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ARTICLE

## Monitoring of Chromosome Dynamics of Single Yeast Cell in a Microfluidic Platform with Aperture Cell Traps

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Chromosome movement plays important roles in DNA replication, repair, genetic recombination, and epigenetic phenomena during mitosis and meiosis. In particular, chromosome movement in the nuclear space is essential for the reorganization of the nucleus. However, conventional methods to analyze the chromosome movements *in-vivo* have been limited by technical constraints of cell trapping, cell cultivation, oxygenation, and *in situ* imaging. Here, we present simple microfluidic platform with aperture-based cell trapping arrays to monitor the chromosome dynamics in single living cells for a desired period. Under the optimized condition, our microfluidic platform shows a 57% of single cell trapping efficiency. This microfluidic approach enables *in-situ* imaging of intracellular dynamics in living cells responding to variable input stimuli under the well-controlled microenvironment. As a validation of this microfluidic platform, we investigate fundamental features of dynamic cellular response of individual cells treated with different stimuli and drug. We prove the basis for dynamic chromosome movement in single yeast to be telomere and nuclear envelope ensembles that attach to and move in concert with nuclear actin cables. Therefore, these results illustrate the capacity to monitor cellular functions and obtain dynamic information at high spatiotemporal resolution through the integration of a simple microfluidic platform.

- 1 **Introduction** 19  
 2 Chromosome movement plays an important role in 20  
 3 chromosomal processes during the cell cycle.<sup>1</sup> Organized 21  
 4 chromosomes segregate and segregate at mitosis, and active 22  
 5 movement of chromosome also occurs during DNA replication, 23  
 6 DNA repair, epigenetic regulation, and meiotic recombination. 24  
 7 In particular, chromosome movement is significant during 25  
 8 meiosis ("prophase I") because homologous maternal and 26  
 9 paternal chromosome have to recognize each other or 27  
 10 chromosome pair efficiently.<sup>1,2</sup> In meiotic cells, heterogeneity 28  
 11 of dynamic chromosome movements is frequently identified. 29  
 12 Thus, there exists a growing interest to track chromosome 30  
 13 dynamics of meiotic cells at the single cell level. 31  
 14 Budding yeast is a widely used eukaryotic model organism 32  
 15 to study chromosome dynamics due to its simple morphology, 33  
 16 well-defined cell cycle, and facile genetics.<sup>1-5</sup> We can identify 34  
 17 gene's function and role by simply disrupting, deleting, 35  
 18 inserting genes.<sup>4-10</sup> Several budding yeast mutants exhibit 36  
 37 aberrant chromosome dynamics.<sup>3,4</sup> Fluorescent proteins (FPs) 38  
 39 are used to label chromosomal and nuclear proteins and 40  
 41 specific chromosomal regions allowing to track dynamic 41  
 42 chromosomal organization during yeast cell cycles.<sup>10-13</sup> 42  
 43 However, it is still difficult to image and track *in vivo* 43  
 44 chromosome dynamics in single cells due to cellular 44  
 45 movement, oxygen limitation, and the uneven imaging focal 45  
 46 plane even with specific control of a microenvironment. 46  
 47 In order to monitor the dynamics of chromosomes, 47  
 48 budding yeast cells are conventionally immobilized into low 48  
 49 melting (37 °C) agarose gel containing the appropriate 49  
 50 medium.<sup>12,14,15</sup> This conventional method of hydrogel based- 50  
 51 immobilization can be elaborate, limits initial time-point access 51  
 52 during imaging time course experiments, and poses a barrier 52  
 53 to rapid and efficient chemical microenvironment control of 53  
 54 individual cells. While in other fields progress in assessing 54  
 55 cellular response and dynamics derives from improvements in 55  
 56 microscopic imaging technique, including microenvironment 56  
 57 controls to permit cell growth during extended monitoring 57  
 58 time and auto-focusing system enhanced imaging quality, the 58  
 59 detailed understanding of chromosome movement has been 59  
 60 slowed by the inadequate cell immobilization methodology. 60  
 61 Currently, high-resolution light microscopy depends on 61  
 62 dedicated imaging instrumentation and is generally restricted 62  
 63 to serial analysis.<sup>16,17</sup> Recent progress of robotics, 63  
 64 microfabrication, and miniaturization technology has 64  
 65 facilitated the investigation of cellular responses to many 65  
 66 stimuli in serial and parallel mode.<sup>18-20</sup> In particular, 66

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1 microfluidic approaches have been developed for the culture  
2 of a wide range of cell types.<sup>22-26</sup> However, prevailing  
3 application of these microfluidic devices has been limited due  
4 to critical technical issues such as complex microfabrication,  
5 elegant operation of multilayer micro-valve devices,  
6 integration with high-resolution imaging and automation  
7 system, and difficulties in microfluidic design with multiple  
8 purpose.

9 Here, we present a microfluidic platform for live cell  
10 imaging with capacity for high-resolution imaging techniques  
11 space and time. The design of the microfluidic platform  
12 embodies a balance among long-term monitoring of living cells  
13 or cultivation, the analysis of dynamic cellular response at  
14 single cell level, imaging resolution, experimental convenience,  
15 and simplicity for easy implementation. The microfluidic  
16 platform can accommodate optical objectives with high  
17 magnification and numerical aperture (N.A.) for high  
18 resolution imaging of cellular response. This microfluidic  
19 platform with a cell trap array of horizontal aperture efficiently  
20 immobilizes yeast cells, enables us to image high spatial  
21 resolution of single cells, and analyze chromosome dynamics  
22 in single meiotic yeast cells. Also, after trapping cells, we easily  
23 induce meiosis by providing sporulation medium at a specific  
24 time, disrupt actin cables by Latrunculin B treatment, and  
25 continuously monitor the dynamics of target proteins at single  
26 cell level. In this study, we obtain key measurements of yeast  
27 cell response in the microfluidic platform, revealing that  
28 pachytene chromosome motion requires both actin and  
29 telomere/nuclear envelop (NE) association. These data,  
30 consistent with conventional methodological results,  
31 demonstrate the benefit of a simple microfluidic platform in  
32 which high resolution time-lapse microscopic imaging can be  
33 performed under an array of experimental conditions and with  
34 longer monitoring time.

