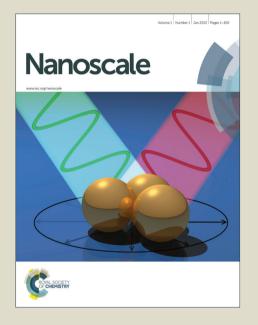
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Paper

Facile synthesis of zwitterionic polymer coated core-shell magnetic nanoparticles for highly specific capture of N-linked glycopeptides

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The highly selective and efficient capture of glycosylated proteins and peptides from complex biological samples is of profound significance to the discovery of disease biomarkers in biological systems. Recently, hydrophilic interaction liquid chromatography (HILIC)-based functional materials have been 10 extensively utilized for glycopeptide enrichment. However, the low amount of immobilized hydrophilic groups on the affinity material has limited the specificity, detection sensitivity and binding capacity in the capture of glycopeptides. Herein, a novel affinity material was synthesized to improve the binding capacity and detection sensitivity for glycopeptides by coating poly (2-(methacryloyloxy) ethyl) dimethyl-(3-sul-fopropyl) ammonium hydroxide (PMSA) shell onto Fe₃O₄@SiO₂ nanoparticles, taking 15 advantage of reflux-precipitation polymerization for the first time (denoted as Fe₃O₄@SiO₂@PMSA). The thick polymer shell endows the nanoparticles with excellent hydrophilic property and a great deal of functional groups on the polymerization chains. The resulting Fe₃O₄@SiO₂@PMSA demonstrated an outstanding ability for glycopeptides enrichment with high selectivity, extremely high detection sensitivity (0.1 fmol), large binding capacity (100 mg g⁻¹), high enrichment recovery (above 73.6 %) and 20 rapid magnetic separation. Furthermore, in the analysis of real complicated biological sample, 905 unique N-glycosylation sites from 458 N-glycosylated proteins were reliably identified in three replicate analysis of 65 µg protein sample extracted from mouse liver, showing the great potential in detection and identification low-abundant N-linked glycopeptides biological samples.

Introduction

25 Protein glycosylation, one of the most significant posttranslational modifications (PTMs) in proteome, attaches great importance to multiple biological processes including signal transduction, intracellular transport, immune response and cell growth.¹⁻⁴ Abnormal glycosylation is associated with various 30 diseases such as cancer and neurodegenerative diseases.⁵ To better understand these biological processes as well as discover disease biomarkers, it is necessary to identify glycoproteins and determine their glycosylation sites. Currently, mass spectrometry (MS)-based techniques have become the most important and 35 effective tools for analyzing and characterizing protein glycosylation. Unfortunately, the tremendous heterogeneity of each glycosylation site, inherent low abundance of glycopeptides and serious signal suppression caused by the co-existence of abundant non-glycosylated peptides make the direct MS analysis 40 of glycopeptides still a challenge. Therefore, an efficient approach for glycopeptide enrichment from complex biological sample prior to MS analysis is imperative.

Up to now, several materials and methods embracing lectin chromatography, 6-8 affinity boronic acid affinity 45 chromatography, 9-13 hydrazide beads, 14, 15 titanium dioxide, 16 and hydrophilic interaction chromatography (HILIC) adsorbents 17, 18

have been developed for glycopeptides enrichment. Among them, the enrichment strategy based on HILIC has been well developed and gained increasing popularity due to its simple operating 50 process, high selectivity, excellent reproducibility, no bias and reversible alterations of glycan composition. A variety of hydrophilic matrices, such as sepharose, cellulose, saccharides, ZIC-HILIC beads and metal-organic framework, 19-22 have been used for the selective separation and extraction of glycopeptides. 55 Nevertheless, the relatively low density of the hydrophilic molecules on the surface of traditional HILIC absorbents has limited the specificity, detection sensitivity and binding capacity of glycopeptides. It was demonstrated that HILIC beads with a high amount of functional molecules bonded could further 60 improve the enrichment performance. 23 Thus, it is highly desirable for novel HILIC materials with abundant hydrophilic groups to improve the glycopeptides enrichment efficiency.

In the last decade, magnetic nanoparticles have gained immense interest due to their unique biocompatibility, easy 65 preparation, versatile modification and rapid magnetic response, and are widely used in magnetic resonance imaging, drug delivery, sensing, and proteomic research. 24-28 A combination of magnetic nanomaterial and covalently bonded hydrophilic functional molecule could simultaneously achieve the simple and 70 efficient capture of the glycopeptides from the complex mixture

by magnetic separation. Several kinds of functionalized magnetic nanoparticles (e.g. poly (4-vinyl-pyridinium ethanesulfonate) coated Fe₃O₄, ²⁹ Fe₃O₄@SiO₂@PEG-Maltose²³) were developed and showed great selectivity for glycopeptides. Yet, the synthesis ⁵ procedures of these materials were tedious. Recently, Zou et al. ³⁰ fabricated a kind of multilayer polysaccharide shells coated magnetic nanoparticles using a simple and convenient approach (layer-by-layer) and the obtained composite material exhibited high selectivity, high detection sensitivity and large binding 10 capacity for glycopeptides enrichment. Fang et al. 31 developed an one-pot method for the synthesis of chitosan coated magnetic nanoparticles, and the thick chitosan shell was beneficial to improve the enrichment efficiency. Notwithstanding these successful examples, the design and synthesis of novel 15 hydrophilic polymer coated magnetic nanoparticles is drawing extensive attentions to the improvement of the detection sensitivity and binding capacity of glycopeptides.

