

# Journal of Materials Chemistry B

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1           **Formulation of Robust Organic-Inorganic Hybrid Magnetic**  
2           **Microcapsules through Hard-Template Mediated Method for**  
3           **Efficient Enzyme Immobilization**

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9       A mild and facile method for the construction of robust organic-inorganic hybrid  
10       magnetic microcapsules was developed by a hard-template mediated method  
11       coordinated with polydopamine (PDA) and Fe<sub>3</sub>O<sub>4</sub> nanoparticles onto CaCO<sub>3</sub>  
12       microparticle template. More specifically, negatively charged Fe<sub>3</sub>O<sub>4</sub> nanoparticles  
13       were adsorbed on the surface or into the lumen of porous CaCO<sub>3</sub> microparticles  
14       through electrostatic interaction and physical absorption. Then the magnetic sacrificial  
15       templates were coated with PDA through self-polymerization of dopamine to obtain  
16       the magnetic PDA-CaCO<sub>3</sub> microparticles, which were followed by the template  
17       removal using EDTA to construct organic-inorganic hybrid magnetic microcapsules.  
18       Characterizations confirmed the microcapsules possess a robust hollow structure so  
19       that enzyme inside exists in a free state. The Fe<sub>3</sub>O<sub>4</sub> nanoparticles acted critical factors  
20       in microcapsules for both recyclable component and tough scaffold to sustain the  
21       microcapsules away from collapse and fold. Combing the merits of the organic layer  
22       and inorganic component, the microcapsules were applied for encapsulation of

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23 *Candida Rugosa* Lipase (CRL). The encapsulated CRL was demonstrated to have  
24 several advantages, including increased encapsulation efficiency, enzyme activity and  
25 long-term storage stability. Hopefully, the as-prepared microbioreactor may provide a  
26 facile and generic approach for other biochemical applications.

## 27 **1. Introduction**

28 Protein capsules with tailored structures and properties have intrigued increased  
29 interesting from scientific research to technological applications such as drug/gene  
30 delivery, biocatalysis, bioreactor and nutrition<sup>1-4</sup>. When applied in specific  
31 applications, high reactive activity, controllable wall structure, and tunable protein  
32 loading amount of protein capsules should be possessed. More importantly, preferred  
33 materials to prepare protein capsules should be biocompatible, non-toxic, the  
34 operation conditions should be facile, moderate, and avoided use of harmful organic  
35 solvents and chemical cross-linkers.

36 The method currently used to fabricate protein capsules include sol-gel processing,  
37 emulsion/phase separation and layer-by-layer (LbL) self-assembly technique etc.<sup>5</sup>,  
38 which proteins can be encapsulated either in the capsule lumen or within the  
39 multilayer shells in a controlled mode<sup>6</sup>. Yu et al. and Wang et al. prepared protein  
40 capsules by protein adsorption on mesoporous silica particles templates followed by  
41 LbL self-assembly of polyelectrolyte and template removal in hydrofluoric acid  
42 buffer<sup>7,8</sup>. Chang et al. reported an easy one-pot microemulsion-templating method for  
43 protein encapsulation<sup>9,10</sup>. Cui et al. prepared protein capsules by a one-step interfacial  
44 polymerization method and the emulsion template was removed by ethanol<sup>11</sup>.

45 Although these methods demonstrated their success, some of them are inevitably  
46 suffered from tedious and time-consuming process as well as involving organic  
47 reagents and harsh post-treating conditions (such as heating, UV irradiation) which  
48 are environment unfriendly and protein deactivated<sup>12, 13</sup>. Besides, the expanded  
49 capsulizing procedures mainly composed of LbL technique which is  
50 charge-dependent interactions can be disintegrated by mutation of the pH value or the  
51 ionic strength of the surroundings, resulting in distortion, breakage, or even  
52 decomposition of capsules. Therefore, developing some facile and generic approaches  
53 for the preparation of protein capsules with desirable performance and ultimately  
54 scalable production are highly desired.

55 Our approach was inspired by the latent significance of organic-inorganic hybrid  
56 materials. Organic-inorganic hybrid materials such as carbon molecular sieves (CMS),  
57 metal-organic frameworks (MOFs), porous organic frameworks (POFs), have been  
58 widely used as outstanding templates and precursors to fabricate porous carbons and  
59 related functional materials based on their high surface areas, delicate structures,  
60 controllable features and abundant metal/organic species in their scaffolds<sup>14-16</sup>.  
61 Comprehensively, it would be ingenious and effectual to incorporate the superior  
62 separation performance and operational stability of inorganic component and the  
63 profound functionality and flexibility of organic material to fabricate hybrid  
64 microcapsules in a facile and controllable way.

65 In this study, we first introduced the magnetic property to construct the polydopamine  
66 (PDA) microcapsules to fabricate the well biocompatible and non-toxic

67 microenvironment for enzyme immobilization with convenient practical application  
68 helped by magnetic field. PDA as a wall component provides a simple, green and  
69 efficient approach to form a biocompatible microreactor with a thick-controllable,  
70 uniform and interconnectivity outer shell. In particular, the prepared magnetic PDA  
71 microcapsules not only showed practical application importance which can be easily  
72 recycled by an external magnetic field, but also helped to sustain the robust, plump,  
73 and spherical microcapsules structure when incorporated  $\text{Fe}_3\text{O}_4$  nanoparticles in the  
74 inner wall of PDA layer. As for Enzyme immobilization, CRL was encapsulated in the  
75 microcapsules accompanied with  $\text{CaCO}_3$  templates formation and then the CRL  
76 microcapsules were formed by template removal using EDTA. The shell thickness  
77 and the protein loading amount was tuned by the dopamine amount and protein  
78 doping amount, respectively. The activities and stabilities of the enzyme  
79 microcapsules over pH, temperature, kinetic behaviors, recyclability and storage time  
80 were investigated as well.

## 81 **2. Experimental Section**

### 82 **2.1 Materials**

83  $\text{FeCl}_3 \cdot 6\text{H}_2\text{O}$  and  $\text{FeCl}_3 \cdot 6\text{H}_2\text{O}$  were purchased from AiHua Fine Chemicals Co., Ltd.  
84 (China); Dopamine hydrochloride, Candida rugosa lipase (CRL, Type VII) and  
85 Bovine serum albumin (BSA) were purchased from Sigma Chemical Co.;  
86 Tris(hydroxymethyl)-amionethane (Tris), ethylenediamine tetraacetic acid disodium  
87 (EDTA), hydrochloric acid (HCl), and other chemicals and reagents were analytical  
88 grade, obtained from Tianjing Chemical Reagent Company (China).

