REVIEW

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Self-assembling protein cages: from coiled-coil module to machine learning-driven *de novo* design of next-generation biomaterials

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The rational design of self-assembling protein nanocages holds great promise for synthetic biology, biotechnology and biomedical applications. Protein nanocages are well-defined nanoparticles with an inner cavity formed by self-assembly of repetitive protein building blocks. These cavities can be tailored to encapsulate and protect cargo molecules such as drugs, enzymes, or imaging agents. The ability to design *de novo* protein cages has recently been revolutionized by new concepts of modular protein design, computational design of interacting surfaces and machine learning-based generative protein design. Protein cages can be designed in diverse architectures and sizes, and their assembly and disassembly can be regulated by chemical, biological, and physical signals. Here, we focus on the review of engineering strategies for the designed protein cages based on coiled coils or other modular protein domains, their functionalization and opportunities of customized engineered protein cages.

1. Introduction

The emergence of self-assembling protein nanostructures has opened new avenues in biomaterials, with applications spanning nanomedicine, drug delivery, vaccine development, enzymatic catalysis, and synthetic biology. Ranging from 10 to 200 nm in diameter, these nanocages possess internal cavities that could be used to encapsulate therapeutic molecules and reactive sites amenable to functionalization. Naturally occurring protein cages such as virus-like particles (VLPs), ferritin, heat-shock proteins, and chaperonins have been repurposed for biomedical and biotechnological applications, owing to their well-defined architectures and biocompatibility.[1,2] These systems offer valuable insights into how symmetry, interface complementarity, and non-covalent interactions contribute to

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the stability of multimeric assemblies. Inspired by these natural systems, synthetic nanocages have been designed by precisely arranging protein subunits into diverse shapes and enabling the controlled encapsulation and targeted delivery of diverse molecular cargoes.[3,4]

De novo design strategies allow the construction of user-defined protein nanocages with tailored geometries and functional surfaces. In recent years, approaches have relied on a combination of computational tools that operate at different stages of the design process. Rosetta provides a versatile framework for backbone remodeling and sequence optimization, with specialized protocols such as HBNet enabling the design of stabilizing hydrogen-bond networks at protein–protein interfaces.[5,6] However, the most critical advances in nanocage design have come from the development of symmetry-aware rigid-body docking platforms, with RPXDock unifying and extending earlier methods such as tcDock, sicDock, and sicAxel.[7–11] These algorithms systematically sample symmetric configurations of protein subunits, allowing the construction of highly ordered architectures with precise control over symmetry and assembly.[7–11] In parallel, recent advances in machine learning-based generative design have streamlined and accelerated de novo protein design workflows, complementing established physics-based methods such as Rosetta and enabling more efficient exploration of diverse scaffold geometries.[12–15]

Depending on the design strategy, protein nanocages fall into four main categories: assemblies based on genetic fusion of natural oligomeric proteins; structures derived from computational interface design; geometries built using coiled-coil modules and machine learning-based generative protein cage design. In the genetic fusion approach, naturally oligomerizing protein domains are connected via rigid helical linkers to produce symmetric complexes.[16–18] Computationally designed interfaces offer excellent control and precision, enabling the assembly of complex symmetrical cages from one or several different protein components.[6,19–21] A transformative advance

in this approach has been provided by machine learning/artificial intelligence (ML/AI). Tools such as ProteinMPNN enable rapid optimization of interface residues and large-scale sequence screening, supporting the design of megadalton-scale nanocages with improved assembly efficiency, stability, and solubility.[13–15] While diffusion-based backbone generators are promising in other areas of protein design, their application to protein cage-level backbone generation remains limited and is under active development.[12,22,23]

Parallel to these developments, coiled-coil domains have emerged as a powerful modular platform for designing nanocages. The modularity and orthogonality of coiled-coil interactions enable precise control over nanocage geometry, size, and responsiveness.[24,25] A highly useful tool is the CoCoPOD (coiled-coil protein origami design) platform, which uses orthogonal coiled-coil dimers and higher oligomeric modules arranged in a defined order to fold into single-chain polyhedral cages.[26] Recent advances in computational modeling and protein engineering have expanded the capabilities of coiled-coil nanocages, enabling direct programming of folding pathways through stimuli-responsive modules. These modules are engineered structural elements that undergo conformational changes or trigger assembly and disassembly in response to specific environmental cues, such as pH, metal ions, redox conditions, temperature, or light. By incorporating such features, one can achieve dynamic and reversible control over nanocage formation, resulting in highly adaptable and customizable architectures suited for responsive biomedical applications.[27,28]

This review highlights recent advances in the rational and computational design of protein nanocages, particularly coiled coil-based modular architectures. We explore their applications in drug delivery, immunotherapy, and diagnostics, and discuss current challenges, including immune compatibility and stability. As design strategies continue to integrate synthetic biology and AI-guided optimization, protein nanocages are set to

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become central components in the future of biomolecular engineering and therapeutics.

2. Designed protein cages

Non-natural protein nanocages are at the forefront of nanomedicine, providing innovative solutions for targeted drug delivery, gene therapy, vaccine development, and biocatalysis.[1,29–34] Computational tools for the design of protein nanocages have greatly enhanced their potential as molecular carriers capable of encapsulating a variety of therapeutic agents, including nucleic acids, and proteins.

In the design of protein nanocages, symmetry defines the overall architecture, while the final dimensions also depend on the number and size of the constituent components. The overall stability of the nanocage, however, depends not only on the detailed molecular interactions at the interfaces but also on the degree of cooperativity imposed by the underlying symmetry. The seminal studies from the Yeates group[16,35–37] provided both theoretical and experimental insights into the critical role of symmetry in building protein nanocages. Readers are encouraged to refer to these studies for a deeper understanding of symmetry principles in molecular design. However, in this review, we primarily focus on recently developed nanocages intended for therapeutic applications. We review two main groups of synthetic nanocages: (1) assembled from modular oligomeric protein domains, and (2) constructed using coiled-coil modules.

2.1 Nanocages based on modular oligomeric proteins

The structural and compositional features of protein nanocages assembled from modular oligomeric domains span a broad spectrum of architectures. Beginning with early symmetry-based designs from the Yeates group and later expanded by the Baker and King groups, the field has advanced toward more complex assemblies through programmed symmetry breaking. This strategy, related to concepts such as pseudo-symmetry and quasi-equivalence, introduces slight variations between subunits to enable deviations from perfect symmetry and supports the construction of larger and more versatile nanocages. These nanocages, typically ranging from 10 to 90 nm in size, are categorized here according to five dominant design methodologies: (1) genetic fusion of oligomerizing domain-based protein cages, (2) interface design-based *de novo* protein cages, (3) regulated cage assembly through interface interactions, (4) directed evolution-based redesign of protein nanocages, and (5) designs guided by ML/AI.