Zwitterionic molecules functionalized materials are wellknown superhydrophilic and ultralow biofouling materials. ³² The 20 zwitterionic groups on the nanoparticles can bind water molecules more strongly via electrostatically induced hydration, in comparison with the water retention materials based on hydrogen-bonding-induced hydration. The large amount of the zwitterionic groups enables a thick layer of water molecules, 25 which contributes greatly to the stronger hydrophilic interaction. ³³⁻³⁶Among silica based HILIC materials, ZIC-HILIC has shown the best enrichment performance in the analysis of protein glycosylation. 37, 38 However, ZIC-HILIC materials related magnetic nanoparticle have rarely been reported. Yeh et al. ²⁹ 30 prepared zwitterionic polymer coated magnetic nanoparticles by employing spontaneous acid-catalyzed polymerization. Being applied for the glycopeptides enrichment, the material presented high selectivity and recovery. However, the synthesis process was tedious, and the thickness of polymer shell was difficult to 35 control and lack of stability. Therefore, the synthesis of zwitterionic polymer coated magnetic nanoparticles by a convenient, effective and robust method for glycopeptides enrichment would be very attractive.

Herein, we report a facile approach for the synthesis of 40 zwitterionic polymer coated magnetic nanoparticle (Fe₃O₄@SiO₂@PMSA) via reflux-precipitation polymerization for the first time. The thick zwitterionic polymer shell endows the composite not only with excellent hydrophilic surface property, but also with a great deal of zwitterionic functional sites on the 45 polymerization chains for high detection sensitivity and large binding capacity of glycopeptides. Moreover, the unique magnetic property will facilitate the rapid and complete recovery of the composite. The specificity, detection sensitivity, enrichment and enrichment capacity recovery 50 Fe₃O₄@SiO₂@PMSA for glycopeptides enrichment have been evaluated by using different biological samples. Besides, the practical applicability of Fe₃O₄@SiO₂@PMSA was demonstrated by capture of low-abundance of glycopeptides in tryptic digest of proteins extracted from mouse liver. The outstanding selectivity, 55 extreme sensitivity, excellent enrichment recovery glycopeptides, and high magnetic susceptibility also revealed its great capability in glycoproteome analysis for real biological samples.

Experimental section

60 Materials and chemicals

Iron (III) hexahydrate (FeCl₃·6H₂O), ethanol, ethylene glycol (EG), ammonium hydroxide (NH₃·H₂O, 28 wt%), tetraethyl orthosilicate (TEOS) and sodium acetate (NaAc) were obtained from Tianjin Chemical Plant (Tianjin, China). γ- methacryloxy-65 propyltrimethoxysilane (MPS), 3-methacryloxypropyltrimethoxysilane, N, N'-methylenebisacrylamide (MBA), methacrylic acid (MAA), trifluoroacetic acid (TFA), HPLC grade acetonitrile (ACN) and ammonium bicarbonate (NH₄HCO₃) were purchased Aladdin (Shanghai, China). 2,2-Dimethoxy-2-70 phenylacetophenone (DMPA) was from Acros Organics (New USA). PNGase F was from New England Biolabs (Ipswich, MA). Human serum immunoglobulin G (human IgG), chicken avidin, horseradish peroxidase (HRP), trypsin (TPCK treated), dithiothreitol (DTT), iodoacetamide (IAA) and 2, 5-75 dihydroxyl benzoic acid (DHB) were got from Sigma-Aldrich (St, Louis, MO, USA). 2, 2-azobisisobutyronitrile (AIBN) was supplied by Sinopharm Chemical Reagents Company (Shanghai, China), GELoader tips (20 µL) were purchased from Eppendorf (Hamburg, Germany). All the chemical agents were used without 80 further purification. Purified water was obtained with a Milli-Q apparatus (Millipore, Bedford, MA, USA).

