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## Review

# Overcoming inactivation of the lung surfactant by serum proteins: a potential role for fluorocarbons?

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In many pulmonary conditions serum proteins interfere with the normal adsorption of components of the lung surfactant to the surface of the alveoli, resulting in lung surfactant inactivation, with potentially serious untoward consequences. Here, we review the strategies that have recently been designed in order to counteract the biophysical mechanisms of inactivation of the surfactant. One approach includes protein analogues or peptides that mimic the native proteins responsible for innate resistance to inactivation. Another perspective uses water-soluble additives, such as electrolytes and hydrophilic polymers that are prone to enhance adsorption of phospholipids. An alternative, more recent approach consists of using fluorocarbons, that is, highly hydrophobic inert compounds that were investigated for partial liquid ventilation, that modify interfacial properties and can act as carriers of exogenous lung surfactant. The latter approach that allows fluidisation of phospholipid monolayers while maintaining capacity to reach near-zero surface tension definitely warrants further investigation.

## 1. Introduction

The native lung surfactant is a complex mixture comprising about 90% of lipids (mainly dipalmitoylphosphatidylcholine, DPPC) and about 10% of specific proteins (SP-A, SP-B, SP-C and SP-D) that forms a monolayer at the surface of the alveoli in mammals. This monolayer lowers the tension at the alveolus-air interface upon compression during expiration, thus reducing the work of breathing, and respreads quickly on expansion during inspiration. As the lung is ceaselessly submitted to compression/expansion cycles (~15–20 cycles per minute) and undergoes a typical total volume variation of ~20%, one easily understands that the viscoelastic properties of the monolayer of pulmonary surfactant is a critical determinant of the lung's functionality.

There are many pulmonary diseases in which the lung surfactant is either absent or inactivated. The surfactant deficiency that results from lung immaturity in preterm babies leads to the neonatal respiratory distress syndrome (NRDS). In NRDS, the lack of surfactant results in progressive lung failure characterised by alveoli collapse (atelectasis), decreased lung compliance, systemic hypoxia and lung oedema. In new-borns, surfactant inactivation can be due to meconium inhalation immediately before or during delivery, as in the meconium aspiration syndrome (MAS). In children and adults, surfactant inactivation often occurs as a consequence of acute lung injury (ALI) and is a primary cause of acute respiratory distress syndrome (ARDS). ALI/ARDS may result from both direct lung injury (pneumonia, aspiration, drowning or toxic inhalation) and

indirect lung injury (sepsis, nonthoracic trauma, multiple blood transfusions, major surgery, acute pancreatitis or shock).<sup>1–3</sup>

Three sequential pathological phases are commonly encountered:<sup>4</sup> a first acute exudative phase is characterized by the influx of protein-rich oedema fluid into the air spaces as a consequence of increased permeability of the alveolar–capillary barrier; a second phase consists of proliferation of type II cells and accumulation of fibroblasts associated with collagen deposition in the extracellular matrix. This phase may result in a third fibrotic phase that leads to obliteration of alveolar spaces by deposition of extracellular matrix proteins. Although ARDS has a more complicated pathology than the simple deficiency of surfactant, it has similar symptoms than NRDS, including reduced lung compliance, restriction of lung volume and refractory hypoxemia, necessitating mechanical ventilation. ALI is diagnosed by  $\text{PaO}_2/\text{FiO}_2 \leq 300$  mmHg) and ARDS by  $\text{PaO}_2/\text{FiO}_2$  ratio  $\leq 200$  mmHg.<sup>5</sup>

The occurrence of NRDS is nowadays low in developed countries (current neonatal mortality rate is ~4 per 1000 live births in the US).<sup>6</sup> This is due to the fact that, since 1990, NRDS can be prevented or efficiently reverted by surfactant therapy (administration of exogenous surfactant), along possibly with other major innovations, such as antenatal corticosteroids and advanced care technologies (high-frequency oscillations).<sup>6</sup> Neonatal mortality contributes however to up ~40% to the mortality rate for children younger than 5 years worldwide. Several lung surfactant substitutes consisting of purified and complemented lung extracts from porcine

or bovine tissues (*e.g.* Curosurf, Surfacta, Alveofact and BLES) have proven effective in NRDS treatment.<sup>7,8</sup>

Where ALI/ARDS is concerned, the situation is different. Over a period of 25 years, the annual incidence of ALI/ARDS is predicted to be 335 000, with 147 000 deaths per year.<sup>9</sup> Although surfactant therapy has demonstrated some improvements in gas exchange and survival in animal ARDS models, its efficacy in human clinical trials is limited and mortality remains high.<sup>3, 10, 11</sup> It has been recognised that surfactant inactivation is a major factor in ARDS and also that the lack of clinical inefficacy of the exogenous surfactant preparations results from such inactivation. The inhibitors responsible for inactivation of both native and exogenous lung surfactants include serum proteins (albumin, fibrinogen monomer, fibrinogen, immunoglobulin, C-reactive protein), red blood cell components (haemoglobin), pro-inflammatory cytokines (IL-1, TNF), lipopolysaccharides (LPS), and certain lipids such as cholesterol (a major component of meconium), fatty acids, bile salts and lysophosphatidylcholine. The surfactant components can also be hydrolysed by phospholipases or proteases (the concentration of which can increase strongly during microbial infection), or peroxidised by reactive oxygen species (ROS), or altered by various pollutants (acids, fumes, particles). In order to design lung substitute preparations that are more efficient against ARDS, it is necessary to better understand the biophysical mechanisms of lung surfactant inactivation, especially by the most damaging inhibitors.

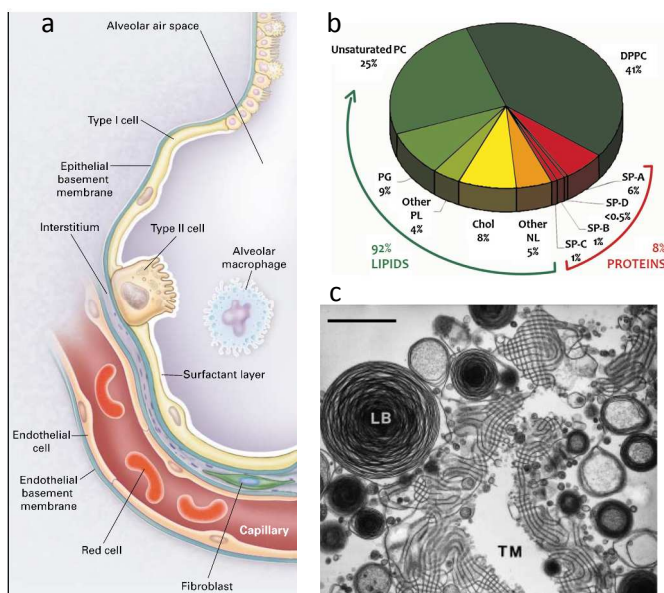
This short review presents the strategies that have recently been proposed to overcome the inactivating effect of proteins on the pulmonary surfactant. In one approach, SP-B/SP-C protein analogues or simpler peptides have been designed that mimic the constituents of the native surfactant that are responsible for its innate resistance to inactivation. Another new and cost-effective approach consists of using hydrophilic polymers and electrolytes. A markedly different approach makes use of the unique properties of fluorocarbons (biological inertness, gas transport capacity, spreadability, low surface tension and high vapour pressure with regard to molecular weight). These water-insoluble compounds have been investigated in the 1990's in clinical trials of partial liquid ventilation and as injectable oxygen carriers.<sup>12</sup> Fluorocarbon gases are routinely utilised as ophthalmic tamponades for repair of retina detachment and as stabilisers of the commercial gas microbubbles used as ultrasound diagnosis contrast agents. Fluorinated compounds also have potential as reporters for <sup>19</sup>F magnetic resonance imaging (MRI).<sup>13</sup> The review emphasises recent investigations that demonstrate the potential of fluorocarbons as components for lung surfactant therapy.

## 2. The native lung surfactant

### 2.1. A complex bio-interface

The respiratory pulmonary gas exchange takes place through a complex physical barrier that includes the thin aqueous film that lines up the alveolus (the alveolar lining layer), the alveolar epithelial cells, the interstitial layer, the endothelial cells that form blood capillaries, the blood plasma and the erythrocyte membrane (Scheme 1a).<sup>7, 14, 15</sup> In mammals, the native lung surfactant typically

contains a large proportion of lipids (~90% by surfactant mass), primarily DPPC (~40%), small fractions of polyunsaturated fatty-acid-based phospholipids, anionic phospholipids such as phosphatidylglycerols, neutral lipids such as diacyl- and triacylglycerols, free fatty acids such as palmitic acid, plasmalogens, and cholesterol (~8%) (Scheme 1b).<sup>16, 17</sup>



Scheme 1. a) Structure of the alveolus; from <sup>1</sup>. b) Typical composition of the lung surfactant in mammals; from <sup>18</sup>. c) Electron micrograph of a rat lung showing lamellar bodies forming tubular myelin (bar 1 μm); from <sup>19</sup>.

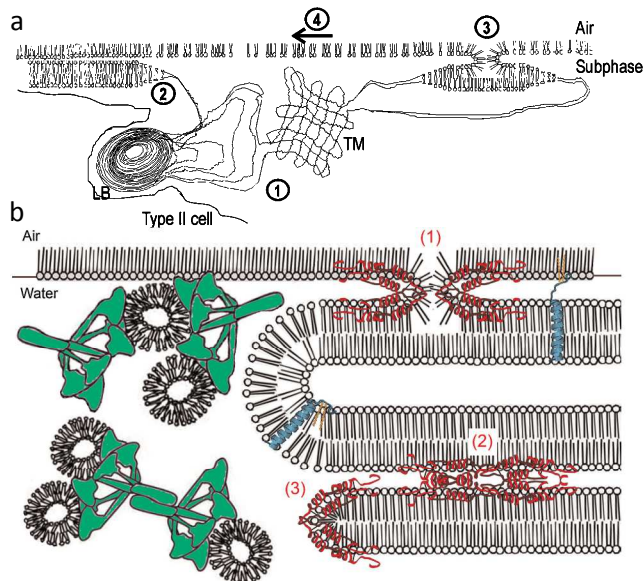
The remaining 10% of the composition comprises four proteins, named surfactant proteins SP-A, SP-B, SP-C and SP-D.<sup>20</sup> SP-A (monomeric, MW 26–38 kDa) and SP-D (43 kDa) are large hydrophilic glycoproteins that belong to the calcium-dependent carbohydrate-binding collectin family.<sup>21, 22</sup> SP-A and SP-D play important roles in pulmonary host defence and control of lung inflammation. These proteins bind to various microorganisms and pathogen-derived components and modulate leukocyte functions such as chemotaxis, cytokine function and phagocytosis.<sup>23</sup> By associating with cell surface pattern recognition receptors, SP-A and SP-D regulate inflammatory cellular responses such as the release of lipopolysaccharides-induced pro-inflammatory cytokines.<sup>22</sup> SP-A associates with surfactant membranes via its globular carbohydrate recognition domains and can promote surfactant vesicle aggregation in the presence of calcium.<sup>18</sup> SP-A also facilitates formation of surfactant tubular myelin, thus regulating surfactant secretion and recycling. Contrary to SP-A, SP-D is not associated with surfactant membranes. SP-D participates in surfactant reuptake and recycling and has potent protective antioxidant properties. The smaller hydrophobic proteins SP-B and SP-C play important roles for determining the surface activity of the lung surfactant, including efficient surface adsorption, film stability and re-spreading processes of surfactant during the continuous compression–expansion breathing cycles.<sup>24</sup> SP-B, a 79-residue polypeptide (MW 8.7 kDa) composed of amphiphilic  $\alpha$ -helices connected by amino acids containing apolar loops, belongs to the saposin-like protein family.<sup>25, 26</sup> It exhibits a positive net charge, which results in interactions with anionic phospholipids. It was suggested that SP-B



