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1 **A combined experimental and theoretical insight into**
2 **the drug delivery of nanoporous metal-organic**
3 **frameworks**

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15 **Abstract**

16 _____
17 Two isostructural nanoporous MOFs with $[\text{Zn}_3(\mu_3\text{-O})(\text{BTC})_2(\text{H}_3\text{O})]_n$ (**NTU-Z11**)
18 and $\{[\text{Zn}_3(\mu_3\text{-O})(\text{BTC})_2(\text{DMF})] \cdot 2\text{NH}_2(\text{CH}_3)_2 \cdot 4\text{H}_2\text{O}\}_n$ (**GDMU**) (BTC
19 =1,3,5-benzenetricarboxylate) have been used as drug carriers of 5-fluorouracil
20 (5-FU). The incorporation of the 5-FU into the desolvated **NTU-Z11** and **GDMU** was
21 around 0.38 g/g and 0.22 g/g, respectively. **NTU-Z11** presents a pH-triggered
22 controlled drug release property in 6.0, 7.4, 9.18 and water media. In addition, we
23 performed GCMC simulations to investigate the loading of 5-FU to **NTU-Z11** and
24 **GDMU** at the molecular level. The results from simulations reproduce the
25 experimental trend with respect to drug loading capacity of each material.
26 Comparison between calculated drug loading values and some molecular level
27 properties indicates the existence of a relationship between the void space of material
28 and drug loading capacity.

29 **Introduction**

30 Porous metal-organic frameworks (MOFs) have particularly highlighted for their

1 excellent gas-storage and catalysis properties [1-3]. Recently, tremendous efforts on
2 MOF carriers have been made to boost their way toward medical applications [5-8].
3 Férey's group first described the potential loading and release properties of some
4 drugs on MOFs[9], whereas Lin *et al.* have constructed a Pt-based drug at the
5 nanoscale by using it as one building block to create a new coordination polymer[10].
6 Horcajada and his co-workers had also reported that porous MOFs can load and
7 release drugs, acting as a promising non-toxic drug carrier [11].

8 Zhang and his co-worker reported a facile route to synthesize a series of
9 NTU-based MOFs [12]. NTU-Z11 is the isostructure of MOF-38 and can be
10 repeatedly synthesized with high yield [13]; moreover, its channels are empty and
11 have a dimension of about 11.5×11.5 Å. Inspired by these works, our strategy is to
12 explore a neutral MOF that its structural feature is similar with NTU-Z11.
13 Unfortunately, only a negative GDMU was obtained. But we are still interested to
14 develop the loading and release properties of 5-FU on the two MOFs because the
15 efficiency of drug delivery is related to the pore characteristics and the nature of
16 host-guest interactions. GCMC simulation is a powerful technique to explain and
17 predicate the gas adsorption to porous materials. However, there is still a challenging
18 work to use the GCMC simulations to investigate the loading of large molecules to
19 porous materials due to the requirement of the conformational sampling and fitting of
20 such molecules inside tight pores [14-16].

21 Herein, we demonstrated two Zn(II)-based frameworks with additional negative
22 charges that have been used as drug carriers of 5-FU. The incorporation of the 5-FU
23 into the desolvated NTU-Z11 and GDMU was around 0.38 g/g and 0.22 g/g,
24 respectively. NTU-Z11 presents a pH-triggered controlled drug release property in pH
25 6.0, 7.4, 9.18 and water media. In addition, we performed GCMC simulations to
26 investigate the loading of 5-FU in NTU-Z11 and GDMU at the molecular level.
27 Comparison between calculated drug loading values and some molecular level
28 properties indicates the existence of an important relationship between the void space
29 of material and drug loading capacity.

30 **Materials and Method**

1 All reagents were purchased from commercial sources and used as received. IR
2 spectra were recorded with a Perkin–Elmer Spectrum One spectrometer in the region
3 4000–400 cm^{-1} using KBr pellets. TGA were carried out with a Mettler–Toledo TA 50
4 under dry dinitrogen flux (60 $\text{mL}\cdot\text{min}^{-1}$) at a heating rate of 5 $^{\circ}\text{C}\cdot\text{min}^{-1}$. X-ray powder
5 diffraction (PXRD) data were recorded on a Rigaku RU200 diffractometer at 60KV,
6 300mA for $\text{Cu } K_{\alpha}$ radiation ($\lambda = 1.5406 \text{ \AA}$), with a scan speed of 2 $^{\circ}\text{C}/\text{min}$ and a step
7 size of 0.02 $^{\circ}$ in 2θ .

