbidden  $^3ML'CT/LL'CT$  transitions. These assignments also agree with those found for other related cyclometalated Ir(III) complexes.<sup>25</sup>

The solid state diffuse reflectance UV-vis (DRUV) spectra of all the organometallo-silica NPs (*IS*, Fig. 2a and *G*, Fig. S7, ESI<sup>†</sup>) display essentially a similar profile to that observed for complex **1** in solution, confirming the preservation of the molecular structure of the complex during its incorporation into the silica matrix.

In degassed THF solution, complex **1** emits brightly ( $\phi$  56%) in the yellow spectral region, featuring a long-life (0.7  $\mu s$ ) structureless emission band with  $\lambda_{max}$  at 550 nm (Fig. S8, ESI<sup>†</sup>). As shown in Fig. 3, the SOMO and SOMO-1 are analogous to the LUMO and HOMO in the ground state. Therefore, this emission is attributed to a mixture of  $^3ML'CT$  (Ir  $\rightarrow$  N<sup>^N</sup>)/ $^3LL'CT$  (dfppy  $\rightarrow$  N<sup>^N</sup>) with a remarkable metal character. According to this assignment, the emission is notably blue-shifted at 77 K (510 nm; Fig. S8, ESI<sup>†</sup>), and also markedly red shifted in a more polar solvent like MeOH ( $\lambda_{em}$  585 nm, 298 K; 530 nm 77 K;  $\phi$  66.4%), features that are commonly observed in cyclometalated iridium(III) polypyridine systems. There is good correlation with the calculated emission values in both solvents [ $\Delta E(T_1-S_0)$  575 nm (THF) and 587 nm (MeOH)]. The observed bathochromic shift (positive solvatochromism) indicates that



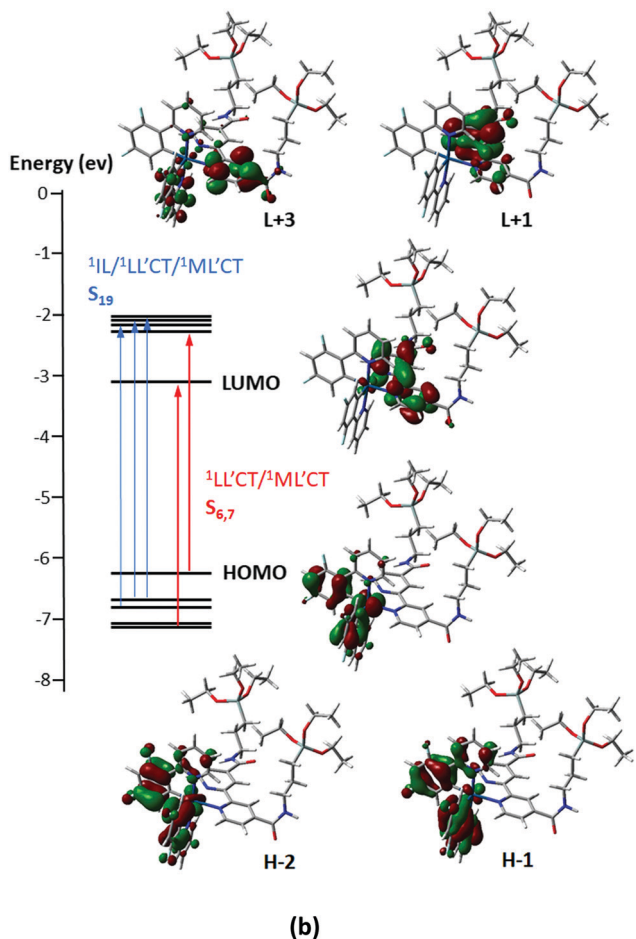
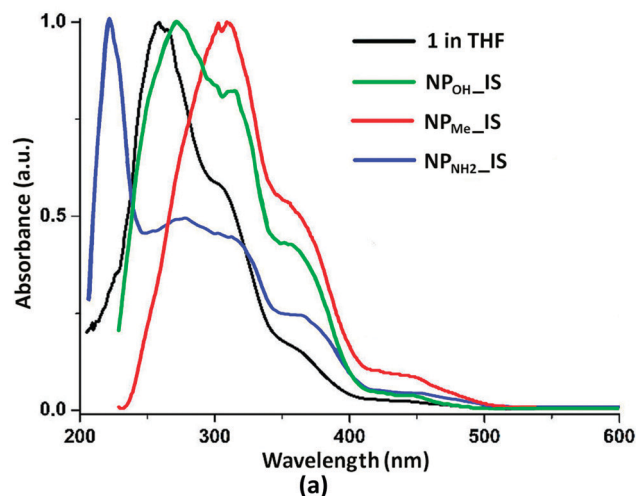


