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3 **One-step fabrication of gold nanoparticles/carbon nanosheets hybrid**
4 **by sonoelectrochemical technique for efficient surface-enhanced**
5 **Raman scattering**

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Abstract

23

24 A simple, fast, reproducible and efficient one-step fabrication method was
25 successfully developed to prepare gold nanoparticles/carbon nanosheets hybrids (Au
26 NPs/CNS) by sonoelectrochemical technique. This method involved simultaneous
27 generation of carbon nanosheets (CNS) by oxidation of graphite anode and Au NPs
28 by reduction of AuCl_4^- on the surface of cathode. Then the Au NPs modified with
29 poly(diallyl dimethyl ammonium chloride) were self-assembled on the surface of
30 CNS. A homemade sonoelectrochemical device which can provide both high electric
31 field and ultrasonic field was applied. Benefit from the synergy effect of electric field
32 and ultrasonic field, Au NPs with controlled size and distribution on the surface of
33 CNS could be obtained, which exhibited high-quality and distinctive SERS activity.
34 The enhancement factor of the developed substrate was 1.2×10^6 using 4-
35 aminothiophenol as the probe molecule. Taking advantage of the high affinity of CNS
36 toward aromatic molecules and the SERS activity of Au NPs, Au NPs/CNS showed a
37 great increase of Raman signals for aromatic molecules. The SERS substrate also
38 showed the charge selectivity to the cationic aromatic dyes, due to the negative charge
39 on the surface of CNS. Subsequently, the potential practical application of the SERS
40 substrate was evaluated by quantitative analysis of adenine. The results foresee the Au
41 NPs/CNS nanomaterials as sensitive SERS-active substrates having great potential for
42 detection of biomolecules.

43

44 **Keywords:** One-step fabrication, gold nanoparticles/carbon nanosheets,
45 sonoelectrochemical technique, surface-enhanced Raman scattering.

46

47 Introduction

48 Surface-enhanced Raman spectroscopy (SERS), as an ultra-sensitive and
49 powerful analytical technique for molecular sensing and detection, has received
50 increasing attention.¹⁻⁴ It has been generally accepted that the large enhancement of
51 normally weak Raman signals arises from an electromagnetic mechanism and a
52 chemical mechanism. Electromagnetic mechanism is based on the enhancement of the
53 local electromagnetic fields generated at or near nanostructured surfaces, while
54 chemical mechanism is based on the physical or chemical adsorption of the analyte to
55 metal surface to produce charge-transfer states between adsorbed molecules and metal
56 surface.⁵⁻⁸ In this sense, both the electromagnetic mechanism and chemical
57 mechanism enhancement require a close proximity of the analyte toward the metal
58 surface.

59 However, the adsorption ability of analyte on the surface of the metal
60 nanoparticles has a strong relation with their molecular structures. Hence the poor
61 affinity of the molecules toward the metal surface restricted direct analysis of diverse
62 molecules. To address this issue, various approaches have been proposed to improve
63 affinity of the analyte to the surface of metal nanoparticles⁹⁻¹⁵, such as removing the
64 undesired capping agents for SERS, the functionalization of nanoparticles by different
65 surface function groups, exploiting the mechanical trapping, and conversion of the
66 analytes by derivatization reaction. Nevertheless, the fixed functional molecules
67 make them only trap organic molecules who have strong interaction with functional
68 molecules. Recently, many researchers focus on fabricating metal nanoparticles
69 (MNPs) on the surface of carbon nanomaterials (e.g. carbon nanotube¹⁶⁻¹⁸, graphene¹⁹⁻
70 ²¹ and graphene oxide²²⁻²⁶), which have exhibited fascinating potential in the SERS
71 analysis of diverse target molecules due to its high affinity to these compounds. These

72 carbon nanomaterials with high specific large surface area had been used as effective
73 absorbent for aromatic molecules through electrostatic bonding or π - π cooperative
74 interaction.²⁶ In addition, these carbon nanomaterials, which were functionalized by
75 different functional reagents, showed potential in selective trap of the target analytes.
76 ²³ So, we believe that this kind of hybrids may serve as a useful tool to trap target
77 molecules with poor affinity toward the metal surface and thus to provide strong
78 SERS signals.

79 To apply SERS in routine studies for molecular detection, SERS-active substrate
80 should be reproducible, inexpensive and easy to be fabricated. Up to now, there have
81 been two common approaches for the hybridization of carbon nanomaterials and
82 MNPs: (1) reduction of the metal ionic precursor along with simultaneous deposition
83 of resultant MNPs on the surface of carbon nanomaterials (*in situ* method),^{20, 21, 26, 27}
84 (2) dispersion of pre-synthesized MNPs in a carbon nanomaterials solution followed
85 by the adsorption of MNPs on the surface of carbon nanomaterials (self-assembled
86 method).^{22,28-31} Hu *et al*²⁶ reported a direct growth of Au NPs on reduced graphene
87 oxide (rGO) film. This method involved an anode oxidation of bulk Au as sacrificial
88 anode to generate Au ion precursor, which was then reduced on the pre-fabricated
89 rGO/polyethylene terephthalate film by the electric field. However, these carbon
90 nanomaterials needed to be pre-synthesized in the above methods. Up to now, some
91 carbon nanomaterials including graphene and graphene oxide was usually prepared
92 through oxidative exfoliation of graphite by modified Hummers' method^{23, 24}, which
93 is time-consuming and complex. Recently, our group³² developed a one-step
94 sonoelectrochemical method for preparing the carbon nanoparticles in the pure water,
95 which is rapid and facile. Our interest was to develop a facile and one-step strategy to
96 prepare the hybrid of the carbon nanomaterials and noble metal.