## 89 **2.2 Preparation of citric acid coated Fe<sub>3</sub>O<sub>4</sub> nanoparticles**

90 Citric acid coated Fe<sub>3</sub>O<sub>4</sub> nanoparticles were prepared via co-precipitation of  
91 FeCl<sub>3</sub>·6H<sub>2</sub>O and FeCl<sub>2</sub>·4H<sub>2</sub>O by the addition of NH<sub>3</sub>·H<sub>2</sub>O<sup>17</sup>. In a typical procedure,  
92 3.25 g FeCl<sub>3</sub>·6H<sub>2</sub>O and 1.195 g FeCl<sub>2</sub>·4H<sub>2</sub>O were completely dissolved in 50 ml  
93 deionized water in a 100 mL round-bottom flask. The aqueous solution was heated to  
94 50 °C to obtain a clear yellow solution under vigorous stirring and purged with N<sub>2</sub>.  
95 After 30 min, 6.25 ml NH<sub>3</sub>·H<sub>2</sub>O was added into the round-bottom flask dropwise and  
96 the temperature was raised to 75 °C with the stirring continued for 60 minutes. After  
97 that, 1.5 M 6.25 ml trisodium citrate was introduced, the temperature was raised to  
98 85 °C and the stirring continued for another 90 minutes under N<sub>2</sub>. After the reaction  
99 completed, the black precipitate was collected by an external magnetic field, followed  
100 by washing several times with saturated sodium chloride, abundant deionized water  
101 and ethanol successively. Finally, the nanoparticles were dried at 40 °C in an oven  
102 under vacuum for 24 h.

## 103 **2.3 Preparation of magnetic CaCO<sub>3</sub> microparticles**

104 Uniform, spherical CaCO<sub>3</sub> microparticles with narrow size distribution (~3 μm in size)  
105 were prepared by colloidal crystallization from supersaturated solution<sup>18</sup>. Typically,  
106 0.33 M Na<sub>2</sub>CO<sub>3</sub> solution was rapidly poured into an equal volume of 0.33 M CaCl<sub>2</sub>  
107 solution at room temperature with intense agitation on a magnetic stirrer for 30  
108 seconds, and after settling without stirring for 10 minutes, the white precipitate was  
109 filtered off, thoroughly washed with deionized water and ethanol, then dried in air.  
110 To prepare magnetic CaCO<sub>3</sub> microparticles, 0.1% (w/v) Fe<sub>3</sub>O<sub>4</sub> nanoparticles was

111 suspended in deionized water and stirred under ultrasonic for 20 minutes. Then  
112  $\text{CaCO}_3$  microparticles ( $10 \text{ mg ml}^{-1}$ ) were added to the above suspension and stirred  
113 mildly for another 30 minutes. After that, the black brown powder was collected by an  
114 external magnetic field, followed by washing several times with deionized water and  
115 ethanol, and dried at  $40^\circ\text{C}$  in an oven under vacuum for 24 h.

#### 116 **2.4 Preparation of magnetic PDA microcapsules**

117  $100 \text{ mg Fe}_3\text{O}_4$  doped  $\text{CaCO}_3$  microparticles was suspended in Tris-HCl buffer (40 ml,  
118  $50 \text{ Mm}$ , pH 8.5) with a concentration of  $2 \text{ mg ml}^{-1}$ ,  $4 \text{ mg ml}^{-1}$  and  $8 \text{ mg ml}^{-1}$  of  
119 dopamine hydrochloride. The polymerization was proceed for 10 h with constant  
120 stirring at ambient temperature. Next, the black microparticles were collected by an  
121 extenal magnetic field, and washed with fresh Tris-HCl buffer until the supernatant  
122 became colorless. The magnetic PDA microcapsules were obtained after removal of  
123  $\text{CaCO}_3$  microparticles with  $0.1 \text{ M}$  EDTA solution at room tempreture.

#### 124 **2.5 Assay of CRL immobilization**

##### 125 2.5.1 CRL immobilization

126 A certain amount of CRL was dissolved in 1 ml of Tris-HCl buffer solution ( $50 \text{ Mm}$ ,  
127 pH 7.0). The enzyme solution was added into 4 ml of  $0.33 \text{ M}$   $\text{CaCl}_2$  solution and the  
128 CRL doped magnetic PDA microcapsules were prepared following the same  
129 procedure described as above (section 2.3-2.4). After the reaction completed, the  
130 immobilized CRL was filtered off and washed with Tris-HCl buffer solution ( $50 \text{ Mm}$ ,  
131 pH 7.0) several times to remove the unreacted CRL. Especially, the reaction solution  
132 and washing solution were collected to assay the amount of residual lipase.

## 133 2.5.2 Determination of Immobilization Efficiency and Lipase Activity

134 The immobilization efficiency was expressed by the amounts of enzyme bounded on  
135 supports of unite mass, and the amount of enzyme was determined by the Bradford  
136 method<sup>19</sup>, using BSA as the standard. The enzymatic activities of free and  
137 immobilized lipase were measured by the titration of the fatty acid which comes from  
138 the hydrolysis of olive oil<sup>20</sup> and reverse titration was adopted. One unit of lipase  
139 activity (U) is defined as the amount of enzyme needed to hydrolyze olive oil  
140 liberating 1.0  $\mu\text{mol}$  of fatty acid per min in the assay condition.

141 The efficiency of immobilization was evaluated in terms of activity yields and  
142 immobilization yield as follows:

$$143 \quad \text{activity yield (\%)} = \frac{C}{A}100\%$$

$$144 \quad \text{immobilization yield (\%)} = \frac{A-B}{A}100\%$$

145 Where A is the activity of lipase added in the initial immobilization solution, B is the  
146 total activity of the residual lipase in the immobilization and washing solution after  
147 the immobilization procedure, and C is the activity of the immobilized lipase,  
148 respectively.

149 The relative activity (%) is the ratio between the activity of every sample and the  
150 maximum activity of the sample.

151 The residual activity (%) is the ratio between the activity of each sample and the  
152 initial activity of the sample.

153 All data used in these formulas are the average of triplicate of experiments.

154 2.5.3 Effect of pH and temperature of free and immobilized lipase activities

155 A certain amount free and the immobilized CRL were incubated in 0.1 M 50 ml  
156 phosphate buffer under the variety of pH (3.0-9.0) by hydrolysis of olive oil in a water  
157 bath at 37 °C for 30 min with continuous stirring, respectively. Then the enzymatic  
158 activities were determined and the relative activity was calculated.

159 The effect of temperature on the activities of free and the immobilized CRL were  
160 measured among the temperature range of 20-90 °C for 30 min and the relative  
161 activity was compared.

162 2.5.4 Reusability and storage stability

163 The reusability of immobilized CRL were determined by hydrolysis of olive oil with  
164 the recovered lipase after magnetic separation and thoroughly washed with phosphate  
165 buffer (0.1 M pH 7.0). Finally, the activities of the subsequent enzymatic reaction  
166 were compared with that of the first running (relative activity defined as 100%).

167 The storage stability was determined by measuring the residual activity of  
168 encapsulated CRL at 37 °C after it was stored at 4 °C for a certain period of time.

