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1 **A biosensing platform for sensitive detection of concanavalin A based on**
2 **fluorescence resonance energy transfer from CdTe quantum dots to graphene oxide**

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1 In this paper, we constructed a novel fluorescence resonance energy transfer (FRET) system between
2 CdTe quantum dots (QDs) and graphene oxide (GO) for sensitive detection of concanavalin A (Con
3 A). In this system, CdTe QDs as an energy donor and GO as an energy acceptor were both covalently
4 functionalized by glucosamine via an amide linkage. The specific combination of Con A with
5 glucosamine could bring CdTe QDs and GO into appropriate proximity and therefore induce efficient
6 energy transfer. The concentration of Con A caused the modulation of the energy transfer efficiency
7 between GO and QDs, thus enabling the Con A detection. Under the optimized experimental
8 conditions, the decrease of fluorescence intensity ratio I/I_0 (I_0 and I were the fluorescence intensity of
9 the sensing system in the absence and presence of Con A, respectively) is proportional to the
10 concentration of Con A in the range of 9.8-196.1 nM. This method has high sensitivity with the
11 detection limit as low as 3.3 nM. The results suggested that the graphene FRET platform could be
12 used for sensitive and selective sensing of Con A and could be applied for protein-carbohydrate
13 studies.

14

15 **Key words:** Graphene oxide; CdTe quantum dots; Fluorescence; Concanavalin A.

1 Introduction

2 Graphene with fascinating thermal, electronic and mechanical properties has attracted persistent
3 attention in nanoelectronic devices, electron transportation and supercapacitor since its discovery.¹⁻³
4 Graphene oxide (GO), an intermediate obtained during the graphene preparation by modified
5 Hummer's method, has numerous kinds of hydrophilic functional groups on its surfaces and edges,
6 such as epoxy, carboxyl and hydroxyl groups to enable its high water dispersibility and facile surface
7 modification.⁴⁻⁷ Semiconductor quantum dots (QDs), a type of promising fluorescent materials, have
8 been widely used as effective energy transfer donor due to their unique optical properties such as high
9 quantum yield, narrow emission peaks and tunable size-dependent emission.^{8,9} In the previous studies,
10 scientists have devoted their attentions to develop fluorescence assays based on the high efficiency
11 energy transfer between GO and fluorescent dyes, such as DNA assays,¹⁰⁻¹² proteins assays,^{13,14} and
12 other molecules.¹⁵⁻¹⁷ Researchers discovered that GO also had an extraordinary quenching efficiency
13 for various kinds of quantum dots, such as CdSe, CdTe and CdSe-ZnS.¹⁸⁻²¹ For example, Li *et al.*
14 reported a fluorescence method for sensitive detection of matrix metalloproteinase and thrombin
15 activity using a protease substrate peptide as the linker between the donor (CdSe-ZnS QDs) and the
16 acceptor (GO).¹⁸ The high efficiency of GO in quenching the donor emission make it a perfect
17 selection to develop new fluorescence sensors in analytical chemistry.

18 Recently, a class of proteins that could interact with many carbohydrates by means of specific
19 molecular recognition came into the forefront of biological research, such as concanavalin A (Con A)
20 and peanutagglutinin (PNA).²²⁻²⁷ It is well known that concanavalin A is a legume lectin from Jack
21 beans containing four identical binding sites. Each monomer subunit of Con A is approximately
22 4×4×4 nm with a single small binding site capable of binding to α -D-glucopyranose with unmodified