97 In this paper, a facile one-step fabrication method was developed to fabricate
98 sized-controlled gold nanoparticles/carbon nanosheets hybrid (Au NPs/CNS) by
99 sonoelectrochemical technique. Carbon nanosheets (CNS) were generated by direct
100 oxidation of graphite anode under the high intensity electric field. Simultaneously, Au
101 NPs were generated by reduction of AuCl_4^- ions on the cathode. Both components
102 were dispersed into the electrolytic solution under ultrasonic field. Thereafter, Au
103 NPs/CNS nanomaterials were formed by self-assembly of the Au NPs on the surface
104 of CNS. To obtain this goal, a homemade sonoelectrochemical device providing both
105 high intensity electric field and ultrasonic field was applied. Benefit from the synergy
106 effect of electric field and ultrasonic field, the method was quite simple, fast,
107 reproducible and efficient. The resultant hybrids were supposed to possess the
108 combined properties of CNS and Au NPs, including the high affinity of CNS toward
109 aromatic molecules and the localized surface plasmon resonance based SERS
110 property of Au NPs. Furthermore, we show the potential of Au NPs/CNS
111 nanomaterials for SERS detection of biomolecules.

112

113 **Experimental**

114 **Sonoelectrochemical device**

115 A homemade sonoelectrochemical device³² reported in our previously published
116 work was used to synthesize Au NPs/CNS hybrids. The scheme of the
117 sonoelectrochemical device was shown in **SI Fig. 1**. The body of electrolyzer was
118 made from polymethyl methacrylate. A spectrum pure graphite ring and a titanium
119 tube were placed in the center of electrolyzer as anode and cathode respectively. The
120 thin O-ring with a thickness of 2 mm was used to separate the anode and cathode. The
121 ultrasonic generator was placed through the titanium tube cathode. The hollow shape

122 of cathode ensured that the ultrasonic power acted on the graphite anode. The hollow
123 shape of the anode made the high intensity electric field almost uniform. The graphite
124 anode's external diameter was 20 mm with its inner diameter and height of 12 and 15
125 mm respectively. This sonoelectrochemical device can provide the high intensity
126 electric field and ultrasonic field.

127

128 **Reagents and apparatus**

129 Polyvinylpyrrolidone (PVP, $M_w \approx 58,000$, K29-32), poly(diallyl dimethyl
130 ammonium chloride) (PDDA, 35% wt in water, $M_w < 100,000$), chloroauric acid
131 (HAuCl_4), methylene blue (MB), crystal violet (CV), sunset yellow (SY), congo red
132 (CR), anthracene (Ant), pyrene (Py) and 4-aminothiophenol (4-ATP) were purchased
133 by Shanghai Jingchun Reagent Co., Ltd. (Shanghai, China). KNO_3 was brought from
134 Sinopharm Group Chemical Reagent Co. Ltd. (Shanghai, China). Adenine, thymine,
135 cytosine, uracil and guanine were purchased from Sigma (USA). Fish sperm and calf
136 thymus DNA were obtained from Shanghai Chemical Co. Ltd. (Shanghai, China).
137 Perchloric acid and sodium hydroxide were brought from Damao Chemical Reagent
138 Factory (Tianjin, China). The all chemicals were analytical grade and used without
139 any further treatment. Ultrapure water was used throughout the study.

140 A Zhaoxin KXN-3002D DC power source was used to provide the electrolytic
141 voltage. A XinZhi JY92-□ ultrasonic disruptor was used to provide the ultrasonic field.
142 A battery-powered Raman spectrometer (model Inspector Raman, diode laser
143 excitation wavelength $\lambda_{\text{ex}} = 785 \text{ nm}$) in the range $200\text{-}2200 \text{ cm}^{-1}$ was used to provide
144 the Raman spectra. This system consists of a liquid- N_2 -cooled CCD detector (Model
145 Spec-10:400B, Roper Scientific, Trenton, NJ) with a spectral resolution of 8 cm^{-1} and
146 a data acquisition system (Photometrics, Tucson, AZ). Renishaw inVia Laser micro-
147 Raman spectrometer with He/Ne laser excitation at 532 nm was also used to provide

148 the Raman spectra. A 100× objective was used to focus the laser beam and to collect
149 the Raman signals. Ultraviolet-visible absorption spectra were performed on a Cary-
150 100Conc UV-vis spectrophotometer (Varian, American). Zeta-potential
151 measurements were performed by a Nanoparticle size-zeta potential and molecular
152 weight analyzer (Brookhaven, American). Transmission electron microscopy (TEM)
153 characterization was performed on a PHILIPS TECNAI 10 TEM instrument (Philips,
154 Netherlands). X-ray diffractometry (XRD) was carried out using a RIGAKU
155 diffractometer. X-ray photoelectron spectroscopy (XPS) experiments were performed
156 on an ESCA LAB 250 XPS instrument, which was equipped with the Mono AlK α X-
157 ray radiation as the source for excitation at a pressure of less than 2×10^{-9} mbar in the
158 chamber. Infrared absorption spectra were performed on a NICOLET AVATAR 330
159 Fourier transform infrared (FT-IR) spectrometer.