8 **X-ray Crystallography:** Single crystal X-ray diffraction analyses of the two
9 compounds were carried out on a *Bruker SMART APEX II CCD* diffractometer
10 equipped with a graphite monochromated $\text{Mo } K_{\alpha}$ radiation ($\lambda = 0.71073 \text{ \AA}$) by using
11 ϕ/ψ scan technique at room temperature. The intensities were corrected for Lorentz
12 and polarization effects as well as for empirical absorption based on multi-scan
13 techniques; all structures were solved by direct methods and refined by full-matrix
14 least-squares fitting on F^2 by SHELX-97[17]. Absorption corrections were applied by
15 using multi-scan program SADABS[18]. Non-hydrogen atoms were refined
16 anisotropically. The structure contains large (37 % volume) regions of intensely
17 disordered cations and solvent. These were impossible to model at atomic resolution
18 and their presence in the structure is assumed on the basis of the elemental analysis,
19 TGA and the PLATON/SQUEEZE calculations [19]. The latter were used to calculate
20 the diffraction contribution of the solvent molecules and, thereby, to produce a set of
21 solvent-free diffraction intensities for the refinement of the MOF structure.
22 Crystallographic data for complexes **GDMU** are given in Table 1. Selected bond
23 distances and bond angles are listed in Table 2. **CCDC:** 1405443 for **GDMU**.

24 **Syntheses of these complexes**

25 $[\text{Zn}_3(\mu_3\text{-O})(\text{BTC})_2(\text{H}_3\text{O})]_n$ (**NTU-Z11**)

26 We only synthesized the **NTU-Z11** according to the reference. The sample purity
27 was confirmed by the PXRD.

28 $\{[\text{Zn}_3(\mu_3\text{-O})(\text{BTC})_2(\text{DMF})] \cdot 2\text{NH}_2(\text{CH}_3)_2 \cdot 4\text{H}_2\text{O}\}_n$ (**GDMU**)

29 A mixture of $\text{Zn}(\text{NO}_3)_2 \cdot 6\text{H}_2\text{O}$ (0.450g, 0.1mmol), L(4,4'-bis(pyrid-4-yl)biphenyl)
30 (0.015g, 0.04mmol), and H_3BTC (0.450mg, 0.2mmol), DMF (4mL) in a

1 screw-capped vial. After five drops of HNO₃ was added into the mixture. The vial
2 was capped and placed in an oven at 110 °C for 3 days. The resulting colorless single
3 crystals were washed with absolute CH₃CH₂OH three times to give **1**. Anal. Calcd for
4 C₂₅H₃₇N₃O₁₈Zn₃ (863.68), C, 34.77; H, 4.32; N, 4.87. Found C, 34.28.; H, 4.15;
5 N,4.55. IR (KBr, cm⁻¹) : 3480(vs); 2940(m); 1632(vs); 1428(v); 1390(v); 1099(m);
6 938(m); 708(v); 547(m).

7 **Computational Details**

8 The 5-FU adsorption in **NTU-11** and **GDMU** was studied using grand canonical
9 ensemble Monte Carlo (GCMC) simulations, employed with the RASPA code at 298
10 K[20]. The structures of 5-FU and MOFs are described with an all-atom model in this
11 work. The structures for 5-FU and MOFs can be found in Figures S1 and S2. For
12 MOFs structures, the framework atoms were kept rigid during the simulations. The
13 guest-guest and guest-host interactions were computed with a Lennard-Jones (LJ) and
14 Coulombic potential. The Antechamber program of AmberTools1.27 was used to
15 generate the force field for 5-FU with the general amber force field parameters [21].
16 The atomic partial charges for 5-FU were computed with CHELPG method based on
17 the Gaussian 03 suite with the 6-31++g* basis set. The Lennard-Jones parameters and
18 partial charges can be found in Table S1- S3.

19 The atomic positions of **NTU-Z11** and **GDMU** structures were taken from the
20 PXRD data(The Rietveld refinement for the 5-FU@MOFs complexes was performed
21 with the software GSAS/EXPGUI, using the X-ray structure of the MOF as initial
22 atomic coordinates.). The cations of H₃O⁺ and NH₂(CH₃)₂⁺ are included in **NTU-Z11**
23 and in **GDMU**, respectively. The cations of NH₂(CH₃)₂⁺ were not removed in the
24 uptake of 5-FU. Thus we also did not remove these molecules in these simulated
25 structures. The Lennard-Jones parameters for the MOFs structure atoms were taken
26 from the UFF force field (listed in Table S2) [22]. The accurate prediction of
27 adsorption in various MOFs could be achieved by a number of simulation
28 investigations using the UFF force field [23-24]. The molecular geometries for cations
29 were optimized by DFT method. In canonical ensemble, the desired number of cation
30 were inserted into the pore and attempted to accelerate the equilibrium with

1 reinsertion-move. The obtained configurations were used to simulate the adsorption of
 2 5-FU in MOFs. The solvent molecules of the MOFs in the simulations are allowed to
 3 move (including translation and rotation).

