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Tuning the surface properties of hydrogel at nanoscale with focused ion irradiation

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Abstract

With site-specific machining capability of Focused Ion Beam (FIB), we aim to tailor the surface morphology and physical attributes of biocompatible hydrogel at nano/micro scale particularly for tissue engineering and other biomedical studies. Thin film of Gtn-HPA/CMC-Tyr hydrogels were deposited on gold coated substrate and were subjected to irradiation with kiloelectronvolts (keV) gallium ion beam. The sputtering yield, surface morphology and mechanical property changes were investigated using Scanning Electron Microscopy (SEM), Atomic Force Microscopy (AFM) and Monte Carlo simulation. The sputtering yield of hydrogel was found to be approximately $0.47 \mu\text{m}^3/\text{nC}$ compared with Monte-Carlo simulation results of $0.09 \mu\text{m}^3/\text{nC}$. Compared to the surface roughness of pristine hydrogel approximately 2 nm, the average surface roughness significantly increased with the increase of ion fluence with measurements extended to 20 nm at $100 \text{ pC}/\mu\text{m}^2$. Highly packed submicron porous patterns were also revealed with AFM, while significantly decreased pore size and increased porosity were found with ion irradiation at oblique incidence. The Young's modulus of irradiated hydrogel determined using AFM force spectroscopy was revealed to be dependent on ion fluence. Compared to the original Young's modulus value of 20 MPa, irradiation elevated the value to 250 MPa and 350 MPa at $1 \text{ pC}/\mu\text{m}^2$ and $100 \text{ pC}/\mu\text{m}^2$, respectively. Cell culture studies confirmed that the irradiated hydrogel samples were biocompatibility, and the generated nanoscale patterns remained stable under physiological conditions.

Keywords: hydrogel, Focused Ion Beam (FIB), ion irradiation, surface morphology, elastic modulus

1 **1. Introduction**

2 Hydrogels are crosslinked network composed of either natural or synthetic polymers, and the
3 hydrophilic properties of hydrogels make them great materials for bioengineering^{1, 2}. It is
4 well known that the shapes and physiochemical properties of hydrogels have strong influence
5 on cell growth and migration, and various approaches have been developed to tune these
6 properties for improved cell growth and biocompatibilities. For example, porosity and pore
7 size could be altered through additional porogens, freeze-drying, photopatterning, foam
8 generation, etc.³⁻⁷, while elastic modulus is a function of component concentrations^{8, 9}. In
9 addition to physical and chemical properties, topographic properties at micro and nanoscale
10 have been recently suggested to play critical roles in cellular interaction with its surrounding
11 environments¹⁰⁻¹³. For tissue engineering applications, it is now also advantageous to create
12 nanoscale features on surface with properties similar to those in extracellular matrix in order
13 to control cellular behaviour, enhance cell growth, adhesion and proliferation^{10, 11, 13-15}.

14

15 Previous studies on shape control of surface nanotopology were typically based on soft
16 lithography¹⁶ or the intrinsic elastic property^{16, 17}, dominantly on Polydimethylsiloxane
17 (PDMS), there are only limited reports on altering surface topology of hydrogels at micro and
18 nanoscale, possibly due to the technical difficulties involved in fabricating micro/nanoscale
19 structure on soft materials, or limited knowledge of fundamental mechanisms involved.
20 Recent reports showed that ion beam irradiation was capable of forming nanoscale wrinkle
21 features on polymer surfaces¹⁸⁻²⁴. Typically equipped with a gallium ion (Ga^+) or Helium
22 (He^+) source, a modern Focused Ion Beam (FIB) instrument allows the accelerated ions to
23 perform site specific milling with electrostatic lenses²⁵⁻²⁷. In conjunction with scanning
24 electron microscope (SEM), micro- and nano-machining with resolution down to single digit
25 nanometer can be done while imaging and analysing at the same time. FIB/SEM has been
26 successfully applied for imaging applications such as three dimensional hydrogel⁴, cell-
27 material interfaces and even single cells²⁸⁻³⁰. However, the capability of site specific FIB
28 milling is not fully utilized for biomaterial applications.