Synthesis of Fe₃O₄@SiO₂@PMSA nanoparticles

The Fe₃O₄ nanoparticles were firstly prepared by means of a solvothermal reaction, and then coated with a thin layer of SiO₂ 85 through a sol-gel process, subsequently modified with γ-MPS to obtained Fe₃O₄@SiO₂-MPS. ³⁹⁻⁴¹ The procedure was described in detail in ESI †. The coating of PMSA layer onto Fe₃O₄@SiO₂-MPS nanoparticles was carried out by a one-step refluxprecipitation polymerization of MSA in mixed solvent of 90 acetonitrile and water, with MAA as the auxiliary monomer, MBA as the cross-linker and AIBN as the initiator. Typically, 50 mg of the as prepared Fe₃O₄@SiO₂-MPS nanoparticles were dispersed ultrasonically in 80 mL of acetonitrile/water (3:1, v/v) in a dried 100 mL single-necked flask. Then, 200 mg of MSA, 50 95 µL of MAA, 200 mg of MBA and 6 mg of AIBN were added together into the flask. With ultrasonication for 20 min, the flask was submerged in a heating oil bath. The reaction mixture was then heated from ambient temperature to 95 °C within 30 min and reacted for 1.5 h under the micro-boiling state. The obtained 100 Fe₃O₄@SiO₂@PMSA nanoparticles were collected by magnetic separation and washed with ethanol for 3 times to eliminate the excessive reactants and the self-polymerized PMSA. Finally, the product was dried under vacuum at 50 °C for 24 h.

Synthesis of monolayer MSA molecules functionalized nanoparticles (Fe $_3O_4@SiO_2$ -MSA)

Fe₃O₄@SiO₂-SH was firstly synthesized and the process was given in ESI †. Then Fe₃O₄@SiO₂-MSA was synthesized according to a previous literature with a slight change. ⁴² Briefly, 50 mg of Fe₃O₄@SiO₂-SH nanoparticles were dispersed evenly in 30 mL of acetonitrile/water (3:1, v/v), then 5 mg of MSA and 0.5 mg of DMPA were added into it, and then the mixture was irradiated using a spectrolinker XL-1500 UV crosslinker (Spectronics Corporation, Westbury, New York) at room

temperature for 15 min. The obtained Fe₃O₄@SiO₂-MSA was washed with ethanol for 3 times, and dried under vacuum at 50 °C for 5 h.

Material characterization

5 Field emission scanning electron microscopy (FE-SEM) images were collected on a JSM-7001F scanning electron microscope and transmission electron microscopy (TEM) images were obtained by JEOL JEM-2000 EX transmission electron microscope (JEOL, Tokyo, Japan). Fourier-transform infrared 10 (FT-IR) spectrum was conducted on Thermo Nicolet 380 spectrometer using KBr pellets (Nicolet, Wisconsin, USA). Thermogravimetrci (TG) analysis was performed under nitrogen atmosphere with a heating rate of 10 °C min⁻¹ from room temperature to 700 °C (NETZSCH, Selb, Germany). The 15 saturation magnetization curve was obtained on a Physical Property Measurement System 9T (Quantum Design, San Diego, USA) at room temperature.

Tryptic digestion of standard glycoproteins and proteins extracted from mouse liver

20 1 mg of human IgG, chicken avidin or HRP was respectively dissolved in 400 µL of buffer containing 100 mmol L⁻¹ NH₄HCO₃ and 8 mol L⁻¹ urea. After the addition of 10 µL DTT (1 mmol L⁻¹) and being kept at 60 °C for 1 h, the protein was alkylated by 3.7 mg IAA at room temperature in the dark for 40 min. Then the 25 solution was diluted ten-fold with NH₄HCO₃ (50 mmol L⁻¹) and digested with trypsin (protein: enzyme = 25: 1, w/w) at 37 °C for 16 h. The tryptic digest was lyophilized and stored at -20 °C for further use.

The proteins from mouse liver were extracted by following a 30 literature procedure, 43 and the proteins (2 mg) were dissolved in 1 mL denaturing buffer containing 50 mmol L⁻¹ Tris-HCl and 8 mol L⁻¹ urea. After the addition of 20 μL DTT (1 mol L⁻¹) at 60 °C for 1 h, the proteins were alkylated by 7.4 mg IAA at room temperature in the dark for 40 min. Then the solution was diluted 35 ten-fold with 50 mmol L-1 Tris-HCl and digested with trypsin (protein: enzyme = 25: 1, w/w) at 37 °C for 16 h. The peptides mixture was desalted by C₁₈-SPE column, then lyophilized and kept at -20 °C for further use.

Selective enrichment glycopeptides by 40 Fe₃O₄@SiO₂@PMSA nanoparticles

The Fe₃O₄@SiO₂@PMSA nanoparticles were firstly washed and dispersed in 400 µL of loading buffer (ACN/H₂O/TFA, 86: 13.9: 0.1, v/v/v). Subsequently, 3 µg of tryptic digest of human IgG, chicken avidin, or HRP was added into it and incubated 45 moderately at room temperature for 30 min, respectively. After that, the nanoparticles were separated from the mixed solution by applying a permanent magnet and washed with the loading buffer (400 µL) three times to remove the non-specifically adsorbed peptides, then the captured glycopeptides were eluted with the 50 eluting buffer (ACN/H₂O/TFA, 30: 69.9: 0.1, v/v/v, 10 μL) twice and subjected to further MALDI-TOF MS analysis, or deglycosylation for LC-MS/MS analysis.