4 The heats of adsorption were computed using the equation:

$$Q_{st} = RT - \frac{\langle UN \rangle - \langle U \rangle \langle N \rangle}{\langle N^2 \rangle - \langle N \rangle^2}$$

5
 6 where $\langle \rangle$ refers to the average over the simulation, and U is the energy, N is the
 7 number of adsorbed molecules.

8 For the interactions of unlike sites were computed with Lorentz-Berthelot mixing
 9 rules. The Lennard-Jones interactions were cut and shifted at the 13 Å. The partial
 10 charges of the **NTU-Z11** and **GDMU** atoms were computed from density functional
 11 theory (DFT) with the B3LYP functional. For the metal atoms, the LanL2DZ basis set
 12 was applied. The 6-31++g* basis set was used to optimized for all other atoms. The
 13 atomic partial charges can be obtained by fitting the electrostatic potentials after DFT
 14 computation. The Coulombic interactions were computed using the Ewald sum
 15 technique. The details of simulated boxes are listed in Table S4. After the initial 10^6
 16 Monte Carlo (MC) cycles, the production of 10^6 cycles was used to compute the
 17 ensemble averages properties. For each cycle, the MC moves include the molecule of
 18 insertion, deletion, translation, rotation or re-growth. We used the equal probability
 19 for each MC moves.

20 Results and Discussion

21 $[\text{Zn}_3(\mu_3\text{-O})(\text{BTC})_2(\text{H}_3\text{O})]_n$ (**NTU-Z11**) and $\{[\text{Zn}_3(\mu_3\text{-O})(\text{BTC})_2(\text{DMF})] \cdot 2\text{NH}_2(\text{CH}_3)_2 \cdot 4\text{H}_2\text{O}\}_n$
 22 (**GDMU**)

23 The **NTU-Z11** and **GDMU** are isostructural, which are composed of the
 24 $[\text{Zn}_3(\mu_3\text{-O})(\text{COO})_6]$ subunits (Fig. 1a-1b). The subunits are connected by BTC ligands,
 25 which results in an infinite 3-D (3,6)- connected framework with 1-D channel of
 26 about 11.5×11.5 Å dimension along the *c*-axis (Figure 1c-1d). But we should state
 27 herein, if the L was absent in this reactive system, the final product of **GDMU** could
 28 not be obtained. Furthermore, the pores of **GDMU** were occupied by the $\text{NH}_2(\text{CH}_3)_2$

1 and DMF molecules. This structural feature was also similar with MOF-38, which
2 holds some disordered HTEA molecules. However, the MOF-38 cannot be repeated
3 as mentioned in the literature[13].

4 **Thermogravimetric Analyses**

5 The thermogravimetric analyses (TGA) of complex **GDMU** was performed (Fig.
6 S3). It shows three weight loss steps. The first weight loss begins at 25°C and is
7 completed at 80°C. The observed weight loss of 8.6% is corresponding to the loss of
8 the free water molecules (calcd 8.3%). The second weight loss occurs latterly, and can
9 be attributed to the elimination of $\text{NH}_2(\text{CH}_3)_2$ cations(obsd: 9.5%; calcd 10.4%). A
10 gradual weight loss from 210 °C indicates that the complex decomposes continuously
11 when the temperature is raised. The mass remnant at ~700 °C of 25.4 % is roughly
12 consistent with the deposition of ZnO (calcd 28.3%) (a weight loss of 4.0% is larger
13 than the calculated value, probably resulting from the sensitivity to temperature and
14 humidity or a very slow absorbability of the guest molecules from the air at room
15 temperature).