29 An example of periodic pattern of micron size dots presented in In Figure 1a was designed
30 and preliminarily patterned on hydrogel surface within minutes, without the use of chemicals
31 or sophisticated masks. This provided a prompt method for fabricating nano/micro scale
32 features on hydrogel, and the final pattern was visible by optical microscope with clearly
33 defined geometry (Figure 1b). Under SEM, however, some morphological artefacts on

1 surface could be observed, and inconsistent geometries such as milling depth were also
2 present due to lacking of information (Figure 1c). As such, the primary aim of the present
3 research is to provide an in-depth investigation on the surface topology and physical
4 properties of hydrogel at nano/micro scale by utilizing FIB, to achieve designed patterns of
5 high precision. The engineering issues including yield and angular effects were investigated
6 through both Monte Carlo simulation and experimental studies. Other questions such as
7 surface roughness and modulus of hydrogel were measured by Atomic Force Microscopy
8 (AFM) prior to and after ion irradiation. Based on these results, patterns on hydrogel with
9 tailored surface topology and physical attributes could be precisely achieved by setting the
10 beam parameters, e.g. acceleration voltage, ion fluence and incident angle. The compatibility
11 and stability of the patterned hydrogels were also tested in cell culture to demonstrate the
12 applicability of this patterning method for bioapplications.

13

14 **2. Materials and methods**

15 **Sample preparation**

16 Carboxylmethylcellulose-tyramine (CMC-Tyr) and gelatin-hydroxyphenylpropionic (Gtn-
17 HPA) were synthesized according to ⁴. CMC-Tyr conjugate and Gtn-HPA conjugates were
18 each dissolved in phosphate buffer saline (PBS) solution at a concentration of 5%. A
19 hydrogel precursor solution was prepared by mixing Gtn-HPA and CMC-Tyr to 80:20 weight
20 ratio, respectively. This precursor went through a vigorous vortex for a few minutes.
21 Horseradish peroxide (HRP) and diluted H₂O₂ were then added to the precursor as cross-
22 linking reagent, each reagent was pre-diluted with PBS solution. A final concentration of
23 15.5units/L of HRP and 49.8×10^{-6} M of H₂O₂ was used in this research. This precursor was
24 then vigorously vortexed for a few minutes. The pH level of PBS solution, hydrogel before
25 and after cross-linking is measured using a pH metre (Thermo Fisher Scientific, Scoresby,
26 VIC Australia). For PBS solution, pH level was measured to be 7.51 and pH level of
27 hydrogel before and after crosslinking was 7.35 and 7.41 respectively.

28 An aliquot of 100 μ l of the precursor was deposited on a gold plated cover glass and any air
29 bubbles were removed by gently stirring with the tip of micropipette. In order to achieve a
30 thin, uniform layer of hydrogel, spin coating was performed in three stages. In the first stage,
31 spin coating was span for 500 rpm for 10 seconds, followed by 3000 rpm for 40 seconds.

1 Finally, another 500 rpm for 10 seconds of spin coating provided a thin uniform layer of
2 mixture with the thickness of approximately 1 μm . The precursor was then allowed to
3 crosslink to form hydrogel.

4 **Focused Ion Beam (FIB) irradiation**

5 FIB milling was performed on a FIB/SEM system (FEI Helios NanoLab 600) equipped with
6 a gallium liquid metal ion source (LMIS). Thin film of hydrogel samples were first
7 transferred to the system chamber until high vacuum status is reached. Ion current used in the
8 experiment ranges from 0.92 pA to 0.97 nA. Without additional notes, default overlapping
9 and dwell time were 0% and 3 μs respectively. Ion fluence of the Ga^+ ranging from 0.05
10 $\text{pC}/\mu\text{m}^2$ to 600 $\text{pC}/\mu\text{m}^2$ was regulated to irradiate $10 \times 10 \mu\text{m}$ square region. Default incident
11 angle was kept at 0° (normal incidence), and to study the effect of the incident angle, the
12 stage was tilted from 0° to 62° . SEM images were typically acquired with a secondary
13 electron detector with 5 keV acceleration voltage and 86 pA current.

