This is an Accepted Manuscript, which has been through the Royal Society of Chemistry peer review process and has been accepted for publication.

Accepted Manuscripts are published online shortly after acceptance, before technical editing, formatting and proof reading. Using this free service, authors can make their results available to the community, in citable form, before we publish the edited article. We will replace this Accepted Manuscript with the edited and formatted Advance Article as soon as it is available.

You can find more information about Accepted Manuscripts in the Information for Authors.

Please note that technical editing may introduce minor changes to the text and/or graphics, which may alter content. The journal’s standard Terms & Conditions and the Ethical guidelines still apply. In no event shall the Royal Society of Chemistry be held responsible for any errors or omissions in this Accepted Manuscript or any consequences arising from the use of any information it contains.
Microfluidic studies of polymer adsorption in flow

Zhaoyi Wang, a,b Dan Voicu, a Ling Tang, c,d Wei Li, d,e and Eugenia Kumacheva, *a

Received (in XXX, XXX) Xth XXXXXXXXX 20XX, Accepted Xth XXXXXXXXX 20XX
DOI: 10.1039/b000000x

Abstract

Adsorption of polymers from solutions moving past solid or liquid surfaces controls a broad range of phenomena in science, technology, and medicine. In the present work, a microfluidic methodology was developed to study polymer adsorption in flow under well-defined conditions by integrating an attenuated total reflection-Fourier transform infrared (ATR-FTIR) spectroscopy with a microfluidic device. Polymer adsorption in flow was studied for exemplary polyelectrolytes such as polystyrene sulfonate and polyacrylic acid under varying flow rates, polymer concentrations, pH, and ionic strengths of the solution. Furthermore, the microfluidic platform was utilized to study layer-by-layer adsorption of alternating anionic and cationic polyelectrolytes such as polyacrylic acid and polyallylamine hydrochloride. The proposed methodology paves the way for studies of in-flow adsorption of biologically relevant molecules, which would mimic processes occurring in the cardiovascular microcirculation system.

Introduction

Adsorption of polymers on liquid and solid surfaces has a vast range of applications in science and technology, including the stabilization of colloid particles, adhesion, lubrication, control of wetting phenomena, compatibilization of otherwise incompatible phases, and site-specific drug delivery. 1-3 Polymer molecules and their supramolecular assemblies undergo adsorption from their quiescent solutions, when an attraction energy between the polymer and the surface exceeds the entropy loss upon adsorption. 4 In the absence of flow, polymer adsorption includes three successive steps, namely, diffusion of macromolecules to a surface, attachment to the surface, and chain relaxation toward its equilibrium state. 4 Less attention has been paid to adsorption of polymers from solutions moving past solid or liquid surfaces, although this phenomenon is important for a broad range of disciplines, including tribology, biology, and medicine. 5 For example, the formation of biofilms is initiated by adsorption of macromolecules from the aqueous milieu to the surface of rocks, sewage pipes, teeth, or boat hulls. 6,7 The formation and growth of thrombi occurs under the flow of blood, which imparts shear forces on adsorbing fibrinogen and transports coagulation factors and anticoagulation molecules to and from the thrombus and blood vessel walls. 5,8 Polymer adsorption in flow exhibits at least, three additional features, in comparison with adsorption under quiescent conditions, that is, the change in molecular conformation and orientation due to hydrodynamic forces, the competition between polymer adsorption and its transverse motion past the surface, and the shear force affecting the orientation and conformation of polymer molecules on the surface.