16 Both of **NTU-Z11** and **GDMU** were desolvated at 120 °C for 10 h prior to
17 insertion of the drug. As confirmed by PXRD and TGA, 5-FU containing sample
18 maintains its crystallinity (Fig. S3 and Fig. S4), thus, the drug encapsulation did not
19 alter the structure of these materials. Only a decrease in the intensity of the low angle
20 reflections on the PXRD patterns (~5-8° 2 θ) was observed after encapsulation,
21 following the change in pore content that is known to strongly affect the relative
22 intensities of the Bragg peaks^{2b}. This was confirmed by N₂ adsorption analyses
23 showing that the BET surface area significantly decrease upon drug molecules loading
24 (see Supplementary Information Fig. S5).

25 Incorporation of the drug molecule during loading process has been recorded by
26 Fourier transformed infrared spectroscopy (FTIR) (Figure S6). The absorption bands
27 of C–F deformations were discovered in the 820–550 cm⁻¹ regions. The absorption
28 band at about 1240 cm⁻¹ may be due to fluorine atom on the ring [25-26]. Based on
29 the above structural analyses, these two compounds may be taken as a good drug
30 carrier. The loading of anticancer 5-FU was carried out by impregnating **NTU-Z11**

1 and **GDMU** under stirring in 5-FU containing ethanol solutions.

2 UV-vis absorption spectroscopy has been used to determine the effective storage
3 capacity, To reach a maximal drug loading, 5-FU to porous solid relative ratio and
4 contact time were evaluated (Table S5)[6]. The loading amount of 5-FU increased
5 with initial 5-FU/material ratio repressed in weight and optimal value 1:1 and 1:3 for
6 **NTU-Z11** and **GDMU** in ethanol, respectively. The contact time was also important,
7 the maximum adsorption was obtained after 2 days and 3 days for **NTU-Z11** and
8 **GDMU**, respectively. Thus, the best results were obtained when **NTU-Z11** was
9 soaked for 2 days within a 5-FU to material weight ratio of 1:1, while **GDMU** was
10 soaked for 3 days within a 5-FU to material weight ratio of 1:3. 5-FU was
11 incorporated into desolvated **NTU-Z11** and **GDMU** with loadings of 0.382 and 0.206
12 g/g, respectively. The difference between **NTU-Z11** and **GDMU** shows that the
13 $\text{NH}_2(\text{CH}_3)_2$ takes as gate and blocks the drug molecules access to inner pores [27].

14 Fig. 2 shows the release profile of the drug delivery system of **NTU-Z11** and
15 **GDMU** in PBS solution at 37 °C. At the first stage (24 hours), the **NTU-Z11** and
16 **GDMU** have the similar releasing behavior and approximately 65 % of the drug was
17 released. However, the other part released gradually in **GDMU**, implying a strong
18 host-guest interaction involved in this process. Compared with the **NTU-Z11** carrier,
19 there is a big cation in the host channels in **GDMU**, which can take as donor/acceptor
20 and bind to drug molecules resulting in the dramatically releasing behavior. Thus,
21 5-FU with flat molecular shape diffuses along the hexagonal channels. Similar results
22 were also found in MIL-53 with a pore size of 8.6 Å exhibited a drug loading capacity
23 of 0.22 g/g for drug IBU (IBU = ibuprofen) [3].

24 To further explore the pH-responsive drug release feature of **NTU-Z11**, release
25 profile were performed in pH 6.0, 9.18 and water medium. Around 62.5% of the
26 loaded 5-FU was released fast within 24 h, and 63.1% within 30 h. More than 40% of
27 5-FU released around one hour, which consistent with dissolution of **NTU-Z11** in
28 acidic environment. Compared with other MOF carriers[28], **NTU-Z11** shows a fast
29 release rate for 5-FU. In the water medium, the released profile of 5-FU exhibits a flat
30 shape and occurs no burst effect. The delivery of 5-FU occurred within 96 h and 47 %

1 of the loaded drug was released. However, three stages related to the drug release
2 could be distinguished in pH 9.18, around 48% of the loaded drug was released in the
3 first stage (33 h) and only almost not more than 10% of the loaded drug was released.
4 Thus, a rapid releasing process was observed during the first stage followed by a
5 slower in the high pH. These results imply that the loaded drug can be decreased
6 during blood circulation and the drug release rate is suddenly accelerated after release
7 into cancer cells [25, 29].

8 **Computational Simulations of 5-FU Adsorption**

9 The amount of drug per porous material or drug loading is one of the main
10 quantities of interest in the use of MOFs for controlled drug release [30]. We have
11 used GCMC simulations to investigate the loading of 5-FU to two compounds at the
12 molecular level. These simulations were used to determine the preferential binding
13 sites of the 5-FU in the porous materials, to estimate the maximum drug loading
14 capacity of each material, and propose a molecular mechanism for drug loading and
15 release.

