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ARTICLE TYPE

Europium- and Lithium-Doped Yttrium Oxide Nanocrystals that Provide a Linear Emissive Response with X-ray Radiation Exposure[†]

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Eu- and Li-doped yttrium oxide nanocrystals $[Y_{2-x}O_3; Eu_x, Li_y]$, in which Eu and Li dopant ion concentrations were systematically varied, were developed and characterized (TEM, XRD, Raman

- ¹⁰ spectroscopic, UV-excited lifetime, and ICP-AES data) in order to define the most emissive compositions under specific x-ray excitation conditions. These optimized $[Y_{2-x}O_3; Eu_x, Li_y]$ compositions display scintillation responses that: (i) correlate linearly with incident radiation exposure at x-ray energies spanning from 40 - 220 kVp, and (ii) manifest no evidence of scintillation intensity saturation at the highest evaluated radiation exposures [up to 4 Roentgen per second]. For the most emissive nanoscale
- ¹⁵ scintillator composition, [Y_{1.9}O₃; Eu_{0.1}, Li_{0.16}], excitation energies of 40, 120, and 220 kVp were chosen to probe the dependence of the integrated emission intensity upon x-ray exposure-rate in energy regimes having different mass-attenuation coefficients and where either the photoelectric or the Compton effect governs the scintillation mechanism. These experiments demonstrate for the first time for that for comparable radiation exposures, when the scintillation mechanism is governed by the photoelectric effect
- ²⁰ and a comparably larger mass-attenuation coefficient (120 kVp excitation), greater integrated emission intensities are recorded relative to excitation energies where the Compton effect regulates scintillation (220 kVp) in nanoscale $[Y_{2-x}O_3; Eu_x]$ crystals. Nanoscale $[Y_{1.9}O_3; Eu_{0.1}, Li_{0.16}]$ (70 ± 20 nm) was further exploited as a detector material in a prototype fiber-optic radiation sensor. The scintillation intensity from the $[Y_{1.9}O_3; Eu_{0.1}, Li_{0.16}]$ -modified, 400 µm-sized optical fiber tip, recorded using a CCD-photodetector
- ²⁵ and integrated over the 605 617 nm wavelength domain, was correlated with radiation exposure using a Precision XRAD 225Cx small-animal image guided radiation therapy (IGRT) system. For both 80 and 225 kVp energies, this radiotransparent device recorded scintillation intensities that tracked linearly with total radiation exposure, highlighting its capability to provide alternately accurate dosimetry measurements for both diagnostic imaging (80 kVp) and radiation therapy treatment (225 kVp).

30 Introduction

Inorganic scintillators have long been exploited as radiation sensing materials due to their high stabilities and emission characteristics, and the fact that the emissive wavelengths of these species are compatible with conventional photomultiplier

- ³⁵ tubes.¹⁻³ Factors such as crystal growth conditions and the need for cryogenic cooling, for example, have limited the extent to which many of these materials can be deployed. Modern photodetectors, such as those based on CCD cameras and Siphotodiodes, enable enhanced scintillation emission detection
- ⁴⁰ sensitivities, and open up new possibilities to exploit scintillators that are smaller, easier to produce, and scintillate within the photodetector spectral regime that affords optimal quantum efficiency of the photovoltaic response (generally between 500-1000 nm).
- ⁴⁵ Bulk yttrium oxide activated with europium ions, [Y₂O₃; Eu], has been utilized as the red-phosphor in early cathode ray

televisions⁴ and as the scintillator material in a wide variety of xray computed tomography (CT) detectors:⁵ both of these applications exploit the material's peak emissions near 600 nm. ⁵⁰ While nanoscale [Y₂O₃; Eu] has found utility in white light emitting diodes⁶ and in vitro imaging,⁷ its x-ray scintillation properties have yet to be fully interrogated, despite the fact that the per-mass scintillation yield of highly crystalline [Y₂O₃; Eu] nanoscale materials was shown to exceed that of their bulk ⁵⁵ counterparts under electron-beam excitation.⁸ Further, while scintillating nanomaterials have been delineated and demonstrate considerable potential,⁹⁻¹³ relatively little work has capitalized upon such materials in device architectures.

