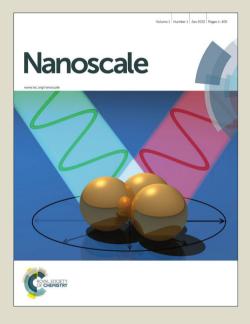
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ARTICLE TYPE

Biodegradation of Carbon Nanohorns in Macrophage Cells

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Abstract

With the rapid development in the medical application of carbon nanomaterials such as carbon ²⁰ nanohorns (CNHs), carbon nanotubes, and graphene based nanomaterials, understanding the long-term fate, health impact, excretion, and degradation of these materials have become crucial. Here, the *in vitro* biodegradation of CNHs was determined using a non-cellular enzymatic oxidation method and two types of macrophage cell lines. Approximately 60% of the CNHs were degraded within 24 h in a phosphate buffer solution containing myeloperoxidase. Furthermore, approximately 30% of the CNHs

²⁵ were degraded by both RAW 264.7 and THP-1 macrophage cells within 9 days. Inflammation markers such as pro-inflammatory cytokines interleukin 6 and tumor necrosis factor α were not induced by exposure to CNHs. However, reactive oxygen species were generated by the macrophage cells after uptake of CNHs, suggesting that these species were actively involved in the degradation of the nanomaterials rather than in an inflammatory pathway induction.

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1. Introduction

Carbon nanomaterials such as carbon nanohorns (CNHs),^[1]

- carbon nanotubes (CNTs),^[2,3] and nanographene^[4,5] have many ⁵ interesting properties and potential applications in the development of optics and electronics.^[6] Nanocarbons also have potential applications in nanomedicine; for example, CNTs and CNHs may be excellent carriers in drug delivery systems,^[7–13] or may be useful as photo-thermal agents for hyperthermia
- ¹⁰ therapy.^[14–18] Although CNTs and CNHs present low toxicity,^[19–21] they are still viewed with skepticism because of their accumulation in cells of the mononuclear phagocytic system such as macrophages and their incomplete excretion or clearance from tissue once administrated into animals.^[22–25] In addition, the long
- ¹⁵ term fate of accumulated nanomaterials and impact of their accumulation on tissues have been scarcely investigated. Therefore, evaluating and characterizing the potential degradation of carbon nanomaterials in professional phagocytes such as macrophages is crucial for understanding both their safety and ²⁰ potential use in nanomedical applications.
- Historically, it was generally believed that carbon nanomaterials could not be degraded in tissues due to their stable and inert graphitic structures; however, recent studies have shown that peroxidase enzyme-based processes can lead to the oxidation
- ²⁵ and biodegradation of CNTs and graphene.^[26–31] Oxidized singlewall carbon nanotubes were degraded in stimulated neutrophils without causing obvious pulmonary inflammation when the products of degradation was instilled in the lungs.^[28] In addition, it was shown that these same materials can also be directly
- ³⁰ degraded in the lungs of mice after pharyngeal aspiration.^[32] Following stereotactic administration into the brain cortex, amino-functionalized multi-walled carbon nanotubes were also partially degraded in mice,^[33] and a long-term study of tangled oxidized multi-walled carbon nanotubes in rat subcutaneous
- ³⁵ tissue showed that the majority of agglomerates located outside macrophage cells did not undergo degradation, whereas the small agglomerates inside macrophages were degraded gradually.^[34] However, only a few *in vitro* studies on CNT biodegradability have been reported to date, and details of the degradation of
- ⁴⁰ CNTs in macrophage cells is still scarce. Kagan *et al.* have first demonstrated that monocyte-derived macrophages freshly isolated from healthy adults can degraded oxidized CNTs,^[28] and have recently reported in a follow-up study that the oxidative degradation of oxidized CNTs in PMA activated THP-1 ⁴⁵ macrophages was actually taking place mainly via a 'super-

 $oxide/NO^* \rightarrow peroxynitrite'$ -driven oxidative pathway.^[35] To our knowledge, the biodegradation of CNHs, which have high potential in the field of nanomedicine, has not yet been

