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34 **Introduction**

35 Nanostructured materials have much attention role in many biology related 36 applications and advanced nanodevices in recent day scenario of bio-nanotechnology. 37 The assembly of nanostructures across several length-scales is also of paramount 38 importance in the synthesis of organized materials with advanced functions. Chitosan, a 39 natural based-polymer obtained by alkaline deacetylation of chitin, is nontoxic, 40 biocompatible, and biodegradable. Owing to its properties, chitosan can be used in 41 medicine, pharmacy, biotechnology, agriculture, biodegradability, biocompatibility, and 42 antimicrobial activity and the food industry¹⁻⁴. The polycationic biopolymer is receiving a 43 great deal of attention for biosensing, medical, and pharmaceutical applications $5-7$ and it 44 is the most commonly used natural polymer in regenerative medicine and tissue 45 engineering ⁸. Chitosan micro- or nanofibers have been widely accepted as biomedical 46 scaffolding materials to restore, maintain, or improve the functions of various tissues $9-10$. 47 Therefore, the creation of chitosan nanostructures with controllable morphology is highly 48 desirable, but has met with limited success yet. However, one elegant method, 49 electrospinning, has been reported for producing chitosan nanofibers. Because of their 50 biocompatibility and biodegradability, the resulting chitosan nanostructures can be 51 potentially tailored to mimic a natural extracellular matrix, to achieve controlled drug 52 delivery, and to develop tissue-compatible scaffolds for tissue cultures. Thus, derived 53 chitosan possesses many useful biological properties such as biocompatibility, 54 biodegradation, woundhealing and anti-bacterial action $1, 11$ -13. Therefore, much attention 55 has been paid to develop chitosan-based biomedical materials. Chemical modification of

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56 chitosan is useful for the association of bioactive molecules to polymer and controlling 57 the drug release profile.

58 In this study, the nanostructure mechanical property, and biocompatibility of the 59 novel chitosan/16-DPA particles were evaluated. It has been widely used in pharmaceutical 60 research and in industry as a carrier for drug delivery and as biomedical material 14 . Chitosan was 61 selected for nanoparticles because of its recognized mucoadhesivity and ability to enhance the 62 penetration of large molecules across mucosal surface 15 .

63 Our effort has been concentrated to synthesized hybrid nanoparticles using a 64 convenient one-pot method and by literature survey no work has been reported, 65 particularly 16-Dehydropregnenolone Acetate. Significantly, our results show that a 66 polymer of single composition and short length could contribute to the growth of highly 67 anisotropic structures. Such an anisotropic aggregation is most likely due to the 68 nonuniform distribution of capping agents on the steroid nanoparticle amorphous 69 surfaces. The aim of the present investigation has been describe the synthesis and 70 characterization of novel biodegradable nanoparticles based on chitosan for encapsulation 71 of 16-DPA and the product has screened for antifungal activity against the fungus 72 *Colletotrichum gleosporioides.* The drug loading capacity (LC), encapsulation efficiency 73 (EE) and drug release study were investigated using UV spectrophotometer.

74 **2. Materials and methods**

75 *2.1. Materials and chemicals*

76 Chitosan (CH) (MW 2.4 $x10^6$), 16-dehydropregnanolone acetate (16-DPA), N, N-77 dicyclo-hexyl carbodiimide (DCC) and 4-dimethyl amino pyridine (DMAP) were 78 purchased from Sigma-Aldrich and used directly without purification. Acetonitrile, ethyl 79 acetate, methanol, NaCl, Na2HPO4 and KH2PO4 were purchased from CDH analytical

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80 grade and only distilled solvents were used for the reactions. Triple distilled $H₂0$ was 81 used for preparation of the solutions.

- 82 *2.2. Methodology*
- 83 *2.2.1. Synthesis of Chitosan-16-DPA nanoparticles*

84 A solution of 16-DPA (100 mg) in MeOH (60 ml) was stirred for 10 min. at room 85 temperature and 25 ml of 1% chitosan solution was added slowly. A solution of DCC 86 (100 mg) in MeOH (5 ml) was added and after that DMAP (300 mg) in MeOH (5 ml) 87 was added to catalyze the reaction system 16 . The reaction mixture was stirred for 24 hrs 88 at room temperature. In order to enhance the precipitation of the by-products the resulting 89 suspension was treated with acetonitrile (30 ml). The resulting solution was filtered and 90 the filtrate was evaporated under reduced pressure to get the product. After that the 91 product was redissolved in ethyl acetate (50 ml) and discard the undissolved by-products 92 by filtration. Ethyl acetate was evaporated under reduced pressure to get the final 93 required product. Purified the product by washing with MeOH and finally white 94 crystalline solid products was formed.