Fig. 2 (a) Comparison of the absorption spectrum of complex **1** in THF ( $5 \times 10^{-5}$  M) with those of the *in situ* NPs in the solid state. (b) Selected frontier molecular orbitals and transitions involved in the absorption spectra for complex **1**.

the excited state is more polar than the ground state as it is stabilized by the solvent polarity and consequently has a decrease in the emission energy.<sup>32</sup> In the solid state, complex **1** emission exhibits a slight red-shift ( $\lambda_{em}$  560 nm, 298 K; 550 nm 77 K; Fig. S8, ESI<sup>†</sup>), but with a shorter life time and a

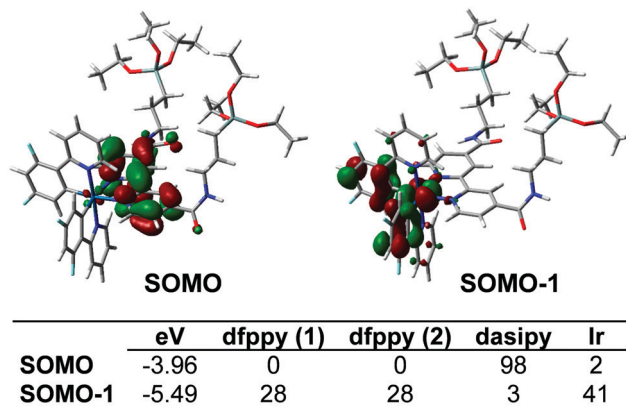


Fig. 3 SOMO and SOMO-1 orbitals and their composition (%) for the lowest excited triplet state in complex **1**.

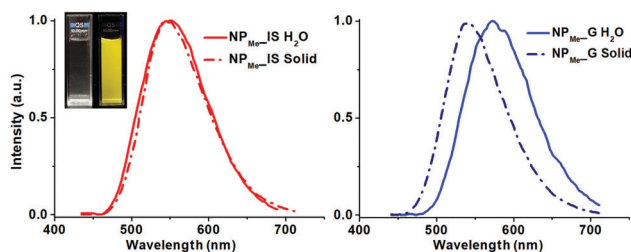


Fig. 4 Emission spectra at room temperature of  $\text{NP}_{\text{Me}}\text{-IS}$  (left, red) and  $\text{NP}_{\text{Me}}\text{-G}$  (right, blue) in the solid state (dotted line) and in water suspension (solid line). Inset: photograph of the aqueous suspension of  $\text{NP}_{\text{Me}}\text{-IS}$  under visible and UV  $\lambda_{exc}$  370 nm illumination.

lower quantum yield ( $0.35 \mu\text{s}$  and  $\phi$  29.4%), which are indicative of faster non-radiative decay compared to what occurs in solution. These features can be tentatively attributed to the presence of  $\pi$ - $\pi$  interactions in the solid state, which favor quenching due to triplet-triplet annihilation.