- investigated. In our previous mouse study, approximately 40% of ⁵⁰ a dose of intravenously injected CNHs was cleared from the body after 1 month, of which 15% was excreted in feces and the remaining 25% was thought to first accumulate and then degrade in macrophages of the liver,^[24] although this proposal has not yet been confirmed. To test the hypothesis of macrophage-mediated
- ⁵⁵ degradation of CNHs, we investigated here the biodegradability of CNHs in a non-cellular model as well as in two cell lines, namely RAW 264.7 mouse leukemia macrophage cells and THP-1 human leukemia cells. The results confirmed that CNHs are degraded by both myeloperoxidase (MPO)-catalyzed oxidation
- ⁶⁰ and by macrophage cells, as previously reported for CNTs.^[28, 30] An estimated 30% of the CNHs were degraded in the RAW 264.7 and THP-1 macrophages. To determine their roles in the degradation of CNHs, the induction of reactive oxygen species (ROS) and cytokines in macrophages by CNHs was also

⁶⁵ investigated. The results presented here contribute to the current understanding of the biodegradation of other carbon nanomaterials, particularly those that are free from impurities, such as metals.^[1,36]

70 2. Results

2.1. Degradation of CNHs by enzymatic oxidation

Previous studies showed that only oxidized CNTs are degraded:^[28,29] therefore, oxidized CNHs generated by lightassisted oxidation with H₂O₂ were used throughout the study, ⁷⁵ unless otherwise specified.^[37] Thermal gravimetric analysis of the oxidized CNHs (Figure S1) showed that the weight loss between room temperature and 1000°C in helium was approximately 12%, indicating the creation of abundant oxygenated functional groups, such as carbonyls and carboxylic groups on the surface.^[37] The 80 CNHs were then treated with a solution of human MPO supplemented with a low concentration of H_2O_2 (800 μ M), which is a little higher than that used in a previous study on MPOmediated CNT degradability (200 µM).^[28] The dark dispersion of the treated CNHs lightened gradually over 24 h, while the dark 85 color of the CNH-dispersion treated with H₂O₂ alone did not change during the same time period (Figure 1a). Optical absorption measurements^[38] showed that the quantity of CNHs decreased by approximately 40 wt% and 60 wt% after treatment with a combination of MPO and H₂O₂ for 5 h and 24 h, ⁹⁰ respectively (Figure 1b). Transmission electron microscopy (TEM) images of untreated CNHs (starting materials) showed that they formed aggregates of approximately 100 nm in size and had clearly visible horn-shaped tips (Figure 2a). By contrast, after enzymatic oxidation for approximately 24 h, the CNHs were 95 severely damaged and the horn-shaped tips and spherical forms had collapsed (Figures 2b-d). A large amount of non-CNH materials, probably MPO, were also observed in the samples (Figure 2c). The structures of imperfectly-degraded CNHs (Figures 2c and 2d) were similar in appearance to amorphous ¹⁰⁰ carbon or graphite-like carbon nanoparticles.^[39]

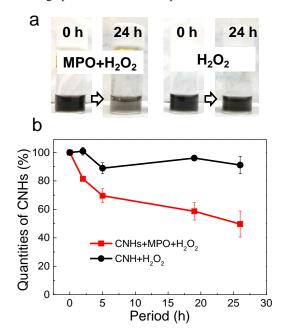


Figure 1. Human MPO-mediated degradation of CNHs. (a) Photographs of the CNH dispersions before and after treatment with a low concentration of H_2O_2 and with or without MPO. (b) The quantities of ¹⁰⁵ CNHs after treatment with H_2O_2 and with or without MPO for the

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indicated times. The quantities of CNHs were estimated based on the optical absorbance at 700 nm. Data represent the percentage of CNHs

relative to the starting concentration and are expressed as the mean \pm SD of n = 3 independent replicates.

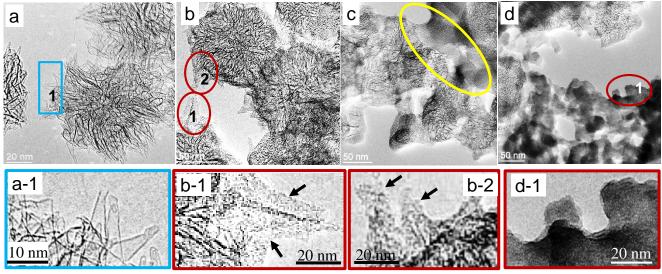


Figure 2. (a–d) TEM images of CNHs before (a) and after (b–d) enzymatic oxidation for 24 h. The inset panels (a-1, b-1, b-2, and d-1) show magnified images. The arrows indicate the structural change in the CNHs after treatment with MPO and H_2O_2 . (c) Some amorphous-like materials were probably MPO-molecules aggregates (yellow ellipse).