In this report, we describe Eu- and Li-doped yttrium oxide ⁶⁰ nanocrystals $[Y_{2-x}O_3; Eu_x, Li_y]$ in which dopant ion concentrations have been systematically varied in order to define the most emissive compositions under specific sets of x-ray excitation conditions. We show that $[Y_{2-x}O_3; Eu_x, Li_y]$ compositions display scintillation responses that: (i) correlate linearly with incident radiation exposure at x-ray energies spanning from 40 - 220 kVp, and (ii) manifest no evidence of scintillation intensity saturation at the highest evaluated radiation exposures [up to 4 Roentgen per second (R/s; $1 \text{ R} = 2.58 \text{ x } 10^4$ Coulomba of abarea produced hu x, or true per hilogram of

⁵ Coulombs of charge produced by x- or γ-rays per kilogram of air)]. We further show that the most emissive of these nanoscale scintillator compositions provides a linear emission response as a function of radiation exposure for 80 and 225 kVp x-ray energies in a micro-CT dual imaging and high precision cone-beam
 ¹⁰ therapy instrument utilized for small-animal image guided

Results and Discussion

radiation therapy (IGRT).



Figure 1. TEM images of: (A) $[Y_{1,9}O_3; Eu_{0,1}]$ and (B) $[Y_{1,9}O_3; Eu_{0,1}, Li_{0,16}]$ nanocrystal compositions. (C) Raman spectra of $[Y_2O_3; Li_v]$ compositions acquired at a 632 nm irradiation wavelength. The increases in size and crystallinity observed in the TEM images as a function of increased Li concentration correlate with an observed increase in the Raman scattering intensity measured at 376 cm⁻¹.

The flame-combustion technique, utilizing glycine and metal nitrate salts at a fixed ratio, was employed to systematically 15 synthesize nanocrystal compositions.^{14, 15} X-ray diffraction (XRD) spectra confirmed that all compositions displayed a cubic structure, and inductively coupled plasma atomic emission (ICP-AES) provided $[Y_{2-x}O_3; Eu_x]$ spectroscopy Li_{v}] compositional analysis (Figure S1; Table S1, Supporting 20 Information). Figure 1A-B displays representative TEM images of the most emissive Eu-doped [Y19O3; Eu01] and Eu/Li codoped [Y_{1.9}O₃; Eu_{0.1}, Li_{0.16}] compositions determined for 130 kVp (5 mA) x-ray excitation. Analyses of the Figure 1 TEM images, and the TEM images for the $[Y_{1,9}O_3; Eu_{0,1}, Li_v]$ $_{25}$ compositional series (y = 0 to 0.25; Figure S2), reveal that as Li doping is increased from y = 0 to y = 0.25, crystalline size increases from ~20 - 40 nm to ~50 - 90 nm, and crystalline boundaries become better defined. Increased nanocrystal sizes and the corresponding reduction of amorphous content are

30 evident in TEM images and the Raman spectra of these samples;

note that as the Li ion doping concentration increases, the Raman scattering intensity of the dominant optical phonon of cubic- Y_2O_3 at 376 cm⁻¹ increases (**Figure 1C**), congruent with data acquired for corresponding heterogeneous bulk-phase samples.¹⁶ While ³⁵ increased levels of Li ion doping of bulk phase [Y_2O_3 ; Eu] compositions have been demonstrated to track qualitatively with augmented cathodoluminescence intensity,^{17, 18} the experimental data presented herein highlight that the increased nanoscale size and crystallinity of the Y_2O_3 host lattice that occurs with Li⁺ 40 doping also results in an increased scintillation intensity of the nanocrystalline [$Y_{2-x}O_3$; Eu_x, Li_y] compositions (*vide infra*).

To obtain $[Y_{2-x}O_3; Eu_x, Li_v]$ compositions that display enhanced emission, Eu concentrations were initially varied over a $[Y_{1.98}O_3; Eu_{0.02}]$ to $[Y_{1.69}O_3; Eu_{0.31}]$ compositional range, and 45 interrogated via solid-state x-ray emission spectroscopy (XES) using a 130 kVp (5 mA) x-ray cabinet-confined irradiation source. In these studies, 5 mg of $[Y_{2-x}O_3; Eu_x]$ nanocrystals were pressed into a 7 mm diameter disk and placed on a Teflon mount; an optical fiber was utilized to collect scintillated emission, which 50 was quantitated using an Edinburgh FLS920 spectrometer (Supporting Information). These studies demonstrated that the $[Y_{1,9}O_3; Eu_{0,1}]$ composition was the most emissive member of this compositional series; Figure 2A displays the x-ray emission intensities determined over a 575 - 675 nm range for these 55 nanoscale $[Y_2O_3; Eu_x]$ compositions. Note that this experimental trend in x-ray emission intensity determined as a function of Eu ion concentration depicts characteristic activator ion emission behavior in yttrium oxide host crystals,^{4, 19-21} *i.e.*, an optimal concentration of emitting ions exists, beyond which cross-ion 60 quenching drives reductions of x-ray emission intensity.



