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# 1 Structure and Flow of Dense Suspensions of Protein Fractal Aggregates in

- 2 Comparison with Microgels.
- 3

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4

## 5 Abstract

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7 Solutions of the globular whey protein  $\beta$ -lactoglobulin ( $\beta$ -lg) were heated at different protein concentrations leading to the formation of polydisperse fractal aggregates with different 8 9 average sizes. The structure of the solutions was analyzed with light scattering as a function 10 of the protein concentration. The osmotic compressibility and the dynamic correlation length 11 decreased with increasing concentration and became independent of the aggregate size in 12 dense suspensions. Results obtained for different aggregate sizes could be superimposed after normalizing the concentration with the overlap concentration. Dense suspensions of fractal 13 14 protein aggregates are strongly interpenetrated and can be visualized as an ensemble of fractal 15 'blobs'. The viscosity of heated  $\beta$ -lg solutions increased extremely sharply above 80 g/L and diverged at 98 g/L, mainly due to the sharply increasing aggregate size. At fixed aggregate 16 size, the viscosity increased initially exponentially with increasing concentration and then 17 diverged. The increase was stronger when the aggregates were larger, but the dependence of 18 19 the viscosity on the aggregate size was weaker than that of the osmotic compressibility and 20 the dynamic correlation length. The concentration dependence of the viscosity of solutions of 21 fractal  $\beta$ -lg aggregates is much stronger than that of homogeneous  $\beta$ -lg microgels. The 22 behavior of fractal aggregates formed by whey protein isolate was similar.

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## 25 Introduction

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Globular proteins may be considered as dense nanoparticles that are stabilized in aqueous solutions by electrostatic repulsion. Heating aqueous protein solutions renders the rigid structure of the globular proteins mobile which may allows formation of bonds between

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30 the proteins and can cause irreversible aggregation. Aggregation leads to the formation of a percolating network above a critical gel concentration (Cg), but at lower concentrations stable 31 suspensions of finite size aggregates are obtained<sup>1-2</sup>. The size of the aggregates increases with 32 increasing protein concentration and diverges at Cg. The local structure of the aggregates and 33 the value of  $C_g$  depend on the type of protein, the pH and the added salt. However, for a 34 number of different globular proteins it has been shown that the large scale structure of the 35 aggregates is self-similar<sup>3-9</sup>. Self-similar aggregates are characterized by their fractal 36 dimension (d<sub>f</sub>) which relates the molar mass (M) to the radius (R):  $M \propto R^{df}$ . The value of d<sub>f</sub> 37 was found to increase weakly from 1.7 when electrostatic interaction are strong to 2.0 when 38 39 they are weak, but it does not depend on the type of protein.

40 Fractal protein aggregates have been studied extensively in dilute solutions, but as far 41 as we are aware no systematic investigation has been done on the flow properties of dense 42 suspensions of such aggregates. More in general, while dense suspensions of homogeneous spherical particles have been investigated in much detail <sup>10-13</sup>, dense suspensions of fractal 43 aggregates have received relatively little attention <sup>14-17</sup>. An important difference between 44 45 homogeneous particles and fractal aggregates is that the density of the former does not depend on their size, but for the latter it decreases with increasing size. Considering that the 46 aggregates are spherical we may define their density as  $\rho=3M/(4\pi N_a R^3)$ , with N<sub>a</sub> Avogadro's 47 number so that  $\rho \propto R^{df-3}$ . It has therefore been suggested that the viscosity of dense fractal 48 49 aggregates can be understood in the same way as for homogeneous particles, by treating them 50 as particles with a lower density. However, since fractal aggregates have an open structure, they are to certain extent interpenetrable. This is especially important for fractal globular 51 52 protein aggregates, which are very polydisperse, and are strongly interpenetrated in dense suspensions. In addition, it has been shown that fractal protein aggregates have some degree 53 of flexibility <sup>18</sup>. Recently, it was demonstrated that interpenetration and flexibility of the 54 fractal aggregates has important effects on the viscosity in dense suspensions<sup>19</sup>. 55

Here we present an investigation of the structure and the viscosity as a function of concentration for aqueous suspensions of fractal globular protein aggregates with different sizes. We will compare the viscosity of fractal aggregates with that of microgels formed by the same proteins <sup>20</sup>, which enables a direct assessment of the effect of the structure of protein particles. The globular protein used in this investigation was  $\beta$ -lactoglobulin ( $\beta$ -lg), which is the main component of whey. Stable suspensions of aggregates with different average sizes were formed by heating aqueous  $\beta$ -lg solutions at different protein concentrations at pH 7.0

until steady state was reached. It has already been reported elsewhere that at these conditions β-lg forms initially small curved strands with a hydrodynamic radius  $R_h \approx 15$ nm. At higher protein concentrations these strands randomly associate into self similar aggregates with d<sub>f</sub>=1.7. In order to render our findings more relevant for applications we have compared the results obtained for aggregates formed by pure β-lg with those formed by a commercial whey protein isolate.

