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1	Thermally Activated Long Range Electron Transport in Living Biofilms
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6 7 8 9 10 11 12 13 14 15 16 17 18 19 20 21	<ul> <li><sup>1</sup>Center for Bio/Molecular Science and Engineering, Naval Research Laboratory, Washington, DC, 20375 USA</li> <li><sup>2</sup>George Mason University, Fairfax, VA, 22030 USA</li> <li><sup>3</sup>Chemistry Division, Naval Research Laboratory, Washington, DC, 20375 USA</li> <li><sup>4</sup>Departments of Physics, Biological Sciences, and Chemistry, University of Southern California, Los Angeles, CA, 90089 USA</li> <li><sup>5</sup>Department of Chemical Engineering and Materials Science, Michigan State University, East Lansing, MI, 48824 USA</li> <li>Correspondence and requests for materials should be addressed to L.M.T. (tender@nrl.navy.mil)</li> <li>M.D.Y.: Postdoctoral fellow, National Research Council, Washington, DC USA 20418</li> <li>Abstract</li> </ul>
22	Microbial biofilms grown utilizing electrodes as metabolic electron acceptors or donors
23	are a new class of biomaterials with distinct electronic properties. Here we report that
24	electron transport through living electrode-grown Geobacter sulfurreducens biofilms is a
25	thermally activated process with incoherent redox conductivity. The temperature
26	dependency of this process is consistent with electron-transfer reactions involving hemes
27	of <i>c</i> -type cytochromes known to play important roles in <i>G. sulfurreducens</i> extracellular
28	electron transport. While incoherent redox conductivity is ubiquitous in biological
29	systems at molecular-length scales, it is unprecedented over distances it appears to occur
30	through living G. sulfurreducens biofilms, which can exceed 100 microns in thickness.
31	
32	Introduction

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33 Extracellular electron transport (EET) is a widespread microbial respiratory strategy that drives global biogeochemical cycles,<sup>1, 2</sup> and is actively investigated for biocatalysis in 34 renewable energy and synthesis technologies.<sup>3</sup> By performing EET, certain 35 36 microorganisms transport electrons between intracellular metabolic processes and 37 extracellular insoluble electron acceptors or donors ranging from natural minerals to electrodes.<sup>4</sup> For example, the highly studied iron-reducing bacterium G. sulfurreducens 38 39 can utilize insoluble iron (oxy)hydroxides as electron acceptors, providing it a distinct 40 metabolic niche in otherwise oxidant-scarce environments. When grown using acetate as 41 a metabolic electron donor and an electrode poised at a sufficiently positive potential to 42 act as an inexhaustible metabolic electron acceptor, G. sulfurreducens forms a multi-cell 43 thick biofilm on the electrode surface comprised of cells and secreted extracellular substances that include biopolymers, protein filaments, and redox proteins.<sup>5</sup> Electrons 44 45 resulting from intracellular oxidation of acetate are transported to outer surfaces of cells 46 and through the biofilm to the electrode surface over distances that can exceed 100 microns.<sup>6</sup> In this living system the G. sulfurreducens cells catalyze electrode oxidation of 47 48 acetate, conserving a portion of the liberated energy to satisfy their energy needs; the 49 extracellular substances act as a conducting matrix electrically connecting cells to the electrode surface;<sup>7</sup> and catalytic current collected by the electrode is proportional to the 50 51 net rate of acetate turnover by the cells. While electrode-grown G. sulfurreducens biofilms have received considerable attention,<sup>8-13</sup> the mechanisms underlying the nature 52 of their conductivity remain debated.<sup>14, 15</sup> A mechanistic understanding is further 53 54 motivated by the recent demonstration of microbial bioelectrodes, such as those that catalyze electrode reduction of nitrate<sup>16</sup> and carbon dioxide,<sup>17, 18</sup> and recent observations 55

indicating possible centimeter length-scale electron transport through multi-cellular
 microbial cable assemblies.<sup>19</sup>

