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ARTICLE TYPE

Switching an O₂ sensitive glucose oxidase bioelectrode into an almost insensitive one by cofactor redesign

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In the 5-8 mM glucose concentration range, of particular interest for diabetes management, glucose oxidase bioelectrodes are O₂ dependent. Thereby decreasing their ¹⁰ efficiencies. By replacing the natural cofactor of glucose

oxidase, we succeeded in turning an O_2 sensitive bioelectrode into an almost insensitive.

Glucose oxidase (GOx) is one of the most frequently used enzymes in enzymatic biofuel cells and glucose biosensors ¹⁻⁴, ¹⁵ due in part to its high stability in physiological conditions (neutral pH, 37°C, in presence of NaCl) and its narrow substrate specificity towards glucose. In numerous electrochemical devices, redox mediators (M) are used to electrically connect the GOx active site (FAD/FADH₂) to the electrode. These ²⁰ compounds are able to oxidize the reduced form of GOx and

shuttle electrons to the electrode surface. (eq 1)

$$GOx\text{-}FADH_2 + (2/x) \text{ } M_{(OX)} \rightarrow GOx\text{-}FAD + (2/x) \text{ } M_{(RED)} + 2 \text{ } H^+ \qquad (1)$$

 $_{25}$ (where x = 1 or 2 is the number of electrons collected by the oxidized redox mediator from the GOx)

However, this process is intrinsically limited by the competition with molecular oxygen, which is the natural substrate for the oxidative half-reaction. (eq 2)⁵ In addition, O₂ may also

³⁰ interact with the reduced form of the redox mediator if its redox potential is not chosen properly. ⁶

$$GOx-FADH_2 + O_2 \rightarrow GOx-FAD + H_2O_2$$
(2)

- ³⁵ Minimizing the competitive oxidation by O₂ is a long standing issue of bioelectrochemists and efforts have been essentially directed to the design of new redox mediators or the improvement of enzyme immobilization.⁷⁻¹¹ The use of oxygen-tolerant enzymes such as cellobiose dehydrogenase or FAD-Glucose ⁴⁰ dehydrogenase is also a promising alternative. ¹²⁻¹⁴
- In their pioneering work to decipher the electron transfer in GOx from *Aspergillus niger*, Klinman et al ^{15, 16} showed that the Michaelis–Menten constant, K_M (O₂), was dramatically increased for enzymes containing modified flavins and was attributed to a
- ⁴⁵ change in the driving force for outer sphere electron transfer. The rate constants, k_{cat}/K_M (O₂), for native glucose oxidase was $(1.6 \pm 0.2) \times 10^6 \text{ M}^{-1} \text{ s}^{-1}$ and $(7.5 \pm 1.6) \times 10^4 \text{ M}^{-1} \text{ s}^{-1}$ for a GOx modified with a flavin analogue; 7,8-dichloro-FAD.

Inspired by this work, we elaborated a GOx bioelectrode $_{50}$ where the native flavin has been replaced by a flavin analogue and studied electrochemically the effect of such substitution on the oxidation of glucose under O₂ et Ar.

As illustrated in Scheme 1, 6 steps are required to obtain GOx ⁵⁵ where the native flavin has been replaced with 7,8-dichloro-FAD. All experimental details can be found in supporting information and have been adapted from previous reports to simplify the methodology and improve the yield of production.¹⁷⁻¹⁹ Briefly, we first optimized and reported a two-step protocol for the ⁶⁰ synthesis of 7,8-dichloro-riboflavin with a 2.5-fold increase in yield compared to previous five-step protocol methods (step 1).²⁰ After overexpression, production and purification of Holo-FAD synthetase (step 2), apo-FAD synthetase is prepared (step 3) and mixed with 7,8-dichloro-riboflavin in presence of an excess of ⁶⁵ ATP and MgCl₂, leading to the formation of 7,8-dichloro-FAD (step 4). Apo-glucose oxidase (step 5) is finally reconstituted with 7,8-dichloro-FAD (step 6) leading to the formation of FADCl₂ with a yield of ~ 49%.



Scheme 1. Preparation of FADCl₂ - Glucose Oxidase. 1) synthesis of 7,8-dichloro-riboflavin; 2) production/purification of FAD-synthetase; 3) preparation of apo-FAD synthetase; 4) preparation of 7,8-dichloro-FAD;
5) preparation of apo-glucose oxidase; 6) reconstitution of glucose oxidase with 7,8-dichloro-FAD.