14 **Atomic force microscopy (AFM)**

15 Surface properties were examined using an AFM instrument (Dimension Icon, Bruker
16 Corporation, Santa Barbara, CA, US) under cleanroom environment. For measuring surface
17 topology, cantilevers of 70 kHz of resonance frequency and 0.4 N/m of spring constant were
18 used. By default, $20 \times 20 \mu\text{m}$ regions were scanned to obtain reliable statistics. The sputtering
19 yield of hydrogel was calculated by examining the volume removed by the ion beam
20 irradiation and ion fluence applied. Surface roughness and the characteristics of regular
21 patterns were calculated using software package (NanoScope Analysis 1.4, Bruker
22 Corporation, Santa Barbara, CA, US). For the force measurement and modulus calculation,
23 cantilever with 0.06 N/m spring constant was used to accommodate the low modulus of
24 hydrogel sample with JPK NanoWizard2 AFM (JPK Instruments AG, Berlin, Germany)
25 under ambient conditions. Calibration of the cantilever was conducted prior to the force
26 mapping using mica sheet, measuring sensitivity and spring constant of the cantilever. Force
27 mapping of the sample of $5 \times 5 \mu\text{m}$ regions were done with 16×16 resolution. Analysis was
28 carried on using JPKSPM Data Processing software (JPK Instruments AG, Berlin, Germany)
29 which allows to do batch processing.

30

31 **SRIM Monte-Carlo simulation**

1 Monte-Carlo simulation of the sputtering process of hydrogel was performed with software
2 package SRIM (The Stopping and Range of Ions in Matter) version 2013³¹. Hydrogel was set
3 up as a new compound consisting of carbon, hydrogen and oxygen with atomic stoichiometry
4 of 8:8:1 respectively. Density of hydrogel was obtained by measuring the bulk weight and
5 volume, and the average values 1.655 g/cm³ obtained was input for all the simulations. At
6 least 5000 ions were simulated in each run, and parameters including angle of incident and
7 ion energy were varied based on the parameters used in the experiments.

8

9 **Cell culture of COS-7 cells and cytotoxicity test**

10 African green monkey kidney cells (COS-7 cells) were grown and maintained in Dulbecco's
11 Modified Eagle Medium (DMEM) supplemented with 10% fetal bovine serum (FBS), 2mM
12 L-glutamine, and 50 units/ml penicillin-streptomycin (P/S) at 37°C in a 5% humidified
13 carbon dioxide incubator. The patterned, unpatterned hydrogel samples and the tissue culture
14 plate were sterilized under UV for 3 hrs before cell seeding. Cell seeding was conducted at a
15 density of 3×10^4 cell per sample, and in each sample, the diameter of the hydrogel thin film
16 was approximately 1 cm. The plate was incubated at 37 °C in a humidified 5% CO₂ incubator
17 for 3 hrs for cell attachment to take place, and then 3 mL of fresh culture medium was added
18 and the cells were allowed to further cultivate on the hydrogel. Visualization of the cells on
19 patterned hydrogel was executed using an inverted optical microscope at different time point.
20 The viability of cells after immobilization in the hydrogel was examined using a live/dead
21 viability assay kit, and pristine hydrogels without patterning were used as control. The
22 hydrogels were incubated in 5 μM calcein acetoxymethyl ester solution (Life Technologies,
23 Australia) for half an hour, followed by 1.5 μM Propidium Iodide (Life Technologies,
24 Australia) for 5 mins in DMEM at 37 °C. Images of live (green) cells were then acquired on
25 day 5 by using an inverted laser confocal fluorescence microscope (Nikon A1 Rsi MP,
26 Australia). For SEM imaging, the samples were then kept in the -20 °C freezer followed by
27 lyophilization in a freeze-dryer (HETO PowerDry PL6000, Thermo Scientific, Australia) for
28 24 hrs.

29

30

31 **3. Results and discussions**

32

1 Milling yield of hydrogel by keV ion beam

2 The sputtering yield of hydrogel with ion beam irradiation was measured by volume loss
3 method and compared with the results from Monte Carlo simulation based on SRIM. Ion
4 fluence applied for determining the yield ranged from $0.05 \text{ pC}/\mu\text{m}^2$ to $600 \text{ pC}/\mu\text{m}^2$ to obtain
5 an adequate amount of data points prior to significant redeposition, and sputtering rate was
6 represented as volume (μm^3) removed per ion dose (nC) measured by AFM. The milling was
7 performed on a typical hydrogel surface area of $10 \times 10 \mu\text{m}$, and total volume of material
8 removed was calculated and plotted in Figure 2a. The sputtering rate of hydrogel by 30 keV
9 Ga^+ estimated by the gradient of the plotted curve is $0.47 \mu\text{m}^3/\text{nC}$, while the results of MC
10 simulation with SRIM returned $0.09 \mu\text{m}^3/\text{nC}$ were also plotted in Figure 2a for comparison.