1 hydroxyls at positions C3, C4 and C6.²⁸⁻³⁰ In addition, Con A has been shown to interact with many
2 mannosyl and glucosyl residues of polysaccharides, such as dextran, β -cyclodextrin, chitosan and
3 glycodendrimer.^{25, 31-34} Carbohydrate recognition is predominant in many important functions, such
4 as cell-surface recognition, host pathogen interactions, cell-cell interactions and immune response.
5 Studying on the carbohydrate-protein interactions have been developed because it is the foundation of
6 the pathogen detection and prevention of bacterial infection. Although various methods have been
7 widely used for Con A detection, some of them are time-consuming, technical expertise and low
8 sensitivity.³⁵⁻³⁹ Thus, fluorescence methods have been devoted to overcome such shortcomings due to
9 their simplicity, convenience and high sensitivity. The fluorometric assays for lectin detection were
10 generally based on the agglutination of sugar-QDs,^{27, 40} for example, Badu and co-workers reported a
11 assay for lectin detection through the agglutination of carbohydrates stabilized CdSe-ZnS QDs.⁴⁰ Few
12 methods had been exploited with the combination of CdTe QDs and GO to develop for fluorescence
13 Con A determination.

14 The previously reported FRET models based on graphene oxide as a fluorescence quencher most
15 rely on the π - π stacking interaction. In this work, we constructed a different model in which donor and
16 acceptor were brought into FRET proximity through specific molecular recognition. The present
17 fluorescence sandwich assay for Con A detection was based on the FRET between CdTe quantum
18 dots and graphene oxide (GO). In this system, Con A was firstly interacted with glucosamine
19 functionalized GO (GO-G) to form GO-G/Con A hybrid, and subsequently the free identical binding
20 sites of Con A specifically combined with glucosamine modified QDs (QDs-G) to form a sandwich
21 configuration (GO-G/Con A/QDs-G), which allowed QDs-G and GO-G to be in appropriate
22 proximity. Then the fluorescence of QDs-G could be quenched by GO-G, and therefore assembled an

1 efficient FRET biosensing system for Con A detection. Compared with the previous reports, the
2 proposed sandwich method is simpler and more sensitive and can possibly provide a versatile tool for
3 the analysis of different kinds of lectins containing several binding sites with high sensitivity just by
4 exchanging the carbohydrates functionalized on the QDs and GO.

5 **2. Experimental**

6 **2.1 Reagents and chemicals**

7 All chemicals used were of analytical reagent grade and used without further purification. Graphite
8 powder and Tris(hydroxymethyl)aminomethane (Tris) were attained from Sinopharm Chemical
9 Reagent Co. Ltd. (China). Tellurium powder (200 mesh, 99.8%), cadmium chloride (CdCl_2 , 99+%),
10 Mercaptopropionic acid (MPA) (99%), glucosamine and Con A were obtained from Sigma-Aldrich
11 Chemical Co. 1-ethyl-3-(3-dimethylaminopropyl) carbodiimide hydrochloride (EDC) and
12 *N*-Hydroxy-sulfosuccinimide (NHS) were purchased from Aldrich Chemical Co. Ltd. Bovine serum
13 albumin (BSA), trypsin, pepsin, human serum albumin (ALH) and lysozyme (Lys) were attained from
14 Sino-American Biotechnology Co. Ltd. The water used in all experiments had a resistivity higher than
15 $18 \text{ M}\Omega \text{ cm}^{-1}$.

16 **2.2 Instrumentation**

17 The FT-IR spectra were recorded on a Nicolet 400 Fourier transform infrared spectrometer.
18 Fluorescence measurements were performed on a Shimadzu RF-5301 PC spectrafluorophotometer
19 with a 1 cm path-length quartz cuvette. The fluorescence spectra were recorded with the excitation
20 wavelength of 400 nm. The slit widths of the excitation and emission were 5, 10 nm, respectively.