For glycopeptides enrichment from complex sample, 3 mg of Fe₃O₄@SiO₂@PMSA was incubated with tryptic digests of 55 proteins extracted from mouse liver in 500 µL loading buffer

(ACN/H₂O/TFA, 86: 13: 1, v/v/v). The mixture was incubated at room temperature for 40 min. After being washed by the loading buffer to remove the non-specifically adsorbed peptides, the captured glycopeptides were eluted with the eluting buffer 60 (ACN/H₂O/TFA, 30: 69.9: 0.1, v/v/v, 100 μL) three times. Finally, the eluate was lyophilized and deglycosylated for LC-MS/MS analysis.

Selective enrichment of glycopeptides by HILIC-SPE tips

The fabrication of HILIC SPE tips and the enrichment procedure 65 were carried out according to a previously described method with minor modification.⁴⁴ The detailed information was given in ESI

Deglycosylation of N-linked Glycopeptides by PNGase F

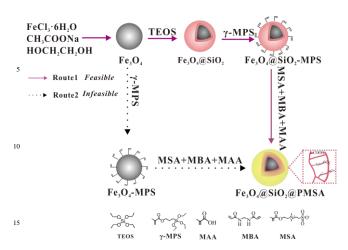
The captured glycopeptides in the eluate were lyophilized and 70 then redissolved in 40 μL NH₄HCO₃ (10 mmol L⁻¹). Then, 50 units of PNGase F were added into the solution and the mixture was incubated at 37 °C for 12 h.

Mass spectrometry analysis

All the MALDI-TOF MS experiments were carried out in a 75 reflector positive mode with a pulsed Nd/YAG laser at 355 nm on AB Sciex 5800 MALDI-TOF/TOF mass spectrometer (AB Sciex, CA). A 0.5 µL aliquot of the eluate and 0.5 µL of DHB matrix were successively dropped onto the MALDI plate for MS analysis. As a fine matrix, DHB was dissolved in $_{80}$ ACN/ H_2 O/ H_3 PO₄ (70: 29: 1, v/v/v, 25 mg mL⁻¹). The mouse liver protein sample was analyzed by a Thermo Q Exactive mass spectrometer (Thermo, San Jose, CA) with a nanospray ion source and a U3000 RSLC nano-system (Thermo, San Jose, CA, USA). The deglycosylated peptides were lyophilized and 85 redissolved in FA/H₂O (0.1: 99.9, v/v), subsequently loaded on a trap column (200 μm i.d.) packed with C_{18} AQ beads (5 μm , 120 Å, Daison, Osaka, Japan). The peptides were separated by a capillary analysis column (75 μm i.d.) packed with C₁₈ AQ beads (3 μm, 120 Å, Daison, Osaka, Japan). The eluting buffer were 90 99.9% H₂O with 0.1% FA (buffer A) and 99.9% ACN with 0.1% FA (buffer B). The gradient elution was performed as follows: from 0 to 4 % buffer B (FA/ACN, 0.1: 99.9) for 15 min, from 4% to 45 % buffer B (FA/ACN, 0.1: 99.9) for 100 min and from 45% to 80 % buffer B (FA/ACN, 0.1: 99.9) for 5 min. After ruing with 95 80 % buffer B for 10 min, the separation system was equilibrated by buffer A (FA/H₂O, 0.1: 99.9, v/v) for 15 min. The MS/MS spectra were obtained in a data-independent collision induced dissociation (CID) mode, and the full mass scan was acquired from m/z 400 to 2000 with resolution of 70000. The 12 most 100 intense ions with charge over 2 and intensity threshold higher than 104 were selected for MS/MS. The dynamic exclusion was set as 30 s.

Database searching

All the LC-MS/MS raw data were searched with MaxQuant 105 version (1.3.0.5) against a database (uniprot.Mouse, updated on July 9th, 2014). The mass tolerances were 20 ppm for initial precursor ions and 0.5 Da for fragment ions. Two missed cleavages were allowed for trypsin restriction. The cut off false discovery rate (FDR) for all the peptides identifications including



Scheme 1 Schematic illustration of the synthetic procedure for preparation of Fe₃O₄@SiO₂@PMSA nanoparticles.

the glycopeptides was controlled below 1 %. Only peptides with N-! P-S/T were considered as N-linked glycopeptides.

Results and discussion

Fabrication and characterization of Fe₃O₄@SiO₂@PMSA 25 nanoparticles

The protocol for the synthesis of Fe₃O₄@SiO₂@PMSA nanoparticle was illustrated in Scheme 1 (Route1). Firstly, the Fe₃O₄ nanoparticle was synthesized by a modified solvothermal reaction, and then modified with a thin layer of SiO₂ shell via a 30 sol-gel method. Subsequently, MPS was grafted onto the Fe₃O₄@SiO₂ nanoparticle to form abundant active double bonds for the next polymerization. Finally, a robust layer of PMSA was coated on the Fe₃O₄@SiO₂-MPS core by one step refluxprecipitation polymerization with MAA as the auxiliary 35 monomer, MSA as the zwitterionic monomer and MBA as the cross-linker to form Fe₃O₄@SiO₂@PMSA. For comparison, the Fe₃O₄@SiO₂ nanoparticle was also modified with a monolayer of MSA to obtain Fe₃O₄@SiO₂-MSA.