2.1.1 Genetic fusion of oligomerizing domain-based protein cages. Genetic fusion takes advantage of natural oligomerization interfaces, making it possible to build complex assemblies without needing an extensive interface redesign. A major strength of this method is that it provides precise control over the assembly process, facilitating the construction of stable and symmetric structures. A classic example comes from the work of Padilla, Colovos, and Yeates in 2001, who

fused trimeric bromoperoxidase (PDB ID: 1BRO) with the dimeric M1 matrix protein (PDB ID: 1AA7) using a nine-residue α-helical linker. This design formed a ∼15 nm tetrahedral protein cage (Fig. 1A).[16] The structure was initially validated through electron microscopy and dynamic light scattering, and later confirmed by X-ray crystallography at a 3.0 Å resolution (Fig. 1A).[17] Building on these early designs, Lai and colleagues (2014) used a similar strategy to create a porous cubic cage by fusing different oligomeric proteins. Interestingly, they also observed alternative assemblies, including a 12-subunit tetrahedron and an 18-subunit triangular prism, depending on the conditions.[37] The strategy was pushed even further by Cannon *et al.* who created even larger icosahedral cages (∼30 nm in diameter) by combining trimeric, pentameric, and dimeric building blocks (Fig. 1B).[18] Despite its advantages, the genetic fusion approach faces notable challenges. The precise alignment of fused domains is essential, linker properties must be carefully optimized, and the pool of compatible oligomeric building blocks remains limited. Interestingly, recent advances in computational tools such as WORMS have addressed several key limitations. By computationally sampling rigid-body fusion geometries between oligomeric building blocks and enforcing symmetry constraints, it enables the design of highly ordered, multimeric protein assemblies without the need for flexible linkers or extensive interface redesign. This systematic and modular approach significantly expands the range of accessible geometries and sizes, and has now been extended to *de novo* building blocks using both physics-based and machine learning-guided fusion strategies.[38–41]

2.1.2 Protein cages guided by the interface design. Computational methods such as Rosetta, RPXDock, sicDock, and tcDock enable the exploration of symmetric oligomeric configurations, while interface design is performed through sequence-optimization protocols within Rosetta.[7–11,20,42] These methods have resulted in several successful examples of *de novo*-designed protein nanocages. The computational design of self-assembling protein nanomaterials with atomic-level precision was first demonstrated in 2012 through the *de novo* construction of tetrahedral (T3-08, T3-10) and octahedral (O3-33) nanocages from a single trimeric protein building block using RosettaDesign and Foldit (Fig. 2A).[5] This work was later expanded by designing tetrahedral assemblies (T33 and T32) based on two distinct protein components (Fig. 2B).[9] Further to address the solubility limitations of these computationally designed cages, Yeates and colleagues designed tetrahedron nanocages (T33-51 and T33-53) using Rosetta's HBNet protocol to stabilize assemblies through engineered hydrogen-bond networks.[6,43] A significant advancement was achieved with the design and experimental characterization of megadalton-scale, two-component icosahedral protein cages (I53, I52, and I32), with diameters ranging from 24 to 40 nm (Fig. 3A–C).[44] These structures were generated using symmetry-guided modeling, a strategy that employs defined geometric rules to direct the self-assembly of protein subunits into complex architectures and it was worth noting that the I52 and I32 architectures
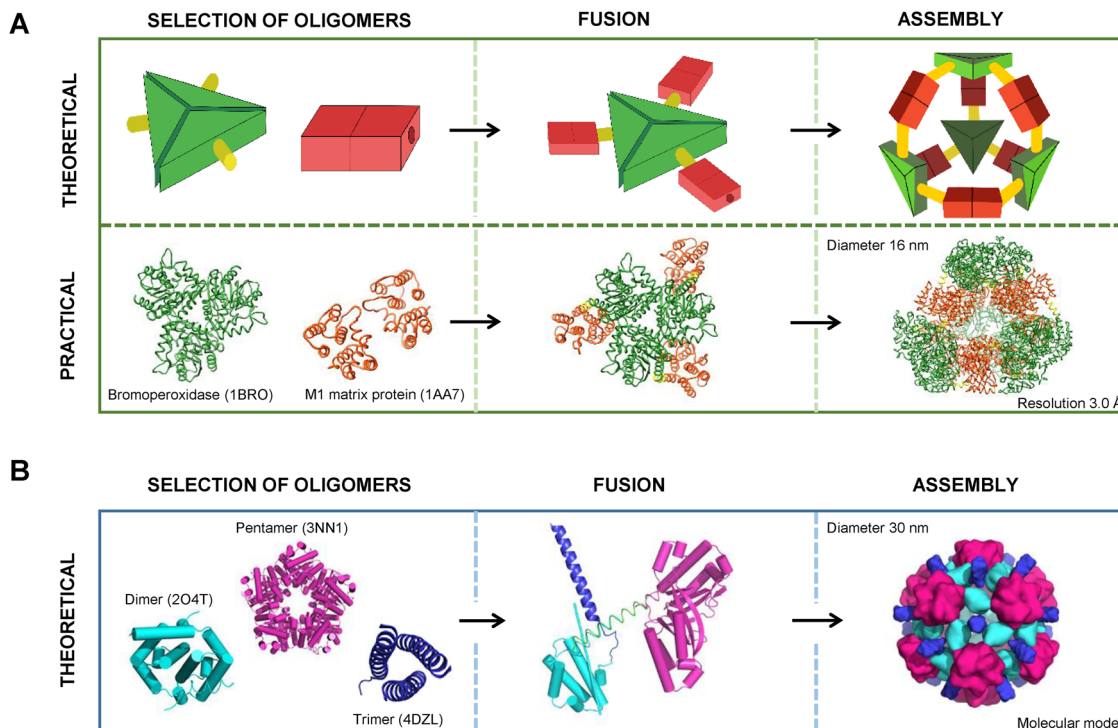
Fig. 1 Genetic fusion-based protein nanocage design: (A) schematic representation of tetrahedral assembly by genetically fusing trimeric and dimeric proteins *via* a nine-residue α-helical linker, resulting in the construction of a tetrahedral cage (PDB ID: 4D9J). (B) An icosahedral protein cage (I532) was constructed using a similar genetic fusion strategy, combining a dimeric DUF1048 protein, a designed coiled-coil trimer, and a pentameric chlorite dismutase.
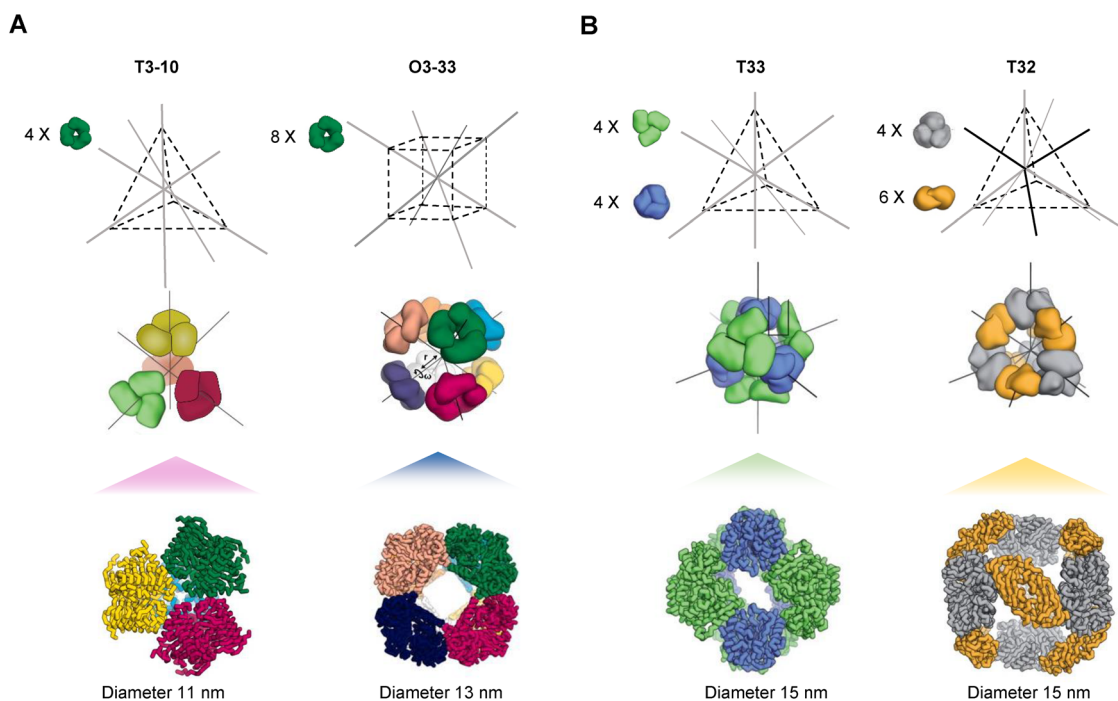