## 35 Experimental

### 36 Yeast strains and liquid mediums

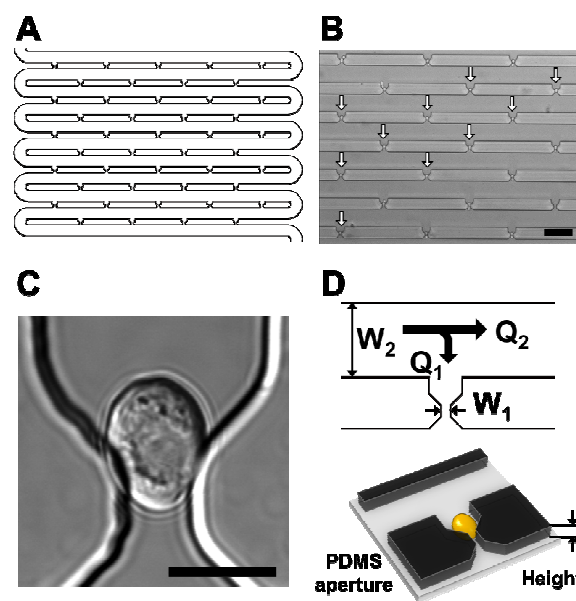
37 The yeast strains used in this study were isogenic heterothallic  
38 SK1 derivatives. Cell image analysis utilized the following  
39 strains: *lys2::tetO x 240::URA3+*, *leu2::LEU2-TetR-GFP*  
40 (KKY619); *ZIP1-GFP (700)* (KKY1319); *NUP49-GFP::URA3*  
41 (KKY623). All yeast strains were selected in YPG medium (1%  
42 w/v yeast extract, 2% w/v bactopectone, 2% w/v glycerol) at  
43 30 °C for 16 hr. Cells were then inoculated into YPD medium  
44 (1% w/v yeast extract, 2% w/v bactopectone, 2% w/v glucose)  
45 at 30 °C. After overnight incubation, 4  $\mu$ l of cell suspension  
46 were re-suspended in 4 ml of fresh YPD medium and sub-  
47 cultured at 30 °C, 6 hour. Before loading cell suspension into  
48 microfluidic device, the cell suspensions were diluted fresh  
49 YPD medium until the cell suspension measured OD<sub>600</sub> to 0.1.  
50 Sporulation media (SPM, 1% w/v potassium acetate, 0.02%  
51 raffinose) and Latrunculin B (LatB) were purchased from  
52 Sigma-Aldrich (MO, USA).

### 54 Microfluidic device fabrication

We fabricated the microfluidic devices by soft lithography with  
microfabricated wafers and poly(dimethylsiloxane) (PDMS,  
Sylgard 184, Dow Corning, MI, USA). The wafer molds were  
fabricated by using a negative photoresist (SU-8 3005,  
MicroChem, MA, USA). Uncured PDMS mixture (10:1 mixing  
ratio of elastomer and cross-linker) was poured onto the wafer  
mold to obtain a 5 mm thick layer and then fully cured at 65 °C  
for 4 hour. It was later peeled off from the wafer mold and  
individual devices were cut to size. Holes for fluidic  
connections were introduced with 0.75 mm diameter biopsy  
tools. PDMS devices were plasma bonded onto a cover glass  
(150  $\mu$ m) for high-resolution imaging.

### Image analysis

Yeast cells and GFP signals were imaged with a Nikon TE  
2000U inverted fluorescence microscope with a 100x oil-  
immersion objective (*N.A.* = 1.45), and FITC filter sets. Image  
analysis was performed with Image-pro (Media Cybernetics,  
MD, USA) and ImageJ software. The 3D shapes of  
chromosomes were imaged with a Nikon A1 confocal  
microscope with a 100x oil-immersion objective (*N.A.* = 1.45).  
Image analysis was performed with the NIS-Elements (Nikon,  
Japan) and the reconstructed image was acquired using the  
Imaris (Bitplane, MA, USA) image software.



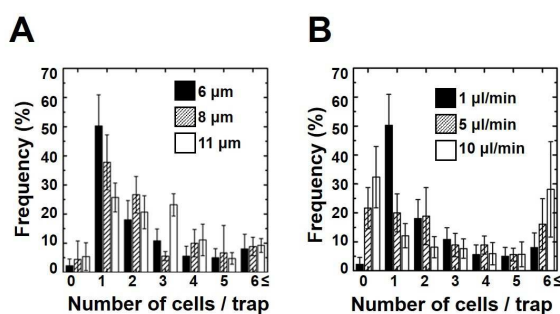
**Fig. 1** Microfluidic platform for single cell trapping and tracking of cell dynamics. (A) Each microfluidic aperture trap array consists of wide main cell-delivery channel arranged in a 10-column format and an array of cross-flow channels that connect each section of the main channel. (B) Bright-field image showing an array of aperture trap filled with single cells that are identified by white arrows (trap width;  $W_1 = 3 \mu\text{m}$ ). Scale bar indicates 50  $\mu\text{m}$ . It shows efficient trapping capacity of single-cell in the array (57 %). White dots indicate single cell trapping. (C) Enlarged image of single yeast cell trapped (Scale bar = 5  $\mu\text{m}$ ). (D) Schematic drawing of the trajectory of flow, indicating important variables influencing trapping efficiency.

