

RSC Advances



This is an *Accepted Manuscript*, which has been through the Royal Society of Chemistry peer review process and has been accepted for publication.

Accepted Manuscripts are published online shortly after acceptance, before technical editing, formatting and proof reading. Using this free service, authors can make their results available to the community, in citable form, before we publish the edited article. This *Accepted Manuscript* will be replaced by the edited, formatted and paginated article as soon as this is available.

You can find more information about *Accepted Manuscripts* in the [Information for Authors](#).

Please note that technical editing may introduce minor changes to the text and/or graphics, which may alter content. The journal's standard [Terms & Conditions](#) and the [Ethical guidelines](#) still apply. In no event shall the Royal Society of Chemistry be held responsible for any errors or omissions in this *Accepted Manuscript* or any consequences arising from the use of any information it contains.

1 **Simultaneous determination of two flavonoids based on disulfide linked**
2 **β -cyclodextrin dimer and Pd clusters functionalized graphene-modified electrode**

3
4
5 Xin Ran^{a,1}, Long Yang^{a,1}, Genfu Zhao^a, Hanzhang Ye^a, Yanqiong Zhang^a, Shuangmei
6 Fan^a, Xiaoguang Xie^{a,*}, Hui Zhao^{b,*}, Can-Peng Li^{a,*}

7
8
9 ^a School of Chemical Science and Technology, Yunnan University, Kunming 650091,
10 PR China.

11 ^b Laboratory for Conservation and Utilization of Bio-resource, Yunnan University,
12 Kunming 650091, PR China.

13
14
15
16
17
18 ¹These authors contributed equally to this work.

19 * Corresponding authors.

20 Fax or Tel: 86-871-65031119. E-mail: xgxie@ynu.edu.cn (X. xie);

21 zhaohyau@yahoo.com.cn (H. Zhao); lcppp1974@sina.com (C.-P. Li)

22

23 **Abstract:** In the present work, ultrafine Pd clusters with a uniform size of ~2.0 nm
24 were monodispersed on the surface of reduced graphene oxide (RGO) using a clean
25 and green approach in the absence of additional reductants and surfactants. Disulfide
26 linked β -cyclodextrin dimer (SS- β -CD) was non-covalently bonded to the surface of
27 Pd@RGO. By combining the merits of Pd@RGO and the SS- β -CD, a highly sensitive
28 electrochemical sensing platform was developed based on the SS- β -CD-Pd@RGO
29 nanohybrids. Electrochemical simultaneous detection of baicalin and luteolin using
30 SS- β -CD-Pd@RGO nanohybrids-modified electrode is described for the first time.
31 The SS- β -CD showed higher supramolecular recognition capability than the native
32 β -CD, which may be caused by the cooperative binding abilities of two adjacent CD
33 units. Due to the synergistic effects from the Pd@RGO (*e.g.* the good electrochemical
34 properties and large surface area) and SS- β -CD (*e.g.* a hydrophilic external surface, a
35 high supramolecular recognition, and a good enrichment capability), the
36 SS- β -CD-Pd@RGO modified electrode was found to have linear response ranges of
37 0.02–20.00 μ M for baicalin and 0.01–10.00 μ M for luteolin with relatively low
38 detection limits of 0.0052 μ M for baicalin and 0.0070 μ M for luteolin, respectively.
39 The results indicated that SS- β -CD-Pd@RGO nanohybrids are excellent sensing
40 materials for the electrochemical determination of flavonoids. The proposed method
41 could be successfully utilized to detect baicalin and luteolin in serum samples, and
42 exhibited a promising application in practice.

43

44 **1. Introduction**

45 Flavonoids, plant polyphenolic compounds abundant in fruits and vegetables,
46 exhibit a wide variety of biochemical and pharmacological effects, including
47 antioxidant free-radical scavenging, anti-inflammatory, anti-carcinogenic, etc. ¹ In
48 plants, they are utilized in response to microbial infection. However, in animals and
49 humans, flavonoids protect cells against damage caused by reactive oxygen species. ²
50 Moreover, they have the capacity to inhibit the growth of a wide range of bacteria via
51 disruption of bacterial cell walls following by their complexation with the
52 extracellular soluble protein components. ³ Flavonoids also exert anti-viral actions
53 due to their favourable oxidation potentials. ⁴ Baicalin (**Scheme 1A**) and luteolin
54 (**Scheme 1B**), belonging to the class flavonoids, are two important anti-inflammatory
55 and anticancer drugs, which are widely used in medical practice. As a result of the
56 above pharmacological effects, different kinds of concentrated composite herbal
57 preparations that contain baicalin and luteolin as the active component have been used
58 clinically as therapeutical medicine. Besides, a lot of health functional foods and
59 different beverages usually contain baicalin and luteolin. Therefore, establishment of
60 highly sensitive analytical techniques for the determination of baicalin and luteolin is
61 of great significance in clinics, pharmaceuticals, and functional foods. So far, several
62 methods such as thin layer chromatography, ⁵ capillary electrophoresis, ^{6,7} GC, ^{8,9}
63 HPLC, ¹⁰⁻¹² fluorimetry, ¹³ and LC-MS ^{14,15} have been developed for the analysis of
64 baicalin and luteolin. Although these methods have advantages of sensitivity and
65 accuracy, their high cost and complicated operation limit their extensive application.
66 Electrochemical detection is an attractive alternative to these techniques because it

67 features high sensitivity, instrument simplicity, fast response, low cost, and feasibility
68 of miniaturization. Although the electrochemical methods have been reported for
69 determination of the different type of flavonoids,¹⁶⁻²¹ to the best of our knowledge,
70 there are no reports yet for simultaneous determination of baicalin and luteolin by an
71 electrochemical method.

72 Noble metals with ultrafine sizes have attracted considerable attention because of
73 their large surface areas and high number of edge and corner atoms that enhance the
74 catalytic properties of noble metal nanocomposites.^{22,23} Therefore, the synthesis of
75 small metal particles with high accessible surface areas is a worthwhile endeavor.
76 Unfortunately, surface energies increase with decreased noble metal particle size,
77 leading to serious aggregation of small particles.^{24,25} Particularly, the synthesis of
78 small sized particles with the sizes of less than 2 nm, which are also known as clusters
79 differentiating from nanoparticles (NPs) due to their small sizes and narrow size
80 distribution, represents many more challenges because of its high requirement of
81 control over the nucleation and growth processes compared with that of NPs.^{26,27}
82 Thus, the metal particles were usually anchored to suitable supports to overcome the
83 aggregation.^{27,28} Graphene, which is a robust 2D sheet of sp²-hybridized carbon, is
84 the most promising one among all the available support materials.²⁹ Pd cluster and its
85 composite are widely used for many applications because of their lower cost than
86 other noble metals.³⁰ Research based on first-principles calculations indicates that Pd
87 could interact with and bind more strongly to graphene because more interaction
88 states and transmission channels are generated between them and because Pd tends to

89 grow into three-dimensional structures on graphene surfaces.²⁵ This provides a hint
90 that graphene could be an ideal substrate for growing and anchoring Pd clusters for
91 high-performance electrocatalytic or electrochemical devices.

92 Supramolecular host–guest recognition based on noncovalent interaction has
93 attracted great attention in nowadays, which has been widely employed to develop
94 different electrochemical sensors by modifying organic macrocyclic hosts on various
95 electrodes.^{18,31-38} Cyclodextrins (CDs), as the typical macrocyclic molecules, are
96 oligosaccharides composed of six, seven, or eight glucose units (α -, β -, γ -CD,
97 respectively), which are toroidal in shape with a hydrophobic inner cavity and a
98 hydrophilic exterior and are capable of forming inclusion complexes with a wide
99 variety of hydrophobic guests.^{39,40} Graphene is a material that holds great promise for
100 potential applications in many technological fields because of its high surface area,
101 low cost, and high conductivity.^{36,39} It has been reported that the composites of CDs
102 and graphene could be formed by van der Waals force, hydrogen-bonding, and
103 hydrophobic interaction.^{34,37,39} A graphene that is functionalized with CDs is likely to
104 obtain new functionalized materials that simultaneously possess the unique properties
105 of graphene (*e.g.* high electrical conductivity and large surface area) and CDs (*e.g.*
106 high supramolecular recognition and good enrichment capability). Thus, the
107 integration of graphene and CDs can be potentially applied in the field of
108 electrochemical sensing or biosensing. As a recently developing family of CD
109 derivatives, bridged bis(β -CD)s exhibit significantly enhanced binding abilities and
110 molecular recognition through the cooperative binding of two adjacent CD units in

111 comparison with native CDs.^{41,42} Therefore, considerable efforts have been devoted
112 in this field to design and synthesize various CD dimers with considerable structural
113 diversity to achieve the enhanced binding abilities.⁴³ Hence, diverse functional
114 groups such as organoseleniums,⁴⁴ disulfides,⁴⁵ pyridines,^{46,47} ethylene glycol,⁴⁸
115 aromatic diamine,⁴⁹ and pyrene⁵⁰ have been used as the linker between two CD units.
116 Unexpectedly, their molecular recognition behaviors have not been extensively
117 investigated. In addition, these bridged bis(β -CD)s are rarely employed to construct
118 electrochemical sensing or biosensing platforms.