160

161 **One-step fabrication method of Au NPs/CNS hybrid**

162 The synthesis of Au NPs/CNS was performed in a homemade
163 sonoelectrochemical device mentioned above. The electrolytic solutions were
164 consisted of KNO₃ (50 mmol L⁻¹), PDDA (0.05%, wt) and HAuCl₄ (0.05%, wt).
165 PDDA served as chemical functional agent to modify Au NPs and connect Au NPs
166 with CNS. The electrolysis was carried out in a constant current at 100 mA. The
167 ultrasonic power was 40 W. After ultrasonic electrolysis for 5 min, the Au NPs/CNS
168 was obtained.

169 In the control experiment, Au NPs and CNS were also synthesized respectively
170 by the sonoelectrochemical method. In detail, Au NPs were prepared in a similar way
171 except that graphite electrode was replaced by Au electrode as anode. CNS was also
172 prepared in the similar way except that HAuCl₄ was not added to electrolytic

173 solutions. The other reaction conditions were the same as the synthesis of Au
174 NPs/CNS.

175

176 **SERS experiments**

177 For preparation of SERS substrates, the silicon substrate was first washed by
178 ultrasonication in acetone, ethanol, and water in turn. Then the substrate was treated
179 in Piranhasolution (98% H_2SO_4 /30% H_2O_2 =3:1, v/v; *CAUTION*: piranha solution
180 should be handled with great care) to clean the organic compounds and provide a
181 hydroxylated surface. Au NPs, CNS or Au NPs/CNS were then deposited on the
182 surface of the silicon substrate by simple drop-casting.³³ The number of the adsorbed
183 dye molecules on the substrate may not well control by solution soaking method. One
184 way to overcome this difficulty was to employ vacuum deposition.^{29, 34} To ensure the
185 comparable substrates with the same target molecules, 10 μL of CV, MB, Ant, Py, SY
186 or CR solution with the same concentration (10^{-6} mol L^{-1}) were dropped onto the
187 substrate respectively and dried by vacuum evaporation to ensure an equal
188 distribution. Raman spectra of the samples were measured by a portable Raman
189 spectrometer equipped with wavelength of 785 nm and a power of 30 mW with the
190 range 200-2200 cm^{-1} . The typical exposure time for each measurement in this study
191 was 1s with five accumulations unless specified.

192

193 **Result and discussion**

194 **Fabrication of Au NPs/CNS**

195 One-step sonoelectrochemical technique was used to fabricate Au NPs/CNS. The
196 schematic illustration of fabrication was shown in **Fig. 1**. Generally, the CNS was
197 generated by oxidation of graphite anode under the high intensity electric field.

198 Simultaneously, Au NPs were produced by reduction of AuCl_4^- ions on the surface of
199 titanium cathode. Afterwards, the resultant CNS and Au NPs modified with PDDA
200 were dispersed into the electrolytic solution under ultrasonic field. At the same time,
201 Au NPs/CNS nanomaterials were acquired by self-assembling Au NPs on the surface
202 of CNS. This synthetic strategy possesses several superiorities over the previous
203 method. Firstly, the fabrication of the Au NPs/CNS hybrid can be accomplished in a
204 one-step procedure, which simplifies the operation and facilitates the synthetic
205 efficiency. Secondly, the fabrication is completely "green" and no toxic reagents or
206 solvents are required. Thirdly, highly dispersive and homogenous attachment of Au
207 NPs on the surface of CNS owing to the synergy effect of electric field and ultrasonic
208 filed as compared with other synthetic strategies.

209

210

Fig.1

211 During the procedure of formation of Au NPs/CNS, the modifier plays an
212 important role. At the beginning of the experiment, we attempted to synthesize the Au
213 NPs/CNS without adding any chemical functional agent. However, this would lead to
214 the deposition of Au NPs on the surface of titanium cathode instead of dispersion in
215 the electrolytic solution. To solve this problem, the use of chemical functional agent is
216 needed to prevent the Au NPs depositing on the surface of titanium cathode. PVP³⁵
217 was the commonly used stabilizing agent for Au NPs due to its unique chemical
218 structure and properties. But to our surprise, the Au NPs was dispersive in electrolytic
219 solution but not self-assembled on the surface of CNS by using PVP as modifier.
220 PDDA is a kind of cation polyelectrolyte which can usually act as stabilizing agent in
221 the synthesis of colloids³⁶ and a chemical functional agent³⁷. In order to achieve the
222 Au NPs/CNS, PDDA was chosen as chemical functionalized agent in our study owing

223 to the following reasons. PDDA is good candidate as modifier to stabilize the Au NPs.
224 Au NPs modified with PDDA exhibited positive charges, and can be self-assembled
225 on the surface of CNS with negative charges by electrostatic adsorption. The
226 concentration of PDDA had an impact on the generation and SERS activity of Au
227 NPs/CNS. When the concentration of PDDA was less than 0.05%, Au NPs cannot be
228 completely dispersed. The stable Au NPs/CNS nanomaterials were formed until the
229 concentration of PDDA was above 0.05%. Excess PDDA had negative effect to the
230 SERS performance of Au NPs/CNS (SI Fig. 2). Therefore, the concentration of the
231 PDDA was optimized to 0.05%.