11

12 The difference between experimental and simulation results could be due to a few reasons.
13 As MC simulation has certain limitations, including not all the factors such as binding energy
14 of atoms, segregation of elements at the surface are clearly defined for hydrogel. Some
15 estimations were supplemented during the setup phase based on previous reports and data ^{21,}
16 ²². The surfaces of the irradiated hydrogel were roughened as discussed in later sections and
17 contained porous features which may affect the measurements. Some additional effects such as
18 charging during the irradiation of insulated hydrogel as well as redeposition may also have
19 contributed to the variations in simulation ^{21, 22, 32, 33}. The experimentally determined yield of
20 this study ($0.47 \mu\text{m}^3/\text{nC}$), however, is close to the reported yield of Polymethyl methacrylate
21 (PMMA) with the same ion energy ³⁴, and will provide a reference value for future tasks.

22

23 The effect of beam incident angle (angular effects) on yield was also investigated. As a rule
24 of thumb, an inverse cosine rule was typically applied, in which the yield increases by
25 $1/\cos^n(\varphi)$, where φ is the incident angle measured from the normal of the surface. The
26 simulation result reasonably follows the trend with $n \approx 3$, consistent with the published results
27 in literatures ^{22, 35, 36}. Incident angle larger than 62° could not be directly measured due to the
28 restrictions of the currently instrument, thus was not examined in this study. The yield of
29 hydrogel with ions of different acceleration voltage in the keV range was also simulated with
30 SRIM. The results suggested that sputtering yield gradually increased and reached the peak
31 point close to 30 keV. With acceleration voltage approaching 60 keV, the yield of hydrogel
32 started to decrease. This result also agrees with the trends found in previous reports for
33 various materials ^{35, 37}.

34

1 **Surface morphology of irradiated hydrogel**

2 Surface roughness of hydrogel surface prior to and after irradiation was investigated with
3 AFM, with ion fluence ranging from $0.05 \text{ pC}/\mu\text{m}^2$ to $100 \text{ pC}/\mu\text{m}^2$. Two examples of ion
4 fluence at $0.1 \text{ pC}/\mu\text{m}^2$ and $100 \text{ pC}/\mu\text{m}^2$ were presented in Figure 3a and b respectively. For
5 each obtained images, measurements were performed at multiple locations in both pristine
6 and irradiated regions. At ion fluence of $0.1 \text{ pC}/\mu\text{m}^2$, no significant morphological change
7 was observed, and even the original swelling islands on the pristine hydrogel remained
8 unchanged after the irradiation (Figure 3a). In Figure 3b, a dramatic porous pattern were
9 introduced on bottom of the milled cavity after significantly extended irradiation (100
10 $\text{pC}/\mu\text{m}^2$) compared to the smoother pristine surface. Detailed measurements of the surface
11 roughness are presented in Figure 3c including side-by-side comparisons with regard to ion
12 irradiation. It is evident that surface roughness was at least doubled after irradiation; however,
13 the average values remained below 10 nm at initial ion fluences. A surge occurred at ion
14 fluence of $1 \text{ pC}/\mu\text{m}^2$, and average surface roughness was elevated to 20 nm at ion fluence of
15 $100 \text{ pC}/\mu\text{m}^2$. This result suggest that nanoscale roughening occurs since initial radiation,
16 while after achieving a certain threshold, erosion type of morphology becomes the dominant
17 appearance on hydrogel surface.

18

19 Previous reports showed directional patterns on polymers^{18, 35, 38-41}, such as oriented ripples,
20 wrinkles, etc., which are mainly induced by the interplay of sputtering erosion and surface
21 relaxation mechanisms, e.g. surface expansion in the direction perpendicular to the direction
22 of the ion beam³⁹. In addition to surface roughness, these unique patterns and the
23 distributions are also interesting phenomena and were the subjects to investigation with
24 different ion irradiation parameters in this study. Figure 4a and b presented selected AFM
25 images after FIB irradiation at 0 incident angles (normal) on hydrogel, while the incident
26 angle was raised to 50° and 60° incident angles with results presented in Figure 4c-d
27 respectively. A 2D profile of the AFM measurements is presented in Figure 4g to
28 demonstrate the typical cross section. Overall, porous structures were observed across all the
29 irradiated samples, with average diameters in the order of several hundred of nanometers.
30 Contrary to previous reports, no significant orientation was observed in the patterns generated
31 on the hydrogel surface in this study regardless of the ion fluence or incident angle. This may
32 be due to the fact that synthetic hydrogel possesses more heterogeneous structures compared
33 to single-component polymers, and the sputtering yield was varied across the surface to
34 promote the formation of porous structures. Although it is feasible for hydrogel to have the

1 controlled microscale porous morphology for scaffolding⁴, the proposed ion irradiation
2 approach provides unique controllable submicron pores which are challenging for other
3 approaches.