119 In the present paper, ultrafine Pd clusters with a uniform size of ~ 2.0 nm were
120 monodispersed on the surface of reduced graphene oxide (RGO) using a clean and
121 green approach in the absence of additional reductants and surfactants. The disulfide
122 linked β -cyclodextrin dimer (SS- β -CD) was non-covalently bonded to the surface of
123 Pd@RGO. By combining the merits of Pd@RGO and the SS- β -CD, a highly sensitive
124 electrochemical sensing platform was developed based on the SS- β -CD-Pd@RGO
125 nanohybrids. The designed electrochemical sensing platform is illustrated in **Scheme**
126 **2**. Two flavonoid compounds, namely, baicalin and luteolin were chosen as
127 simultaneous probes to verify the performance of the SS- β -CD-Pd@RGO
128 nanohybrids.

129

130 **2. Materials and methods**

131 **2.1 Chemicals**

132 Graphite oxide was purchased from Nanjing XFNANO Materials Tech Co., Ltd.

133 (Nanjing, China). PdCl₂ and β-CD were obtained from Sigma Chemical Co. (St.
134 Louis, MO, USA). Thiol-β-cyclodextrin (SH-β-CD) was purchased from Shandong
135 Binzhou Zhiyuan Bio-Technology Co., Ltd (Shandong, China). Baicalin and luteolin
136 were obtained from Aladdin Chemical Reagent Co., Ltd. All aqueous solutions were
137 prepared with deionized water (DW, 18 MΩ cm). All other reagents were of analytical
138 grade.

139

140 **2.2 Apparatus**

141 Electrochemical impedance spectroscopy (EIS) and differential pulse
142 voltammetry (DPV) experiments were performed with a CHI 660E Electrochemical
143 Workstation from Shanghai Chenhua Instrument (Shanghai, China) and conducted
144 using a three-electrode system, with the modified GCE as working electrode, a
145 platinum wire as the counter electrode, a saturated calomel electrode (SCE) as the
146 reference electrode. The morphologies of the prepared samples were characterized by
147 a QUNT200 scanning electron microscopy (SEM, USA) and a JEM 2100
148 transmission electron microscopy (TEM, Japan). UV–visible spectra were analyzed in
149 a U-2001 Hitachi (Tokyo, Japan) UV spectrophotometer. Fourier transform infrared
150 (FTIR) study was performed over the wavenumber, range of 4000–400 cm⁻¹ by a
151 Thermo Fisher SCIENTIFIC Nicolet IS10 (Thermo Fisher, Massachusetts, USA)
152 FTIR impact 410 spectrophotometer using KBr pellets. Thermogravimetric analysis
153 (TGA) was carried out on a Q50 TGA (TA Instruments, New Castle, DE, USA), at a
154 heating rate of 5 °C min⁻¹ from 25 to 800 °C in argon.

155

156 **2.3 UV-vis spectroscopic measurements**

157 Inclusion complexes formation of baicalin/SS- β -CD, baicalin/ β -CD,
158 luteolin/SS- β -CD, and luteolin/ β -CD were studied in DW using the spectral shift
159 method. The concentration of baicalin and luteolin were kept constant at 50 μ M, the
160 SS- β -CD concentration was 0.36 mM, while the β -CD concentration was 0.72 mM.
161 Initially, stock solutions of baicalin, luteolin, SS- β -CD, and β -CD in DW were
162 prepared. Aliquots from each solution were transferred to a 25 mL volumetric flask
163 and the volume was made up using DW so that the required concentrations are
164 obtained. The prepared solutions were stirred for 30 min at room temperature, filtered
165 through 0.45 μ m membrane filter, and the UV-vis absorption spectra were recorded in
166 the wavelength range from 200 to 500 nm against blank solutions containing the same
167 concentrations of SS- β -CD or β -CD. The recorded spectra were compared to the
168 spectrum of free baicalin or luteolin.

169

170 **2.4 Preparation of the RGO**

171 The graphite oxide was exfoliated in to graphene oxide (GO) sheets by
172 ultrasonication at room temperature for 1 h. The as-obtained yellow-brown aqueous
173 suspension of GO was stored at room temperature and used for further experiment.
174 Compared with the traditional procedure using highly toxic hydrazine as reductant, a
175 green approach was adopted to prepare RGO reported by Fan et al.⁵¹ with some
176 modifications. In a typical experiment, the pH of 50.0 mL of 0.5 mg mL⁻¹ GO

177 aqueous suspension was adjusted to 11.0 using 1.0 M NaOH. Then it was transferred
178 to a round bottom flask and stirred at 90 °C in an oil bath for 5.0 h. After cooling to
179 room temperature, the resulting stable black dispersion was centrifuged at 16000 rpm
180 and washed with DW for three times. Finally, the RGO material was obtained by
181 freeze-drying.

182

183 **2.5 Preparation of the Pd@RGO**

184 For preparation of the Pd@RGO material, 10.0 mg RGO was dispersed into 20.0
185 mL of DW via sonication. Then 0.80 mL of 5.0 mM PdCl₂ aqueous solution was
186 added to the RGO suspension dropwise and stirred in an ice bath for 0.5 h. After
187 centrifuging and washing with DW for three times, the resulting Pd@RGO was
188 obtained by freeze-drying.

189

190 **2.6 Synthesis of SS-β-CD dimer**

191 SS-β-CD dimer was synthesized using the method reported by Tang and
192 co-workers.⁵² Briefly, the SH-β-CD (2.0 g) was dissolved in 10% H₂O₂ (25 mL) by
193 heating, and the mixture was stirred at room temperature for 5 h. A white precipitate
194 was obtained after the solvent was added to acetone. The precipitate was filtered.
195 After evaporation of acetone and water in vacuo, SS-β-CD dimer was obtained. The
196 yield of the SS-β-CD was calculated to be 94.1%.

197

198 **2.7 Preparation of the SS-β-CD-Pd@RGO nanohybrids**

199 The fabrication of the SS- β -CD-Pd@RGO nanohybrid was carried out by
200 sonicating 10 mg of Pd@RGO in 20 mL of 0.5 mg mL⁻¹ SS- β -CD at room
201 temperature for 2 h and stirred for another 10 h. Finally, the resulting stable black
202 suspension was centrifuged and washed with DW for three times to remove unbound
203 SS- β -CD, and then lyophilized to obtain SS- β -CD-Pd@RGO nanohybrid. The
204 β -CD-Pd@RGO composite was prepared using the similar procedure by replacing
205 SS- β -CD with native β -CD.

206

207 **2.8 Preparation of the modified electrodes**

208 GC electrode (3 mm in diameter) was polished with 0.3 and 0.05 μ m Al₂O₃
209 powder respectively and subsequently sonicated in ethanol and DW to remove the
210 adsorbed substance and dried in air. The SS- β -CD-Pd@RGO was dispersed in DW at
211 a concentration of 0.5 mg mL⁻¹ with the aid of ultrasonic agitation for 20 min,
212 resulting in a homogeneous suspension. To prepare the SS- β -CD-Pd@RGO modified
213 electrode, 5 μ L of the SS- β -CD-Pd@RGO suspension was dropped onto the electrode
214 surface and dried at room temperature. The obtained electrode was noted as
215 SS- β -CD-Pd@RGO/GC electrode. The β -CD-Pd@RGO/GC, Pd@RGO/GC, and
216 RGO/GC electrodes were prepared in the same way.

217

218 **2.9 Electrochemical measurements**

219 Before electrochemical measurements, the RGO/GC, Pd@RGO/GC,
220 β -CD-Pd@RGO/GC, and SS- β -CD-Pd@RGO/GC electrodes were electrochemically

221 reduced in 0.1 M phosphate buffer (PBS, pH 7.0) by cycling the potential between 0
222 and -1.4 V for 15 cycles. Prior to the electrochemical reduction, the PBS was
223 completely saturated with nitrogen gas to remove the dissolved oxygen. After that,
224 DPV was carried out 0.1 M PBS (pH 3.0) containing different concentrations of
225 baicalin and luteolin by scanning the potential from 0.0 to 0.7 V with an amplitude of
226 0.05 V and a pulse width of 0.05 s. EIS was recorded in the frequency range from 10^1
227 to 10^5 Hz with an amplitude of 5 mV using 2.0 mM $[\text{Fe}(\text{CN})_6]^{3-/4-}$ redox couple (1:1)
228 with 0.1 M KCl as supporting electrolyte. All the measurements were carried out at
229 room temperature.