58 Two incongruent mechanisms have been proposed to describe EET occurring 59 through electrode-grown G. sulfurreducens biofilms. One mechanism, thought to be 60 specific to G. sulfurreducens, invokes coherent metallic-like conductivity similar to that 61 of organic semiconductors attributed to  $\pi$ -stacking of aromatic residues of PilA subunits of type IV pili (a type of protein filament).<sup>20, 21</sup> The other mechanism invokes incoherent 62 redox conductivity<sup>22, 23</sup> similar to that of redox polymers<sup>24</sup> stemming from sequential, 63 64 thermally activated electron transfer reactions among immobilized redox cofactors, which 65 are thought to be hemes of outer membrane or extracellular *c*-type cytochromes known to 66 play central roles in extracellular electron transfer by G. sulfurreducens and other organisms.<sup>25-28</sup> Resolving the specific contributions of c-type cytochromes and type IV 67 68 pili to EET of electrode-grown G. sulfurreducens biofilms has been confounded by the 69 role type IV pili play in surface attachment, secretion, and extracellular localization of ctype cytochromes; <sup>29, 30</sup> the lack of analytical techniques with sufficient resolution to 70 71 provide definitive information regarding spatial organization of *c*-type cytochromes 72 within G. sulfurreducens biofilms; and results in which deletion of pilA or certain types 73 of *c*-type cytochromes only partially inhibits EET by *G*. sulfurreducens to iron (oxy)hydroxides and electrodes.<sup>31</sup> 74 75 Temperature is an experimentally tractable parameter for which the two proposed 76 mechanisms predict very different dependencies: coherent metallic-like conductivity

increases with decreasing temperature, whereas incoherent redox conductivity decreases
 with decreasing temperature.<sup>20</sup> Thus far, the only reported temperature dependency

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79 measurements of electrical conductivity of electrode-grown G. sulfurreducens biofilms have been of the mutant strain CL-1,<sup>20</sup> in which a gene containing a putative PilZ domain 80 81 (involved in type IV pili biogenesis) was deleted, significantly altering the extracellular 82 matrix, abundance of PilA protein, abundance of at least two types of extracellular *c*-type cytochromes, and turnover current compared to the wild type strain.<sup>32</sup> Moreover, these 83 84 measurements were not performed on living biofilms, but rather performed ex situ under 85 vacuum on non-living biofilms peeled off of the electrodes on which they were grown. 86 Here we report results of *in situ* electrical conductivity measurements performed 87 at different temperatures on living electrode-grown wild-type G. sulfurreducens biofilms. 88 The conductivity of the biofilms decreases with decreasing temperature and exhibits an 89 Arrhenius behavior, which supports a redox gradient driven mechanism of EET. Fitting 90 the data to the Arrhenius equation yielded activation and reorganizational energies 91 consistent with electron self-exchange among *c*-type cytochromes acting as the charge 92 carriers. 93 **Results and Discussion** 94 95 The electrical conductivity of living electrode-grown wild type G. sulfurreducens 96 biofilms decreases with decreasing temperature (Fig. 1A). Fitting the temperature 97 dependency of conductivity to the Arrhenius rate expression (Fig. 1B) yields an activation energy  $(E_a)$  of  $0.13 \pm 0.02$  eV and a reorganizational energy  $(\lambda = 4E_a)^{33}$  of 0.52 98 99  $\pm 0.08$  eV, consistent with electron transfer reactions involving hemes of *c*-type cytochromes.<sup>34-37</sup> These measurements were performed at different temperatures in the 100 101 same aqueous medium and under conditions at which G. sulfurreducens biofilms are