95 *2.2.2. General Methods*

96 Melting points were measured with a Buchi B-540 melting point apparatus and 97 are uncorrected. The progress of each of the reaction was monitored on Merck thin layer 98 chromatography silica gel 60 F254. IR spectra were recorded with a Perkin-Elmer model 99 2000 series FT-IR spectrometer for solutions in chloroform. Infrared absorbance is 100 reported in reciprocal centimeters cm^{-1}). ¹H and ¹³C NMR spectra were recorded on a 101 Bruker DPX (300 MHz) spectrometer using CDCl₃ or DMSO- d_6 as solvent with 102 tetramethylsilane (TMS) as internal standard on ppm scale (δ). Multiplicity of the

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103 resonance peaks are indicated as singlet (s), broad singlet (bs), doublet (d), triplet (t), 104 quartet (q) and multiplet (m). The surface morphologies were examined by using a 105 Scanning Electron Microscopy (SEM; JSM-35, JEOL, Japan). The particles were made 106 conductive by sputter-coating with palladium prior to SEM analysis. The particle size of 107 the polymeric aggregates was observed using a TEM (JEM-2000 FX II, JEOL, Japan). A 108 drop of the product suspension was placed on a copper grid coated with carbon film, 109 dried at 25 $\mathrm{^{0}C}$ and observation was performed at 80 kV.

110 2.2.3. *In vitro* antifungal activity

111 2.2.3.1. Fungus and media

112 The antifungal activity of the new modified chitosan (CHDPA) was studied 113 against the fungus *Colletotrichum gleosporioides.*

114 The inhibitory effects of the samples were tested in vitro on mycelia growth of *Alternaria alternata*. Poisoned Food technique¹⁷⁻¹⁸ was used to test the antifungal activity 116 of the sample. Samples were used at concentrations of 100, 200, 300, 400 and 500 ppm. 117 Petriplates (90 mm dia.) each containing 20 ml of potato dextrose agar (PDA) medium 118 amended with the desired concentrations of samples were inoculated with test fungus. A 119 5 mm diameter disc of the test fungus with a corkborer, cut from the periphery of an 120 actively growing 8 -days old culture on PDA plates and was placed at the center in each 121 treated petriplate PDA plates without sample served as control, which consist of 100, 122 200, 300, 400 and 500 ppm of the solvent. The experiments were conducted with three 123 replications. Then plates were kept in incubator at temp. $25 \pm 1^{\circ}$ C. Fungal growth was 124 observed at every 24 hrs. interval. At the end of the incubation period, after 72 hrs. the 125 minimum inhibitory concentration (MIC) that caused complete inhibition of the mycelia

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126 growth was measured. The percentage of inhibition of mycelial growth was calculated

127 from mean values of colony diameter in treated and control petridishes using the 128 following formula 18 . 129 Inhibition $\% = 100$ (Control-Treatment) / Control 130 *2.2.4. Phosphate Buffer Saline pH 7.4* Phosphate buffered saline is a buffer solution commonly used in biological research¹⁹. 132 1 liter stock of 10x PBS was prepared by dissolving 8 g NaCl, 1.44 g Na₂HPO₄ and 0.24 133 g KH₂PO₄ in 800 ml of distilled water, and topping up to 1 Lit. The pH is ~6.8, but when 134 diluted to 1x PBS it should change to 7.4. 135 *2.2.5. Standard graph for Drug content* 136 137 Stock solution was prepared¹⁹ by dissolving DPA (10 mg) in suitable solvent or 138 buffer (1ml solvent+9 ml buffer) and 1 ml of mixture from the stock solution was diluted 139 with 9 ml of phosphate buffer saline pH 7.4 which is used as a standard solution. Aliquots 140 of standard solution were further diluted with phosphate buffer saline pH 7.4 to get 141 working solution of 5, 10, 15, 20 and 25 µg/ml. The working standards were scanned 142 using UV spectrophotometer which shows the maximum absorbance at lambda max. The 143 same λ max was used for the further measurement of the drug. Finally, the prepared 144 standards were measured, in each case against a solvent blank similarly prepared and 145 calibration the graphs of the absorbance *versus* the concentration of the drug was plotted. 146 *2.2.6. Determination of DPA Loading Capacity (LC) & Encapsulation Efficiency (EE)* 147 148 Proper amounts of product were mechanically ground in a mortar with a pestle. 149 About 5 mg of the product were placed into a 10 ml standard flask with a cap and add 10 150 ml of suitable solvent. After the mixture in the flask was broken up by ultrasonication for