4

5 The patterns measured by AFM were further analysed to obtain the details of the submicron
6 pores. By converting the original AFM data to binary images as shown in Figure 4e-f,
7 porosity, as defined by the percentage of void to overall area, could then be quantified. The
8 measured pore size and porosity at varied ion fluence and incident angles were summarized
9 in Figure 5 a-d. The results showed that the size of the porous patterns was not significantly
10 changed with the increase of ion fluence, and the average pore size and porosity are
11 approximately 600 nm and 0.45 respectively (Figure 5a and c). This also suggests that pore
12 formation requires limited ion fluence even at $1 \text{ pC}/\mu\text{m}^2$, and then with the increase of ion
13 fluence, hydrogel surface underwent uniform erosion with similar porous structures. In
14 comparison, results based on higher incident angle (50 to 60 degree) showed similar porous
15 structures (Figure 4c and d) but with significantly smaller pore size and higher porosity
16 (Figure 5b and d). It is a common practice for ion sputtering at oblique incidence to introduce
17 different morphology for inorganic materials⁴². For the current study, the average
18 implantation depth of the incident gallium ion was reduced at higher incident angles, and the
19 overall transferred kinetic energy is in closer proximity of the top surface layer. This allowed
20 sputtering at top layer to be more effective compared to other dynamic surface mechanisms,
21 and thus resulted in pores of higher density.

22

23 **Modulus of irradiated hydrogel**

24 Mechanical elasticity has been widely accepted as a controllable factor for cell growth and
25 differentiation^{9,43}. Though it is feasible to tune the elasticity of polymers including hydrogel
26 in bulk forms by varying the concentrations⁸, controlled elasticity modification particularly
27 at submicron scale has never been established. Previous studies^{39,44} showed significant
28 higher modulus of PDMS after keV ion irradiation, and in the present study, we also aim to
29 investigate the modulus through FIB irradiation *in situ*. The results measured by AFM force
30 spectroscopy are presented in Figure 6 with ion fluence from $1 \text{ pC}/\mu\text{m}^2$ to $100 \text{ pC}/\mu\text{m}^2$.
31 Compared to pristine hydrogel, the average modulus was significantly elevated with the
32 increase of ion fluence, from less than 20 MPa for pristine hydrogel to 250 MPa at ion
33 fluence $1 \text{ pC}/\mu\text{m}^2$ and 350 MPa at ion fluence $100 \text{ pC}/\mu\text{m}^2$. All the AFM modulus
34 measurements were performed under ambient conditions, and although preferred, measuring

1 modulus of hydrogel in liquid medium remains a challenge, as it is well known that hydrogel
2 response in water is varied. Also in order to accommodate the estimated modulus range of
3 hydrated hydrogel, soft cantilevers with spring constant of 0.03 N/m were initially used in a
4 few attempts, and cantilevers were likely broken at the air-liquid interface, possibly due to
5 surface tension at the air-liquid interface. The fittings based on a few successful
6 measurements suggested that the modulus of hydrated is in the range of 100 kPa to 1 MPa,
7 consistent with the reported hydration induced effects^{45, 46}. The increased water content in
8 the hydrogel may have resulted in larger probe-surface contact area, and the actual
9 relationship of hydration-modulus after ion irradiation will be an interesting topic of future
10 study.

11

12 It is interesting to note that site specific modulus tuning of post-crosslinking hydrogel
13 accomplished in this study has not been feasible with other existing approached. Although
14 focused electron beam was deployed for localized crosslinking of hydrogel^{47, 48}, the
15 fabricated features were attached to substrate such as silicon and was not applicable for tissue
16 engineering. Swelling effect of the electron patterned hydrogel was reported, but so far no
17 details on modulus were provided. In the current study, nuclear stopping of the gallium ions
18 is expected to be dominant in conjunction with the MC simulation results, and that causes
19 substantial nuclear displacements and scission of bonds in the target hydrogel. A transition
20 from one-dimensional chains into a three-dimensional matrix may provide the explanation for
21 the elevated Young's modulus^{49, 50}, although a more conclusive study is needed in the future.