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102	typically grown and studied. Measurements were performed using interdigitated
103	microelectrode arrays (IDA) – a 2-electrode configuration comprised of 2 interdigitated
104	electrodes (source and drain) used extensively to characterize conductivity of polymer
105	films <sup><math>38, 39</math></sup> – on which stationary phase <i>G. sulfurreducens</i> biofilms were grown (Fig. 2;
106	Experimental replicates depicted in Supplementary Fig. S3-5). <sup>22, 23</sup> Conductivity at 30°C,
107	the temperature at which G. sulfurreducens biofilms are typically grown and studied, was
108	unaffected by changing the temperature to 10°C and then back to 30°C (Fig. 1A and 1B),
109	indicating that the effect was reversible over this temperature range. Source-drain
110	currents measured upon cooling and heating are both plotted in Fig. 1A and 1B and are
111	statistically indistinguishable from one another. These measurements were performed at
112	a fixed gate potential to eliminate background current due to biofilm Faradic charging
113	(discussed below) and in the absence of acetate (non-turnover condition) to eliminate
114	background current due to acetate oxidation by cells in the biofilm (i.e., turnover current).
115	When placed back under turnover condition at 30°C the biofilm resumed generating
116	catalytic current at the same level as before these measurements were made, indicating
117	that the biofilm was not adversely affected by the temporary change in temperature or by
118	the temporary removal of acetate. (Supplementary Fig. S6).

- 119 In the case of an ideal redox conductor:<sup>22, 24</sup>
- 120
- 121 Eqn. 1  $I_{SD} = nFDSC[P_S P_D]$
- 122 Eqn 2.  $P_{S} = \frac{1}{1 + e^{\left[\frac{nF}{RT}\left(E_{G} \frac{V_{SD}}{2} E^{o'}\right)\right]}}$
- 123 Eqn 3.  $P_D = \frac{1}{1 + e^{\left[\frac{nF}{RT}\left(E_G + \frac{V_{SD}}{2} E^{o'}\right)\right]}}$

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- 124 Eqn. 4  $E_G = \frac{(E_D + E_S)}{2}$
- 125 Eqn. 5  $V_{SD} = E_D E_S$
- 126 Eqn. 6  $D = \frac{k_{ex}C\delta^2}{6}$
- 127 Eqn. 7  $k_{ex} = Ae^{-E_a/kT}$
- 128

129	where $E_S$ and $E_D$ are potentials applied to the source and drain; $I_{SD}$ is the resulting source-
130	drain current (proportional to the rate of electron transport (ET) through the material from
131	the source to the drain); $E_G$ is gate potential (average of source and drain potentials); $V_{SD}$
132	is source-drain voltage (difference between drain and source potentials); $P_S$ and $P_D$ are
133	probabilities that cofactors involved in the heterogeneous electron transfer reactions
134	(across the 2 biofilm/electrode interfaces) are reduced (can donate an electron) vs.
135	oxidized (can accept an electron), which range from 0 (all are oxidized) to 1 (all are
136	reduced); $T$ is temperature; $n$ is the number of electrons transferred per electron transfer
137	reaction $(n = 1)^{40}$ ; <i>F</i> , <i>R</i> , and <i>k</i> are the Faraday, gas, and Boltzmann constants; <i>S</i> is a
138	geometric factor dependent on the electrode configuration and material thickness
139	numerically determined to be 14.5 cm for the specific IDAs and biofilms examined here
140	(Supplementary Information); $D$ is the effective diffusion coefficient for electrons in the
141	material <sup>24, 41</sup> ; C, $\delta$ , and $E^{o'}$ are the redox cofactor concentration, spacing, and formal
142	potential; and $k_{ex}$ , A, and $E_a$ are the rate constant, frequency factor, and activation energy
143	for electron transfer reactions between cofactors. Eqn. 1 is analogous to Fick's 1st law of
144	diffusion. In the case of a redox conductor, application of source and drain potentials
145	induces a redox gradient – a gradient of reduced (or oxidized) cofactors on which
146	electrons (or holes) momentarily reside during ET – across the material between the

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o the
<b>D</b> 1

- 148 magnitude of this redox gradient, which is proportional to  $SC[P_S P_D]$ .<sup>24</sup> (See
- 149 Supplementary Information for a description of Eqn. 1-7).
- 150 Eqn. 1 predicts that redox conductors should exhibit a peak-shaped dependency of