Fig. 2 Interface design-based *de novo* assembly of protein cages: (A) single-component designs of a tetrahedron (PDB ID: 4EGG) and an octahedron (PDB ID: 3VCD). (B) two-component designs of the tetrahedral assemblies T33 (PDB ID: 4NWO) and T32 (PDB ID: 4NWN).

were structurally different from any natural protein complexes characterized. In parallel, Hsia *et al.* reported the design of a

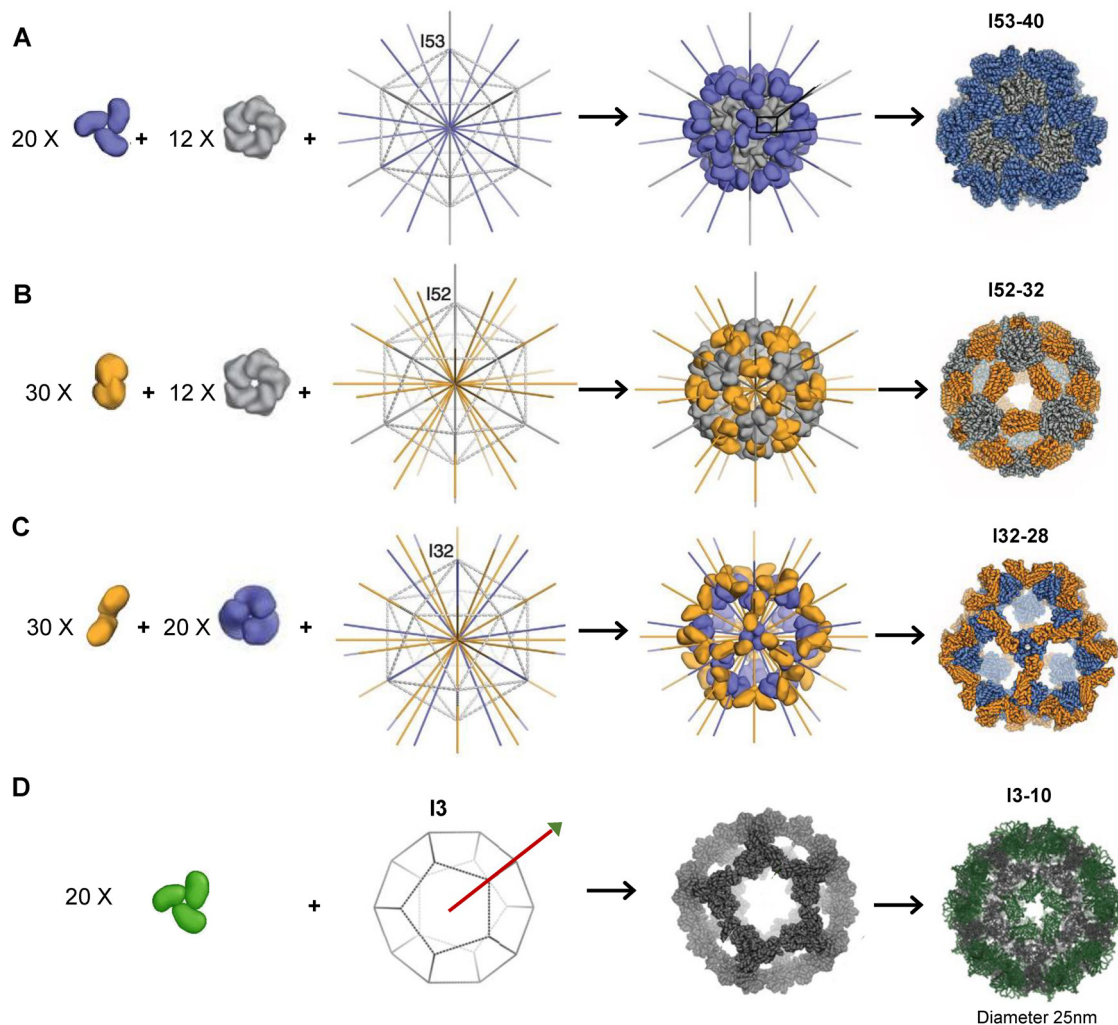highly stable, 60-subunit icosahedral nanocage constructed from a single trimeric protein building block (Fig. 3D).[45]

Fig. 3 Design of megadalton icosahedral protein complexes: (A)–(C) two-component designs of icosahedral protein cages with different symmetries: I53 (PDB ID: 5IM5), I52 (PDB ID: 5IM4), and I32 (PDB ID: 5IM6). (D) Single-component design of an icosahedral cage (I3).

Beyond one- and two-component assemblies, Yang *et al.* designed a three-component nanocage, an octahedral system (O432) combining a tetramer, a pH-responsive trimeric plug, and an antibody Fc domain, illustrating how additional components enable greater modularity and functional control.[46]

Recent studies have significantly advanced protein nanocage design by introducing programmed symmetry breaking to create larger and more complex structures.[32,47] The four-component nanocage strategy overcome the previous size and complexity limits by using pseudosymmetric heterotrimers to build tetrahedral (33 nm), octahedral (43 nm), and icosahedral (75 nm) architectures (Fig. 4A–C). However, through a hierarchical assembly strategy incorporating pseudosymmetry, designs were further scaled to produce icosahedral cages comprising up to 960 subunits and reaching diameters of 96 nm, representing the largest computationally designed protein structures to date (Fig. 4D and E).