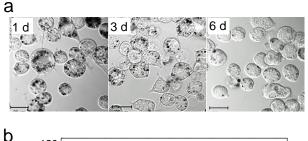
10 2.2. Degradation of CNHs in macrophage cells

Next, the cellular degradation of CNHs in mouse leukemia RAW 264.7 macrophage cells was investigated. The cells were incubated with CNHs (10 μ g ml⁻¹) for 24 h, washed with phosphate-buffered saline (PBS), and then re-seeded with CNH-¹⁵ free fresh medium for a further 9 day period (recovery period).

- Confocal microscopy differential interference contrast (DIC) images revealed that a lot of the CNHs, which appeared as black spots inside the cells, were taken up by the macrophages after the 24 h incubation (**Figure 3a**). Most of the CNHs were located in
- ²⁰ lysosomes, as confirmed by staining the cells with LysoTracker Red DND-99 dye (Figure S2), as well as by the results of our previous study.^[40] The black spots representing the CNHs disappeared gradually during the recovery period (from days 1–9) and optical absorption measurements revealed that approximately
- 25 30% of the CNHs inside the cells disappeared within this time period (**Figure 3b**).

The same process was then performed using macrophages derived from human leukemia THP-1 cells. Prior to the addition of CNHs, the cells were differentiated from monocyte to

- ³⁰ macrophage by adding phorbol 12-myristate 13-acetate (PMA) to the culture medium.^[41] After differentiation, the number of cells was stable due to a loss of their ability to replicate (**Figure S3**), which was helpful for evaluating the degradation of the CNHs. Confocal microscopy DIC analyses showed that, similar to the
- ³⁵ observations in RAW 264.7 cells, the number and size of the black particles (representing CNHs) decreased gradually over time after the THP-1 cells were incubated with CNHs for 24 h and then re-seeded with fresh CNH-free medium and observed for a further 9 days (Figure 4a). Optical absorption
- ⁴⁰ measurements revealed that approximately 30% of the CNHs inside the THP-1 cells disappeared within the 9-day observation period, which was consistent with the results obtained for RAW 264.7 cells.



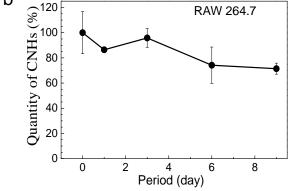


Figure 3. Degradation of CNHs in RAW 264.7 macrophages. The cells were incubated with CNHs for 24 h and then re-seeded in fresh medium and incubated for a further 1–9 days. (a) Confocal microscopy DIC images of RAW264.7 cells at days 1, 3, and 6. The black spots represent ⁵⁰ CNHs. Scale bar, 20 μ m. (b) The quantities of CNHs inside the cells on days 0–9, which were estimated based on the optical absorbance at 700 nm. Data represent the percentage of CNHs relative to the starting concentration and are expressed as the mean \pm SD of n = 3 independent replicates.

2.3. ROS generation

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After the uptake of CNHs by RAW 264.7 macrophages, we have previously reported that ROS were generated.^[40] Despite their role in oxidative stress response to nanomaterial exposure, ⁶⁰ ROS are known to be important oxidizing agents for enzymatic oxidation degradation:^[28, 42] therefore, the ROS levels in naïve

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and CNH-treated RAW 264.7 cells were compared. The ROS level in the cells incubated with CNHs ($10 \ \mu g \ ml^{-1}$) for 24 h was approximately 1.5-fold higher than that in untreated naïve cells and was stable for the 9 day observation period (**Figure 5**). The ⁵ amounts of ROS released from THP-1 cells incubated with CNHs

for 24 h or 72 h were also higher than that released by the corresponding untreated naïve cells (**Figure S4**).

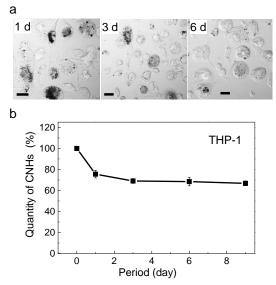


Figure 4. Degradation of CNHs in macrophages derived from THP-1 cells. The cells were differentiated by adding PMA, incubated with CNHs for 24 h, and then re-seeded in fresh medium and incubated for a further 1–9 days. (a) Confocal microscopy DIC images of THP-1 cells at days 1, 3, and 6. The black spots represent CNHs. (b) The quantities of CNHs inside the cells on days 1–9. Data represent the percentage of CNHs is relative to the starting concentration and are expressed as the mean \pm SD of n = 3 independent replicates.

