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Amperometric sensing of urea using edge activated Graphene Nanoplatelets

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ABSTRACT

Sensing of urea is the key component in the diagnosis of kidney related diseases and milk adulteration. Till now the methods developed for urea sensing are not easy to perform, and very little attention has been paid to commercialization of such sensors. Herein, we first time report the low cost Graphene nanoplatelets (GNPLts) based sensing platform for urea. Specifically edge functionalized GNPLts are used for keeping graphitic activity of graphene planes intact. We have successfully sensed variable ranges of urea concentrations from 0.1-0.8mg/ml. The amperometric characterization showed a linear variation in current as a function of urea concentration. The developed platform has a rapid response time of 15 sec with good sensitivity ($33 \mu\text{A} (\text{mg ml}^{-1})^{-1}$) and specificity. This developed nanoplatform could be highly beneficial for the development of ultrasensitive, disposable, routine use sensor for urea.

Keywords: Graphene nanoplatelets, Amperometric sensing, Nanoprobe, Urease, Urea.

1. Introduction

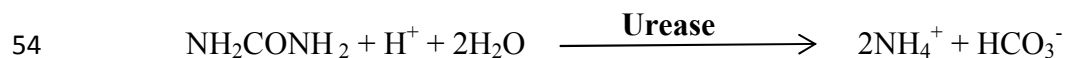
Urea is an organic compound present in milk and urine of mammals and is synthesized from the metabolism of nitrogen containing compounds like proteins, etc. Presence of high concentration of urea in the body is a major indicator of kidney failure. On the other hand, urea is also a main adulterant of milk and any change in the urea concentration (lower or higher) in milk is a symbol of adulteration^{1,2,3}. The allowable range of urea in milk is 0.2 to 0.4 mg/ml and any

29 deviation from this concentration reports the milk as adulterated⁴. Therefore, the development of
30 urea sensing platform with good accuracy and precision is of utmost importance. Till now
31 enzyme coupled, Infrared (IR) spectroscopy, pH, amperometric, flow injection and fiber optics
32 based methods are developed for urea sensing but all these techniques are not easy to perform in
33 meager instrumental facilities^{5,6,7}. At the same time, commercial viability of these techniques is
34 also very low. With the increasing commercialization of milk products, parameterization and
35 standardization of milk is essential, thus there is a need to develop efficient urea sensors. In
36 addition, urea sensing is also needed for the diagnosis of kidney related diseases. Exploiting new
37 materials like graphene, which has been reported highly efficient for ballistic conductance and
38 amperometric sensing can give a unique platform for sensitive and specific sensors.

39 This article is focused on sensing of urea by employing urease conjugated graphene
40 nanoplatelets (GNPLts). Like graphene, GNPLts are also extraordinary in their chemical and
41 physical properties, but have short stacks of sheets and platelets like morphology. GNPLts show
42 superiority over other porous materials as the surface area of GNPLts is very less affected by the
43 pore distribution^{8,9,10}. Rather, porosity provides high surface for electrolyte movement even on
44 agglomeration as the ions still manage to migrate through interstices to access the GNPLts surface
45^{11, 12}. This property of GNPLts makes them excellent candidate for development of
46 electrochemical sensors. The edge functionalization of GNPLts can further improve sensing
47 strategy because it preserves the graphitic nature of basal plane and due to repulsion among
48 functional groups on the edges they tends to self-exfoliate, resulting in high quality GNPLts films
49¹³. Such sensing platforms made up of GNPLts used in this work will be further beneficial for the
50 economy and commercialization.

51 Urease is an enzyme, which causes hydrolysis of urea. The hydrolysis results in generation of
52 ammonium (NH_4^+) and carbonic ions (HCO_3^-)^{14,15}.

53



55 The main purpose of this research is to efficiently sense the ions, produced during hydrolysis of
56 urea. The GNPLts were edge functionalized with urease to improve sensitivity. Conjugation of
57 urease was done via EDC-NHS coupling and the activity of conjugated GNPLts-urease is tested
58 by conducting indothymol and pH based study. The developed platform has been transferred on

