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## Spray coated all-solid-state potentiometric sensors

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### Abstract

A novel fully spray coating based method of preparation of all-solid-state ion-selective electrodes of simplified construction is proposed. This method is alternative for screen-printed electrodes used sometimes in potentiometric applications. The benefits of herein proposed approach include fully automatic sensor preparation as well as minimized use of chemicals allowing production of low cost sensors that can be applied as disposables.

A spray coated carbon nanotubes layer on inert support was used both as electrical lead and as transducer, to simplify sensor layout and to avoid possible problems of changing in time composition of this layer, as previously observed in the case of screen-printed supporting electrodes in potentiometric applications.

The ion-selective poly(vinyl chloride) based membrane and the insulator layer were spray-coated, too. Obtained sensors, as model system potassium-selective sensors were prepared, were characterized with analytical parameters well comparable with those of conventional all-solid-state ion-selective electrodes. The applicability of herein proposed approach to prepare also other ion-selective electrodes was tested on example of H<sup>+</sup> and Cl<sup>-</sup> sensor.

## Introduction

Internal solution free ion-selective electrodes have nowadays established position in the potentiometry [1]. All-solid-state ion-selective electrodes (ASS-ISEs) can offer analytical parameters well comparable with those of conventional internal solution containing potentiometric sensors, including stability of potential values recorded in time [1,2]. In principle ASS-ISEs can be a low cost, easy to produce, miniature, reliable and disposable alternative to conventional potentiometric sensors; however, this idea has not been fully accomplished in practice, yet. The classical set up of ASS-ISEs applies a macroscopic inert substrate electrode [1,2], which is further modified by application of a transducer layer (required to achieve high stability of potential readings in time) and an ion-selective membrane. The cost and size of supporting electrode and the manual operations required to obtain ASS-ISEs hinder mass scale preparation of cost-effective, miniature, disposable sensors.

Application of simple low cost methods leads to substantial improvements in electronics and related fields offering a simple, disposable elements [e.g. 3]. In this respect screen-printed electrodes are of interest, too. They allow not only miniaturization but also custom tailored arrangements of electrodes and they are successfully used e.g. in amperometric sensing; a range of screen-printed electrodes for this purpose is available commercially [4]. Although application of screen-printing technique to automatize production of sensors containing sparingly soluble salts dispersed within electrochemically inactive matrix (analogues of sparingly-soluble salts membranes) has been reported [e.g. 5], this approach for obvious reasons is applicable only to a few systems.

Screen-printed *substrate* electrodes have been also used to prepare potentiometric sensors. This approach requires modification of screen-printed substrate with conducting polymers (CPs) [6,7,8] or carbon nanotubes (CNTs) [9], i.e. materials typically applied as ion-to-electron transducers for ASS-ISEs. Both CNTs and CPs are often applied by drop casting of their solution / dispersion [7,8,9]. CPs layers can be also obtained by direct electropolymerization on screen-printed substrate [e.g.6]. The next step is usually manual drop casting of solution / dispersion of an ion-solution membrane cocktail [6-9]. Thus, similarly as for classical ASS-ISEs, a few manual operations are necessary to prepare a potentiometric sensor, even though the substrate electrodes can be produced automatically, increasing cost and material consumption hinder practical application as disposable electrodes.

The obtained sensors (as model mainly K<sup>+</sup>-selective electrodes were prepared) are usually characterized with analytical parameters slightly worse (detection limit, selectivity) when

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3 compared with arrangements using classical ASS-ISEs [6-9]. Although this deviation from  
4 typical (the best achievable) parameters in principle is acceptable for many applications,  
5 usage of screen-printed electrodes in potentiometry is limited, in contrary to their popularity  
6 in e.g. amperometry. Clearly one of the reasons lies in the combination of nature of screen-  
7 printing method and time scale of potentiometric vs. amperometric measurements. The latter  
8 are usually completed within seconds or a few minutes at the most. On the other hand,  
9 potentiometric measurements, even using nominally disposable electrodes, take significantly  
10 longer – due to nature of technique (calibration required, signal stabilization). Occasionally,  
11 even disposable sensors are required to work continuously for a few hours or days. In this  
12 time scale unwanted spontaneous processes occurring within the screen-printed layer, e.g.  
13 hydrolysis of the applied paint components, can occur and adversely affect the performance of  
14 the sensor. These processes usually result in formation of species that can partition into the  
15 ion-selective membrane ultimately affecting the analytical parameters of the sensors [e.g.<sup>6</sup>].  
16 In short time scale (e.g. in amperometric measurements) these effects are insignificant; however,  
17 can be severe in potentiometric experiment time scales, especially as the details of the  
18 composition of the screen-printing paste is usually unknown. The other issue that increases in  
19 significance in longer time scale is adhesion of layers constituting the sensor. In the case of  
20 screen-printed substrate electrode, to solve this problem introduction of adhesive admixture to  
21 the membrane composition was required [7,8].