16 **Adsorption isotherm of 5-FU in MOFs**

17 We calculated the adsorption isotherms of 5-FU in **NTU-Z11** and **GDMU** 298 K.
18 As observed in Figure 3, there are some differences between **NTU-Z11** and **GDMU**.
19 The **NTU-Z11** has much higher saturation capacity for 5-FU, which is about 0.4 g/g.
20 The saturation capacity is around 0.22 g/g for **GDMU**. The bigger molecules of
21 **GDMU** result in a low saturation capacity compared to that of **NTU-Z11**. Also,
22 **GDMU** show a saturation uptake at the low fugacity range due to the stronger
23 5-FU-MOF interactions. The presence of stronger interaction due to the existence of
24 cations in **GDMU** strengthens the host-guest interactions and results in the steep
25 adsorption of 5-FU at lower fugacity than in **NTU-Z11**.

26 **Heat of adsorption**

27 The heats of adsorption (Q_{st}) for 5-FU in **NTU-Z11** and **GDMU** studied are shown
28 in Fig. 4. The heat of adsorption is closely related with the pore structure, in which
29 could be taken as an index of the adsorption materials heterogeneity [30]. Fig. 4

1 shows the Q_{st} for **NTU-Z11** and **GDMU** as the function of uptake. As observed in
2 Fig.4, the **NTU-Z11** shows the low Q_{st} (about 120-150 kJ/mol) at the loadings process.
3 This observation shows that the 5-FU molecules can load into MOFs pores with
4 strong interaction. The stronger interaction results in the higher adsorption heat of
5 5-FU than in **NTU-Z11** because of the presence of DMF in **GDMU**. The **GDMU**
6 shows the higher Q_{st} (160-228 kJ/mol) at the range of loadings. The medicine
7 molecules can be strongly retained in the MOF structures due to the high Q_{st} at the
8 loadings and it is very favorable for the long release process. **GDMU** shows higher
9 Q_{st} values than **NTU-Z11** at high loadings, with the important contributions of the
10 solvent molecules. The results are consistent with experimental released process.

11 **Density plots**

12 **NTU-Z11** consists of the trimetric SBU and BTC ligand. The 3-D framework has
13 two channel systems with dimension of $7.5 \times 7.5 \text{ \AA}$ (refer to as A) and $11.5 \times 11.5 \text{ \AA}$
14 (refer to as B) along the *c*-axis. As observed in Fig. 5, the 5-FU molecules are
15 primarily distributed in the two favorable regions. The 5-FU loading is closely packed
16 in the pores because the solvent molecules have a smaller size in A region. The bigger
17 cations present in **GDMU** hinder the adsorption of 5-FU in A region. Then the
18 adsorption of 5-FU in **NTU-Z11** increases with the increase of fugacity. However, the
19 adsorption of 5-FU in **GDMU** rapidly approaches to a platform at same range of
20 pressure.

21 **Conclusion**

22 In summary, two isostructural nanoporous MOFs were used to load anti-cancer
23 chemotherapy drug 5-FU and demonstrated a remarkable different capacity due to
24 their various pore spaces. Owing to pH-sensitive property of **NTU-Z11**, it was
25 observed that it released much faster in mild acidic buffer solution than at a neutral
26 medium, suggesting that this pH-triggered feature may be useful property for drug
27 delivery to tumors. GCMC simulations suggested that the anti-cancer drug 5-FU
28 could load to the **NTU-Z11** in high loading capacity. Our findings indicate that the
29 combined experimental-computational approach is a powerful strategy for the
30 efficient identification and incorporation of bioactive compounds in porous materials.