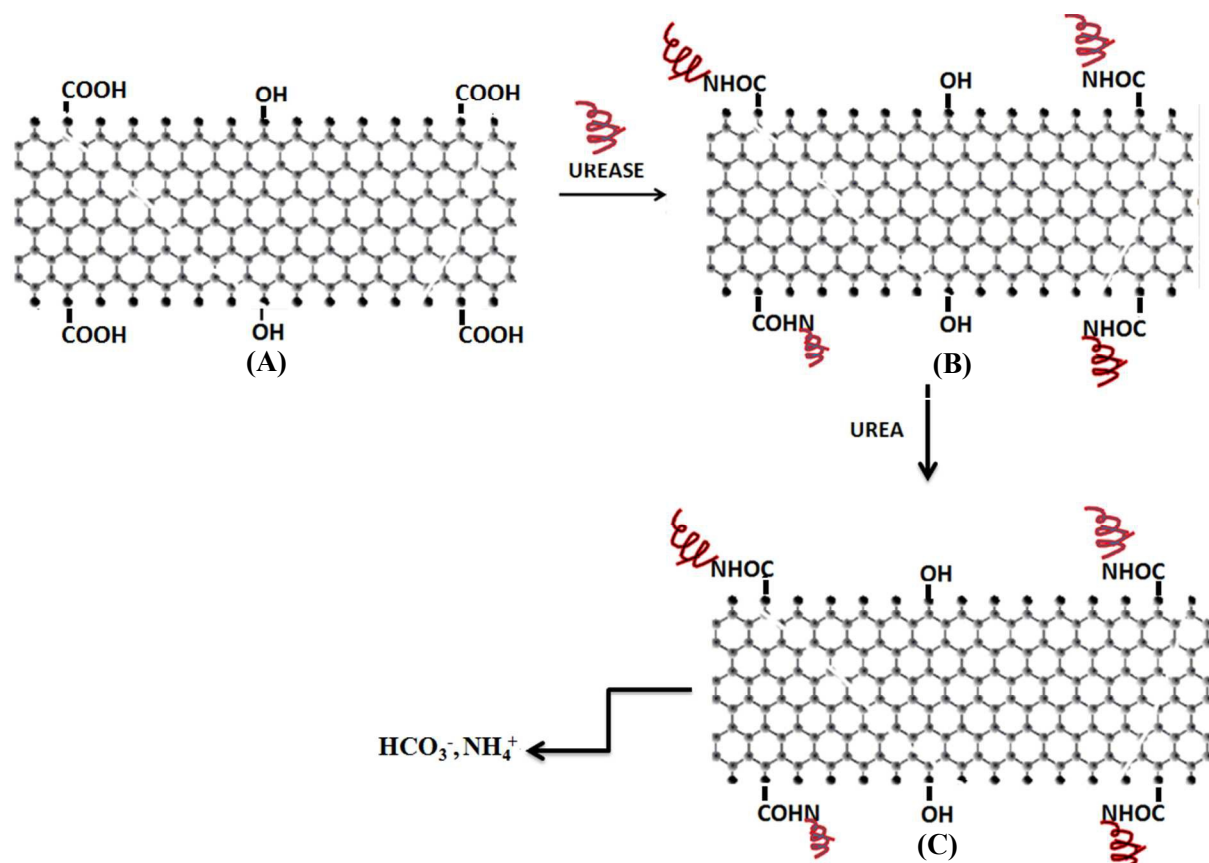
59 the working region of carbon nanotubes coated Screen Printed Electrodes (SPE). This
60 GNPIts/CNT-SPE platform can easily and efficiently detect the generation of ions, which
61 ultimately leads to urea estimation present in samples. It was observed that when a voltage sweep
62 of 0V to +1V is applied across the platform, it gave a residual current at 0V on interactions of
63 urea and urease. This residual current is explored to measure the estimation of urea.

64 **2. Materials and Methods**

65 GNPIts were purchased from XG sciences, (Michigan) having typical surface area of 50-
66 80 m²/g with average particle diameter of 25 microns and bulk density of 0.03 to 0.1 g/cc. CNT-
67 SPE were purchased from DropSens, India. EDC and NHS were purchased from Sigma-Aldrich.
68 Other chemicals like H₂SO₄, HNO₃, and HCl were purchased from Merck & Co., Inc, (India).
69 All the materials used in the present study were of analytical grade.

70 **Bioconjugation of urease:** Edge functionalized GNPIts were obtained by controlled oxidation of
71 GNPIts. GNPIts were mixed in a solution of H₂SO₄:HNO₃ (3:1) and ultrasonicated continuously
72 for one hour. After obtaining the uniform dispersion, the sample is placed in an ice bath and 2ml
73 of 10 M HCl was added drop wise. The sample was again subjected to sonication for 30 min and
74 left for 4 hours at room temperature¹⁶. The solution obtained was filtered through hydrophilic
75 PTFE filter membrane (0.2 μm pore size) and washed repeatedly with deionized (DI) water to
76 remove excess acid. Carboxylated GNPIts were dried and dispersed in aqueous solution for
77 urease bio-conjugation. The urease was attached to GNPIts with the help of EDC-NHS cross
78 linker. EDC is a zero length cross linker which facilitates the amide bond formation between
79 amine and carboxyl functionalized species. NHS increases the bonding efficiency (10 to 20 fold)
80¹⁷. GNPIts (1mg/ml), Urease (1mg/ml) were mixed with 0.05 M of EDC and 5 mM of NHS at
81 room temperature for 2 hour and then stored at 4°C overnight. The overnight storage hydrolyzes
82 unreacted EDC and causes loss of activity¹⁸. The unreacted enzyme and chemicals were
83 removed by vacuum filtration with repeated washing. Further, the conjugate was mixed with DI
84 water and ultra-centrifuged at 15,000 rpm leading to complete removal of excess unconjugated
85 materials. At last, urease conjugated GNPIts were immobilized on CNT-SPEs for urea sensing.
86 Different concentrations of urea ranging from 0.1 mg/ml to 0.8 mg/ml were prepared for
87 conducting experiments. Keithley's 4200 SCS system was used to investigate the current-voltage
88 (IV) characteristics of the sensing probe during the hydrolysis of urea. Furthermore, conjugation