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The issue of adhesion of the PVC based membrane to the substrate (in the case of internal  
solution free sensors and optical sensors) has been discussed in literature for many years now,  
mainly looking at SiO<sub>2</sub> based substrates [e.g.<sup>10, 11, 12, 13, 14</sup>]. In this respect Kapton (polyimide)  
support, in the arrangement using gold tracks as electrical lead/substrate, covered with  
hydrogel layer and then by solvent cast PVC membrane [15] has been found a promising  
material for miniature, planar potentiometric sensors for bio-medical applications [16] already  
20 years ago.

The above mentioned issues related to application of screen-printed sensors in potentiometry,  
have stimulated search for alternative approaches that can lead to planar, low-cost, and  
potentially disposable ion-selective electrodes. There is a clear research interest in  
development of such sensors, especially in recent years. This has led for example to  
application of ink-jet printing for sensor development [17].

Also alternative approaches have been studied, their common feature is manual application of  
a conducting material (as e.g. suspension), most often conducting polymer [18, 19, 20], graphene  
[21] or carbon nanotubes [22] that play a role of both substrate and transducer on inert

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3 supporting material: acetate foil [<sup>18,19,20,21</sup>] or paper [<sup>22</sup>]. Alternatively semi-manual methods  
4 using aerograph, manually operated type devices are used to obtain e.g. carbon nanotubes  
5 layers [<sup>22,23</sup>]. Sometimes this step is also followed by additional manual treatment (washing)  
6 of the obtained layer [e.g.<sup>22</sup>]. The next manual step required is drop casting an ion-selective  
7 membrane cocktail [<sup>18-22</sup>]. Definitely, this approach is free from risk related to unknown and  
8 unstable (in time, in water environment) composition of the substrate layer; however, the  
9 manual operations required still hinder mass scale production. Moreover, these are potentially  
10 less reproducible and more material consuming compared to automatic alternatives,  
11 highlighting the need for alternative approach.

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13 On the other hand, electronic devices (e.g. field effect transistors or solar cells) benefit from  
14 spray coating method of (conducting) layers application [e.g.<sup>24,25,26</sup>]. This method, to our best  
15 knowledge, has not been applied to prepare ion-selective membrane layers, or to prepare  
16 potentiometric sensors, yet. Among layers that can be spray coated on different substrates,  
17 including plastic and glass, are carbon nanotubes (CNTs) of high electrical conductivity [e.g.  
18 <sup>27</sup>]. The CNTs layers thus obtained conveniently can be used as electrical lead and substrate/  
19 transducer of potentiometric sensors. From the potentiometric application point of view it is  
20 also important that spray coated layers do not contain any binders, thickening agent or any  
21 material that can undergo uncontrolled changes during even long time contact with water  
22 based sample. Moreover, spray coating offers higher reproducibility and better control of  
23 resulting layers compared to manual (e.g. paintbrush [<sup>22</sup>] or drop casting [<sup>18-21</sup>]) application,  
24 and the usage of materials can be minimized, too. Spray coating – due to mild conditions of  
25 the process – can be applicable to the (sensitive) ion-selective membrane as well. The demand  
26 of preparing all layers of a sensor in the same technology can be achieved, moreover, in  
27 automatized procedure.

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29 In this work, we report for the first time on ion-selective electrodes prepared using solely a  
30 spray coating method. As an electrical lead support and transducer - spray coated CNTs layers  
31 were used. The ion-selective membrane was also coated by spraying membrane cocktail over  
32 (part of) the CNTs layer. As an insulating layer (PVC protective layer) – separating the part of  
33 CNTs used as electrical lead, from the substrate layer, a plasticized poly(vinyl chloride)  
34 (PVC) film was spray coated. As a model system, potassium-, hydrogen ion- and chloride-  
35 selective electrodes using plasticized PVC membranes were prepared.