21 **2.3 Synthesis of graphene oxide**

22 Graphene oxide was prepared by a modified Hummer's method and characterized in our previous

1 work⁴¹. Briefly, graphite powder (2 g) was added to 98% H₂SO₄ (12 mL) consisting of K₂S₂O₈ (2.5 g)
2 and P₂O₅ (2.5 g) and reacted for 4.5 h at 80 °C. The mixture was then diluted with 0.5 L water. Then,
3 the mixture was filtered and washed with water to remove the residual acid. The product was dried
4 under ambient conditions overnight. This pre-oxidized graphite was stirred in 98% H₂SO₄ (120 mL),
5 KMnO₄ (15 g) was gradually added while keeping the temperature < 20 °C. This mixture was stirred
6 at 35 °C for 30 min and 90 °C for 90 min. Afterwards, the mixture was diluted with water (250 mL)
7 and kept at 105 °C for 25 min. After the resulting mixture was stirred for 2 h, the reaction was
8 terminated by addition of 0.7 L water and 20 mL of 30% H₂O₂. For purification, the mixture was
9 filtered and washed with 1:10 HCl aqueous solution and water many times. Finally, the product was
10 further purified by dialysis for 1 week to remove the remaining metal species. The obtained dispersion
11 was centrifuged at 10000 rpm to remove any unexfoliated GO. The supernatant solution was collected
12 and freeze dried. The GO powder was redispersed in water to obtain 0.5 mg mL⁻¹ GO stock solution.

13 **2.4 Synthesis of MPA-capped CdTe quantum dots**

14 CdTe QDs were synthesized by refluxing routes as described in detail in our previous paper.⁴² Briefly,
15 the precursor solution of CdTe QDs was formed in water by adding fresh NaHTe solution to CdCl₂
16 solution at pH 11 in the presence of MPA as stabilizing agent in N₂ atmosphere. Cd²⁺/MPA/HTe⁻
17 ratio was set at 1:2.4:0.5. The CdTe precursor solution was subjected to reflux at 100°C under
18 open-air conditions with condenser attached, and CdTe QDs with different sizes would be obtained at
19 different refluxing time. The fluorescence emission wavelength of CdTe QDs used in this study was
20 630 nm.

21 **2.5 Preparation of glucosamine functionalized CdTe QDs and GO**

22 The synthesis of glucosamine functionalized CdTe QDs (QDs-G) and GO (GO-G) were both carried

1 out using the EDC and NHS linkage reaction for covalently attaching the glucosamine to the carboxyl
2 groups of the QDs and GO via amide bond formation. In a typical experiment, appropriate amount of
3 EDC and NHS were respectively added to the CdTe QDs and GO solution with stirring for 30 min.
4 Next, glucosamine was added to the above solutions and incubated 3 h with continuous gentle mixing.
5 After the reaction was complete, the solution of GO-G was filtered and washed with water to move
6 free glucosamine as well as other molecules. In order to block the adsorption site of GO-G surface,
7 the obtained GO-G was dissolved in water consisting of 0.5% Tween 20. The QDs-G solution was
8 precipitated by centrifugation at 8000 rpm for 10 min after the addition of ethanol, then redissolved
9 in water and stored at 4 °C in the darkroom.

10 **2.6 Fluorescence experiments**

11 In our experiment, the detection of Con A was carried out in Tris-HCl buffer solution (20 mM, pH 7.0)
12 at room temperature. Con A was dissolved in Tris-HCl buffer solution (20 mM, pH 7.0) augmented
13 with CaCl₂ (0.5 mM) and MnCl₂ (0.5 mM) to obtain a stock solution (1.0 mg mL⁻¹) that was stored at
14 4°C. 15 µg mL⁻¹ GO-G was mixed with different concentrations of Con A and incubated for 1 h, and
15 then 20 µL QDs-G was added into above solution and allowed to react for 30 min before
16 measurement. The fluorescence spectra were recorded in the 500–780 nm emission wavelength range
17 with the excitation of 400 nm.