22

23

24 **Results of cell culture on patterned hydrogel**

25 To assess the stability of the generated patterns, ion irradiated samples were kept in
26 physiological environment for 48 hrs, i.e. with the same culture medium and temperature but
27 without seeding cells. After dehydration, the samples were finally investigated with both
28 optical and SEM imaging (Figure 7a-b), and the original FIB milled patterns were clearly
29 present without noticeable changes. This suggests that the FIB milled patterns are stable in
30 cell culture environment, at least prior to the controlled dissolution of hydrogel. Although
31 increased roughness after ion irradiation resulted in larger contact surface area, hardening of
32 the top layer as shown by the increased modulus may provide additional barrier against
33 physical and chemical modifications of the patterns.

1 To demonstrate the biocompatibility of FIB patterning on hydrogel, cell culture experiment
2 was performed on the irradiated samples. Optical images recorded right after seeding and at
3 44 hrs after seeding are presented in Figure 7c-f. For both irradiated and non-irradiated
4 samples, the COS-7 cells reached confluence, and displayed typical spread out morphology.
5 The same morphology was observed in the 10 μm ion irradiated square regions (Figure 7d)
6 compared to the cells grown on the irradiated hydrogel surface. In addition, confocal
7 microscopy was performed to provide higher magnification investigations, with results
8 presented in Figure 7g-h. It is clear that, for both irradiated and non-irradiated samples,
9 COS-7 cells were firmly adhered to hydrogel, a scenario consistent with this type of hydrogel
10 in the literature⁴. For the cells grown on the rectangle patterned regions as shown in Figure
11 7h, no measurable difference in morphology was found. The viability of these cells was
12 confirmed by the consistent green fluorescent color, without the presence of any dead cells.
13 These results confirmed that gallium ion beam irradiation has negligible effects on cell
14 growth, although gallium is generally considered as toxic^{51,52}. From SRIM results, majority
15 of the incident gallium will be eventually implanted in the target hydrogel, and possible
16 source of the toxicity, the free gallium ions, are expected to be minimal on the hydrogel
17 surface. It can also be inferred that patterns generated by other commercial available FIB
18 sources based on noble gases such as Helium, Neon, etc. will likely be biocompatible,
19 although additional studies will be preferred to confirm it. The results of both experiments
20 presented above proved the stability and compatibility of these nano/micro scale patterns on
21 hydrogel, and paved road towards various bioapplications.

22 **Conclusion**

23 In conclusion, Focused Ion Beam milling was performed on the thin films of hydrogels to
24 tune various surface properties including surface morphology and modulus, characterized by
25 electron microscopy and AFM. The sputtering yield of hydrogel by keV gallium ion was
26 examined experimentally and compared to results obtained from Monte-Carlo simulation. It
27 was revealed that the surface roughness was doubled after low dose irradiation, and
28 significant increase of Young's modulus was also confirmed. During irradiation, unique
29 nanoscale porous features in regular formation were also observed, and the pore parameters
30 are subjects of ion incident angles. Cell culture experiments confirmed the biocompatibility
31 and stability of the patterns generated based on FIB with gallium sources. Given the *in situ*
32 high precision capability and sufficient yield compared to laser and electron beam based

1 approaches, we expect the proposed approach will provide tunable submicron features on
2 hydrogel which are unique for future research in tissue engineering and biosensing.