The photophysical properties of all the organometallo-silica NPs have been measured at room temperature in the solid state and in aqueous suspensions ( $5 \times 10^{-4}$  M) (Table S2, ESI<sup>†</sup>). The three *in situ* materials ( $\text{NP}_{\text{IS}}$ ) feature, in the solid state and in aqueous suspension, a non-structured emission band with  $\lambda_{max}$  and lifetime values ( $\lambda_{em}$  550–558 nm,  $\tau$  0.70–0.80  $\mu\text{s}$  in the solid state) similar to those found for complex **1** in the fluid THF (Fig. 4 for  $\text{NP}_{\text{Me}}\text{-IS}$  and see also Fig. S9, S10, ESI<sup>†</sup>). It is noteworthy that in spite of the small amount of chromophore incorporated into the nanoparticles (less than 1 wt% of complex **1**), the materials are highly emissive, exhibiting in the solid state comparable emission quantum yields to those found for the pure complex in THF solution ( $\phi$  41.2%  $\text{NP}_{\text{OH}}\text{-IS}$ , 50.1%  $\text{NP}_{\text{Me}}\text{-IS}$  and 52.0%  $\text{NP}_{\text{NH}_2}\text{-IS}$  vs. 56.0% complex **1**) and slightly lower values in aqueous suspension ( $\phi$  25.8%  $\text{NP}_{\text{OH}}\text{-IS}$ , 39.6%  $\text{NP}_{\text{Me}}\text{-IS}$  and 27.5%  $\text{NP}_{\text{NH}_2}\text{-IS}$ ). This is consistent with homogeneous and well-dispersed incorporation of the chromophore throughout the silica matrix during the *in situ* formation of the actual  $\text{NP}_{\text{IS}}$  hybrid, as well as with the presence of a



**Table 2** Cytotoxic  $IC_{50}$  values ( $\mu\text{g mL}^{-1}$ ) of the different organometallo-silica *in situ* (IS) and grafted (G) nanoparticles in A549 and HeLa human cell lines

Sample	A549	HeLa
$NP_{OH\_IS}$	$166.00 \pm 23.93$	$219.30 \pm 7.64$
$NP_{OH\_G}$	$184.30 \pm 32.93$	NT
$NP_{Me\_IS}$	NT	NT
$NP_{Me\_G}$	NT	NT
$NP_{NH_2\_IS}$	$93.36 \pm 5.70$	$94.36 \pm 11.82$
$NP_{NH_2\_G}$	$74.28 \pm 11.33$	$80.23 \pm 14.29$

$IC_{50}$  values are presented as mean  $\pm$  standard error of the mean of three different experiments. NT, non-toxic ( $IC_{50}$  values could not be determined).

rigid environment around the cyclometalated iridium complex. Thus, incorporation of the organometallic dye into the silica framework not only increases its rigidity, decreasing non-radiative deactivation due to molecular distortion, but also precludes the occurrence of non-covalent interactions between the chromophores. It is noteworthy that in both media the capped NPs ( $NP_{Me\_IS}$  and  $NP_{NH_2\_IS}$ ), which are smaller in size, demonstrated better emissive performance than  $NP_{OH\_IS}$ .

On the other hand, the three grafted materials ( $NP\_G$ ) show a similar broad emission ( $\lambda_{em}$  545–550 nm, Table S2, ESI<sup>†</sup>) in the solid state, but with shorter life times and lower quantum yields ( $\phi$  28–41%;  $\tau$  0.50–0.65  $\mu\text{s}$ ) than those observed for their related *in situ* nanoparticles ( $NP\_IS$ ). This fact can be attributed to a decreased protection of superficially grafted molecules of the chromophore, which are therefore exposed to the external media. Interestingly, in aqueous suspensions, all  $NP\_G$  display a clearly red-shifted emission maxima ( $\lambda_{em} \sim 570$  nm, Table S2, ESI<sup>†</sup>), a feature attributable to the likely stabilization of the excited state of the chromophore by easier interaction with the polar solvent.