interact and connect surfactant bilayers and monolayers due to its amphiphilic character and presence of charged residues. SP-B is essential for the biogenesis of lamellar bodies, the organelles used by type II pneumocytes to assemble, store and secrete surfactant membranes (Scheme 1c). SP-C is a 35 residues monomer (4.2 kDa) that forms a single  $\alpha$ -helix rich in branched aliphatic residues and has a trans-membrane orientation in surfactant bilayers.<sup>27</sup>

## 2.2. Formation of the surfactant monolayer and its role in respiration

The lipids and hydrophobic proteins SP-B and SP-C are synthesized mainly in the alveolar space by epithelial type II pneumocytes where they are stored in lamellar bodies (1-3  $\mu$ m in diameter) before being secreted by exocytosis into the alveolus. The lipids of the lamellar bodies rearrange in the alveolus into an expanded membrane called tubular myelin, from which the monolayer is formed and spreads at the air-fluid interface just above the alveolar epithelium (Scheme 2a). SP-A and SP-D are secreted independently of the lamellar bodies and are associated with the surfactant lipids in the alveolar lumen. From the alveolus, the surfactant components are recycled into type II cells, where they are re-utilised or removed from the cycle by phagocytosis and degraded within alveolar macrophages. One key role of the lung surfactant is to form a monolayer at the interface between air and the fluid hypophase that lines the alveoli. The surfactant monolayer is in charge of reducing the surface tension upon compression (i.e., during expiration), thus reducing the work of breathing, and must respread easily on expansion (i.e., during inspiration) with spreading rates compatible with respiration.



Scheme 2. a) A model illustrating surfactant secretion from the alveolar type II cells and the steps by which it forms a surface layer on the alveolar sub-phase, including 1) secretion of lamellar bodies from type II cells and formation of tubular myelin surfactant; 2) spreading of the tubular myelin surfactant as individual bilayers; 3) fusion and conversion of bilayers to monolayers; and 4) lateral spreading of surfactant monolayers; from <sup>2</sup>. b) A model for surfactant reservoirs associated with the interfacial monolayer showing the possible roles of SP-A (green), SP-B (red) and SP-C (blue) in the dynamic folding and re-spreading of interfacial films. SP-B is represented in three hypothesized roles: 1) facilitating formation of the intermediate lipid structure between monolayer and bilayer; 2) generating stacks of bilayers via protein-protein interactions; and 3) promoting formation of bilayer disks; from <sup>18</sup>.

These conflicting requirements are achieved by a combination of specialised compounds that work synergistically to promote adsorption and spreading during dynamic compression-expansion cycling. DPPC alone can generate near-zero surface tension at the air-water interface during compression, but cannot respread fast enough upon expansion because it forms highly cohesive (semi-crystallised liquid-condensed) two-dimensional domains at the air-water interface due to strong lateral interactions. It is the presence of unsaturated lipids such as phosphatidylglycerols and phosphatidylcholines, and of the amphiphilic proteins SP-B and SP-C that allows reversion to the fluid liquid-expanded phase.<sup>7, 28</sup> On the other hand, fluid monolayers would not allow reaching the low surface tensions necessary for proper lung function. Therefore, in order to reach low tensions some minor components (predominantly non-phosphatidylcholine compounds) are squeezed out from the monolayer upon compression, which results in an enrichment of the monolayer in DPPC and allows transition to the condensed phase. Surface tension is then reduced while alveolar collapse is prevented. A concept involving a “surface-associated reservoir” was developed to account for the fact that phospholipid uptake occurs too fast to be explained solely by *de novo* adsorption.<sup>7, 18, 29</sup> In this model, layers of surfactant are folded in the sub-phase and remain in contact with the monolayer at the air/liquid interface, ready for rapid replenishment of the surfactant layer (Scheme 2b).

## 2.3. Lung surfactant substitutes

Surfactant therapy involves the administration of exogenous surfactant preparations in order to replace the absent or damaged native surfactant.<sup>7, 8, 18</sup> Clinically used surfactant preparations consist mostly in two classes. A first class includes surfactants that are extracted from animal sources and are depleted in SP-A and SP-D, such as BLES (BLES Biochemicals, London, ON, Canada), Curosurf (Chiesi Farmaceutici, Parma, Italy), Infasurf (ONY, Amherst, NY, US), Survanta (Abbott Laboratories, North Chicago, IL, US), Surfacten (Tokyo Tanabe Co., Tokyo, Japan) and Surfacten (CENSA, Mayabeque, Cuba). Despite their intrinsic drawbacks, such as potential risks of pathogen transmission, variability in composition and high cost, the modified “natural” surfactants are generally more effective than the synthetic formulations (Table 1). Their efficacy is limited, however, to the treatment of NRDS. They were found to improve oxygenation, but did not reduce mortality in the case of surfactant inactivation such as in ARDS or MAS.<sup>8, 3, 30, 31</sup> A second class of more recently developed preparations includes synthetic surfactants that contain lipids and recombinant SP-C (Venticute, Altana Pharm. Konstanz, Germany),<sup>32</sup> SP-B/SP-C protein analogues or simple peptides that mimic surfactant proteins (KL4 peptide, Surfaxin, Discovery Laboratories, Warrington, PA, US).<sup>33</sup> Other exogenous surfactant preparations include combinations of lipids with Hel 13-5 peptide (mimic of SP-C)<sup>34, 35</sup> or with polymers (poly-L-lysine electrostatically complexed with poly-L-glutamic acid, Synsurf).<sup>36</sup>

## Review

Table 1 Advantages, limitations and challenges of the current approaches to develop lung surfactant preparations capable of overcoming inactivation by serum proteins

Approaches	Development	Advantages	Limitations and challenges
Modified animal surfactants complemented with SP-B & C	Commercial In the clinic	<ul style="list-style-type: none"> <li>• Available</li> <li>• Adequate surface activity</li> <li>• Variable sensitivity to inactivation</li> <li>• Variable results in ARDS/ALI treatment</li> </ul>	<ul style="list-style-type: none"> <li>• Transmission risks (lack of SP-A &amp; D)</li> <li>• Batch-to-batch variations</li> </ul>
Synthetic preparations with surfactant protein mimics or peptides	In the clinic or preclinical	<ul style="list-style-type: none"> <li>• Batch-to-batch consistency</li> <li>• Large scale production</li> <li>• Cost effectiveness</li> </ul>	<ul style="list-style-type: none"> <li>• Under development</li> <li>• Less effective than modified natural surfactants</li> </ul>
Polymers	Preclinical	<ul style="list-style-type: none"> <li>• Surfactant preparation adsorption enhancement</li> <li>• Resistance to inactivation</li> <li>• Versatility and cost-efficiency</li> </ul>	<ul style="list-style-type: none"> <li>• Under development</li> <li>• Not yet defined formulations</li> <li>• Need tests in animal models</li> </ul>
Fluorocarbon gases & liquids	Basic research	<ul style="list-style-type: none"> <li>• DPPC monolayer fluidisation &amp; near-zero surface tension</li> <li>• DPPC adsorption enhancement</li> <li>• Resistance to inactivation (albumin)</li> <li>• Biological acceptance of fluorocarbons demonstrated</li> <li>• Versatility and cost efficiency</li> </ul>	<ul style="list-style-type: none"> <li>• Need defined formulations, delivery systems, administration modes</li> <li>• Need tests in animal models</li> </ul>
Fluorinated surfactants	Basic research	<ul style="list-style-type: none"> <li>• DPPC adsorption enhancement</li> <li>• Resistance to inactivation (fibrinogen)</li> </ul>	<ul style="list-style-type: none"> <li>• Assessment of toxicity</li> <li>• Non defined formulations, delivery modes</li> <li>• Need tests in animal models</li> </ul>

### 3. Biophysical mechanisms of surfactant inactivation by proteins

The various processes by which the normal activity of the pulmonary surfactant is reduced or suppressed are referred to as surfactant inactivation. Common conditions related to surfactant inactivation include ALI/ARDS, MAS and pulmonary oedema. Certain mechanisms of surfactant inactivation are related to chemical degradation of surfactant constituents or to alteration of the surfactant's aggregate structure and morphology. These impairments can occur at various time-points of the surfactant's life-time, including during secretion of the lamellar bodies into the alveolar liquid layer and unpacking in membrane vesicles, during formation of the monolayer, or during reuptake by type II cells or macrophages. Impairments can also occur during transport from the alveoli to the airways.<sup>14, 18, 37</sup> All these abnormalities may prevent the phospholipids from reaching low surface tension values during monolayer compression or hamper their re-spreading during expansion. In most of these cases, surfactant inactivation is slow and permanent.<sup>18, 37</sup>

By contrast, in ARDS and ALI, inactivation is rapid and often correlated with increased concentration of various substances, including plasma proteins, unsaturated phospholipids, lysophospholipids, free unsaturated acids (e.g. oleic acid), bile salts,

diacylglycerol and cholesterol, or meconium.<sup>7, 38</sup> Despite large variations, most studies consistently report an increase of albumin concentrations in the alveolar fluid during ARDS (~25 mg mL<sup>-1</sup> in ARDS patients versus ~5 mg mL<sup>-1</sup> in healthy patients).<sup>39</sup> The protein concentration in the alveolar fluids of ARDS patients correlates actually with the severity of the disease.<sup>40</sup> Leakage of plasma proteins into the alveolar space due to impaired function of the alveolar-capillary barrier was recognised as an early event in the pathogenesis of ARDS and may contribute substantially to surfactant alterations.<sup>8, 41</sup>