151 source-drain current on gate potential centered at  $E_G = E^{o'}$  when a constant source-drain

- 152 voltage is maintained across the electrodes (electrochemical gating measurements,
- 153 (Supplementary Fig. S7). The peak-shaped dependency of source-drain current on gate
- 154 potential observed here (Fig. 3A) sharply contrasts the sigmoid-shaped dependency
- exhibited by organic semiconductors such as poly(3-methyl thiophene)<sup>38</sup> and is strong
- 156 evidence that redox conductivity occurs in living, electrode-grown G. sulfurreducens
- 157 biofilms.<sup>42</sup> It also sharply contrasts with a previous electrochemical gating study, which is
- based on results acquired with methods that have been called into question,<sup>43</sup> that finds
- 159 living, electrode-grown *Geobacter sulfurreducens* biofilms to be metallic-like
- 160 conductors.<sup>20</sup>

161 The redox cofactor formal potential indicated by Fig. 3A (-0.390 V vs. Ag/AgCl) 162 is consistent with formal potentials of redox cofactors in living, electrode-grown G. 163 sulfurreducens biofilms determined by spectroelectrochemical methods to be c-type cytochromes.<sup>12, 44, 45</sup> Visualization using immuno-gold labeling of three different *c*-type 164 165 cytochromes proposed to be involved in EET of electrode-grown G. sulfurreducens 166 biofilms indicates that these proteins were distributed throughout the biofilms, associated with cell membranes and the extracellular polysaccharide matrix.<sup>32, 50, 51</sup> Antibody size 167 168 and label efficiency, however, precludes immuno-gold labeling from determining 169 whether these *c*-type cytochromes are spaced close enough ( $\leq 2 \text{ nm}$ ) for redox

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170	conductivity to occur. <sup>52</sup> The genome of <i>G. sulfurreducens</i> potentially encodes over 100
171	different <i>c</i> -type cytochromes many of which have yet to be identified and experimentally
172	evaluated for involvement in EET. The apparent redox cofactor formal potential nearly
173	coincides with the catalytic midpoint potential $(E_M)$ indicated by turnover voltammetry
174	performed on the same biofilm (Fig. 3C). <sup>46</sup> This suggests that the same cofactors are
175	involved in EET for source-drain current, when an electrode is the source of electrons, as
176	for turnover current, when acetate turnover by cells is the source of electrons. <sup>46</sup> Current
177	peaks wider than predicted by Eqn. 1 are consistent with a distribution in formal
178	potentials of redox cofactors involved in EET (Supplementary Fig. S7). <sup>23</sup>
179	For the electrochemical gating measurements performed here, the source-drain
180	voltage is sufficiently small ( $V_{SD} \le 0.05$ V (Supplementary Fig. S8) that Eqn. 1 can be
181	linearly approximated by Ohm's Law:
182	
183	Eqn. 8 $I_{SD} = GV_{SD}$
184	Eqn. 9 $G = \sigma S$
185 186	where G is conductance and $\sigma$ is conductivity, such that conductivity scales linearly with
187	experimentally measured source-drain current (scaling factor = $1/V_{SD}S = 6.90$ cm <sup>-1</sup> V <sup>-1</sup>
188	for $S = 14.50$ cm and $V_{SD} = 0.01$ V, used to scale right-hand vertical axes of Fig. 1 and 3)
189	For an ideal redox conductor:
190	
191	Eqn. 10 $\sigma = \frac{n^2 F^2 DC}{RT} \left( \frac{e^{\left[\frac{nF}{RT}(E_G - E^{o'})\right]}}{1 + 2e^{\left[\frac{nF}{RT}(E_G - E^{o'})\right]} + e^{\left[\frac{2nF}{RT}(E_G - E^{o'})\right]}} \right)$
102	