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151 30 min, the flask was capped and shaked for 24 h at room temperature. Finally, the 152 mixture was transferred into a 25 mL flask and diluted to 25 mL with solvent. The 153 suspension was filtered through a 0.45 µm membrane. The concentration of drug in the 154 filtered solution was measured at wavelength of lamda max¹⁹.

155 The recovery of the product (final product amount) was defined as the weight 156 ratio of dried product to the initial loadings of polymer and drug. The dried product was 157 dissolved in acetonitrile, sonicated for 5min and then distilled water was added to 158 precipitate the polymer preferentially. The drug content in the supernatant after 159 centrifugation (15,000 for 15min) was measured spectrophotometrically at particular 160 lambda max for each drug by Ultra Violet spectroscopy (UV). The product recovery, 161 drug loading capacity and encapsulation in the product were calculated using the 162 following equations¹⁹.

Percentage of Nanoparticle Recovery

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167 *2.2.7. DPA Release Study* 168

169 For *DPA* release, weighed polymeric nanoparticles were suspended in 2 ml 170 phosphate buffer saline pH 7.4 was placed in sigma dialysis tubing. The tube containing 171 dispersion of polymeric nanoparticles was then introduced into a 200 ml beaker 172 containing 100 ml release media (phosphate buffer pH 7.4), which was stirred at 400 + 20 173 rpm using magnetic stirrer. Drug release was assessed by intermittently sampling the 174 receptor media (5ml) at predetermined time intervals each time the 5 ml of fresh 175 phosphate buffer saline pH 7.4 was replaced. The amount of drug release in the buffer 176 solution was quantified by a UV spectrophotometer at lambda $max¹⁹$.

177 **3. Results and Discussions**

178 3.1. *Chemistry*

179 *3.1.1. UV Studies*

180 UV-spectra of chitosan shows a sharp prominent peak at 190 nm and for 16-DPA, 181 it shows the prominent band at 246 nm. In case of CHDPA product, it shows the peak at 182 259 nm. After conjugation reaction the shifted signal, indicating the formation of the new 183 ketimine bond shown in Figure 1.

184 *3.1.2. Chitosan (CH)*

185 186

The FT-IR spectra of chitosan (CH) spectra shows characteristic band at 2920 cm-187 188 ¹ to 3378 cm⁻¹ corresponds to N-H stretching with hydrogen bonded amino groups, 1726 189 cm⁻¹ peak is assigned to the C-O stretching (C=O in carboxylic acid), 1612 cm⁻¹ is due to 190 amide I group (C-O stretching along with N-H deformation mode), 1560 cm^{-1} peak is 191 attributed to the NH₂ group due to N-H deformation, 1460 cm⁻¹ is assigned to the

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192 symmetrical deformation of CH₃ and CH₂ group, 1425 cm^{-1} peak is due to C-N axial 193 deformation (amine group band), 1384 cm⁻¹ peak is due to COO- group in carboxylic 194 acid salt, 1196 cm⁻¹ is assigned to the special broad peak of β (1-4) glycosides band in 195 polysaccharide unit, 1108 cm^{-1} is attributed to the stretching vibration mode of the 196 hydroxyl group, 1020 cm⁻¹ stretching vibration of C-O-C in glucose circle and 1060-1015 197 cm^{-1} bands corresponds to CH-OH in cyclic compounds $^{20-21}$. Band between at 590 to 770 198 due to O-C=O in carboxylic acid due to preparation of CS solution in acetate buffer 199 solution. The absorption band at 1650 cm⁻¹ was attributed to the carbonyl of $O=C-NHR$ 200 of chitosan ²² and the absorption band at 1599 cm⁻¹ was assigned to the amino groups of 201 chitosan with high deacetylation degrees. This signal shifted to 1528 cm^{-1} after the 202 conjugation reaction, indicating the formation of new amide bonds by acylation of amino 203 groups of chitosan. A weak shoulder peak occurred at 1738 cm^{-1} assigned to the carbonyl 204 of ester bond of CS shown in Figure 2.