Polymer adsorption is generally studied by ellipsometry, 9,11 atomic force microscopy (AFM), 12 total internal reflection fluorescence, 13,15 radiolabeling, 16 quartz crystal microbalance, 17 and attenuated total reflection-Fourier transform infrared (ATR-FTIR) spectroscopy 18,19 techniques. Among these methods, ATR-FTIR spectroscopy is a label-free, non-destructive tool with the capability to detect multiple components simultaneously in a fast, cost- and labor-efficient manner, 20,21 which can be used to study polymer adsorption under static and dynamic conditions. Moreover, ATR-FTIR spectroscopy can provide detailed molecular-level information on the conformation or orientation of macromolecules on the surface. 22 Integration of ATR-FTIR with microfluidic (MF) devices offers the ability to study adsorption of polymers in flow under highly controllable shear rates, in addition to the benefits of low reagent consumption, the capability of high-throughput change in the composition of polymer solutions, and excellent control over heat and mass transfer. 23-26 The MF-integrated ATR-FTIR characterization tool has been utilized to study the composition of multicomponent polymer solutions, 27 and kinetics of polymerization reactions. 28 In addition, the FTIR imaging platform was utilized to obtain chemical information on reactants and products at different points of time and at different locations of the MF device. 29,31 Yet, since ATR-FTIR spectroscopy acquires information on the analyte present both on the surface of the ATR crystal and up to several micrometers from the crystal surface, the characterization of polymer adsorbed on the surface, rather than in the polymer solution in the vicinity of the surface is yet to be studied.

In the present work, we used ATR-FTIR spectroscopy integrated with a MF device to explore adsorption of single-component polyelectrolyte layers under different flow rate conditions from solutions with varying polymer concentration, pH, and ionic strength. The ATR-FTIR technique integrated with microfluidics characterizes changes in the IR spectra of analytes both in the solution flowing past the ATR crystal (typically, several micrometers away from the crystal surface) and in the analyte adsorbed on the crystal surface. In our earlier work, we characterized polymers in the solution flowing past the ATR...
crystal\textsuperscript{22} and studied polymerization kinetics in solution\textsuperscript{28}. In the present work, we focused only on the polymer adsorbed on the ATR-crystal surface.

To show the versatility of the method, we applied it to study in-flow adsorption of multi-component, layer-by-layer (LbL) polymer layers of alternating anionic and cationic polyelectrolyte layers.\textsuperscript{15,16}

For the L-b-L adsorption, we selected polyacrylic acid and polyallylamine hydrochloride as complementary polymers due to (i) their propensity to form stable complexes in aqueous solutions\textsuperscript{37,38} and (ii) the presence carboxylic acid and amine functional groups,\textsuperscript{70} which are common for biological\textsuperscript{65} and synthetic\textsuperscript{66} and can be readily identified using IR spectroscopy.\textsuperscript{41} The developed methodology combines the advantages of ATR-FTIR methodology which are common for biological\textsuperscript{37,38} and synthetic\textsuperscript{65} and can be readily identified using IR spectroscopy.\textsuperscript{41} The developed methodology combines the advantages of ATR-FTIR characterization and MFs. It paves the way for studies of in-flow adsorption of biologically relevant molecules, which would mimic processes occurring in the cardiovascular microcirculation system.

**Materials and methods**

Polystyrene sulfonate, polyacrylic acid, polyallylamine hydrochloride with the average molecular weights of 70 000, 450 000, and 58 000 g mol\textsuperscript{−1}, respectively, were purchased from Sigma-Aldrich Canada and used as received. Tris(hydroxymethyl)-aminomethane (99+%) (Tris) and piperidine (99.5+%) were purchased from Sigma-Aldrich Canada. Phosphoric acid was purchased from Caledon Laboratories Ltd. Sodium chloride was purchased from ACP Chemicals (Quebec, CA). Photore sist (SU-38 3050) and SU-8 developer were supplied by Microchem Corporation (USA). Polycarbonate (PC) (Lexus 9034-112) was supplied by Sabic (USA) and dehydrated by pre-heating at 80 °C for 40-80 min before embossing. Polycarbonate film with a thickness of 175 µm was purchased from McMaster Carr (USA). Deionized water was purified using a Milli-Q Plus purification system (Millipore Corp., USA). Viscosity of the polymer solution was measured with a programmable rheometer (Brookfield, Model DV-III) at room temperature.