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193	obtained by linearly approximating Eqn. 1 for the case of a sufficiently small source-
194	drain voltage for which Eqn.8 applies (Supplementary Information). When the gate
195	potential is equal to the formal potential ( $E_G = E^o$ '), Eqn. 10 can be expressed as:
196	
197	Eqn. 11 $\sigma = \frac{X}{T} e^{-E_a/kT}$
198	Eqn. 12 $X = \frac{n^2 F^2 C^2 \delta^2 A}{24R}$
199	
200	where <i>X</i> is a temperature independent constant. Fitting temperature dependency of $\sigma$
201	when $E_G = E^o$ ' based on Eqn. 11 is expected to yield the activation energy for the redox
202	cofactor electron self-exchange reaction (Fig. 1B). The maximum conductivity at 30°C is

203 on the order of  $10^{-6}$  S cm<sup>-1</sup> (Fig. 3A). This conductivity corresponds to electron mobilities 204 orders of magnitude below the lower limit of coherent band transport, further ruling out 205 that the mechanism of biofilm transport is similar to  $\pi$ -stacked materials and organic 206 semiconductors.<sup>47, 48</sup>

207 Regardless of the assumed mechanism of EET, G. sulfurreducens biofilms 208 possess intrinsic redox activity in which a change in gate potential induces a net change 209 in oxidation state of electrode-accessible redox cofactors throughout the biofilm (i.e., Faradaic charging),<sup>5</sup> which occurs through a combination of heterogeneous EET (across 210 211 the biofilm/electrode interfaces) and homogenous EET (within the biofilm). This process 212 results in voltammetric current peaks observed under non-turnover condition (when not 213 obscured by acetate turnover current) that scale linearly with the square root of scan rate 214 and that exhibit negligible splitting with increasing scan rate (Fig. 4A). A net change in 215 oxidation state of biofilm redox cofactors also results in current transients that decay with

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216	the square root of time when the gate potential is abruptly changed under non-turnover
217	condition (Fig. 4B) across the cofactor formal potential. Both results are observed for
218	redox conductors <sup>41, 49</sup> and are consistent with non-limiting heterogeneous electron
219	transfer and with diffusive homogeneous electron transport occurring in $G$ .
220	sulfurreducens biofilms described by Eqn. 1.41
221	
222	Conclusions
223	The results described here provide strong evidence that living electrode-grown $G$ .
224	sulfurreducens biofilms act as redox conductors in which hemes of c-type cytochromes
225	are the apparent redox cofactors involved in EET. Redox conduction over distances only
226	recently determined to occur in electrode-grown in G. sulfurreducens biofilms is
227	unprecedented in biological systems based on classical molecular-scale redox reactions.
228	However, long-range redox conduction may be prevalent in biological systems, <sup>19, 53</sup> and
229	understanding this process provides a framework for increased understanding of
230	environmental nutrient cycling and potential for biotechnology applications.
231	
232	Materials and Methods
233	Unless otherwise noted methods and materials used here were the same as
234	previously reported. <sup>7, 23</sup>
235	Interdigitated microelectrode arrays.
236	IDAs (interdigitated microelectrode arrays), used extensively to perform
237	conductivity measurements on electrochemically grown polymers, <sup>38, 39, 54</sup> are a variation
238	of the double-band electrode configuration (see Fig. 1a, Kankare and Kupila (1992) <sup>55</sup> and