18 **3. Results and discussion**

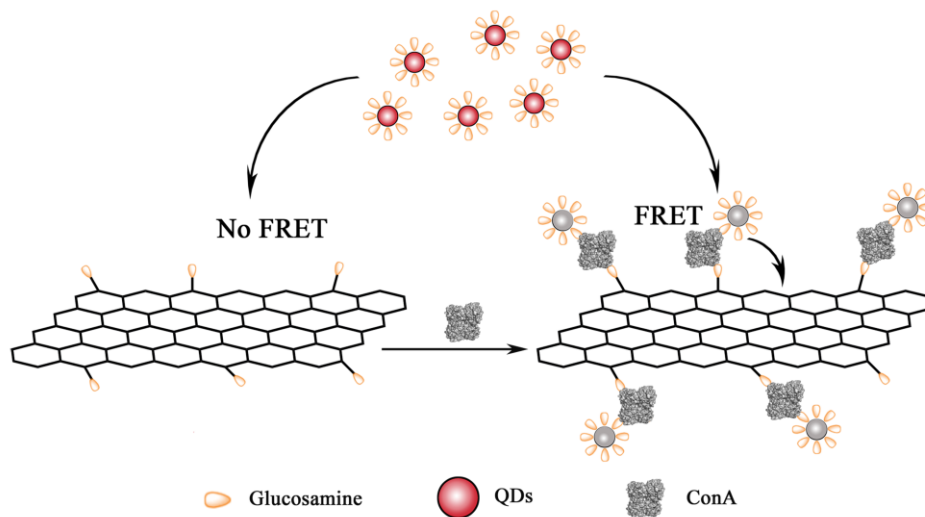
19 **3.1 FT-IR spectra of CdTe QDs, QDs-G, GO and GO-G.**

20 Glucosamine functionalized CdTe quantum dots (QDs-G) and graphene oxide (GO-G) complex were
21 obtained by covalently linking glucosamine with the carboxyl group of CdTe quantum dots (QDs) and
22 graphene oxide (GO) in our study. Fig. S1 and Fig. S2 showed the FT-IR spectra of the CdTe QDs,

1 QDs-G, GO and GO-G. For the QDs-G and GO-G complex, the peak at $\sim 1035\text{ cm}^{-1}$ was the signature
2 of C-O bond in glucosamine. As seen in Fig.S1 the amide I band (1656 cm^{-1}) for amide-carbonyl
3 stretching vibration appeared which was due to the conjugation of glucosamine to the MPA-capped
4 CdTe QDs. It can be seen from Fig. S2 that the amide II band (1560 cm^{-1}) and the amide III band
5 (1384 cm^{-1}) for -CONH group were appeared, suggesting that the GO was modified with glucosamine
6 via amide bound.

7 **3.2 Design of the fluorescence sensing system**

8 A previous study reported that GO could quench the fluorescence of QDs when brought GO and QDs
9 into appropriate proximity.¹⁸ The biosensing platform for concanavalin A (Con A) detection is based
10 on the modulation of the fluorescence resonance energy transfer (FRET) efficiency between the
11 glucosamine functionalized CdTe QDs (QDs-G) and GO (GO-G) complex. The mechanism of
12 GO-based sensing system is outlined in scheme 1. The specific combination of Con A with
13 glucosamine allows GO-G and QDs-G to be in proximity, resulting in the efficient fluorescence
14 quenching. As shown in Fig. 1A, the fluorescence of QDs-G was greatly quenched by GO-G hybrid
15 in the presence of Con A, while the fluorescence quenching of QDs-G in the absence of Con A was
16 only 80.2% of its original intensity. Considering that GO-G complex could influence the fluorescence
17 intensity of QDs-G, the effect of incubation times of GO-G on the fluorescence of QDs-G without
18 Con A was investigated firstly. As demonstrated in Fig. 1B, a slow decrease in the fluorescence
19 intensity of QDs-G/GO-G system was observed and the fluorescence intensity gradually decreased
20 before 10 min and was relatively stable after 10 min. It implied that GO-G was not responsible for
21 further fluorescence quenching in the following experiment.