232 Ultrasonic field plays a crucial role in the fabrication of Au NPs/CNS. The Au
233 NPs and CNS formed must be rapidly transferred from the cathode and anode vicinity
234 to the bulk solution, thus to facilitate the self-assembly of Au NPs on the surface of
235 CNS. If the fabrication of the Au NPs/CNS was carried out without ultrasonic field,
236 deposition of Au NPs and CNS on the respective electrode would occur. Other
237 conditions that affected the fabrication and SERS of Au NPs/CNS were also
238 investigated (SI Fig. 2 and SI Fig.3). The size and density of Au NPs on the CNS,
239 and Raman activity of Au/CNS were depended strongly on the concentration of
240 HAuCl_4 . When the concentration of HAuCl_4 was 0.05%, the best SERS signal can be
241 obtained. The concentration of KNO_3 (50 mmol L^{-1}), ultrasonic power (40 W), electric
242 current (100 mA) and electrolytic time (5 min) were used for generating high SERS
243 active Au NPs/CNS substrate.

244

245 **Characterization of Au NPs/CNS**

246 The morphology and structure of CNS and Au NPs/CNS were first examined by
247 TEM (Fig. 2 A and Fig. 2B). The TEM image of the CNS clearly illustrated the
248 flake-like shape with some corrugations. The TEM of Au NPs/CNS showed that

249 roughly spherical Au NPs with diameters of 56.0 ± 10.1 nm were attached on the
250 surface of CNS. Furthermore, the presence of Au element in the hybrids was
251 confirmed by the XPS. As shown in **Fig. 2C**, the XPS revealed that Au NPs/CNS
252 consisted of the elements of C, O, Au and N. The signals of C and O originated from
253 CNS. The presence of Au element in Au NPs/CNS confirmed the successful
254 decoration of CNS with Au NPs. The existence of N element was supposed to be
255 induced by PDDA modifier. Large number of C=C and C-C existed on the surface of
256 CNS and Au NPs/CNS (**Fig.2 E and Fig.2F**), which showed the potential of Au
257 NPs/CNS to adsorbed target analytes by π - π interaction.^{23,28} The result of XPS and
258 FT-IR (**SI Fig.4**) exhibited that abundant of carboxyl groups existed on the surface of
259 CNS. The zeta potentials (ζ) of the as-synthesized CNS were -35 mV, which further
260 proved that large amounts of negative charges were present on the surface of CNS.
261 On the other hand, as shown in **Fig. 2D**, the Au 4f for Au NPs/CNS can be detected
262 and the binding energy of 83.6 eV for Au 4f_{7/2} state and 87.2 eV for Au 4f_{5/2} state are
263 identified respectively.

264

265 **Fig.2**

266

267 UV-vis absorption spectra of aqueous dispersion of CNS and Au NPs/CNS were
268 shown in **Fig. 3A**. After decoration with Au NPs on the surface of CNS, there was
269 evidently a new peak at about 543 nm. This was the characteristic of Au NPs due to
270 the surface plasmon absorption, which implied Au NPs attaching on the surface of
271 CNS. XRD was also used to verify the formation of Au NPs/CNS. As shown in **Fig.**
272 **3B**, four peaks were observed at $2\theta = 38.187, 44.385, 64.576$ and 77.567 , which can
273 be indexed to the (111), (200), (220) and (311) reflections of metal gold, respectively

274 (JCPDS No. 65-2870). The result indicated that Au NPs had been successfully self-
275 assembled on the surface of CNS.

276 Raman spectrum of carbon nanomaterials^{17, 19-21, 23, 26, 38} usually exhibited the
277 regular two peaks, corresponding to the D-band line (1350 cm⁻¹) and the G-band line
278 (1580 cm⁻¹). The D-band at 1352 cm⁻¹ is a disorder-activated Raman mode that
279 indicates extensive oxidation of the graphite, whereas the G-band centered at 1595
280 cm⁻¹ is characteristic of the sp²-hybridized carbon atoms in the hexagonal framework,
281 which is important for the adsorption of molecules through noncovalent interaction.
282 With decoration of Au NPs, the intensity of the D and G bands of CNS obviously
283 increase by 503% and 506% respectively in comparison with those of the CNS under
284 the same test conditions (**Fig. 3C**), which could be attributed to the coupled surface
285 plasmon resonance absorption of the Au NPs on the CNS.