- 69
- 70 Materials and methods
- 71
- 72 Materials
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74 The  $\beta$ -lactoglobulin (Biopure, lot JE 001-8-415) used in this study was purchased from 75 Davisco Foods International, Inc. (Le Sueur, MN, USA) and consisted of approximately equal 76 quantities of variants A and B. Whey protein isolate (WPI) powder was purchased from Lactalis (Laval, France), which contained 95% protein on dry weight basis of which 70%  $\beta$ -lg 77 and 20%  $\alpha$ -lactalbumin. The molar masses of  $\beta$ -lactoglobulin and  $\alpha$ -lactalbumin are 18 78 kg/mol and 14 kg/mol, respectively<sup>21</sup>. The powders were dissolved in Milli-Q water to which 79  $200 \text{ ppm NaN}_3$  was added to prevent bacterial growth. The pH of the solution was adjusted to 80 7 by adding small amounts of NaOH 0.1 M. For light scattering; dilute solutions were filtered 81 through 0.2 µm pore size Anotop filters. The protein concentration was determined by UV 82 absorption at 278 nm using extinction coefficient 0.96 Lg<sup>-1</sup>cm<sup>-1</sup> and 1.05 Lg<sup>-1</sup>cm<sup>-1</sup> for  $\beta$ -lg and 83 WPI, respectively. Protein solutions were concentrated by ultrafiltration utilizing the KrosFlo 84 85 Research II/i/Tangential Flow Filtration (TFF) System (Spectrum Europa B.V.)

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## 87 Light scattering

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Light scattering measurements were done using an ALV-5000 multibit, multitau, full digital correlator in combination with a laser emitting vertically polarized light at  $\lambda = 632$  nm (ALV-Langen). The temperature was controlled by a thermo-stat bath to within  $\pm 0.1$  °C. The relative excess scattering intensity (I<sub>r</sub>) was determined as the total intensity minus the solvent scattering divided by the scattering of toluene at 20°C. I<sub>r</sub> is related to the osmotic compressibility (( $d\pi/dC$ )<sup>-1</sup>) and the z-average structure factor (S(q))<sup>22-23</sup>:

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$$I_r = K.C.RT.(d\pi/dC)^{-1}S(q)$$

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with R the gas constant and T the absolute temperature and q the scattering wave vector.

100 
$$K = \frac{4\pi^2 n^2}{\lambda^4 N_a} \cdot \left(\frac{dn}{dC}\right)^2 \cdot \left(\frac{n_s}{n}\right)^2 \cdot \frac{1}{R_s}$$
 2

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where (dn/dC) is the refractive index increment, and R<sub>s</sub> is the Rayleigh ratio of toluene. 102  $(n_{e}/n)^{2}$  corrects for the difference in scattering volume of the solution with refractive index n 103 and toluene with refractive index ns. S(q) describes the dependence of Ir on the scattering 104 wave vector:  $q=(4\pi n/\lambda).sin(\theta/2)$ , with  $\theta$  the angle of observation. We used dn/dC=0.189105 cm<sup>3</sup>/g and R<sub>s</sub>=  $1.35 \times 10^{-5}$  cm<sup>-1</sup>. In dilute solutions and in the limit of q $\rightarrow$ 0, I<sub>r</sub>/KC is equal to the 106 weight average molar mass (M<sub>w</sub>). At finite concentrations we measure an apparent molar 107 mass (M<sub>a</sub>) that is proportional to the osmotic compressibility:  $M_a=RT/(d\pi/dC)$ . The initial 108 concentration dependence of M<sub>a</sub> can be expressed in terms of a virial expansion: 109

110

111 
$$M_a = M_w / (1 + 2A_2 M_w C + ...)$$
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113 The initial q-dependence of the structure factor extrapolated to  $C \rightarrow 0$  can be used to obtain the 114 z-average radius of gyration (R<sub>g</sub>):