230

231 **3. Results and Discussion**

232 **3.1 UV-vis spectroscopic measurements**

233 The UV-vis spectroscopy was used to investigate the interactions between baicalin
234 and SS- β -CD or β -CD. As shown in **Fig. 1A**, the baicalin shows two strong
235 absorptions at 277 and 318 nm, respectively. The two absorbances increased slightly
236 when the β -CD was added to the aqueous solution of baicalin. However, significant
237 increases of the two absorbances were observed when the SS- β -CD was added to the
238 aqueous solution of baicalin. Complexation of baicalin with SS- β -CD exhibited
239 greatly enhanced absorbances compared to the complexation with native β -CD. The
240 luteolin shows two strong absorptions at 269 and 352 nm, respectively, as shown in
241 **Fig. 1B**. Similar to baicalin, complexation of luteolin with SS- β -CD exhibited greatly
242 enhanced absorbances compared to the complexation with native β -CD. The enhanced

243 absorbances was caused by the cooperative binding of two adjacent hydrophobic
244 cavities with baicalin in SS- β -CD.^{41,43,53}

245

246 **3.2 Characterization of the SS- β -CD-Pd@RGO nanohybrids**

247 The SEM image of RGO was obtained as shown in **Fig. S1**. The microstructure
248 image reveals that the RGO material consists of randomly aggregated thin, wrinkled
249 sheets closely associated with each other. The morphologies and microstructures of
250 Pd@RGO was investigated by TEM observation as shown in **Figs. 2A–C**. The most
251 striking feature is that the Pd clusters with a uniform size \sim 2.0 nm are fairly well
252 monodispersed on the surface of RGO. The driving force for Pd clusters deposition on
253 RGO could be caused by the redox reaction between Pd²⁺ and RGO. The RGO is the
254 electron donors or the reductants for subsequent Pd cluster growth on the RGO
255 surface. Previous reports have explored that both single-wall carbon nanotubes
256 (SWNTs)⁵⁴ and GO²⁵ could, respectively, reduce AuCl₄³⁻ and PdCl₄²⁻ to generate Au
257 NPs and Pd NPs without any additional reductant. These phenomena are explained by
258 the difference in the redox potentials of AuCl₄³⁻ ions and SWNTs (0.5 V vs SCE) or
259 PdCl₄²⁻ and GO (0.48 V vs SCE), which facilitates the reduction of noble metal ions.
260 Similar to these carbon materials, RGO is also good reducing agents for the formation
261 of Pd@RGO nanocomposites. The small size of Pd clusters deposited on the RGO
262 surface indicates that the remaining oxygen-containing groups, (generally the
263 graphene produced via the reduction method has some oxygen-containing groups),
264 may play an important role in controlling the formation of Pd clusters through

265 increasing the anchoring ability of Pd nuclei on the RGO surface and avoiding
266 Ostwald ripening following nuclei.²⁵ The β -CD-Pd@RGO and
267 SS- β -CD-Pd@RGO nanohybrids were characterized by FTIR and TGA analysis. **Fig.**
268 **2D** shows the FTIR spectra of the RGO, β -CD-Pd@RGO, and SS- β -CD-Pd@RGO
269 materials. It is found that the FTIR spectrum of RGO is essentially featureless except
270 some weak absorptions of the remaining oxygen-containing groups. Whereas the
271 FTIR spectra of β -CD-Pd@RGO and SS- β -CD-Pd@RGO exhibit the typical CD
272 absorption features of the coupled C–O–C stretching/O–H bending vibrations at 1204
273 cm^{-1} , the coupled C–O/C–C stretching/O–H bending vibrations at 1090 cm^{-1} , and
274 O–H stretching vibrations at 3435 cm^{-1} . The presence of these peaks confirmed that
275 the β -CD and SS- β -CD molecules were successfully attached to the surface of the Gra.
276 The prepared SS- β -CD-Pd@RGO and the related materials were also characterized
277 by TGA, as shown in **Fig. 2E**. For the pristine RGO, there is a minor loss in mass
278 (24%) at a temperature of approximately 600 °C owing to the pyrolysis of a small
279 amount of the labile oxygen-containing functional groups. The β -CD-Pd@RGO
280 material exhibited an abrupt mass loss when the temperature was approximately 260
281 °C because of the decomposition of β -CD; the mass loss reached about 60 wt% when
282 the temperature was 600 °C. Similarly, the SS- β -CD-Pd@RGO nanohybrid also
283 exhibited an abrupt mass loss when the temperature was approximately 260 °C owing
284 to the decomposition of SS- β -CD; the mass loss reached approximately 61 wt% when
285 the temperature was 600 °C. The amount of β -CD and SS- β -CD grafted to RGO were
286 estimated to be approximately 36.0% and 37.0%, respectively. It should be noted here

287 that the amount of SS- β -CD attached to RGO is approximately equal to that of β -CD.

288

289 3.3 Electrochemical characterization of the modified electrodes

290 The value of the charge transfer resistance (R_{ct}) of the modified electrode was
291 estimated by the semicircle diameter. **Fig. 2F** illustrates the EIS of the bare GCE,
292 RGO/GCE, Pd@RGO/GCE, β -CD-Pd@RGO/GCE, and SS- β -CD-Pd@RGO/GCE.
293 Obviously, the bare GCE exhibited a semicircle portion and the value of R_{ct} was
294 estimated to be approximately 800 Ω . While the R_{ct} decreased dramatically, nearly to
295 zero at RGO/GCE, indicating that RGO/GCE formed high electron conduction
296 pathways between the electrode and electrolyte. When the Pd@RGO modified on the
297 bare GCE, the semicircle decreased further, revealing that Pd clusters with excellent
298 conductivity can facilitate the electron transfer. For the β -CD-Pd@RGO/GCE and
299 SS- β -CD-Pd@RGO/GCE, their semicircles both increased to approximately 1500 Ω .
300 This is because of the β -CD or SS- β -CD layer hindered the electron transfer and made
301 the interfacial charge transfer difficult. The β -CD and SS- β -CD are successfully
302 immobilized of on the graphene, which was directly proved by the TGA analysis. The
303 increased R_{ct} is not a direct proof that β -CD or SS- β -CD are immobilized on the
304 grapheme. but it can be a auxiliary evidence.

305 The kinetics of the electrode reactions was investigated by studying the effect of
306 scan rate at the SS- β -CD-Pd@RGO/GCE using 2.0 mM $[\text{Fe}(\text{CN})_6]^{3-/4-}$ redox couple
307 (1:1) with 0.1 M KCl as supporting electrolyte. As shown in **Fig. S2A**, both anodic
308 peak current (I_{pa}) and cathodic peak current (I_{pc}) increased with the increase of scan

309 rate in the range of 50–400 mV s^{-1} . Also, the I_{pa} and I_{pc} showed a linear relationship
310 with the scan rate respectively (**Fig. S2B**), suggesting that the electrode reaction is a
311 adsorption-controlled electrochemical process.⁵⁵ It can be seen that both I_{pa} and I_{pc} of
312 the modified electrode increased linearly and were proportional to the scan rate
313 according to Eqs. $I_{\text{pa}} (\mu\text{A}) = 0.30 v (\text{mV/s}) + 36.3$ and $I_{\text{pc}} (\mu\text{A}) = -0.27 v (\text{mV/s}) -$
314 65.3 . The separation of peaks suggests that the process is not perfectly reversible;
315 however, stable redox peak current and position during repeated scans at a particular
316 scan rate suggests that the SS- β -CD-Pd@RGO/GCE exhibit a quasi-reversible
317 process.⁵⁶ Moreover, both anodic peak potential (E_{pa}) and cathodic peak potential (E_{pc})
318 demonstrated a linear relationship with the scan rate respectively (**Fig. S2C**),
319 indicating that the electron transport from redox moieties to the electrode is very
320 facile.⁵⁷

321

322 **3.4 Electrochemical behavior of baicalin and luteolin on the modified electrodes**

323 The electrochemical behaviors of baicalin and luteolin toward the modified
324 electrodes were investigated using CV and DPV. The CVs for the oxidation and
325 reduction of 20 μM baicalin at bare GCE, RGO/GCE, Pd@RGO/GCE,
326 β -CD-Pd@RGO/GCE, and SS- β -CD-Pd@RGO/GCE were obtained in 0.1 M PBS
327 (pH 3.0) as shown in **Fig. 3A**. Enhanced redox currents of baicalin using the
328 RGO-modified GCE were observed in comparison with that in the bare GCE. This
329 increase indicated that the high surface area and high conductivity of the RGO
330 increased the effective electrode area and improved the electroactivity towards

331 baicalin oxidation and reduction. Another reason for the enhancement of the currents
332 at the RGO-modified GCE is considered to be the π - π interaction between the
333 baicalin and the RGO film on the GCE.⁵⁸ In the case of Pd@RGO/GCE, the redox
334 currents of baicalin were enhanced compared with that of the RGO-modified GCE,
335 indicating that Pd clusters with excellent conductivity can amplify the electrochemical
336 signal. Generally, an increase in the peak current and a decrease in the peak potential
337 could be ascribed to the electrocatalysis. However, the peak potential here is almost
338 no change. Recently, Compton et al. reported that the electrochemical reaction at a
339 thin film-modified electrode being facilitated without a change in the electrochemical
340 rate constant could be considered to alter the solubilities and diffusion coefficients of
341 the electroactive species.⁵⁹ Thus, the enhancement of the redox currents at
342 Pd@RGO/GCE may also be caused by the altered solubilities or diffusion coefficients
343 of the electroactive species. In addition, the redox currents increased remarkably
344 when the β -CD-Pd@RGO nanohybrid was immobilized onto the surface of GCE.
345 This may be attributed to the β -CD molecules with excellent supramolecular
346 recognition capability that formed inclusion complexes with baicalin. Interestingly,
347 due to the cooperative binding abilities of two adjacent CD units, the redox currents
348 of baicalin at SS- β -CD-Pd@RGO/GCE increased dramatically. This result
349 demonstrated that SS- β -CD possesses higher supramolecular recognition capability
350 than the native β -CD. The CVs for the oxidation and reduction of 10 μ M luteolin at
351 bare GCE, RGO/GCE, Pd@RGO/GCE, β -CD-Pd@RGO/GCE, and
352 SS- β -CD-Pd@RGO/GCE in 0.1 M PBS (pH 3.0) were also obtained as shown in **Fig.**