2.1.3 Regulated cage assembly based on interface interactions. Metal-directed protein cages rely on the coordination of metal ions to drive and stabilize self-assembly. By incorporating

metal-binding residues such as histidine, cysteine, aspartate, or glutamate at protein interfaces, 3D assemblies can be designed, governed by the coordination preferences of specific metal ions. The designed TRAP protein variants, which self-assemble into stable cage-like structures through coordination with metal ions such as $Zn(\text{II})$ and $Co(\text{II})$[48] highlight the cages' ability to disassemble reversibly when exposed to external signals such as EDTA or changes in pH, with re-assembly occurring upon re-introduction of metal ions. A monomeric protein equipped with hydroxamate groups and zinc-binding motifs assembles through concurrent $Fe(\text{III})$ and $Zn(\text{II})$ coordination into discrete dodecameric and hexameric cages, representing some of the most compositionally complex designed assemblies. These cages can assemble and disassemble in response to diverse stimuli.[49] Metal ions have also been used as direct chemical inducers of cage formation, as demonstrated in ferritin, where self-assembly was rendered controllable by $Cu(\text{II})$ binding, and $Cu(\text{II})$ acts as a structural template for cage assembly that can be removed without disrupting the architecture.[50,51]
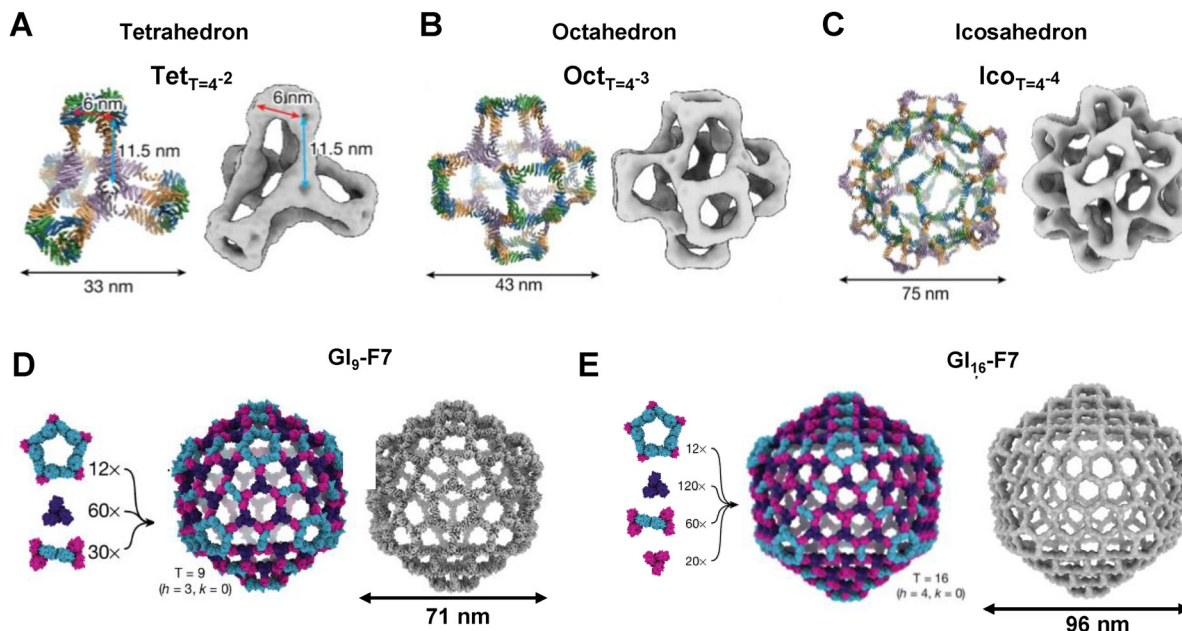
Fig. 4   Protein nanocages designed by programmed symmetry breaking: (A) a tetrahedral nanocage (Tet$_{T=4}$) composed of 48 subunits, (B) an octahedral nanocage (Oct$_{T=4}$) with 96 subunits, and (C) an icosahedral nanocage (Ico$_{T=4}$) containing 240 subunits. (D) A 540-subunit nanocage (GI$_4$-F7) assembled from 12 pentasymmetrons, 60 cyclic C3 (CCC) homotrimers, and 30 disymmetrons. (E) A 960-subunit nanocage (GI$_{16}$-F7), constructed from the same modular components, was visualized by low-resolution cryo-EM. Note: GI$_T$–X, where G stands for Goldberg, I for icosahedral symmetry, T is used to denote the triangulation number of a particular architecture, and X is a unique identifier for each design.

Disulfide-mediated assembly leverages intra- and inter-subunit covalent linkages to induce structural transformations in a controlled manner.[52,53] The study published by Zhao group presents a novel disulfide-mediated approach to create diverse protein nanocages using a single 8-mer bowl-like building block (NF-8).[53] Through selective deletion of intra-subunit disulfide bonds and insertion of inter-subunit linkages, they successfully reprogrammed NF-8 into three distinct quaternary structures: a 24-mer ferritin-like cage, a 16-mer lenticular assembly, and a 48-mer hollow nanocage. Complementing these strategies, a chemically induced protein cage has been reported in which building blocks are covalently connected using DTME or BMH, forming stable cage-like architectures.[54] This chemically driven assembly allows controlled cage opening and cargo release.

2.1.4 Directed evolution-based re-design of protein nanocages. Directed evolution is a laboratory process that mimics natural selection and has been used to enhance the desired functional properties of proteins.[55] In the context of protein nanocages, it is used to optimize properties such as self-assembly efficiency, structural stability, and cargo encapsulation.[56–58] A prominent example is the evolution of *Aquifex aeolicus* lumazine synthase, where the introduction of negative charge into the interior lumen enabled the encapsulation of toxic poly-arginine tagged HIV protease.[59] Baker group demonstrated the role of directed evolution in packaging RNA into computationally designed non-natural protein cages.[57] The evolved variant, I53-50-v4, achieved remarkable genome packaging efficiency, showing over a 133-fold improvement.

Hilvert's group used directed evolution to transform the non-viral enzyme lumazine synthase (AaLS) into virus-like nucleocapsids capable of packaging their own full-length RNA genomes.[56,58] By fusing cationic peptides such as λN+ and applying iterative mutagenesis and selection, RNA encapsulation and stability were improved. Further work using error-prone PCR produced NC-4, a 240-subunit icosahedral capsid with significantly improved RNA packaging efficiency.[56] Together, these studies show that iterative evolution can fine-tune features such as assembly yield, interface packing, cooperativity, and stability that are often difficult to optimize through rational design alone.[60] With machine learning entering the field, there is an enormous potential to speed up directed evolution by predicting function-enhancing mutations and exploring sequence space more efficiently, although the tools still lack the sensitivity to point mutations and reliable ranking of most stable assemblies. While the fraction of successful designs is strongly improved, it is still required to screen tens of constructs.