169 2.5.5 Kinetic Parameters ( $K_m$  and  $V_{max}$ ) of free and immobilized CRL

170 The Michaelis constant ( $K_m$ ) and the maximum reaction velocity ( $V_{max}$ ) of free and  
171 immobilized CRL were determined by measuring initial rates of the reaction in  
172 phosphate buffer (0.1 M, pH 7.0) at 37 °C. Equivalent free or the immobilized CRL  
173 was added into olive oil emulsification solution with different concentrations from  
174 0.4-2.0 mg ml<sup>-1</sup>, and the enzymatic activities were determined.  $K_m$  and  $V_{max}$  for the  
175 free and immobilized CRL were calculated using the Michaelis-Menten model:

$$\frac{1}{V} = \frac{K_m}{V_{max}} \times \frac{1}{[S]} + \frac{1}{V_{max}}$$

176  
177 where  $V$  ( $U\ mg^{-1}$ ) was the initial reaction rate,  $[S]$  ( $ml\ mg^{-1}$ ) was the initial substrate  
178 concentration,  $V_{max}$  ( $U\ mg^{-1}$ ) was the maximum reaction rate obtained at infinite  
179 initial substrate concentration, and  $K_m$  ( $mg\ ml^{-1}$ ) was the Michaelis-Menten constant.

## 180 **2.6 Characterization**

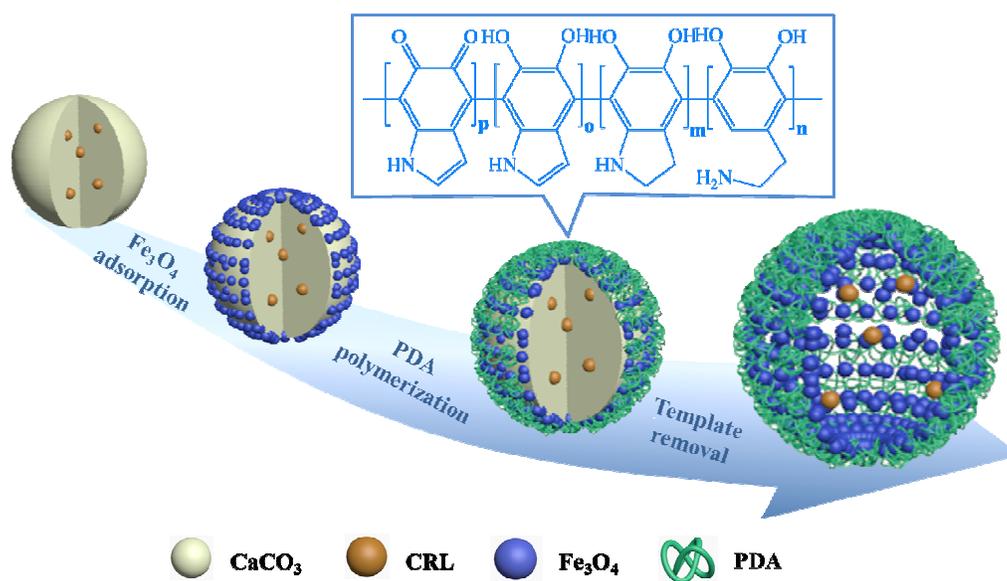
181 Fourier transform infrared (FTIR) spectra were obtained in transmission mode on a  
182 FTIR spectrometer (American Nicolet Corp. Model 170-SX) using the KBr pellet  
183 technique. The morphologies of the samples were characterized by a field-emission  
184 scanning electron microscopy (SEM, Hitachi S-4800, Japan) and transmission  
185 electron microscope (TEM, FEI Tecna G<sup>2</sup>F30) equipped with energy-dispersive  
186 X-ray spectroscopy (EDX, Oxford Instrument), high angle annular dark field  
187 (HAADF) and scanning transmission electron microscopy (STEM) to elucidate the  
188 dimensions and the structural details of the microcapsules. Magnetization  
189 measurements were performed on a Vibrating sample magnetometer  
190 (LAKESHORE-7304, USA) at room temperature. The thermal stability of samples  
191 was studied with a thermogravimetry (TG) analyzer (STA449C, Netzsch, Germany) at  
192 heating rate of  $10\ ^\circ C\ min^{-1}$  in a nitrogen atmosphere.

## 193 **3. Result and discussion**

### 194 **3.1 Preparation and characterization of hybrid microcapsules**

195 Our approach to formulate hybrid microcapsules by depositing polydopamine onto  
196 magnetic sacrificial template is shown in Fig. 1. Construction of biological capsules is  
197 limited by the crucial prerequisite conditions such as mild formation and gentle

198 removal of templates. The porous  $\text{CaCO}_3$  microparticles have been widely used as  
 199 templates for bioactive compounds encapsulation<sup>14, 21-23</sup>. The pore size distribution of  
 200 the as-prepared  $\text{CaCO}_3$  microparticles is from 20 to 60 nm and the  $\xi$ -potential at pH  
 201 7.0 is positively charged<sup>18</sup>. Based on the ingenious features,  $\text{CaCO}_3$  microparticles can  
 202 adsorb negatively charged  $\text{Fe}_3\text{O}_4$  nanoparticles (modified by citric acid in this work)  
 203 with a diameter of about 10-15 nm into the lumen or on the surface of  $\text{CaCO}_3$   
 204 microparticles. After the spontaneous self-polymerization of dopamine on the surface  
 205 of the magnetic  $\text{CaCO}_3$  template, the subsequent dissolution of  $\text{CaCO}_3$  using EDTA  
 206 was performed so that the complex of  $\text{Ca}^{2+}$  with EDTA could easily permeate through  
 207 the polymer walls. Thus the PDA- $\text{Fe}_3\text{O}_4$  microcapsules were successfully acquired.

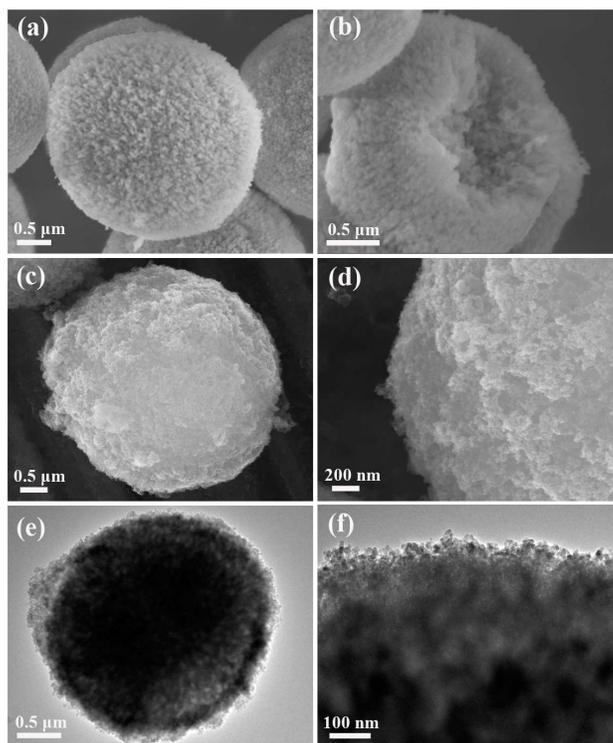


208

209 **Fig. 1** Schematic illustration of the synthesis process used to produce  $\text{Fe}_3\text{O}_4$ -PDA  
 210 microcapsule.