286

287 **Fig. 3**
288

289 **SERS properties**

290 The as-prepared Au NPs/CNS nanomaterials were used as efficient SERS
291 substrate for organic molecule sensing. The Raman signals of the model molecules on
292 bare silicon, CNS, Au NPs and Au NPs/CNS substrates were measured and compared
293 under the same conditions (integration time, laser power, focus, etc.). In this case, CV
294 and MB (positively charged molecule), Ant and Py (neutral molecule), SY and CR
295 (negatively charged molecule) were used as model probe molecules. For the above six
296 molecules, the SERS spectra obtained from the Au NPs/CNS were more intense than
297 those from Au NPs (**Fig.4**). These observations indicated that CNS modification
298 indeed amplified the SERS signals of the six model molecules. It is supposed to be

299 strong interaction between CNS and the aromatic molecules because of the π - π
300 electrostatic stacking properties originated in GO material.^{29, 39}

301

302 **Fig.4**

303

304 The enhancement effect of CNS was quantitatively analyzed by applying SERS
305 intensity ratio (n) between the Au NPs/CNS and Au NPs substrates, and described by
306 the following equation: $n=I_{di}/I_{ci}$.²³ As schematically shown in **Fig.4**, I_{di} and I_{ci} were
307 the intensity of Raman shift (i) obtained on the Au NPs/CNS and Au NPs,
308 respectively. The SERS intensity ratios and the assignment of the Raman bands of the
309 four Raman probe molecules were summarized and compared in **Table. 1**. Obviously,
310 the enhancement effect of the Au NPs/CNS to probe molecules from high to low were
311 positively charged molecules, neutral molecule and negatively charged molecules in
312 turn. This phenomenon can be rationalized by different affinity of the Au NPs/CNS to
313 the different kinds of molecules. In detail, negatively charged CNS had strong
314 electrostatic attraction with model molecules by the π - π interaction and charge
315 interaction, which enabled the direct adsorption of these molecules near the metal
316 surface thus gave high SERS enhancement. On the other hand, Au NPs modified with
317 PDDA can drive easily negatively charged molecules on their surfaces. According to
318 above results, negatively charged CNS played more important role than Au NPs
319 modified with positively charged PDDA on the adsorption molecules to the surface of
320 Au NPs/CNS. The charge tendency of the Au NPs/CNS would benefit to improve
321 SERS selectivity.

322

323

Table 1

324 On the basis of the above results, we propose that the driving force of the mainly
325 effects of CNS on the SERS intensity is dictated by strong adsorption of analytes both
326 by π - π interaction and charge interaction.

327 For quantitative detection, it is very important for SERS substrates to have good
328 uniformity and reproducibility. It was reported that a substrate with poor uniformity
329 and reproducibility would lead to Raman intensity different of 2-3 times from one
330 spot to another.²³ Consequently, the uniformity and reproducibility of Au NPs/CNS as
331 SERS substrate were evaluated using 4-ATP as the probes molecules. We checked the
332 reproducibility of the SERS measurement by recording spectra from the 40 randomly
333 selected places on the same batch and taking SERS spectra with 30 different batches
334 of the samples. The relative stand deviations of the 1073 cm^{-1} were 9.9% and 12.9%
335 respectively (**SI Fig. 5**), which indicated the Au NPs/CNS as SERS substrate had high
336 uniformity and good reproducibility. Additionally, we estimated the enhancement
337 ability of Au NPs/CNS substrate by calculating the enhancement factors (EF) of 4-
338 ATP molecular. The EF was calculated to be 1.2×10^6 at 1073 cm^{-1} for the Au
339 NPs/CNS (**SI Fig. 6**), which is comparable to other Au NPs decorated carbon
340 nonmaterial hybrid SERS substrates.²⁰ However, this sonoelectrochemical method
341 may offer a simple and effective way for fabrication hybrid of CNS and metal
342 nanoparticles with controlled size and distribution.

343

344 **SERS detection of adenine**

345 Adenine plays a significant role in biological system as it has widespread effect
346 to coronary and cerebral circulation, energy transduction, enzymatic reactions as
347 cofactors, and even in cell signaling.^{45, 46} Abnormal changes of its concentration may
348 indicate the presence of various diseases. Therefore, quantification of adenine is

349 critical for the investigation of a wide variety of biological issues. Adenine can be
350 protonated in acid and deprotonated in base (SI Fig.7). As shown in Fig. 5A, the
351 SERS of adenine at pH 4.00 was 1.34 times of that at pH 11.00. This result can be
352 explained that CNS had more adsorption of protonated adenine near the metal surface
353 thus gave high SERS enhancement.

354 To examine the linear range in SERS detection of adenine, the pronounced and
355 isolated band of adenine located at 734 cm^{-1} (Fig. 5A) was selected for quantitative
356 detection. Fig. 5B shows the obtained concentration-response curve for adenine in
357 aqueous solution at pH 4.00. Based on Fig. 5B, SERS signal of adenine increases as
358 concentration of adenine and remains almost constant after 10 mg L^{-1} . The linear
359 regression coefficient value is 0.9966 in the concentration range of $0.1\text{--}10.0\text{ mg L}^{-1}$.
360 The limit of detection was 0.04 mg L^{-1} .

361

362

Fig. 5

363 To examine the feasibility of the Au NPs/CNS in determination of adenine under
364 interference of other nucleobases, adenine solutions (0.7 mg L^{-1}) were mixed with
365 equimolar concentration of the other nucleic bases such as guanine, cytosine, thymine
366 and uracil. The SERS intensity of adenine ring breathing mode at 734 cm^{-1} was used
367 to determine the adenine under co-existing of second nucleobases. The results
368 indicated that the investigated nucleic bases did not interfere the determination of
369 adenine, since a variation of the Raman intensity at 734 cm^{-1} was less than $\pm 5\%$. The
370 result reveals a high selectivity for adenine determination.

