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Journal:	<i>ChemComm</i>
Manuscript ID:	CC-COM-03-2014-001689.R1
Article Type:	Communication
Date Submitted by the Author:	04-Apr-2014
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Cite this: DOI: 10.1039/c0xx00000x

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ARTICLE TYPE

Semiconducting Polymer Dots with Monofunctional Groups

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Received (in XXX, XXX) Xth XXXXXXXXXX 20XX, Accepted Xth

XXXXXXX 20XX

DOI: 10.1039/b000000x

This communication describes an approach for preparing monovalent semiconducting polymer dots (*m*Pdots) with size of 5nm where each *m*Pdot was composed of precisely a single active functional group.

Monovalent fluorescent probes with sizes less than 10 nm are desirable for in vitro and in vivo biological applications.^[1] Although conventional organic dyes have nanometer sizes and monovalency, they usually suffer from low absorptivity and poor photostability. These drawbacks have limited their application in high-sensitivity imaging techniques and high-throughput assays. Semiconducting quantum dots (Qdots) have been developed as brighter and more photostable probes than conventional organic dyes, but their relatively large hydrodynamic diameter and multivalency are critical constraints for biological applications.^[2] Multivalency of Qdots may result in the cross-linking of surface proteins, which can activate signaling pathways and dramatically reduce receptor mobility. As a result, much effort has been devoted in the past several years to develop monovalent Qdots with smaller sizes.^[3]

Semiconducting polymer dots (Pdots) have recently emerged as a new group of fluorescent probes which possess large absorption cross-sections, high quantum yields, and fast emission rates.^[4] The brightness of Pdots has been shown to be an order of magnitude higher than that of Qdots (e.g. 30 times) of comparable dimensions.^[4c, 4i] Moreover, several reports^[5] showed that Pdots were nontoxic to cells, an important advantage over Qdots, which can be toxic if heavy metal ions leak from the inorganic core.^[6] Finally, Pdots with sizes comparable to typical water-soluble Qdots (~ 15 nm) do not blink, which is an important feature in many single-molecule experiments.

These properties of Pdots make them excellent fluorescent probes for many biological applications. For example, they recently have been used for biological detection,^[4i] biosensing platforms,^[7] specific cellular^[4i] and subcellular targeting and imaging,^[8] bioorthogonal labelling,^[4j] protein detection^[4b] and in vivo tumor targeting.^[9] To further optimize Pdots for biological applications, the development of small and monovalent Pdots is the next critical step. Monovalent Pdots (*m*Pdots) have significant advantages over conventional multivalent Pdots because a single functional group is desirable for biological applications that are sensitive to protein/nanoparticle clustering and aggregation. For example, we