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116 
$$S(q)=(1+q^2.R_g^2/3)^{-1}$$
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118 At higher concentrations, when interactions cannot be neglected, the initial q-dependence of 119 structure factor can be expressed in terms of the static correlation length ( $\xi_s$ ):

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121 
$$S(q)=(1+q^2.\xi_s^2)^{-1}$$
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The normalized intensity autocorrelation  $(g_2(t))$  that is measured with dynamic light scattering (DLS) is related to the normalized electric field correlation function,  $g_1(t)$ :  $g_2(t)=1+g_1(t)^{2}$ ,  $g_1(t)$  was analyzed in terms of a distribution of relaxation times using the REPES routine <sup>25</sup>:

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$$g_1(t) = \int A(\log \tau) \exp(-t/\tau) d\log \tau$$

129

In all cases monomodal distributions were observed and the correlograms could be welldescribed using the following an analytical expression for A(logτ):

132

A(log 
$$\tau$$
) =  $k\tau^{p} \exp\left[-\left(\tau / \tau^{*}\right)^{s}\right]$  6

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In binary solutions the relaxation of the intensity fluctuations is caused by cooperative diffusion of the solute and cooperative diffusion coefficient can be calculated from the average relaxation rate:  $D_c = (q^2.\tau)^{-1}$ . The dynamic correlation length ( $\xi_d$ ) can be calculated from  $D_c$  at  $q \rightarrow 0$ :

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$$140 \qquad D_c = \frac{kT}{6\pi\eta\xi_d}$$

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with  $\eta$  the viscosity, k Boltzman's constant, and T the absolute temperature. When interactions can be neglected, i.e. at low concentrations,  $\xi_d$  is equal to the z-average hydrodynamic radius. We note that the z-average values of  $R_h$  and  $R_g$  determined by light scattering give strong weight to the larger particles in the distribution and even more so for  $R_g$ than for  $R_h$ .

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#### 148 Rheology

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The viscosity was measured as a function of the shear rate using a rheometer 150 (AR2000, TA Instruments) with a cone and plate or a couette geometry. After loading the 151 samples were pre-sheared at 100 s<sup>-1</sup> during 1 min. The viscosity was determined during 152 subsequent shear ramps with increasing and decreasing shear rates. The results obtained with 153 154 increase and decreasing shear rates were found to be the same. Measurements done using the cone and plate geometry showed an upturn at low shear rates, which was due to the formation 155 of a weak elastic surface layer of proteins. In ref.<sup>26</sup> it was shown that this effect can be much 156 reduced by using a couette geometry. Therefore for one series of samples we have used both 157 geometries and found that indeed the artificial increase was no longer observed. Nevertheless, 158 159 the same results can be obtained with both geometries after superposition of the data at

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different concentrations, see Supplementary Information. As a much larger quantity of
solution is needed for the couette geometry, we have used for the other series of
measurements the cone and plate geometry.

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164 **Results** 

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## 166 Characterization of the aggregates.

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168 Fractal aggregates of  $\beta$ -lg with different sizes were prepared by heating at 80°C aqueous solutions with different protein concentrations at pH 7.0 until steady state was 169 170 reached. At steady state all proteins are denatured and for C>40g/L more than 90% of the proteins form aggregates<sup>18</sup>. The remaining proteins are present in the form of monomers, 171 172 dimers and trimers. As was mentioned in the Introduction, detailed investigations of the fractal structure of aggregates formed by heating  $\beta$ -lg or WPI in aqueous solution have 173 already been reported elsewhere<sup>3-4, 18</sup>. Characterization of the aggregates used for the present 174 175 investigation by light scattering showed that their structure was same as that reported in the literature. 176

177 The weight average molar mass  $(M_w)$  of the aggregates was determined using light scattering as described in the Material and Methods section. The dependence of  $M_w$  on the 178 179 concentration at which the aggregates were formed is shown in figure 1a. At low 180 concentrations relatively monodisperse strands were formed, but for C>40g/L, random 181 aggregation of these strands led to an increase of M<sub>w</sub> with increasing concentration. The molar mass diverged at a critical gel concentration Cg=98g/L. The z-average radius of 182 gyration  $(R_g)$  and the z-average hydrodynamic radius  $(R_h)$  increased with increasing  $M_w$ 183 following a power law, which is expected for fractal aggregates, see figure 1b. The 184 dependence of both R<sub>h</sub> and R<sub>g</sub> on M<sub>w</sub> is compatible with d<sub>f</sub>=1.7, but R<sub>h</sub> is systematically 185 smaller than R<sub>g</sub> by a factor of about 0.7, in agreement with findings reported earlier <sup>18</sup>. The 186 principal reason for this difference is the polydispersity of the aggregates, R<sub>g</sub> is derived from 187 the z-average of  $R_g^2$  and  $R_h$  from the z-average of  $R_h^{-1}$ . Therefore  $R_g$  is more sensitive to 188 larger aggregates. 189