371 The method was then applied to the analysis of adenine in acid hydrolyzate of
372 the beer and DNA (fish sperm), respectively (Fig. 6). The recoveries were evaluated
373 by adding known amounts of standard adenine solution to the samples. The recoveries

374 varied from 82.4 to 94.2%, showing the excellent performance of the method for the
375 examined samples (**Table 2**). To evaluate the proposed SERS method, the samples
376 were also analyzed by HPLC.^{47, 48} The results (**Table 2**) indicated that there was no
377 significant difference between two methods. The result agreed well with the
378 conventional HPLC method, suggesting the potential application for detection of
379 biomolecules.

380 **Fig. 6**

381 **Table 2**

382 **Conclusion:**

383 In summary, we have illustrated a simple, fast, reproducible and efficient one-
384 step strategy to fabricate Au NPs/CNS by sonoelectrochemical technique. The all
385 process was finished in a homemade sonoelectrochemical device, which can provide
386 the high intensity electric field and ultrasonic field. The electric and ultrasound field
387 plays a crucial role in the production and dispersion of Au NPs and CNS. The as-
388 prepared Au NPs/CNS nanomaterials combined the unique properties of Au NPs and
389 CNS, and exhibited significantly SERS enhancement to aromatic molecules. The Au
390 NPs/CNS as SERS substrate also showed the charge selectivity to the cationic
391 aromatic dyes, due to role of the CNS nanomaterials with negatively charges.
392 Significantly, the SERS substrate could produce highly enhanced Raman signals
393 ($EF \sim 1.2 \times 10^6$) with good uniformity and reproducibility. Furthermore, Au NPs/CNS
394 can be as an active SERS substrate for quantitative detection of adenine. These results
395 foresee the Au NPs/CNS nanomaterials will have great potential as sensitive SERS-
396 active substrates in routine studies for biomolecules. Considering the well-established
397 sonoelectrochemical method in the preparation of nanomaterials, the present strategy

398 may also be applied in preparing other carbon nanomaterial based nanocomposites as
399 well.

400

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405

406

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496 Table 1 SERS intensity ratio (n) and the assignments of several Raman bands of
 497 six Raman probe molecules

Probe molecules	Raman shift (cm^{-1})	n	Band assignment ^{23,40-44}
CV	915	5.0	ring skeletal vibration
	1177	4.6	ring C-H bending
	1613	4.5	ring C-C stretching
MB	673	5.9	out-of-plane C-H bending
	1397	6.0	in-plane ring C-H deformation
	1619	5.3	ring C-C stretching
Ant	1161	4.4	ring C-C stretching
	1403	4.5	ring C-C stretching/ring stretching
	1557	4.3	ring C-C stretching
Py	1237	4.0	ring C-C stretching/C-H in-plane bending
	1408	4.3	ring C-C stretching/ring stretching
	1620	3.9	ring C-C stretching
CR	1178	1.9	ring C-H bending
	1453	2.3	N=N stretching
	1591	1.9	ring C-C stretching
SY	1230	2.0	C-N stretching
	1391	3.2	in-plane ring C-H deformation
	1596	2.5	ring C-C stretching

498 The assignments of the peaks of CV, MB, Ant, Py, SY and CR are based on previous reports.^{23,40-}

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504 Table 2 Determination of adenine in acid hydrolyzate of the DNA and beer by
 505 SERS and HPLC

sample	SERS				HPLC found ^a
	found ^{a,b}	Added	Recovery ^{a,b} (%)	RSD ^c (%)	
fish sperm	68.0	10.0	82.4	6.7	72.9 ± 6.4
DNA (mg g ⁻¹)		50.0	85.9	5.6	
calf thymus	44.1	10.0	90.2	6.8	40.1±3.5
DNA (mg g ⁻¹)		50.0	83.2	6.7	
beer 1 (mg L ⁻¹)	14.2	5.0	85.6	6.1	15.6± 0.9
		25.0	92.7	7.3	
beer 2 (mg L ⁻¹)	11.5	5.0	94.2	8.4	12.8±1.0
		25.0	85.0	7.3	

506 ^a Diluted appropriate times before analysis

507 ^b Quantitative date at 734 cm⁻¹.

508 ^c n=5, quantitative date from five different spots

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516 **Figure captions:**

517 Fig.1 Schematic illustration of the fabrication of Au NPs/CNS by the one-step
518 sonoelectrochemical method

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520 Fig.2 TEM of (A) CNS and (B) Au NPs/CNS, (C) Survey XPS spectra of CNS and
521 Au NPs/CNS, (D) Au4f XPS spectra of Au NPs/CNS, C1s XPS spectra of (E) CNS
522 and (F) Au NPs/CNS

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524 Fig. 3 (A) UV-Vis absorption spectra of (a) CNS and (b) Au NPs/CNS, (B) XRD of
525 Au NPs/CNS, (C) Raman spectra of (a) CNS and (b) Au NPs/CNS

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527 Fig.4 Raman spectra of CV, Ant, SY, MB, Py and CR (a) on silicon (the black line),
528 (b) CNS (the red line), (c) Au NPs (the blue line) and (d) Au NPs/CNS (the green
529 line). They were recorded under the same conditions where the concentration is 10^{-6}
530 mol L^{-1} . Molecular structures of dyes are drawn inset. The excitation wavelength is
531 785 nm.