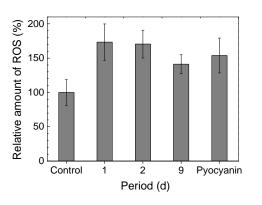
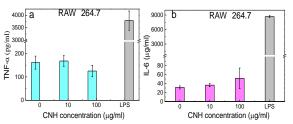


Figure 5. Generation of ROS in RAW264.7 macrophages induced by incubation with CNHs. The cells were incubated with CNHs for 24 h and ²⁰ then observed for 9 days. Naïve cells were not treated with CNHs and treatment of the cells with pyocyanin (200 μ M) was used as a positive control. Data represent the percentage of ROS relative to that in the untreated naïve cells and are expressed as the mean \pm SD of n = 3 independent replicates.

2.4. Cytokine detection

Next, the amounts of the interleukin 6 (IL-6) and tumor necrosis factor α (TNF- α) cytokines released from RAW 264.7 macrophage cells incubated with CNHs (0, 10, or 100 µg ml⁻¹)

³⁰ were measured. For both cytokines, there were no obvious differences between the amounts released by the untreated and CNH-treated cells (**Figure 6**).



³⁵ **Figure 6.** (a, b) Generation of TNF- α (a) and IL-6 (b) by RAW264.7 macrophages induced by incubation with the indicated concentration of CNHs for 24 h. Lipopolysaccharide (LPS, 20µg/ml) was used as a positive control. Data are expressed as the mean \pm SD of n = 6 independent replicates.

3. Discussion

3.1. CNHs are less susceptible to enzymatic oxidation-induced degradation than CNTs

Although some of the CNHs were degraded by MPO-catalyzed 45 oxidation in the non-cellular experiment, the degradation was incomplete; by contrast, in a previous study, CNTs were completely degraded within 24 h following a similar MPO-H₂O₂ process.^[28] In addition, although the concentrations of MPO (50 μg ml⁻¹) and H₂O₂ (800 μ M) used here were higher than those so used in the CNT study (MPO, 30 μ g ml⁻¹; H₂O₂, 200 μ M), 40% of the CNHs remained intact after 24 h. MPO generates hypochlorous acid from H₂O₂ and chlorine ions,^[41] therefore the quantity of chlorine ions is an important factor for MPO-catalyzed CNT degradation.^[28,41] Here, we used PBS containing 55 137 mM NaCl, which is higher than that used in the previous study of CNT degradation (approximately 200 µM NaCl),^[28] suggesting that the concentration of NaCl employed here should have been sufficient to promote MPO-catalyzed CNH degradation in a similar fashion to the MPO mediated CNT 60 degradation.

Because oxidized CNTs are more susceptible to degradation than non-oxidized CNTs,^[28–29] we also investigated the MPOcatalyzed degradation of CNHs that were strongly oxidized *via* pre-treatment with H₂SO₄ and HNO₃ (S-CNH) instead of being ⁶⁵ pre-oxidized with H₂O₂ as for the CNHs described in this manuscript.^[38] The strongly oxidized CNHs presented more defects and more oxygenated groups than those pre-treated with H₂O₂ (Figure S1, S5 and S6); however, MPO-catalyzed degradation of the S-CNHs was not enhanced by the strong acid ⁷⁰ pre-treatment (**Figure S7**). Taken together, these results suggest that the lower susceptibility of CNHs to enzymatic oxidationinduced degradation compared to CNTs may be due to a weaker effect of the MPO catalytic sites and/or the specific structural characteristics of CNHs.

The tyrosine residues at positions 293 and 313 of MPO, which are located at the proximal end of the heme group, are the catalytic sites of the enzyme.^[43] Simulations have moreover revealed that the potential sites of interaction of MPO with oxidized CNTs are also located at the proximal end of the MPO ⁸⁰ heme group where the carboxyl groups of CNTs interact with positively charged tyrosines 293 and 313.^[28] However, considering the molecular modeling analyses performed for CNTs ^[28] we believe that the morphology and size of CNHs would preclude their location near the catalytic site of MPO.
⁸⁵ Indeed, this interaction would likely be sterically restricted because CNHs form dense spherical aggregates that exhibit large overall curvatures with diameters of approximately 100 nm. To test this hypothesis, CNHs were mixed with 50 μg of MPO for 1–5 h, leading to a concentration of MPO attached to the CNHs of ⁹⁰ about 50–60 μg mg⁻¹ (Figure S8), which is lower than that

described previously for CNTs (180 µg mg⁻¹),^[28] suggesting that the interaction of MPO with CNHs is weaker than that with CNTs. In addition, as mentioned above, enrichment of the carboxyl groups *via* strong acid pre-treatment did not enhance the 5 degradation of the acid-treated CNHs by MPO (**Figure S7**),