Figure 2. Integrated, solid-state x-ray emission spectral intensities determined over a 575 - 675 nm range for: (A) $[Y_2O_3; Eu_x]$ and (B) $[Y_{1.9}O_3; Eu_{0.1}, Li_v]$ compositions (note: trend lines added for visualization purposes). (C) The x-ray emission spectra of the most emissive Eu and Eu/Li co-doped samples, recorded for 130 kVp (5 mA) x-ray excitation.

Holding the optimized Eu activator ion concentration of $[Y_{1.9}O_3; Eu_{0.1}]$ constant, progressively increasing Li ion concentrations were incorporated into combustion reactions used ⁶⁵ to synthesize the $[Y_{1.9}O_3; Eu_{0.1}, Li_y]$ compositions; ICS-AES was used to determine the ion doping levels of the isolated nanocrystalline products (**Table S1**). Figure 2B shows the integrated solid-state x-ray emission intensities determined over a 575 - 675 nm range for $[Y_{1.9}O_3; Eu_{0.1}, Li_y]$ (y = 0 to 0.25) ⁷⁰ compositions recorded for 130 kVp (5 mA) x-ray excitation. These XES data show that $[Y_{1.9}O_3; Eu_{0.1}, Li_{0.16}]$ is the most emissive of the $[Y_{1.9}O_3; Eu_{0.1}, Li_y]$ compositions under these

conditions, displaying more than twice the emission intensity of the parent $[Y_{1,9}O_3; Eu_{0,1}]$ nanocrystalline material (**Figure 2C**). Emission lifetime data acquired for these $[Y_{1,9}O_3; Eu_{0,1}, Li_y]$ (y = 0 to 0.25) compositions utilizing pulsed-lamp UV-excitation of

- s the Eu-O charge transfer band showed that each composition displayed a single exponential lifetime decay of 2.12 ± 0.04 ms (**Figure S3**). These identical emissive lifetimes, along with TEM and Raman spectroscopic data (**Figure 1**), indicate that the emission intensity augmentation observed under x-ray excitation
- ¹⁰ with Li-doping results from the enhanced quantum efficiency of the larger, more crystalline nanocrystals on a per-unit mass basis; earlier literature notes that this effect derives from a combination of reduced surface quenching sites, increased phonon-electron coupling, and diminished internal reflections in more crystalline ¹⁵ samples.^{17, 22-24}



Figure 3. Integrated solid-state x-ray emission spectral intensity recorded over the 500 - 700 nm range as a function of radiation exposure (R/s) for: (A) 40, (B) 120, and (C) 220 kVp excitation.

Energy and flux dependent x-ray emission spectroscopic measurements of the most emissive nanoscale composition, [Y_{1.9}O₃; Eu_{0.1}, Li_{0.16}], were determined for solid-state samples at 20 40, 120, and 220 kVp excitation through modulation of the x-ray tube current (mA). For a given x-ray tube voltage, the tube current was adjusted in 2-5 mA steps to provide a range of x-ray exposure rates (R/s). **Figure 3** shows the linear response of the integrated emission intensity over the 500 - 700 nm emission 25 range recorded for 40, 120, and 220 kVp x-ray excitation energies. For 120 and 220 kVp excitation, integrated scintillation intensities were recorded over identical exposure-rate ranges (0.6

- 4.0 R/s) in order to assess the energy dependence of the scintillation intensity. Note that the dependences of scintillation ³⁰ intensity upon radiation dose differ slightly at these two excitation energies (**Figure 3B-C**), as the slope determined at 120
- kVp surpasses that at 220 kVp by a factor of 1.2. As both of these x-ray excitation energies exceed that of the yttrium k-edge (17 keV), this effect is congruent with the facts that (i) yttrium-oxide ³⁵ displays a higher mass-attenuation coefficient (ionizing radiation
- absorption) at 120 kVp than 220 kVp,²⁵ and (ii) the scintillation mechanism is dominated by the photoelectric effect at 120 kVp, and the Compton effect at 220 kVp, for yttrium's Z-number of $39.^{26}$ These data further underscore that the scintillation intensity
- ⁴⁰ observed for the nanoscale [Y_{1.9}O₃; Eu_{0.1}, Li_{0.16}] composition for photoelectric energy region absorption exceeds that for Compton energy region absorption, for comparable high-energy photon exposures and this nanocrystalline lattice.
- The spectroscopically demonstrated linear response of 45 scintillation intensity with x-ray energy and flux for these nanocrystals, across broad, medically relevant energy and exposure ranges (**Figure 3**), underscores the potential utility of these nanomaterials. As such, a prototype device for measuring radiation exposure (dosimetry), based on the most emissive