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### Experimental

#### Chemicals

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3 Tetrahydrofuran (THF), poly(vinyl chloride) (PVC), bis(2-ethylhexyl) sebacate (DOS),  
4 valinomycin, sodium tetrakis[3,5-bis(trifluoromethyl)phenyl]borate (NaTFPB), potassium  
5 tetrakis(4-chlorophenyl)borate (KTChPB), tridodecylamine, tridodecylmethylammonium  
6 chloride (TDDM-Cl), multiwalled carbon nanotubes (MWCNTs) were from Fluka AG  
7 (Buchs, Switzerland) or from Aldrich (Germany).  
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11 All reagents used were analytical grade salts (Aldrich (Germany). Deionised water (resistance  
12 18.2 MΩcm, Milli-Qplus, Millipore) was used throughout this work.

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14 As a substrate layers for spray coating either polyimide - Kapton<sup>®</sup> HM (DuPont) or  
15 polyethylene terephthalate (PET) Hostaphan<sup>®</sup> (Mitsubishi) sheets were used.  
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## 19 *Apparatus*

### 20 *Spray coating*

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22 For spray coating the layers a pneumatically controlled Krautzberger M10 spray head was  
23 used, with nitrogen as atomizing gas. Samples were placed on a hotplate under the spray gun  
24 and coated with the different materials at different sample to nozzle distances. In case of the  
25 CNT layer the coating was done in several cycles with breaks in between to allow a drying of  
26 the layers. Otherwise big droplet formation would be present on the sample causing  
27 inhomogeneous layers. Thickness of layers is defined by the number of spray cycles as  
28 thickness is increasing linearly with spray time. In case of the CNT layer the coating was  
29 made in several cycles with breaks in between to allow drying of the layers. This was not  
30 necessary for the ion-selective membrane/ PVC protective layer as the THF used as solvent  
31 was evaporating much faster, allowing a continuous coating of the substrates. The patterns  
32 were achieved by the use of different shadow masks resembling the pattern needed for each  
33 layer. Like in optical lithography these shadow masks block the sprayed material in areas  
34 where it is not desired. A new pattern can be implemented quickly by just replacing the  
35 shadow mask. A drawback of spray coating when used in small scale with a stationary setup  
36 is the amount of material needed. If the spray head is not moved across the sample, only the  
37 centre of the sprayed area shows homogenous layer thickness. However, this can be overcome  
38 easily by the use of non-stationary spraying devices and/or up scaling the fabrication for  
39 example in roll-to-roll processes.  
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### 53 *Electrochemical measurements*

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55 In the potentiometric experiments and electrochemical measurements, an experimental setup  
56 described earlier e.g. [28] was used. The recorded potential values were corrected for the liquid  
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3 junction potential calculated according to Henderson approximation. The glass electrode used  
4 was from Moeller AG, Switzerland.  
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### 7 *Ion-selective membranes*

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9  $K^+$ -selective membranes contained (by weight): 1.2 % NaTFPB, 2.8 % valinomycin, 64.4 %  
10 DOS and 31.6 % PVC. Total 200 mg were dissolved in 20 ml of THF.

11 The insulation mask membrane contained (by weight): 40 % PVC and 60 % DOS. Total 400  
12 mg were dissolved in 40 ml of THF.

13  $H^+$ -selective membrane contained (by weight): 1.0 % of tridodecyl amine, 0.6 % KTChPB,  
14 63.8 % DOS and 34.6 % of PVC. Total 200 mg were dissolved in 20 ml of THF.

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16  $Cl^-$ -selective membrane contained (by weight): 5 % TDDM-Cl, 32.9 % PVC and 62.1 %  
17 DOS. Total 200 mg were dissolved in 20 ml of THF.  
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### 26 *Fabrication of CNT ink*

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28 6 g of sodium dodecyl sulfate (SDS) were dissolved in 60 ml water and stirred for 1 hour.  
29 Subsequently 30 mg of MWCNT (0,05 wt %) were added and the mixture was sonicated with  
30 a horn sonicator (Branson Digital Sonifier 450) three times for 5 minutes each with 5 minutes  
31 breaks in between for cooling. Then, the solution was centrifuged for 1.5 hours at 15000 rpm.  
32 After centrifugation the top 75 % of the solution was used as ink.  
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### 38 *Substrate preparation*