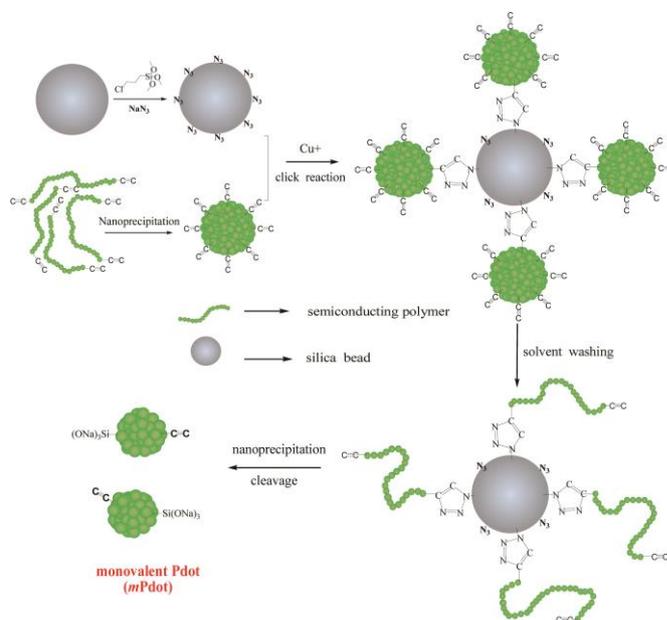


Figure 1. The procedure to prepare monovalent Pdots (*m*Pdots). A silica particle with a diameter of ~ 200 nm was prepared and its surface modified with a layer of chloride ($\text{SiO}_2\text{-Cl}$) via the hydrolysis and condensation of chloridetriethoxysilane. The $\text{SiO}_2\text{-Cl}$ groups were then modified to azide to form a clickable silica nanoparticle (ESI). Separately, regular multivalent PPV-PPA Pdots were prepared using nanoprecipitation (ESI); these Pdots had alkyne groups so they could react with the $\text{SiO}_2\text{-N}_3$ on the silica surface via click chemistry. Once the regular PPV-PPA Pdots were clicked onto the surface of the silica nanoparticle, the solvent was changed from aqueous solution to THF and the silica-polymer complex was washed in THF several times. This step removed all the polymer chains in the regular Pdot that were not covalently attached to the silica surface. The single polymer chains attached to the surface of the silica nanoparticles were then re-precipitated into small and monovalent *m*Pdots by re-introducing the silica-polymer complex to aqueous solution from THF. Finally, the *m*Pdots were cleaved from the silica surface and released into solution in the presence of NaOH and Triton 100. To remove NaOH and Triton 100, the *m*Pdot solution was dialyzed overnight in water or buffer.

reported a technique for counting protein copy numbers in synaptic vesicles and subcellular organelles^[10] using fluorescent antibodies and single-molecule counting. For these applications, it is imperative that the fluorescent labels do not have excess functional groups that may cause cross-linking and accumulate multiple antibodies per fluorescent label.

Additionally, small Pdots (<10 nm in diameter) are desirable for certain applications. For example, we have recently developed two types of small Pdots (~9 nm), a compact yellow emitting CN-PPV Pdot^[8] and a cross-linked Pdot.^[11] We found

that these small Pdots were able to label subcellular features more efficiently than larger Pdots (~ 15 nm). For example, microtubules labelled with large Pdots tend to appear spotty in a confocal fluorescence image,^[41] while those same microtubules appear crisp and resolved when labelled with small Pdots.^[8,11] Small Pdots also are less prone than large Pdots to alter the diffusional and biological activity of the biomolecules that they label, and small Pdots can access size-restricted cellular regions, such as synapses. To meet these demands for the next generation of Pdots with monovalent functional group and small size, this paper describes an approach based on surface attachment and washing for generating *m*Pdotes.

The strategy we developed to prepare *m*Pdotes is shown in Fig. 1. Here, we first form Pdots that have multiple polymer chains and are multivalent. We then attach the Pdots onto the surface of silica beads using Click chemistry. Once the Pdots are attached to the bead surface via a functional group (i.e. alkyne group), we wash the bead-Pdot with THF, which causes the Pdot to unfold and the entangled chains to fall apart, leaving a single chain of polymer attached to the bead. Re-introduction of aqueous solution causes the chain to re-collapse to form a single-chain Pdot, and subsequent release of the Pdot from the bead surface results in a monovalent Pdot (ESI).