89 of urease was confirmed by FTIR (Thermo Scientific NICOLET iS10), Raman (Renishaw inVia
 90 Raman microscope) and UV-Vis (Varian-5000 UV-VIS spectrophotometer) spectroscopy,
 91 whereas the edge functionalization (immobilization of urease) was ascertained by EDS (Energy-
 92 dispersive X-ray spectroscopy) attached with FE-SEM (Hitachi S-4800).



93
 94 **Fig.1.** Schematic representation of (A) Edge carboxylated GNPLts, (B) Graphene urease conjugate, (C)
 95 Generation of ions after the addition of urea.

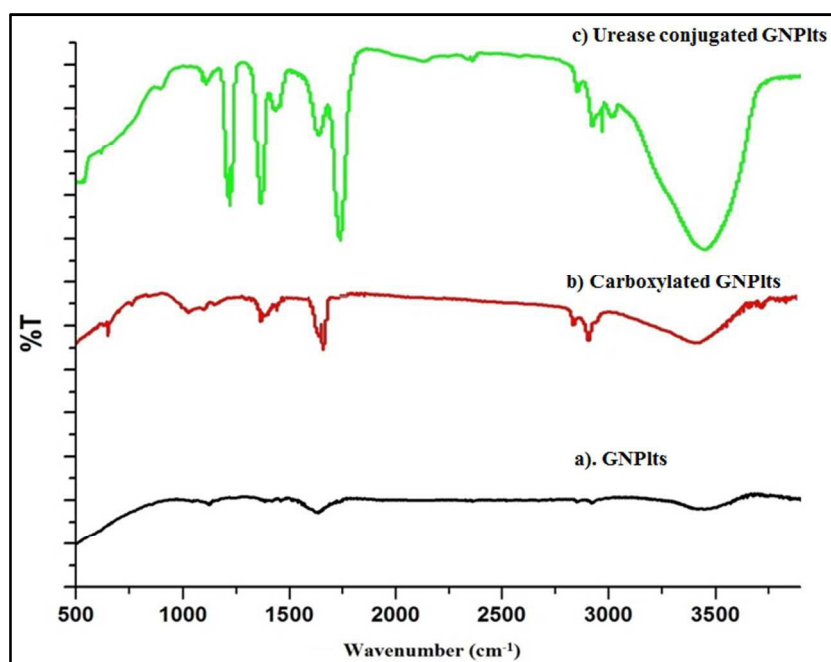
96 3. Results and discussion

97 The main focus of this article is on efficient sensing of urea with urease edge modified
 98 GNPLts. In this study, we have conjugated urease with GNPLts. Sensing of urea is done using this
 99 conjugate immobilized on CNT-SPE and employed for urea sensing (Fig. 1).

100 3.1 FTIR characterization

101 FTIR spectrum of GNPLts (Fig. 2) shows weak peaks at 3420 and 2920 cm^{-1} which are
 102 due to O-H and graphitic skeletal respectively. In case of carboxylated graphene, various peaks
 103 of oxygen containing groups were observed. The intensity of 3420 cm^{-1} peak found to be

104 increased to a great extent due to generation of –OH groups on GNPIts surface. The peak at 1736
105 cm^{-1} is due to C=O stretching of –COOH group present on the edges of GNPIts. The peak at
106 1635 cm^{-1} may be attributed to O-H deformation^{19,20}. The peak observed at 1365 cm^{-1} is due to
107 C–O–H vibrations present in carboxylic group²¹. The above results confirmed that oxygen
108 containing groups were generated on the GNPIts surface after treatment with acids. However,
109 untreated GNPIts also have few peaks which are responsible for oxygen containing groups, but
110 the intensity of these peaks is very less. The oxygen containing groups in untreated GNPIts may
111 be due to air oxidation or presence of moisture on GNPIts. The carboxylic groups generated on
112 the surface of GNPIts were utilized for amide bonding with amine group of urease. In case of
113 urease conjugated GNPIts, the prominent peaks of amide bond were observed at 1650 cm^{-1}
114 (amide C=O stretch) and 3440 cm^{-1} (amide N-H stretch)^{22,23}.