The MF device was fabricated using a thermoembossing method using a Carver Laboratory Press (Model M Carver Inc., Wabash, IN). An imprint template for hot embossing was fabricated as described elsewhere.\textsuperscript{40} An ATR-FTIR spectrometer (Vertex 70, Bruker Corp.) was interfaced with the MF device using a single reflection diamond ATR crystal (MIRacle, Pike Technologies). The fluidic connections were interfaced with the MF device using an interface component (FlowJEM Inc.). A detailed description of the fabrication of the MF device and an integration of the ATR crystal are provided in Supporting Information.

Multilayer films of polyacrylic acid and polyallylamine hydrochloride (LbL films) were prepared using a static dipping method.\textsuperscript{32} The dip-wash-dip process was repeated for 5 times. The same LbL films were prepared under flow conditions on the surface of silicon wafer that was covered by a microchannel.\textsuperscript{33} The details of film preparation are given in Supporting Information. The thickness of the dried LbL film was measured using Dektak XT surface profilometer.

**Experimental design**

A MF device comprising a microchannel with a width and height of 200 and 50 µm, respectively, was fabricated in polycarbonate (see Supporting Information). The device was integrated with a diamond ATR crystal with a diameter of 1.8 mm (Fig. 1a, b and c), as described elsewhere.\textsuperscript{32} A microscopy image of the channel segment integrated with the ATR crystal is shown in Fig 1b. The polymer solution was supplied to the MF device using a syringe pump (PHD 2000, Harvard Apparatus) at a constant volumetric flow rate, Q. After a particular time, typically, 25 min, the supply of the polymer solution was terminated and deionized water was introduced into the channel to remove the free and loosely-adsorbed polymer from the system. Fig. 1d-f illustrates different stages of the experimental study of polymer adsorption in flow: (i) exposure of the ATR crystal surface (a substrate) to an aqueous polymer solution introduced in the MF device; (ii) polymer adsorption onto the crystal surface, reaching a steady state after a particular time interval; and (iii) the removal of the loosely-surface-attached and free polymer by insertion of deionized water at a volumetric flow rate, Q.

The IR spectra were collected in the course of polymer adsorption and after the washing step. The spectra were generated from 32 scans at 10 kHz with 4 cm\textsuperscript{−1} spectral resolution. The computer-controlled data acquisition and analysis of the spectra were performed using Opus 6.5 software.

To form a multilayer LbL polymer film on the surface of the ATR crystal, alternating streams of PAA and PAH solutions were introduced in the MF device, with the washing step between the infusion of each polymer solution. The IR spectra were acquired after each washing step.
Results and discussion

To explore the feasibility of MF studies of polymer adsorption in flow, we used two exemplary anionic polyelectrolytes, namely, polystyrene sulfonate (PSS) and polyacrylic acid (PAA). Fig. 2a shows the IR spectra of PSS after 25 min-long introduction of the polymer solution in the MF device (solid line) and 25 min-long injection of deionized water (dashed line). Two characteristic peaks at 1178 cm$^{-1}$ and 1125 cm$^{-1}$ correspond to the asymmetric stretching vibrations of the S=O; the bending at 1037 cm$^{-1}$ was assigned to the S=O symmetrical stretching vibrations, and the peak at 1008 cm$^{-1}$ was attributed to aromatic in-plane vibrations. Adsorption of PSS on the ATR crystal surface was characterized by monitoring the intensity of the peak at 1125 cm$^{-1}$ (indicated with an arrow in Fig. 2a). The IR spectra of PAA before and after washing steps are shown in Fig. 2b. A sharp narrow peak at 1726 cm$^{-1}$, indicated by an arrow, corresponds to C=O stretching, and a weaker, broader peak at 1285 cm$^{-1}$ corresponds to the C-O stretching. The time-dependent intensity of the peak at 1726 cm$^{-1}$ was monitored to study PAA adsorption.