39 About 50 mm x 20 mm PET or Kapton sheets were put in an ultrasonic bath with isopropanol  
40 for 20 minutes and dry blowed with nitrogen. Before spray coating both kinds of substrates  
41 were put into an oxygen plasma (150 W, TePla 100-E) for 1 minute to increase wettability.  
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### 46 *Spray coating of CNTs layers*

47 The substrates were put onto a hot plate and heated up to 30°C and then coated with 1 bar  
48 atomizing gas pressure and 25 cm nozzle to substrate distance 25 times for 30 seconds with  
49 15 seconds drying steps in. A line pattern with 4 mm width and 30 mm length was fabricated  
50 by using a shadow mask. After spray coating, the substrates were dried for one hour at room  
51 temperature. To remove the SDS, the substrates were put in water for 15 minutes, afterwards  
52 in isopropanol for 10 minutes and finally blown dry with nitrogen.  
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### *Spray coating of ion-selective membrane/ PVC protective layer*

On top of the CNT electrode a circle with 4 mm diameter of the ion-selective membrane was deposited with a substrate to nozzle distance of 15 cm and 1 bar atomizing gas pressure for 40 s at room temperature, resulting in a layer with a thickness close to 40  $\mu\text{m}$ .

As last step the PVC protective layer was deposited on top with a substrate to nozzle distance of 17 cm and 1 bar atomizing gas pressure for 60 s also at room temperature, as well resulting in a layer thickness close to 60  $\mu\text{m}$ . During this step the ion-selective membrane was covered by a circular shadow mask with a 3mm diameter, forming an active window of 7.06  $\text{mm}^2$ . The 0.5 mm overlap of both layers ensures that no gap between the membrane and the protective layer is present. Thus obtained ion-selective electrodes before measurement were conditioned in  $10^{-3}$  M KCl for 1 h. In-between measurements electrodes were stored in air.

### **Results and Discussion**

The spray coating of substrate with CNTs has resulted in conducting layers characterized with resistivity close to 40 kOhm/square. They were composed of a porous network of tangled carbon nanotubes, as shown in Fig. 1. The thickness of the spray coated layer was about 200 nm. Thus obtained MWCNTs layers can be used as substrate to obtain ion-selective electrodes by spray coating ion-selective membrane and insulating PVC film, Fig. 1.

Potentiometric responses of spray coated potassium selective electrodes are shown in Fig. 2. For sensors prepared on Kapton as well as on PET linear responses within the activities range from 0.1 to  $10^{-6}$  M with Nernstian slope equal to  $59.8 \pm 0.4$  mV/dec ( $R^2 = 0.9998$ ) and  $59.6 \pm 0.5$  mV/dec ( $R^2 = 0.9996$ ), respectively, and the detection limits (DLs) equal to  $10^{-6.5}$  M were obtained. Spray coated sensors characteristics obtained are well comparable with those of classical ASS-ISEs potassium sensors reported, including those examined in our group [e.g. <sup>2</sup>]. They are also well comparable with planar arrangements based on screen-printed substrates and CNTs transducer [<sup>9</sup>] or manually coated layers of graphene/ CNTs used both as transducer and electrical lead [<sup>21</sup>], and show more favorable DLs compared to paper based sensors using CNTs as transducer and electrical lead [<sup>22</sup>].

The obtained logarithms of selectivity coefficients  $\pm$  SD, for activities range from 0.1 to  $10^{-4}$  M (separate solution method, using experimental slope values) were:  $\log K_{K,Na}$   $-3.3 \pm 0.4$  and  $-2.8 \pm 0.3$ ;  $\log K_{K,Mg}$   $-4.4 \pm 0.4$  and  $-3.4 \pm 0.3$ ;  $\log K_{K,Ca}$   $-4.6 \pm 0.3$  and  $-3.6 \pm 0.4$ ;  $\log K_{K,H}$   $-4.5 \pm 0.3$  and  $-4.0 \pm 0.6$ , for Kapton and PET substrate, respectively. Although selectivity coefficients obtained are well comparable with those obtained for other (nominally disposable) systems [e.g. <sup>18,22</sup>] prepared using PVC based membranes, there were some

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3 differences between sensors prepared using Kapton and PET substrates. Despite the sensors  
4 were pretreated/ tested in parallel, repeatedly Kapton substrate based sensors prove to be  
5 characterized by somewhat higher selectivity for divalent interfering ions compared to PET.  
6 In our opinion this effect, consistently seen in tested sensors, can be related to the substrate  
7 effect, especially as relatively thin ion-selective membrane were used (c.a. 4 times thinner  
8 compared to standard membrane thickness used [e.g.<sup>2</sup>]).