205 The ¹H NMR spectrum of chitosan shows the chemical shifts of the protons 206 appears at 4.58 ppm for acetal proton (-CH) of the glucosamine, 3.01 ppm for -CH-NH2, 207 3.75 ppm for -CH-OH, 3.59 ppm for -CH2-OH and 1.94 ppm for acetamido protons 208 (-NH-CO-CH3).

209 The ¹³C NMR spectra of chitosan shows : δ 98.3(C-1), 56.9(C-2), 70.9(C-3), 210 78.0(C-4), 75.7(C-5), 61.4(C-6).

211 3.1.3.*16- Dehydropregnenolone Acetate (16-DPA)*

212 ¹H NMR (CDCl₃): 1.0 (s, 3H, Me-19), 1.1 (s, 3H, Me-18), 1.3–2.2 (m, –CH and 213 –CH2), 2.0 (s, acetate proton), 2.3 (s. methyl ketone proton), 4.6 (m, 1H, C-3 Proton 214 under acetate), 5.3 (m, 1H,C-6 olefinic proton), 6.7 (m, 1H, 16-vinyl hydrogen); ¹³C NMR 215 (CDCl₃): δ 31.5(C-1), 32.2(C-2), 76.6 (C-3), 46.0(C-4), 144.4(C-5), 121.9(C-6), 30.1(C-216 7), 31.5(C-8), 50.3.0(C-9), 38.1(C-10), 20.6(C-11), 27.7(C-12), 36.7(C-13), 36.8 (C-14), 217 31.5(C-15), 140.2(C-16), 144.4(C-17), 196.8(C-18), 19.2(C-19), 20.6(C-20), 21.4(C-21), 218 15.7 (C–CH3COO), 170.5 (C–C=O); IR (CHCl3) : 2933, 2851, 1732, 1666, 1435, 219 1245 cm^{-1} ²³.

220 3.1.4. *Chitosan – 16*-*dehydropregnanolone acetate ketimine Product*

221 IR spectra of Chitosan- dehydropregnanolone acetate ketimine Product shows 222 peaks at 3394 (br) cm⁻¹ for –OH stretching, 2929 and 2852 cm⁻¹ for C-H stretching, 1702 223 cm⁻¹ for C-O stretching of the acetyl group (amide II), 1649 cm⁻¹ corresponds to C=N 224 stretching (ketimine), N-H deformation (NH₂) peak is shifted to 1564 cm⁻¹, 1406 cm⁻¹ for 225 asymmetric C-H bending of CH₂ group and 1605 cm^{-1} for CO-bridge stretching of 226 glucosamine residue.

227 The ¹H NMR spectrum revealed the signals at δ 3.2 for –NHCO- group, at 1.1 for 228 -NH- group, 4.6 (s-br, for H-1) of chitosan and 3.2–3.5 (s-sh, br, H-2, H-3, H-4, H-5 & 6) 229 for CH2OH the peak at 2.4 (s-sh), 1.0 (s, 3H, H-18), 1.3 (s, 3H, H-19), 7.2 (16-vinyl 230 hydrogen), 4.5 (s, 3H, methyl ketone).

231 In¹³C NMR of the product shows some new peaks at δ 49.8 (C-N-C), 176.5 (- 232 C=N-, ketimine) and 71.4 (CH₂OH) with other peaks of the steroid and chitosan part.

233 3.1.5. *SEM and TEM Analysis*

234 The general morphology of the product was investigated by SEM images. Figures 235 3a and b showed representative images of the nano rods with the image size 30-50 μ m. 236 Moreover, the latter shows that the particles are aggregates consisting of much smaller 237 amorphous particles growing and has very small (300-500 nm) amorphous particles

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238 comprise high surface. On the other hand, these particles are already amorphous, which 239 makes them sufficiently stable in a system different from the starting one, they used to 240 grow^7 . The presence of both, single isolated amorphous particles and complex 241 aggregates, suggests that the growth process is promoted by two types of nanoparticles: 242 (i) a single isolated bred released from the aggregates and (ii) complex aggregates 243 comprising large number of single bred-nuclei.