### Biological properties

Given the advantageous properties shown by all the nanoparticles, such as high quantum yields, long lifetimes and good

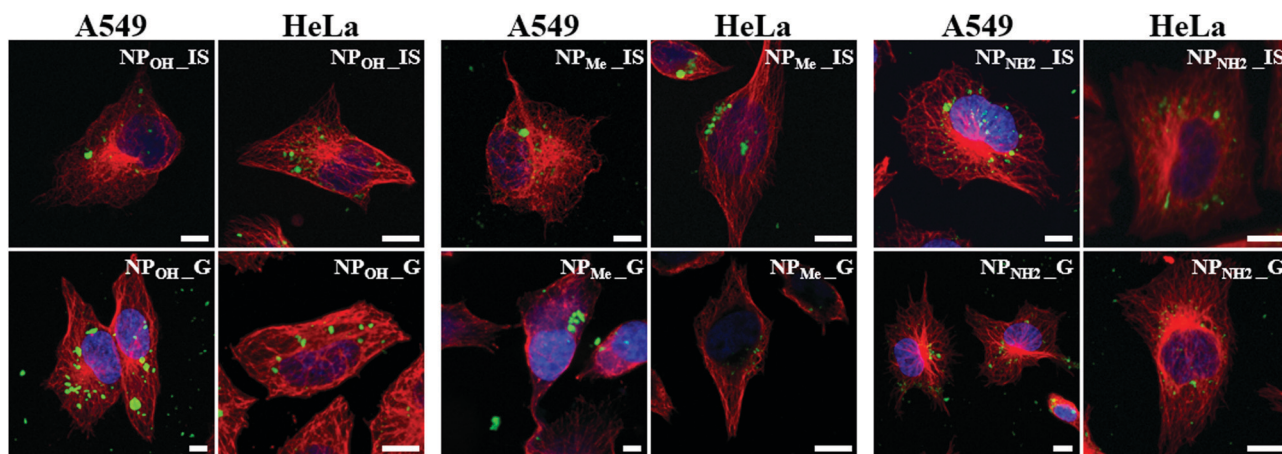
dispersion and stability in aqueous and ionic media, we decided to investigate their biocompatibility and possible use as biological markers.

### Cell viability assay

To find any possible cytotoxic effect of the organometallo-silica nanoparticles,  $IC_{50}$  values ( $\mu\text{g mL}^{-1}$ ) were determined against human tumor A549 (lung carcinoma) and HeLa (cervix carcinoma) cell lines.  $IC_{50}$  values for each of the NPs were measured *in vitro* using the MTT assay<sup>33</sup> after cellular exposure for 72 h, as we have previously described for other compounds.<sup>34</sup> All silica nanoparticles tested showed very low cytotoxicity values towards both cell lines (Table 2 and Fig. S15, S16, ESI<sup>†</sup>). Actually, both *in situ* and grafted  $NP_{Me}$  and  $NP_{OH\_G}$  nanoparticles did not affect cell viability, since their  $IC_{50}$  values could not be determined at any concentration tested. The negligible cytotoxicity shown by  $NP_{NH_2}$  ( $IC_{50}$ ,  $\mu\text{g mL}^{-1} \approx 90$  IS, 80 G) could be related to the presence of amino groups on the nanoparticle surface or to the release of these groups into the cellular environment, as previously observed in other similarly functionalized MSNs.<sup>35</sup> Interestingly, regardless of whether the iridium chromophores were primarily located in the silica matrix or on the nanoparticle surface, each nanoparticle type (OH, Me or  $NH_2$ ) presents similar  $IC_{50}$  values in spite of being IS or G, respectively. Moreover,  $IC_{50}$  values did not change significantly after six months of storage in the culture medium (Fig. S15 and S16, ESI<sup>†</sup>), corroborating the above-mentioned nanoparticle stability and the fact that they do not release any derivative with cytotoxic activity into the medium.