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10 The preliminary conclusions drawn from conducted experiments related to reproducibility of  
11 automatic manufacturing production method are highly encouraging. The differences in  $E^0$   
12 potential value between sensors prepared in one manufacturing batch (regardless type of the  
13 substrate used) were in the range of a few mV. The response time of spray coated sensors was  
14 dependent on activity of sample solution, however, it was observed that sensors prepared  
15 using Kapton substrate were characterized with shorter responses time compared to PET ones,  
16 reaching about 20 s and about 70 s, respectively; as shown in Fig. S1 for electrolyte  
17 concentration change from  $10^{-2}$  to  $10^{-3}$  M.

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19 The reproducibility of potential readings of nominally disposable spray coated made  
20 potentiometric sensors (within day) was tested in a non-optimized setup – simply in a beaker.  
21 Mean values  $\pm$  SD of potentials recorded for each activity during four consecutive calibrations  
22 performed within the broad KCl activity range (from 0.1 to  $10^{-9}$  M) are presented in Fig. 2.  
23 Fig. 2 clearly shows that both supports used result in sensors characterized with similar and  
24 high reproducibility of potential values recorded (SD of values recorded  $\leq$  9 mV). The results  
25 presented clearly confirm that although herein proposed system is prepared using relatively  
26 small amount of chemicals per sensor (relatively thin layers of automatically applied  
27 materials) the sensor offers sufficient long term stability to enable multiple measurements.

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29 Moreover, the potentiometric performance of sensors tested both shortly after preparation  
30 (e.g. < 2 weeks, including the transport between cooperating groups laboratories) or after  
31 significantly longer storage (in fridge, due to valinomycin ionophore used) was the same  
32 within the range of experimental error, which is promising for practical applications.

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34 The reproducibility of potential values is well comparable with that obtained by us in similar  
35 tests performed for traditional sensors (glassy carbon supporting electrode) with one of the  
36 most trusted transducer – poly(3-octylthiophene) [29]. This result is highly promising from the  
37 point of view of possible practical application of the simplified sensors herein proposed.