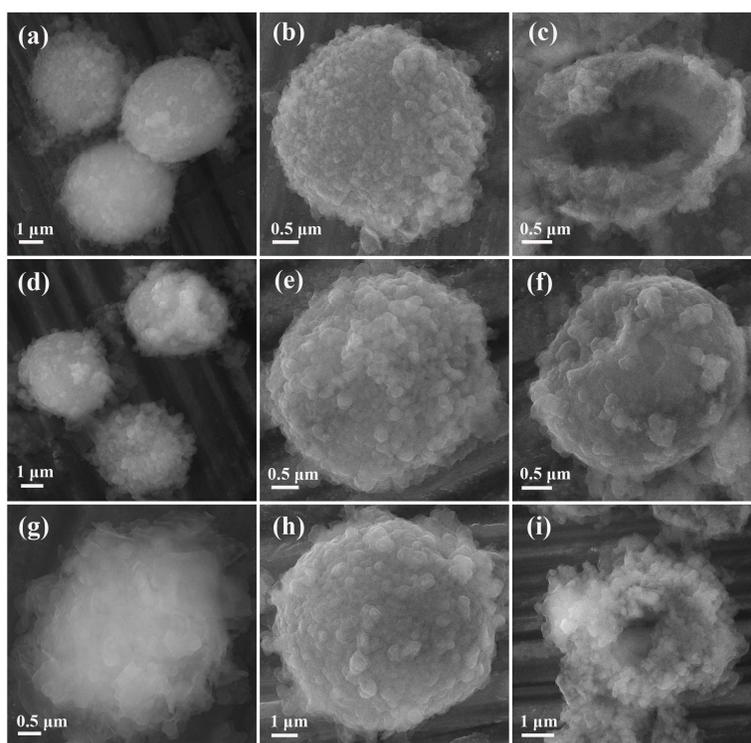
211 The morphologies of the prepared magnetic  $\text{CaCO}_3$  templates are characterized by  
 212 SEM and TEM. As shown in Fig. 2, the spherical  $\text{CaCO}_3$  microparticles with a  
 213 diameter about  $\sim 3 \mu\text{m}$  possessed porous, channel-like internal structure (Fig. 2a, b).

214 Actually, the microparticles were formed by the instant aggregation of amorphous  
215 nanoprecipitates upon mixing the  $\text{CaCl}_2$  and  $\text{Na}_2\text{CO}_3$  solutions, and the size  
216 distribution and pore density of the  $\text{CaCO}_3$  microparticles are directly dependent on  
217 the agitation speed. The rapid and intense agitation would lead to a smaller particle  
218 size and loose porous structure<sup>23</sup>. After adsorption of negatively charged  $\text{Fe}_3\text{O}_4$   
219 nanoparticles at neutral condition, the surface of  $\text{CaCO}_3$  microparticles became coarse  
220 and texture overload (Fig. 2c, d), and it also can be observed clearly from the TEM  
221 images of magnetic  $\text{CaCO}_3$  microparticles that many  $\text{Fe}_3\text{O}_4$  nanoparticles were  
222 assembled on  $\text{CaCO}_3$  microparticles (Fig. 2e, f), suggesting that the  $\text{Fe}_3\text{O}_4$   
223 nanoparticles were deposited homogeneously.



224  
225 **Fig. 2** SEM images of (a, b)  $\text{CaCO}_3$  microparticles, (c, d)  $\text{Fe}_3\text{O}_4$ - $\text{CaCO}_3$  microparticles,  
226 and TEM images of (e, f)  $\text{Fe}_3\text{O}_4$ - $\text{CaCO}_3$  microparticles.

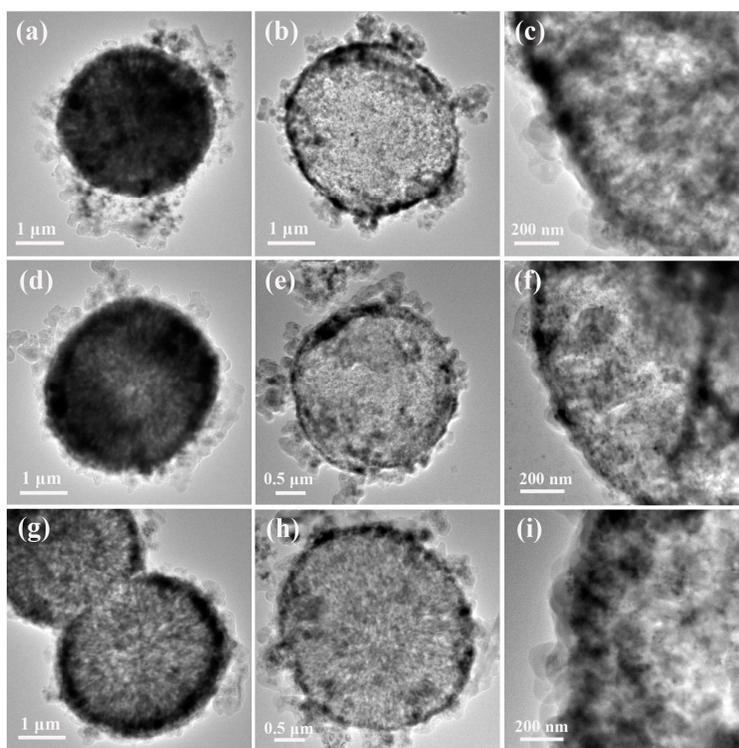
227 Several batches of  $\text{Fe}_3\text{O}_4$ -PDA microcapsules were prepared to vary the concentration  
228 of dopamine in reaction mixtures as followed:  $2 \text{ mg ml}^{-1}$  ( $\text{PDA}_2\text{-Fe}_3\text{O}_4$ ),  $4 \text{ mg ml}^{-1}$   
229 ( $\text{PDA}_4\text{-Fe}_3\text{O}_4$ ), and  $8 \text{ mg ml}^{-1}$  ( $\text{PDA}_8\text{-Fe}_3\text{O}_4$ ). As shown by SEM (Fig. 3), after PDA  
230 polymerization, the surface of the  $\text{Fe}_3\text{O}_4\text{-CaCO}_3$  microparticles became rough with the  
231 increased concentration of dopamine (Fig. 3a, d, g), and high concentration of  
232 dopamine lead to a grainy surface, as illustrated in the case of  $\text{PDA}_8\text{-Fe}_3\text{O}_4\text{-CaCO}_3$   
233 microparticles (Fig. 3g). Interestingly, after template dissolved by EDTA, all the three  
234 kinds the  $\text{PDA-Fe}_3\text{O}_4$  microcapsules holded the plump, spherical structure away from  
235 collapse and fold upon a large cavity (Fig. 3b, c, e, f, h, i), which is superior to the  
236 same sort of polymer microcapsules prepared in other reports<sup>1,5,11,23,24</sup>. This  
237 phenomenon can be attributed to the  $\text{Fe}_3\text{O}_4$  nanoparticles wrapped in the thick PDA  
238 layers which acted as scaffold in each microcapsules.