Fig. 1a Molar mass of  $\beta$ -lg aggregates formed in heated aqueous solutions as a function of 192 193 the protein concentration.

Fig. 1b Dependence of the molar mass of  $\beta$ -lg aggregates on the radius of gyration (circles) 194 195 or the hydrodynamic radius (triangles).

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#### Structure of the aggregate solutions 197

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199 All solutions of fractal aggregates were optically clear and their structure was studied with light scattering over a range of concentrations. Fig. 2 shows Ir/KC for large aggregates 200 201 that were formed by heating at C=96 g/L and that were subsequently progressively diluted. At high protein concentrations the structure factor was independent of q in the range covered by 202 203 light scattering, implying that the correlation length of the concentrated solutions was less

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than 15nm. It was shown elsewhere<sup>27</sup> using small angle X-ray scattering experiments that the structure factor of concentrated aggregate solutions shows a peak implying a certain degree of order in the distribution of the proteins. The osmotic compressibility and the correlation length of the concentration fluctuations increased with decreasing concentration causing an increase of  $I_r/KC$  and a stronger q-dependence.

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Fig. 2 Dependence of  $I_r/KC$  on q for aggregates formed by heating at C=96 g/L and subsequently diluted to different concentrations as indicated in the figure.

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Fig. 3a shows the concentration dependence of the apparent molar mass ( $M_a = I_r/KC_{(q\to 0)}$ ) for protein aggregates with different sizes obtained by heating at different concentrations. As was mentioned above,  $M_a$  is proportional to the osmotic compressibility and is equal to  $M_w$  if interactions are negligible, i.e. at low concentrations. In all cases the osmotic compressibility decreased with increasing concentration, due to electrostatic and excluded volume interactions between the aggregates and at the highest concentrations  $M_a$  became independent of the aggregate size. The latter implies that in dense suspensions the

- aggregates are strongly interpenetrated and that the osmotic compressibility is determined by
- 222 interaction between the elementary units of the aggregates.



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Fig. 3a Concentration dependence of  $M_a$  for aggregates formed by heating at different protein concentrations indicated in the figure. The same data are plotted in fig. 3b after normalizing  $M_a$  with  $M_w$  and C with C\*. The solid line in fig. 3b represents eq.8.

229

230 For non-interacting hard spheres,  $M_a/M_w$  can be well described by the following 231 equation<sup>28</sup>:

$$\frac{M_a}{M_w} = \frac{(1-\phi)^4}{1+4\phi+4\phi^2-4\phi^3+\phi^4}$$

234

where  $\phi$  is the volume fraction of the particles. For solutions of polydisperse soft particles 235 236 such as the protein aggregates, the initial concentration dependence of M<sub>a</sub>/M<sub>w</sub> can still be described by eq.8 if for  $\phi$  we use an effective volume fraction:  $\phi_e = C/C^*$ , where C\* is the 237 concentration at which the effective volume fraction of the particles is unity and is related to 238 the second virial coefficient:  $C^*=A_2/(4M_w)$ . When expressed in units of volume the second 239 240 virial coefficient is 4 times the effective volume of the particles. Fig. 3b shows that eq.8 describes the results in this representation up to C/C\*≈0.2. At higher protein concentrations, 241 M<sub>a</sub> decreased less steeply than for equivalent hard spheres, because the aggregates are 242 polydisperse and can interpenetrate. As expected, the values of C\* decreased with increasing 243 244 aggregate size, see fig. 4.

For spherical particles C\* can also be calculated from their molar mass and their radius:

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$$C^{*}=3M_{w}/(4\pi R^{3}N_{a}).$$
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For monodisperse non-interacting hard spheres the two methods give the same value, but for polydisperse or interacting particles they will be different. For the polydisperse protein aggregates studied here, the values calculated using eq. 9 are smaller if one uses  $R_g$  for the radius than if one uses  $R_h$ , see fig. 4. The values of C\* obtained from the comparison of the concentration dependence of  $M_a$  with eq. 8 were intermediate between those calculated using eq. 9 with R=R<sub>h</sub> or R=R<sub>g</sub>. However, the molar mass dependence was weaker, which is a consequence of the increasing polydispersity with increasing M<sub>w</sub>.