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39 The stability of potentiometric responses within longer time period was also studied.  
40 Although such tests are generally rarely performed for nominally disposable sensors, in our  
41 opinion this is an important long term stability test for any new proposed arrangement. The  
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3 SD of mean value of potentials recorded were changing with electrolyte concentration, lower  
4 SD values were obtained for linear range of responses (close to 7 mV), somewhat higher  
5 values were obtained for lower activities, Fig. S2.  
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8 The usual set of tests applied for novel type potentiometric all-solid-state sensors includes  
9 impedance spectroscopy [2]. Fig. 3 presents complex plane impedance plots for sensors with  
10 Kapton and PET support, respectively. For the Kapton support, the spectrum contains a single  
11 semicircle at higher frequencies followed by a linear part recorded at lower frequencies (slope  
12 close to 45 degrees) and then the slope of dependence increases with decreasing frequency.  
13 For the PET substrate the picture is more complicated suggesting overlapping of two  
14 semicircles at high frequencies. This effect can result from additional resistance in the  
15 presence of the PET support. It can be noticed that the shapes of plots for  $Z'$  higher than  $6 \cdot 10^5$   
16  $\Omega$  (Kapton) and  $3 \cdot 10^5 \Omega$  (PET) are similar. The plot obtained for PET support seems to be  
17 shifted to  $3 \cdot 10^5 \Omega$  higher resistances compared to the Kapton one, suggesting the same  
18 properties in the case of both supports, related to the membrane, CNT transducer, and their  
19 interface. The shape of the EIS response suggests that it can be analyzed using the simplified  
20 equivalent circuit, proposed in [21] for the glassy carbon and plastic electrodes with CNT  
21 layer, Fig.3. This circuit consists of solution resistance,  $R_s$ , and parallel connected  $R$  and  $C_g$ ,  
22 representing the membrane resistance (as the most resistive component of the sensor) and  
23 geometric capacitance of the sensor (membrane), respectively.  $Z_w$  represents Warburg  
24 impedance resulting from diffusion limitations in the membrane, while  $C_b$  corresponds to bulk  
25 capacitance of the CNT layer responsible for its transducing properties. For the data  
26 presented, Fig. S3 shows the results of a fitting procedure which was applied to the  
27 experimental data for the sensor with Kapton support, leading to good concordance with  
28 experimental data. The  $R$  resistance and  $C_g$  are typical values obtained for PVC based  
29 membrane ( $4.8 \cdot 10^5 \Omega$  and  $1.7 \cdot 10^{-10} \text{ F}$ , respectively), while  $C_b$  around  $2 \cdot 10^{-6} \text{ F}$  is typical for  
30 carbon supports [30]. Similar (within the range of experimental error) values of the  $R$  and  $C_b$   
31 were obtained also from chronopotentiometric experiment (results not shown).  
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48 The same methodology was used to prepare  $\text{H}^+$ -selective electrodes (on PET substrate) using  
49 tridodecylamine as ionophore. Thus obtained sensors were characterized with linear responses  
50 of slope equal to  $53.7 \pm 1.1 \text{ mV/dec}$  ( $R^2 = 0.997$ ) for hydrochloric acid concentration change  
51 from 0.1 to  $10^{-5} \text{ M}$ . Thus obtained sensor was used to determine  $\text{H}^+$  concentration of 3  
52 different branches of orange juices. The results obtained using herein prepared nominally  
53 disposable  $\text{H}^+$  sensitive sensor were within the range of experimental error comparable with  
54 that of performed in parallel experiment with glass electrode determination in unoptimized  
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3 experimental setup – in beaker measurements (3.83 and 3.85; 3.72 and 3.74; 3.91 and 3.95,  
4 for spray-coated and glass H<sup>+</sup> selective electrode, respectively). These results clearly show  
5 that herein proposed sensors can be used as cost effective devices (relatively low chemicals  
6 consumptions to prepare sensor) in analysis of real samples.  
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9 As model anion-selective sensor Cl<sup>-</sup>-selective electrode was also prepared (on PET substrate).  
10 Thus obtained sensors were characterized with linear responses within the KCl concentration  
11 range from 0.1 to 10<sup>-5</sup> M with slope equal to  $-56.3 \pm 1.3$  mV/dec ( $R^2 = 0.994$ ). The selectivity  
12 of thus obtained sensor was tested for model interferens Br<sup>-</sup> and NO<sub>3</sub><sup>-</sup> anions. Obtained  
13 selectivity coefficients (for ions that are known to be severe interferents for chloride-ion  
14 selective sensor; separate solution method within the activity range from 10<sup>-1</sup> to 10<sup>-3</sup> M) were  
15 equal to  $\log K_{Cl,Br}$  1.3 and  $\log K_{Cl,NO_3}$  1.6. These values are more favorable than reported  
16 earlier for other classical size all-solid-state chloride-selective electrode of the similar  
17 membrane [<sup>31</sup>], clearly showing that herein proposed method can be used to prepare sensors  
18 responding to different ions.  
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## 28 **Conclusions**