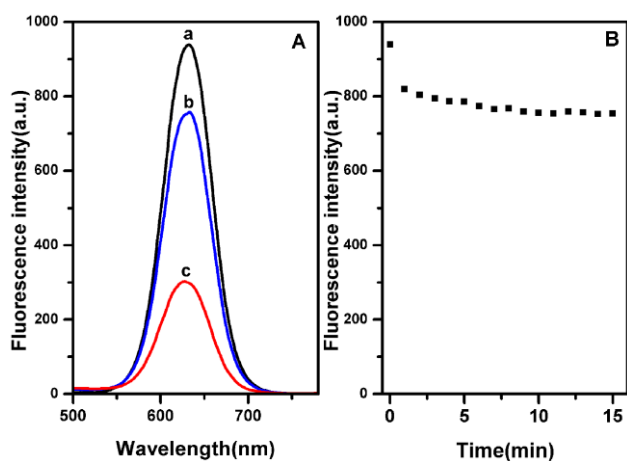


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2 **Scheme 1** Schematic illustration of the GO-based fluorescence resonance energy transfer platform for concanavalin A

3 detection.

4



5

6 **Fig.1** (A) The fluorescence spectra of QDs-G (a) and GO-based sensing system in the absence (b) or presence (c) of

7 Con A. (B) The effect of incubation times of GO-G on the fluorescence of QDs-G without Con A.

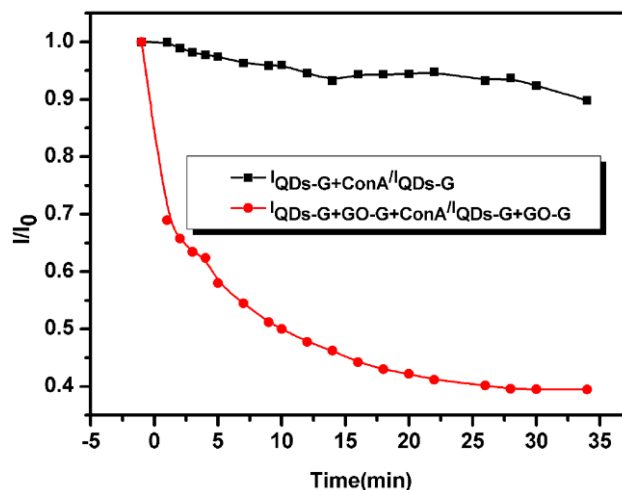
8 **3.3 The influence of incubating time**

9 In order to achieve the maximum sensitivity for Con A detection, we studied the effect of incubation

10 times on the fluorescence of sensing system. Fig. 2 showed the fluorescence intensity changes as a

11 function of incubating time in the absence and presence of GO-G. In the presence of GO-G, the

1 fluorescence intensity ratio I/I_0 (I_0 and I referred to the fluorescence intensity of QDs-G/GO-G system
2 in the absence or presence of Con A, respectively) decreased rapidly with the increasing of incubation
3 time and reached a plateau within 30 min at room temperature. So we chose 30 min as the optimal
4 reaction time in the following experiments. To demonstrate that the fluorescence quenching of QDs-G
5 was resulted from the existence of GO-G in the presence of Con A, the effect of Con A on the
6 fluorescence of QDs-G was performed in the absence of GO-G. From Fig. 2, it could be seen that the
7 fluorescence intensity ratio I/I_0 (I_0 and I referred to the fluorescence intensity of QDs-G in the absence
8 or presence of Con A, respectively) decreased gradually with the increasing of incubation time in the
9 absence of GO-G. The fluorescence quenching extent of QDs-G/GO-G system was obviously greater
10 than that of QDs-G system, which indicated that the fluorescence quenching of QDs-G was more
11 efficient by using GO-G as a fluorescence quencher.

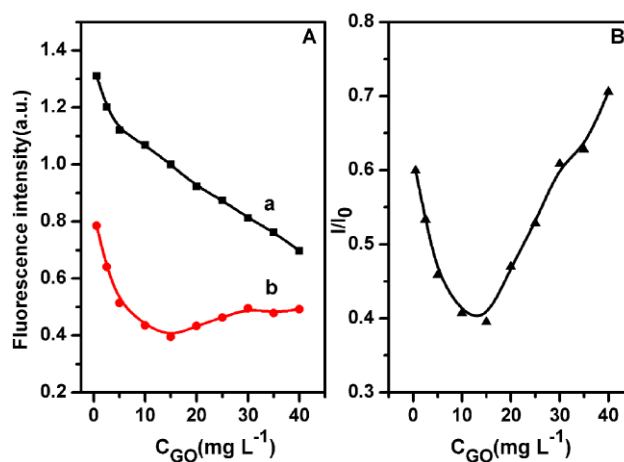


12
13 **Fig. 2** The effect of incubating time on the fluorescence intensity of QDs-G in the absence (Square) and presence
14 (Circle) of GO-G.