239

240 **Fig. 3** SEM images of (a) PDA<sub>2</sub>-Fe<sub>3</sub>O<sub>4</sub>-CaCO<sub>3</sub> microparticles, (b, c) PDA<sub>2</sub>-Fe<sub>3</sub>O<sub>4</sub>  
241 microcapsule, (d) PDA<sub>4</sub>-Fe<sub>3</sub>O<sub>4</sub>-CaCO<sub>3</sub> microparticles, (e, f) PDA<sub>4</sub>-Fe<sub>3</sub>O<sub>4</sub> microcapsule,  
242 (g) PDA<sub>8</sub>-Fe<sub>3</sub>O<sub>4</sub>-CaCO<sub>3</sub> microparticle, and (h, i) PDA<sub>8</sub>-Fe<sub>3</sub>O<sub>4</sub> microcapsule  
243 (half-capsules of c and i were made from broken CaCO<sub>3</sub> microparticles by grinding  
244 and ultrasound of the as-prepared CaCO<sub>3</sub> microparticles).

245 To further confirm the inner structure of PDA-Fe<sub>3</sub>O<sub>4</sub> microcapsules, we conducted the  
246 TEM images. As can be seen from Fig. 4, after template removal the hollowed  
247 microcapsules were formed and no folds and creases appeared (Fig. 4 a, b, d, e, g, h).  
248 The wall of the microcapsules PDA<sub>2</sub>-Fe<sub>3</sub>O<sub>4</sub>, PDA<sub>4</sub>-Fe<sub>3</sub>O<sub>4</sub>, and PDA<sub>8</sub>-Fe<sub>3</sub>O<sub>4</sub> became  
249 thicker with the increase of the dopamine concentrations (Fig. 4 b, e, h). Besides, it  
250 can be clearly observed that Fe<sub>3</sub>O<sub>4</sub> nanoparticles were wrapped in the polymer layer  
251 after CaCO<sub>3</sub> microparticles dissolution (Fig. 4 c, f, i). Thus, the hollow and intact  
252 structure of PDA-Fe<sub>3</sub>O<sub>4</sub> microcapsules inheriting the superior structural stability of  
253 the hybrid microcapsules were successfully obtained.

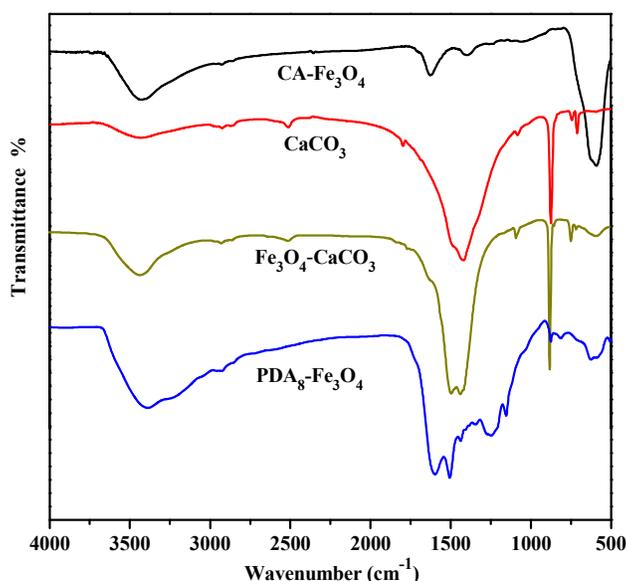


254

255 **Fig. 4** TEM images of (a) PDA<sub>2</sub>-Fe<sub>3</sub>O<sub>4</sub>-CaCO<sub>3</sub> microparticle, (b, c) PDA<sub>2</sub>-Fe<sub>3</sub>O<sub>4</sub>  
256 microcapsule, (d) PDA<sub>4</sub>-Fe<sub>3</sub>O<sub>4</sub>-CaCO<sub>3</sub> microparticle, (e, f) PDA<sub>4</sub>-Fe<sub>3</sub>O<sub>4</sub> microcapsule,  
257 (g) PDA<sub>8</sub>-Fe<sub>3</sub>O<sub>4</sub>-CaCO<sub>3</sub> microparticles, and (h, i) PDA<sub>8</sub>-Fe<sub>3</sub>O<sub>4</sub> microcapsule.

258 The functional groups of the as-prepared hybrid microparticles and microcapsules  
259 were examined using FTIR (Fig. 5). Compared with pure CaCO<sub>3</sub> microparticles, new  
260 characteristic peak at 580 cm<sup>-1</sup> of Fe<sub>3</sub>O<sub>4</sub>-CaCO<sub>3</sub> microparticles appeared after  
261 adsorption of Fe<sub>3</sub>O<sub>4</sub> nanoparticles, which can be ascribed to the lattice absorption of  
262 Fe<sub>3</sub>O<sub>4</sub> nanoparticles. In the spectrum of PDA<sub>8</sub>-Fe<sub>3</sub>O<sub>4</sub> microcapsules, the broad  
263 adsorption bands within new peaks at 1599 cm<sup>-1</sup> and 1508 cm<sup>-1</sup> originated from the  
264 benzene ring structure. The adsorption bands from 1400 to 1100 cm<sup>-1</sup> can be attributed  
265 to -CH<sub>2</sub> bending vibration (1347 cm<sup>-1</sup>), C-O-H asymmetric bending vibration (1288  
266 cm<sup>-1</sup>), C-O asymmetric vibration (1249 cm<sup>-1</sup>) and C-N stretching vibration (1155

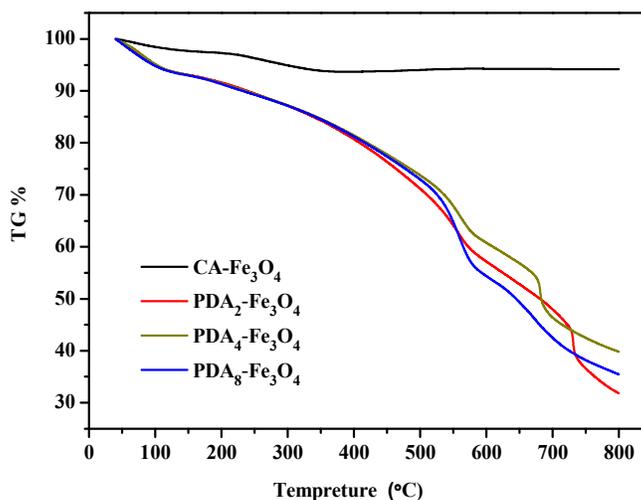
267  $\text{cm}^{-1}$ ), respectively<sup>25</sup>. In addition, it could be noted that the peak at about  $3390 \text{ cm}^{-1}$  of  
 268  $\text{PDA}_8\text{-Fe}_3\text{O}_4$  microcapsules is broader than that of  $\text{Fe}_3\text{O}_4\text{-CaCO}_3$  microparticles,  
 269 which resulted from the overlapping of hydroxyls, water adsorbed in PDA polymer  
 270 and amines of PDA<sup>26</sup>.