353 **3B**. Similar to baicalin, the redox currents of luteolin at the modified electrodes
354 increased in sequence. As can be seen, the peak to peak potential difference both for
355 baicalin and luteolin in **Fig. 3A and B** that were close to 0 mV, indicated that the
356 process was adsorption controlled.⁵⁵

357 **Fig. S3A** shows the CVs of 20 μM baicalin at SS- β -CD-Pd@RGO/GCE for
358 different scan rates. The accumulation condition was carried out at -0.2 V for 200 s.
359 Both anodic peak current (I_{pa}) and cathodic peak current (I_{pc}) increase gradually with
360 an increase in scan rate. As shown in **Fig. S3B**, the peak current increases linearly
361 with the scan rate in the 50 to 400 mV s^{-1} range, and the equation can be expressed as
362 $I_{\text{pa}} (\mu\text{A}) = 0.136 v (\text{mV/s}) + 9.15$ ($R^2 = 0.9985$) and $I_{\text{pc}} (\mu\text{A}) = -0.042 v (\text{mV/s}) +$
363 0.757 . The representation of redox peak current vs. scan rate was linear, indicating
364 that in this case, the process was adsorption controlled.⁵⁵ In addition, both anodic
365 peak potential (E_{pa}) and cathodic peak potential (E_{pc}) demonstrated a linear
366 relationship with the scan rate respectively (**Fig. S3C**).

367 Similarly, the effect of scan rate on the redox of luteolin was also studied. **Fig.**
368 **S4A** shows the CVs of 10 μM luteolin at SS- β -CD-Pd@RGO/GCE for different scan
369 rates. As shown in **Fig. S4B**, both anodic peak current (I_{pa}) and cathodic peak current
370 (I_{pc}) increase linearly with the scan rate in the 50 to 400 mV s^{-1} range, and the
371 equation can be expressed as $I_{\text{pa}} (\mu\text{A}) = 0.155 v (\text{mV/s}) + 10.59$ ($R^2 = 0.9985$) and I_{pc}
372 ($\mu\text{A}) = -0.146 v (\text{mV/s}) - 7.05$, indicating that the redox of luteolin on
373 SS- β -CD-Pd@RGO/GCE is a typical adsorption-controlled process.⁵⁵ Also, both
374 anodic peak potential (E_{pa}) and cathodic peak potential (E_{pc}) demonstrated a linear

375 relationship with the scan rate respectively (**Fig. S4C**).

376 The DPVs for the oxidation of 20 μM baicalin at bare GCE, RGO/GCE,
377 Pd@RGO/GCE, $\beta\text{-CD-Pd@RGO/GCE}$, and SS- $\beta\text{-CD-Pd@RGO/GCE}$ were
378 obtained in 0.1 M PBS (pH 3.0) as shown in **Fig. 3C**. The oxidation of 20 μM
379 baicalin at the bare GCE showed a small peak current of 1.5 μA . Enhanced oxidation
380 peak current of baicalin using the RGO-modified GCE was observed in comparison
381 with that in the bare GCE. In the case of Pd@RGO/GCE, the oxidation current of
382 baicalin was enhanced compared with that of the RGO-modified GCE. In addition,
383 the oxidation current increased remarkably when the $\beta\text{-CD-Pd@RGO}$ nanohybrid
384 was immobilized onto the surface of GCE. Furthermore, the oxidation current of
385 baicalin at SS- $\beta\text{-CD-Pd@RGO/GCE}$ increased dramatically, which is 1.5 and 24.8
386 times higher than that of the $\beta\text{-CD-Pd@RGO/GC}$ and bare GC electrodes,
387 respectively. The DPV results were in accordance with that of CV. Although the
388 amount of SS- $\beta\text{-CD}$ attached to RGO measured by TGA is approximately equal to
389 that of $\beta\text{-CD}$, the higher oxidation peak current of baicalin at
390 SS- $\beta\text{-CD-Pd@RGO/GCE}$ than that at $\beta\text{-CD-Pd@RGO/GCE}$ was obtained. This is
391 only caused by the higher supramolecular recognition capability of SS- $\beta\text{-CD}$. The
392 DPVs for the oxidation of 10 μM luteolin at bare GCE, RGO/GCE, Pd@RGO/GCE,
393 $\beta\text{-CD-Pd@RGO/GCE}$, and SS- $\beta\text{-CD-Pd@RGO/GCE}$ in 0.1 M PBS (pH 3.0) were
394 also obtained as shown in **Fig. 3D**. Similar to baicalin, the oxidation peak currents of
395 luteolin at the modified electrodes increased in sequence, indicating that the
396 SS- $\beta\text{-CD-Pd@RGO/GCE}$ nanohybrid is highly suitable for the detection of baicalin

397 and luteolin by combining the merits of Pd@RGO and SS- β -CD. **Fig. 3E** shows the
398 oxidation of 20 μ M of baicalin (a), 10 μ M of luteolin (b), and a mixture (c) containing
399 20 μ M of baicalin and 10 μ M of luteolin at the SS- β -CD-Pd@RGO/GCE in 0.1 M
400 PBS (pH 3.0). Two well-defined peaks that were present at 0.30 and 0.42 V
401 corresponded to baicalin and luteolin, respectively, which were well separated from
402 each other with a potential difference of 120 mV. The potential differences were large
403 enough to simultaneously determine the concentrations of baicalin and luteolin. **Fig.**
404 **3F** shows the oxidation of a mixture containing 20 μ M of baicalin and 10 μ M of
405 luteolin at bare GCE, RGO/GCE, Pd@RGO/GCE, β -CD-Pd@RGO/GCE, and
406 SS- β -CD-Pd@RGO/GCE in 0.1 M pH 3.0 PBS. Improved oxidation currents of
407 baicalin and luteolin using these modified electrode were observed. The results are in
408 accordance with that for individual baicalin and luteolin in **Figs. 3C and D**. These
409 results suggested that the SS- β -CD-Pd@RGO nanohybrid-modified electrode was a
410 better electrode for the simultaneous electrochemical sensing of baicalin and luteolin
411 than β -CD-Pd@RGO/GCE.

412

413 **3.5 Simultaneous determination of baicalin and luteolin using DPV**

414 Under optimal conditions (the optimal solution pH is 3.0, the optimal
415 accumulation condition is -0.2 V for 200 s, see **ESI** for details), DPV was used to
416 determine the concentrations of baicalin and luteolin because it is a highly sensitive
417 and low-detection limit electrochemical method. **Fig. 4A** shows the DPV curves of
418 baicalin and luteolin on the SS- β -CD-Pd@RGO/GCE under the different solution

419 concentrations. The oxidation peak currents increased with the increased baicalin and
420 luteolin concentrations. **Fig. 4B** shows the corresponding calibration curve for
421 baicalin. The oxidation currents were proportional to the baicalin concentrations
422 between 0.02 and 20.0 μM with a detection limit of 0.0052 μM ($S/N = 3$). The
423 corresponding regression equation was calculated as $I (\mu\text{A}) = 1.88C (\mu\text{M}) + 1.12$ with
424 a correlation coefficient of 0.996. **Fig. 4C** shows the corresponding calibration curve
425 for luteolin. The oxidation currents were also proportional to the concentration of
426 luteolin between 0.01 and 10.0 μM with a detection limit of 0.0070 μM ($S/N = 3$).
427 The corresponding regression equation was calculated as $I (\mu\text{A}) = 3.80C (\mu\text{M}) + 1.27$
428 with a correlation coefficient of 0.995. The performance of the proposed
429 SS- β -CD-Pd@RGO-modified electrode was compared with those of other reported
430 electrodes. **Table 1** shows that the SS- β -CD-Pd@RGO/GCE exhibited a lower
431 detection limit and wider linear range than the other electrodes. Thus, the modified
432 electrode that was fabricated can be used to simultaneously detect baicalin and
433 luteolin in solutions with high sensitivity. In the present work, the excellent detection
434 performance of the proposed electrochemical sensor may be attributed to two factors:
435 (1) the RGO with the unique structure and outstanding properties (good
436 electrochemical properties and large surface area) loaded lots of Pd clusters and large
437 amount of SS- β -CD; (2) the SS- β -CD with higher supramolecular recognition and
438 enrichment capability than the native β -CD provided more binding sites for
439 recognition abundant of guest molecules.

440

441 3.6 Selectivity, reproducibility, and stability

442 Interference during the simultaneous detection of baicalin and luteolin was caused
443 by glucose, oxalic acid, citric acid, urea, ascorbic acid, uric acid, dopamine, which
444 were studied using the SS- β -CD-Pd@RGO-modified GCE. The currents for
445 oxidation of 20 μ M of baicalin and 10 μ M of luteolin at the SS- β -CD-Pd@RGO/GC
446 electrode were compared with the signal obtained in the presence of interfering
447 species. As shown in **Fig. S10**, a ten-fold concentration of glucose, oxalic acid, citric
448 acid, urea, and AA did not affect the baicalin and luteolin responses. In addition, no
449 significant interference from common ions, such as Na⁺, K⁺, Ca²⁺, Mg²⁺, Cl⁻, NO₃⁻,
450 SO₄²⁻, CO₃²⁻, Cu²⁺, Zn²⁺, and Al³⁺, was observed, even at 100-fold excess
451 concentrations (Data not shown). Thus, the simultaneous and quantitative detection of
452 baicalin and luteolin was reliable at ambient conditions.