15 3.4 The optimized concentration of GO-G

16 The concentration of GO-G is also a key parameter in the sensing system for sensitive Con A
17 detection. A series of different concentrations of GO-G hybrid were incubated in the fixed Con A and

1 subsequently incubated in the solution of QDs-G to form a sandwich configuration (GO-G/Con
 2 A/QDs-G). As shown in Fig. 3A, the fluorescence of QDs-G was quenched with the increasing
 3 amount of GO-G without the existence of Con A. However, in the presence of Con A, the
 4 fluorescence intensity decreased obviously when the concentration of GO-G complex below 15 mg
 5 L⁻¹. Con A could specifically combine with the GO-G to form more GO-G/Con A hybrid, the free
 6 binding sites of Con A on the formed GO-G/Con A hybrid could capture QDs-G and bring QDs-G and
 7 GO-G into appropriate proximity, resulting in the remarkable fluorescence quenching. When the
 8 concentration of GO-G was higher than 15 mg L⁻¹, the free binding sites of Con A on the formed
 9 GO-G/Con A hybrid would continually bind to the excess GO-G before the addition of QDs-G,
 10 leading to the less fluorescence quenching. Fig. 3B showed the relationship between the fluorescence
 11 intensity ratio I/I_0 (I_0 and I referred to the fluorescence intensity of QDs-G with different
 12 concentrations of GO-G hybrid in the absence or the presence of Con A, respectively) and the
 13 concentrations of GO-G hybrid. It could be seen that the fluorescence intensity ratio I/I_0 decreased
 14 with the increasing concentrations of GO-G up to 15 mg L⁻¹ and then increased. Therefore, 15 mg L⁻¹
 15 of GO concentration was chosen as the optimal concentration in the following experiments.

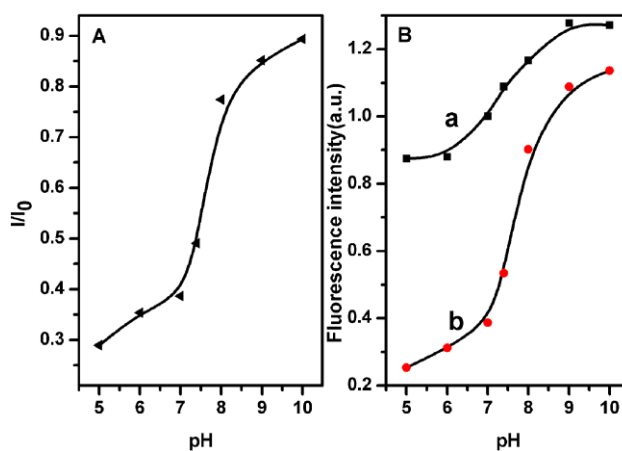


16
 17 **Fig. 3** The influence of the different concentrations of GO-G on the concanavalin A detection system. (A) The

1 fluorescence intensity of the GO-based sensing system in the absence (a) or presence (b) of Con A. (B) The
2 fluorescence intensity ratio I/I_0 of the sensing system (I_0 and I referred to the fluorescence intensity of QDs-G with
3 different concentration of GO-G hybrid in the absence or presence of Con A, respectively).