244 The detailed microstructure of product CHDPA nanorods was further investigated 245 by TEM images. The examination of the amorphous products shows that a great part of 246 material is in the form of random aggregates 24 and the structure, self-aggregate behavior 247 etc of CHDPA were shows in the TEM photographs in Figure 4a and b. The shapes of 248 CHDPA nanoparticles observed were mostly spherical and cubical. The diameters of the 249 nanoparticles were 300-500 nm.

250 Nevertheless, abundant intergrowth was observed in the products and the number 251 of isolated well-shaped amorphous was limited. The most likely origin for the abundant 252 intergrowth is the presence of nanoparticles, which are governing the growth in the 253 system. The drawing in Figure 4a and b, supported by TEM images, represents the two 254 types of particles. The domination of the aggregates in the product is in good agreement 255 with the above suggestion. The mass of aggregated nanoparticles growing into 256 amorphous is much higher than that of single bred nuclei. The low number of single 257 isolated structure can be explained by either limited breeding or by the released bred 258 nuclei staying in close proximity of parent aggregate and thus their development into 259 amorphous results in complex aggregates. Therefore, the formation of nanoparticles with

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260 narrow particle size distribution cannot be expected if the growth in the system is 261 promoted by complex aggregates, even being with nanometric size.

262 3.2. *Biology*

263 The synthesized compound showed in good antifungal activity in general. The 264 data and the experimental photographs are given in Table 1 and Figure 5(E1-E5).

265 The antifungal activity of the new modified chitosan (CHDPA) was studied 266 against the fungus *Colletotrichum gleosporioides.* The inhibitory effects of the samples 267 were tested in vitro on mycelia growth of *Colletotrichum gleosporioides* using Poisoned 268 Food technique with the five concentrations of 100, 200, 300, 400 and 500 ppm. Data 269 reveals that with increasing the concentration, inhibition percentage also increases.

270 *3.3. DPA Loading Capacity (LC), Encapsulation Efficiency (EE) and DPA Release study*

271 272 The synthesized products showed in good Drug loading capacity (LC) ie. 23.2% 273 and encapsulation efficiency (EE) 20.9% respectively, which has been given in Table 2. 274 And also showed the good release behavior described by the Figure 6.

275

276 **4. Conclusion**

277 In this contribution, we successfully utilized chitosan, a biocompatible polymer 278 and steroid to synthesis chitosan-16-DPA nanoparticle linear aggregates. The chitosan 279 employed herein, not only served as the reducing agent and stabilizer, but also led to the 280 assembly of chitosan-16-DPA nanoparticles. TEM images and UV- spectra confirmed the 281 existence of the nanoparticle linear aggregates in solution. One could obtain highly 282 branched long chains and isolated short chains by adjusting the molar ratio of the 283 chitosan repeat unit to 16-DPA. Moreover, the process of growth and assembly for the

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284 chitosan-16-DPA nanoparticle was studied by SEM. This method provides a novel way 285 to fabricate chitosan-16-DPA nanoparticle linear aggregates by virtue of its one-pot 286 simplicity and chain-length tunability. From the analyzed result, compound was found to 287 be the most promising antifungal activities against the fungus *Colletotrichum* 288 *gleosporioides.* The drug loading capacity (LC) was found to be 23.2% and encapsulation 289 efficiency (EE) was 20.9% respectively. The drug release study was investigated using 290 UV spectrophotometer and shown in good result.

291

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List of Table, Schemes, Figures have been given below.

403 **Table 1 : The Inhibitory effects of the samples on mycelia growth of C and 7 days** 404 **after inoculation (percent inhibition).**

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407

408

409

410 **Table 2 : Effect of percent of drug loading capacity (LC) and encapsulation** efficiency (EE) of Chitosan-16DPA. 412

413

416 **Scheme 1 : Schematic representation of reaction mechanism for Chitosan-16-DPA.**

437

438 **Figure 2 : FT-IR spectra (A) Chitosan and (B) (a) 16-DPA (b) Chitosan-16-DPA.**

Figure 3 : SEM Photographs of Chitosan-16DPA.