## 1 Results and discussion

2 Fig. 1 illustrates basic design of single-layer microfluidic  
3 platform for high-resolution time-lapsed imaging with  
4 inexpensive, disposable, easy fabrication, simple operation  
5 and expandable multiplexing capacity of cell culture and  
6 analysis. The microfluidic device consists of a wide serpentine  
7 like main delivery channel and several cell traps located  
8 vertically (Fig. 1A). The cell trap array has parallel apertures  
9 whose dimension fit the size of yeast, with the width of a  
10 single aperture ( $W_1 = 3 \mu\text{m}$ ) smaller than the average size of  
11 yeast cell ( $5 \mu\text{m}$ ) allowing capture along the main channel  
12 (Fig. 1B and C). Images of the fabricated microfluidic channel  
13 filled with yeast cell are shown in Fig. 1B and C.

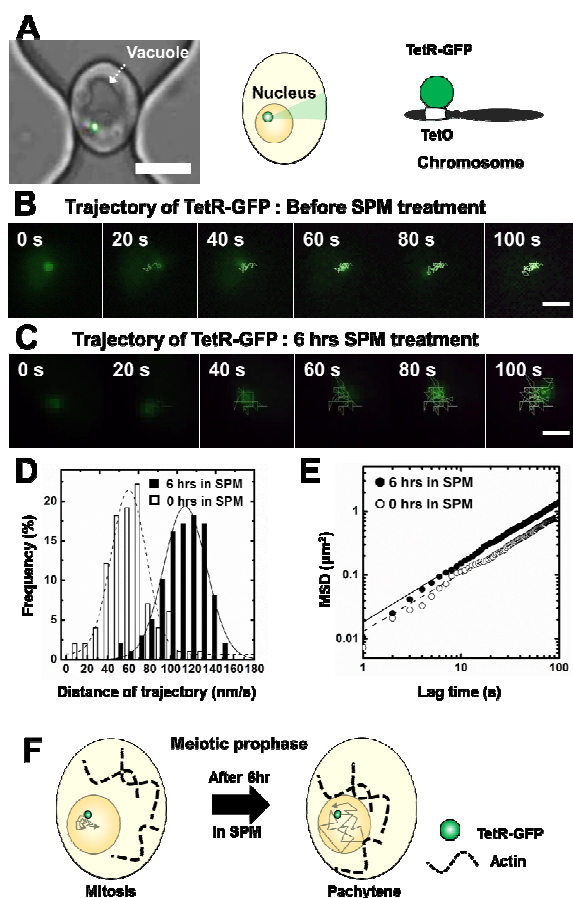
14 The basic principle of the cell trapping is depicted in Fig. 1D  
15 and is similar to that of a sieve.<sup>26-31</sup> Simply, cells smaller than  
16 the trap gap size ( $W_1$ ) pass through the trap, whereas cells  
17 larger than the gap size are trapped geometrically. In addition,  
18 we use the fluidic pressure difference as a driving force for  
19 trapping cells. Specifically, while yeast cells pass through a  
20 main delivery channel, cells near an aperture trap are drifted  
21 into two streams: the main stream ( $Q_2$ ) flowing along the main  
22 delivery channel and a second stream ( $Q_1$ ) that directs a cell  
23 into the trap. Cell trapping is similar to the cellular valving  
24 method based on a differential fluidic resistance of two  
25 streams which is adopted from the serpentine microfluidic  
26 arraying system.<sup>27-31</sup> The process enables the serial arraying of  
27 cells while the cells are trapped, acting as a valve in the open  
28 state. In this manner we successfully form array of more than  
29 95 single living cells in a single microchannel.

30 The dimensions of the microfluidic aperture and optimum  
31 flow rate for efficient cell trapping were optimized. We varied  
32 the height of the aperture ( $H$ ) from 6 to  $11 \mu\text{m}$ , whereas the  
33 width of  $W_1$  and  $W_2$  were fixed at 3 and  $30 \mu\text{m}$ , respectively  
34 (Fig. 2A). The number of trapped cells was highly related to the



**Fig. 2** Experimental result of cell trapping in the microfluidic aperture with various heights and flow rates. Each bar represents the percentage of microfluidic aperture occupied by zero, one, two, three, four, five, and above six cells. (A) The different height of the main channel ( $H$ ) varied from 6 to  $11 \mu\text{m}$  on the frequency of cell trapping while the width of main channel ( $W_2$ ) and trap ( $W_1$ ) are fixed at  $30 \mu\text{m}$  and  $5 \mu\text{m}$ , respectively. The percentage of the microfluidic aperture containing zero, one, two, three, four, five, and above six cells is shown in accordance with different heights of the microfluidic aperture at constant flow rate ( $1 \mu\text{l min}^{-1}$ ). (B) The effect of flow rate on the number of cells trapped at  $6 \mu\text{m}$  height of the microfluidic aperture. The error bars in both (A) and (B) indicate the standard deviations.

dimension of the microfluidic aperture. Higher height allowed more available space for cell occupancy. The effect of dimension of the microfluidic aperture on trapping was investigated with 6, 8, and  $11 \mu\text{m}$  height with a flow rate at  $1 \mu\text{l min}^{-1}$ . In microfluidic device with  $6 \mu\text{m}$  height, the  $Q_1/Q_2$  value is equal to 1.42 and 59% of the stream flows toward the aperture cell trap. At  $11 \mu\text{m}$  height, the  $Q_1/Q_2$  value is equal to 0.58, and only 37% of the stream flows toward the aperture cell trap. Following these ratios, different percentage values for cell trapping were obtained at each height of the microfluidic aperture. All results were generated from average values of five data series measured in five tested devices under the same experimental conditions. Fig. 2A shows that  $6 \mu\text{m}$