453 The oxidation peak currents of 20 μ M of baicalin and 10 μ M of luteolin using six
454 equal SS- β -CD-Pd@RGO/GCEs were compared to evaluate the fabrication
455 reproducibility of the SS- β -CD-Pd@RGO-modified electrode. The six modified
456 electrodes exhibited similar electrochemical responses with a relative standard
457 deviation (RSD) of 4.6%, indicating satisfactory reproducibility.

458 Successive cyclic potential scans for 50 cycles and long-term storage assays were
459 used to examine the stability of the SS- β -CD-Pd@RGO-modified electrode. A 7.5%
460 decrease in the initial peak current was observed after 30 continuous cycle scans.
461 Additionally, a long-term stability experiment was performed intermittently (every 5
462 days). The constructed sensor was stored in a refrigerator at 4 °C when not in use.

463 Initial responses of over 94.2% and 84.6% remained after storage for 15 and 30 days,
464 respectively, revealing an acceptable stability of the SS- β -CD-Pd@RGO-modified
465 electrode.

466

467 **3.7 Real sample analysis and potential application of the constructed sensor**

468 The SS- β -CD-Pd@RGO/GCE sensor was used to detect baicalin and luteolin in
469 human serum samples using standard addition methods to evaluate the feasibility of
470 the SS- β -CD-Pd@RGO-modified electrode for real sample analysis. The serum
471 sample was diluted one hundred times with 0.1 M PBS (pH 3.0). Results showed
472 apparent recoveries ranging from 96.6% to 106.0% and RSDs ranging from 2.9% to
473 5.6% (**Table 2**). These findings demonstrated that the SS- β -CD-Pd@RGO-based
474 sensor that was fabricated in this study has practical applications.

475 The proposed sensor may also be expanded to potential applications in biological
476 and functional food samples. It is worth noting that, as an oligosaccharide, SS- β -CD
477 is stable enough under complex conditions, and thus seems to be more suitable for
478 analysis of practical samples. In addition, SS- β -CD possesses higher molecular
479 recognition capability than native β -CD and its synthesis is very easy. Therefore, this
480 sensor could be used to determine the flavonoids in biological samples and provide
481 new opportunities for analysis of flavonoids metabolites in organisms in the future.

482

483 **4. Conclusions**

484 In summary, by combining the merits of Pd@RGO and the SS- β -CD, a highly

485 sensitive electrochemical sensing platform was developed based on the
486 SS- β -CD-Pd@RGO nanohybrids. Electrochemical simultaneous detection of baicalin
487 and luteolin using SS- β -CD-Pd@RGO nanohybrids-modified electrode is described
488 for the first time. Due to the synergistic effects from the Pd@RGO and SS- β -CD, the
489 SS- β -CD-Pd@RGO modified GC electrode was found to have linear response ranges
490 of 0.02–20.00 μ M for baicalin and 0.01–10.00 μ M for luteolin with relatively low
491 detection limits of 0.0052 μ M for baicalin and 0.0070 μ M for luteolin, respectively,
492 implying that SS- β -CD-Pd@RGO nanohybrids are excellent sensing materials for the
493 electrochemical determination of flavonoids. In addition, the proposed sensing
494 platform was employed for detection of baicalin and luteolin in human serum samples
495 with satisfactory results. Thus, the present work might broaden the electrochemical
496 application of various bridged bis(β -CD)s in electrochemical sensing or biosensing
497 field.

498

499 **Acknowledgements**

500 This work was supported by the Natural Science Foundation of China (31160334)
501 and the Natural Science Foundation of Yunnan Province (2012FB112, 2014RA022),
502 People's Republic of China.

503

504 **References:**

- 505 1 L. Zhang, A. S. Ravipati, S. R. Koyyalamudi, S. C. Jeong, N. Reddy, P. T. Smith,
506 J. Bartlett, K. Shanmugam, G. Münch, M. J. Wu, *J. Agric. Food Chem.*, 2011, **59**,

- 507 12361–12367.
- 508 2 M. E. Carlotti, S. Sapino, E. Ugazio, G. Caron, *J. Incl. Phenom. Macro.*, 2010, **70**,
- 509 81–90.
- 510 3 E. Pinho, M. Grootveld, G. Soares, M. Henriques, *Carbohydr. Polym.*, 2014, **101**,
- 511 121–135.
- 512 4 D. D. Orhan, B. Ozçelik, S. Ozgen, F. Ergun, *Microbiol. Res.*, 2010, **165**,
- 513 496–504.
- 514 5 M. Okamoto, M. Ohta, H. Kakomn, T. Omori, *Chromatographia*, 1993, **35**,
- 515 281–284.
- 516 6 S. J. Sheu, C. F. Lu, *J. High Resolut. Chromatogr.*, 1996, **19**, 409–412.
- 517 7 Y. M. Liu, S. J. Sheu, *Anal. Chim. Acta*, 1994, **288**, 221–226.
- 518 8 C. S. Liu, Y. S. Song, K. J. Zhang, J. C. Ryu, M. Kim, T. H. Zhou, *J. Pharm.*
- 519 *Biomed. Anal.*, 1995, **13**, 1409–1414.
- 520 9 M. C. Lin, M. J. Tsai, K. C. Wen, *J. Chromatogr. A*, 1999, **830**, 387–395.
- 521 10 Q. Chang, M. Zhu, Z. Zuo, M. Chow, W. K. Ho, *J. Chromatogr. B: Biomed. Sci.*
- 522 *Appl.*, 2001, **760**, 227–235.
- 523 11 F. M. Areias, P. Valentao, P. B. Andrade, F. Ferreres, R. M. Seabra, *Food Chem.*,
- 524 2001, **73**, 307–311.
- 525 12 S. M. Wittemer, M. Veit, *J. Chromatogr. B*, 2003, **793**, 367–375.
- 526 13 G. Favaro, C. Clementi, A. Romani, V. Vickackaite, *J. Fluoresc.*, 2007, **17**,
- 527 707–714.
- 528 14 J. G. Renee, C. K. Geoffrey, A. Z. Mamdouh, J. A. Louise, *Phytochem. Anal.*,

- 529 2000, **11**, 257–267.
- 530 15 D. A. van Elswijk, U. P. Schobel, E. P. Lansky, H. Irth, J. van der Greef,
531 *Phytochemistry*, 2004, **65**, 233–241.
- 532 16 D. M. Zhao, X. H. Zhang, L. J. Feng, Q. Qi, S. F. Wang, *Food Chem.*, 2011, **127**,
533 694–698.
- 534 17 S. H. Wu, B. J. Zhu, Z. X. Huang, J. J. Sun, *Electrochem. Commun.*, 2013, **28**,
535 47–50.
- 536 18 Z. Liu, A. Zhang, Y. Guo, C. Dong, *Biosens. Bioelectron.*, 2014, **58**, 242–248.
- 537 19 P. F. Pang, Y. P. Liu, Y. L. Zhang, Y. T. Gao, Q. F. Hu, *Sens. Actuators B*, 2014,
538 **194**, 397–403.
- 539 20 A. Y. Tesio, A. M. Granero, N. R. Vettorazzi, N. F. Ferreyra, G. A. Rivas, H.
540 Fernández, M. A. Zon, *Microchem. J.*, 2014, **115**, 100–105.
- 541 21 H. Ibrahim, Y. Temerk, *Sens. Actuators B*, 2015, **206**, 744–752.
- 542 22 M. L. Pang, J. Y. Hu, H. C. Zeng, *J. Am. Chem. Soc.*, 2010, **132**, 10771–10785.
- 543 23 J. A. Farmer, C. T. Campbell, *Science*, 2010, **329**, 933–936.
- 544 24 R. J. White, R. Luque, V. L. Budarin, J. H. Clark, D. J. Macquarrie, *Chem. Soc.*
545 *Rev.*, 2009, **38**, 481–494.
- 546 25 X. M. Chen, G. H. Wu, J. M. Chen, X. Chen, Z. X. Xie, X. R. Wang, *J. Am.*
547 *Chem. Soc.*, 2011, **133**, 3693–3695.
- 548 26 W. Chen, S. Chen, *Angew. Chem., Int. Ed.*, 2009, **48**, 4386–4389.
- 549 27 H. J. Yin, H. J. Tang, D. Wang, Y. Gao, Z. Y. Tang, *ACS Nano*, 2012, **6**,
550 8288–8297.