As it was known to all, it is hard to synthesize hydrophilic coated nanoparticles by reflux-precipitation polymerization to some extend due to some hydrophilic monomers (like MSA) are insoluble in the commonly used solvent like acetonitrile. Herein, acetonitrile/water co-solvent was introduced to dissolve the monomers, cross-linker and initiator. 45 Because of their low solubility in the co-solvent, the formed oligomers precipitated from the homogeneous solution were easily captured by the Fe₃O₄@SiO₂-MPS and the out-surface PMSA layer was obtained. To investigate the influence of the cosolvent on the following polymerization, several mixed solvent 50 with different ratio of ACN and water (9: 1, 3: 1, 1: 1, v/v) were employed. As demonstrated in Fig. S1 (ESI†), no size increase was found when the ratios of ACN and water were 9: 1 and 1: 1. The main reason is that the mixed solvent of 90 % ACN couldn't dissolve the monomer totally so that it would prevent the 55 following polymerization reaction. However, the co-solvent with high ratio of water was unfavourable for the reaction due to the

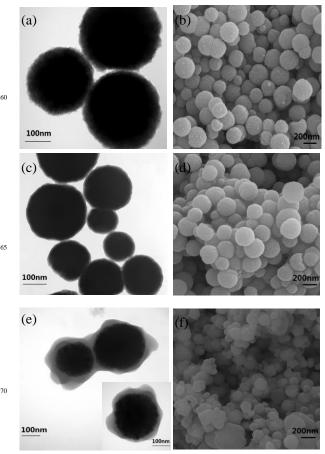


Fig.1 a) TEM and b) FESEM images of Fe₃O₄ cores. c) TEM and d) FESEM images of Fe₃O₄@SiO₂. e) TEM and f) FESEM images of 75 Fe₃O₄@SiO₂@PMSA nanoparticles.

inner hydrogen bonding force. Besides, the addition of MAA was also a significant factor to the formation of core-shell structured nanoparticles because that the hydrogen bonding among MAA 80 units and electrostatic bonding between MAA and MSA units make great contributions to the subsequent polymerization.

Representative TEM and FESEM images of Fe₃O₄, Fe₃O₄@SiO₂, Fe₃O₄@SiO₂@PMSA nanoparticles are shown in Fig.1. The Fe₃O₄ nanoparticles are uniform in both shape and size with an 85 average diameter of ca. 280 nm. After coating with SiO₂, a welldefined core-shell structure appeared and the surface was smoother than Fe₃O₄ nanoparticles (Fig. 1b and Fig. 1d). The size slightly increases and the SiO₂ layer is estimated to be 10 nm in thickness (Fig. 1c). The TEM image of Fe₃O₄@SiO₂@PMSA 90 nanoparticles (Fig. 1e) clearly indicates that the cross-linked PMSA layer has been successfully coated on the surface of Fe₃O₄@SiO₂-MPS, and the thickness of the polymer shell is around 60 nm. Furthermore, the FESEM image of Fe₃O₄@SiO₂@PMSA (Fig. 1f) with an obvious agglomeration 95 compared to that of the Fe₃O₄@SiO₂ also reveals the successful coating of the PMSA.

Modification of Fe₃O₄ nanoparticles with SiO₂ shell is essential for the coating of the next PMSA layer. We tried to directly coat a PMSA layer onto the Fe₃O₄-MPS surface without modification

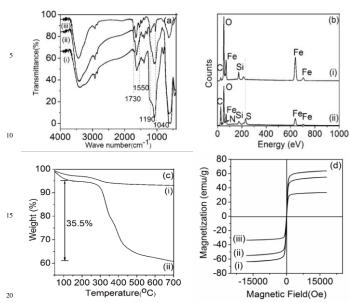


Fig. 2 (a) FT-IR spectra of (i) Fe₃O₄, (ii) Fe₃O₄@SiO₂ and (iii) Fe₃O₄@SiO₂@PMSA, (b) EDX spectrums and (c) TGA curves of (i) Fe₃O₄@SiO₂ and (ii) Fe₃O₄@SiO₂@PMSA. (d) Magnetization hysteresis loops of (i) Fe₃O₄, (ii) Fe₃O₄@SiO₂ and (iii) Fe₃O₄@SiO₂@PMSA.

(Scheme 1, Route 2). Unfortunately, no final core-shell structurewas obtained. We infer the primary reason is that both the Fe₃O₄ and MSA take charges in the solvent and there is a strong mutual interaction between the core and the zwitterionic 30 monomer, subsequently seriously influencing the dispersive stability of the Fe₃O₄ nanoparticles in the solvent. The Fe₃O₄ nanoparticles subside quickly without any further reaction. Therefore, a proper interim layer is required. The interim layer should not only ensure the seed nanoparticles have a good 35 dispersibility in the co-solvent but also give high accessibility to MSA for further polymerization reaction. Taking all these into consideration, due to its excellent hydrophilcity as well as easy modification character, the silica layer was introduced naturally to obtain the coating layer of PSMA on the magnetic cores.