**Fig. 3** Chromosome movement with TetR-GFP. (A) Model of chromosome movement; schematic diagram of visualization of chromosome expressing TetR-GFP that carries GFP-labeled *tetO* repeats. Enlarged optical image of single yeast trapped. The scale bar represents  $2 \mu\text{m}$ . (B) Time-lapse fluorescent microscopic images (20 second intervals) of single live cells undergoing chromosome movement with monitoring displacement of TetR-GFP before treatment of sporulation medium (SPM). We monitor movement of TetR-GFP and evaluated the trajectory of TetR-GFP in a single cell. (C) Movement of TetR-GFP after 6 hours incubating in SPM medium. The treatment of SPM makes the cell pachytene stage. Scale bar indicates  $2 \mu\text{m}$ . (D) Histogram of the distances of TetR-GFP movement per second before and after treatment of SPM medium for 6 hours, respectively. (E) Mean square displacement (MSD) of chromosome movement with TetR-GFP before and after 6 hrs of SPM treatment. (F) Schematic diagram of TetR-GFP movement in each cell stage of meiosis.

1 height of the microfluidic aperture enabled efficient single cell trapping. The height increase of the microfluidic aperture increased the number of cells trapped. The flow rate is another important variable parameter for cell trapping (Fig. 2B). The microfluidic device strongly depended on fluidic pressure difference as the main driving force for trapping into the microfluidic aperture. Hence, if the velocity of the bulk flow ( $Q_2$ ) was increased, cells easily drifted the microfluidic aperture due to the decrease of trapping flow ( $Q_1$ ). In single cell trapping, low flow rate ( $1 \mu\text{l min}^{-1}$ ) showed 50% efficiency and the increase of flow rate dramatically decrease single cell trapping efficiency.

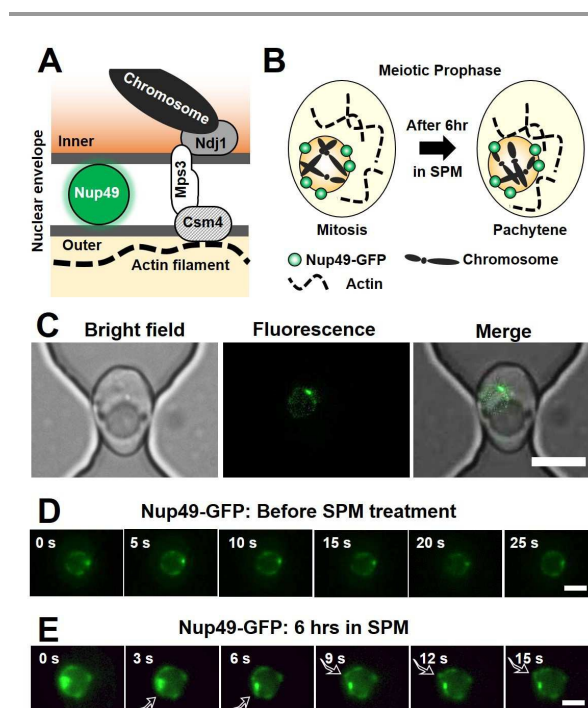
13 The geometric confinement of the aperture cell trap is another important technical issue that can affect the life of budding yeast. Diploid budding yeast initiates meiosis under starvation conditions, but sufficient aeration and nutrients and the appropriate acidity (pH) are necessary for efficient meiosis and chromosome movement. If traps are too tight, budding yeast will not progress efficiently through the meiotic cell cycle due to oxygen limitations and pH changes. Under optimized conditions, we analyzed the growth rate of yeast cells in our aperture cell trap to investigate the effects of geometric confinement on cell growth. The results clearly confirm that our aperture cell trap did not influence yeast growth (Fig. S1A, ESI $\dagger$ ). The measured doubling time of the KKY 619 strain in the aperture cell traps was approximately 2 hours 40 min. In comparison, the growth curve analysis performed with identical strains and measured using a UV spectrometer indicated that the doubling time was approximately 2 hours 44 min (Fig. S1B, ESI $\dagger$ ). These experimental results imply identical cell viabilities between the aperture cell trap and conventional flask culture. Thus, it is reasonable to conclude that the aperture cell trap with geometric confinement provides favorable cell culture conditions.

35 We perform an on-chip viability study of budding yeast to determine whether trapping and given-perfusion flow induce cell damage during budding and division (Fig. S1 and 2, ESI $\dagger$ ). The platform of the microfluidic device allowed imaging of budding initiation (arrow in Fig. S2B, 3 hour) and mitotic cell division while continuously providing cell culture media (Yeast extract Peptone Dextrose (YPD)) during 6 hours (Fig. S2A and B, ESI $\dagger$ ). Budding yeast divide asymmetrically in nutrient rich medium, while nutrient limitation induces meiosis and sporulation. Thus, meiosis is induced by switching the cell culture media to sporulation media (SPM) lacking glucose and nitrogen source. As expected, budding yeast cells in microfluidic aperture traps are first exposed to sporulation medium to initiate meiosis and observe the typical morphology of meiosis that forms four daughter cells (Fig. S2C and D, ESI $\dagger$ ). Together our results indicate that the microfluidic device is suitable for the investigating yeast cell biology over a range of cell stages, and that we can monitor individual cells undergoing the developmental transition from mitosis phase to meiosis at the single cell level.