Various *in vitro* studies have reported that different inhibitors, including plasma proteins and certain lipids, can interfere at different stages with phospholipid functions by hindering phospholipid adsorption and formation of a functional surfactant film, by preventing the film from reaching low  $\gamma$  values or by increasing film compressibility, and by affecting phospholipid re-spreading from surfactant reservoirs upon expansion.<sup>7</sup>

#### 3.1. Proteins prevent access of surfactant to the alveolar interface by competitive adsorption

Soluble proteins such as fibrinogen, fibrinogen monomer, haemoglobin and albumin were found to interfere with surfactant

phospholipid *de novo* adsorption.<sup>2, 42-53</sup> Surfactant adsorption was also strongly impaired by lysophosphatidylcholine, while supraphysiological concentrations of neutral lipids (monoacylglycerol, diacylglycerol, unsaturated fatty acids, cholesterol and cholesterol esters) showed little effect on adsorption. All serum proteins are surface active and can compete with surfactant membranes for adsorption at the air–water interface. Phospholipids, which are present in the form of large aggregates, adsorb and spread slowly at the interface through “unzipping” processes.<sup>7</sup> Despite their lower surface tension, they adsorb more slowly than small amphiphilic proteins, which adsorb rapidly by molecular diffusion. Once adsorbed at the interface, the film of protein prevents phospholipids from reaching the interface by creating a steric and/or electrostatic (DLVO-type) energy barrier.<sup>37</sup> It is reasonable to think that, at the surfactant/albumin concentration ratios that prevail in ARDS conditions, competitive adsorption plays a role in the inhibition of the surfactant. However, other mechanisms have been proposed that suggest interaction and/or binding of the proteins with the surfactant.<sup>54</sup> It is important to note that albumin is a relatively weak inhibitor, as compared to other serum proteins, such as fibrinogen.

### 3.2. Proteins prevent surfactant from reaching low surface tension and from re-spreading at the alveolar interface

The ability of the surfactant phospholipids to attain low surface tensions during compression is hampered by serum proteins, fibrinogen, fibrinogen monomer, and C-reactive protein, which bind to the polar phosphorylcholine group, and to a lesser extent, by albumin.<sup>53</sup> Simultaneous increase in C-reactive protein and decrease in SP-A in the alveolar space were associated with ALI.<sup>55</sup> It was suggested that C-reactive protein inhibits the surfactant by fluidising the surfactant film.<sup>56</sup> Surfactant compressibility is markedly increased by supraphysiological concentrations of cholesterol. Surface tension reduction at end-expiration is also affected by high monoacylglycerol, diacylglycerol, unsaturated fatty acids, bile salts and cholesterol (a major component of meconium) and cholesterol esters.<sup>18</sup> Respreading of surfactant phospholipids from surface-associated reservoirs is inhibited by CRP and, at high surface tensions, by albumin. Supraphysiological concentrations of cholesterol have also a deleterious effect on surfactant re-spreading.

### 4. Optimising lipids and proteins in order to resist surfactant inactivation

The higher efficiency of modified natural surfactants over protein-free synthetic surfactants demonstrates the importance of the native proteins in overcoming surfactant inactivation (Table 1). In animal experiments, surfactant preparations containing SP-A showed higher resistance to inactivation than those without SP-A.<sup>57</sup> Addition of SP-A increased the resistance of lipid extract surfactants to blood proteins<sup>46, 47</sup> and meconium<sup>58</sup>. Both SP-B<sup>7, 50</sup> and SP-C<sup>59, 60</sup> have been reported to increase the resistance of lung surfactant to inactivation by various agents. These proteins have therefore been proposed for optimizing the surface behaviour of the surfactant.<sup>15</sup> A preparation containing a synthetic C16:0 diether phospholipid

(DEPN-8, structurally resistant to phospholipase degradation) and SP-B/C was found to be highly resistant to inhibition by serum proteins, phospholipase A<sub>2</sub> and lysophosphatidylcholine.<sup>61</sup> Addition of peptide analogues of SP-B and/or SP-C also improved the resistance to surfactant inactivation.<sup>62, 63</sup> Recently, a new generation of synthetic analogues, which incorporates recombinant proteins or SP-B/SP-C peptides, has been tested *in vivo*. CHF 5633 is a fully synthetic surfactant containing two phospholipids, DPPC and 1-palmitoyl-2-oleoyl-glycerol-3-phospho-1-glycerol sodium salt (reported to inhibit lung inflammation) and two peptidic analogues of human SP-B and SP-C, designed to resist to oxidative injury.<sup>64</sup> The SP-C analogue is a 33-amino acid protein that includes both the N-terminal and C-terminal helical segments found in native SP-C. The SP-B analogue is a 34-amino acid protein derived from the full-length natural SP-B. A study demonstrated superior oxygenation and lung compliance in ventilated preterm lambs treated with CHF 5633 as compared to animal-derived surfactant preparations.<sup>64</sup> In another study led after surfactant inactivation in preterm lambs, CHF 5633 showed a survival benefit over the gold standard treatment Curosurf at the same doses.<sup>65</sup>

## 5. Using hydrophilic polymers and electrolytes

Introduced in the late 1990's, certain water-soluble polymers were found to enhance adsorption and increase the surface activity of various surfactant substitutes and to reverse or reduce inactivation by serum, meconium, albumin and other substances, both *in vitro* and *in vivo*.<sup>2, 66-69</sup> Many polymers were found effective, including non-ionic polymers (poly(oxyethylene) PEG 10000, dextran 9500 and 71000, polyvinylpyrrolidone PVP), anionic polymers (hyaluronan) and cationic polymers (chitosan).

### 5.1. Nonionic and anionic polymers--Generating depletion forces

The enhancement of surfactant adsorption by addition of PEG 10000 or hyaluronan was found to be a function of both polymer concentration and molecular weight (Figure 1, Table 1), which supported a model based on polymer-induced depletion-attraction, a non-specific polymer-induced entropic force.<sup>2, 37, 52</sup> A quantitative theory of surfactant inactivation by charged surface-active serum proteins has been proposed.<sup>2, 37, 52</sup> This theory uses Smolukowski's analysis of colloidal stability and suggests formation of a repulsive energy barrier by serum protein at the interface, with contributions of both steric effects and electrostatic repulsions.<sup>2, 37</sup> When two vesicles of lung surfactant are approaching each other, there is a point at which the polymer can no longer fit into the space available between these vesicles and will be excluded from this space. The resulting enrichment in polymer in other zones produces an increase in osmotic pressure that draws water from the polymer-depleted region, thus promoting vesicle fusion. A similar process occurs at the air/water interface. The resulting polymer depletion drives the vesicles towards this interface, thus decreasing the energy barrier for surfactant adsorption. The depletion attraction is purely entropic and independent of the chemical composition of the surfactant, protein and polymer, which explains that PEG, dextran and hyaluronan



were all effective at enhancing adsorption of various surfactant substitutes (Survanta, Curosurf and Infasurf).<sup>2, 37, 52</sup>

This view has recently been confirmed by a study of the rheological dilational properties of surface films formed by Exosurf, Survanta, Curosurf or Alveofact in the presence of albumin and PVP, PEG or dextran. The hydrophilic polymers were found to restore the DPPC content of the surface film.<sup>70</sup>

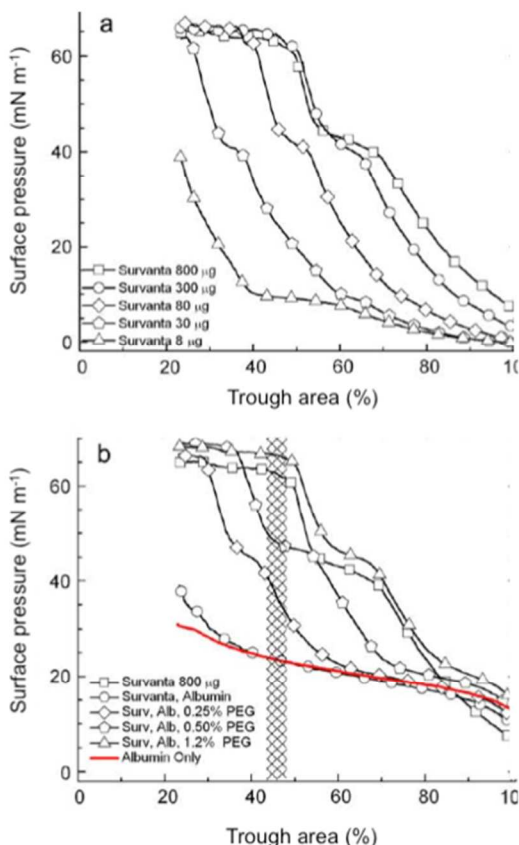


Fig 1 Compression isotherms of a) Survanta on a buffer sub-phase, showing increased adsorption with increased concentration, and b) Survanta (800 µg) on sub-phases containing albumin (2 mg mL<sup>-1</sup>) with increasing PEG concentrations. Albumin produces the same effect as decreasing Survanta concentration. Adding increasing amounts of PEG produces the same effect as increasing Survanta concentration. From <sup>71</sup>.

In another recent study, the effect of hydrophilic polymers was investigated using thin (black) foam films.<sup>72</sup> It was indeed suggested that the lung surfactant exists as an intrapulmonary foam of air bubbles filling the terminal lung unit.<sup>73</sup> The contacts between bubbles, and between bubbles and cell surfaces consist of black foam films. The ability of the polymers to decrease the effect of albumin inhibition was expressed by their capacity of restoring stable and homogeneous black films (Figure 2).

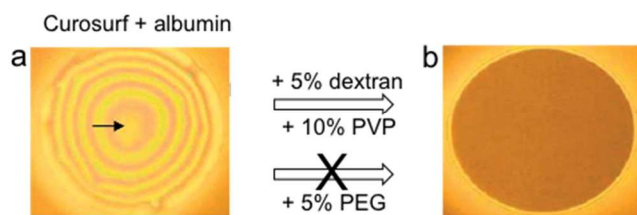


Fig 2 Inhibition of Curosurf by albumin in foam films, and effect of hydrophilic polymers (dextran, PVP or PEG) on the recovery of surfactant surface properties. Dextran and PVP were efficient, but not PEG. Foam films thicknesses were a) ~1133 nm and b) ~15 nm; from <sup>72</sup>.