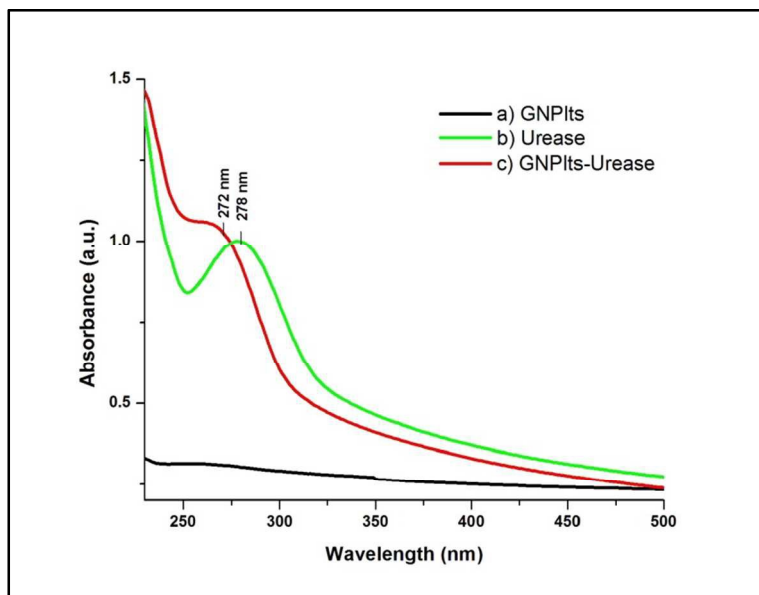
115

116 **Fig.2.** FTIR spectra for a) GNPIts, b) Carboxylated GNPIts, and c) Urease conjugated GNPIts.

117 3.2 Bioconjugation studies of GNPIts with urease

118 The bioconjugation of GNPIts with urease is confirmed by means of UV-Vis and Raman
119 spectroscopies. As shown in Fig. 3, the conjugate formation resulted in UV absorption at 278
120 nm, which is due to the presence of urease enzyme in the conjugate. Urease contain some
121 aromatic amino acids (Trp, Tyr and Phe) which shows π - π^* transition, hence resulting in UV
122 absorption at 278 nm. The peak at 278 nm shows blue shift with hyperchromatic effect after

123 conjugation of urease with GNPIs (i.e., it shifts to 272 nm). This blue shift may be attributed to
 124 the interaction between urease and GNPIs²⁴.



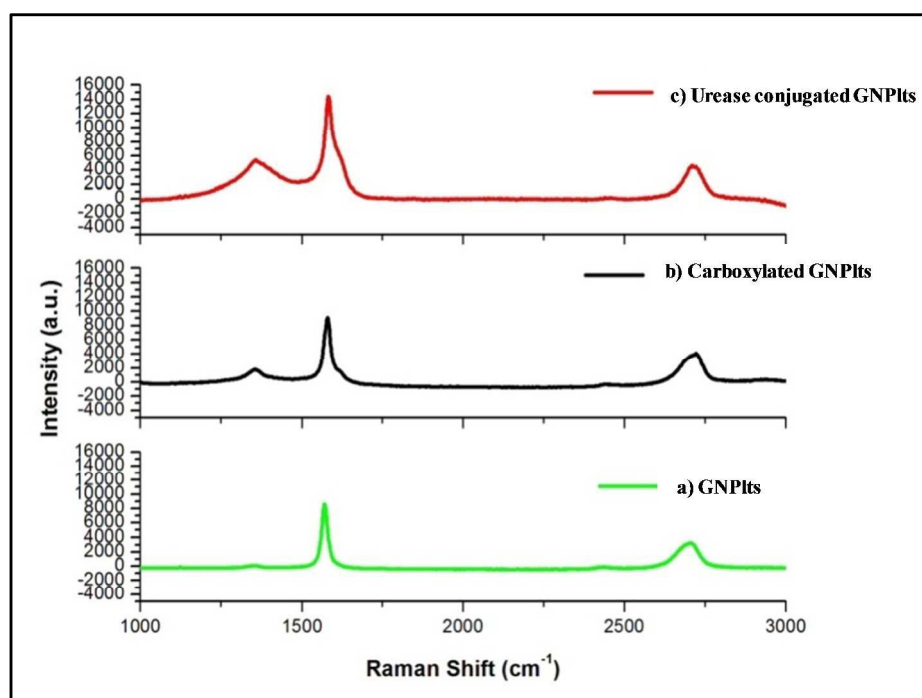
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126 **Fig.3.** UV-VIS spectra for a) GNPIs, b) Urease and c) GNPIs-Urease conjugate.