Fig. 2. Characterization of adsorption of PSS and PAA. IR absorption spectra of PSS (a) and PAA (b), both acquired after 25 min-long infusion of the polymer solution (solid lines) and after 25 min-long washing step (dotted lines). Polymer concentration in both solutions was 8 mg/mL. The arrows show the IR peaks used to the characterization of polymer adsorption. The flow rate of the polymer solutions and deionized water in the washing step was 1 mL/hr.

In the next series of experiments, the effect of the concentration, of the PAA solution was examined for 0.5$\leq C_{PAA} \leq$40 mg/mL. As shown in Fig. 3b, for $C_{PAA}$$\leq$20 mg/mL, the absorbance intensity of C=O group increased with polymer concentration, indicating that a larger amount of PAA adsorbed to the surface. At $C_{PAA}$$>$20 mg/mL, absorbance leveled off, suggesting that a saturated polymer layer formed on the surface.

Fig 3c shows the variation in intensity of the characteristic PAA absorption peak, plotted as a function of time of insertion of the PAA solution in the MF device and the time of washing. The experiments were conducted for three values of $C_{PAA}$ of 0.5, 15 and 40 mg/mL at Q=1 mL/hr. For all solutions, a steady state absorbance was reached in ~5 min after the polymer solution front reached the ATR crystal surface. When $C_{PAA}$ increased from 0.5 to 15 mg/mL, the amount of adsorbed PAA notably increased after washing, however, no significant change in adsorption occurred upon further increase in $C_{PAA}$ from 15 to 40 mg/mL. The latter effect suggested the formation of the saturated PAA layer at $C_{PAA}$$=$15 mg/mL.

Next, we explored the effect of pH of the solution on PAA adsorption. Phosphate, Tris, and Piperidine buffers were used to adjust the value of pH of PAA solutions to 2, 8 and 11, respectively. For the PAA solution at pH of 8 and 11, Fig. 4, b, c and d show the characteristic symmetrical and asymmetric stretching bends of the COO$^-$ group at 1408 and 1562 cm$^{-1}$, respectively, and the CH$_2$ stretching frequency at 1453 cm$^{-1}$. For pH=2 (Fig 4e and f), the IR spectra exhibited the stretching bend of C=O group at 1717 cm$^{-1}$, the CH$_2$ stretching bend at 1455 cm$^{-1}$, and the C-O stretching bend at 1265 cm$^{-1}$. The characteristic peaks used to analyze the adsorption behavior of PAA are specified by arrows in Fig. 4. We also examined the effect of ionic strength on PAA adsorption by adding an electrolyte NaCl to the polymer solution to the concentration $C_{NaCl}$ of 0.1 and 1 M.
This journal is © The Royal Society of Chemistry [year].

Fig. 3 Variation in absorbance, plotted as a function of velocity of PAA solution (a) and PAA concentration, \( C_{\text{PAA}} \), in the solution (b). In (a) \( C_{\text{PAA}} = 5 \text{ mg/mL} \). In (b) \( Q = 1 \text{ mL/hr} \). All experiments included 25 min infusion PAA solution and 25 min-long washing step. (c) Temporal variation in absorbance \( C_{\text{PAA}} \) (bottom to top) of 0.5, 15 and 40 mg/mL, all monitored over polymer infusion time and washing time. In (a-c), each experimental point represents the average of the results of three independent experiments.

Fig. 4 shows that at pH=11 and \( C_{\text{NaCl}} = 0.1 \text{ M} \), the PAA did not adsorb to the surface, however upon an increase in the ionic strength (Fig. 4b), a decrease in pH (Fig. 4c), or at a simultaneous change in both characteristics (Fig. 4d), polymer adsorption took place. An increase of an ionic strength of the solution did not affect the spectral position of the characteristic IR band of PAA, but resulted in a stronger adsorption of PAA (compare Fig. 4a and b or Fig. 4c and d). When the COOH group of PAA was not ionized at pH=2, an increase in ionic strength of the solution had little effect on polymer adsorption (Fig. 4e and f). The PAA adsorption on the ATR crystal surface decreased with an increasing pH of the solution, as evidenced by comparing Fig. 4a and c (or 4b and d) at the same NaCl concentration.