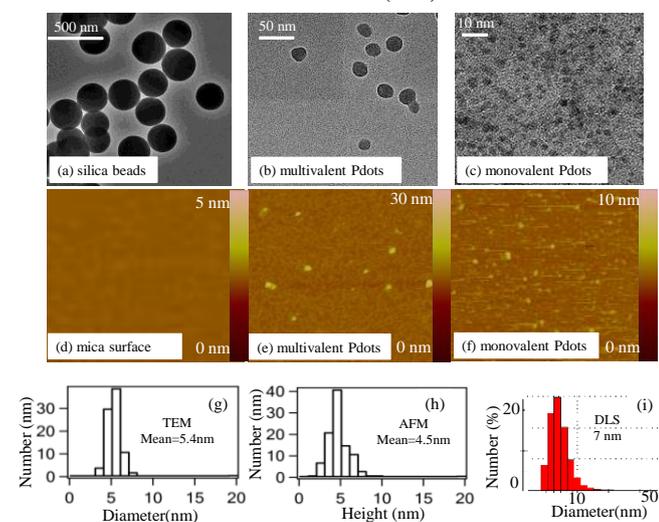


Figure 2. Size distribution of *m*Pdotes measured with TEM, AFM, and DLS. (a) TEM image of silica beads showing a diameter of ~ 200 nm. (b) TEM image of regular PPV-PPA Pdotes, which had an average diameter of 34 ± 4 nm, from measurements on 80 Pdotes. (c) TEM image of PPV-PPA *m*Pdotes. (d) AFM image ($1 \mu\text{m} \times 1 \mu\text{m}$) of 3-aminopropyltriethoxysilane (APTEOS)-coated mica surface without any nanoparticles. (e) AFM image ($0.6 \mu\text{m} \times 0.6 \mu\text{m}$) of multivalent regular PPV-PPA Pdotes. (f) AFM image ($1.2 \mu\text{m} \times 1.2 \mu\text{m}$) of PPV-PPA *m*Pdotes. (g) Size distribution of *m*Pdot shown in (c); average diameter was 5.4 ± 0.5 nm from images of 88 *m*Pdotes. (h) Height distribution of *m*Pdotes measured with AFM; average value was 4.5 ± 0.4 nm from measurements on 100 *m*Pdotes. (i) DLS result of *m*Pdotes in aqueous solution showing a hydrodynamic diameter of 7 nm.

To implement the above strategy, we designed and synthesized a green emitting semiconducting polymer (alkyne terminated linear poly(p-phenylenevinylene) derivative containing two pendent pentaphenylene (PPV-PPA)). The PPV-PPA polymer had only two terminating alkyne click-functional groups (Fig. S1 and S2). And because there was only two alkyne groups in the initial PPV-PPA polymer chain, during the

preparation process one of the two alkyne groups was used to covalently bind to the silica surface, and later converted to the terminated $\text{Si}(\text{ONa})_3$ group after NaOH cleavage when single chain PPV-PPA was formed. Therefore, there is only one alkyne group left in the single chain PPV-PPA Pdot, resulting in an *m*Pdot with a monovalent alkyne group.

Figure 2 shows the size information for the silica beads, regular PPV-PPA Pdotes, and PPV-PPA *m*Pdotes. As established by transmission electron microscopy (TEM), the silica bead ($\text{SiO}_2\text{-N}_3$) had a diameter of ~ 200 nm and the regular PPV-PPA Pdot had a 32-nm diameter (Fig. 2a & 2b). A representative TEM image of the *m*Pdotes (Fig. 2c) shows that the mean diameter was 5.4 ± 0.5 nm (from 88 *m*Pdotes measured; Fig. 2g). Atomic force microscopy (AFM) measurements reported similar results (Fig. 2f); the mean height of *m*Pdotes was 4.5 ± 0.4 nm (from 100 *m*Pdotes imaged) (Fig. 2h). DLS showed the hydrodynamic diameter of *m*Pdotes was 7 nm (Fig. 2i). These three measurements are consistent because the lateral dimension of the collapsed *m*Pdot imaged in TEM should be slightly larger than the height of the collapsed *m*Pdot measured with AFM. The hydrodynamic size is ~ 1 -2 nm larger than TEM and AFM measurements as anticipated because of slight swelling of *m*Pdotes in aqueous solution. The molecular weight of PPV-PPA we synthesized was 86,000 g/mol. For a single chain of PPV-PPA that is fully collapsed into a Pdot with a density of ~ 1.0 g/cm³, the resulting *m*Pdot would have a diameter of ~ 6 nm, consistent with the results from both the TEM and AFM experiments.

Our PPV-PPA *m*Pdot had a linear chain polymer with a $\text{Si}(\text{ONa})_3$ group on the end of the polymer attached to the silica surface and an alkyne group on the other end. To validate that each *m*Pdot had only a single alkyne functional group, we followed the established approach described in the literature for confirming monovalency of nanoparticles,^[12] and carried out two experiments. In the first experiment, we introduced a linker with two azide groups to crosslink *m*Pdotes. Figure 3a shows the linker (PEG7-BIS-Azide). If *m*Pdot was monofunctional, then after crosslinking, we expect to see dumb-bell structures (Fig. 3a). If the *m*Pdotes had more than one alkyne group, then we should see aggregates of *m*Pdotes.