127 Fig. 4 represents the Raman spectra of GNPIs, carboxylated GNPIs and Urease conjugated
 128 GNPIs. Raman spectroscopy plays an important role in the characterization of carbon based
 129 materials. The main peaks arises in the carbonic samples are D peak ($\sim 1350\text{ cm}^{-1}$), G peak
 130 ($\sim 1580\text{ cm}^{-1}$) and 2D peak ($\sim 2700\text{ cm}^{-1}$). Raman spectroscopy potentially differentiates between
 131 sp^2 carbons from other carbonic structures^{25,26,27,28}. Raman spectra obtained at each step majorly
 132 of three samples- pristine GNPIs, carboxylated GNPIs and urease conjugated GNPIs. The
 133 spectra revealed very interesting peaks and alteration in intensities (Fig. 4). Raman spectra of all
 134 the three samples is mainly consisted of D (1355 cm^{-1}), G (1584 cm^{-1}) and 2D (2710 cm^{-1}) band.
 135 The relative intensities of D, G and 2D-Bands were altered after functionalization. Oxidation of
 136 GNPIs causes generation of defects and results in skeletal deformation of sp^2 structure which
 137 give rise to increase in the relative intensity of D-band after carboxylation. The increase in the
 138 intensity of D-band is proportional to the deformation in the sp^2 skeletal, which ultimately
 139 confirms the functionalization. The extent of functionalization was further confirmed by I_D/I_G
 140 ratio. The I_D/I_G ratio for GNPIs, carboxylated GNPIs and urease functionalized GNPIs were
 141 found to be 0.0167, 0.23, and 0.35 respectively. The pristine GNPIs have very less I_D/I_G ratio
 142 due to presence of very few defects in sp^2 skeletal. In case of carboxylated GNPIs this ratio

143 increased sharply due to generation of numerous defects during acid treatment. Upon
 144 conjugation of urease a little increase of 0.12 was observed in I_D/I_G ratio. This increase is mainly
 145 due to further functionalization of GNPIts and shielding of sp^2 signals due to wrapping/covering
 146 of GNPIts surface with urease²⁹.

147 It is further to mention that the edges of GNPIts are very fragile and whenever a chemical
 148 treatment is given it is likely to attack the edges. 2D peak in Raman is the result of interlayer
 149 interaction of GNPIts and after getting functional groups at the edges, these GNPIts have more
 150 tendency to self exfoliate leading to more intense peak at 2700 cm^{-1} .³⁰



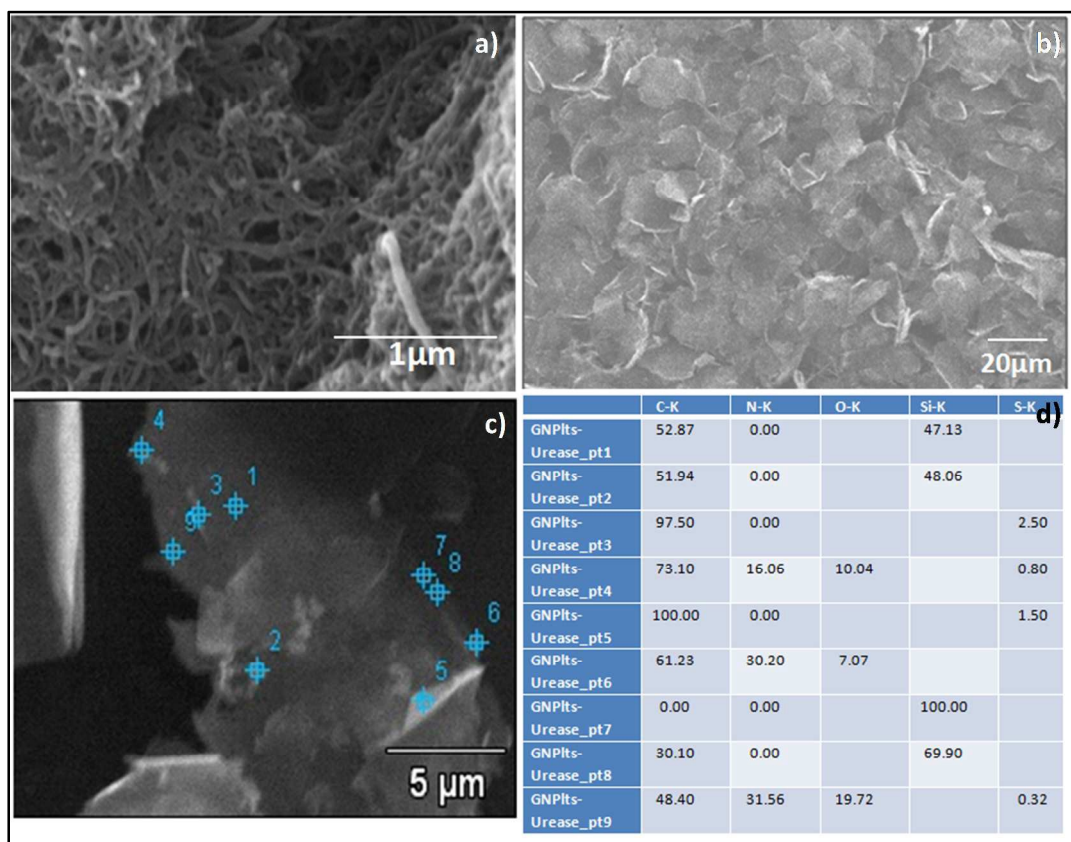
151
 152 **Fig.4.** Raman spectra of a) GNPIts, b) Carboxylated GNPIts, c) GNPIts-Urease.