FTIR spectroscopy was conducted to inspect the chemical of $Fe_3O_4(a)SiO_2$ Fe₃O₄@SiO₂-MPS Fe₃O₄@SiO₂@PMSA. Compared to the FI-IR spectrum of $Fe_3O_4@SiO_2$ (581 cm⁻¹, $v_{Fe-O-Fe}$, 1091 cm⁻¹, $v_{Si-O-Si}$), a new characteristic adsorption peak (1730 cm⁻¹, $v_{C=0}$) in the spectrum 45 of Fe₃O₄@SiO₂-MPS (Fig. 2a) could demonstrate the successful graft of MPS. And the new characteristic peaks appear at 1040 and 1190 cm⁻¹ are ascribed to the stretching vibration of O=S=O in the -SO₃⁻ group. 45 The peak at 1550 cm⁻¹ corresponds to the bending vibration of N-H in the MBA. In addition, the adsorption 50 peak at 1730 cm⁻¹ attributed to the C=O stretching vibration is enhanced. All the evidences reveal the successful coating of PMSA on the surface of Fe₃O₄@SiO₂-MPS.

Energy dispersive X-ray (EDX) spectra and thermogravimetric analysis (TGA) were also recorded to confirm the introduction of 55 PMSA. As shown in Fig. 2b, C, O, Si, Fe are the main elements. And the emerging of N and S elements indicates the successful modification of PMSA. TGA curve reveals that the weight loss of

6.70 % of Fe₃O₄@SiO₂ is attributed to the adsorbed water. It could be calculated that the weight loss Fe₃O₄@SiO₂@PMSA nanoparticles is 35.5 demonstrates the high amount of PMSA on the composite nanoparticles.

The magnetic properties of three nanoparticles were studied by using a vibrating sample magnetometer at room temperature (Fig. 2d). The magnetic hysteresis loop curves show that the three kinds of materials have no obvious remanence or coercivity at room temperature, indicating that they all possess a superparamagnetic character. The superparamagnetism is coming from the small nanocrystals in the Fe₃O₄ cores, which behave as superparamagnets with a saturation magnetization (Ms) value of 64.3 emu g⁻¹. As a comparison, the Ms value of the Fe₃O₄@SiO₂ nanoparticle was 55.5 emu g⁻¹. After coating the polymer layer and the Ms value strikingly decreased to about 33.6 emu g⁻¹. The Fe₃O₄@SiO₂@PMSA nanoparticles were observed having better dispersibility and stability in water compared to Fe₃O₄@SiO₂-MSA when no external magnet field was applied. However, thanks to the high-magnetic response of Fe₃O₄ core, the final product of Fe₃O₄@SiO₂@PMSA microspheres could be separated from the solution in only 30 s by using a magnet.

80 Selective enrichment of glycopeptides from tryptic digest from standard glycoproteins

On the basis of hydrophilic interaction chromatography, hydrophilic materials, i.e., immobilized polysaccharides and MOFs and etc. have been reported to selectively enrich 85 glycopeptides. 46-48 Thus, to evaluate the practicability of the Fe₃O₄@SiO₂@PMSA in the selective enrichment glycopeptides, a tryptic digest of standard glycoprotein (human IgG) was employed as the testing sample. The workflow of glycopeptides enrichment is presented in Scheme S1a. As shown 90 in Fig. 4a, only four glycopeptides with weak MS signal intensity and low signal-to-noise ratio (S/N) was detected for the direct analysis of IgG tryptic digest on account of the low abundance of glycopeptides and the strong signal suppression by the abundant non-glycosylated peptides. However, after being enriched by 95 Fe₃O₄@SiO₂@PMSA nanoparticles, the signals of nonglycosylated peptides were eliminated and twenty six N-linked glycopeptides were detected and identified with high intensity and S/N ratio (Fig. 4b). For comparison, the tryptic digest of human IgG was also treated with Fe₃O₄@SiO₂-MSA, only eight 100 glycopeptides could be detected with an inferior signal intensity and S/N ratio (Fig. 4c). The enrichment efficiency of Fe₃O₄@SiO₂@PMSA was evidently superior to that of Fe₃O₄@SiO₂-MSA, which can be ascribed to the higher surface density of zwitterionic groups on the material and stronger 105 multivalent hydrophilic interactions. The detailed structures and the S/N ratios of the glycopeptides are listed in Tables S3 and S4 (ESI†), respectively. In addition, compared with the HILIC tips (Scheme S1b, S1c), only six glycopeptides could be noted and the intensity is relatively low (Fig. 4d) after enrichment. The 110 enrichment performance of Fe₃O₄@SiO₂@PMSA is obviously better than that of the HILIC tips. Subsequently, on the one hand, all the enriched peptides were analyzed by MALDI-TOF MS/MS

and the spectrum of a representative glycopeptide (m/z=2763.8) with the explicite glycan structure was given in Fig. S2 (ESI[†]), indicating that the enriched peptides all geared to glycopeptides. On the other hand, the eluted glycopeptides were deglycosylated 5 by PNGase F and only two deamidated peptides (m/z=1158.54, 1190.53) were detected (Fig. 4e), which further confirmed that those peaks appearing in the Fig. 4b all belonged to N-linked glycopeptides. The result indicates that Fe₃O₄@SiO₂@PMSA nanoparticles have high enrichment selec- tivity for human IgG 10 enrichment. Superficial functional group density of the magnetic composite nanoparticles attaches great importance to the biological enrichment. In our work, a high density of zwitterionic groups on the polymerization chain is critical for achieving high performance in specific enrichment of glycopeptides.