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Main Figures and Tables

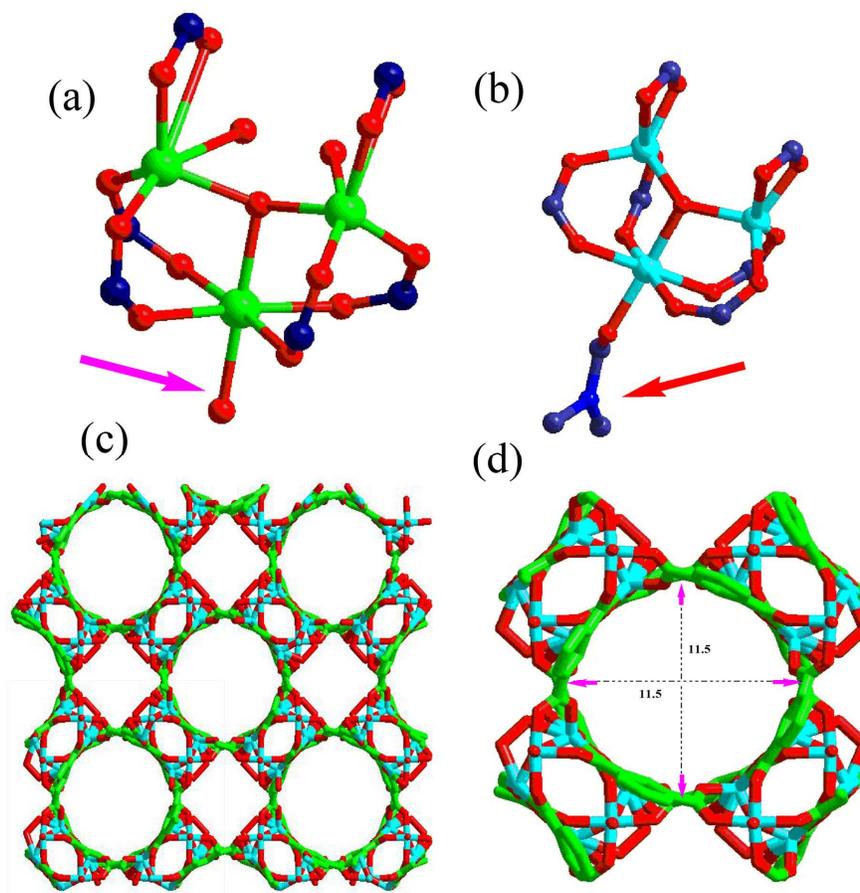


Fig. 1 (a) the geometries of metal and ligands in NTU-Z11; (b) view of the geometries of the metal and ligands in **GDMU**; (c) view of the 3D frameworks and (c) the larger hexagonal channel in the MOFs.

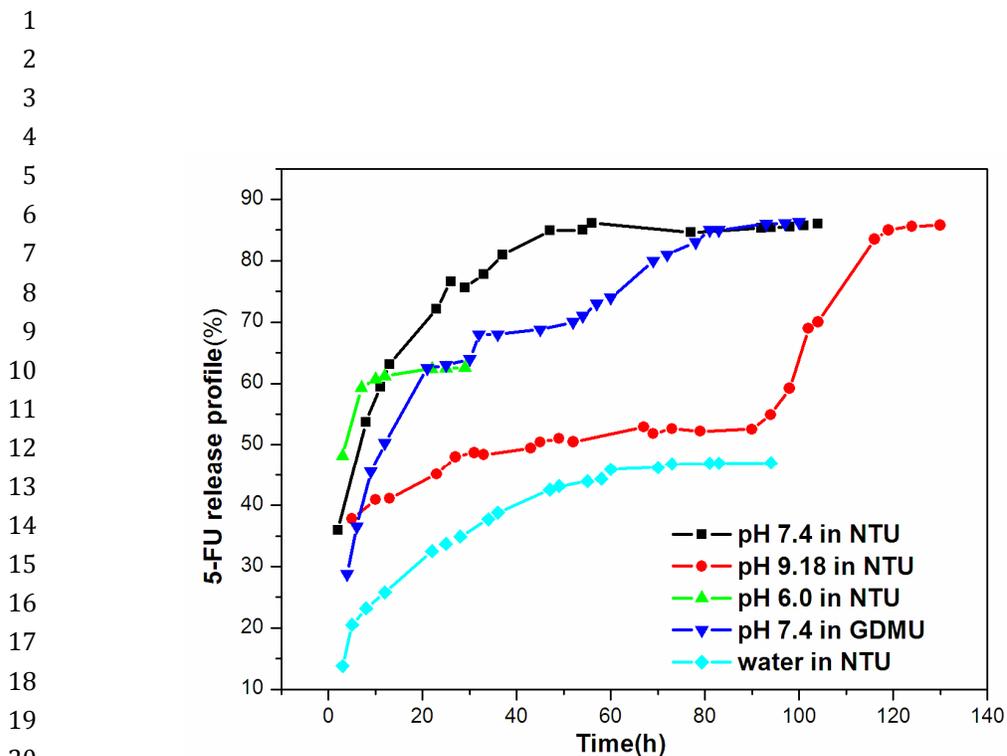


Fig.2 5-FU delivery (% 5-FU vs. t) from NTU and GDMU and schematic illustration shows the 5-FU load and release process.