55 To examine a capability of the microfluidic device for the analysis of cellular events at a single cell level, we investigated chromosome dynamics of yeast in meiosis by precise

quantification of chromosome movement using the microfluidic device to enable cell trapping and *in-situ* cell imaging with relatively high resolution (oil immersion objective lens,  $N.A.=1.45$ ). When GFP-repressor fusions bind to operator arrays, they produce a bright dot that can be followed in live cells by time-lapse monitoring of fluorescent signal. In this study, we used diploid yeast strain carrying GFP-labeled Tet-operator (*tetO*) repeats to visualize chromosomes as single bright dots in the cell (Fig. 3A). Cells expressed protein tagged with green fluorescent protein (GFP), TetR-GFP, serving as a visual marker for chromosome movement because a small fluorescent dot is present on chromosomes at the positions of the *tetO* arrays.

Sequential images were able to quantify chromosome movement by measuring the total distance of the bright fluorescence dot's trajectory during an imaging time series (Fig. 3B and 3C). We compare dynamic chromosome behavior of mitotic (before treatment of SPM) and meiotic chromosomes (after 6 hour treatment of SPM medium) (Fig. 3D). In yeast, the zygotene and pachytene stages occur



**Fig. 4** Movement of nuclear envelope at pachytene state. (A) Schematic diagram of telomere-led chromosome and nuclear envelope (NE): In this study, nuclear pore component labeled with GFP (Nup49-GFP) is utilized for visualization. Mono-Polar Spindle 3 (Mps3); Non-Disjunction 1 (Ndj1); Chromosome Segregation in Meiosis 4 (Csm4). (B) Schematic representation of the dynamics of nuclear envelope: the attachment of actin would be associated in meiosis phase. (C) Representative images of Nup49-GFP in single cell that trapped in microfluidic device (Bright field, Fluorescence, and Merged image). Scale bar indicates 5  $\mu\text{m}$ . (D) 2D time-lapse images of pachytene nuclei with Nup49-GFP labeled NE, captured at 5 second intervals before SPM medium treatment. Scale bar indicates 2  $\mu\text{m}$ . (E) 2D time-lapse images of pachytene nuclei with Nup49-GFP labeled NE, captured at 3 second intervals after incubated in the SPM medium for 6 hour. Arrows indicate angular deformation. The movement of Nup49-GFP becomes more active at pachytene, with long protrusions limited to the period. Scale bar indicates 2  $\mu\text{m}$ . (See the Movie S3, ESI $\dagger$ )

1 sequentially. Chromosome movement exhibits the same 58  
2 progression. Chromosome dynamics were independently 59  
3 examined by monitoring of TetR-GFP movement (Fig. 3B and 60  
4 3C). Analysis of TetR-GFP trajectories reveals that mobility 61  
5 changed from mitotic chromosome ( $t = 0$ ; before SPM 62  
6 treatment) through meiotic chromosome ( $t = 6$  hour) and 63  
7 even more dramatic at pachytene ( $t = 6$  hour) (Fig. 3B to 64  
8 S3A in ESI†). The movement of chromosome initiates propha 65  
9 although beginning of zygotene is tightly linked to a key step 66  
10 meiotic recombination. In meiosis, onset of motion may 67  
11 part of the basic cellular program that becomes coupled 68  
12 progression of recombinational progression by coordinating  
13 regulatory mechanisms.<sup>4</sup> Statistically, the average movement  
14 of GFP dot obtained from 45 individual cells were tracked and  
15 analyzed (Fig. 3D and S3A, ESI†). Trajectory analysis of  
16 chromosomes in live cells showed that chromosome  
17 movement is relatively slow before treatment of SPM while  
18 average chromosome movement is induced in the SPM  
19 medium. As a result, following incubation in the SPM medium  
20 for 6 hours, pachytene chromosomes showed more movement  
21 than either the mitotic chromosome or the zygotene  
22 chromosome (Fig. 3D and S3A, Movie S1† and 2†). We  
23 quantitatively analyzed the movement of the tracking label in  
24 single cells by mean square displacement (MSD) and its trend  
25 in accordance with the observed lag time from the first  
26 analyzed time-point in the trajectory analysis (Fig. 3E). The  
27 correlation between lag time and the MSD of a particle in 2  
28 dimensions can be calculated using equation (1).

$$30 \quad \text{MSD} = 4D\tau^\alpha \quad (1)$$

31 where,  $D$  indicates the diffusivity and  $\tau$  stands for the observed  
32 lag time. Generally, the exponent  $\alpha$  distinguishes the type of  
33 diffusion that particles encountered:  $\alpha = 1$ , normal Brownian  
34 diffusion in purely viscous (liquid-like) material, e.g. water;  $\alpha <$   
35  $1$ , sub-diffusion in elastic material; and  $\alpha > 1$ , super-diffusion  
36 or active movement. The results clearly indicate that the labels  
37 moved sub-diffusively, which may be due to the crowding of  
38 the nucleus (exponents for  $\alpha$  were 0.9598 and 0.989 before  
39 treatment and after 6 hours of treatment with SPM,  
40 respectively) and the elastic property of the cytosolic fluid,  
41 which contains several biomaterials (i.e., DNA, proteins,  
42 carbohydrates, lipids, etc.). More interestingly, the diffusivity  
43 of the label increased when we treated with SPM medium over  
44 6 hours (the diffusivity equaled  $2.67 \times 10^{-3}$  and  $3.77 \times 10^{-3} \mu\text{m}^2$   
45  $\text{s}^{-1}$ , before and after 6 hours of treatment with SPM,  
46 respectively). This result implies that actin filaments contribute  
47 to the movement associated with the nuclear envelope in the  
48 pachytene stage, as illustrated in Fig. 3F and Fig. 4A and B. We  
49 believe that the results presented here shed very original  
50 perspectives on the potential interplay between the  
51 chromosome/chromatin physical status and the biological  
52 events processed at the same time under controlled  
53 conditions. Taken together, accurate and precise  
54 quantification of chromosomal dynamics indicates that the  
55 movement of meiotic chromosomes is particularly significant  
56 at the pachytene state (Fig. 3F). All of the results provide clear  
57

evidence in budding yeast that nutrients strongly affect rapid  
chromosome movements. Taken together, our microfluidic  
approach enables analysis of chromosome dynamics by simple  
monitoring of GFP-tagged chromosomes in which arrays of  
*Tet*-operator sites are integrated into defined sites in the  
genome followed by TetR-GFP expressed. On the basis of these  
observations, we can confirm that during meiotic prophase the  
presence of rapidly moving chromosomes over an extended  
period of time.