2.1.5 Protein cage design based on machine learning. Machine learning is rapidly reshaping the landscape of protein nanocage design. Current ML-based approaches encompass a broad family of deep-learning architectures including protein language models, geometric neural networks, and diffusion-based generative models that learn sequence–structure relationships from large structural datasets. These methods can predict, optimize, or generate protein sequences capable of assembling into stable nanocages, enabling faster and broader exploration of sequence space than traditional physics-based design strategies. Protein-message-passing neural network (ProteinMPNN), a deep learning-based protein sequence design tool, has been particularly impactful because it achieves high

native sequence recovery across monomers, homo-oligomers, protein nanoparticles, and protein–protein interfaces with 52.4% recovery compared with 32.9% for Rosetta, while operating more than 200-fold faster for 100-residue backbones.[13] Importantly, ProteinMPNN rescues previously failed nanocage and oligomer designs by generating sequences that fold more accurately to the intended backbone, such as for cyclic homo-oligomers and tetrahedral nanoparticles. Extensions of the framework, such as LigandMPNN, further expand its applicability by incorporating explicit small-molecule, nucleotide, and metal atoms, outperforming Rosetta and ProteinMPNN at recovering interacting residues.[61] This is particularly relevant for nanocage designs requiring metal-binding sites, catalytic centers, or small-molecule responsive assembly mechanisms. Similarly, nucleic acid MPNN (NA-MPNN) generalizes the architecture to protein–nucleic acid complexes, enabling unified inverse folding of proteins, DNA, and RNA using a single message-passing framework, providing opportunities for nanocages that interface with nucleic-acid cargos or regulatory elements.[62] Complementing these design-focused models, ThermoMPNN provides rapid and accurate prediction of mutation-induced stability changes, achieving state-of-the-art performance on large experimental datasets and enabling identification of stabilizing substitutions that enhance robustness of designed assemblies.[63] Large-scale inverse-folding models leverage millions of AlphaFold2-predicted structures to improve fixed-backbone sequence recovery, while structure-guided models like Frame2Seq and Potts-based approaches such as TERMinator expand sequence design capabilities by incorporating geometric features and tertiary-motif statistics to better capture sequence–structure relationships.[64–66]

Recent studies also highlight the transformative potential of ProteinMPNN in advancing protein nanocage engineering beyond traditional computational methods.[14,15] De Haas et al. showed a fully automated workflow that eliminates the extensive manual optimization while reducing computational cost by orders of magnitude. Importantly, ProteinMPNN achieved an experimental success rate of ∼17% for two-component tetrahedral assemblies, comparable to the ∼18% reported for the original Rosetta-only designs, accomplished with much greater efficiency and without expert intervention.[9,15] Their work further demonstrated that ProteinMPNN preferentially generates more polar interface residues than Rosetta, resulting in components with reduced aggregation propensity and improved *in vitro* assembly behavior.[15] Parallel efforts using hybrid fragment-based and ML-guided protocols have similarly shown that integrating ProteinMPNN into cage design pipelines increases the diversity and quality of viable cage candidates compared with traditional fragment- or Rosetta-based sequence design alone.[14]

Additionally, hallucination-based approaches offer an alternative route for generating new protein structures by optimizing random amino acid sequences until deep neural networks predict well-defined distance and orientation maps. This method produces monomeric proteins with diverse all-α, all-β, and mixed α–β topologies, many of which fold as intended,

as confirmed by X-ray crystallography and NMR.[67] The strategy has also been extended to symmetric oligomers, where AlphaFold2-guided hallucination generates cyclic assemblies without predefined protomer structures, yielding oligomers with sequences and architectures distinct from natural proteins and validated by crystallography and cryo-EM.[68]

2.2 Designed nanocages based on modular coiled coils

Coiled coils are a widespread protein structural motif that has been recognized as an excellent building module for the construction of *de novo*-designed protein nanostructures. The interactions that govern the specificity and orthogonality of coiled-coil dimers are well understood.[24,69–72] The seven-amino acid periodicity provides the structural regularity to the coiled-coil dimer motif (heptad repeat), in which each residue is represented as a letter in the sequence *abcdefg*. The specificity of coiled-coil dimer pairing is primarily based on electrostatic interactions between residues at positions *a* and *d*, and *e* and *g* of the heptad repeat (Fig. 5A). The affinity, length, stability, and orthogonality of coiled-coil pairs can be precisely tuned through amino acid modifications and sequence design.[24,69] Several sets of *de novo* designed, orthogonal coiled coils with different stabilities, sizes, affinities and orientations have been reported.[24,73–81]

The Marsh group recognized the potential of the coiled coils for *de novo* protein design and introduced them as helical linkers fused to the natural oligomeric domains that self-assemble *via* coiled-coil dimerization.[82–85] In a complementary approach, the Woolfson group demonstrated that short, designed coiled-coil forming peptides could assemble into bundles that form a hexagonal network with pores. These pores subsequently closed into larger spheres with diameters of approximately 100 nm.[86]

2.2.1 Coiled coil-based assemblies from a single chain (single-chain CCPO). The coiled-coil protein origami (CCPO) concept, pioneered by the Jerala group, provides a flexible framework for constructing programmable coiled-coil nanostructures.[26,87] Inspired by DNA origami principles, CCPO allows for the construction of programmable protein nanostructures using modular coiled-coil interactions. This group developed the CoCoPOD (coiled-coil protein origami design) platform which provides tools for designing sequences and modeling the structures of polyhedral CCPO cages (Fig. 5B–D).[26] In this approach, the edges of the polyhedral structure are decorated with dimeric coiled-coil building modules, and flexible linkers are introduced at the vertices to interrupt helicity and allow precise folding. Using CoCoPOD, several single-chain nanocages in the shapes of a tetrahedron, a four-sided pyramid, a trigonal prism, and a trigonal bipyramid have been successfully designed and characterized.[26,88] More recently, designs comprise four helical bundles have been reported.[89] The structure of a tetrahedral cage was determined by cryo-electron microscopy, and the first high-resolution crystal structure of a coiled coil-based trigonal structure revealed that it forms a topological knot.[90]

The proof of principle was first demonstrated experimentally using a tetrahedron, which is the simplest three-
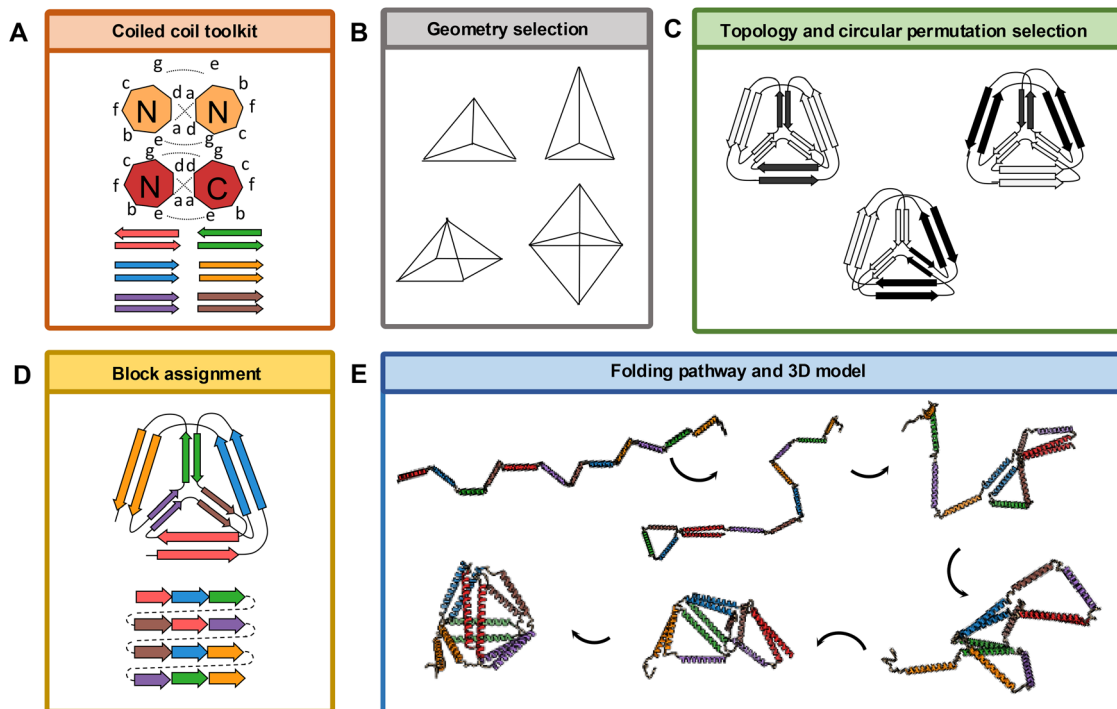
Fig. 5 Design of CCPO nanocages: (A) selection of parallel and antiparallel coiled coils from a set of building modules. (B)–(E) CoCoPOD polyhedral design and modelling process: (B) selection of polyhedral geometry, (C) calculation of optimal topology and circular permutation, (D) assignment of coiled-coil modules to selected topology and (E) assembling process of a protein 3D model.