50 nanoscale composition, was developed. [Y_{1.9}O₃; Eu_{0.1}, Li_{0.16}] nanocrystals (1 mg) were pressed into a 7 mm flat disk; a fractured piece of ~400 µm diameter (~3.3 µg) was employed as the device detection element, and optically-glued to one end of a 400 µm (inner diameter) optical fiber. The other end of the fiber 55 was connected to a high-sensitivity, high-spectral resolution CCD-spectrometer (Figure 4A). The scintillation intensity from the [Y_{1.9}O₃; Eu_{0.1}, Li_{0.16}]-modified optical fiber tip, integrated over the 605 - 617 nm wavelength domain (note that this integration range is limited by the CCD-spectrometer spectral 60 window), was correlated with radiation exposure using a Precision XRAD 225Cx small-animal image guided radiation therapy (IGRT) system, in order to highlight the relevance of this prototype device to in vivo radiation dosimetry. A key feature of the Precision XRAD 225Cx instrument is that it employs low 65 dose x-ray computed tomography (CT) to image a specific organ or tissue area of interest, prior to delivery of therapeutic x-ray doses via an x-ray pencil-beam that targets millimeter-sized areas of malignant tissue at high precision, thus minimizing healthy tissue damage.²⁷ The spatial dimensions of the x-ray pencil-beam 70 precludes use of conventional dosimetry devices to measure the radiation dose delivered to small treatment areas, and thus underscore one potential role for nanoscale scintillating materials in medicine.



Figure 4. (A) A schematic of the sub-mm-sized optical fiber prototype dosimeter based on nanoscale [$Y_{1.9}O_3$; Eu_{0.1}, Li_{0.16}]. (B) An x-ray CT image acquired at 40 kVp, showing the optical fiber device adjacent to an ion-chamber radiation detector. (C) The linear scintillation intensity recorded by the device integrated over 605 - 617 nm that measures the total dose deposited at 80 kVp (imaging) and 225 kVp (therapy) energies. The CT image was acquired in a Precision XRAD 225Cx small-animal image guided radiation therapy (IGRT) system; the scintillation data were recorded using IGRT 80 and 225 kVp excitation. Note that all data points were measured in triplicate, and the standard deviation for a given data point was < 0.9%. The inset of (C) shows that the device scintillation response tracks linearly with exposure to the highest levels tested (117.8 Roentgen at 225 kVp).

Figure 4B shows an x-ray image taken at 40 kVp of the fiber-⁷⁵ optic device next to a standard ion-chamber radiation detector used to calibrate the radiation exposure on the Precision XRAD 225Cx image guided radiation therapy (IGRT) system. Note that the copper wires present in the ion-chamber show dark contrast, highlighting that the sensor portion of the prototype detector ⁸⁰ based on nanoscale [Y_{1.9}O₃; Eu_{0.1}, Li_{0.16}] is effectively radiotransparent during diagnostic imaging, due to the lowdensity, low Z-number, and small size of the fiber-optic. The radio transparency of the fiber-optic device underscores its *invivo* utility with the IGRT system as it alternately provides ⁸⁵ accurate dosimetry measurements for both diagnostic imaging and radiation therapy treatment, while precluding the possibility for significant imaging artefacts that accompany the use of ion chamber- or MOSFET-based dosimeters.