Next, we focus on chromosome dynamics associated with  
the nuclear-envelop (NE) and actin to study the basis of

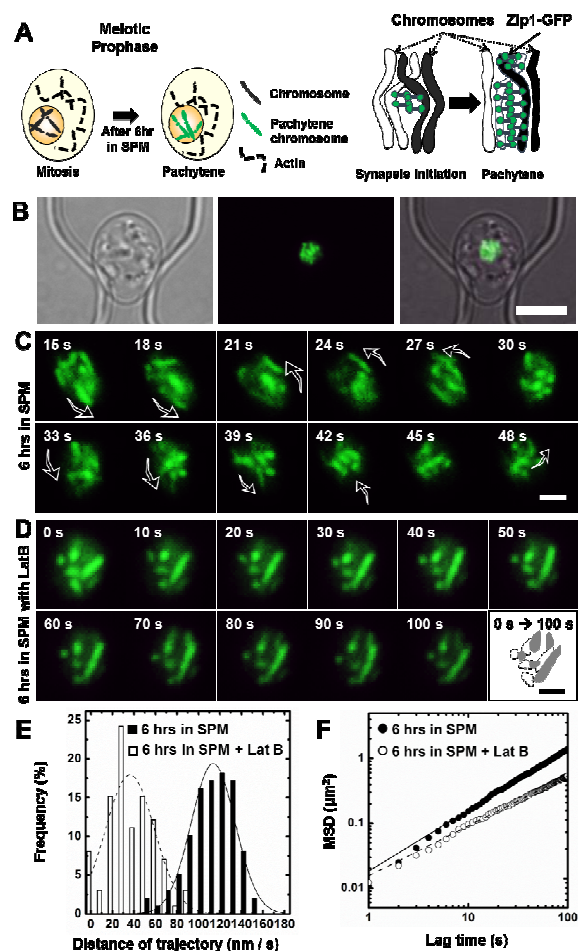


Fig. 5 Actin associated chromosome movement at pachytene state. (A) Schematic diagram of the Zip1-GFP strain. At prophase, ZIP1 acts as a molecular zipper to bring homologous chromosomes into close apposition. ZIP1 may encode the transverse filaments of the synaptonemal complex. (B) Experimental images of a single cell trapped in the microfluidic device with expression of Zip1-GFP (Bright field, Fluorescence, and Merged image). Scale bar = 5 μm. 3D reconstruction of pachytene chromosomes obtained from confocal images is available in Movie S4†. (C) Time-lapsed images of pachytene chromosome with expressing Zip1-GFP (6hr after meiosis induction; 3s intervals) before the treatment of LatB. Arrows indicate discrete and directed motion. See also Movie S5†. (D) Time-lapsed images of pachytene chromosome with expression of Zip1-GFP after the treatment with 20 μM LatB. The treatment of LatB significantly reduces movement of pachytene chromosome. Scale bar = 2 μm. (E) Frequency of distance of trajectory of TetR-GFP at the pachytene stage without or with treatment of 20 μM LatB. (Movie S6, ESI†). (F) Mean square displacement (MSD) of chromosome movement with or without 20 μM LatB treatment.

1 dynamic mid-prophase I (pachytene) telomere-led  
2 chromosome motion in budding yeast. Previous studies have  
3 implied that individual telomere/nuclear envelope (NE)  
4 complexes associate with nucleus-hugging actin cables that are  
5 continuous with the global cytoskeletal actin network and  
6 move for a few seconds in conjunction with the cables (Fig. 4B  
7 and 4B).<sup>1,4</sup> Conformational deformation of NE results in  
8 telomere-led chromosome movement because pachytene  
9 chromosome ends are robustly associated with the NE.<sup>1,4</sup> With  
10 our microfluidic device, we visualize the NE by time-lapse  
11 imaging of fluorescently expressed nuclear pore component  
12 Nup49-GFP (Fig. 4C). After trapping single cells, confocal  
13 fluorescence microscopy image clearly showed the NE. Time  
14 time-lapse analysis of Nup49-GFP dynamics confirmed that  
15 telomere-led chromosome movement is accompanied by  
16 concomitant local NE deformation. In vegetative growth and  
17 early meiosis, the NE exhibited a static spherical or oval shape.  
18 However, at the pachytene chromosome state (at  $t = 6$  hours  
19 NE showed dynamic conformational changes (Fig. 4D and  
20 Movie S3†). Common local shape changes were angular  
21 deformations of NE, in which the deformation evolved into  
22 thin and short protrusions or recession (up to  $0.3 \mu\text{m}$ ).  
23 Dynamic changes of NE shape could also be correlated with  
24 directional telomere-led chromosome movement. As shown in  
25 the sequence of Fig. 4E, at 0 to 6 second, an angular  
26 deformation, likely with a short protrusion, occurred at the  
27 leading end of a single chromosome. At a different position  
28 the nucleus (9 to 15 second, Fig. 4E), outward-directed  
29 movement accompanied elongation of the surrounding  
30 segment. This change was followed by movement of the body  
31 of the nucleus in the opposite direction. Thus, we conclude  
32 that directional force is exerted specifically on telomere/  
33 ensembles, moving the targeted chromosome end and  
34 concomitantly deforming the NE at the affected point.  
35 The process of chromosome pairing and chromosome  
36 motility after pairing are of interest because reciprocal  
37 recombinations between homologous chromosomes take  
38 place during the prophase of first meiotic division and these  
39 are essential for proper segregation.<sup>32-34</sup> The consecutive  
40 changes that occur to chromosomes during prophase have  
41 only begun to be characterized by live imaging techniques at  
42 single cell level. Thus, we wanted to investigate the feasibility  
43 of the microfluidic device to monitor and analyze sequential  
44 changes of chromosome behavior. For the study of the  
45 dynamics of synaptonemal complexes (SCs) during prophase  
46 meiosis, a Zip1-GFP (molecular zipper) was applied to visualize  
47 SCs in live sporulating yeast cells because ZIP1 is an integral  
48 and essential protein component of the central element of  
49 synaptonemal complexes (SCs)<sup>6</sup> and is believed to be  
50 ortholog of the mammalian protein SYCP1.<sup>35</sup> Overall schematic  
51 diagram of chromosome pairing with Zip1-GFP imaging is  
52 shown in Fig. 5A.  
53 After trapping single cells in the microfluidic device,  
54 pachytene chromosomes were clearly observed by confocal  
55 fluorescence microscopy (Fig. 5B). At prophase, ZIP1 acts as a  
56 molecular zipper to bring homologous chromosomes into close  
57 apposition. ZIP1 may encode the transverse filaments of the