3

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10

1 **References**

- 2 1. J. Kopeček, *Biomaterials*, 2007, **28**, 5185-5192.
- 3 2. A. C. Jen, M. C. Wake and A. G. Mikos, *Biotechnology and Bioengineering*, 1996, **50**, 357-364.
- 4 3. Q. Liu, E. L. Hedberg, Z. Liu, R. Bahulekar, R. K. Meszlenyi and A. G. Mikos, *Biomaterials*, 2000,
5 **21**, 2163-2169.
- 6 4. A. Al-Abboodi, J. Fu, P. M. Doran, T. T. Tan and P. P. Chan, *Advanced healthcare materials*,
7 2013.
- 8 5. S. J. Bryant, J. L. Cuy, K. D. Hauch and B. D. Ratner, *Biomaterials*, 2007, **28**, 2978-2986.
- 9 6. S. P. Hoo, Q. L. Loh, Z. Yue, J. Fu, T. T. Y. Tan, C. Choong and P. P. Y. Chan, *Journal of*
10 *Materials Chemistry B*, 2013, **1**, 3107-3117.
- 11 7. J.-y. Lin, W.-j. Lin, W.-h. Hong, W.-c. Hung, S. H. Nowotarski, S. M. Gouveia, I. Cristo and K.-h.
12 Lin, *Soft Matter*, 2011, **7**, 10010-10016.
- 13 8. J. R. Tse and A. J. Engler, *Current protocols in cell biology*, 2010, 10.16. 11-10.16. 16.
- 14 9. A. J. Engler, S. Sen, H. L. Sweeney and D. E. Discher, *Cell*, 2006, **126**, 677-689.
- 15 10. F. Boccafoschi, Rasponi, M., Mosca, C., Bocchi, E., Vesentini, S., *Advanced Materials*, 2012,
16 **409**, 109-110.
- 17 11. Z. Pan, C. Yan, R. Peng, Y. Zhao, Y. He and J. Ding, *Biomaterials*, 2012, **33**, 1730-1735.
- 18 12. M. M. Stevens and J. H. George, *Science*, 2005, **310**, 1135-1138.
- 19 13. W. Chen, L. G. Villa-Diaz, Y. Sun, S. Weng, J. K. Kim, R. H. W. Lam, L. Han, R. Fan, P. H.
20 Krebsbach and J. Fu, *ACS Nano*, 2012, **6**, 4094-4103.
- 21 14. L. Csaderova, E. Martines, K. Seunarine, N. Gadegaard, C. D. W. Wilkinson and M. O. Riehle,
22 *Small*, 2010, **6**, 2755-2761.
- 23 15. E. K. F. Yim, E. M. Darling, K. Kulangara, F. Guilak and K. W. Leong, *Biomaterials*, 2010, **31**,
24 1299-1306.
- 25 16. P. Kim, W. E. Adorno-Martinez, M. Khan and J. Aizenberg, *Nat. Protocols*, 2012, **7**, 311-327.
- 26 17. Y. Zhang, E. A. Matsumoto, A. Peter, P.-C. Lin, R. D. Kamien and S. Yang, *Nano Letters*, 2008,
27 **8**, 1192-1196.
- 28 18. M.-W. Moon, S. H. Lee, J.-Y. Sun, K. H. Oh, A. Vaziri and J. W. Hutchinson, *Scripta Materialia*,
29 2007, **57**, 747-750.
- 30 19. T. Kaito, in *Introduction to Focused Ion Beams*, eds. L. Giannuzzi and F. Stevie, Springer US,
31 2005, ch. 4, pp. 73-86.
- 32 20. K. M. Lee, A. Neogi, J. M. Perez and T. Y. Choi, *Nanotechnology*, 2010, **21**, 205303.
- 33 21. J. J. L. Mulders, D. A. M. de Winter and W. J. H. C. P. Duinkerken, *Microelectronic Engineering*,
34 2007, **84**, 1540-1543.
- 35 22. H. Ostadi, K. Jiang and P. D. Prewett, *Microelectronic Engineering*, 2009, **85**, 1021-1024.
- 36 23. M. Serantoni, A. S. Sarac and D. Sutton, *Surface and Coatings Technology*, 2005, **194**, 36-41.
- 37 24. F. A. Stevie, L. A. Giannuzzi and B. I. Prenitzer, in *Introduction to Focused Ion Beams*, eds. L.
38 Giannuzzi and F. Stevie, Springer US, 2005, ch. 1, pp. 1-12.
- 39 25. A. Gaston, A. Z. Khokhar, L. Bilbao, V. Sáez-Martínez, A. Corres, I. Obieta and N. Gadegaard,
40 *Microelectronic Engineering*, 2010, **87**, 1057-1061.
- 41 26. A. Al-Abboodi, J. Fu, P. M. Doran and P. P. Y. Chan, *Biotechnology and bioengineering*, 2012,
42 **110**, 318-326.
- 43 27. F. Boccafoschi, M. Rasponi, C. Mosca, E. Bocchi and S. Vesntini, *Advanced materials research*,
44 2012, **409**, 105-110.
- 45 28. G. E. Murphy, K. Narayan, B. C. Lowekamp, L. M. Hartnell, J. A. Heymann, J. Fu and S.
46 Subramaniam, *Journal of structural biology*, 2011, **176**, 268-278.
- 47 29. J. A. Heymann, D. Shi, S. Kim, D. Bliss, J. L. Milne and S. Subramaniam, *Journal of structural*
48 *biology*, 2009, **166**, 1-7.
- 49 30. B. Liu, H. H. Yu, T. W. Ng, D. L. Paterson, T. Velkov, J. Li and J. Fu, *Microscopy and*
50 *Microanalysis*, 2014, **20**, 537-547.
- 51 31. SRIM - The Stopping and Range of Ions in Matter, www.srim.org, 2014.