dimensional polyhedron. A tetrahedral nanocage (TET12), composed of 12 coiled-coil forming segments (each comprising four heptads) concatenated with flexible linkers, was successfully designed and characterized (Fig. 6A).[87] Building on this

work, the Jerala group expanded the CCPO platform to include more complex architectures, such as a four-sided pyramid (PYR16) and a triangular prism (TRIP18).[26] The polypeptides for these second-generation structures had improved folding
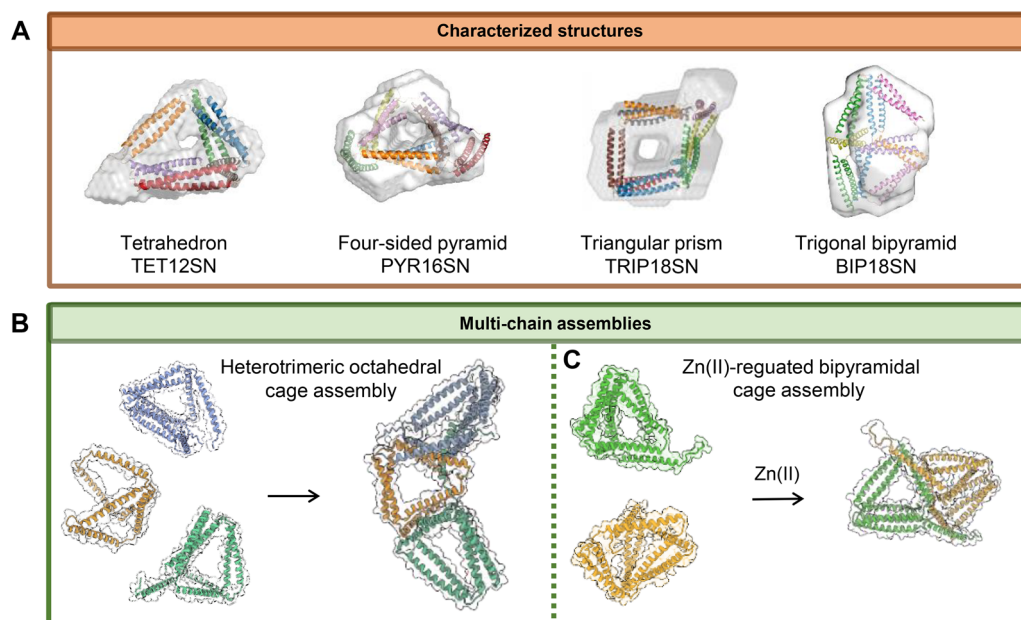

Fig. 6 Polyhedral nanocages composed of coiled coils: (A) models of single-chain polyhedral CCPO structures overlaid with *ab initio* SAXS-derived molecular envelopes. (B) Self-assembly of an asymmetric octahedral structure from three pre-organized subunits. (C) Zn(ɪɪ)-regulated assembly of a bipyramidal nanocage from two pre-organized tetrahedral subunits.

properties and were self-assembled *in vivo* under the physiological conditions in bacteria, mammalian cells and mice without causing inflammation. The structures of the tetrahedron, four-sided pyramid and triangular prism were validated using single-particle TEM reconstruction and SAXS analysis. These analyses revealed the maximum diameters of the structures to be in the range of 10–15 nm (Fig. 6A). Additionally, computational and experimental analyses revealed that CCPO folding proceeds through a sequential, stepwise pathway that is critically dependent on the precise arrangement of coiled-coil modules (Fig. 5E).[91] Understanding this process enabled the control of the folding pathway and the construction of cages with multiple copies of the same module within a single chain while avoiding misfolding. Recently, tetrameric coiled-coil modules were introduced to CCPOs in addition to CC dimers. This expanded the range of topological solutions and allowed for the construction of cages from two identical polypeptide chains. This also facilitated structure determination by cryo-electron microscopy, as the tetrameric modules improved the stability at the air–water interface, which hindered previous attempts.[89]

2.2.2 Coiled coil-based multiple chain assembly (multi-chain CCPO). The single-chain CCPO strategy was further expanded to enable the construction of larger assemblies from pre-organized, modular subunits whose assembly could be controlled. Lapenta *et al.* demonstrated this concept by developing a triangular bipyramidal nanocage (BIP18), assembled from 18 coiled-coil forming segments organized into two pre-structured subunits (Fig. 6A).[88] This two-chain self-assembly CCPO strategy enables the formation of designed nanostructures from either asymmetric or pseudosymmetric pre-organized structural modules. Furthermore, they devised a proteolysis-mediated conformational switch by introducing protease-cleavable masking elements. They appended two complementary coiled-coil-forming segments to the termini of both pre-structured subunits to mask the interaction interface. They introduced a cleavage site for a site-specific protease right before these masking segments, at the end of the polypeptide chain. This allowed them to trim off the two masking coiled-coil-forming segments from each subunit. Proteolysis fully exposed the triangular interface for interaction, triggering the dimer's structural rearrangement into a bipyramidal cage upon the addition of the site-specific protease. This demonstrates that the dynamic regulation of protein cages can be achieved through modular, bottom-up design.

Building on these advances, the Jerala group also described a strategy for assembling modular architectures based on structurally and covalently preorganized subunits. They employed the covalent cyclization of pre-organized subunits through the spontaneous self-splicing of split inteins and intramolecular connections. The cyclization and coiled-coil dimer-based interactions of the polypeptide chains provide the necessary structural constraints to facilitate the desired assembly (Fig. 6B).[92] This strategy enables the self-assembly of higher-order nanostructures with improved folding fidelity and reduced conformational heterogeneity.

2.2.3 Metal-based regulation of CCPO assembly. Similar to the concept discussed in Section 2.1.3, the Jerala group explored the design of metal-binding sites to engineer a peptide-based conformational switch (SwitCCh). This switch assembles into a parallel homodimeric coiled-coil in response to the addition of Zn(II) ions or low pH.[27] The peptide can be reversibly cycled between the coiled-coil and random conformations in the presence or absence of Zn(II) ions. Building on this principle, the group rationally designed an orthogonal set of Zn(II)-responsive coiled-coil heterodimers to enable the programmable folding of CCPO nanostructures. This concept has been demonstrated with several coiled coil-based nanostructures, from a protein triangle to a two-chain bipyramidal protein cage that opens and closes depending on the metal ion (Fig. 6C).[28] By incorporating Zn(II)-dependent coiled-coil dimers into the interface between two subunits, the subunits can selectively assemble in the presence of Zn(II) ions and dissociate reversibly upon metal ion sequestration. This approach demonstrates a reversible, externally controllable system for dynamic protein assembly.