A microinterferometric method allowed direct visualisation of foam film morphology, evaluation of its stability and viscosity, and provided access to the disjoining pressure, a measure of the interactions (electrostatic, van der Waals, steric, etc.) between two interfaces. This study indicated that some specific interactions might take place, as certain polymers have an effect on certain surfactant substitutes, but not on all of them (e.g., Survanta recovered its effectiveness with PEG, PVP, and hyaluronan, while Curosurf recovered it with dextran, PVP, and hyaluronan) and suggested that both depletion attraction and specific interaction were operative.

## 5.2. Electrolytes—Decreasing Debye length

Classical methods of manipulation of the double-layer repulsion in colloids using electrolytes were shown to have similar predictable effects on surfactant adsorption.<sup>37</sup> In vitro studies showed that increasing NaCl concentration above physiological levels decreases the Debye length and the magnitude and range of the double-layer repulsion, and restores surfactant adsorption in the presence of albumin (Figure 3).<sup>71</sup>

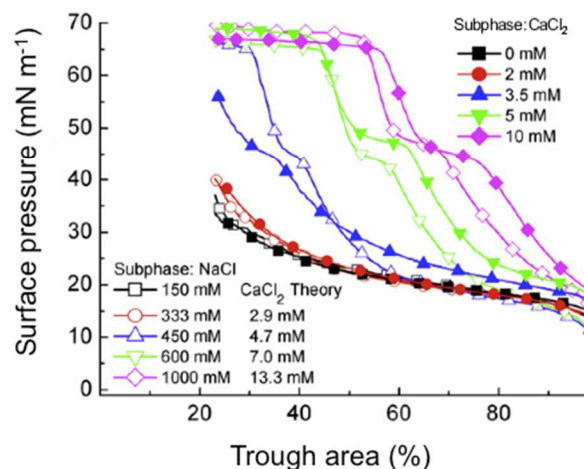


Fig 3 Compression isotherms of Survanta (800 µg) on a buffered saline sub-phase (0.2 mM NaHCO<sub>3</sub>, pH 7) containing albumin (2 mg mL<sup>-1</sup>). Various electrolyte concentrations are plotted. For each NaCl concentration, the theoretical CaCl<sub>2</sub> concentration according to the Schulze-Hardy rule, is given; from <sup>71</sup>.

It would obviously be impracticable to use high levels of saline because of their osmotic effect on lung tissue. However, it has been calculated (using the Schulze-Hardy rule) that divalent calcium would enhance surfactant adsorption at concentrations 2<sup>-6</sup> lower than monovalent sodium. It was experimentally verified that CaCl<sub>2</sub> concentrations of ~15-20 mM would be sufficient to overcome albumin adsorption and would have minimal effects on the fluid balance in a rat lung.<sup>71</sup>

## 5.3. Cationic additives (polyelectrolytes and peptides)—Flocculating surfactant aggregates

The interactions between a cationic polyelectrolyte, chitosan (612, 113 and 213 kDa), or two cationic peptides (polylysine 50 kDa and polymyxin B), and BLES were studied using dynamic compression/expansion cycles of dilute BLES preparations.<sup>74, 75</sup> Extremely low concentrations of both chitosan and of the two peptides were found to improve the adsorption of the surfactant substitute at the air/water interface in the presence of albumin. The optimal additive/surfactant ratio was determined based on the minimal surface tension that could be reached upon dynamic compression carried out in a constrained sessile drop device in the presence of serum. The zeta potential of the lung surfactant aggregates in the sub-phase suggests that chitosan and the peptides bind to the anionic lipids (phosphatidylglycerols) in BLES, and that this binding is responsible for the changes in surface activity (elasticity and stability) observed for these surfactant–polyelectrolyte mixtures. However, unlike calcium or PEG, increasing chitosan concentration above optimal caused less surfactant to adsorb, and inactivation occurred again. The optimal formulation containing these peptides were able to reach low minimum surface tensions in systems containing 500  $\mu\text{L mL}^{-1}$  of serum, thereby matching the effectiveness of the complete lung surfactant.

## 6. Using fluorocarbon compounds in lung therapy

### 6.1. Relevant physicochemical properties of fluorocarbons and fluorinated surfactants

Fluorocarbons and perfluoroalkylated surfactants have properties of their own that distinguish them markedly from their alkylated analogues.<sup>76, 77</sup> Fluorocarbons (FCs) have been investigated for various biological applications due to their high biological inertness, remarkable ability to solubilize gases, extremely low solubility in water and low surface tension, including for intravascular oxygen transport<sup>12, 78</sup> and stabilization of gaseous microbubbles used as contrast agent in ultrasound imaging.<sup>79–82</sup> The surface tension of lungs has been measured in situ by depositing small droplets of various fluorocarbons on excised lungs of rats.<sup>83</sup> Interactions among fluorinated chains are weak, due to the lower polarisability of fluorine as compared to hydrogen (and hence, lower van der Waals forces), resulting in extremely low water solubility. Perfluoroalkyl chains are much more hydrophobic than alkyl chains, and have also a lipophobic character. Consequently, fluorinated surfactants can reduce air–water superficial tension more effectively than their hydrogenated counterparts, reaching values that cannot be obtained with the latter. Their capacity for segregation and self-association is also much more pronounced, fostering higher organization, including with phospholipids.<sup>78, 84–86</sup>

### 6.2. Partial liquid ventilation with fluorocarbons: improvement of lung compliance, recruitment of lung alveoli and anti-inflammatory effects

At the end of the 1960's the discovery that rodents immersed in a liquid fluorocarbon can survive by breathing the oxygen solubilised in this fluid<sup>87, 88</sup> coincided with the initial description of ARDS.<sup>89</sup> In the 1990's, there have been numerous studies aiming at assessing

the utility of fluorocarbons in partial liquid ventilation (PLV) for the treatment of ARDS. Perfluorooctyl bromide (PFOB) in particular has been extensively investigated for its capacity to act as liquid positive end-expiratory pressure ("liquid PEEP") to recruit collapsed alveoli and improve oxygenation and ventilation.

PLV with FC has been described in many animal models (premature, full-term neonatal and adults) and a few human studies. Improved oxygenation and lung compliance were achieved in preterm animal models,<sup>90</sup> as well as in premature infants.<sup>91, 92</sup> Adequate gas exchange could be maintained in healthy rabbits at airway pressures comparable to those used in conventional ventilation. A study on a saline lavage rabbit model of respiratory failure showed improvement in oxygenation with PFOB, effective gas exchange at relatively low airway pressures, and overall improvement in both pulmonary mechanics and lung histology as compared with conventional ventilation.<sup>93, 94</sup> In another study, severe respiratory failure was induced with oleic acid in young sheep.<sup>95</sup> Improved pulmonary mechanics (increased compliance), improved oxygenation, and marked reduction in alveolar haemorrhage, lung fluid accumulation and inflammatory infiltration was demonstrated in the PFOB group, as compared to the gas ventilated animals. A human adult trial found significant improvement in physiological shunt and static pulmonary compliance.<sup>96</sup> Studies were also conducted on human neonates that were impressive regarding oxygenation.<sup>91, 97</sup> Another study evaluated the use of PLV in trauma patients as compared with conventional mechanical ventilation.<sup>98</sup> The alveolar inflammatory response was investigated, as measured by white cell infiltration and capillary leak. The sequence of pro-inflammatory and anti-inflammatory cytokines exhibited an anti-inflammatory effect in the alveolar environment with reduction of pro-inflammatory interleukins IL-1 and IL-6, white blood cell count, and protein capillary leak.<sup>98</sup> PLV also reduced alveolar neutrophils independent of IL-8. Administration of PFOB reduced total white cell and neutrophil infiltration into the alveoli, capillary leak of proteins, and expression of the inflammatory cytokines IL-1 and IL-6. The anti-inflammatory IL-10 was also reduced. All of these alveolar responses appeared to be beneficial when viewed individually, but did not result in significant clinical improvement. The fact that FCs attenuate the pro-inflammatory and pro-coagulatory responses of activated monocytes and of alveolar macrophages may contribute to the protective role of FCs in injuries associated with local activation of inflammatory processes.<sup>99</sup> Delivery of vaporized FCs to oleic acid-injured ARDS sheep resulted in significant and sustained improvements of gas exchange and of lung compliance.<sup>100</sup> PLV trials were abandoned when improved, less damaging ventilators became available.

### 6.3. Combined administration of exogenous surfactant and fluorocarbons

It was suggested that the low efficacy of the surfactant substitutes in the treatment of ARDS could be related, in addition to surfactant inactivation, to inhomogeneity in patient aeration due to adjacent atelectatic and overinflated areas.<sup>101</sup> Since exogenous surfactant preferably distributes in aerated areas,<sup>102</sup> alveolar recruitment is



required prior to surfactant therapy.<sup>103</sup> In PLV, deficiency of endogenous surfactant persists and respiratory insufficiency reappears after evaporation of the *FC*. In order to re-open atelectatic areas and substitute the inactivated surfactant, surfactant administration was used in animal studies both prior<sup>90, 104-107</sup> and after PLV,<sup>108</sup> without clear beneficial results.<sup>101</sup> In surfactant-depleted rats, administration of *FC*-in-surfactant emulsions (surfactant: Curosurf; *FC*: PFOB, perfluorooctane (PFO), or a blend of perfluorinated cyclic ethers (RM101)) led to a more homogenous distribution of gas (in the Curosurf group) and fluids in the case of *FC*- or *FC*-in-Curosurf emulsion groups) and aeration of the lung than with surfactant alone (Figure 4).

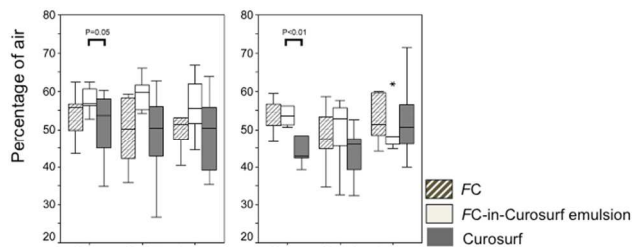


Fig 4 Percentage of gas-filled areas (in Curosurf group) or fluid-filled areas (in the *FC* or *FC*-in-Curosurf emulsion groups) in total parenchyma. Values are shown as median, range and outliers (\*) for the upper, middle and lower part of the left lung; from <sup>101</sup>.