271  
 272 **Fig. 5** FTIR spectra of the as-prepared CA-Fe<sub>3</sub>O<sub>4</sub> nanoparticles, CaCO<sub>3</sub> microparticles,  
 273 Fe<sub>3</sub>O<sub>4</sub>-CaCO<sub>3</sub> microparticles, and PDA<sub>8</sub>-Fe<sub>3</sub>O<sub>4</sub> microcapsules.

274 The composition of PDA-Fe<sub>3</sub>O<sub>4</sub> microcapsules were characterized by TG analysis  
 275 under N<sub>2</sub> atmosphere (Fig. 6). CA-Fe<sub>3</sub>O<sub>4</sub> showed a mild weight loss (3.7 wt%) below  
 276 200 °C which can be assigned to the evaporation of absorbed water and solvent.  
 277 When the temperature rose to 400 °C, another weight loss (2.3 wt%) was observed  
 278 due to the decomposition of citric acid. Then it kept no decline until the temperature  
 279 rose to 800 °C which is indicative of the remarkable thermo-stability of Fe<sub>3</sub>O<sub>4</sub>. The  
 280 TG curves of three kinds of PDA-Fe<sub>3</sub>O<sub>4</sub> microcapsules retained the same trend under  
 281 200 °C until the temperature rose to 600 °C. A large mass loss (43.7 wt% for  
 282 PDA<sub>2</sub>-Fe<sub>3</sub>O<sub>4</sub>, 45.1 wt% for PDA<sub>4</sub>-Fe<sub>3</sub>O<sub>4</sub>, and 48.8 wt% for PDA<sub>8</sub>-Fe<sub>3</sub>O<sub>4</sub>, respectively)

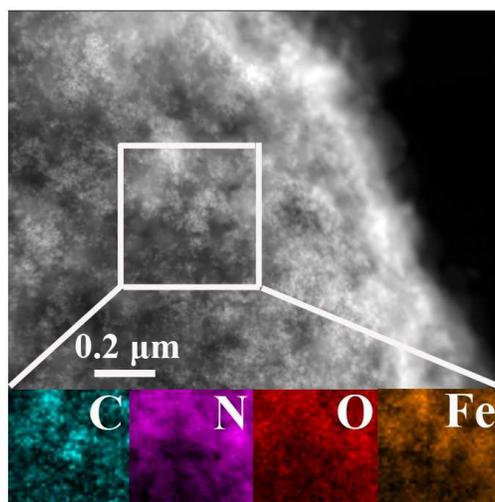
283 was observed between 200 and 700 °C which was resulted from the decomposition of  
284 PDA. TG analysis also improved the successful preparation of the magnetic hybrid  
285 microcapsules.



286

287 **Fig. 6** TG curves of CA-Fe<sub>3</sub>O<sub>4</sub> nanoparticles and PDA-Fe<sub>3</sub>O<sub>4</sub> microcapsules.

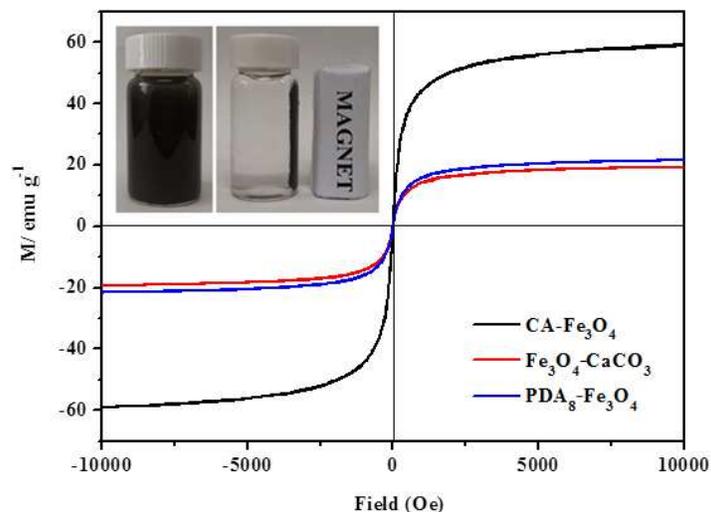
288 Next, energy-dispersive X-ray spectroscopy elemental mapping was used to  
289 understand the distribution of elements in the microcapsules. From the elemental  
290 distribution of carbon, nitrogen, oxygen and iron in Fig. 7, we can recognize that C, N,  
291 O and Fe distributed uniformly throughout the specific area in PDA<sub>8</sub>-Fe<sub>3</sub>O<sub>4</sub>  
292 microcapsules. To further characterize the porosity of PDA<sub>8</sub>-Fe<sub>3</sub>O<sub>4</sub> microcapsules,  
293 BET analysis was employed. The specific surface area of hybrid layer was 29 m<sup>2</sup> g<sup>-1</sup>,  
294 the pore size and volume were 15.6 nm and 0.11 m<sup>3</sup> g<sup>-1</sup>, respectively. Thus, the  
295 mesoporous structure of the hybrid microcapsules would act as a semipermeable  
296 membrane which could selective through molecules to prevent the large encapsulated  
297 molecules (cell and proteins) from leaching and make small molecules access and  
298 leave easily<sup>22</sup>.



299

300 **Fig. 7** STEM image and corresponding carbon, nitrogen, oxygen and iron elemental  
301 mapping of PDA<sub>8</sub>-Fe<sub>3</sub>O<sub>4</sub> microcapsules.

302 The hysteresis loops of the prepared magnetic nanoparticles are shown in Fig. 8. From  
303 Fig. 8 we can see that the saturation magnetization (MS) values are about 59.21 emu  
304 g<sup>-1</sup> for CA-Fe<sub>3</sub>O<sub>4</sub> nanoparticles, 19.45 emu g<sup>-1</sup> for Fe<sub>3</sub>O<sub>4</sub>-CaCO<sub>3</sub> microparticles and  
305 21.72 emu g<sup>-1</sup> for PDA<sub>8</sub>-Fe<sub>3</sub>O<sub>4</sub> microcapsules, respectively. Although the MS value of  
306 PDA<sub>8</sub>-Fe<sub>3</sub>O<sub>4</sub> microcapsules declined seriously, it still has an accepted property for  
307 simple magnetic separation. Furthermore, there are no hysteresis in the magnetization  
308 with both remanence and coercivity being zero, indicating that the as-prepared  
309 PDA<sub>8</sub>-Fe<sub>3</sub>O<sub>4</sub> microcapsules are superparamagnetic at room pempreture<sup>27</sup>. The insert  
310 of Fig. 8 demonstrated that PDA<sub>8</sub>-Fe<sub>3</sub>O<sub>8</sub> microcapsules can be easily manipulated by  
311 an external magnetic field, which reveals that the magnetic support possessed a  
312 suitable property for magnetic actuation and manipulation.