- 551 28 Y. J. Wang, D. P. Wilkinson, J. Zhang, *Chem. Rev.*, 2011, **111**, 7625–7651.
- 552 29 M. J. Allen, V. C. Tung, R. B. Kaner, *Chem. Rev.*, 2010, **110**, 132–145.
- 553 30 L. Yang, H. Zhao, S. Fan, B. Li, C.-P. Li, *Anal. Chim. Acta*, 2014, **852**, 28–36.
- 554 31 J. Zhou, M. Chen, G. W. Diao, *ACS Appl. Mater. Interfaces*, 2013, **5**, 828–836.
- 555 32 G. Zheng, M. Chen, X. Y. Liu, J. Zhou, J. Xie, G. W. Diao, *Electrochim. Acta*,
556 2014, **136**, 301–309.
- 557 33 M. Chen, Y. Meng, W. Zhang, J. Zhou, J. Xie, G. W. Diao, *Electrochim. Acta*,
558 2013, **108**, 1–9.
- 559 34 Y. Yao, L. Zhang, J. Xu, X. Wang, X. Duan, Y. Wen, *J. Electroanal. Chem.*, 2014,
560 **713**, 1–8.
- 561 35 J. M. Gong, X. M. Han, X. L. Zhu, Z. Q. Guan, *Biosens. Bioelectron.*, 2014, **61**,
562 379–385.
- 563 36 L. Yang, H. Zhao, Y. C. Li, C.-P. Li, *Sens. Actuators B*, 2015, **207**, 1–8.
- 564 37 L. Yang, S. Fan, G. Deng, Y. Li, X. Ran, H. Zhao, C.-P. Li, *Biosens. Bioelectron.*,
565 2015, **68**, 617–625.
- 566 38 L. Yang, H. Zhao, C.-P. Li, S. M. Fan, B. C. Li, *Biosens. Bioelectron.*, 2015, **64**,
567 126–130.
- 568 39 Y. Guo, S. Guo, J. Ren, Y. Zhai, S. Dong, E. Wang, *ACS Nano*, 2010, **4**,
569 4001–4010.
- 570 40 G. Zhu, X. Zhang, P. Gai, X. Zhang, J. Chen, *Nanoscale*, 2012, **4**, 5703–5709.
- 571 41 Y. Zhao, J. Gu, Y. C. Yang, H. Y. Zhu, R. Huang, B. Jing, *J. Mol. Struct.*, 2009,
572 **930**, 72–77.

- 573 42 P. Li, Y. Liu, X. Wang, B. Tang, *Analyst*, 2011, **136**, 4520–4525.
- 574 43 Y.-M. Zhang, H.-Z. Chen, Y. Chen, F. Ding, Y. Liu, *New J. Chem.*, 2013, **37**,
575 1554–1560.
- 576 44 Y. Liu, B. Li, C. C. You, T. Wada, Y. Inoue, *J. Org. Chem.*, 2001, **66**, 225–232.
- 577 45 Y. Okabe, H. Yamamura, K. Obe, K. Ohta, M. Kawai, K. Fujita, *Chem. Commun.*,
578 1995, **5**, 581–582.
- 579 46 T. Jiang, D. K. Sukumaran, S. D. Soni, D. S. Lawrence, *J. Org. Chem.*, 1994, **59**,
580 5149–5155.
- 581 47 H. F. M. Nelissen, M. Feiters, R. J. M. Nolte, *J. Org. Chem.*, 2002, **67**,
582 5901–5906.
- 583 48 Y. Hasegawa, M. Miyauchi, Y. Takashima, H. Yamaguchi, A. Harada,
584 *Macromolecules*, 2005, **38**, 3724–3730.
- 585 49 Y. Liu,; Y. W. Yang,; Y. Zhao,; L. Li,; H. Y. Zhang,; S. Z. Kang, *J. Inclusion*
586 *Phenom. Macrocyclic Chem.*, 2003, **47**, 155–160.
- 587 50 T. Ogoshi, M. Hashizume, T. Yamagishi, Y. Nakamoto, *Langmuir*, 2010, **26**,
588 3169–3173.
- 589 51 X. B. Fan, W. C. Peng, Y. Li, X. Y. Li, S. L. Wang, G. L. Zhang, F. B. Zhang, *Adv.*
590 *Mater.*, 2008, **20**, 4490–4493.
- 591 52 B. Tang, H. Liang, K. Xu, Z. Mao, X. Shi, Z. Chen, *Anal. Chim. Acta*, 2005, **554**,
592 31–36.
- 593 53 D. Chen, Z. Chen, K. Xu, B. Tang, *J. Agric. Food Chem.*, 2011, **59**, 4424–4428.
- 594 54 H. C. Choi, M. Shim, S. Bangsaruntip, H. Dai, *J. Am. Chem. Soc.*, 2002, **124**,

- 595 9058–9059.
- 596 55 J. Molina, J. Fernández, C. García, A. I. del Río, J. Bonastre, F. Cases,
597 *Electrochim., Acta*, 2015, **166**, 54–63.
- 598 56 E. Topoglidis, Y. Astuti, F. Duriaux, M. Gratzel, J. R. Durrant, *Langmuir*, 2003,
599 **19**, 6894–6900.
- 600 57 A. Kaushik, A. Vasudev, S. K. Arya, , S. Bhansali, *Biosens. Bioelectron.*, 2013,
601 **50**, 35–41.
- 602 58 M. A. Raj, S. A. J ohn, *Anal. Chim. Acta*, 2013, **771**, 14–20.
- 603 59 W. G. Hepburn, C. Batchelor-McAuley, K. Tschulik, E. O. Barnes, R. T.
604 Kachoosangi, R. G. Compton, *Phys. Chem. Chem. Phys.*, 2014, **16**,
605 18034–18041.
- 606 60 G. Chen, H. Zhang, J. Ye, *Talanta*, 2000, **53**, 471–479.
- 607 61 D. Lu, S. Lin, L. Wang, T. Li, C. Wang, Y. Zhang, *J. Solid State Electrochem.*,
608 2014, **18**, 269–278.

609

610 **Figure captions:**

611 **Scheme 1.** Chemical structures of baicalin (A) and luteolin (B).

612

613 **Scheme 2.** The illustration of the SS- β -CD-Pd@RGO nanohybrids simultaneously
614 sensing baicalin and luteolin by an electrochemical strategy.

615

616 **Fig. 1. (A)** UV-vis spectra of free baicalin (50 μ M), 50 μ M baicalin + 0.72 mM β -CD,

617 50 μM baicalin + 0.32 mM SS- β -CD, free β -CD (0.72 mM), and free SS- β -CD (0.32
618 mM) in aqueous solution. **(B)** UV-vis spectra of free luteolin (50 μM), 50 μM luteolin
619 + 0.72 mM β -CD, 50 μM luteolin + 0.32 mM SS- β -CD, free β -CD (0.72 mM), and
620 free SS- β -CD (0.32 mM) in aqueous solution.

621

622 **Fig. 2.** **(A–C)** TEM images of Pd@RGO at different magnifications. **(D)** FTIR spectra
623 of RGO, β -CD-Pd@RGO, and SS- β -CD-Pd@RGO. **(E)** TGA curves of RGO,
624 β -CD-Pd@RGO, and SS- β -CD-Pd@RGO. **(F)** EIS characterization of bare GCE,
625 RGO/GCE, Pd@RGO/GCE, β -CD-Pd@RGO/GCE, and SS- β -CD-Pd@RGO/GCE
626 using 2.0 mM $[\text{Fe}(\text{CN})_6]^{3-/4-}$ redox couple (1:1) with 0.1 M KCl as supporting
627 electrolyte.

628

629 **Fig. 3.** CVs of 20 μM baicalin **(A)** and 10 μM luteolin **(B)** at bare GCE, RGO/GCE,
630 Pd@RGO/GCE, β -CD-Pd@RGO/GCE, and SS- β -CD-Pd@RGO/GCE in 0.1 M PBS
631 (pH 3.0). DPVs of 20 μM baicalin **(C)** and 10 μM luteolin **(D)** at bare GCE,
632 RGO/GCE, Pd@RGO/GCE, β -CD-Pd@RGO/GCE, and SS- β -CD-Pd@RGO/GCE in
633 0.1 M PBS (pH 3.0). **(E)** DPVs obtained for the oxidation of 20 μM baicalin (a), 10
634 μM of luteolin (b), and a mixture (c) containing 20 μM baicalin and 10 μM of luteolin
635 at the SS- β -CD-Pd@RGO/GCE in 0.1 M PBS (pH 3.0). **(F)** DPVs obtained for the
636 oxidation of a mixture containing 20 μM of baicalin and 10 μM of luteolin at bare
637 GCE, RGO/GCE, Pd@RGO/GCE, β -CD-Pd@RGO/GCE, and
638 SS- β -CD-Pd@RGO/GCE in 0.1 M PBS (pH 3.0). Pulse width: 0.05 s; amplitude:

639 0.05 V.

640

641 **Fig. 4. (A)** DPV curves obtained for the oxidation of baicalin and luteolin at
642 SS- β -CD-Pd@RGO/GCE for different concentrations. Calibration curves for
643 simultaneous determination of baicalin (**B**) and luteolin (**C**) using the proposed sensor.
644 The error bars represent the standard deviations of three parallel tests.