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Fig. 4. Dependence of C\* on the molar mass for fractal  $\beta$ -lg aggregates. The data obtained from fits of the initial concentration dependence of  $M_a$  to eq. 8 are indicated by squares, whereas the circles and the triangles indicate the values calculated using eq. 9 with  $R_h$  and  $R_g$ , respectively. The dashed lines indicate the power law dependence corresponding to the one shown in fig. 1b.

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264 As can be seen in fig.2, interpenetration of the aggregates caused a decrease of the 265 correlation length with increasing concentration. At higher concentrations, the static 266 correlation length became too small to be determined with light scattering, but the dynamic 267 correlation length ( $\xi_d$ ) obtained from dynamic light scattering could be determined over the whole concentration range. Examples of correlograms and the corresponding relaxation time 268 269 distributions are shown in fig. S3 of the supplementary information. As was discussed in ref. 270 <sup>18</sup>, in dilute solutions the q-dependence of the diffusion coefficient increases with increasing 271 aggregate size, because the fractal aggregates are semi-flexible. With increasing concentration the q-dependence of D<sub>c</sub> decreased, because the correlation length of the concentration 272 273 fluctuations decreased, see fig.S4 of the supplementary information.  $\xi_d$  obtained from the 274 cooperative diffusion coefficient extrapolated to zero-q, see eq.7, decreased with increasing 275 concentration down to values approaching the radius of monomeric  $\beta$ -lg that is about 2nm. Fig. 5 shows that  $\xi_d$  has the same power law dependence on  $M_a$  as  $R_h$  on  $M_w$  independent of 276 the aggregate size. The structure of the interpenetrated aggregate solution can thus be 277 278 visualized as an ensemble of fractal 'blobs' with radius  $\xi_d$  and molar mass  $M_a$ , independent

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of the aggregate size. The peak in the structure factor at larger q-values that was found with

280 SAXS <sup>27</sup> implies that the 'blobs' are regularly distributed in salt free solutions.



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Fig. 5 Dependence of the apparent molar mass on the dynamic correlation length for solutions of aggregates with different sizes measured at different protein concentrations. The filled symbols represent values at infinite dilutions where  $M_a=M_w$  and  $\xi_d=R_h$ . The solid line has slope 1.7. The symbols are as in fig.3a.

286

287 Viscosity

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Solutions of  $\beta$ -lg at different concentrations were loaded on the rheometer after 289 heating and the viscosity (n) was determined as a function of the shear rate ( $\dot{\gamma}$ ). For the more 290 viscous solutions we observed shear thinning at larger shear rates, see fig.6a. We also 291 292 observed an increase of the viscosity with decreasing shear rate at low shear rates. However, 293 as was mentioned in the materials and methods section, this increase is an artifact caused by 294 the formation of a layer of proteins at the interface. If we ignore the artificial increase at low shear rates, the results obtained at different concentrations can be superimposed by horizontal 295 and vertical shift factors, see fig. 6b. This allowed us to obtain the limiting low shear viscosity 296  $(\eta_0)$  at all concentrations. 297





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303 Fig. 6a Shear rate dependence of the viscosity of heated  $\beta$ -lg solutions at different 304 concentrations. Fig. 6b shows a master curve of the same data obtained by horizontal and 305 vertical shifts with respect to the data at C=96 g/L. The artificial upturns at low shear rates 306 were removed from the master curve.

 $\eta_0$  increased very sharply with increasing protein concentration for C>70g/L and diverged at the gel concentration, see fig. 7a. The sharp increase of  $\eta_0$  was caused by a combination of increasing protein concentration and increasing aggregate size. In order to distinguish these two effects, we measured the shear rate dependent viscosity as a function of the protein concentration keeping the aggregate size fixed. To this end, a solution of aggregates formed at C=96g/L with Rg=320 nm was progressively diluted. Master curves could be obtained by superposition of the results obtained at different dilutions, see supplementary results. The concentration dependence of  $\eta_0$  for the aggregates with fixed size formed at C=96g/L and subsequently diluted is compared in fig. 7a with that of aggregates with different sizes formed at different concentrations. Even though the concentration dependence of  $\eta_0$  for solutions with the same large aggregates was steep, it was much more progressive than that of aggregates formed at different concentrations. This clearly demonstrates that the effect of increasing the aggregate size is more important than the effect of increasing the protein concentration. Similar results were obtained with a commercial WPI sample, see fig. 7b, which is not surprising, because WPI forms similar fractal aggregates in heated aqueous solutions<sup>4</sup>. The WPI solutions gelled at a slightly lower protein concentration (95g/L) and therefore the steep increase of the viscosity occurred at slightly lower concentrations. In the following we focus on the results obtained with pure  $\beta$ -lg.