4 3.5 The effect of pH

5 Con A appears to be dimeric below pH 5.5 and exists as a tetramer when the pH was higher than 7.0.
6 And there is a smooth transition between the dimer and tetramer as a function of the pH value.⁴³
7 Therefore, we systematically investigated the effect of pH on the sandwich assay for Con A. From Fig.
8 4A, it could be observed that the fluorescence intensity ratio I/I_0 increased with the increase of pH in
9 the range of pH 5-10. When pH value was lower than 7.0, the fluorescence intensity ratio I/I_0
10 increased slowly, which might be ascribed to the isoforms of Con A in different pH values. However,
11 high pH value caused the denaturation of Con A, resulting in low binding amount of Con A and the
12 rapid increasing of the fluorescence intensity ratio I/I_0 . The fluorescence intensity of the sandwich
13 system with and without of Con A at different pH were also shown in Fig. 4B. To ensure higher
14 sensitivity of the sensing system, a pH 7.0 Tris-HCl buffer solution was selected for the determination
15 of Con A.



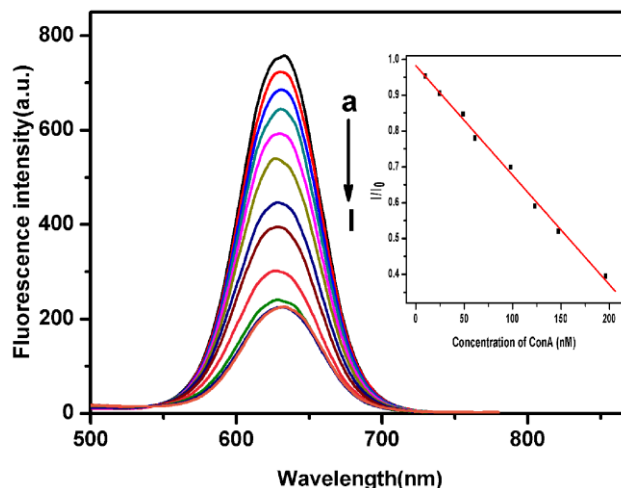
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17 **Fig. 4** The effect of the pH on the sensing system. (A) The fluorescence intensity ratio I/I_0 of the sensing system (I_0 and

1 I referred to the fluorescence intensity of sensing system at different pH value in the absence or the presence of Con A,
2 respectively). (B) The fluorescence intensity of the GO-based sensing system in the absence (a) or presence (b) of Con
3 A.

4 **3.6 Con A detection**

5 To further study the performance of the GO-based sandwich assay for Con A detection, we
6 investigated the fluorescence emission spectra of this system with different concentrations of Con A
7 under the optimized conditions. As shown in Fig. 5, the fluorescence intensity of QDs-G decreased
8 upon the increasing concentration of Con A from 0 to 392.2 nM. The inset of Fig. 5 showed a good
9 linear relationship between the fluorescence intensity ratio I/I_0 (I_0 and I were the fluorescence
10 intensity of the sensing system in the absence and presence of Con A, respectively) and the
11 concentrations of Con A in the range of 9.8 to 196.1 nM with a correlation coefficient $R^2 = 0.994$. The
12 linear regression equation was $I/I_0 = 0.982 - 0.003C_{\text{Con A}}$ (nM) and the detection limit for Con A was
13 found to be 3.3 nM based on 3σ rule, the standard deviation for six replicate measurements of 24.5
14 nM Con A was 1.0%. These results indicated that the sensing system could be applied to quantitative
15 determination of Con A with high sensitivity. Compared with the previous reports for Con A
16 determination in linear range and detection limit (Table 1), our method obtained the similar or
17 superior detection limit and linear range.

18



1

2 **Fig.5** Fluorescence emission spectra of the sensing system with different concentrations of Con A, a-1 represented the
 3 concentrations of Con A of 0, 9.8, 24.5, 49.0, 61.3, 98.0, 122.5, 147.1, 196.1, 245.1, 294.1 and 392.2 nM. The inset
 4 showed the calibration curve between the fluorescence intensity ratio I/I_0 and the concentrations of Con A in the range
 5 of 9.8 to 196.1 nM (B). I_0 and I referred to the fluorescence intensity of the proposed system in the absence or the
 6 presence of Con A, respectively.