### Cellular uptake and cytolocalization

Once the favorable non-toxic properties of the organometallo-silica NPs were observed, their possible use as luminescent biomarkers was studied by fluorescence and confocal microscopy. To this aim,  $NP_{OH\_IS}$  and  $NP_{Me\_IS}$  were first examined in living cells by fluorescence microscopy, after being incubated for 24 h with A549 and HeLa cells in the presence of the dye Hoechst 33258 nucleic acid stain. Living cell preparations and



**Fig. 5** Cellular uptake and intracellular localization of silica nanoparticles in A549 and HeLa cells. Laser scanning confocal microscopy images of fixed cells incubated with nanoparticles (green) for 24 h and immunostained for  $\beta$ -tubulin (red). Blue: Nuclei marker (DAPI). Scale bars: 10  $\mu\text{m}$ .



documentation were performed as previously reported.<sup>36</sup> Superimposition of images obtained by alternate imaging with Nomarski visualization, Hoechst staining of nuclear DNA, and fluorescence emission of nanoparticles enabled us to decipher the fluorescence emission site inside the cells (Fig. S17, ESI†). Both types of nanoparticles seemed to be successfully internalized in the living cells and emissions were restricted to the cytoplasm, with a tendency to accumulate in perinuclear areas, excluding the nucleus in both cell lines (Fig. S17, ESI†).

Next, in order to ascertain the cytoplasmic accumulation of NPs inside the cells, we analyzed cellular uptake using confocal fluorescence imaging in fixed cells immunostained for tubulin. This stain labels the microtubules and allows visualization of the cytoskeleton and cell body outline. As expected, in the absence of organometallo-silica nanoparticles, cells did not show any emissive signals (data not shown). Incubation of cells with NPs for 24 h resulted in cellular uptake in all cases. As seen in Fig. 5, the NPs appeared aggregated in the cytoplasm, forming granules with sizes ranging from 200 nm to several microns. Intracellular distribution seems to be random, although with a clear preference for perinuclear zones, as seen in cells *in vivo* (Fig. S17, ESI†). These organometallo-silica nanoparticles are mostly excluded from the cell nucleus, a behavior previously reported with other MSNs sized > 50 nm.<sup>16a,33,37</sup> Thus, as previously suggested and based on their good cellular internalization, intensive fluorescence and low cytotoxicity, we can state that our organometallo-silica MSNs are biocompatible enough for bioimaging applications, keeping in mind that the dosage used for *in vivo* fluorescence imaging is only 50  $\mu\text{g mL}^{-1}$ .<sup>16a</sup>

### Extracellular aggregation

The relationship between the silica nanoparticles in biological media and their colloidal stability is still a matter of discussion.<sup>10b,11a,38</sup> Given the size of the NP aggregates found intracellularly, the question arises whether they were internalized as discrete particles and aggregated intracellularly, or if they aggregated extracellularly and were then internalized as larger agglomerates.

To determine which scenario was the case, we studied phosphorescent NPs found on the extracellular surface of the fixed culture media analyzed by confocal microscopy. As seen in Fig. 6a, all types of NPs located surrounding the cells were found to be forming extracellular aggregates to some degree. Morphological analyses showed that the mean size of the aggregated particles was in the range of 1–3  $\mu\text{m}$ . Nevertheless, the degree of aggregation varied between NP types. Thus,  $\text{NP}_{\text{Me}}_{\text{IS}}$ ,  $\text{NP}_{\text{Me}}_{\text{G}}$  and  $\text{NP}_{\text{OH}}_{\text{IS}}$  showed lower levels of aggregation, while  $\text{NP}_{\text{OH}}_{\text{G}}$ , and especially  $\text{NP}_{\text{NH}_2}_{\text{IS}}$  and  $\text{NP}_{\text{NH}_2}_{\text{G}}$ , showed the highest levels (Fig. 6). This result is not surprising because MSN aggregation in cell culture medium and inside cells has been reported elsewhere.<sup>39</sup> In line with the previously noted behavior observed in aqueous media, methyl functionalization seems to enhance the colloidal stability of  $\text{NP}_{\text{Me}}$  (both for *in situ* and grafted NPs) in biological media, hindering the formation of extracellular aggregates. Previous studies have