3. Application of designed protein nanocages

Nanostructures offer an exciting potential in cargo encapsulation and drug delivery, vaccine development, enzymatic catalysis and bioimaging (Fig. 7). The engineered protein nanocages provide precise control over size, shape, and surface characteristics, allowing for cargo loading through bioconjugation and non-covalent interactions. Their stable architectures protect therapeutic payloads from premature degradation, enhancing delivery accuracy and overall treatment efficacy. Moreover, the use of non-viral protein components in artificial nanocages can lower immunogenicity and decrease the risk of adverse immune responses upon repeated administration.[30,93–95]

The Zhao group demonstrated the principle of therapeutic cargo encapsulation by engineering a 16-mer ferritin-derived nanocage capable of encapsulating curcumin, a yellow polyphenolic compound derived from the turmeric plant (*Curcuma longa*) known for its potent antioxidant, anti-inflammatory, anticancer, and antimicrobial properties.[96] Despite these biological activities, curcumin suffers from extremely poor aqueous solubility, rapid degradation at physiological pH, and low bioavailability. The encapsulation significantly improved curcumin's chemical stability and bioavailability, thereby showcasing the nanocage's potential for delivering hydrophobic bioactives.[97–99] Beyond encapsulation, nanocages can be functionalized with targeting modules such as tumor-homing peptides, cell-penetrating peptides, antibody-binding or receptor-specific ligands to achieve selective uptake and enhanced intracellular delivery of diverse cargoes.[33,46,95,100–104] In addition to therapeutic delivery, protein nanocages can serve as confined environments that enhance enzymatic reactions. By restricting diffusion and stabilizing the enzyme structure, nanocages can increase catalytic efficiency while protecting sensitive proteins
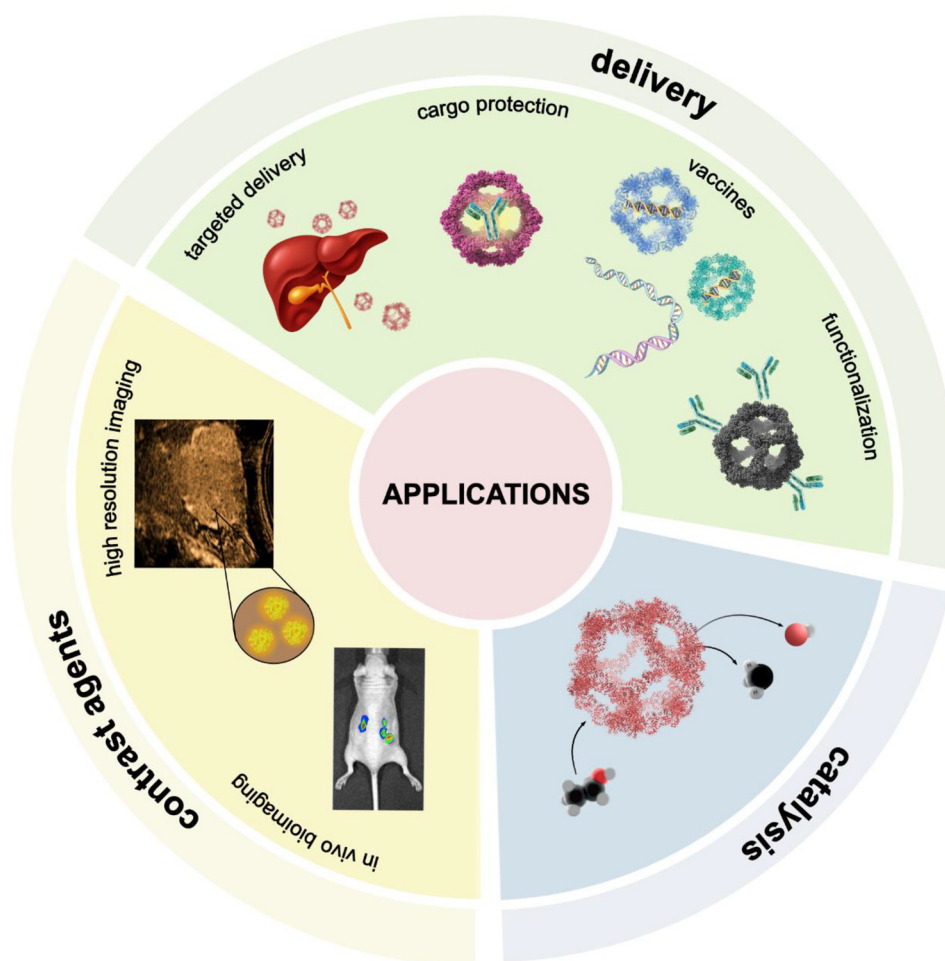
Fig. 7 The schematic illustrations of protein nanocage applications, including cargo delivery, bioimaging, and catalysis.

from degradation.[105–107] Several natural and engineered systems including ferritin, lumazine synthase, encapsulins, and viral capsids have been used to encapsulate enzymes through electrostatic, affinity-based, or genetic fusion strategies. For example, engineered lumazine synthase variants (AaLS-neg, AaLS-13) efficiently encapsulate supercharged enzymes to enable controlled proteolysis or peroxidase reactions, while *Thermotoga maritima* ferritin (TmFtn) encapsulation enhances lysozyme activity through crowding effects.[108] Encapsulins from *Brevibacterium linens* naturally load dye-decolorizing peroxidase (DyP), enabling the construction of cascade nanoreactors when paired with glucose oxidase.[109]

Engineered protein nanocages are being actively explored as platforms for the development of novel vaccines.[31,110] Their symmetrical, virus-like architecture mimics natural pathogens and supports multivalent, ordered display of protein epitopes. This repetitive presentation is crucial for eliciting a strong humoral immune response. By presenting both B cell and T cell epitopes, protein nanocages can elicit robust IgG responses by enhancing antigen uptake and facilitating efficient B cell receptor cross-linking. This leads to potent B cell activation and subsequent differentiation into antibody-secreting

plasma cells. Computationally designed scaffolds such as I3-01 and I53-50 have demonstrated that multivalent display of antigens, such as receptor-binding domain, significantly enhances the magnitude of neutralizing antibody titers compared to soluble antigen formulations alone.[111–114] The well-defined geometry of protein nanocages allows for high-density, multivalent presentation of antigens with controlled spacing, improving immune receptor engagement. This strategy has been investigated in the development of vaccines against various infectious diseases, including hepatitis B, influenza, and respiratory syncytial virus.[113,114] Several protein nanocage platforms have also progressed into clinical trials, including ferritin-based vaccines for SARS-CoV-2 and influenza, and, importantly, a designed icosahedral nanocage-based vaccine (I53-50) against SARS-CoV-2, which is marketed as SKYCovione™.[115–120]

Beyond humoral immunity, protein nanocages such as E2 and I3-01 can also promote robust cellular immune responses, including the activation of CD4$^+$ helper T cells and CD8$^+$ cytotoxic T lymphocytes.[121–124] By incorporating specific T cell epitopes, these nanocages engage MHC class I and class II antigen presentation pathways. This dual engagement enables cytotoxic CD8$^+$ T cells to directly target infected or malignant

cells, while CD4$^+$ helper T cells support sustained immune activity by promoting B cell maturation, CD8$^+$ T cell memory formation, and coordinated cytokine signaling. The activation of a cell-mediated immune response can also be achieved by incorporating T cell epitopes at the interior side of the nanocage.