#### 6.4. Fluorocarbon gases have a fluidising effect on DPPC monolayers, yet allow reaching low surface tensions, and prevent albumin adsorption

*In vitro* studies have shown that a series of fluorocarbon gases (*gFCs*), including PFOB, perfluorooctylethane, perfluorooctane, perfluorodecaline and bis(perfluorobutyl)ethene, are able to inhibit the liquid-expanded (LE)/liquid-condensed (LC) phase transition of DPPC Langmuir monolayers.<sup>109, 110</sup> The formation of semi-crystalline domains of an LC phase, which typically occurs in the LE/LC coexistence region upon compression of DPPC, is prevented when the atmosphere above the DPPC monolayer is saturated with a *gFC* (Figure 5).

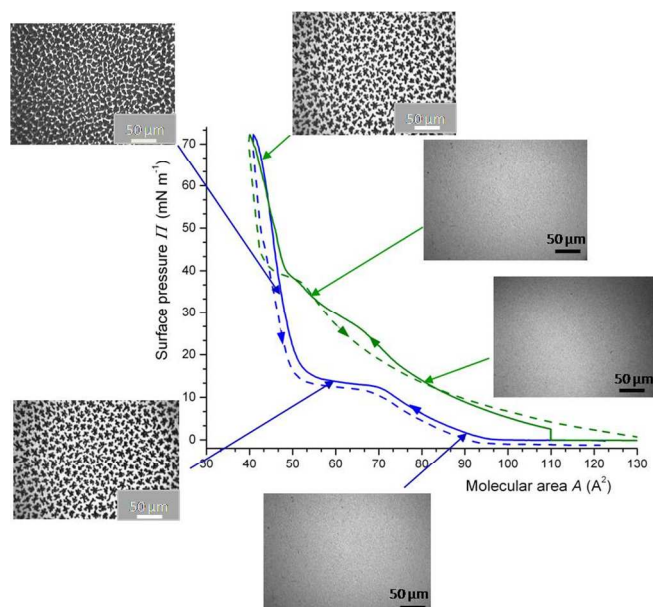


Fig 5 Fluidising effect of *FC* gases on DPPC monolayers as assessed by surface pressure  $\Pi$ / molecular area  $A$  isotherms and fluorescence optical microscopy (25°C). Isotherms of DPPC (compression: solid lines; expansion: dashed lines) in an atmosphere of  $N_2$  (blue) or  $N_2$  saturated with PFOB (green). Insets: fluorescence images showing that the DPPC monolayer in contact with PFOB remains in the liquid expanded phase up to  $\sim 38 \text{ mN m}^{-1}$ , while that in contact with  $N_2$  shows liquid-condensed phase domains at  $\Pi > \sim 10 \text{ mN m}^{-1}$ . At maximum compression, PFOB is totally expelled from the DPPC monolayer and a high  $\Pi$  value ( $\sim 70 \text{ mN m}^{-1}$ ) is reached.  $15 \mu\text{L}$  of a DPPC solution in  $\text{CHCl}_3$  ( $1.0 \times 10^{-3} \text{ mol L}^{-1}$ ) were spread on the water surface. Adapted from <sup>109</sup>.

When contacted with *gFC*, the DPPC monolayer remains in the LE phase for surface pressures lower than  $\sim 40 \text{ mN m}^{-1}$ , as assessed by isotherms and fluorescence microscopy. The images were obtained using the fluorescent dye NBDC6-HPG, which is preferentially soluble in the disordered regions of the monolayer.<sup>111</sup> Interestingly, the *FC* is totally expelled from the monolayer at maximal compression (*i.e.* for molecular area  $\sim 40 \text{ Å}^2$ ) and high surface pressure values ( $\sim 70 \text{ mN m}^{-1}$ ) are reached. *gFCs* also induced the dissolution of pre-existing LC phase domains, thus facilitating re-spreading of DPPC molecules on the water surface, as shown by fluorescence microscopy and grazing incidence x-ray diffraction (Figure 6).<sup>110</sup> A unique situation is created in which *gFCs* have a highly effective fluidizing effect on the DPPC monolayer, without preventing achievement of low surface tension at maximal compression (Table 1).

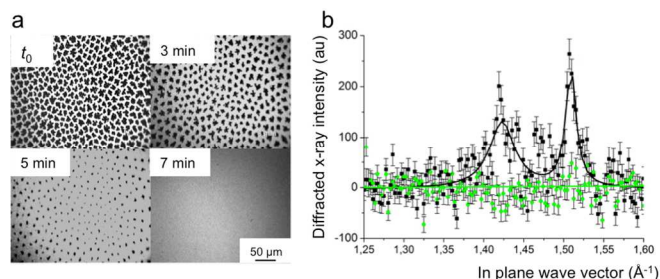


Fig 6 a) Fluorescence micrographs of a DPPC monolayer compressed at  $13 \text{ mN m}^{-1}$  under  $N_2$ . At time  $t_0$ , the atmosphere of  $N_2$  above the monolayer was saturated with *gPFOB*. The LC domains progressively disappear over time. After 7 min, the monolayer is totally fluidized. b) Intensity of the diffracted grazing x rays as a function of the in-plane vector  $q_{xy}$ . When compressed at  $20 \text{ mN m}^{-1}$ , the DPPC monolayer shows the two Bragg peaks characteristic of the tilted LC phase of DPPC at  $1.42$  and  $1.51 \text{ Å}^{-1}$  (black line). When the He atmosphere is saturated with *gPFOB* (green line), the peaks disappear rapidly, establishing the disappearance of the crystalline LC domains, allowing rapid respreading of the DPPC molecules. Adapted from <sup>110</sup>.

Recently, an equation of state for insoluble monolayers was applied to describe the isotherms of phospholipids measured in the presence of a fluorocarbon in the gas phase.<sup>112</sup> The observed co-adsorption mechanism of DPPC and *FC* molecules proposed in references<sup>109, 110</sup> manifests itself by remarkable differences in cohesion surface pressure. Due to the interaction of the adsorbed *FC* molecules with DPPC, the mutual interaction energy between DPPC molecules is reduced, leading to a very effective fluidization of the monolayer.

Another study established that *gPFOB* could counteract the effects of albumin on DPPC Langmuir monolayers.<sup>113</sup> When the *FC* gas is absent, albumin penetrates in the DPPC monolayer during compression, leading to the characteristic pattern shown in Figure 7a ( $\square 30 \text{ mN m}^{-1}$ ) and to liquid condensed phases upon further compression. On the other hand, for pressure values higher than

$\square 30 \text{ mNm}^{-1}$ , gPFOB fluidises the monolayer (Figure 7c), which means that it displaces the albumin from the interface. When expanded under air, the DPPC monolayer remains in a semi-crystalline LC phase, even at large molecular areas ( $80 \text{ \AA}^2$ , Figure 7b), whilst it is in the LE phase when gPFOB is present (Figure 7d). The fact that the pressure is much lower under gPFOB than under air upon expansion (for areas larger than  $\sim 50 \text{ \AA}^2$ ) supports the view that much less albumin is present in the monolayer. Altogether the incorporation of the PFOB molecules into the DPPC monolayer during expansion overcomes the incorporation of BSA, and prevents the latter from penetrating into the DPPC monolayer (Table 1).

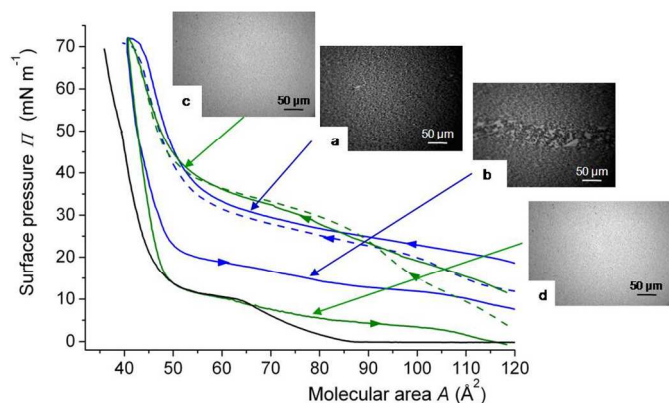


Fig 7. Compression isotherms of a Langmuir monolayer of DPPC spread on a sub-phase containing albumin ( $0.25 \text{ mg L}^{-1}$ ) and compressed under air (blue) or gPFOB-saturated air (green) at  $25^\circ\text{C}$ . The isotherm of DPPC, compressed under air, is shown as a reference (black). The first compression–expansion cycles are represented by solid lines and the second compressions by dashed lines. Fluorescence micrographs of the DPPC monolayer under air (a) upon compression at  $30 \text{ mN m}^{-1}$ , and (b) upon expansion at  $15 \text{ mN m}^{-1}$ ; and under gPFOB saturated air (c) upon compression at  $40 \text{ mN m}^{-1}$ , and (d) upon expansion at  $5 \text{ mN m}^{-1}$ . DPPC:  $15 \text{ }\mu\text{L}$  of a  $1.0 \times 10^{-3} \text{ mol L}^{-1}$   $\text{CHCl}_3$  solution. Adapted from <sup>113</sup>.

### 6.5. Combining the effects of fluorocarbon gases with an oscillatory regime

Applying sinusoidal oscillations to a film adsorbed on the surface of a millimetric bubble of air saturated with a fluorocarbon gas was recently found to constitute a mechanical means of reversing the outcome of the DPPC/albumin competitive adsorption.<sup>114, 115</sup> All the results presented in this section have been obtained using bubble profile analysis tensiometry (Tracker tensiometer, Teclis, Longessaigne, France).

First, prolonged oscillations were applied to a DPPC monolayer adsorbed on the surface of an air bubble (Figure 8).<sup>116</sup>

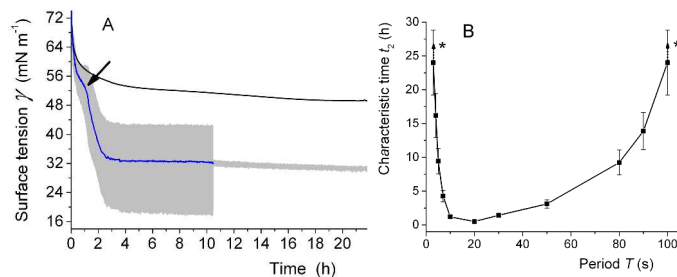


Fig 8 A) Kinetics of adsorption of DPPC ( $10^{-3} \text{ mol L}^{-1}$ , provided as a dispersion of vesicles) at the surface of an air bubble at  $37^\circ\text{C}$ . The bubble was static or submitted to oscillations ( $T 10 \text{ s}$ ,  $\Delta A 15 \%$ ). The oscillations were applied for  $\sim 10 \text{ h}$ , while  $\gamma$  was subsequently monitored for another  $12 \text{ h}$ . The arrow points to an increase in the adsorption rate. The grey area represents the fluctuations in surface tension associated with the oscillations. B) Characteristic time  $t_2$  of the second regime of the DPPC adsorption at  $37^\circ\text{C}$ , as a function of the oscillation period  $T$  ( $\Delta A 15 \%$ ). \*These  $t_2$  values are higher than  $24 \text{ h}$  and could therefore not be determined precisely. From <sup>116</sup>.