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Fig.7a Zero shear rate of the viscosity for  $\beta$ -lg solutions that were heated at different concentrations (open symbols) or that were heated at C=96 g/L and subsequently diluted (closed symbols). Fig. 7b shows the results obtained for WPI heated at different concentrations (open symbols) or that were heated at C=93 g/L and subsequently diluted (closed symbols).

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In order to investigate the effect of the average aggregate size on the concentration 336 dependence of  $\eta_0$ , solutions with different  $\beta$ -lg concentrations were heated. The viscosity of 337 each system was subsequently measured as a function of the protein concentration by dilution. 338 339 The smaller aggregates obtained by heating at C=40 g/L and C=70 g/L were first concentrated 340 by ultrafiltration. Fig. 8a shows that in each case  $\eta_0$  increased exponentially up to approximately 0.03 Pa.s:  $\eta_0 = \eta_s \exp(C/C_c)$ , with  $\eta_s$  the solvent viscosity. The exponential 341 increase obtained for the different aggregates superimposed when  $\eta_0$  was plotted as a function 342 of C/C<sub>c</sub>, see fig. 8b. C<sub>c</sub> decreased weakly with increasing aggregate size from  $C_c=35$  g/L for 343  $M_w$ =1.5x10<sup>6</sup> g/mol to C<sub>c</sub>=16.5 g/L for  $M_w$ =1.1x10<sup>8</sup> g/mol, see inset of fig. 8b. 344

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Fig. 8a Concentration dependence of  $\eta_0$  for solutions of  $\beta$ -lg aggregates with different molar masses indicated in the figure.

Fig. 8b Master curve of the results shown in fig. 8a obtained by dividing C with  $C_c$ . The solid line represents  $\eta_0 = \eta_s \exp(C/C_c)$ . The dependence of  $C_c$  on  $M_w$  is shown in the inset, which also includes results obtained for 2 other aggregate sizes for which the concentration dependence was not shown for clarity.

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At higher protein concentrations,  $\eta_0$  increased more steeply until it diverged and a gel was formed. We also observed that at these higher concentrations the viscosity increased slowly with time and in some cases weak gels were formed with time. It appears that bonds formed slowly between aggregates in these dense protein aggregate suspensions causing a rise

in the viscosity or gelation. This phenomenon of so-called cold gelation is well known to occur when electrostatic repulsion is reduced by adding salt or reducing the pH<sup>1</sup>. The rate of gelation increased with increasing aggregate concentration, but for all systems studied here the effects on the viscosity was negligible during the first two days. Notice, however, that the scattering intensity and  $\xi_d$  were stable even if gels were formed, implying that formation of the bonds occurred without a significant change in the structure of the solutions.

364 We have compared the behavior of large fractal aggregates with that of homogeneous microgels. As was discussed in ref.<sup>29</sup>, microgels can be formed by heating  $\beta$ -lg solutions in 365 the presence of a small amount of CaCl<sub>2</sub>. For the present investigation the microgels were 366 367 formed by heating a  $\beta$ -lg solution at C=40 g/L in the presence of 4.5mM CaCl<sub>2</sub>. With light scattering techniques the following characteristics were obtained:  $M_w=1.1 \times 10^9$  g/mol,  $R_h=160$ 368 369 nm, Rg=200 nm. The structure of concentrated microgel suspensions could not be studied using light scattering, because they were highly turbid. In fig.9 the concentration dependence 370 371 of  $\eta_0$  of microgels is compared to that of the fractal aggregates. The viscosity of the fractal aggregate solutions increased more steeply with increasing protein concentration than for the 372 373 microgel solutions, which was expected because the density of the latter is higher. However, 374 the concentration dependence of the viscosity of the microgel solutions is still much larger 375 than that of native proteins.