Building upon these advancements, protein nanocages have been systematically investigated as platforms for cancer immunotherapy and targeted drug delivery. Functionalizing nanocages with ligands that recognize specific cell surface receptors, such as transferrin or epidermal growth factor receptors, enhances cellular uptake and tumor targeting.[125] Osiński *et al.* demonstrated that the introduction of histidine residues into metal-binding sites of protein cages allows for pH-sensitive disassembly, enabling selective fluorescent protein release under acidic conditions typical of tumor microenvironments.[48] In a complementary approach, Yang *et al.* showed that pH-responsive trimeric building blocks can modulate the porosity of octahedral antibody nanoparticles, providing an additional mechanism for pH-dependent control of assembly and cargo accessibility.[46] In the future, such cargo could be replaced with chemotherapeutic agents, immunostimulatory molecules or nucleic acids, which often face challenges in stability, solubility, or targeted delivery.

Nanocages based on natural proteins bring compelling advantages to biomedical imaging that distinguish them from established clinical agents such as small-molecule gadolinium (Gd) chelates or inorganic nanoparticles.[126] These biologically derived structures like ferritin and heat shock proteins (Hsp16.5) are genetically programmable, uniform, and biocompatible, enabling the site-specific and high-density conjugation of imaging agents for magnetic resonance imaging (MRI), positron emission tomography (PET), fluorescence, and even ultrasound modalities.[127–129] Beyond MRI, designed protein nanocages support multimodal imaging, such as: (1) tobacco mosaic virus-based nanoparticles co-loaded with Dy^{3+} and Cy7.5 fluorophores enabled dual MRI/near-infrared fluorescence imaging[130] and (2) protein-based gas vesicles produced strong acoustic contrast *in vivo* for ultrasound applications.[131]

4. Challenges of designed protein cages

Despite major advances in protein nanocage engineering for catalysis, drug delivery, and bioimaging, several challenges remain to facilitate more effective clinical translation. Key issues include maintaining structural integrity, minimizing immunogenicity, and optimizing biological performance. While immunogenicity and biocompatibility remain important considerations for protein nanocages intended for therapeutic applications, these challenges are also shared by many other protein therapeutics and viral vector-based systems. Although nanocages are typically constructed from biocompatible parts, factors such as specific structural motifs or residual contaminants can still provoke immune response, potentially compromising therapeutic efficacy or increasing toxicity risks. Similar to other advanced delivery systems, ongoing efforts in protein engineering and purification strategies are critical for improving clinical translation.[132] Another fundamental concern is the long-term stability and structural robustness of protein nanocages under the physiological conditions, which has been significantly improved by the hyperstability of ML-based designs. Many protein nanocages struggle to encapsulate sufficient quantities of drug molecules, especially hydrophobic or dual-mode therapeutics. Moreover, tunable and controlled release could be improved in sustained or stimuli-responsive delivery.[103,133] Lastly, cellular permeability and tissue penetration remain inadequate in many formulations. Without surface modifications or targeting ligands, nanocages often demonstrate poor biodistribution and off-target accumulation. Together, these limitations highlight the need for continued innovation in both material design and production methodologies. On the other hand, recent advances are finding solutions to many of these issues. Single-chain designs significantly reduce heterogeneity, although the size of such cages is typically limited to about 100 kDa.

5. Future directions

To enable broader clinical use, future work must address these challenges by integrating bioengineering strategies that improve structural stability, reduce immunogenicity, and enhance targeting and cargo release profiles. Innovative surface modifications such as the conjugation of tumor-targeting peptides, aptamers, and monoclonal antibodies, should be further investigated to enhance target specificity and therapeutic precision.[134,135] Surface functionalization, particularly through polyethylene glycol (PEG) conjugation, offers several advantages such as prolonged circulation half-life, enhanced biocompatibility and protection from enzymatic degradation.[136] Specifically for coiled-coil protein-based nanocages (CCPOs), systematic evaluation of diverse functionalization approaches remains necessary to optimize therapeutic delivery to specific targets. The modular nature of CCPOs provides a unique advantage, offering flexibility in size, shape, complexity, and functionalization, which can be tailored for both medical and biotechnological applications.

Another emerging frontier in protein nanocage design is the development of high-throughput AI/ML pipelines to precisely predict and optimize self-assembly behavior. The field of *de novo* protein design has evolved dramatically over the past decades, transitioning from purely physics-based approaches to the integration of AI-driven methods.[137,138] While advances such as AlphaFold have revolutionized structural prediction, they still fall short when applied to complex architectures like tetrahedral, octahedral, or icosahedral protein cages.[139,140]

In particular, AlphaFold fails to predict the global fold and 3D structures of *de novo* designed CCPOs, likely due to the lack of homologous templates, nonnatural topology and limitations in current training datasets. Recent advances in deep learning-

based structure prediction are becoming an essential validation step for assessing the structure of complex multimeric assemblies.[141] In addition to AlphaFold2 and AlphaFold3, which brought transformative accuracy to single-chain structure prediction, subsequent tools such as RoseTTAFold and AlphaFold-multimer have extended this capability to multimeric complexes, often using paired multiple sequence alignments (MSAs) to model inter-chain interactions.[142–144] To expand capabilities further, Monte Carlo-based frameworks such as MoLPC were developed to simulate large symmetric assemblies through stepwise modeling, although they require prior stoichiometric knowledge of the system.[145] Additionally, UniFold-symmetry demonstrated rapid and accurate modeling of high-order cyclic oligomers using symmetry-aware residue transformations.[146] Although initially limited to cyclic assemblies, its extension to polyhedral nanocages appears promising. Meanwhile, the application of language-based deep learning models has introduced alternative routes for structural prediction without the need for explicit MSAs such as OmegaFold and ESMFold.[147,148] While these models are not yet fully validated for highly complex protein assemblies, they represent scalable and rapid alternatives that may effectively complement traditional design methodologies. Incorporating such tools into synthetic protein design workflows could substantially enhance both predictive accuracy and development throughput.

On the other hand, ML-based designs are highly stable, can be engineered to be protease-resistant, and are also highly homogeneous. By incorporating diverse constraints, they can also avoid T-cell epitopes and immunogenic surfaces. Furthermore, the ability to regulate their assembly and disassembly, as well as cargo packaging, is being improved through the introduction of all-atom ML models.[144,149]

Author contributions

AKG: conceptualization, writing, visualization and original draft. HE: writing, visualization and review. HG: writing, visualization and review. RJ: conceptualization, review and supervision.

Conflicts of interest

The authors declare that there are no conflicts of interest.

Data availability

No primary research results, software or code have been included and no new data were generated or analyzed as part of this review.

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