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30 The results presented above clearly show that the novel, automatized method of preparation of  
31 potentiometric sensors herein proposed – spray coating - is a simple and efficient method of  
32 production leading to reliable potentiometric sensors. The construction proposed – carbon  
33 nanotubes used as support and transducer - resulted in sensor of analytical performance well  
34 comparable with that of traditional solid state ion-selective electrodes based on glassy carbon  
35 support. Elimination of manual application of membrane is advantageous from sensors mass  
36 scale production point of view.  
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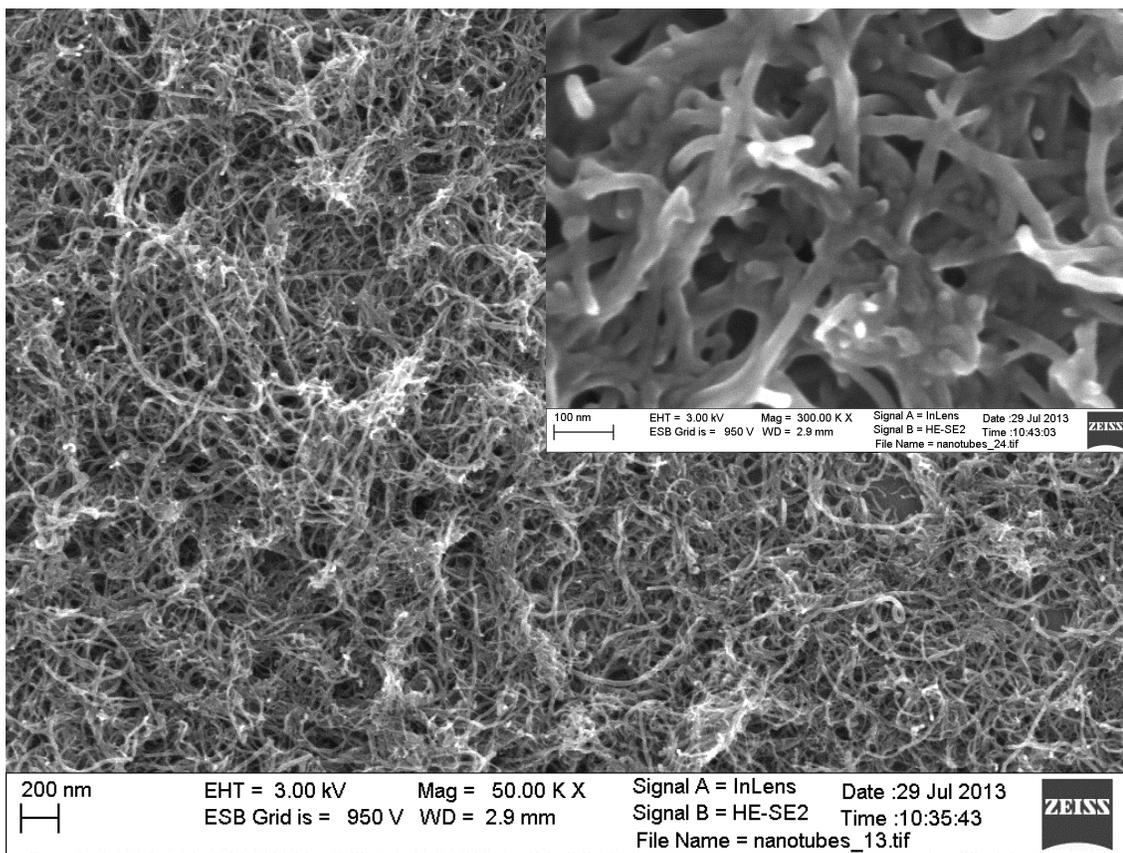
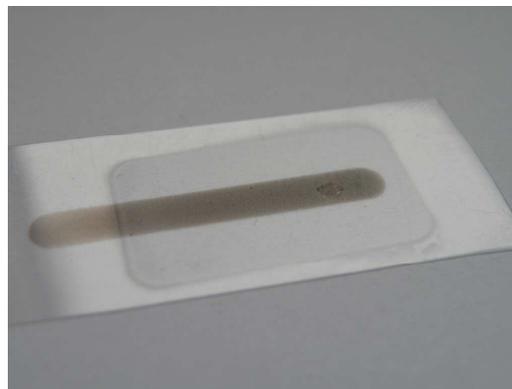
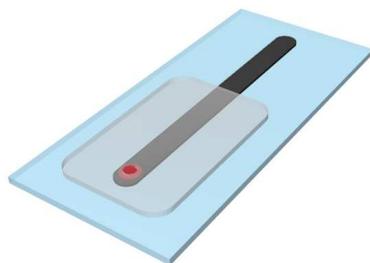


Fig. 1. SEM pictures of spray coated layers of CNTs on glass substrate and the schematic representation of spray coated ion-selective electrodes: substrate (blue), spray coated layer of carbon nanotubes (black), PVC layer – insulation of CNTs (grey), d) PVC ion-selective membrane (red) and picture of prepared electrode.