- s degradation of the acid-treated CNHs by MPO (Figure S7), suggesting that the interaction between CNH and MPO, in contrast to CNTs, is not likely bound to the presence of carboxyl groups.
- The non-degraded CNHs lost their tubule structures (**Figure 2**) and were similar in appearance to that of CNHs after a 70% weight loss caused by combustion in oxygen from room temperature to 590°C,^[39] indicating that the biodegradation may occur from the periphery to the center of the aggregates. Nanohorn tubules are horn-shaped structures with diameters of
- ¹⁵ approximately 2–5 nm that have structural defects (pentagonal and heptagonal rings).^[1] The parts of CNHs with thinner diameters and defect sites are easily combusted and approximately 40% of CNHs containing graphite-like thin sheets in the centers of aggregates are difficult to combust at
- ²⁰ temperatures lower than 590°C.^[39] We propose that the easily combusted sites were enzymatically degraded early, whereas the parts that were difficult to combust accounted for the remaining (non-degraded) CNH material. This also was the reason why that the degradation rates of CNHs by MPO and H_2O_2 became very ²⁵ low after treatment for about 5 hours.

The presence of metal impurities in carbon nanomaterials might be another reason for the lower susceptibility of CNHs to degradation. CNHs do not contain any metals, whereas CNTs contain metal catalyst particles that cannot be completely ³⁰ removed. In fact, consistent with the results of a previous CNT study,^[27] the addition of FeCl₃ catalyzed the degradation of CNHs (**Figure S8**), suggesting that the presence of metallic ions may enhance the non-cellular and cellular degradation of carbon nanomaterials via a Fenton reaction.

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3.2. Causal relationship between ROS and CNH degradation ROS are a family of strong oxidizing agents that can promote CNT degradation.^[28, 42] Here, ROS were generated by RAW264.7

- cells in response to CNH exposure, and the elevated ROS levels 40 were stable for the entire 9-day observation period (**Figure 5**), which presumably sustained a continuous degradation of the CNHs for the same period as evidenced in **Figure 3**. The slight decrease in ROS levels over time could be first explained by their consumption by the enzymatic oxidation-induced degradation
- ⁴⁵ process. However, as degradation of CNHs progressed, fewer CNHs remained to induce further production of ROS, leading to a decrease of those species over time, as observed in **Figure5**, and ultimately to a reduction of the degradation process rate as in **Figure 4**. In addition, the ROS levels in the two types of
- ⁵⁰ macrophage cells used here were not high enough to induce the release of proinflammatory cytokines (**Figure 6**).

4. Conclusion

This study investigated the biodegradation of CNHs by MPO 55 catalyzed oxidation in both a non-cellular model and *in vitro* using mouse and human monocyte-derived macrophages. Approximately 60% and 30% of the CNHs were degraded by MPO catalyzed oxidation and macrophage cells, respectively. Incubation of macrophage cells with CNHs induced ROS release 60 that led to degradation of the nanomaterials but not to an

inflammatory response.

5. Experimental Section

Degradation of CNHs by enzymatic oxidation: As grown

⁶⁵ CNHs that were produced by CO₂ laser ablation of graphite without the use of metal catalysts^[1,36] underwent light-assisted oxidation with H₂O₂ to enhance their hydrophilic properties.^[37] The process used for MPO oxidation-based degradation of CNHs was similar to that described previously for CNTs.^[28] After light-⁷⁰ assisted oxidation with H₂O₂, the CNHs were dispersed in water at a concentration of approximately 1 mg ml⁻¹; this dispersion (0.3 ml) was mixed with Dulbecco's PBS (0.7 ml) (Sigma) containing MPO (50 µg) from human neutrophils (Fisher Scientific) and H₂O₂ (10 µl of 80 mM). The final concentration of H₂O₂ in the ⁷⁵ CNH suspension was approximately 800 µM. The reaction mixture was maintained at 37°C for 3 days. To replenish their

mixture was maintained at 37°C for 3 days. To replenish their levels, additional MPO (50 μ g) was added after 5 h and additional H₂O₂ (10 μ l of 80 mM) was added after 5 h, 24 h, and 30 h. The amount of CNHs in the reaction mixture was estimated based on ⁸⁰ light absorbance at 700 nm using a Lambda 1050 UV-Vis-NIR spectrophotometer (PerkinElmer Japan Co., Ltd.).^[38] The structures were observed by TEM (Topcon 002B).