The adsorption of the phospholipid was drastically accelerated, a transition occurred between the dilute LE phase and the condensed LC phase and the surface tension  $\gamma$  was drastically reduced, reaching low values ( $30 \text{ mN m}^{-1}$ ) (Figure 8A). When the oscillations were stopped,  $\gamma$   $\square\square\square\square\square\square\square\square$  low, meaning that the system has reached its equilibrium value ( $\gamma\square\square\square$ ). Similar values have been measured for DPPC at equilibrium using different techniques.<sup>117</sup> By contrast, when no oscillations were applied (static regime), the phospholipids adsorb very slowly at the air/water interface; the  $\gamma$  value remained very high even after  $24 \text{ h}$ . Maximum  $\gamma$  lowering effect was reached for a period range of  $3 - 50 \text{ s}$  (Figure 8B). Interestingly, this range matches with the period range of respiration ( $15\text{-}20$  cycles per min).

Another study investigated the influence of prolonged sinusoidal oscillations on the competitive adsorption of DPPC and albumin at the surface of an air bubble.<sup>114</sup> It was found that the oscillations totally reversed the outcome of the competitive adsorption. After  $\sim 5 \text{ h}$ , albumin was progressively expelled and replaced by DPPC. Total replacement of albumin by DPPC was obtained in  $\sim 10 \text{ h}$  (Figure 9A).

Next, it was demonstrated that introduction of *F*-hexane in the air phase of the bubble accelerated the displacement of albumin and its replacement by DPPC by roughly an order of magnitude (Figure 9A).<sup>115</sup>

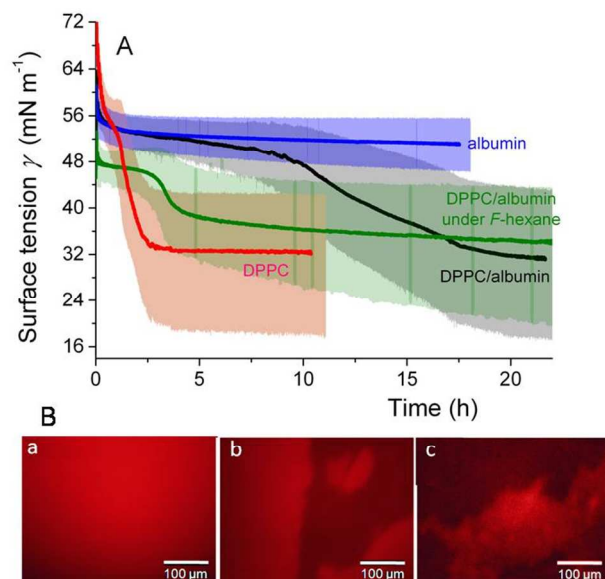


Fig 9 A) Kinetics of adsorption ( $37^\circ\text{C}$ ) at the surface of an air bubble having a shell of DPPC ( $10^{-3} \text{ mol L}^{-1}$ ), albumin ( $7.5 \times 10^{-7} \text{ mol L}^{-1}$ ), or a DPPC/albumin ( $1 \times 10^{-3}; 7.5 \times 10^{-7} \text{ mol L}^{-1}$ ) combination. Also shown is the absorption kinetics of DPPC/albumin at the *F*-hexane-saturated air/water interface. The bubbles were submitted to oscillations ( $T 10 \text{ s}$ ,  $\Delta A 15 \%$ ) throughout the experiments. The lightly colored areas represent the fluctuations in surface tension associated

with the oscillations. B) Fluorescence micrographs of the sequential adsorption of albumin and DPPC (injected 1.5 h after albumin) at the air/buffer interface of a Langmuir trough in the presence or absence of *F*-hexane. a) at  $t = 0$ , albumin (+ 2 mol% of albumin-Texas-Red) is injected in the sub-phase. DPPC is injected 1.5 h later. It takes ~1.5 h (in the presence of *F*-hexane) and ~6 h to replace albumin from ~60% of the interface. Adapted from <sup>114</sup> and <sup>115</sup>.

The replacement of albumin by DPPC was also visualized by fluorescence microscopy on Langmuir films (Figure 9B). A possible mechanism was proposed in which *F*-hexane rapidly goes to the air/water interface. Once there, it is incorporated into the hydrophobic site of albumin and promotes its unfolding, thus facilitating its expulsion towards the aqueous phase.<sup>115</sup> The unique aptitude of fluorocarbon gases to recruit molecules initially solubilised in an aqueous phase at the interface across a monolayer of phospholipids has recently been utilised to immobilise an hypoxia biomarker in a phospholipid monolayer.<sup>118</sup>

These results suggest that combinations of DPPC and a fluorocarbon gas might be useful for the treatment of lung conditions resulting from deterioration of the native lung surfactant function due to plasma proteins, such as in ARDS. Further investigation of the effects of *FC* gases on additional potential inhibitors is needed in order to assess the clinical relevance of this approach, as it was recently shown that albumin is probably not the most important agent responsible for the inhibition of the lung surfactant.<sup>119</sup> The delivery system most adapted to fluorocarbons has to be selected and the mode of administration investigated. Microbubbles, which have been reported for delivering Survanta<sup>120</sup>, are potential candidates as they are often stabilised by fluorocarbon gases.

#### 6.6. Fluorinated surfactants in combination with DPPC provide mixed monolayers with improved resistance to inactivation

Fluorinated and partially fluorinated surfactant additives have been assessed for tailoring potential lung surfactant replacement preparation properties. Fluorinated surfactants are highly surface-active and can generate lower surface tensions than their hydrocarbon analogues (typically ~15 mN m<sup>-1</sup> versus ~30 mN m<sup>-1</sup>). Fluorinated surfactants can be miscible, partially miscible or entirely immiscible with hydrocarbon surfactants, in particular with DPPC, depending on their structure. When they are mixed with DPPC in molar fractions lower than ~0.4, high surface pressures (> 65 mN m<sup>-1</sup>) can be reached. Fluorinated surfactants are generally chemically stable over a wide range of aggressive conditions. Despite concerns related to possible toxicity (perfluorooctane sulfonic acid was found to interact with DPPC, and may thus interfere with the lung surfactant's normal physiological function,<sup>121, 122</sup>) and propensity for bioaccumulation,<sup>123, 124</sup> fluorinated surfactants are technologically useful. They could potentially be used for biomedical applications that usually require small quantities and for which exemptions are allowed.<sup>124</sup> Provided their toxicity is fully assessed, fluorinated surfactants could contribute to tailoring lung surfactant formulation properties.

The miscibility of per- or partially fluorinated surfactants, including alcohols, acids and single-chain derivatives of phosphocholine with DPPC has been investigated.<sup>125-131</sup> Addition of the partially fluorinated (perfluorooctyl)pentanol (C<sub>8</sub>F<sub>17</sub>C<sub>5</sub>H<sub>10</sub>OH) to

DPPC-Hel 13-5 peptide mixtures yielded significant enhancement of surfactant recovery when submitted to repeated compression-expansion cycles, and allowed reaching very low surface tension values upon film compression (Table 1).<sup>132</sup> A mixed fluorocarbon/hydrocarbon ion pair compound (C<sub>8</sub>F<sub>17</sub>SO<sub>3</sub><sup>-</sup>(C<sub>2</sub>H<sub>5</sub>)<sub>3</sub>N<sup>+</sup>(CH<sub>2</sub>OCH<sub>2</sub>)<sub>10</sub>C<sub>16</sub>H<sub>33</sub>) was shown to reduce the inhibitory effect of fibrinogen by selectively interacting with DPPC and mimicking some of the surface properties of SP-C.<sup>133, 134</sup> In particular, it was found that fibrinogen could not penetrate in DPPC monolayers formed in the presence of this partially fluorinated compound.

## Conclusions

The design of exogenous surfactant preparations efficient for the treatment of pulmonary conditions that involve inactivation of the lung surfactant (ARDS/ALI, MAS) is still a challenge. Analogues of the specific surfactant proteins and simple peptides have shown potential in the treatment of ARDS/ALI. Addition of polymers to existing surfactant substitute formulations represents a cost-efficient and versatile approach. Further work is needed however to test the new polymer-containing formulations in appropriate animal models, examine the pulmonary fluid balance and the gas transfer properties. Liquid fluorocarbons, which have shown efficacy in liquid ventilation procedures, could be utilised in the form of targeted emulsions to deliver exogenous surfactant in zones of the lung where it is most needed. Use of fluorocarbon gases, which have demonstrated anti-inflammatory properties and surface activity, and would be easy to administer, certainly warrants preclinical investigations. The protecting effect of fluorocarbon gases against surfactant inhibitors other than albumin warrant further investigation. Fluorinated surfactants that have demonstrated resistance to inactivation by potent inhibitors show promise, as well as, possibly, combinations of fluorinated surfactants and fluorocarbon gases.

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## Notes and references

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1. L. B. Ware and M. A. Matthay, *New Engl. J. Med.*, 2000, 1334-1349.
2. H. W. Taeusch, J. Bernardino de la Serna, J. Perez-Gil, C. Alonso and J. A. Zasadzinski, *Biophys. J.*, 2005, **89**, 1769-1779.
3. A. Dushianthan, R. Cusack, V. Goss, A. D. Postle and M. P. W. Grocott, *Crit. Care*, 2012, **16**, 238-248.
4. R. Marshall, G. Bellingan and G. Laurent, *Thorax*, 1998, **53**, 815-817.
5. G. R. Bernard, A. Artigas, K. L. Brigham, J. Carlet, K. Falke, L. Hudson, M. Lamy, J. R. Legall, A. Morris and R. Spragg, *Am. J. Respir. Crit. Care Med.*, 1994, **149**, 818-824.