(Fig. 5A). Fig. 5B shows that the microfluidic device renders proper condition for sequential imaging of the trapped cells. Also, as expected, we could monitor chromosome motion by imaging Zip1-GFP in the pachytene chromosomes. Dynamic chromosomal movement was monitored with 3 seconds intervals in living cells after incubation for 6 hours in the SPM medium.

To gain further insight into the role of nuclear deformation by actin, we treat the yeast cells with Latrunculin B (LatB). LatB is a disruptor of microfilament organization because it can bind to actin monomers and inhibits actin polymerization *in vitro*, disrupting microfilament organization as well as actin filament-mediated processes during cellular processes.<sup>36</sup> In the absence of LatB, we observe a notable rotation of individual chromosome (SC) (Fig. 5C). However, there was a significant decrease of *in vivo* chromosome motion from cells treated with LatB (Fig. 5D). The treatment of LatB induced chromosome movement to small “jiggling” motions (Fig. 5D). In order to verify the effect of LatB, we quantified chromosome movement in 100 cells by imaging TetR-GFP-labeled *tetO* repeats as we previously show in Fig. 3. Indeed, we found a significant decrease of chromosome movement upon the addition of LatB (Fig. 5E, F and S3B, ES†). After 6 hours of treatment with LatB, the exponent  $\alpha$  was 0.7946, and the diffusivity was  $3.54 \times 10^{-3} \mu\text{m}^2 \text{s}^{-1}$ . This result confirms that actin, which would be disrupted upon LatB addition, contributes to chromosome movement. Taken together, these results are consistent with telomere-led chromosome movement and provide new information about the mechanics and movement of yeast meiotic chromosomes. The behavior of whole chromosomes at the pachytene stage of meiotic prophase I as characterized *in vivo* indicates that pachytene chromosomes link to the NE and dynamic movement of actin cables displaces the attached complex. Further, this movement is critical for meiotic recombination biochemistry and chromosome metabolism, and that it is critical for processes by which homologous sequences find each other, joint molecules are made, and homologs become tightly paired in SC.

## Conclusions

In conclusion, we monitored chromosome dynamic movements in single living cells for a defined period *via* a simple microfluidic platform with aperture-based cell trapping arrays. Main advantage is high accuracy of measurement for a biological event at the single cell level, because each single cell is physically trapped and cannot migrate or move out of the plane of focus. Our microfluidic platform allows easy and efficient single cell loading while maintaining captured cells in a low shear stress environment for long-term studies. We can investigate the dynamic responses of individual cells treated with different stimuli including physical environment and chemicals.

As a proof-of-principle, we demonstrate the tracking and quantification of chromosome dynamics in yeast cell. Our approach can provide new biological information gained from