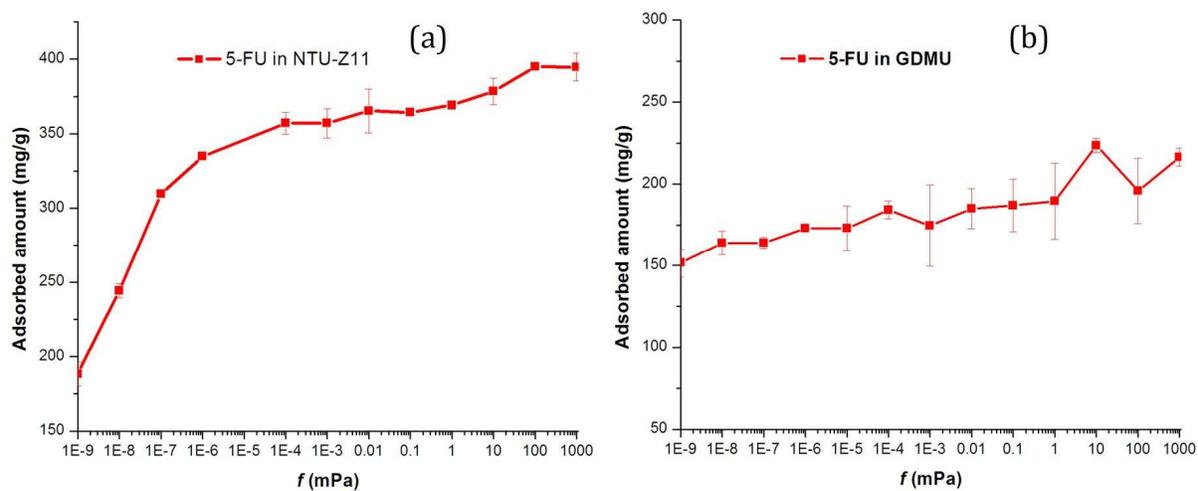
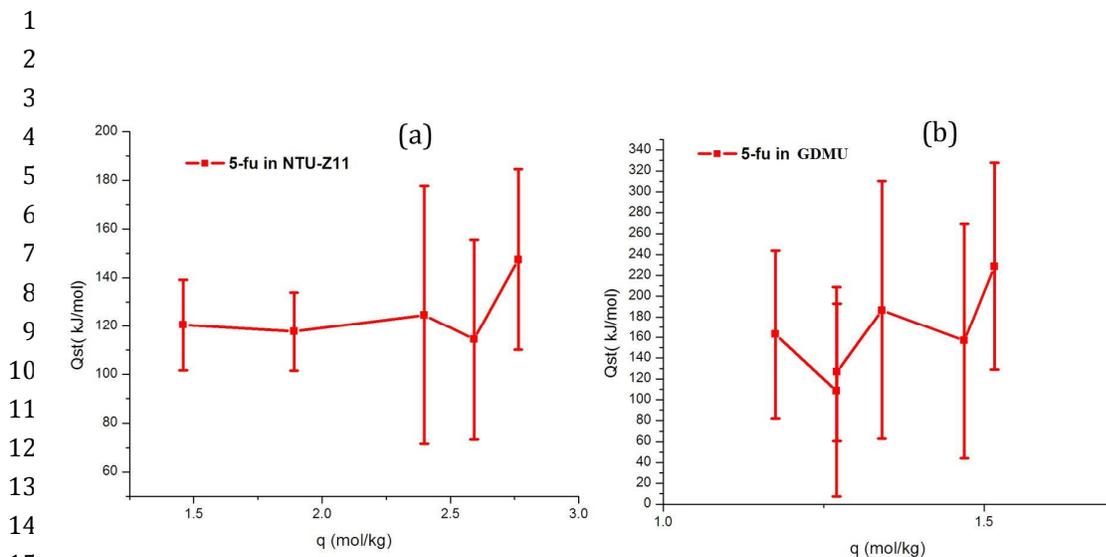
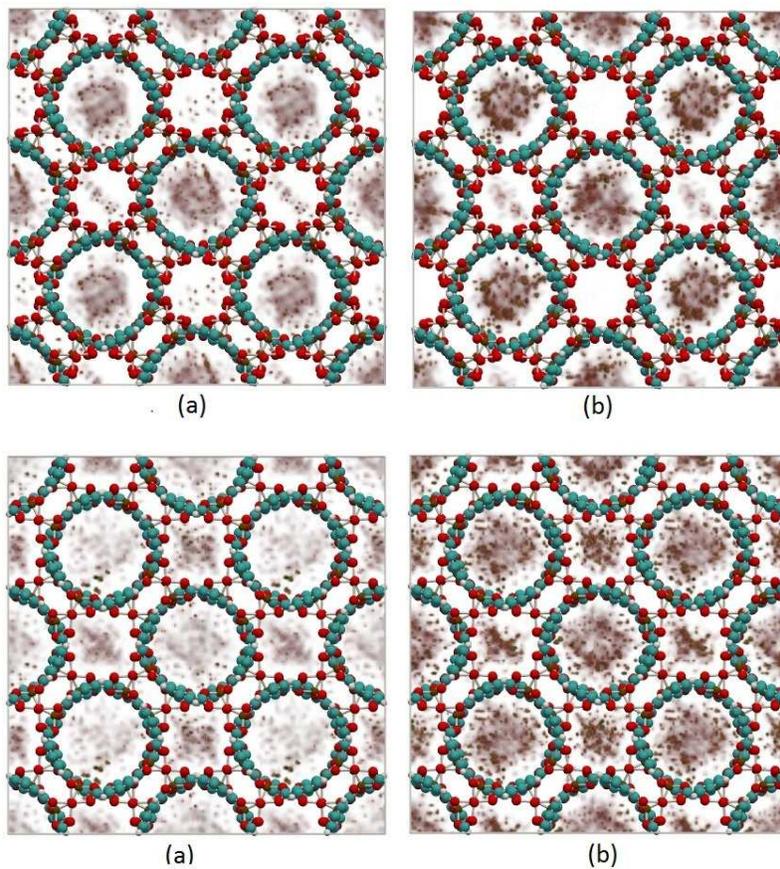