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	Protein	$k_{\rm cat}$	$K_{\rm M}({\rm FM}_{\rm ox})$	K _{Mapp} (FMox)	$k_{\rm cat}/K_{\rm M}({\rm FM_{ox}})$	$k_{\rm cat}/K_{\rm Mapp}({ m FM}_{ m ox})$	<i>K</i> _M (glucose)	$k_{\rm cat}/K_{\rm M}$ (Glucose)
5		(sec^{-1})	(µM)	(µM)	$(\mu M^{-1} \text{ sec}^{-1})$	$(\mu M^{-1} sec^{-1})$	(mM)	$(\mathrm{m}\mathrm{M}^{-1}\mathrm{sec}^{-1})$
	WT-GOx (Ar)	822 ± 9	132 ± 6		6.2 ± 0.3		51 ± 7	16 ± 2
	WT-GOx (O ₂)	689 ± 20		250 ± 27		2.7 ± 0.3	54 ± 11	12 ± 3
10	FADCl ₂ -GOx (Ar)	1602 ± 32	118 ± 10		13.6 ± 0.2	11.9 ± 0.4	37 ± 2	43 ± 3
20	FADCl ₂ -GOx (O ₂)	1505 ± 53		126 ± 38			35 ± 3	43 ± 5

 Table 1. Kinetics parameters (per active site) of native and FADCl2 - Glucose Oxidase with glucose and ferrocinium-methanol as substrates in presence or absence of O2

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Steady state kinetic parameters of the new GOx-FADCl₂ (-0.126 V *vs.* NHE) were evaluated with ferrocinium-methanol (FM_{ox}) under Ar and O₂ and compared to the wild type GOx (Table 1). Contrary to native GOx from *P. amagasakiense*, we

- ³⁰ did not observe any competitive or uncompetitive inhibition of O₂ in presence of FM_{ox} in our experimental conditions.²¹ The reason has yet to be determined. As seen in Table 1, whether under Ar or O₂, GOx-FADCl₂ is more active than the native GOx: its $k_{cat} \sim 2.2$ times higher, K_M (glu) ~ 1,5 times lower and k_{cat}/K_M (Glu) is 3.5 ³⁵ higher; indicating a more efficient glucose oxidation compared to
- ³⁵ might²⁷, indicating a more efficient glucose oxtuation compared to native GOx. The ratio $(k_{cat}/K_{Mapp}(FMox))O_2/(k_{cat}/K_M(FMox))Ar$ for native GOx is ~ 0.44 and ~ 0.88 for GOx-FADCl₂ clearly showing that GOx-FADCl₂ is less sensitive to O₂. The better efficiency is also evidenced by the similar values of $K_M(FMox)$ ⁴⁰ and $K_{Mapp}(FMox)$ for GOx-FADCl₂, indicating that the redox

mediator is the main substrate for the oxidative half-reaction instead of O_2 .

Modified electrodes at their optima enzyme/redox ⁴⁵ polymer/cross-linker ratio were prepared as previously reported. ²² The redox polymer is a PVP –[Os(1,1'-dimethyl-2,2'biimidazole)₂-2-[6-methylpyrid-yl]imidazole)] ^{2+/3+} with a redox potential of -30mV and insensitive to O₂.²³ The ratio was identical for both enzymes and each electrode consisted of 35 ⁵⁰ wt% enzyme, 55 wt% redox polymer and 10 wt% of PEGDGE for a total dry loading of 200 µg.cm⁻².



Fig 1. Cyclic voltammograms of modified electrodes with native GOX (thin line) or FADCl₂-GOX (dotted line) in absence (A) or presence (B) of 100 mM glucose. 35 wt% enzyme, 55 wt% redox polymer and 10 wt% of 65 PEGDGE for a total dry loading of 200 μg.cm⁻². 20 mM phosphate buffer, 140 mM NaCl, pH 7, 37 °C, 1000 rpm and 100 (A) or 5(B) mV.s⁻¹.

Fig 1A shows the resulting cyclic voltammograms under Ar for the native GOx (black line) and GOxFAD-Cl₂ (dotted line) 70 obtained at 100 mV.s⁻¹ in a 20 mM sodium phosphate buffer pH 7.2+140 mM NaCl. Those CVs are characteristics of a polymer bound osmium complex with an apparent redox potential of - 30 mV vs. Ag/AgCl. Peak heights, peak separation between the oxidation and reduction and the width of the peaks at half-height 75 are identical for both electrodes. It suggests a similar structure/morphology of both hydrogels and a similar apparent diffusion coefficient of electrons.²² The electrocatalytic oxidation of 100 mM glucose under Ar obtained at 5 mV.s⁻¹ is seen in Figure 1B. A current density of 2.5 mA.cm⁻² is reached for the ⁸⁰ native GOx (black line) and 3.1 mA.cm⁻² for the FADCl₂ electrode (dotted line). The onset for glucose oxidation is slightly shifted toward more anodic potential because of the difference between the redox potential of both enzymes. It also explains the difference in current densities which are related to some extent to 85 the difference between the redox potential of both enzymes and the redox polymer, as already observed for other systems.^{23, 24} To maximize the effect of O2 at low glucose concentration (<10 mM), we performed our experiments under 1 atm O₂, forced convection and used an hydrogel film of intermediate thickness.²⁵ 90 Because reproducibility is a key issue in those experiments, we tested two different protocols of measure. In the first one, calibration curves were first recorded under Ar at +0.3 V vs. Ag/AgCl with at least two electrodes, which were then washed with buffer and tested under O2. This protocol was also repeated