6. B. D. Kamath, E. R. MacGuire, E. M. McClure, R. L. Goldenberg and A. H. Jobe, *Pediatrics*, 2011, **127**, 1139-1146.
7. Y. Y. Zuo, R. A. W. Veldhuizen, A. W. Neumann, N. O. Petersen and F. Possmayer, *Biochim. Biophys. Acta*, 2008, **1778**, 1947-1977.
8. N. El-Gendy, A. Kaviratna, C. Berkland and P. Dhar, *Ther. Deliv.*, 2013, **4**, doi:10.4155/tde.4113.4172.
9. G. D. Rubinfeld, E. Caldwell, E. Peabody, J. Weaver, D. P. Martin, M. Neff, E. J. Stern and L. D. Hudson, *N. Engl. J. Med.*, 2005, **353**, 11685-11693.
10. R. E. Hoekstra, J. C. Jackson, T. F. Myers, I. D. Franz, M. E. Stern, W. F. Powers, M. Maurer, J. R. Raye, S. T. Carrier, J. H. Gunkel and A. J. Gold, *Pediatrics*, 1991, **88**, 10-18.
11. H. W. Taeusch, *Biol. Neonate*, 2000, **77**, 2-8.
12. J. G. Riess, *Chem. Rev.*, 2001, **101**, 2797-2920.
13. I. Tirotta, V. Dichiarante, C. Pigliacelli, G. Cavallo, G. Terraneo, F. B. Bombelli, P. Metrangola and G. Resnati, *Chem. Rev.*, 2015 **115**, 1106-1129.
14. R. H. Notter, *Lung surfactants: Basic Science and Clinical Applications*, Marcel Dekker, New York, 2000.
15. J. Perez-Gil, *Biochim. Biophys. Acta*, 2008, **1778**, 1676-1695.
16. S. Yu, P. G. Harding, N. Smith and F. Possmayer, *Lipids*, 1983, **18**, 522-529.
17. A. D. Postle, E. L. Heeley and D. C. Wilton, *Comp. Biochem. Physiol. A. Mol. Integr. Physiol.*, 2001, **129**, 65-73.
18. E. Parra and J. Perez-Gil, *Chem. Phys. Lipids*, 2015, **185**, 153-175.
19. J. Goerke, *Biochim. Biophys. Acta*, 1998, **1408**, 79-99.
20. F. Possmayer, *Am. Rev. Respir. Dis.*, 1990, **142**, 749-752.
21. J. R. Wright, *Nat. Rev. Immunol.*, 2005, **5**, 58-68.
22. H. Sano and Y. Kuroki, *Mol. Immunol.*, 2005, **42**, 279-287.
23. P. R. Lawson and K. B. Reid, *Immunol. Rev.*, 2000, **173**, 66-78.
24. A. G. Serrano and J. Perez-Gil, *Chem. Phys. Lipids*, 2006, **141**, 105-118.
25. J. Johansson and T. Curstedt, *Eur. J. Biochem.*, 1997, **244**, 675-676.
26. N. Wüstneck, R. Wüstneck, J. Perez-Gil and U. Pison, *Biophys. J.*, 2003, **84**, 1940-1949.
27. J. Johansson, *Biochim. Biophys. Acta*, 1998, **1408**, 161-172.
28. J. A. Zasadzinski, J. Ding, H. E. Warriner, F. Bringezu and A. J. Waring, *Curr. Opin. Colloid Interface Sci.*, 2001, **6**, 506-513.
29. S. Schürch, R. Qanbar, H. Bachofen and F. Possmayer, *Biol. Neonate*, 1995, **67**, 61-76.
30. J. Kesecioglu, R. Beale, T. E. Stewart, G. P. Findlay, J. J. Rouby, L. Holzapfel, P. Bruins, E. J. Steenken, O. K. Jeppesen and B. Lachmann, *Am. J. Respir. Crit. Care Med.*, 2009, **180**, 989-994.
31. H. Meng, Y. Sun, J. Lu, S. Fu, Z. Meng, M. Scott and Q. Li, *J. Cardiothorac. Vasc. Anesth.*, 2012, **26**, 849-856.
32. R. G. Spragg, J. F. Lewis, W. Wurst, D. Häfner, R. P. Baughman, M. D. Wewers and J. J. Marsh, *Am. J. Respir. Crit. Care Med.*, 2003, **167**, 1562-1566.
33. C. G. Cochrane, S. D. Revak, T. A. Merritt, G. P. Heldt, M. Hallman, M. D. Cunningham, D. Easa, A. Pramanik, D. K. Edwards and M. S. Alberts, *Am. J. Respir. Crit. Care Med.*, 1996, **153**, 404-410.
34. H. Nakahara, S. Lee, G. Sugihara, C.-H. Chang and O. Shibata, *Langmuir*, 2008, 3370-3379.
35. Y. Nakamura, K. Yukiatake, H. Nakahara, S. Lee, O. Shibata and S. Lee, *Biochim. Biophys. Acta* 2014, **1838**, 2046-2052.
36. J. M. van Zyl, J. Smith and A. Hawtrey, *Drug Des. Dev. Ther.*, 2013, **7**, 139-148.
37. J. A. Zasadzinski, P. C. Stenger, I. Shieh and P. Dhar, *Biochim. Biophys. Acta-Biomembranes*, 2010, **1798**, 801-828.
38. B. A. Holm, Z. Wang and R. H. Notter, *Pediatr. Res.*, 1999, **46**, 85-93.
39. A. Ishizaka, T. Matsuda, K. H. Albertine, H. Koh, S. Tasaka, N. Hasegawa, N. Kohno, T. Kotani, H. Morisaki, J. Takeda, M. Nakamura, X. H. Fang, T. R. Martin, M. A. Matthay and S. Hashimoto, *Am. J. Physiol. Lung Cell Mol. Physiol.*, 2004, **286**, L1088-L1094.
40. M. Hallman, V. Glumoff and M. Ramet, *Comp. Biochem. Physiol. A*, 2001, **129**, 287-294.
41. A. Günther, C. Ruppert, R. Schmidt, P. Markart, F. Grimminger, D. Walrath and W. Seeger, *Respir. Res.*, 2001, **2**, 353-364.
42. S. A. Tabak and R. H. Notter, *J. Colloid Interface Sci.*, 1977, **59**, 293-300.
43. B. A. Holm, R. H. Notter and J. N. Finkelstein, *Chem. Phys. Lipids*, 1985, **38**, 287-298.
44. B. A. Holm, G. Enhörning and R. H. Notter, *Chem. Phys. Lipids* 1988, **49**, 49-55.
45. B. A. Holm, A. R. Venkitaraman, G. Enhörning and R. H. Notter, *Chem. Phys. Lipids*, 1990, **52**, 243-250.
46. A. M. Cockshutt, J. Weitz and F. Possmayer, *Biochemistry*, 1990, **29**, 8424-8429.
47. A. R. Venkitaraman, S. B. Hall, J. A. Whitsett and R. H. Notter, *Chem. Phys. Lipids*, 1990, **56**, 185-194.
48. W. Seeger, C. Grube, A. Günther and R. Schmidt, *Eur. Respir. J.*, 1993, **6**, 971-977.
49. Z. Wang and R. H. Notter, *Am. J. Respir. Crit. Care Med.*, 1998, **158**, 28-35.
50. W. Friedrich, G. Schmalisch, P. A. Stevens and R. R. Wauer, *Eur. J. Med. Res.*, 2000, **19**, 277-282.
51. H. E. Warriner, J. Ding, A. J. Waring and J. A. Zasadzinski, *Biophys. J.*, 2002, **82**, 835-842.
52. J. A. Zasadzinski, T. F. Alig, C. Alonso, J. Bernardino de la Serna, J. Perez-Gil and H. W. Taeusch, *Biophys. J.*, 2005, **89**, 1621-1629.
53. M. Martínez Sarraza, A. Cimato, E. Rubin de Celis and G. Facorro, *Respir. Physiol. Neurobiol.*, 2011, **175**, 316-321.
54. K. Nag, A. Hillier, K. Parsons and F. M. Garcia, *Respir. Physiol. Neurobiol.*, 2007, **157**, 411-424.
55. J. Li, R. Sanders, K. McAdam, C. Hales, B. Thompson, J. Gelfand and J. Burke, *J. Trauma*, 1989, **29**, 1690-1697.
56. A. Saenz, A. Lopez-Sanchez, J. Mojica-Lazaro, L. Martinez-Caro, N. Nin, L. Bagatolli and C. Casals, *FASEB J.*, 2010, **24**, 3662-3673.
57. T. I. Yamada, M., B. L. Tabor and A. H. Jobe, *Am. Rev. Respir. Dis.*, 1990, **142**, 754-757.
58. B. Sun, T. Curstedt, G. Lindgren, B. Franzen, A. A. Alaiya, A. Calkovska and B. Robertson, *Eur. Respir. J.*, 1997, **10**, 1967-1974.
59. K. W. Lu, J. Perez-Gil, M. Echaide and H. W. Taeusch, *Biochim. Biophys. Acta*, 2011, **1808**, 2366-2373.
60. L. Gomez-Gil, D. Schürch, E. Goormaghtigh and J. Perez-Gil, *Biophys. J.*, 2009, **97**, 2736-2245.
61. Z. Wang, A. L. Schwan, L. L. Lairson, J. S. O'Donnell, G. F. Byrne, A. Foye, B. A. Holm and R. H. Notter, *Am. J. Physiol. Lung Cell. Mol. Physiol.*, 2003, **285**, L550-L559.
62. J. D. Amirkhanian, R. Bruni, A. J. Waring, C. Navar and H. W. Taeusch, *Biochim. Biophys. Acta*, 1993, **1168**, 315-320.
63. F. J. Walther, J. M. Hernandez-Juviel, P. E. Mercado, L. M. Gordon and A. J. Waring, *Biol. Neonate*, 2002, **8**, 181-187.
64. A. Sato and M. Ikegami, *PLoS ONE*, 2012, **7**, e39392.
65. M. Seehase, J. J. P. Collins, E. Kuypers, R. K. Jellena, D. R. M. G. Ophelders, O. L. Ospina, J. Perez-Gil, F. Bianco, R. Garzia, R. Razzetti and B. W. Kramer, *PLoS ONE*, 2012, **7**, e47631.