Fig. 2b of Snider et al.  $(2012)^{23}$ ). The IDAs used to obtain data depicted in Figs. 1-4 were 239 240 obtained commercially (CH Instruments, model 012125) and consist of 130 parallel gold 241 rectangular bands, each 2 mm long x 10 µm wide x 90 nm thick, patterned onto a flat 242 glass substrate separated by 5  $\mu$ m wide gaps (total electrode area (source + drain): 0.026 243  $cm^2$ , total biofilm coated array area (electrodes and gap): 0.039  $cm^2$ ). Every other band is 244 electrically connected at opposite ends of the array forming two separately addressable 245 interdigitated electrodes, each comprised of 65 bands, separated by a single 25.8 cm long 246 (129 x 2mm) x 5 µm wide gap that weaves back and forth across the array. IDAs were 247 used as received. Teflon insulated wires were affixed to the terminal contact pads of the 248 IDA working electrodes using conductive silver epoxy (Electron Microscopy Sciences, 249 Hatfield, PA). These connections were then sealed in Scotchcast resin (3M, Austin, TX) 250 using the tip of a 15-ml conical centrifuge tube as a mold. IDAs used to obtain replicate 251 data depicted in supplementary Figs. S3-5 were identical to those described above, or fabricated in house following previous methods.<sup>7, 23</sup> 252

# 253 Electrochemical Instrumentation.

WaveDriver bipotentiostats Model WD20 (Pine Instruments, Durham, NC) were
used to perform all experiments presented in Fig 1-4 except for the potential step
experiments (Fig. 4B), which were performed using a Biologic VMP3 8-channel
potentiostat (Biologic Inc., Knoxville, TN).

### 258 Electrochemical reactors.

All biofilm electrochemical experiments were performed in 250-ml water jacketed electrochemical reactors (Pine Instruments, Durham, NC) maintained under anaerobic conditions by constant sparging with an 80% N<sub>2</sub>/ 20% CO<sub>2</sub> gas mix. Reactors

262	contained a Ag/AgCl reference electrode (3M NaCl, Bioanalytical Systems, Inc.) and a
263	non-limiting graphite rod counter electrode (0.6 mm dia, 10 mm length, Electron
264	Microscopy Sciences) as previously described. <sup>22, 23</sup> All potentials reported here are vs.
265	Ag/AgCl (3M NaCl) and can be approximated as vs. SHE by addition of 0.195 V.
266	Temperature was controlled using a Haake AC200 temperature controller (Thermo
267	Scientific) to circulate temperature regulated water through the jackets of the
268	electrochemical reactors. Temperature regulation of the experimental reactors was
269	verified using a glass thermometer upstream in the circulator and a glass thermometer
270	downstream in a second reactor.
271	Biofilm growth.
272	Biofilms were grown at 30°C on IDAs covering the electrode bands and gaps by
273	poising both electrodes at 0.300 V in fresh water media (ATCC 2260, excluding Wolfe's
274	vitamins) containing acetate (10 mM) as the electron donor and carbon source using
275	previously described methods. <sup>22, 23</sup> This resulted in an increase in acetate turnover
276	(catalytic) current over time at both electrodes due to proliferation of cells coupling
277	oxidation of acetate (respiration) with EET to the electrode surfaces. <sup>7, 22, 23, 46</sup> Biofilms
278	were allowed to grow until turnover current plateaued (biofilm stationary phase;
279	approximately10 days after inoculation). Biofilm thickness ( $80 \pm 9 \ \mu m$ ) was determined
280	ex situ by confocal microscopy as previously described (Supplementary Fig. S9). <sup>23</sup>
281	Electrochemical gating measurements were performed on 3 biological replicates and the
282	results depicted in Fig. 1 and 3 are considered typical.
283	Electrochemical gating measurements:

284	Electrochemical gating measurements (Fig. 3) were performed at 30°C in the
285	same electrochemical reactors in the same medium used for biofilm growth to ensure
286	biofilm viability. Measurements were performed using the bipotentiostat to
287	simultaneously scan potentials of the source and drain electrodes, and thus gate potential
288	( $E_G$ , Eq. 4), at the same scan rate ( $v$ ) while maintaining a constant potential offset
289	between the electrodes (source-drain voltage, $V_{SD}$ , Eq. 5) and to measure the source-drain
290	current ( $I_{SD}$ ) separately at each electrode. It was determined that for $v < 2$ mV/s, source-
291	drain current is nearly independent of $v$ , for which source-drain current at each gate
292	potential can be considered to be nearly steady state (Supplementary Fig. S5). For all
293	electrochemical gating measurements depicted here $v = 1$ mV/s. It was also determined
294	that for $V_{SD} < 0.2$ V, source-drain current scales linearly with $V_{SD}$ per Eqn. 8
295	(Supplementary Fig. S8). For all electrochemical gating measurements depicted here $V_{SD}$
296	= 0.01 V. Electrochemical gating measurements were performed with acetate present as
297	during biofilm growth (turnover condition), and after media containing acetate in the
298	electrochemical reactor was replaced with media lacking acetate (non-turnover condition).
299	When performing electrochemical gating measurements (Fig. 3, Fig. S1), at least
300	two types of background current need to be subtracted from current measured at the
301	source and drain electrodes to yield the source-drain current at each gate potential
302	(Supplementary Fig. S1). The first is current due to intrinsic redox activity of the biofilm
303	in which the oxidation state of redox cofactors changes as gate potential changes (i.e.,
304	Faradaic charging current). The second is turnover current due to acetate oxidation,
305	which is expected to occur only under turnover condition. The total background current
306	under both conditions was approximated by sweeping the gate potential at 1 mV/s as

307 above, but with  $V_{SD} = 0$  V such that  $I_{SD} = 0$  (equivalent to simultaneously performing 308 turnover voltammetry when acetate is present and non-turnover voltammetry when 309 acetate is removed at each electrode). The resulting current at each electrode at each gate 310 potential, which constitutes total background current under each condition, was 311 subtracted from current measured at each electrode for  $V_{SD} = 0.01$  V at each gate potential, 312 yielding source-drain current at each electrode for each gate potential (Fig. 3 and 313 Supplementary Fig. S1). Alternatively, subtracting the raw source current directly from 314 the raw drain current yields twice the background subtracted source-drain current, since 315 background currents are expected to be equal at both electrodes and source-drain currents 316 are expected to be equal in magnitude at both electrodes, but opposite in sign (Fig. S2). 317 Both methods of background subtraction were used here. Following all non-turnover 318 measurements, turnover current resumed at previous levels after replacement of media 319 lacking acetate with media containing acetate, indicating biofilm viability throughout the 320 measurements (Supplementary Fig. S6). 321 The methods used here of slowly sweeping the gate potential with  $V_{SD} = 0.01$  and 322 either subtracting background current obtained at  $V_{SD} = 0$ , or subtracting the source from 323 drain current, have been compared to a method in which the gate potential was stepped in 324 0.05 V increments across the same potential range under non-turnover condition while maintaining  $V_{SD} = 0.01$  V, and recording the source and drain current after sufficient time 325 326 had elapsed after each step (~2.5 minutes), so that the current achieved a near steady state value.<sup>43</sup> Ideally, current due to Faradaic charging is expected to decay over time 327 328 following each step as the net oxidation state of cofactors in the biofilm are expected to 329 converge to the gate potential-dependent value. Under non-turnover condition, this

330 method is expected to directly yield the source-drain current at each electrode. The peak 331 shaped conductivity vs. gate potential dependency obtained by incrementally stepping the gate potential correlated with that obtained by sweeping the gate potential.<sup>43</sup> The peak 332 333 magnitude however was approximately 2-fold greater for stepping the gate potential than 334 for sweeping the gate potential, which we attribute to persistent Faradaic charging current. 335 We chose to use the sweeping method because it is less tedious, less prone to human 336 error since data collection can be fully automated, and because it provides greater 337 resolution with respect to gate potential. Moreover, when we performed electrochemical 338 gating measurements of a known redox conducting polymer and known semiconducting 339 polymer by slowly sweeping the gate potential and either subtracting current obtained at  $V_{SD} = 0$ , or subtracting the source from drain current, we obtained the expected results 340 based on prior literature results validating our experimental methods.<sup>43</sup> 341