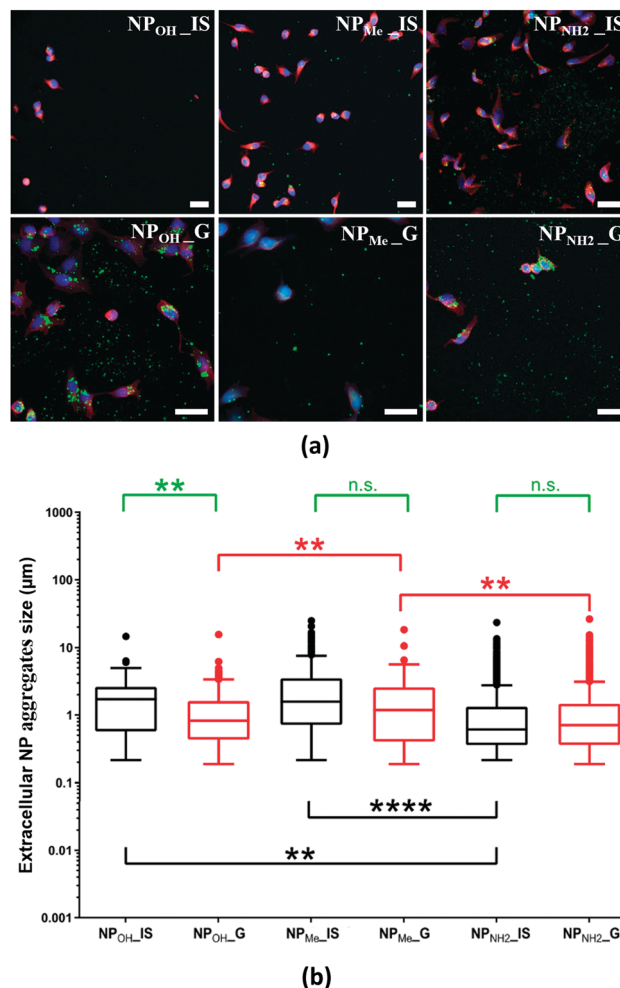


Fig. 6 Distribution and size of extracellular NP aggregates on coverslips containing growing A549 cells analyzed by laser scanning microscopy. (a) Confocal microscopy images of cells in culture showing the NP distribution in extracellular spaces. Green: NPs; red: tubulin antibody staining; and blue: nuclei marker (DAPI). Scale bars: 40  $\mu\text{m}$ . (b) Box plot representation of extracellular NP aggregate size distribution. Black boxes:  $\text{NP}_{\text{IS}}$  and red boxes:  $\text{NP}_{\text{G}}$ . Statistical comparisons were performed between  $\text{NP}_{\text{IS}}$  with different surface functionalization (black asterisks),  $\text{NP}_{\text{G}}$  with different surface functionalization (red asterisks) or between  $\text{NP}_{\text{IS}}$  and  $\text{NP}_{\text{G}}$  with the same functionalization (green asterisks). \*\*:  $p > 0.01$ , \*\*\*\*:  $p > 0.0001$ , n.s.: non-significant.