Fig. 9 Dependence of the zero shear viscosity on the concentration (a) or the volume fraction (b) of solutions of fractal aggregates (open symbols) and microgels (filled symbols). For comparison the concentration dependence of the viscosity of native  $\beta$ -lg is shown in fig. 9a (filled squares). Note that in fig. 9b the horizontal axis is logarithmic. The solid lines in fig. 9b represent exponential increases of  $\eta_0$  with  $\phi$ . Different open symbols represent different molar masses as indicated in fig 8. The inset of fig. 9b shows the molar mass dependence of  $\phi_c$ .

Alternatively, we may compare the viscosity as a function of the effective volume 385 fraction calculated as  $\phi_e = C/C^*$ . In fig. 9b,  $\eta_0$  is plotted as a function of  $\phi_e$  with C\* calculated 386 using in eq. 9 the hydrodynamic radius. The values of C\* calculated in this way are shown in 387 fig. 4 for the fractal aggregates and for the microgels  $C^{*}=110$  g/L. In this representation, the 388 389 viscosity of the microgel suspensions increased more steeply than for fractal aggregates with  $M_w=1.1\times10^8$  g/mol and  $M_w=2.2\times10^7$  g/mol, but less steeply than for the smaller aggregates.  $\eta_0$ 390 diverged at  $\phi_c = C_c/C^* \approx 2$  for the microgels and  $\phi_c \approx 20$ , 3, 0.9 and 0.7 for the fractal aggregates 391 with  $M_w = 1.1 \times 10^8$ ,  $2.2 \times 10^7$ ,  $2.5 \times 10^6$  and  $1.5 \times 10^6$  g/mol, respectively, see inset of fig. 9b. 392 Except for the smallest aggregates,  $\phi_c$  is larger than that of monodisperse hard spheres for 393 394 which the viscosity diverges close to random close packing ( $\phi_c=0.63$ ).

In part this can be explained by the polydispersity of the aggregates, which is large because they were formed by a random reaction limited aggregation process <sup>3</sup>. As was mentioned above, the values of  $R_g$  and  $R_h$  obtained from light scattering are strongly weighted by the largest aggregates so that the calculated value of C\* is too small and therefore  $\phi_e$  is too

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large. The overestimation of  $\varphi_e$  would have been even worse if  $R_g$  or  $A_2$  had been used to calculate C\*. The polydispersity of the fractal aggregates increases with increasing average size, which means that  $\phi_e$  is increasingly overestimated. In fact, as was mentioned in the introduction, the smallest aggregates are not fractal, but relatively monodisperse curved strands and are the building blocks of the larger fractal aggregates. The microgels are much less polydisperse than the larger fractal aggregates so that the overestimation  $\varphi_e$  is less A second reason for the large values of  $\phi_e$  is that the protein particles are soft so that

407 they can be compressed to some extent. Much more importantly, polydisperse fractal aggregates interpenetrate in dense suspensions and the smaller aggregates are embedded 408 within the larger ones. This effect is more important for larger fractal aggregates. As a 409 410 consequence, the increase of the viscosity at a given concentration by using fractal aggregates 411 instead of microgels or by using larger instead of smaller fractal aggregates is much less important than might have been anticipated from the difference in C\* calculated from Mw and 412  $R_h$  or  $R_g$ . 413

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- 415 Discussion
- 416

417 We have compared the behavior of dense suspensions of two types of protein aggregates. In pure water relatively monodisperse protein strands were formed for C < 50g/L, 418 419 which were the elementary units of the larger fractal aggregates formed at higher 420 concentrations. Aggregation of the strands was reaction controlled and led to increasing 421 polydispersity with increasing aggregate size. Solutions of the fractal aggregates were 422 transparent, because smaller aggregates were embedded in the larger aggregates in a 423 hierarchical manner. In addition, electrostatic repulsion between the proteins induced a weak 424 local order. Interpenetration of the fractal aggregates explains why the structure of dense 425 suspensions was independent of the aggregate size. The osmotic compressibility and the 426 correlation length of dense suspensions were determined by the interactions between the elementary units of the fractal aggregates, i.e. small protein strands. 427

428 Spherical microgels of globular proteins were formed by addition of a small amount of CaCl<sub>2</sub> before heating. They probably consist of densely cross-linked network of small strands 429 <sup>20, 30</sup>. The molar mass of microgels is much larger than that of fractal aggregates of the same 430 431 size and therefore they scatter much more light. In addition, they are much less polydisperse

and smaller microgels cannot penetrate larger ones. As a consequence, microgel suspensions
were turbid at higher concentrations and the structure of dense suspensions could not be
evaluated by light scattering techniques.