# 342 Temperature-dependent conductivity measurements:

343 Measurement of the temperature dependency of conductivity (Fig. 1A) of living 344 electrode-grown G. sulfurreducens biofilms was performed by stepping the temperature 345 from 30°C to 10°C in 2°C increments under non-turnover condition. The electrodes used 346 in these measurements (IDA source and drain) were the same ones used to grow the 347 biofilms. The gate potential was fixed at -0.390 V vs. Ag/AgCl, the gate potential for 348 which conductivity was determined to be greatest (Fig. 3). Since the gate potential was 349 fixed, there was no background current due to Faradaic charging to contend with. Current 350 was allowed to stabilize at each temperature after the downstream thermometer indicated 351 the desired temperature (>20 minutes). The temperature was then stepped in  $10^{\circ}$ C 352 increments back to 30°C and conductivity measured again at 20°C and 30°C to confirm

353	that the effect of temperature on conductivity was reversible. Source-drain currents	
354	measured upon cooling and heating are both plotted in Fig. 1A and 1B and are	
355	statistically indistinguishable from one another. Electrochemical reactors were not stirred	
356	during these measurements to minimize electrical noise. Following these measurements,	
357	the biofilms were placed back under turnover condition and turnover current resumed at	
358	prior levels confirming that the biofilms were not adversely affected (Supplementary Fig.	
359	S6).	
360	Activation energy $(E_a)$ was determined by fitting the experimental data to Eqn. 11	
361	to $ln(\sigma T_i)$ vs. $1/T_i$ , where <i>i</i> is the index for the discrete experimental points. Fitting the	
362	experimental data to a straight line using the least squares method with weighted errors	
363	given by $l/\sigma_t$ yielded parameters $ln(A)$ and $E_a$ . Separate fits were applied to the source	
364	and drain data. The corresponding reorganizational energy ( $\lambda$ ) was determined by $\lambda = 4E_a$	
365	following Marcus <sup>33</sup> . Temperature dependency of conductivity measurements were	
366	performed on 3 biological replicates and the results depicted in Fig. 1 are considered	
367	typical (Supplementary Fig. S4-5).	
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- 455 slope was calculated using Eqn. 11. Representative data is shown here. Replicates can be
- 456 found in Supplementary Information.



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458 Fig. 2. Experimental set up. A: Water-jacketed 250-ml anaerobic electrochemical reactor 459 containing freshwater medium in which a living G. sulfurreducens biofilm was grown on 460 an IDA (S: source, D: drain, RE: Ag/AgCl reference electrode, CE: counter electrode). 461 Bipotentiostat separately applies source and drain potentials ( $E_S$  and  $E_D$ ) vs. RE (gate potential,  $E_G = (E_D + E_S)/2$ , source-drain voltage,  $V_{SD} = E_D - E_S$  and separately 462 463 measures resulting source-drain current  $(I_{SD})$  at each electrode. B: Biofilm growth 464 confined to unmasked region of IDA comprised of alternating source and drain electrode 465 bands. C: Schematic of biofilm/IDA cross-section depicting 4 alternating source and 466 drain bands. IDAs used here contained 130 bands. IDA dimensions are provided in the 467 Materials and Methods Section.







**Fig. 3.** Electrochemical gating measurements ( $I_{SD}$  vs.  $E_G$ ) for  $V_{SD} = 0.01$  V under A: nonturnover condition, and B: turnover condition. Background currents have been subtracted out (details in Materials and Methods) leaving only source-drain currents (Raw data can be found in Supplementary Information). C: Turnover condition,  $V_{SD} = 0.0$  V such that  $I_{SD} = 0$  (equivalent to biofilm acetate turnover (catalytic) voltammetry recorded simultaneously at each electrode) where the observed current is attributed to the sum of

- 475 acetate turnover current and Faradaic charging current. Scan rate (v, rate of change of  $E_G$ )
- 476 is 1 mV/s for all three cases to approximate steady current at each value of  $E_G$ .