Indeed, regular PPV-PPA Pdotes aggregated after the addition of linkers in the presence of freshly prepared copper sulfate (0.5 mM) and L-sodium ascorbate (0.2 mM) needed to initiate the click reaction. Before the addition of linker, there was no aggregation, which indicated the aggregation of regular Pdotes was only caused by the cross-linking of Pdotes triggered by multiple click reactions among the Pdotes with multiple alkyne groups. In contrast, when *m*Pdotes were used for the same experiment, we observed dumb-bell features (Fig. 3c). As a control, Figure 3b shows a typical image of *m*Pdotes when no linker was added but in the presence of 0.5 mM copper sulfate. Figure 3d displays the populations (singular, dumb-bell, or aggregates) of *m*Pdotes we observed in the absence and presence of linker: $\sim 96\%$ of *m*Pdot was singular when no linker was present (Fig. 3b), but when linker was added, only $\sim 23\%$ of *m*Pdot remained singular and $\sim 75\%$ of *m*Pdotes formed dumb-bell structures (Fig. 3c). It should be noted that the percentage of dumb-bell structures ($\sim 75\%$) formed by *m*Pdotes are similar to that of dumb-bell structures formed by mono functional gold^[12b, 12c] or

aggregations.^[13] Figure 5e shows the populations of *m*Pdot (singular, dumb-bell, or aggregates) in the AFM images : ~ 94% of multivalent Pdots was observed to form aggregates in the presence of Cu²⁺, but for *m*Pdots in the presence of Cu²⁺, they formed dumb-bell structures instead (60%). Some *m*Pdots remained singular (38%), likely because Cu²⁺ is not as strong a cross linker and the stability of two Pdots linked by a single Cu²⁺ ion is rather low and prone to disruption. In fact, Cu²⁺ attached to a single carboxyl group is not stable and two carboxyl groups are required to form a stable complex, which also explains why having more Cu²⁺ than *m*Pdots in solution did not prevent formation of dumb-bell structures. From these experiments, the strong contrast in the behavior of regular multivalent Pdots and *m*Pdots is evident.

Finally, we investigated the stability of *m*Pdots in different buffer solutions. Figure S4 showed the normalized fluorescence intensity of *m*Pdots in different buffers (including TRIS, TBE, PBS and HEPES buffer) as a function of time. The result indicated that the fluorescence of the *m*Pdots buffer solution did not change over a period of three days. Because any aggregation of Pdots would result in a decrease in the measured fluorescence intensity due to self quenching,^[14] this result confirmed the Pdots are well dispersed and stable over this period, which is suitable for biological applications.

In conclusion, we have developed a method for preparing monovalent and very small Pdots. We carried out two experiments to show that *m*Pdots only had a single functional group. When the *m*Pdots were crosslinked, they formed dumb-bell structures as seen by AFM. We generated clickable *m*Pdots as well as *m*Pdots with a single carboxyl group, which could be used for covalent attachment of a broad range of biological molecules. The importance of having monovalency has been illustrated in the literature for other nanoparticles. For example, monovalent nanoparticles have been shown to label glutamate receptors at neuronal synapses without activating EphA3 tyrosine kinase^[3b] while polyvalent nanoparticles result in activation. Monovalent nanoparticles have also been shown to offer improved quantification in tumor targeting and imaging,^[3a] and better performance in the tracking of individual proteins in live cells.^[15] The development of the very small and monovalent *m*Pdots, coupled with the high brightness of Pdots as we have previously demonstrated,^[4c, 4i] is expected to advance their adoption as a useful fluorescent probe in biomedical applications. You can also put lists into the text

Notes and references

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† Electronic Supplementary Information (ESI) available: materials, characterization and Pdots preparation. See DOI: 10.1039/b000000x/

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