153

154 3.3 FE-SEM and EDS Analysis

155 Surface morphology of bare CNT-SPE and GNPIts immobilised CNT-SPE (working
 156 electrode) is shown in Fig. 5a & b. FE-SEM and EDS analysis of GNPIts conjugated with urease
 157 is shown in Fig. 5c & d. The Microscopic analysis clearly shows GNPIts have an average length
 158 of 10 to 15 μm . On the sheet points 1, 2, 3 and 5 are specifically chosen on the central/Basal
 159 region of graphene while the points 4, 6, 7, 8 and 9 are taken on the edges of the graphene (Fig.

160 5c). The elemental data is taken at all the points through EDS as tabulated (Fig. 5d). On
 161 comparing the data collected from edges and basal points, it is clear that the edges of
 162 nanoplatelets have the peaks for carbon, nitrogen and sulfur, while the central region of the
 163 nanoplatelet has only carbonic content. The main reason for presence of nitrogen and sulfur in
 164 GNPIts is urease as it is composed of nitrogen rich amino acids. The presence of nitrogen at the
 165 GNPIts edges confirms edge functionalization with urease.

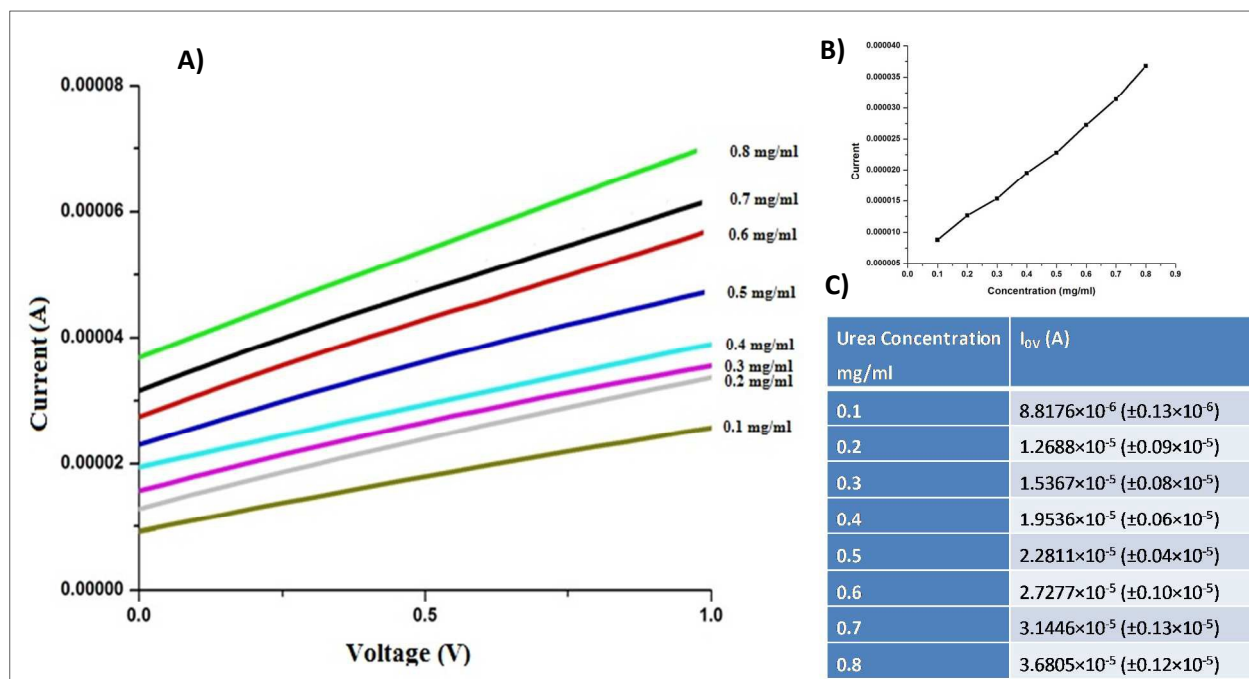


166
 167 **Fig.5.** a) FE-SEM micrograph of CNT-SPE, b) FE-SEM micrograph of GNPIts dropcasted CNT-SPE, c)
 168 and d) FE-SEM micrograph and EDS analysis (at different regions) of urease conjugated GNPIts. The
 169 points in SEM micrograph shown is chosen for EDS analysis. The EDS analysis shown (table) the weight
 170 % of different atom present on urease conjugated GNPIts. The edges of nanoplatelets have the peaks for
 171 carbon, nitrogen and sulfur, while the central region of the nanoplatelet has only carbonic content.