- **Figure 4C** displays a plot of integrated scintillation intensity $_{5}$ (605 617 nm) versus total radiation exposure at both 80 kVp (diagnostic imaging) and 225 kVp (therapy) energies. As noted earlier for data that compared emission intensity for 120 and 220 kVp excitations at equivalent exposures (**Figure 3B-C**) for the [Y_{1,9}O₃; Eu_{0,1}, Li_{0,16}] composition, 80 kVp incident x-rays
- ¹⁰ produce more light than do 225 kVp x-rays over identical 0 6 Roentgen exposure ranges, further highlighting this nanomaterial is more emissive when the scintillation mechanism is dominated by the photoelectric effect. Since the entire scintillation spectrum, not just a single scintillation wavelength, expresses a linear
- ¹⁵ response with respect to radiation exposure (**Figure 3A-C**), simple device architectures that exploit Si-photodiodes can be fabricated that take advantage of Si-photodiodes' maximal sensitivity over the emission range of nanoscale [Y_{1.9}O₃; Eu_{0.1}, Li_{0.16}]. Note that such devices that exploit rare-earth doped
- ²⁰ inorganic nanocrystals will compliment pioneering optical fiber dosimeters that are based on plastic scintillating materials,²⁸⁻³⁰ while providing superior environmental and radiation stability, new scintillation energy ranges, and the opportunity for significantly red-shifted luminescence, in a device architecture
- 25 that provides fast timing speeds, small size, and low powerconsumption.

Conclusions

In summary, Eu- and Li-doped yttrium oxide nanocrystals $[Y_{2-x}O_3; Eu_x, Li_y]$ in which Eu and Li dopant ion concentrations were ³⁰ systematically varied, were developed and characterized (TEM, XRD, Raman spectroscopic, UV-excited lifetime, and ICP-AES data) in order to define the most emissive compositions under specific x-ray excitation conditions. These optimized $[Y_{2-x}O_3; Eu_x, Li_y]$ compositions display scintillation responses that: (i)

- ³⁵ correlate linearly with incident radiation exposure at x-ray energies spanning from 40 - 220 kVp, and (ii) manifest no evidence of scintillation intensity saturation at the highest evaluated radiation exposures [up to 4 Roentgen per second]. For the most emissive nanoscale scintillator composition, $[Y_{1,9}O_3;$
- ⁴⁰ Eu_{0.1}, Li_{0.16}], excitation energies of 40, 120, and 220 kVp were chosen to probe the dependence of the integrated emission intensity upon x-ray exposure-rate in energy regimes having different mass-attenuation coefficients and where either the photoelectric or the Compton effect governs the scintillation
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- ⁵⁰ relative to excitation energies where the Compton effect regulates scintillation (220 kVp) in nanoscale $[Y_{2-x}O_3; Eu_x]$ crystals. Nanoscale $[Y_{1.9}O_3; Eu_{0.1}, Li_{0.16}]$ (70 \pm 20 nm) was further exploited as a detector material in a prototype fiber-optic radiation sensor. The scintillation intensity from a $[Y_{1.9}O_3; Eu_{0.1},$
- $_{55}$ Li_{0.16}]-modified, 400 μm -sized optical fiber tip, recorded using a CCD-photodetector and integrated over the 605 617 nm wavelength domain, was correlated with radiation exposure using

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- ⁶⁰ radiotransparent device recorded scintillation intensities that tracked linearly with total radiation exposure in a micro-CT dual imaging and high precision cone-beam therapy instrument utilized for small-animal image guided radiation therapy (IGRT): these data highlight the capability of these nanomaterials to
- ⁶⁵ provide alternately accurate dosimetry measurements for both diagnostic imaging (80 kVp) and radiation therapy treatment (225 kVp), and underscore one potential role for [Y_{2-x}O₃; Eu_x, Li_y] nanoscale scintillating materials in medicine.
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- † Electronic Supplementary Information (ESI) available: Material synthesis; experimental details; x-ray diffraction (XRD), UV-excited lifetimes, ICP-AES, and additional TEM data. See s5 DOI: 10.1039/b000000x/

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95 Notes and references

- P. A. Rodnyi, *Physical Processes in Inorganic Scintillators* CRC Press, 1997.
- 2. M. Nikl, Meas. Sci. Technol., 2006, 17, R37-R54.
- 3. C. W. E. van Eijk, Phys. Med. Biol., 2002, 47, R85-R106.
- 100 4. L. Ozawa and M. Itoh, Chem. Rev., 2003, 103, 3835-3855.
 - S. J. Duclos, C. D. Greskovich, R. J. Lyons, J. S. Vartuli, D. M. Hoffman, R. J. Riedner and M. J. Lynch, *Nucl. Instrum. Meth.* A., 2003, 505, 68-71.
- Q. Dai, M. E. Foley, C. J. Breshike, A. Lita and G. F. Strouse, J. Am.
 Chem. Soc., 2011, 133, 15475-15486.
 - B. K. Gupta, T. N. Narayanan, S. A. Vithayathil, Y. Lee, S. Koshy, A. L. M. Reddy, A. Saha, V. Shanker, V. N. Singh, B. A. Kaipparettu, A. A. Marti and P. M. Ajayan, *Small*, 2012, 8, 3028-3034.
- 110 8. G. Wakefield, E. Holland, P. J. Dobson and J. L. Hutchison, *Adv. Mater.*, 2001, **13**, 1557-1560.
 - S. S. Brown, A. J. Rondinone and S. Dai, in *Antiterrorism and Homeland Defense: Polymers and Materials*, eds. J. G. Reynolds, G. E. Lawson and C. J. Koester, 2007, p. 117.