Degradation of CNHs by murine RAW264.7 macrophages: Mouse leukemic monocyte macrophage RAW264.7 cells 85 (European Collection of Cell Cultures) were cultured in RPMI-1640 medium (Invitrogen) containing 10% fetal bovine serum (Gibco) and streptomycin/penicillin (Gibco) at 37°C in a 5% CO₂ atmosphere. The cells (3×10^5) were seeded in 10 ml dishes (Iwaki) and incubated for 24 h. The culture medium was then ⁹⁰ replaced with fresh medium containing CNHs (0.01 mg ml⁻¹) and the cells were incubated for a further 24 h, after which the medium was removed and a PBS rinse was performed to eliminate CNHs not taken up by the cells. The cells were then detached from the culture dishes by adding 0.25% Trypsin-95 EDTA, re-suspended in culture medium, seeded into 6-well plates (3 ml well⁻¹, 5×10^5 cells ml⁻¹), and cultured for 1–9 days. The amounts of CNHs inside the cells were estimated by optical absorption measurements.^[38] Briefly, we removed the culture

medium, and then added CelLytic M solution (1 ml) (Sigma, ¹⁰⁰ C2978) to each well. After incubation of the cells for at least 1 h, the cell dispersions were collected and ultra-sonicated (Vibra cell, Sonics Inc.) at power of approximately 300 W for 10 min. The optical absorbance of cell lysis and the culture media was then measured using a Lambda 1050 UV-Vis-NIR spectrophotometer. ¹⁰⁵ The quantities of CNHs were estimated based on the optical

absorption intensities at 700 nm using a calibration curve.^[38] Degradation of CNHs by human leukemia THP-1

macrophages: Human monocytic THP-1 cells (ATCC) were cultured in RPMI-1640 medium supplemented with 10% fetal ¹¹⁰ bovine serum, 1% L-glutamine and streptomycin/penicillin (Gibco) at 37°C in a 5% CO₂ atmosphere. To induce differentiation, the cells (2×10^6 cells ml⁻¹) were seeded in culture medium containing PMA (50 ng ml⁻¹) (Wako),^[41] which is hereafter referred to as complete medium. After incubation for ¹¹⁵ 24 h, the non-adherent cells were removed by aspiration and the adherent cells were incubated in fresh complete culture medium containing CNHs (10 µg ml⁻¹). After a further incubation for 24 h, the cells were washed with PBS and detached from the culture dishes by adding 0.25% Trypsin-EDTA. After centrifugation, the ¹²⁰ cells were re-suspended in complete medium and seeded into 6well plates (3 ml well⁻¹, 6×10^5 cells ml⁻¹). The amounts of CNHs in the cells were estimated as described for the RAW 264.7 cells.

ROS detection: The ROS detection were performed as described previously,^[44] with some minor modifications by M. ¹²⁵ Yang et al. (unpublished data). Briefly, CNH-treated RAW 264.7 or THP-1 cells were rinsed with PBS and incubated with 2',7'-dichlorodihydrofluorescein diacetate (2 ml of 10 μM) (Life Technologies) at 37°C for 30 min. The cells were then washed three times with PBS and lysed with CelLytic M reagent

containing a protease inhibitor cocktail. After centrifugation of the cell lysate at 18000 g for 10 min, the supernatants were collected and examined using a fluorescent spectrophotometer (Florolog 3, Horiba, Ltd.) at excitation and emission wavelengths

- ⁵ of 488 nm and 525 nm, respectively. The fluorescence intensity was normalized to the amount of protein, divided by that in the naïve cells, and then the values for three wells were averaged. The amount of protein in the cell lysate was measured using Bradford reagent (Sigma-Aldrich, B6916), according to the
- 10 manufacturer's instructions. As a positive control, the cells were incubated with medium (2 ml) containing pyocyanin (200 μM) for approximately 3 h.

Cytokine measurement: The cell lysates obtained from CNHtreated RAW 264.7 cells were used for cytokine measurements.

¹⁵ The IL-6 and TNF- α levels were measured using ELISA kits (Thermo Inc.), according to the manufacturer's instructions. As a positive control, the cells were incubated with medium (2 ml) containing Lipopolysaccharide (LPS, $20\mu g/ml$) for approximately 24 h.