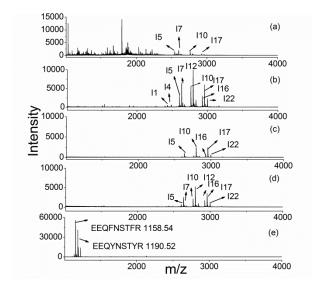


Fig.4 MALDI-TOF MS spectra of (a) direct analysis of the 0.5 pmol of human IgG, (b) after enrichment Fe₃O₄@SiO₂@PMSA, (c) after enrichment by Fe₃O₄@SiO₂-MSA, 20 after enrichment by HILIC Tips and (e) deglycosylation by PNGase F.

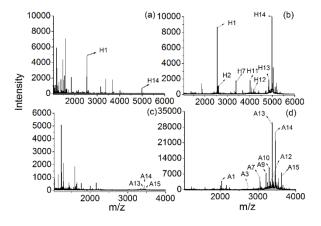


Fig. 5 MALDI-TOF MS spectra of (a) direct analysis of the 1 pmol tryptic digest of HRP, (b) after enrichment by Fe₃O₄@SiO₂@PMSA, (c) direct analysis of the 1 pmol tryptic digest of chicken avidin and (d) after 25 enrichment by Fe₃O₄@SiO₂@PMSA.

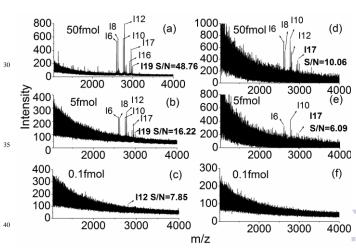


Fig.6 MALDI-TOF MS spectra of (a) 50 fmol, (b) 5 fmol and (c) 0.1 fmol human IgG digest after treatment by Fe₃O₄@SiO₂@PMSA nanoparticles; (d) 50 fmol, (e) 5 fmol and (f) 0.1 fmol human IgG digest 45 after treatment by HILIC tips.

To further evaluate its universality for the glycopeptide enrichment, the tryptic digests of chicken avidin and HRP were also employed. A direct MALDI-TOF mass spectrum of chicken 50 avidin is presented in Fig. 5a, and the MS signals of glycopeptides are severely suppressed by the non-glycosylated peptides. Nevertheless, fifteen glycopeptides with enhanced intensity and S/N ratio dominate the MS spectrum of treated sample (Fig. 5b, Table S2, ESI†). Besides, comparing to the mass 55 spectrum of direct analysis of tryptic digest of HRP in Fig. 5c, fourteen glycopeptides (Fig. 5d, Table S1, ESI†) were identified after the enrichment by Fe₃O₄@SiO₂@PMSA. These results have revealed the high selectivity efficiency Fe₃O₄@SiO₂@PMSA for universal glycopeptides enrichment.

60 Evaluation of the detection sensitivity, binding capacity and enrichment recovery of Fe₃O₄@SiO₂@PMSA in glycopeptides enrichment

As the level of glycopeptides in a complex biological sample could be extremely low, the detection sensitivity 65 Fe₃O₄@SiO₂@PMSA towards glycopeptides was investigated. Tryptic IgG digest with a group of low amount of 50 fmol, 5 fmol 0.1 fmol were treated by Fe₃O₄@SiO₂@PMSA as well as the HILIC tips. As shown in Fig. 6a and Fig. 6e, several glycopeptides were clearly detected in 50 fmol of human IgG 70 tryptic digest after enrichment by both Fe₃O₄@SiO₂@PMSA and HILIC tips. And with the amount of human IgG being decreased to 5 fmol, less glycopeptides with lower S/N ratios enriched by HILIC tips could be detected as presented in Fig. 6b and Fig. 6e. And when the total amount of human IgG was as low as 0.1 fmol, 75 one peptide could still be detected after enrichment by Fe₃O₄@SiO₂@PMSA at S/N ratio of 7.8 with a m/z of 2795.58. However, none of glyopeptide could be identified after treatment by HILIC tips. Furthermore, the resulting detection sensitivity was also higher than previously reported HILIC materials, such 80 as the branched PEG brushes hybrid hydrophilic magnetic nanoparticles (0.5 fmol), zwitterionic polymer brushes hybrid silica nanoparticles

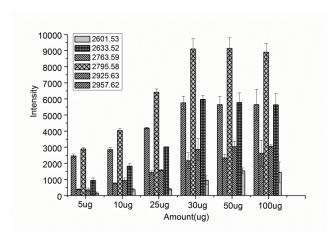


Fig.7 The intensity of six selected N-linked glycopeptides from human 5 IgG digest after treatment with different amount of Fe₃O₄@SiO₂@PMSA nanoparticles.