7

8 **Table 1** Comparison of different methods for the detection of Con A.

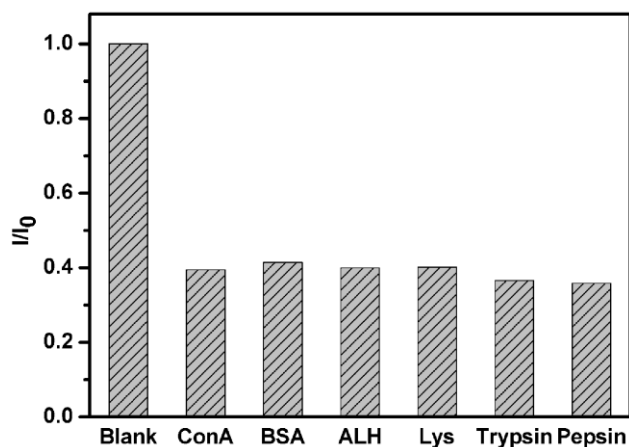
Methods	Linear range (nM)	Detection limit (nM)	Ref.
Electrochemistry	2-80	0.8	[37]
	1.96×10^{-3} -98	1.5×10^{-3}	[38]
Colorimetry	40-100	40	[39]
	80-260	100	[39]
Surface plasmon resonance	9.8-196.1	3.8	[31]
	98.0-588.2	11.2	[40]
Fluorometry	20-1000	0.8	[14]
	1.96-196	0.73	[24]
	0-150	1.5	[26]
	9.8-196.1	3.3	This work

9

10 3.7 Interference study

11 The selectivity of the GO-based sensing system was studied in the paper. Potential interference

1 substances such as bovine serum albumin (BSA), human serum albumin (ALH) and lysozyme (Lys),
2 trypsin and pepsin were examined to assess the selectivity of the presented method for Con A
3 detection. The interference study was carried out at a Con A concentration of 196.1 nM by monitoring
4 the fluorescence response of the sensing system to other coexistence substances. Blank represented
5 the fluorescence intensity ratio I/I_0 of the sensing system without Con A. The concentration of BSA
6 and ALH were 5-folds of Con A, and the concentrations of Lys, trypsin and pepsin were about
7 10-folds higher than Con A. Fig. 6 showed the changes in the fluorescence intensity ratio I/I_0 of the
8 sensing system with the addition of various substances. The results showed that no obvious influence
9 was observed in coexistence with high concentration of the tested substances and the established
10 fluorescence strategy exhibited good selectivity in the determination of Con A.



11
12 **Fig. 6** The selectivity of the established sensing system to other coexistence substances, including bovine serum
13 albumin (BSA), human serum albumin (ALH) and lysozyme (Lys), trypsin and pepsin. The concentration of Con A
14 was 196.1 nM.

15 **4. Conclusion**

16 In summary, we have developed a new fluorescence method for Con A determination by using CdTe
17 QDs as fluorescence donor and GO as fluorescence quencher. Glucosamine functionalized QDs and

1 GO could be used to construct a fluorescence sandwich biosensor for Con A based on the special
2 carbohydrate-protein interactions. GO-G and QDs-G were brought into FRET proximity through the
3 specific molecular recognition of Con A, resulting in the fluorescence decreasing. Under the
4 optimized conditions, a linear correlation was established between the fluorescence intensity ratio I/I_0
5 (I_0 and I were the fluorescence intensity of the sensing system in the absence and presence of Con A,
6 respectively) and the concentration of Con A in the range of 9.8-196.1 nM with the detection limit of
7 3.3 nM. The proposed sandwich method is simpler and more sensitive than other methods and can be
8 conveniently extended to the quantitative analysis of various lectins with high sensitivity just by
9 exchanging the carbohydrates functionalized on the QDs and GO.

10 **Acknowledgements**

11 This work was financially supported by the National Natural Science Foundation of China (No.
12 21075050, No. 21275063)

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