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References

- S. Iijima, M. Yudasaka, R. Yamada, S. Bandow, K. Suenaga, F. Kokai, K. Takahashi, *Chem. Phys. Lett.* 1999, **309**, 165.
- 50 2. S. Iijima, *Nature*, 1991, **354**, 56.
- 3. S. Iijima, T. Ichihashi, *Nature*, 1993, **363**, 603.
- D. V. Kosynkin, A. L. Higginbotham, A. Sinitskii, J. R. Lomeda, A. Dimiev, B. K. Price, J. M. Tour, *Nature*, 2009, **458**, 872.
- 5. L. Jiao, L. Zhang, X. Wang, G. Diankov, H. Dai, *Nature*, 2009, **458**, 877.
- A. Jorio, G. Dresselhaus, M. S. Dressehaus, *Caron Nanotubes*, Springer, New York, USA 2008.
- P. Feazell, N. Nakayama, H. Dai, S. J. Lippard, J. Am. Chem. Soc. 2007, 129, 8438.
- 60 8. Z. Liu, X. Sun, N. Nakayama, H. Dai, ACS Nano, 2007, 1, 50.
- A. Bianco, K. Kostarelos, M. Prato, Curr. Opin. Chem. Bio. 2005, 9, 674.
- Z. Liu, K. Chen, C. Davis, S. Sherlock, Q. Cao, X. Chen, H. Dai, *Cancer Res.* 2008, 68, 6652.
- 65 11. T. Murakami, K. Ajima, J. Miyawaki, M. Yudasaka, S. Iijima, K. Shiba, *Mol. Pharm.* 2004, 1, 399.