66. H. W. Taeusch, K. W. Lu, J. Goerke and J. A. Clements, *Am. J. Respir. Crit. Care Med.*, 1999, **164**, 1531-1536.
67. T. Kobayashi, K. Ohta, K. Tashiro, K. Nishizuka, W.-M. Chen, S. Ohmura and D. Yamamoto, *J. Appl. Physiol.*, 1999, **86**, 1778-1784.
68. K. Tashiro, X. Cui, T. Kobayashi, T. Curstedt and B. Robertson, *Biol. Neonate*, 2003, **83**, 49-56.
69. K. W. Lu, H. W. Taeusch, B. Robertson, J. Goerke and J. A. Clements, *Am. J. Respir. Crit. Care Med.*, 2000, **162**, 623-628.
70. I. Minkov, K. Mircheva, N. Grozev, T. Ivanova and I. Panaiotov, *Colloid Surf B: Biointerfaces*, 2013, **101**, 135-142.
71. P. C. Stenger, S. G. Isbell, D. St. Hillaire and J. A. Zasadzinski, *Langmuir* 2009, **25**, 10045-10050.
72. G. A. Georgiev, C. Vassilieff, A. Jordanova, A. Tsanovad and Z. Lancheva, *Soft Matter* 2012, **8**, 12072-12079.
73. E. M. Scarpelli, *Anat. Rec.*, 1998, **251**, 491-527.
74. N. Kang, Z. Policova, G. Bankian, M. L. Hair, Y. Y. Zuo, A. W. Neumann and E. J. Acosta, *Biochim. Biophys. Acta*, 2008, **1778** 291-302.
75. E. J. Acosta, Z. Policova, S. Lee, A. Dang, M. L. Hair and A. W. Neumann, *Biochim. Biophys. Acta*, 2010, **1798**, 489-497.
76. M. P. Krafft and J. G. Riess, *Chem. Rev.*, 2009, **109**, 1714-1792.
77. M. P. Krafft, *Acc. Chem. Res.*, 2012, **45**, 514-524.
78. M. P. Krafft and J. G. Riess, *J. Polymer. Sci. Polymer. Chem.*, 2007, **45**, 1185-1198.
79. E. S. Schutt, D. H. Klein, R. M. Mattrey and J. G. Riess, *Angew. Chem. Int. Ed.*, 2003, **42**, 3218-3235.
80. J. R. Lindner, *Nature Rev. Drug Disc.*, 2004, **3**, 527-532.
81. S. Sirsi and M. Borden, *Bubble Sci. Eng. Technol.*, 2009, **1**, 3-17.
82. E. Unger, T. Porter, J. Lindner and P. Grayburn, *Adv. Drug Delivery Rev.*, 2014, **72**, 110-126.
83. S. Schürch, *Respir. Physiol.*, 1982, **48**, 339-355.
84. J. G. Riess and M. P. Krafft, *Mater. Res. Soc. Bull.*, 1999, **24**, 42-48.
85. M. Schmutz, B. Michels, P. Marie and M. P. Krafft, *Langmuir*, 2003, **19**, 4889-4894.
86. P. N. Nguyen, T. T. Trinh Dang, G. Waton, T. Vandamme and M. P. Krafft, *ChemPhysChem*, 2011, **12**, 2646-2652.
87. L. C. Clark and F. Gollan, *Science*, 1966, **152**, 1755-1756.
88. L. C. Clark, S. Kaplan, F. Becattini and G. Benzing, *Fed. Proceed.*, 1970, **29**, 1764-1770.
89. D. G. Ashbaugh, D. B. Bigelow, T. Petty and B. E. Levine, *The Lancet*, 1967, 319-323.
90. M. R. Wolfson, N. E. Kechner, R. F. Roache, J. Dechadarevian, H. E. Friss, S. D. Rubenstein and T. H. Shaffer, *J. Appl. Physiol.*, 1998, **84**, 624-640.
91. C. L. Leach, J. S. Greenspan, D. Rubenstein, T. H. Shaffer, M. R. Wolfson, J. C. Jackson, R. DeLemos and B. P. Fuhrman, *New Engl. J. Med.*, 1996, **335**, 761-766.
92. M. Sukumar, M. Bommaraju, J. E. Fisher, F. C. Morin, M. C. Papo, B. P. Fuhrman, L. J. Hernan and C. L. Leach, *J. Appl. Physiol.*, 1998, **84**, 327-334.
93. A. S. Tütüncü, N. S. Faithfull and B. Lachmann, *Crit. Care Med.*, 1993, **21**, 962-969.
94. A. S. Tütüncü, K. Akpir, P. Mulder, W. Erdmann and B. Lachmann, *Anesthesiology*, 1993, **79**, 1083-1093.
95. R. B. Hirschl, A. Parent, R. Tooley, M. McCracken, K. Johnson, T. H. Shaffer and M. R. Wolfson, *Ann. Surg.*, 1995, **221**, 79-88.
96. R. B. Hirschl, T. Pranikoff, C. Wise, M. C. Overbeck, P. Gauger, R. J. Schreiner, R. Dechert and R. H. Bartlett, *J. Am. Med. Assoc.*, 1996, **275**, 383-389.
97. P. G. Gauger, T. Pranikoff, R. J. Schreiner, F. W. Moler and R. B. Hirschl, *Crit. Care Med.*, 1996, **24**, 16-22.
98. M. A. Croce, T. C. Fabian, J. H. Patton, S. M. Melton, M. Moore and L. L. Trentham, *J. Trauma*, 1998, **45**, 273-282.
99. T. Koch, M. Ragaller, D. Haufe, A. Hofer, M. Grosser, D. M. Albrecht, M. Kotzsch and T. Luther, *Anesthesiology*, 2001, **94**, 101-109.
100. J. U. Bleyl, M. Ragaller, U. Tschöhl, M. Regner, M. Hübner, M. Kanzow, O. Vincent and M. Albrecht, *Crit. Care Med.*, 2002, **30**, 1340-1347.
101. W. Burkhardt, S. Kraft, M. Ochs, H. Proquitté, L. Mense and M. Rüdiger, *PLoS ONE*, 2012, **7**, e47923.
102. R. V. Dimel, M. Walch, H. P. Haagsman and G. Putz, *Crit. Care Med.*, 2002, **30**, 1083-1090.
103. M. F. Krause, C. Jäckel, J. Haberstroh, J. Schulte-Möntig, J. U. Leitis and M. Orłowska-Volk, *Pediatr. Res.*, 2001, **50**, 34-43.
104. A. Hartog, D. Gommers, J. J. Haitsma and B. Lachmann, *Br. J. Anaesth.*, 2000, **2000**, 752-756.
105. S. E. Chappell, M. Wolfson and T. Shaffer, *Respir. Med.*, 2001, **95**, 612-617.
106. S. Wolf, H. Lohbrunner, T. Busch, A. Sterner-Kock, M. Deja, A. Sarrafzadeh, U. Neumann and U. Kaisers, *Br. J. Anaesth.*, 2001, **87**, 593-601.
107. M.-J. Jeng, Y. R. Kou, C.-C. Sheu and B. Hwang, *Crit. Care Med.*, 2003, **31**, 1166-1174.
108. J. D. Mrozek, K. M. Smith, S. C. Simonton, D. R. Bing, P. A. Meyers, J. E. Connett and M. C. Mammel, *Crit. Care Med.*, 1999, **27**, 1916-1922.
109. F. Gerber, M. P. Krafft, T. F. Vandamme, M. Goldmann and P. Fontaine, *Angew. Chem. Int. Ed.*, 2005, **44**, 2749-2752.
110. F. Gerber, M. P. Krafft, T. F. Vandamme, M. Goldmann and P. Fontaine, *Biophys. J.*, 2006, **90**, 3184-3192.
111. C. M. Knobler and R. C. Desai, *Annu. Rev. Phys. Chem.*, 1992, **43**, 207-236.
112. M. P. Krafft, V. B. Fainerman and R. Miller, *Prog. Colloid Polym Sci.*, 2015, accepted.
113. F. Gerber, M. P. Krafft and T. F. Vandamme, *Biochim. Biophys. Acta - Biomembranes*, 2007, **1768**, 490-494.
114. P. N. Nguyen, G. Waton, T. Vandamme and M. P. Krafft, *Soft Matter*, 2013, **9**, 9972-9976.
115. P. N. Nguyen, M. Veschgini, M. Tanaka, G. Waton, T. Vandamme and M. P. Krafft, *Chem. Commun.*, 2014, **50**, 11576-11579.
116. P. N. Nguyen, G. Waton, T. Vandamme and M. P. Krafft, *Angew. Chem. Int. Ed.*, 2013, **52**, 6404-6408.
117. S. Lee, D. H. Kim and D. Needham, *Langmuir*, 2001, **17**, 5544-5550.
118. G. Yang, M. O'Duill, V. Gouverneur and M. P. Krafft, *Angew. Chem. Int. Ed.*, 2015, DOI: 10.1002/anie.201502677R2.
119. A. B. Kharge, Y. Wu and C. E. Perlman, *J. Appl. Physiol.*, 2014, **117**, 440-451.
120. S. Sirsi, C. Pae, D. K. T. Oh, H. Blomback, A. Koubaa, B. Papahadjopoulos-Sternberg and M. Borden, *Soft Matter*, 2009, **5**, 4835-4842.
121. S. M. Vyas, J. Turánek, P. Knötigová, A. Kašná, V. Kvardová, V. Koganti, S. E. Rankin, B. Knutson and H.-J. Lehmler, *New J. Chem.*, 2006, **30**, 944-951.
122. C. Lau, K. Anitole, C. Hodes, D. Lai, A. Pfahles-Hutchens and J. Seed, *Toxicol. Sci.*, 2007, **99**, 366-394.
123. C. Lau, *Reprod. Toxicol.*, 2012, **33**, 405-409.
124. M. P. Krafft and J. G. Riess, *Chemosphere*, 2015, **129**, 4-19.
125. H. Lehmler, M. Jay and P. Bummer, *Langmuir*, 2000, **16**, 10161-10166.

126. T. Hiranita, S. Nakamura, M. Kawachi, H. M. Courrier, T. F. Vandamme, M. P. Krafft and O. Shibata, *J. Colloid Interf. Sci.*, 2003, **265**, 83-92.
127. H. Nakahara, S. Nakamura, H. Kawasaki and O. Shibata, *Colloids Surf. B*, 2005, **41**, 285-298.
128. H. J. Lehmler and P. M. Bummer, *Colloids Surf. B*, 2005, **44**, 74-81.
129. S. Nakamura, H. Nakahara, M. P. Krafft and O. Shibata, *Langmuir*, 2007, **23**, 12634-12644.
130. H. Nakahara, S. Lee, M. P. Krafft and O. Shibata, *Langmuir*, 2010, **26**, 18256-18265.
131. A. Eftaiha, S. M. K. Brunet and M. F. Paige, *Langmuir*, 2012, **28**, 15150-15159.
132. H. Nakahara, M. P. Krafft, A. Shibata and O. Shibata, *Soft Matter*, 2011, **7**, 7325-7333.
133. N. Aydogan, B. Uslu and H. Tanaci, *J. Colloid Interface Sci.*, 2011, **360**, 163-174.
134. G. U. Dilli, H., B. Uslu and N. Aydogan, *Colloid Surf B: Biointerfaces*, 2014, **122**, 566-575.