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533 Fig. 5 (A) SERS of adenine (5 ppm) at different pH, (B) SERS intensity of adenine at
534 734 cm^{-1} from different concentration

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536 Fig.6 (A) SERS of adenine from the beer spiked with 0 (a), 5.0 (b) and 25.0 (c) mg L^{-1} ,
537 (B) SERS of adenine from the fish sperm DNA spiked with 0 (a), 10.0 (b) and 50.0 (c)
538 mg g^{-1} (diluted appropriate times before determination).

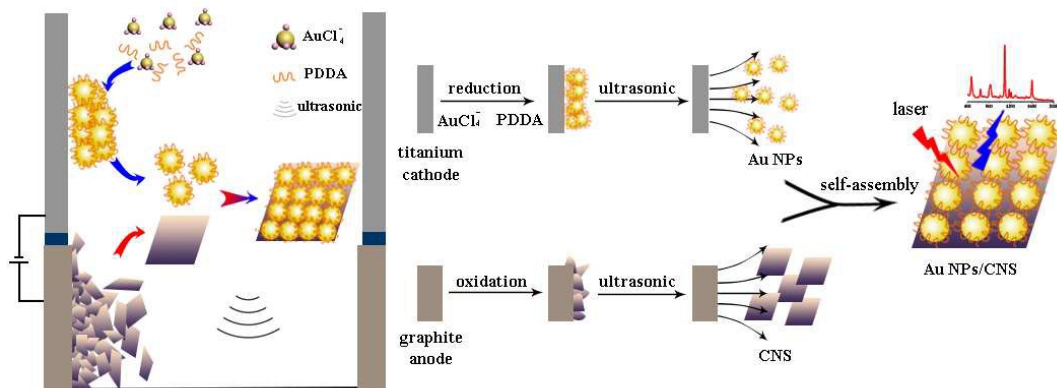
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543 Fig.1



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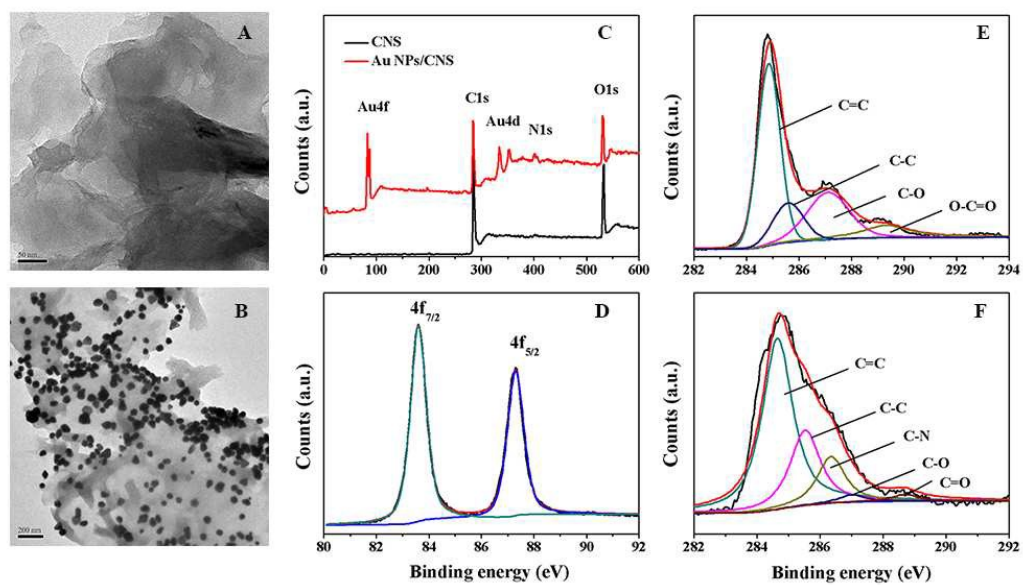
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561 Fig.2

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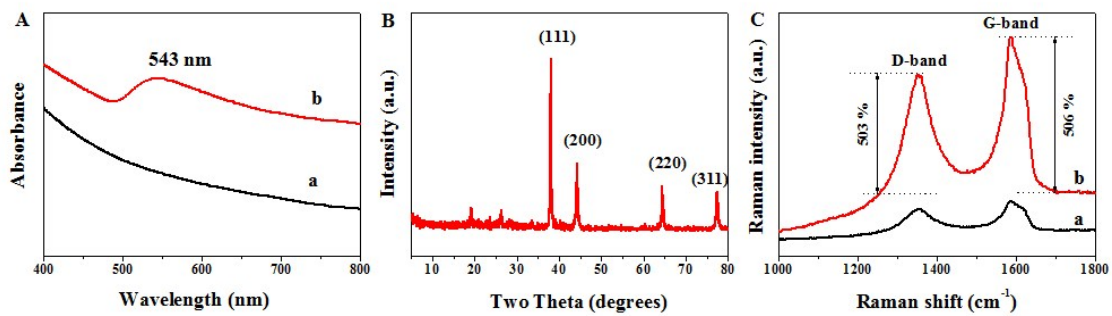
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580 Fig.3