- K. Ajima, T. Murakami, Y. Mizoguchi, K. Tsuchida, T. Ichihashi, S. Iijima, M. Yudasaka, ACS Nano. 2008, 10, 2057.
- 13. K. Yang, L. Feng, X. Shi, Z. Liu, Chem. Soc. Rev. 2013, 42, 530.
- 70 14. NWS. Kam, M. O'Connel, J. Wisdom, H. Dai, *Proc. Nat. Acad. Sci.* U. S. A. 2005, **102**, 11600.
 - M. Zhang, T. Murakami, K. Ajima, K. Tsuchida, A. Sandanayaka, O. Ito, S. Iijima, M. Yudasaka, *Proc. Natl. Acad. Sci. U.S.A.* 2008, **105**, 14773.
- 75 16. H. Moon, S. Lee, H. Choi, ACS Nano 2009, 3, 3707.
 - J. Robinson, K. Welsher, S. Tabakman, S. Sherlock, H. Wang, R. Luong, H. Dai, *Nano research*. 2010, 3, 779.
- K. Yang, S. Zhang, G. Zhang, X. Sun, S. Lee, Z. Liu, *Nano Lett.* 2010, **10**, 3318.
- 80 19. L. Yan, F. Zhao, S. Li, Z. Hu, Y. Zhao, Nanoscale, 2010, 3, 362.
 20. S. Lin, W. Thelore, M. Des, C. Caduru, A. Lin, P. Mathur,
 - 20. S. Jain, V. Thakara, M. Das, C. Godugu, A. Jain, R. Mathur, K. Chuttani, A. Mishra, *Chem. Res. Toxical.* 2011, **24**, 2028.
- 21. J. Miyawaki, T. Azami, Y. Kubo, S. Iijima, *ACS Nano*, 2008, **2**, 213.
- Z. Liu, D. Corrine, W. Cai, L. He, X. Chen, H. Dai, *Proc. Nat. Acad. Sci. U. S. A.* 2008, **105**, 1410.
- 23. J. Miyawaki, S. Matsumura, R. Yuge, T. Murakami, S. Sato, A. Tomida, T. Tsuruo, T. Ichihashi, T. Fujinami, H. Irie, K. Tsuchida, S. Iijima, K. Shiba, M. Yudasaka, ACS Nano, 2009, 3, 1399.
- 24. M. Zhang, Y. Tahara, M. Yang, X. Zhou, S. Iijima, M. Yudasaka, *Adv. Healthcare Mater.* 2014, **3**, 239.
- K. Al-Jamal, A. Nunes, L. Methven, H. Ali-Boucetta, S. Li, F. Toma, M. A. Herrero, W. Al-Jamal, H. M. Eikelder, J. Foster, S. Mather, M. Prato, A. Bianco, K. Kostarelos, *Angew. Chem. Int. Ed.* 2012, 51, 6389.
- 95 26. B. L. Allen, P. D. Kichambare, P. Gou, I. I. Vlasova, A. A. Kapralov, N. Konduru, V. E. Kagan, A. Star, *Nano Lett.* 2008, 8, 3899.
- 27. B. L. Allen, G. P. Kotchey, Y. Chen, N. V. K. Yanamala, J. Klein-Seetharaman, V. E. Kagan, A. Star, J. Am. Chem. Soc. 2009, 131, 17194.
- 100 28. V. Kagan, N. Konduru, W. Feng, B. Allen, J. Conroy, Y. Volkov, I. Vlasova, N. Belikova, N. Yanamala, A. Kapralov, Y. Tyurina, J. Shi, E. Kisin, A. Murray, J. Franks, D. Stolz, P. Gou, J. Klein-Seetharaman, B. Fadeel, A. Star, A. Shvedova, *Nature Nanotech*. 2010, **5**, 354.
- 105 29. Y. Zhao, B. Allen, A. Star, J. Phys. Chem. A, 2011, 115, 9536.
- G. P. Kotchey, Y. Zhao, V. E. Kagan, A. Star, Adv. Drug Deliv. Rev. 2013, 65, 1921.
- G. P. Kotchey, S. A. Hasan, A. A. Kapralov, S. H. Ha, K. Kim, A. A. Shvedova, V. E. Kagan, and A. Star, *Acc. Chem. Res.* 2012, 45, 110
 1770
- A. Shvedova, A. Kapralov, W. Feng, E. Kisin, A. Murray, R. Mercer, C. St. Croix, M. Lang, S. Watkins, N. Konduru, B. Allen, J. Conroy, G. Kotchey, B. Mohamed, A. Meade, Y. Volkov, A. Star, B. Fadeel, V. Kagan, *PLoS ONE*, 2012, 7, e30923.
- ¹¹⁵ 33. A. Nunes, C. Bussy, L. Gherardini, M. Meneghetti, M. A. Herrero, A. Bianco, M. Prato, T. Pizzorusso, K. Al-Jamal, K. Kostarelos, *Nanomedicine*, 2012, 7, 1485.
- Y. Sato, A. Yokoyama, Y. Nodasaka, T. Kohgo, K. Motomiya, H. Matsumoto, E. Nakazawa, T. Numata, M. Zhang, M. Yudasaka, H. Hara, R. Araki, O. Tsukamoto, H. Saito, T. Kamino, F. Watari, K. Tohji, *Scientific Reports*, 2013, 3, 2516, DOI: 10.1038/srep0216.
- V. E. Kagan, A. A. Kapralov, C. M. St. Croix, S. C. Watkins, E. R. Kisin, G. P. Kotchey, K. Balasubramanian, I. I. Vlasova, J. Yu, K. Kim, W. Seo, R. K. Mallampalli, A. Star, A. A. Shvedova, ACS Nano, 2014, 8, 5610.
 - T. Azami, D. Kasuya, R. Yuge, M. Yudasaka, S. Iijima, T. Yoshitake, Y. Kubo, J. Phys. Chem. C, 2008, 112, 1330.
 - M. Zhang, M. Yudasaka, K. Ajima, J. Miyawaki, S. Iijima, ACS Nano, 2007, 1, 265.
- 130 38. M. Zhang, X. Zhou, S. Iijima, M. Yudasaka, Small, 2012, 8, 2524.
 - M. Irie, M. Nakamura, M. Zhang, R. Yuge, S. Iijima, M. Yudasaka, *Chem. Phys. Lett.* 2010, **500**, 96.
 - Y. Tahara, M. Nakamura, M. Yang, M. Zhang, S. Iijima, M. Yudasaka, *Biomaterials*, 2012, 33, 2762.
- 135 41. E. Park, H. Jung, H. Yang, M. Yoo, C. Kim, K. Kim, *Inflamm Res.* 2007, 56, 45.

- I. I. Vlasova, A. V. Sokolov, A. V. Chekanov, V. A. Kostevich, V. B. Vasilyev, *Russian Journal of Bioorganic Chemistry*, 2011, 37, 453.
- 43. M. L. Olivier, R. O. Paul, *Biochem. Biophys. Res. Commun.* 2000, **1**, 199.
- 5 44. R. Foldbjerg, P. Olesen, M. Hougaard, D. Dang, H. Hoffmann, H. Autrup, *Toxicol. Lett.*, 2009, **190**, 156.