Nanoscale

- 10. S. E. Letant and T. F. Wang, Nano Lett., 2006, 6, 2877-2880.
- C. Sun, G. Pratx, C. M. Carpenter, H. G. Liu, Z. Cheng, S. S. Gambhir and L. Xing, *Adv. Mater.*, 2011, 23, H195-H199.
- 12. S. E. Letant and T. F. Wang, Appl. Phys. Lett., 2006, 88, 103110.
- 5 13. C. Dujardin, D. Amans, A. Belsky, F. Chaput, G. Ledoux and A. Pillonnet, *IEEE T. Nucl. Sci.*, 2010, 57, 1348-1354.
- 14. I. N. Stanton, J. A. Ayres and M. J. Therien, *Dalton Trans.*, 2012, **41**, 11576-11578.
- 15. T. Ye, G. W. Zhao, W. P. Zhang and S. D. Xia, *Mater. Res. Bull.*, 10 1997, **32**, 501-506.
- Y. Repelin, C. Proust, E. Husson and J. M. Beny, J. Solid State Chem., 1995, 118, 163-169.
- S. S. Yi, K. S. Shim, H. K. Yang, B. K. Moon, B. C. Choi, J. H. Jeong, J. H. Kim and J. S. Bae, *Appl. Phys. A-Mater. Sci.*
- 15 *Process.*, 2007, **87**, 667-671.
- J. S. Bae, J. H. Yoon, S. K. Park, J. P. Kim, E. D. Jeong, M. S. Won, J. H. Jeong, K. S. Shim, H. K. Yang and S. S. Yi, *Surf. Rev. Lett.*, 2007, 14, 535-538.
- 19. S. Ray, P. Pramanik, A. Singha and A. Roy, J. Appl. Phys., 2005, 97,
- 20 094312.
- D. R. Tallant, C. H. Seager and R. L. Simpson, J. Appl. Phys., 2002, 91, 4053-4064.
- 21. R. A. Buchanan, K. A. Wickersheim, J. L. Weaver and E. E. Anderson, *J. Appl. Phys.*, 1968, **39**, 4342-4347.
- 25 22. S. M. Yeh and C. S. Su, Mat. Sci. and Eng., B, 1996, 38, 245-249.
- 23. S. S. Yi, J. S. Bae, K. S. Shim, J. H. Jeong, J. C. Park and P. H. Holloway, *Appl. Phys. Lett.*, 2004, 84, 353-355.
- 24. B. L. Abrams and P. H. Holloway, *Chem. Rev.*, 2004, **104**, 5783-5801.
- 30 25. M. J. Berger, J. H. Hubbell, S. M. Seltzer, J. Chang, J. S. Coursey, R. Sukumar, D. S. Zucker and K. Olsen, *XCOM: Photon Cross Section Database (version 1.5)*, 2010, Available: <u>http://physics.nist.gov/xcom</u>. National Institute of Standards and Technology, Gaithersburg, MD.
- 35 26. F. H. Attix, Introduction to Radiological Physics and Radiation Dosimetry, John Wiley & Sons, Inc., 1986.
- 27. L. A. Dawson and D. A. Jaffray, J. Clin. Oncol., 2007, 25, 938-946.
- D. Klein, T. M. Briere, R. Kudchadker, L. Archambault, L. Beaulieu, A. Lee and S. Beddar, *Radiat. Meas.*, 2012, 47, 921-929.
- 40 29. L. Archambault, T. M. Briere, F. Ponisch, L. Beaulieu, D. A. Kuban, A. Lee and S. Beddar, *Int. J. Radiat. Oncol.*, 2010, **78**, 280-287.
- L. Archambault, J. Arsenault, L. Gingras, A. S. Beddar, R. Roy and L. Beaulieu, *Med. Phys.*, 2005, 32, 2271-2278.
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Table of Contents Graphic:



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