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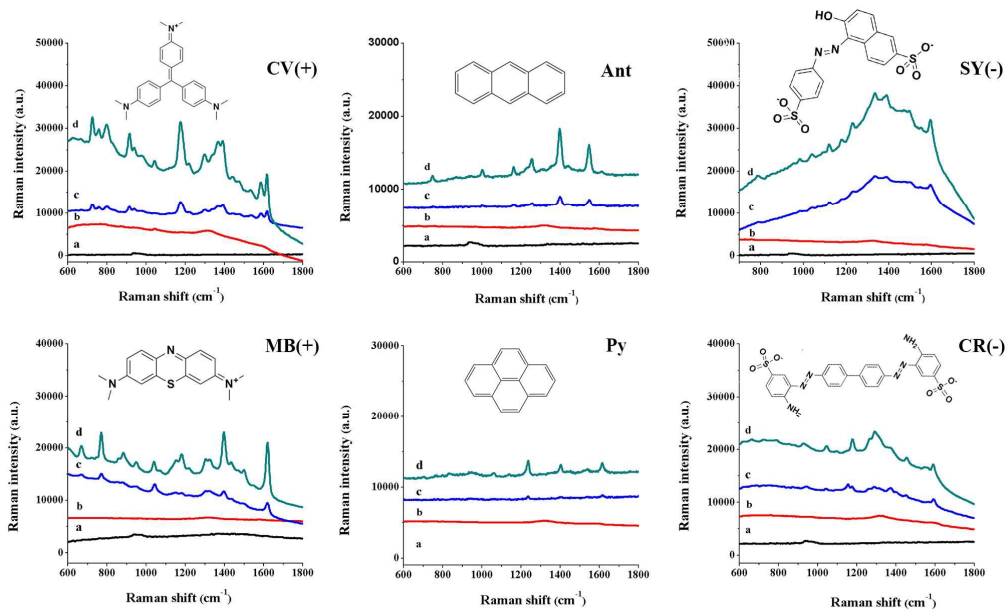
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606 Fig.4

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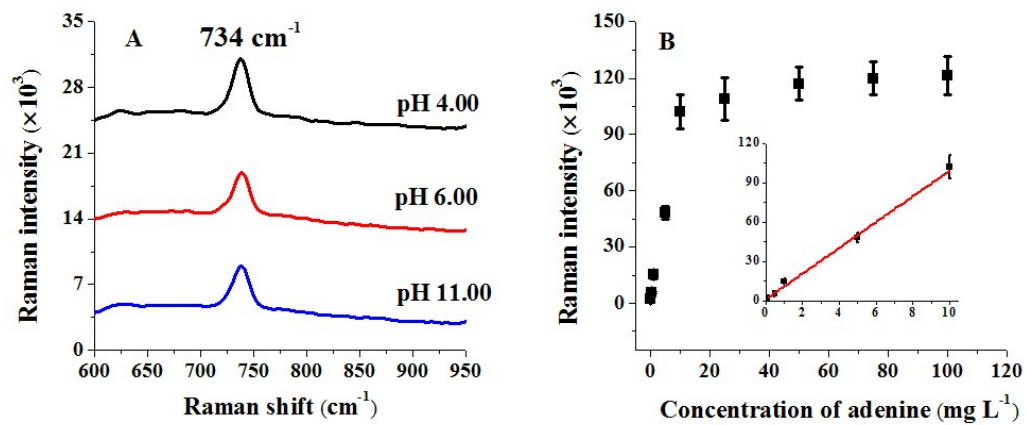
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627 Fig.5



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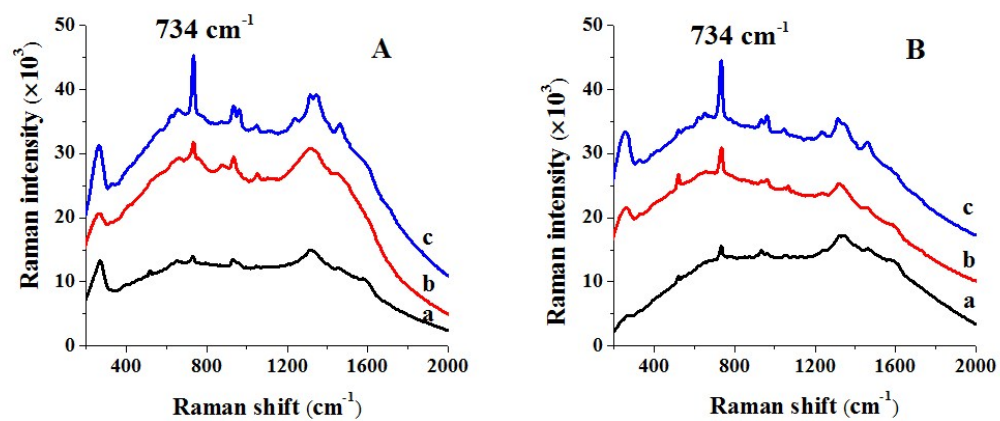
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649 Fig.6



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