172 3.4 Sensing of Urea

173 The urease conjugated GNPIts were immobilized on CNT-SPE by simple dropcasting
 174 method. The prepared substrate is used for sensing of urea. As the edges are active for hydrolysis
 175 of Urea, therefore addition of urea leads to the generation of ammonium and carbonic ions,

176 which are responsible for variation in electron transport parameters. The most important electron
 177 transport parameters here are conductivity, mobility of charge carriers and shift in Dirac point of
 178 Graphene leading to current at 0V. On addition of different concentrations of urea, the
 179 conductivity of the urease conjugated GNPIs immobilized on CNT-SPE platform is measured.
 180 All the measurements are linear and ohmic in nature. From the graph, we can conclude that there
 181 is a considerable variation in the I-V characteristics with varying urea concentration.



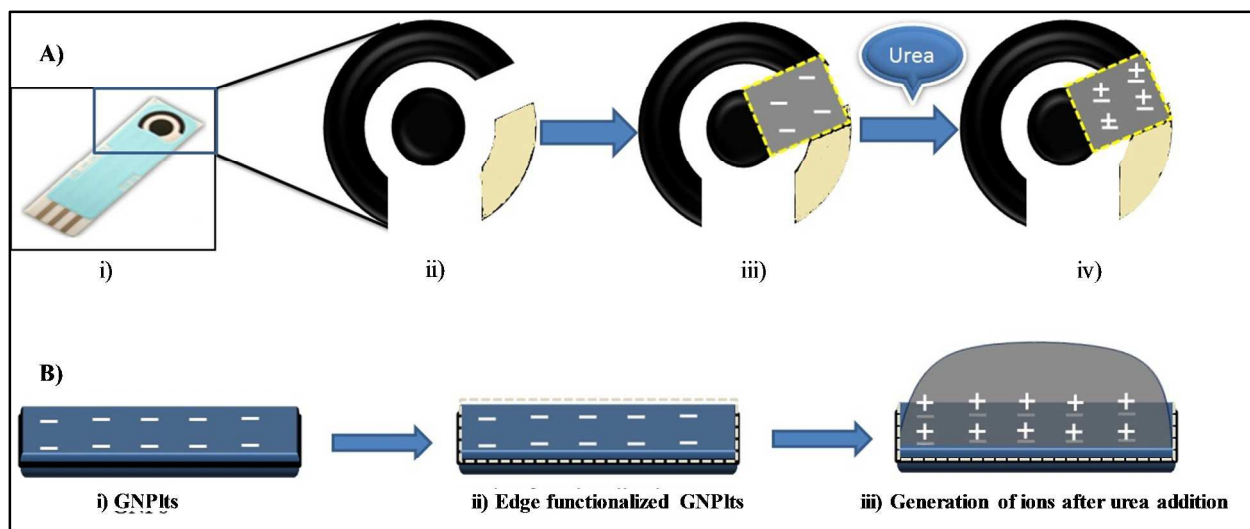
182 **Fig.6.** Sensing of urea by using urease conjugated GNPIs and CNT-SPE. A) IV-characteristics of urease
 183 conjugated GNPIs at different concentration of urea B) Urea concentration (mg/mL) vs average current
 184 (Ampere) produced during sensing of urea C) Table showing average current produced upon addition of
 185 urea on proposed platform.
 186

187 As any straight line graph IV can be understood by the equation

$$188 \quad I = (1/R) V + I_{0V}$$

189 Here I is the measured current and V is the applied voltage, 1/R is the slope of the IV curve and
 190 I_{0V} is the net current at 0 volt as shown in Fig. 6. There is an insignificant increase in the slope
 191 with increasing concentrations of urea. I_{0V} is the measure of conductivity due to the ions adhered
 192 on the graphene substrate. When Urea interacts with Urease, both positive and negative charge

193 carriers are generated. The conductivity is the net resultant of charge carriers generated and
 194 adhered on the surface of GNPIts.



195
 196 **Fig.7.** Accumulation of ions after urea hydrolysis creating electrostatic layer A.i) Screen printed electrodes,
 197 ii) enlarged view of working area, iii) dropcasting of edge functionalized GNPIts at working area of SPE
 198 (edges are represented by yellow dots), iv) Generation and accumulation of ions after addition of urea,
 199 B.i) pristine GNPIts, ii) Edge functionalized GNPIts, iii) Generation and accumulation of ions on the
 200 GNPIts surface.