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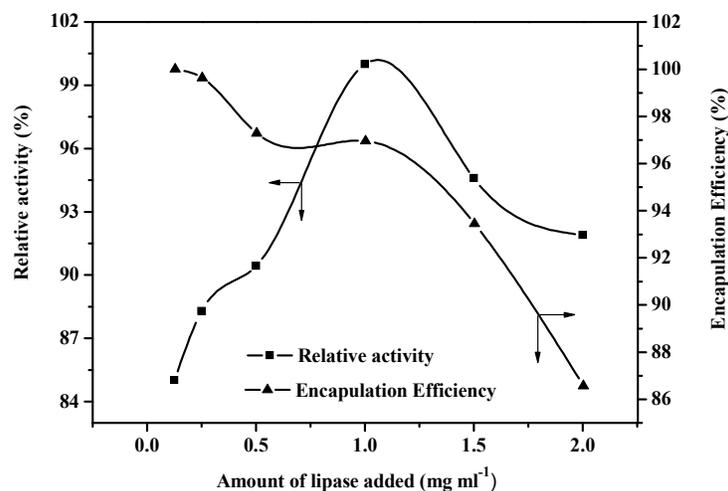
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**Fig. 8** Magnetic hysteresis loops of CA-Fe<sub>3</sub>O<sub>4</sub> nanoparticles, Fe<sub>3</sub>O<sub>4</sub>-CaCO<sub>3</sub> microparticles, and PDA<sub>8</sub>-Fe<sub>3</sub>O<sub>4</sub> microcapsules (the insert is the schematic of the simple magnetic separation of PDA<sub>8</sub>-Fe<sub>3</sub>O<sub>4</sub> microcapsules).

### 3.2 Application of Fe<sub>3</sub>O<sub>4</sub>-PDA hybrid microcapsules for enzyme immobilization and enzyme catalysis

For the CRL immobilization, PDA<sub>8</sub>-Fe<sub>3</sub>O<sub>4</sub> microcapsules were used. The enzyme encapsulation efficiency for PDA<sub>8</sub>-Fe<sub>3</sub>O<sub>4</sub> microcapsules was investigated in detail. Specifically, the enzyme encapsulation efficiency was determined with the enzyme concentration varied from 0.1 to 2.0 mg ml<sup>-1</sup>. Accordingly, as shown in Fig. 9, the enzyme encapsulation efficiency decreased monotonically with the increase of enzyme concentration and the immobilized enzyme exhibited an increased activity, simultaneously. At the concentration of 1.0 mg ml<sup>-1</sup>, the relative activity of immobilized CRL reached the highest value. Then it can be speculated that the CRL was easily to be entrapped by the CaCO<sub>3</sub> microparticles, which finally rendered enhanced effective enzyme encapsulation efficiency. Moreover, to evaluate the

329 enzymatic properites, the kinetics of the immobilized CRL with the concentration of  
 330  $1.0 \text{ mg ml}^{-1}$  in  $\text{PDA}_8\text{-Fe}_3\text{O}_4$  microcapsules ( $\text{CRL}_{1.0}\text{-PDA}_8\text{-Fe}_3\text{O}_4$ ) were calculated  
 331 from an enzymatic assay by Michaelis-Menten enzyme kinetics model (Table 1).  
 332 Compared with free CRL, the  $K_m$  for the  $\text{CRL}_{1.0}\text{-PDA}_8\text{-Fe}_3\text{O}_4$  is lower than the free  
 333 form, suggesting a higher affinity of the CRL towards the substrates after  
 334 encapsulation. The improved affinity was mainly due to the well biocompatibility of  
 335 the PDA which provided increased access probability of the substrate molecules to  
 336 contact CRL in the appropriate inner microenviroment.  $V_{\max}$  of the immobilized  
 337 CRL is also lower than the free CRL, indicated that the microencapsulation restricted  
 338 the activity of enzyme, which possibly due to the diffusional resistance of the capsule  
 339 wall.



340

341 **Fig. 9** Effect of enzyme amount and encapsulation efficiency of  $\text{PDA}_8\text{-Fe}_3\text{O}_4$ 

342

microcapsules.

343

**Table 1.** Kinetic Parameters of Free CRL and  $\text{CRL}_{1.0}\text{-PDA}_8\text{-Fe}_3\text{O}_4$  microcapsules.

$K_m$ ( $\text{mg ml}^{-1}$ )	$V_{\max}$ ( $\text{U mg}^{-1}$ )
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Free CRL	0.43	6.05
CRL <sub>1.0</sub> -Fe <sub>3</sub> O <sub>4</sub> -PDA <sub>8</sub>	0.32	5.04

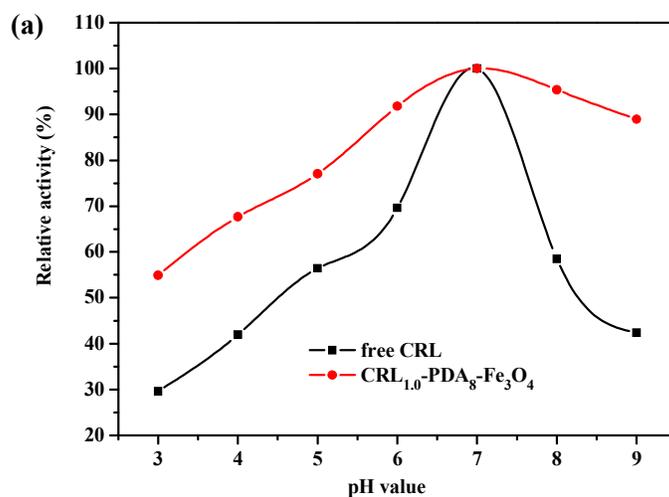
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344 The pH stability of CRL<sub>1.0</sub>-PDA<sub>8</sub>-Fe<sub>3</sub>O<sub>4</sub> microcapsules and free CRL is compared in  
345 Fig. 10a. At pH 3.0, the free CRL retained 29% of the relative activity while  
346 CRL<sub>1.0</sub>-Fe<sub>3</sub>O<sub>4</sub>-PDA<sub>8</sub> kept it at 59%. At pH 9.0, the free CRL retained 42% of the  
347 relative activity while CRL<sub>1.0</sub>-PDA<sub>8</sub>-Fe<sub>3</sub>O<sub>4</sub> kept 89% of its initial activity. In addition,  
348 CRL<sub>1.0</sub>-PDA<sub>8</sub>-Fe<sub>3</sub>O<sub>4</sub> showed broader pH scope. This phenomenon can be explained by  
349 the buffering effect of the organic layer of the microcapsules. The abundant -OH/-O<sup>-</sup>  
350 pairs and the -NH<sub>2</sub>/-NH<sub>3</sub><sup>+</sup> pairs on PDA made it a zwitter-ion under different pH  
351 range<sup>28</sup> which could tune the local pH value. Thus the CRL near the hybrid walls  
352 would stay in the buffer region against the environmental mutation.