645

646

647

648

649

650

651

652

653

654

655

656

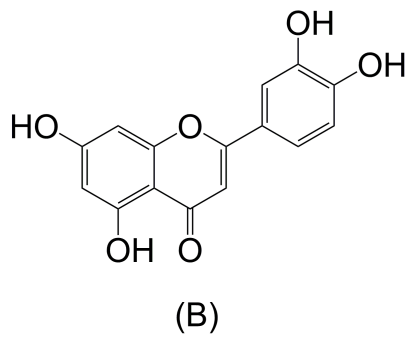
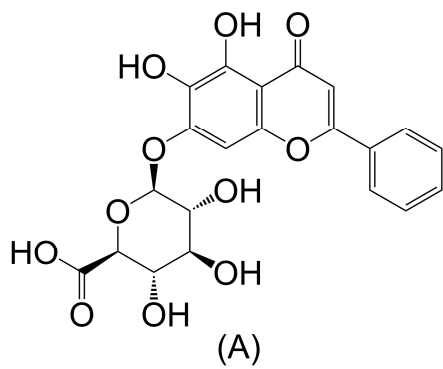
657

658

659

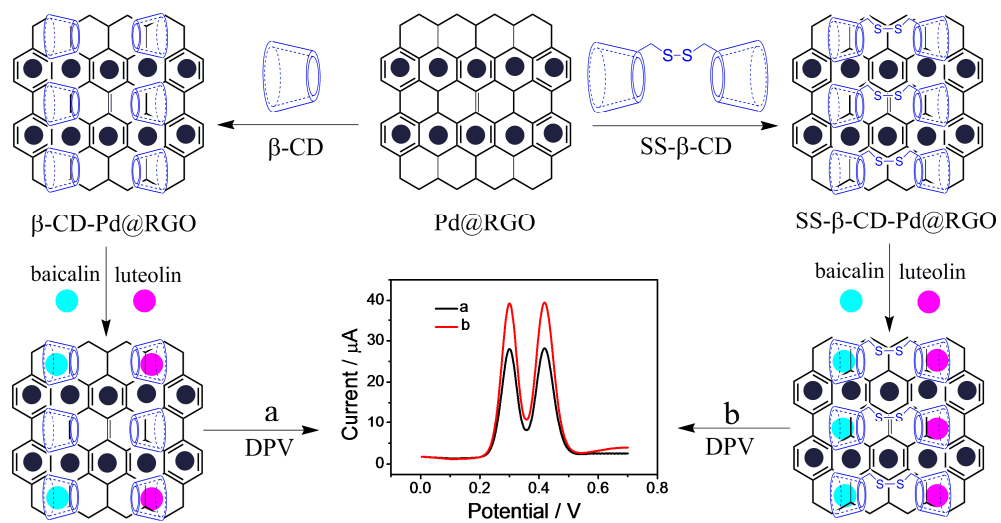
660

Figures:



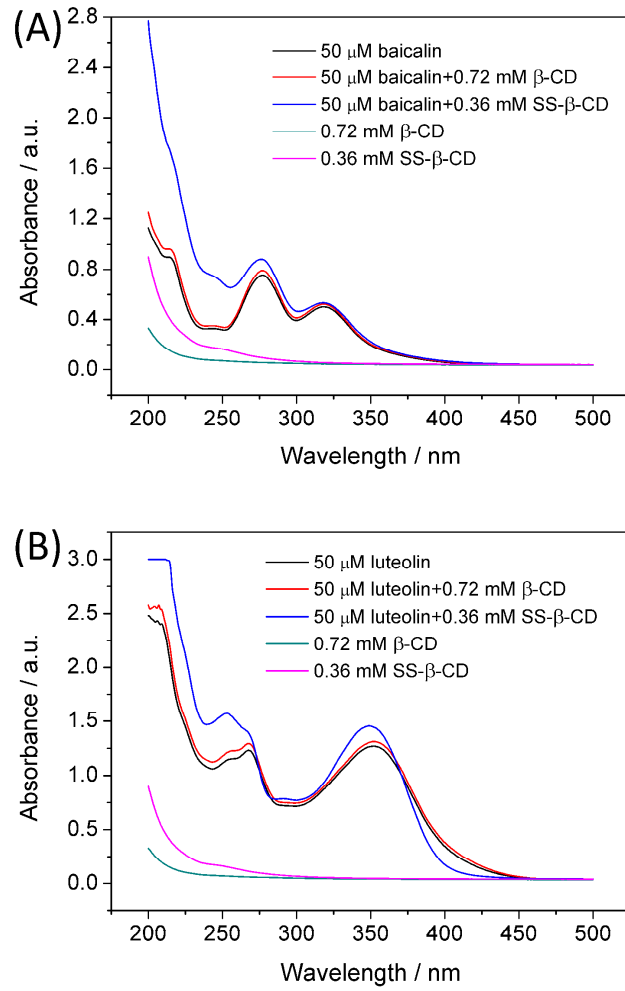
Scheme 1

Ran et al.



Scheme 2

Ran et al.

**Fig. 1****Ran et al.**

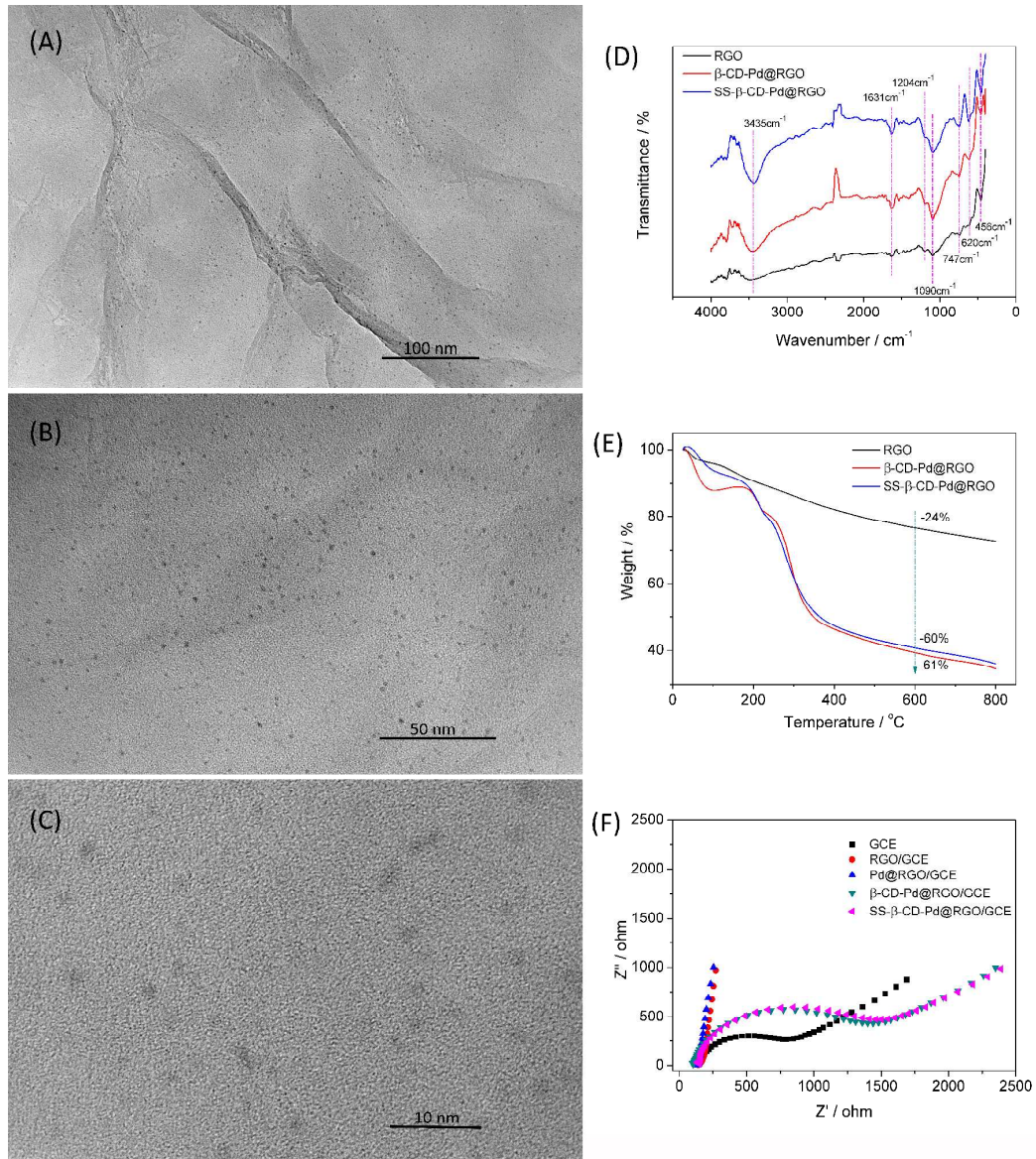


Fig.2

Ran et al.