435 The viscosity of colloidal particles as a function of their concentration has been extensively studied in the past and the effects of their architecture and the interaction between 436 the particles have been reviewed <sup>10-13, 31</sup>. The viscosity diverges at a critical volume fraction 437 and the dependence on  $\varphi$  has often been described by the Krieger-Dougherty equation  $^{32}$  or 438 the Quemada model <sup>33</sup>:  $\eta_0 = \eta_s (1 - \phi/\phi_c)^{-2}$ . For monodisperse hard spheres  $\phi_c$  is the 439 concentration of close-packing, but in order to account for the effects of polydispersity, 440 441 interaction or softness of the colloids  $\phi_c$  has often been considered as an adjustable parameter. 442 The same equation has been used to describe the concentration dependence for rigid clusters of randomly aggregated colloids <sup>14-17</sup>. The critical volume fraction of the colloids was found 443 to decrease with increasing size of the fractal aggregates, because the density of the fractal 444 445 aggregates decreased.

Here we find that the concentration dependence of the viscosity of the protein 446 aggregates is much better described by an exponential increase except close to  $\phi_c$ . An 447 exponential increase of the viscosity was also reported for dendrimers <sup>34</sup>, polymeric micelles 448 <sup>35</sup> and randomly aggregated star polymers<sup>19</sup>. The latter study is particularly relevant here, 449 450 because it is the only investigation of the viscosity of interpenetrated randomly aggregated 451 particles with flexible bonds. Similarly to the fractal protein aggregates, the osmotic 452 compressibility of fractal aggregates of star polymers could be described by eq.8 up to  $\varphi \approx 0.4$ 453 and decreased more slowly at higher concentrations. Also for this system, the osmotic 454 compressibility at high concentrations was found to be independent of the size of the 455 aggregates and was determined by the interaction between the elementary units of the aggregates, i.e. the star polymers. The behavior of flexible fractal aggregates is very different 456 457 from that of the rigid clusters, mainly because they can interpenetrate, but also because they 458 are soft. This means that the viscosity of such systems cannot be interpreted in terms of the 459 cumulated volume fraction of the aggregates.

If size of the aggregates is increased at a fixed concentration, the effect on the viscosity will be different for fractal aggregates and microgels. For fractal aggregates the viscosity will increase with increasing aggregate size, because the density of the aggregates decreases. However, if larger microgels are formed at a fixed concentration the viscosity

remains the same, assuming that the polydispersity and softness of the microgels does not depend on their size, because the volume fraction remains the same. If the size of the aggregates increases with increasing concentration as was the case for the fractal aggregates formed at different concentrations, the viscosity increases very steeply due to the combined effects of increasing size and increasing concentration. Comparison of the two situations for globular protein aggregates showed that former effect was most important.

470

#### 471 Conclusion

472

Fractal aggregates are formed by heating globular proteins in aqueous solutions at pH 473 474 7. The average aggregate size increases if the concentration at which the proteins are heated 475 is increased and diverges at the critical gel concentration. For a given aggregate size the 476 viscosity increases exponentially with the protein concentration. The increase is steeper if the 477 aggregates are larger, because the density of the aggregates decreases with increasing size. 478 However, the effect of the aggregate size is smaller than expected from the decrease of the 479 density, because the aggregates are very polydisperse and smaller aggregates are embedded 480 within the larger ones. The viscosity of protein solutions after heating at different concentrations rises very sharply over a small concentration range close to the critical gel 481 482 concentration, because the average size of the aggregates rises sharply. The osmotic compressibility and the correlation length of the concentration fluctuations decrease with 483 484 increasing concentration and are independent of the aggregate size at high concentrations, 485 where they are determined by the interaction between the elementary units of the aggregates. 486 The behaviour of aggregates formed by WPI is close to that for  $\beta$ -lg aggregates.

The behavior of microgels formed by heating globular proteins in the presence of a small amount of  $CaCl_2$  is different from that of fractal aggregates, because they are denser and cannot interpenetrate. Therefore the increase of the viscosity of microgel solutions with increasing protein concentration is weaker and does not depend on the size of the microgels.

491

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495 **References** 

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# For TOC only



Zero-shear viscosity as a function of the protein concentration for fractal aggregates and microgels.