Fig. 3 (a) and (b) the calculated adsorption isotherm of 5-FU in NTU-Z11 and GDMU at 298K, respectively.



17 Fig. 4 (a) and (b) the calculated heats of adsorption of 5-FU in **NTU-Z11** and **GDMU** at 298K,
18 respectively.



42 Fig. 5 The density of 5-FU in **GDMU** at 298 K (a) 10^{-9} mPa (b) 10^{-7} mPa (above) and The
43 density of 5-FU in **NTU-Z11** at 298 K (a) 10^{-9} mPa (b) 10^{-7} mPa (below).

Table 1. Crystal data and structure refinement information for compound **GDMU**

Crystal system	tetragonal
Space group	<i>I 4 c m</i>
Crystal color	Colorless
<i>a</i> , Å	20.5138(10)
<i>c</i> , Å	17.8100(8)
γ	90
<i>V</i> , Å ³	7494.7(8)
<i>Z</i>	8
ρ_{calcd} , g/cm ³	1.531
<i>F</i> (000)	3536
θ Range, deg	2.49-27.92
Reflns collected/unique(<i>R</i> _{int})	21512/ 4425 (0.0299)
GOF	1.092
<i>R</i> ₁ , <i>wR</i> ₂ (<i>I</i> > 2 σ (<i>I</i>))*	0.0319, 0.0900
<i>R</i> ₁ , <i>wR</i> ₂ (all data)**	0.0357, 0.0924

* $R = \sum(F_o - F_c) / \sum(F_o)$, ** $wR_2 = \{\sum[w(F_o^2 - F_c^2)^2] / \sum(F_o^2)^2\}^{1/2}$.

Table 2. Selected bond distances (Å) and angles (deg) of structure **GDMU**

Zn1-O1	1.945(4)	Zn1- O8	1.9458(17)
Zn1- O4	1.969(3)	Zn1- O5	1.972(3)
Zn2- O7	2.059(5)	Zn2- O3	2.091(3)
Zn2- O3	2.091(3)	Zn2- O8	2.103(4)
Zn2- O6	2.106(3)	Zn2- O6	2.106(3)
O1- Zn1 -O8	113.76(18)	O1- Zn1- O4	123.14(16)
O8- Zn1- O4	105.27(16)	O1- Zn1- O5	103.53(16)
O8 -Zn1- O5	103.27(17)	O4- Zn1- O5	105.86(18)

1	07 -Zn2- 03	86.24(14)	03- Zn2- 03	97.10(17)
2	07- Zn2 -08	171.1(2)	03 -Zn2 -08	87.85(12)
3	03- Zn2 -08	87.85(12)	07- Zn2- 06	91.29(15)
4	03 -Zn2- 06	173.17(14)	03- Zn2- 06	89.08(15)
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