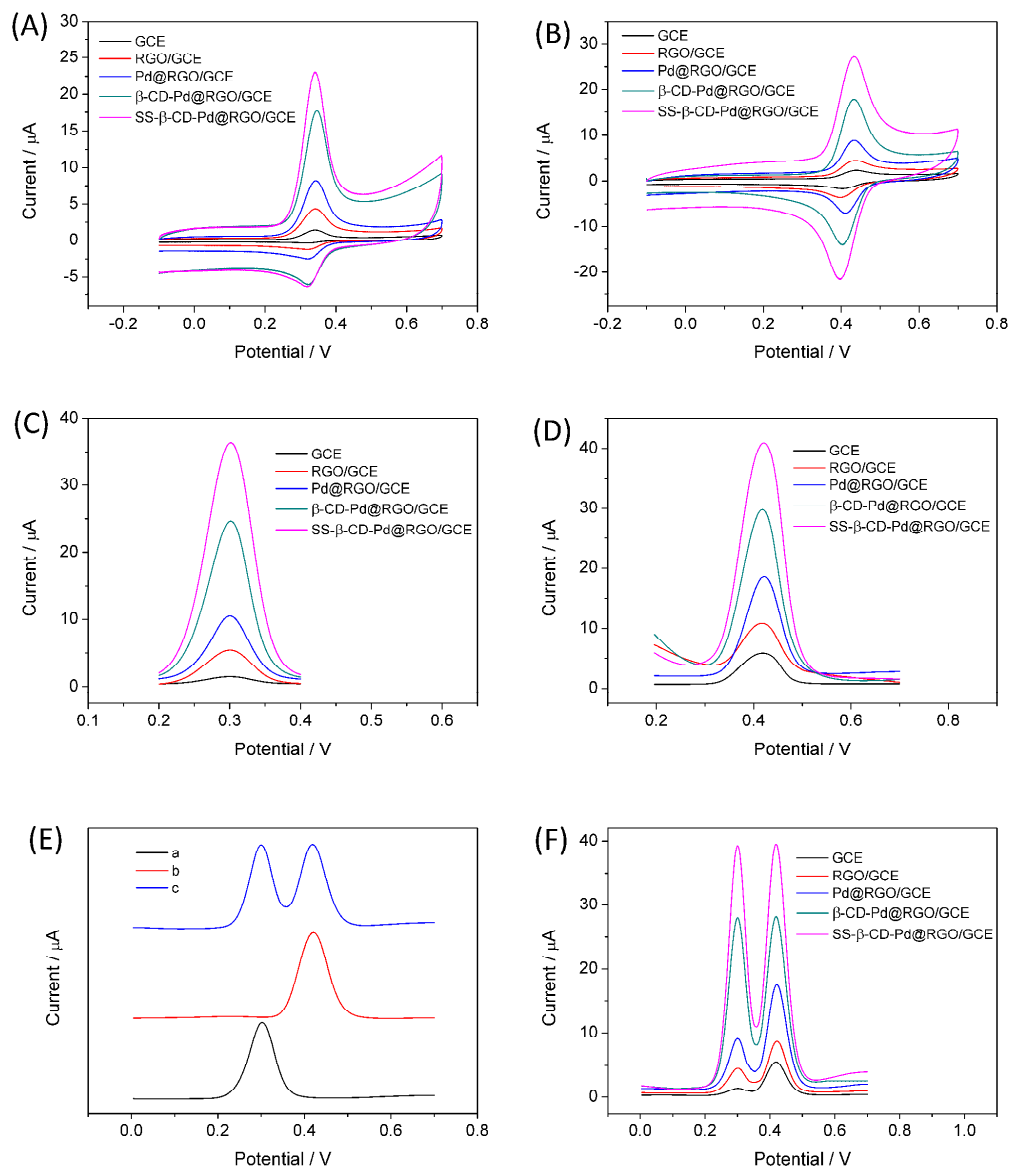


Fig. 3

Ran et al.

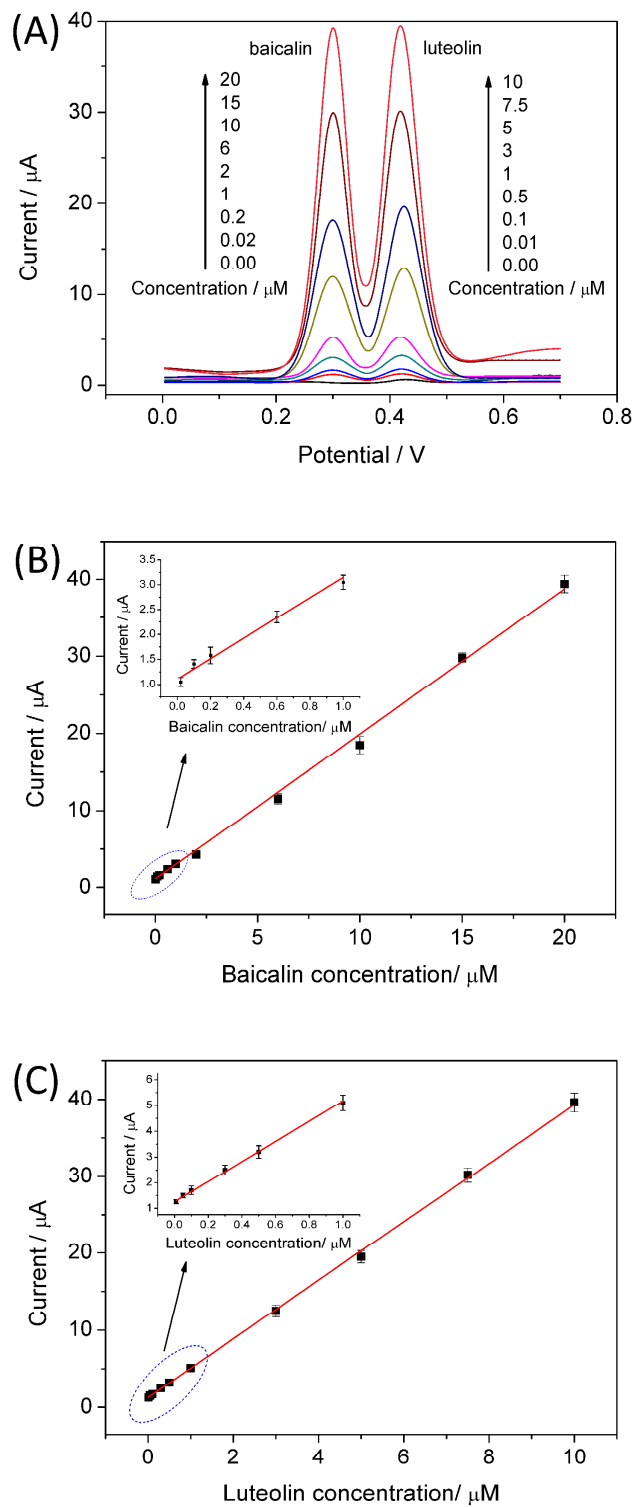


Fig. 4

Ran et al.

Table 1

Comparison of the analytical parameters for baicalin and luteolin detection by different electrodes.

Sample	Electrode	Method	Linear range (μM)	LOD (μM)	Ref
baicalin	Carbon disc electrode	CE-ED	1.0–1000	0.548	60
	DM- β -CD-GNs/GCE	DPV	0.04–3.0	0.01	18
	SS- β -CD-Pd@RGO/GCE	DPV	0.02–20	0.007	This work
luteolin	PDDA-G-CNTs/ β -CD/GCE	DPV	0.05–60	0.02	61
	Carbon disc electrode	SWV	0.004–1.0	0.001	17
	GNs/HA/GCE	DPV	0.02–10	0.01	19
	SS- β -CD-Pd@RGO/GCE	DPV	0.01–10	0.0052	This work

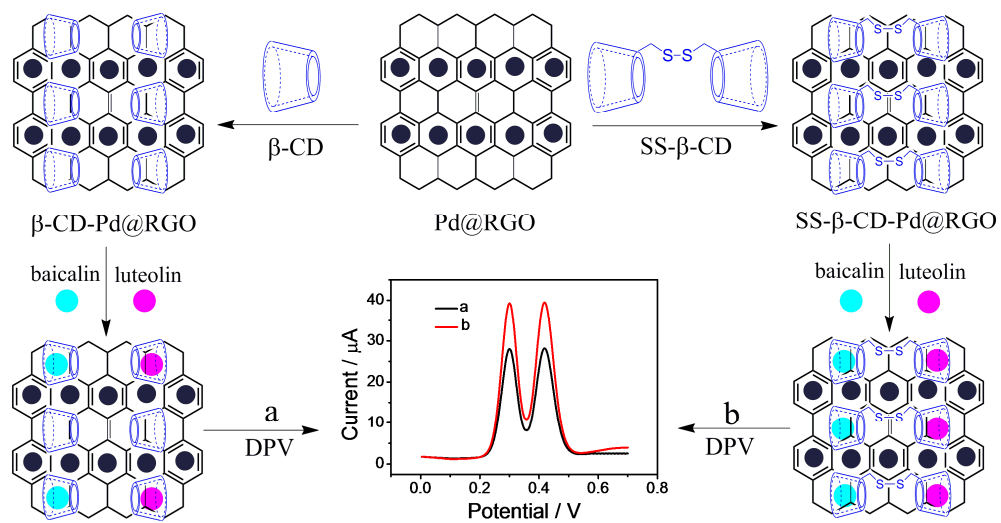
Table 2

Determination of baicalin and luteolin in human serum samples ($n=3$).

Sample	Added (μM)		Founded (μM)		RSD (%)		Apparent recovery (%)	
	baicalin	luteolin	baicalin	luteolin	baicalin	luteolin	baicalin	luteolin
1	1.0	0.5	1.02	0.53	4.5	5.6	102.0	106.0
2	10.0	5.0	9.84	4.83	3.9	4.5	98.4	96.6
3	15.0	7.5	15.53	7.41	3.1	2.9	103.5	98.8

Tables

Ran et al.



Graphic Abstract

The illustration of the SS-β-CD-Pd@RGO nanohybrids simultaneously sensing baicalin and luteolin by an electrochemical strategy.