These results agree with the existing mechanism of polyelectrolyte adsorption, in which the ionization state of charged groups largely determines the quality of the solvent for the polymer. At high pH values and low ionic strength, the quality of the solvent for PAA was improved, which counteracted its adsorption on the ATR crystal surface. For pH<\( pK_a \), the protonated \(-\text{COOH} \) groups are the most prevalent, and PAA readily adsorbed on the crystal from a poor solvent.

In principle, the IR spectra of the adsorbed polymer could provide information on the change in PAA conformation with pH, since at pH=\( pK_a \), PAA molecules undergo a transition from the globular state to the rod-like configuration, which is most likely preserved on the surface. Yet, at pH=2 (below \( pK_a \)) and pH of 8 and 11 (above \( pK_a \)), different characteristic bands were monitored, thereby precluding comparison of the spectral position of the IR peaks. We note however a small difference in the position of the asymmetric stretching bend of the COO\(^-\) group from 1560 to 1553 cm\(^{-1}\), when pH increased from 8 to 11, respectively, in 1M NaCl solution. This shift may reflect the change in the stretched configuration of PAA molecules, due to electrostatic repulsion between the deprotonated -COO\(^-\) groups.

Finally, we utilized the MF-IR method to monitor in-flow layer-by-layer (LbL) adsorption of alternating polymer layers formed by the anionic PAA and cationic PAH molecules. Following 5 min injection of the PAA solution (\( C_{\text{PAA}} = 2 \text{ mg/mL}, Q=1 \text{ mL/hr} \)) and a subsequent washing step with a deionized water, we introduced in the MF device a solution of PAH at the same concentration, flow rate, and insertion time as those of PAA solution. These two steps were repeated 5 times and the IR spectra were collected after each washing step.

Fig. 5a shows the corresponding IR spectra of PAA and PAH,
which exhibit the N-H stretching band at 1560 cm$^{-1}$, characteristic for PAH, and the C=O stretching band of COOH group at 1726 cm$^{-1}$, characteristic for PAA. Thus we monitored changes in IR spectra in the 1400-1800 cm$^{-1}$ spectral region, to study adsorption of PAA and PAH.

Absorbance intensity of the peak at 1726 cm$^{-1}$ increased after the injection of the PAA solution and decreased after the infusion of the solution of PAH. Similarly, absorbance intensity of the peak at 1560 cm$^{-1}$ increased with addition of PAH in the system and decreased with addition of PAA (Fig. 5a). The variation in absorbance intensity of the characteristic peaks of PAA and PAH, both after the washing steps, is plotted in Fig. 5c as a function of the layer number (odd number for infusion of PAA and even number for infusion of PAH). Adsorption of both polymers exhibited a stepwise profile. The change in intensity of the peak at 1560 cm$^{-1}$ was notably stronger than at 1726 cm$^{-1}$, due to the additional contribution of COO$^-$ group of PAA, due to deprotonation of the COOH group after infusion of PAH (pH=7.0). Thus with every addition of PAH, the intensity of the COOH band was reduced, whereas the peak at 1560 cm$^{-1}$ was increased. Upon the addition of PAA solution (pH=3.5) these groups were protonated, again. Another reason for the stronger change in PAH absorption, leading to the asymmetric growth of two polyelectrolyte multilayers, could originate from charge overcompensation at the surface, which occurred mostly upon the addition of a polycation.46

In addition, we conducted IR characterization of PAA and PAH layers adsorbed under quiescent conditions. The corresponding IR spectra of PAA and PAH are shown in Fig. 5b and the variations in absorbance intensity of the characteristic peaks of PAA and PAH, both after the washing steps, are plotted in Fig. 5d. Compared with the quiescent conditions, the IR spectra of both PAA and PAH adsorbed in flow exhibited characteristic bands with higher intensities. This effect indicated that flow favoured LbL adsorption, presumably to the shear-induced exposure of functional groups responsible for adsorption in the preceding polymer layer adsorbed to the ATR crystal..