- 1 32. P. J. Cumpson, J. F. Portoles, A. J. Barlow, N. Sano and M. Birch, *Surface and Interface*
2 *Analysis*, 2013, **45**, 1859-1868.
- 3 33. R. D. Kolasinski, J. E. Polk, D. Goebel and L. K. Johnson, *Journal of Vacuum Science &*
4 *Technology A: Vacuum, Surfaces, and Films*, 2007, **25**, 236.
- 5 34. F. C. FEI Company, *Operation manual of dual beam system*, 2014.
- 6 35. J. Muñoz-García, L. Vázquez, R. Cuerno, J. Sánchez-García, M. Castro and R. Gago, in *Toward*
7 *Functional Nanomaterials*, ed. Z. M. Wang, Springer US, 2009, vol. 5, ch. 10, pp. 323-398.
- 8 36. J. Fu, S. B. Joshi and J. M. Catchmark, *Journal of micromechanics and microengineering*, 2008,
9 **18**, 095010.
- 10 37. J. Fu, S. B. Joshi and J. M. Catchmark, *Journal of Vacuum Science & Technology A: Vacuum,*
11 *Surfaces, and Films*, 2008, **26**, 422-429.
- 12 38. M. Guvendiren and J. A. Burdick, *Biomaterials*, 2010, **31**, 6511-6518.
- 13 39. M.-W. Moon, S. H. Lee, J.-Y. Sun, K. H. Oh, A. Vaziri and J. W. Hutchinson, *Proceedings of the*
14 *National Academy of Sciences*, 2007, **104**, 1130-1133.
- 15 40. C. O. Yang, E. K. Her, K. H. Oh and T. J. Kang, *Journal of Korean Physical Society*, 2012, **61**,
16 297-300.
- 17 41. J. Yin and C. Lu, *Soft Matter*, 2012, **8**, 6528.
- 18 42. B. Ziberi, F. Frost, B. Rauschenbach and T. Höche, *Applied Physics Letters*, 2005, **87**, -.
- 19 43. D. E. Discher, P. Janmey and Y.-I. Wang, *Science*, 2005, **310**, 1139-1143.
- 20 44. C. E. Foerster, I. T. S. Garcia, F. C. Zawislak, F. C. Serbena, C. M. Lepienski, W. H. Schreiner
21 and M. Abbate, *Thin Solid Films*, 2002, **411**, 256-261.
- 22 45. R. A. Frazier, M. C. Davies, G. Matthijs, C. J. Roberts, E. Schacht, S. J. B. Tendler and P. M.
23 Williams, *Langmuir*, 1997, **13**, 4795-4798.
- 24 46. M. Radmacher, M. Fritz and P. K. Hansma, *Biophysical Journal*, 1995, **69**, 264-270.
- 25 47. P. Krsko, S. Sukhishvili, M. Mansfield, R. Clancy and M. Libera, *Langmuir*, 2003, **19**, 5618-
26 5625.
- 27 48. Y. Hong, P. Krsko and M. Libera, *Langmuir*, 2004, **20**, 11123-11126.
- 28 49. J. Jagielski, A. Turos, D. Bielinski, A. M. Abdul-Kader and A. Piatkowska, *Nuclear Instruments*
29 *and Methods in Physics Research Section B: Beam Interactions with Materials and Atoms*,
30 2007, **261**, 690-693.
- 31 50. R. L. Clough, *Nuclear Instruments and Methods in Physics Research Section B: Beam*
32 *Interactions with Materials and Atoms*, 2001, **185**, 8-33.
- 33 51. M. M. Hart and R. H. Adamson, *Proceedings of the National Academy of Sciences*, 1971, **68**,
34 1623-1626.
- 35 52. F. C. FEI Company, *Masterial Safety Data Sheet Gallium*.

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