201 Since graphene is rich in electronic charges on the surface, the electrostatic layers or kind of
 202 gating region is generated by the surface potential at the graphene-liquid interface at the edges
 203 (Fig. 7). When the negative surface charge which is screened by ions attracts mobile positive
 204 charges to the graphene-liquid interface, the negative surface potential is formed on the surface.
 205 These positive charges are both positive charges (holes) in the graphene and positive ions in
 206 interface liquid. As the concentration of ions increases, more and more surface charges get
 207 screened, leading to affect the mobility of charge carriers^{31,32}. When the potential is applied
 208 across the graphene substrate, the ions in close proximity to the graphene can contribute to
 209 Coulomb scattering. Coulomb scattering due to charged impurities/residues adsorbed on the
 210 graphene surface and Coulomb scattering of graphene charge carriers by charged ions can be the
 211 dominant scattering mechanisms, hence a consistent small increase in conductivity for the
 212 conjugate is observed³³.

213 As observed in Fig. 6, the curves are not passing through the origin; instead of 0V the curves are
214 showing a definite positive value of current. The adhered ions/ionic contamination on the
215 graphene substrate lead to shift in dirac point of the graphene, giving rise to conductivity at 0V
216 which could be considered as the measure for urea ions and can be a parameter for sensing³¹.

217 This positive value of current (I_{0V}) is due to the positive shift in dirac point during hydrolysis of
218 urea. As the concentration of urea increases, the urease cause generation of more ions, which
219 resulted in increased I_{0V} . When I_{0V} is plotted w.r.t. concentration, an almost linear graph with
220 average slope $3.3 \times 10^{-5} \text{A}/(\text{mg ml}^{-1})$. This is a direct measure of sensitivity of the developed
221 platform for urea. The results indicate a clear variation in the value of I_{0V} even with minute
222 change in the urea concentration. We successfully sense urea from concentration range of 0.1
223 mg/mL to 0.8 mg/mL with a response time of 15 seconds by using this nanohybrid platform. The
224 sensitivity of the system is quite high and may work well for urea adulteration range present in
225 milk. In order to study the effect of interfering molecules (like calcium phosphate, calcium
226 citrate, and magnesium citrate^{34,35}), control experiments were conducted and we found a
227 negligible change in I_{0V} . Therefore, it can be used as an efficient sensor to monitor the
228 concentration of urea.

229 Conclusion

230 Graphene and graphene based nanomaterials has arisen as the forefront of research in
231 electrochemical sensing due to its promising properties, especially the unique electrical and
232 surface modification features. Sensitivity of electron transport in graphene to the presence of ions
233 in solution may lead to a new paradigm of electrochemical sensors and biosensors.

234 Sensing of urea using nanohybrid platforms especially GNPIts could be a very efficient
235 technique for specific and sensitive detection of urea. The conjugate was immobilized on CNT-
236 SPE and utilized for amperometric sensing. GNPIts/CNT-SPE hybrid successfully achieved
237 good linearity with very less response time for urea sensing. This platform will be helpful in
238 determining urea adulteration and diagnosis of kidney related diseases. The developed platform
239 is reusable and can be used around 20 times without any significant change in results when
240 stored in 0.02M potassium phosphate buffer of pH 7 at 4°C after proper washing.

241 Such devices are stable over days of measurements and exhibit small change in mobility of
242 charge carriers on cycling multiple times. Research on such sensing techniques could be highly
243 beneficial for the development of advance, ultrasensitive, disposable, portable and routine use
244 sensors for other bioanalytes finding application in various areas.

245

246 **Acknowledgement**

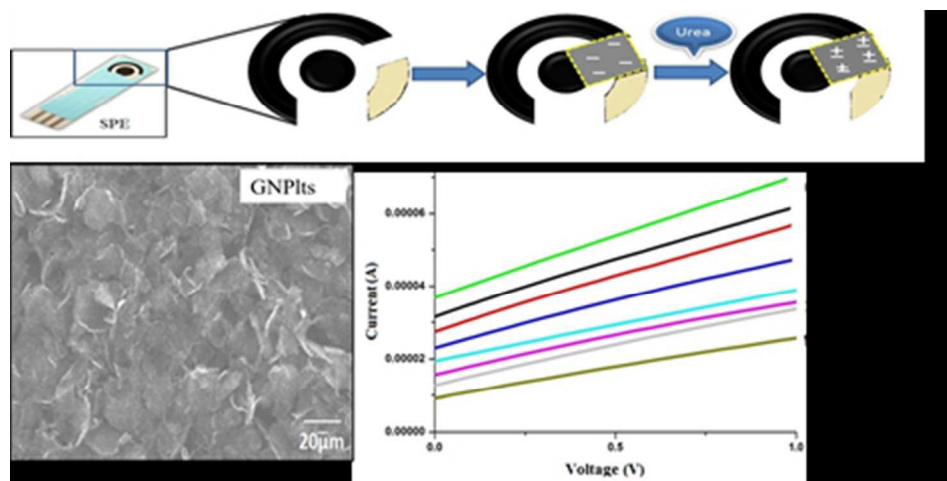
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253

254 **References**

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79x39mm (150 x 150 DPI)

In this study, we demonstrate efficient amperometric sensing of urea using graphene nanoplatelets.