![Fig. 5](image)

**Fig. 5** Infrared spectra of alternating PAA and PAH layers adsorbed under flow (a) and quiescent (b) conditions. The concentration of PAA and PAH solutions was 2 mg/mL. The values of pH were 3.5 and 7.0 for solutions of PAA and PAH, respectively. In MF experiments, the time of solution infusion was 5 min, which was followed by a 5 min washing with deionized water. The flow rate of the polymer solutions and deionized water was 1 mL/hr. For the quiescent adsorption experiments, the solution was introduced onto the ATR-crystal and incubated for 5 min before washing with deionized water. (c, d) Variation in intensity of 1726 cm$^{-1}$ (corresponding to PAA) and 1560 cm$^{-1}$ (corresponding to PAH) peaks, following the formation of each successive layer under flow (c) and static (d) conditions. Odd numbers of layers represent those with the outmost PAH layer; even numbers of layers represents those with the PAA outmost layer.

To validate a MF-IR methodology, we examined the thickness of alternating PAA and PAH layers formed by adsorption in-flow (shear rate 69.4 s$^{-1}$) and under static conditions by using surface profilometry. Adsorption in flow was carried out under conditions similar to MF-IR experiments. Fig. 6 shows that under in-flow conditions, the build-up of the polymer layers was faster than that under the static conditions. Furthermore, in contrast to static conditions, polymer layer growth occurred in a non-linear manner, in agreement with IR-MF experiments (Fig. 5). In particular, in static conditions, the average thickness of the PAA/PAH bilayer was 12 nm, in agreement with earlier reported results,45 while the average thickness of the PAA/PAH bilayers formed in flow was 17.1 nm. A larger thickness of the polymer bilayer adsorbed under flow could be presumably caused by the change in polymer conformation (a larger number of loops), due to the shear stress imposed on the polymer chains during adsorption process.44

![Fig. 6](image)

**Fig. 6** Variation in thickness of PAA/PAH LbL film adsorbed under flow (left) and static (right) conditions. Each bilayer was prepared using PAA solution at pH=3.5 and PAH solution at pH=7.0 at the incubation time of 5 min. The film was rinsed with deionized water and air-dried before the measurement. Odd numbers of layers represent those with the outmost PAA layer and even numbers of layers represents the film with the PAH outmost layer. The
concentration of PAA and PAH solutions ($C_{\text{PAA}}$ and $C_{\text{PAH}}$) are 2 mg/mL. Injection flow rates of PAA solution, water and PAH solution were 1.0 mL/hr. Under both conditions, each experimental point represents the average of the results of three independent experiments.

Conclusions

A MF-IR platform was developed for in-situ studies of polymer adsorption from solutions flowing past a solid surface. Adsorption of polyelectrolytes was studied under varying flow rates, polymer concentrations, pH, and ionic strengths of the solution. The platform was also used to study layer-by-layer adsorption of polyacrylic acid and polyallylamine hydrochloride. Comparison of LbL adsorption in flow and under quiescent conditions showed a stronger polymer adsorption in the former case, the effect that needs further investigation. The developed methodology paves the way for studies of in-flow adsorption of biomacromolecules and their supramolecular assemblies, including proteins, nucleic acids and polysaccharides, thereby mimicking important biological processes occurring in vivo.

Acknowledgements

ZW, DV and EK thank NSERC Canada (Discovery grant) for financial support of this work. DV acknowledges Microfluidic Applications and Training in Cardiovascular Health (MATCH) Scholarship. WL thanks New Faculty Startup Funds from Texas Tech University.

Notes and references