shown that long chain PEG grafting increases the colloidal stability of silica nanoparticles,<sup>11a,38a,40</sup> but as far as we know there are no similar results using aliphatic groups as short as methyl. On the other hand, the presence of amine groups ( $\text{NP}_{\text{NH}_2}_{\text{IS,G}}$ ) at the surface of the NPs favors aggregation. This fact has previously been reported for short alkyl chain amino-silanes such as APTES and can also be related to the interaction of the  $-\text{NH}_2$  groups with the components of the culture media, and easy formation of the protein corona around the nanoparticle.<sup>35a,38a,39d</sup> Finally, the greatest difference in behavior between *in situ* and grafted NPs is observed for the unmodified  $\text{NP}_{\text{OH}}$ , with  $\text{NP}_{\text{OH}}_{\text{IS}}$  showing better colloidal stability than  $\text{NP}_{\text{OH}}_{\text{G}}$  in extracellular media. In any case, the





impact of certain NP aggregation on cytotoxicity and cellular uptake is controversial and not clear,<sup>39b</sup> which indicates that it may depend on each NP structure and composition.

## Conclusions

In summary, beginning with [Ir(dfppy)<sub>2</sub>(dasipy)]PF<sub>6</sub> (1) and TEOS as precursors, we describe herein a one-pot synthetic strategy for preparing chemically inert and well-defined spherical hybrid organometallo-silica nanoparticles (NPs), which are not only highly emissive but also can be easily surface functionalized during the *in situ* procedure. Following this methodology, we prepared three types of MSNs with different surface functionalization (NP<sub>OH-IS</sub>, NP<sub>Me-IS</sub> and NP<sub>NH<sub>2</sub>-IS</sub>), which exhibit better emissive, textural and biological properties than those observed for their respective grafted counterparts (NP<sub>OH-G</sub>, NP<sub>Me-G</sub> and NP<sub>NH<sub>2</sub>-G</sub>). Despite the low chromophore complex load (less than 1 wt%), both *in situ* NPs display an intense and photostable yellow phosphorescence ( $\lambda_{em}$  ca. 550 nm;  $\phi$  40–50%), which can be easily observed in biological media. Also, these *in situ* NPs show mesoporosity with surface areas up to 1100 m<sup>2</sup> g<sup>-1</sup> for NP<sub>Me-IS</sub> and can be easily resuspended in water and biological media, where NP<sub>Me-IS</sub> and NP<sub>OH-IS</sub> show a good colloidal stability. Notwithstanding, every type of NP has been found to form extracellular aggregates in the range of 1–3  $\mu$ m in cultured media, although NP<sub>Me-IS</sub> and NP<sub>OH-IS</sub> clearly exhibit lower levels of aggregation than NP<sub>NH<sub>2</sub>-IS</sub>.

Independently of the zeta potential displayed for the nanoparticles in water (negative for NP<sub>Me-IS</sub> and NP<sub>OH-IS</sub>, and positive for NP<sub>NH<sub>2</sub>-IS</sub>), all are efficiently taken up by cells from the surrounding extracellular space as aggregates that primarily localize in the cytoplasm. This fact, combined with the absence of cytotoxicity toward cells cultured *in vitro*, even after long-term storage, demonstrates that MSNs prepared *in situ* can be used as excellent luminescent probes for cell imaging.

Finally, among all the materials described, NP<sub>Me-IS</sub> seems to be of particular interest. It is well established that long chain PEGylated MSNs show excellent colloidal stability, but in this case, this important property is obtained simply by using diethoxydimethylsilane (DMDDES) as the capping agent in the *in situ* synthesis procedure, which also allows the efficient and homogeneous incorporation of the chromophore into the silica matrix to form discrete nanoparticles of ca. 80 nm with a stellate morphology and a BET area of 1120 m<sup>2</sup> g<sup>-1</sup>. Moreover, NP<sub>Me-IS</sub> nanoparticles can be further functionalized if necessary, as observed in the behavioural study of their related grafted nanoparticle (NP<sub>Me-G</sub>).

Further studies will be needed to determine the viability of the synthetic method using other chromophores, the behavior of these hybrid organometallo-silica NPs in controlled intramolecular delivery and how they perform in *in vivo* applications.

## Conflicts of interest

There are no conflicts to declare.

## Acknowledgements

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