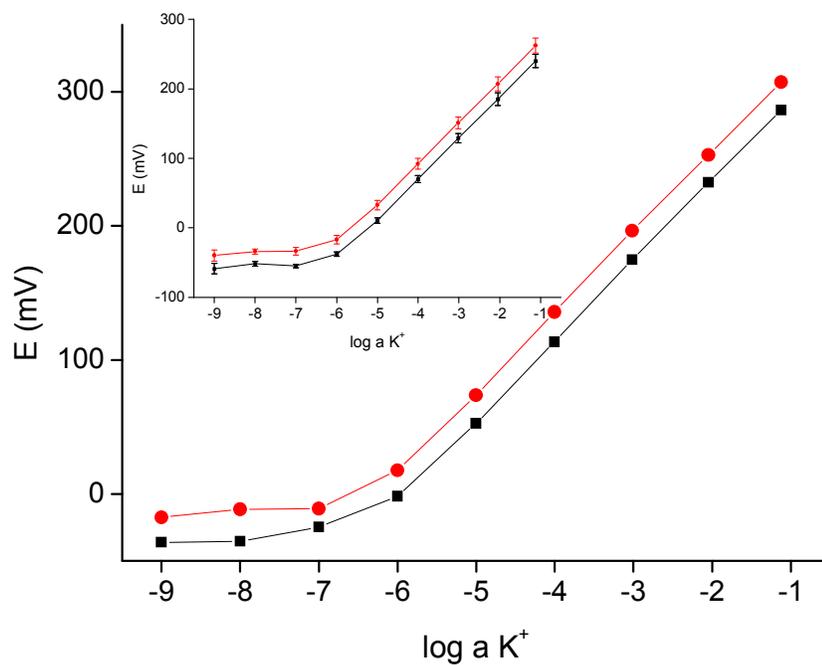


Fig. 2. Potentiometric responses of spray coated ion-selective electrodes prepared using: (■) PET or (●) Kapton substrate, recorded in KCl solutions. Inset: Mean potential values  $\pm$  SD recorded in course of 4 calibrations performed during one day for spray coated sensors using either: (■) PET or (●) Kapton, substrate.

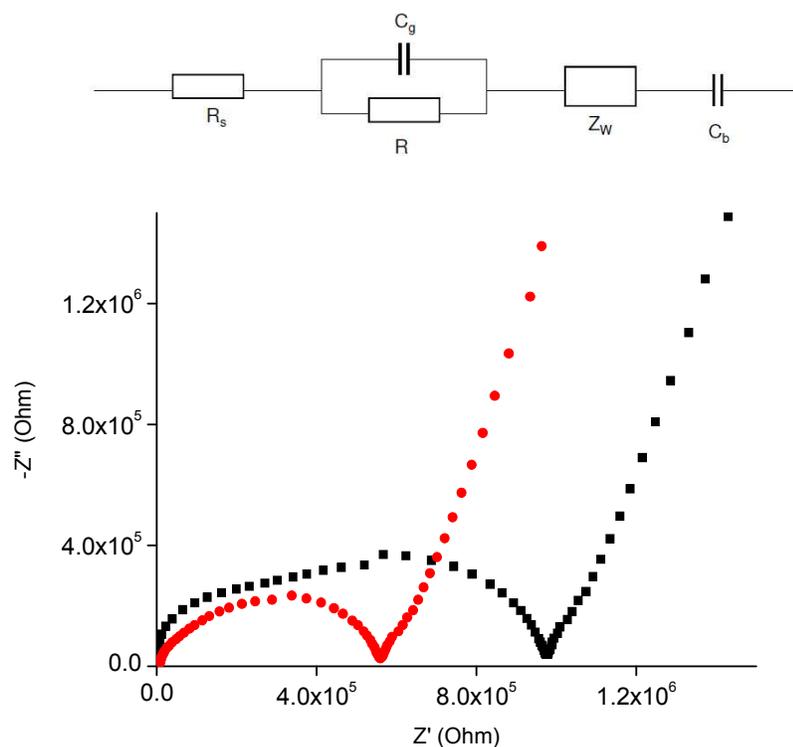
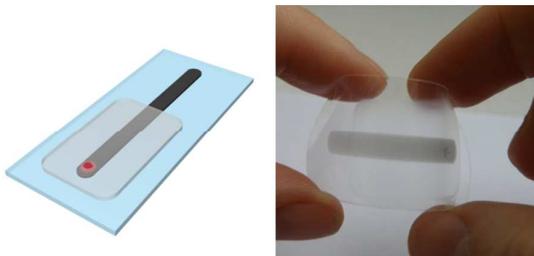


Fig. 3. Complex plane impedance plots of tested spray coated  $K^+$ - electrodes prepared using (■) PET or (●) Kapton, recorded in 0.1 M KCl solution, using 50 mV amplitude at 0.3 V potential, in the frequency range from 0.01 Hz to  $10^5$  Hz and equivalent circuit proposed for the Kapton support electrode.

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6 A novel fully spray coating based method of preparation of all-solid-state ion-selective  
7 electrodes of simplified construction is proposed.  
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