- 1 single-cell level and *in situ* dynamic response and new  
2 opportunities to quantify individual cellular responses  
3 opposed to the averaged information provided  
4 conventional methods. We envision this simple microfluidic  
5 approach in tracking chromosome movements will be useful  
6 investigate other cell biological processes requiring single cell  
7 feature tracking and quantification, since our approach is not  
8 only an ideal imaging platform but also has simplicity  
9 design, inexpensive materials, affordable experimental setup  
10 and adaptability for high-throughput assays.
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- 21 **References**
- 22 1 R. Koszul and N. Kleckner, *Trends Cell Biol.*, 2009, **19**, 716.  
23 2 R. I. Kumaran, R. Thakar and D. L. Spector, *Cell*, 2008, **133**,  
24 929.  
25 3 J. Mine-Hattab and R. Rothstein, *Nat. Cell Biol.*, 2012, **14**,  
26 510.  
27 4 R. Koszul, K. P. Kim, M. Prentiss, N. Kleckner and S. Kameo,  
28 *Cell*, 2008, **133**, 1188.  
29 5 K. P. Kim, B. M. Weiner, L. Zhang, A. Jordan, J. Dekker, and  
30 Kleckner, *Cell*, 2010, **143**, 924.  
31 6 M. Sym, J. Engebrecht and G. S. Roeder, *Cell*, 1993, **72**, 365.  
32 7 S. Hong and K. P. Kim, *Mol. Cells*, 2013, **36**, 446.  
33 8 H. J. Cha and Y. J. Yoo, *Korean J. Chem. Eng.*, 1996, **13**, 172.  
34 9 H. C. Lee and C. Y. Choi, *Korean J. Chem. Eng.*, 1987, **4**, 47.  
35 10 P. Heun, T. Laroche, K. Shimada, P. Furrer and S. M. Gasser,  
36 *Science*, 2001, **294**, 2181.  
37 11 P. Li, H. Jin, M. L. Hoang and H. G. Yu, *Chromosome Res.*,  
38 2011, **19**, 1013.  
39 12 H. Hajjoul, J. Mathon, H. Ranchon, I. Goiffon, J. Mozziconacci,  
40 B. Albert, P. Carrivain, J. M. Victor, O. Gadai, K. Bystrycky and  
41 A. Bancaud, *Genome Res.*, 2013, **23**, 1829.  
42 13 A. Belmont, *Trends Cell Biol.*, 2001, **11**, 250.  
43 14 K. K. Steffen, B. K. Kennedy and M. Kaeberlein, *J. Vis. Exp.*,  
44 2009, DOI: 10.3791/1209.  
45 15 R. K. Mortimer and J. R. Johnston, *Nature*, 1959, **183**, 1751.  
46 16 N. Rosenfeld, J. W. Young, U. Alon, P. S. Swain and M. B.  
47 Elowitz, *Science*, 2005, **307**, 1962.  
48 17 J. M. Pedraza and A. van Oudenaarden, *Science*, 2005, **307**,  
49 1965.  
50 18 A. Roguev, M. Wires, J. S. Weissman and N. J. Krogan, *Nat.*  
51 *Methods*, 2007, **4**, 861.  
52 19 A. H. Y. Tong, G. Lesage, G. D. Bader, H. M. Ding, H. Xu, X. F.  
53 Xin, J. Young, G. F. Berriz, R. L. Brost, M. Chang, Y. Q. Chen, X.  
54 Cheng, G. Chua, H. Friesen, D. S. Goldberg, J. Haynes, C.  
55 Humphries, G. He, S. Hussein, L. Z. Ke, N. Krogan, Z. J. Li, J. N.  
56 Levinson, H. Lu, P. Menard, C. Munyana, A. B. Parsons, O.  
57 Ryan, R. Tonikian, T. Roberts, A. M. Sdicu, J. Shapiro, B.  
58 Sheikh, B. Suter, S. L. Wong, L. V. Zhang, H. W. Zhu, C. G.  
59 Burd, S. Munro, C. Sander, J. Rine, J. Greenblatt, M. Peter, A.  
Bretscher, G. Bell, F. P. Roth, G. W. Brown, B. Andrews, H.  
Bussey and C. Boone, *Science*, 2004, **303**, 808.  
20 S. Cookson, N. Ostroff, W. L. Pang, D. Volfson and J. Hasty,  
*Mol. Syst. Biol.*, 2005, **1**, 2005 0024.  
21 S. S. Lee, I. Avalos Vizcarra, D. H. E. W. Huberts, L. P. Lee and  
M. Heinemann, *Proc. Natl. Acad. Sci. U. S. A.*, 2012, **109**,  
4916.  
22 K. Leung, H. Zahn, T. Leaver, K. M. Konwar, N. W. Hanson, A.  
P. Page, C. C. Lo, P. S. Chain, S. J. Hallam and C. L. Hansen,  
*Proc. Natl. Acad. Sci. U. S. A.*, 2012, **109**, 7665.  
23 Wang, M. C. Kim, M. Marquez and T. Thorsen, *Lab Chip*,  
2007, **7**, 740.  
24 M. C. Kim, B. C. Isenberg, J. Sutin, A. Meller, J. Y. Wong and C.  
M. Klapperich, *Lab Chip*, 2011, **11**, 1089.  
25 R. J. Taylor, D. Falconnet, A. Niemisto, S. A. Ramsey, S. Prinz,  
I. Shmulevich, T. Galitski and C. L. Hansen, *Proc. Natl. Acad.*  
*Sci. U. S. A.*, 2009, **106**, 3758.  
26 H. H. Jeong, S. H. Jin, B. J. Lee, T. Kim and C. S. Lee, *Lab Chip*,  
2015, **15**, 889.  
27 W. H. Tan and S. Takeuchi, *Proc. Natl. Acad. Sci. U. S. A.*,  
2007, **104**, 1146.  
28 J. Kim, J. Erath, A. Rodriguez and C. Yang, *Lab Chip*, 2014, **14**,  
2480.  
29 S. H. Jin, H. H. Jeong, B. Lee, S. S. Lee and C. S. Lee, *Lab Chip*,  
2015, **15**, 3677.  
30 A. Dewan, J. Kim, R. H. McLean, S. A. Vanapalli and M. N.  
Karim, *Biotechnol. Bioeng.*, 2012, **109**, 2987.  
31 T. Teshima, H. Ishihara, K. Iwai, A. Adachi and S. Takeuchi,  
*Lab Chip*, 2010, **10**, 2443.  
32 S. Tesse, A. Storlazzi, N. Kleckner, S. Gargano and D. Zickler,  
*Proc. Natl. Acad. Sci. U. S. A.*, 2003, **100**, 12865.  
33 S. Hong, Y. Sung, M. Yu, M. Lee, N. Kleckner, and K. P. Kim.  
*Mol. Cell*, 2013, **51**, 440.  
34 S. Tournier, Y. Gachet, V. Buck, J. S. Hyams and J. B. Millar,  
*Mol. Biol. Cell*, 2004, **15**, 3345.  
35 R. L. Meuwissen, H. H. Offenberg, A. J. Dietrich, A. Riesewijk,  
M. van Iersel and C. Heyting, *EMBO J.*, 1992, **11**, 5091.  
36 D. Y. Lui, C. K. Cahoon and S. M. Burgess, *PLoS Genet.*, 2013,  
**9**, e1003197.