⁹⁵ with other electrodes in the reverse order. In the second protocol, each experiment started in a buffer saturated with Ar and after each addition of glucose the solution was bubbled with O₂ until the current reached a baseline. It was then bubbled again with Ar before the next addition of glucose. This last protocol gave the ¹⁰⁰ best results in terms of reproducibility (± 10 % vs. ± 25 %) and was therefore used. One example is illustrated in Fig 2 in presence of 0.5 mM glucose. (Fig 2A) and 5 mM glucose. (Fig 2B) for

0.5 mM glucose (Fig 2A) and 5 mM glucose (Fig 2B) for electrodes modified as in Figure 1.

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electrodes with native GOx (thin line) or FADCl₂-GOx (dotted line) in presence of 0.5 mM glucose (A) or 5 mM glucose (B). The arrows show the beginning of the corresponding gas bubbling. Other conditions as in 15 Fig 1

At low glucose concentration, both modified electrodes display the same current density. When O₂ was bubbled, the current density of the electrode modified with the native GOx decreased by 60 % (thin line) but only by 13% for the modified GOx 20 (dotted line). At 5 mM (Fig 2B), the decrease was respectively 52 % and 18% for the native and modified GOx. Resulting calibration curves for native GOx (triangles) and GOx-FADCl₂ (circles), under Ar (black symbol) and O₂ (empty symbols), are

plotted in Fig 3. For both modified electrodes, the current density ²⁵ increased with the glucose concentration up to 50 mM and displays a typical shape for GOx-based electrodes. ²⁵ Fig 3B shows the normalized data of Fig 3A.

current density /mAacm⁻² 2.5 2 J 0,/J Ar 0,6 1.5 0.4 0.5 0,2 0.5 В 10 5 0 20 30 40 50 10 0 10 20 30 40 50 [glucose] /mM [glucose] / mM 35

Fig 3. A) Calibration curves of modified electrodes made with native GOx (triangles) or FADCl₂-GOx (circles) under O₂ (empty symbols) and Ar (full symbols). Measured at +0.3 V vs. Ag/AgCl. B) Dependence of the normalized current density on the glucose concentration for electrodes
⁴⁰ modified with native GOx and polymer I (triangles) and FADCl₂-GOx and polymer I (circles). Inset: Zoom in the 0-10 mm glucose concentration range. Other conditions as in Fig 1

For the lowest glucose concentration (<1 mM), the effect of O₂ is maximal for both electrodes. All the electrons generated by the ⁴⁵ oxidation of glucose are captured by O₂ either directly from the GOx or from the reduced osmium complex (when an O₂-sensitive mediator is used).^{6, 25} It explains the same current observed for both electrodes. For higher glucose concentration (>20 mM), most of the O₂ is consumed in the outer layers of the hydrogel

- ⁵⁰ and its impact is therefore limited on the current density. As a result, JO_2/JAr is identical for both electrodes (Figure 3B). In the 0.5-20 mM glucose concentration range, the current density for the GOx-FADCl₂ modified electrode (circles) is higher because the enzyme is more active and less sensitive to O_2 . Most of the ⁵⁵ electrons generated during the oxidation of glucose are
- $_{55}$ electrons generated during the oxidation of glucose are transferred to the redox mediator and not to O_2 . It is also

evidenced by the values of the apparent Michaelis–Menten constants (K'_M) which are almost identical under O_2 or Ar, $(K'_M)_{Ar}$ (9.8 mM) and $(K'_M)_{O2}$ (11.8 mM). For the native GOx ⁶⁰ (triangles), however, K'_M increases upon increasing the partial pressure of O_2 from $(K'_M)_{Ar}$ (6.71 mM) to $(K'_M)_{O2}$ (18.8 mM); because O_2 competes with the redox mediator for electrons. A greater glucose concentration is then required to reach half of the maximal catalytic current. This trend is in agreement with the ⁶⁵ data of table 1.

Conclusions

For the first time, we report the use of unnatural GOx from *Aspergillus niger* for the electrochemical detection of glucose. By replacing the native FAD by an unnatural flavin, 7,8-dichloro-

⁷⁰ FAD, we succeeded in switching an O_2 sensitive electrode into an almost insensitive. The novel GOx is not only more active than the native GOx but also less sensitive to O_2 . In the 5-8 mM glucose concentration range, of particular interest for diabetes management, an electrode made with a native GOx loses 60 % of ⁷⁵ its current under O_2 , while only 15% with the new electrode.

Large quantities of apo GOx lacking FAD can now be isolated and reconstituted with unnatural flavins with high yields. This strategy may offer a promising alternative to more classical methods such as directed mutations and may be extended to other 80 electrochemical enzymatic systems.

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Notes and references

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† Electronic Supplementary Information (ESI) available: production and 90 purification of the differents enzymes. See DOI: 10.1039/b000000x/

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