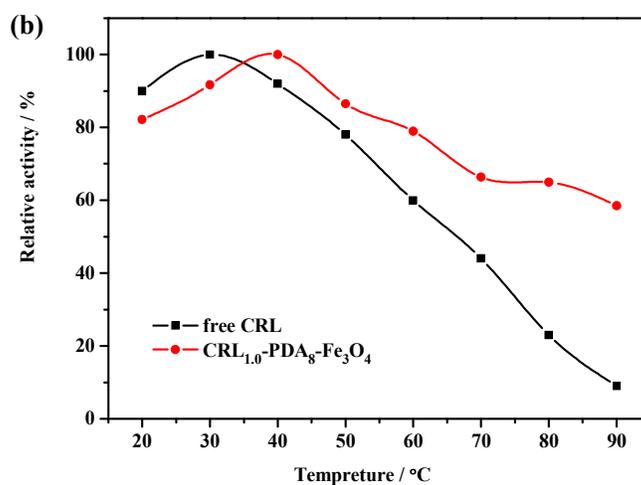
353 When the hydrolysis for olive oil emulsion was operated at a series of temperature  
354 range, the immobilized CRL showed enhanced relative activities than the free CRL  
355 (Fig. 10b). Compared with free lipase, the immobilized CRL kept its relative activity  
356 up to 80% in the temperature range of 20-60 °C and exhibited more than 60% of  
357 relative activity at 90 °C, revealed much superior heat endurance than that of the free  
358 lipase. It seemed that the robust hybrid wall structure conducted a tough performance  
359 with enzymes from denaturation at high temperatures.

360 The well reusability of lipase is critical for the potential application in industry. As  
361 presented in Fig. 10c, the immobilized enzyme kept the high activity at 75% after 12  
362 times reuse due to the sturdy stability of the hybrid microcapsules which effectively  
363 ameliorated the denaturation and leakage of enzyme under multiple reaction circles.

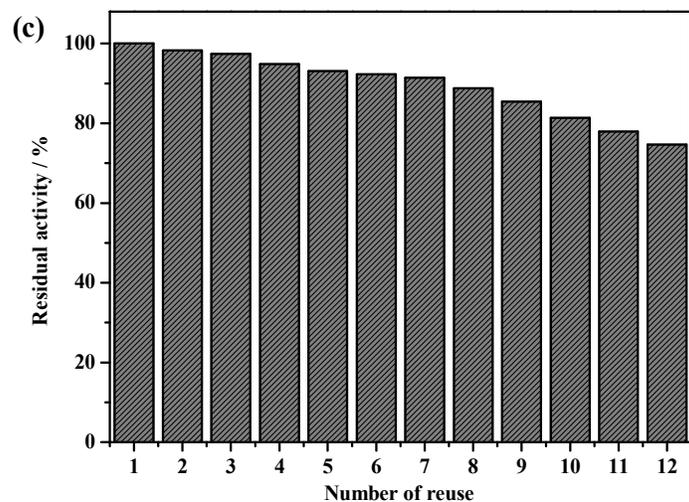
364 The storage stability of  $\text{CRL}_{1.0}\text{-PDA}_8\text{-Fe}_3\text{O}_4$  is shown in Fig. 10d. After storage at  
365 4 °C for 35 days,  $\text{CRL}_{1.0}\text{-PDA}_8\text{-Fe}_3\text{O}_4$  can maintain the residual activity as high as 82%.  
366 The activity of the immobilized enzyme was significantly improved with a lowered  
367 decreasing rate. The enhancement of the stability revealed that the hybrid  
368 microcapsules could provide a feasible environment for the enzyme molecules based  
369 on the well biocompatible property of PDA layer and the integrated and tough wall  
370 structure of the hybrid microcapsules.



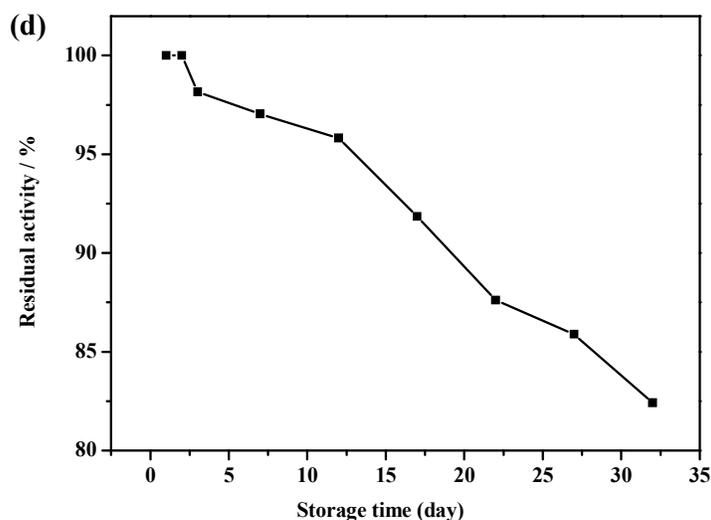
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375 **Fig. 10** Effect of (a) pH value, (b) temperature, (c) number of reuse, and (d) storage  
376 time of free and immobilized CRL.

#### 377 4. Conclusion

378 We developed an easy and effectual method for the fabrication of robust  
379 organic-inorganic hybrid magnetic microcapsules by polydopamine coated magnetic  
380 porous  $\text{CaCO}_3$  microparticle template. The  $\text{Fe}_3\text{O}_4$  nanoparticles acted practical dual  
381 role in the formation of microcapsules; as the recyclable component in the hybrid  
382 microcapsules and the robust scaffold to sustain the microcapsules away from

383 collapse and fold or even rupture during the multiple-use. The shell thickness of the  
384 microcapsules could be easily controlled by the concentration of dopamine. Moreover,  
385 the as-prepared microcapsules exhibited excellent immobilization efficiency towards  
386 CRL. The well biocompatibility and non-toxicity of the hybrid microcapsules  
387 constructed a suitable microenvironment for the immobilized enzyme; especially the  
388 inorganic factor improved the rigidity of the wall to maintain the activity of the  
389 enzyme inside. The immobilized CRL demonstrated significant high mechanical  
390 stability and activity under various conditions, such as pH, temperature, reusability  
391 and storage time. It is reasonable to believe that the robust and flexible Fe<sub>3</sub>O<sub>4</sub> doped  
392 PDA hybrid microcapsules are useful to be applied in many other fields both in  
393 material science and bio-applications.

#### 394 **Acknowledgements**

395 The authors thank the financial supports from the National Natural Science  
396 Foundation of China (No.21374045), the scientific research ability training of  
397 under-graduate students majoring in chemistry by the two patters based on the tutorial  
398 system and top students (J1103307) and the Opening Foundation of State Key  
399 Laboratory of Applied Organic Chemistry (SKLAOC-2009-35).

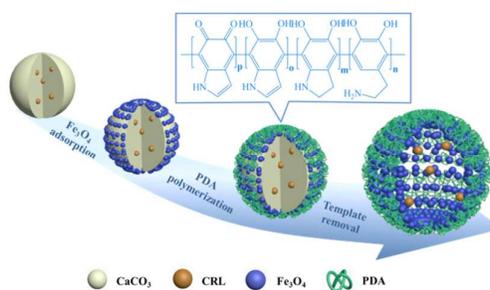
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Graphical abstract:



Fabrication of robust organic-inorganic hybrid magnetic microcapsules coordinated with polydopamine and  $\text{Fe}_3\text{O}_4$  nanoparticles for enzyme immobilization.