Table 1 Recovery of N-linked glycopeptides from human IgG digest by using $Fe_3O_4@SiO_2@PMSA$

No.	m/z	Recovery \pm S.D (%, n=3)
I6	2601.53	73.6 ± 2.8
18	2633.52	94.8 ± 1.5
I10	2763.59	93.9 ± 1.7
I12	2795.58	101.2 ± 0.7
I16	2925.63	106.2 ± 0.8
I17	2957.62	109.3 ± 1.1

(10 fmol) and silica-based click maltose (30 fmol). ^{23, 44, 45} The lower detection limit may be attributed to the excellent hydrophilicity, absolute magnetic separation, a large amount of MSA groups as well as stronger multivalent hydrophilic 15 interactions. This result shows that the prepared Fe₃O₄@SiO₂@PMSA significantly nanoparticle improves detection sensitivity for glycopeptides.

To inspect the binding capacity of Fe₃O₄@SiO₂@PMSA, different amounts of Fe₃O₄@SiO₂@PMSA (5-100 μg) were added to a fixed amount of human IgG digest (3 μg). After the enrichment, the eluted fraction was analyzed by MALDI-TOF MS. The signal intensities of six selected glycopeptides reached the maximum when the addition of the nanoparticles was 30 μg and the binding capacity was calculated to be 100 mg g⁻¹ (Fig. 7). The large binding capacity might be owing to the high amount of zwitterionic groups and the strong multivalent hydrophilic interactions between the glycopeptides and the material.

Stable-isotope dimethyl labeling method ⁴⁹ was utilized for evaluating the recovery yield of Fe₃O₄@SiO₂@PMSA for ³⁰ glycopeptides enrichment. Briefly, equal amount of human IgG (3 μg) tryptic digest was labelled with light and heavy isotopes, respectively. The heavy-tagged digest was enriched with Fe₃O₄@SiO₂@PMSA abiding by the above-mentioned enrichment procedure. The resulting eluent was mixed and the ³⁵ mixture was re-enriched by Fe₃O₄@SiO₂@PMSA, then the eluent

was analyzed by MALDI-TOF MS. The recovery was calculated by the signal intensity ratio of heavy isotope-labelled glycolpeptides divided by the light isotope-labelled glycopeptides. The recovery yields of six selected peptides were all over 73.6 % (Table 1.) The result reveals that the Fe₃O₄@SiO₂@PMSA nanoparticle is an ideal affinity material for the enrichment of glycopeptides.

Application in glycopeptide enrichment from real complex biological sample

45 Inspired by the outstanding enrichment efficiency in standard glycoprotein tryptic digest, the Fe₃O₄@SiO₂@PMSA were further applied to the analysis of nanoparticles glycoproteome of mouse liver. 65 µg of proteins extracted from mouse liver were incubated with Fe₃O₄@SiO₂@PMSA as well as 50 the HILIC tips, and the eluent was loyophilized, deglycosylated and analyzed by nano LC-MS/MS, followed by database searching with controlling the false discovery rate (FDR) for all the peptides identifications including the glycopeptides < 1%. As a result, a total of 905 N-glycosylation sites from 458 N-55 glycoproteins were identified with a consensus sequence of N-! P-S/T motif (Table S5, ESI†). The explicite data of three independent runs are shown in Fig. S3(ESI†). In comparison, only 457 N-glycosylation sites from 269 N-glycoproteins were identified by HILIC tips. The differences in the structure of these 60 materials contributed to the different performance of glycopeptide enrichment. The result clearly demonstrates that the Fe₃O₄@SiO₂@PMSA nanoparticles own high selectivity and effectiveness characters in the enrichment of low-abundant Nlinked glycopeptides from complex biological samples.

65 Conclusions

In summary, a facile, repeatable, and robust synthetic route for preparation of a new HILIC material, Fe₃O₄@SiO₂@PMSA nanoparticle, with well-defined core-shell structure was presented. The characterization results showed that the SiO₂ 70 interim layer and the ratio of the co-solvent had strong effects on the successful preparation. The thick polymer layer improved the hydrophilicity and the amount of zwitterionic molecules on the polymerization chains. The glycopeptides enrichment experiments confirmed that the Fe₃O₄@SiO₂@PMSA 75 nanoparticles have high specificity, extremely high detection sensitivity, large binding capacity and satisfactory recovery. In the selective enrichment of N-linked glycopeptides from tryptic digest of proteins extracted from mouse Fe₃O₄@SiO₂@PMSA shows great practicability in identifying 80 low-abundant glycopeptides from minute amounts of complex biological samples. It can be expected that the as-synthesized Fe₃O₄@SiO₂@PMSA would hold great potential glycoproteome research.

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