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Nanobodies targeting ion channels: advancing therapeutics through precision and structural insights

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Ion channels, which are integral to cellular signaling and homeostasis, are implicated in a variety of diseases, including neurological disorders, cardiovascular conditions, and cancers. Despite their importance, targeting ion channels therapeutically is challenging due to issues such as structural conservation and dynamic conformational changes. Nanobodies, derived from camelid heavy-chain antibodies, have emerged as a transformative tool in biotherapeutics due to their small size, remarkable stability, and high specificity for epitope recognition. They represent a significant advancement in targeting ion channels, offering precision and adaptability not achievable with traditional antibodies or small molecules. This review provides an in-depth analysis of the structural and functional basis of ion channel modulation by nanobodies. We explore how they achieve their effects through diverse mechanisms, including direct pore blocking, allosteric modulation of gating, stabilization of specific conformational states, and isoform-selective recognition. We further examine their therapeutic applications, the potential for engineering multivalent constructs to enhance efficacy, and critical advancements in overcoming challenges like blood–brain barrier (BBB) penetration. Finally, we discuss recent clinical developments, the translational gap for ion channel targets, and the transformative potential of artificial intelligence in accelerating the design of next-generation nanobody-based therapeutics.

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structural, biochemical, and biophysical approaches. His current work integrates biophysical and structural methods to elucidate the molecular principles governing iGluR function.

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Introduction

Ion channels are integral membrane proteins that mediate the selective passage of ions across cellular membranes, playing critical roles in maintaining cellular homeostasis, electrical excitability, and signal transduction.^{1,2} These proteins are essential for various physiological processes, including neuronal firing, muscle contraction, hormone secretion, and fluid regulation. Classified based on their gating mechanisms, ion channels include voltage-gated, ligand-gated, mechanosensitive, and temperature-sensitive channels, each with specialized functions within excitable and non-excitable tissues.^{1,2}

The significance of ion channels extends beyond their physiological roles; their dysregulation has been implicated in

numerous diseases. Neurological disorders such as epilepsy and chronic pain, cardiovascular abnormalities like arrhythmias and hypertension, and cancers characterized by aberrant ion channel expression and function represent a fraction of the conditions associated with ion channel dysfunction.³ Recent studies have also unveiled the roles of ion channels in immune modulation, metabolic regulation, and stem cell differentiation, underscoring their involvement in systemic pathophysiological processes.⁴⁻⁶

Therapeutically targeting ion channels is a complex endeavour. Structural conservation among channel isoforms, particularly in their pore regions, poses challenges for achieving specificity. For instance, sodium channel isoforms Nav1.7, Nav1.8, and Nav1.9 are highly homologous, yet distinct in their physiological roles in pain signaling, necessitating precise targeting to minimize off-target effects.⁷ Moreover, the dynamic conformational states of ion channels during gating further complicate drug development, as therapeutics must interact with transient structural configurations that are not readily accessible. While small molecules and peptide toxins have historically served as modulators, their therapeutic application is often limited by insufficient selectivity and systemic toxicity.

While providing enhanced specificity, conventional monoclonal antibodies are hindered by their substantial size (~150 kDa) and bivalent architecture, which restricts their access to functional epitopes typically concealed within the intricate topography of these transmembrane proteins.⁸ Nanobodies, the 15 kDa single-variable domains (VHH) of camelid heavy-chain-only antibodies, are smaller than conventional antibodies but have comparable or better specificity, stability, and affinity. They are relatively easier and less expensive to purify compared to conventional antibodies. Nanobodies exhibit low immunogenicity and can be engineered into multivalent or biparatopic formats to enhance avidity and functional specificity, further broadening their therapeutic utility. A particularly transformative aspect of nanobody application lies in the



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structural elucidation of ion channels.⁸ Advances in cryo-electron microscopy (cryo-EM) and X-ray crystallography have enabled high-resolution visualization of nanobody-ion channel complexes, revealing mechanisms of action, allosteric modulation, and isoform-specific binding. These structural insights advance our understanding of ion channel biology and facilitate the rational design of next-generation therapeutics. These unique properties make them exceptionally well-suited for targeting proteins and specifically ion channels.

As nanobody-based therapies advance, their ability to cross the blood–brain barrier (BBB) has emerged as a critical advantage for targeting ion channels implicated in central nervous system (CNS) disorders. This review highlights the multifaceted applications of nanobodies in ion channel research and therapy. We organize our discussion around the diverse modulatory mechanisms revealed by structural biology, before examining therapeutic innovation, delivery challenges, and emerging clinical and computational prospects. Through these advancements, nanobody technology is poised to overcome longstanding challenges, offering new avenues for precision medicine in ion channel-associated diseases.

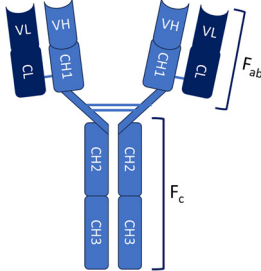
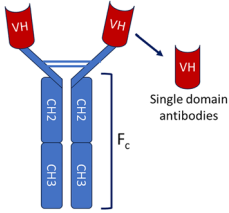
Nanobody – a small, modular and single-domain antibody

The immune system of the camelid family, which includes camels, llamas, and alpacas, produces a unique class of antibodies known

as heavy-chain antibodies (HCABs).^{9,10} These Heavy-chain antibodies are composed exclusively of heavy chains and entirely devoid of light chains, distinguished by the lack of the CH1 domain in their constant region, a structural characteristic that typically promotes the pairing of heavy and light chains. The variable region of the HCAB, which possesses the ability to bind to antigens effectively, is referred to as the variable domain of the heavy-chain antibody (VHH) or single-domain antibody (sdAb).¹¹ VHH/sdAb are frequently referred to as nanobodies (Nb), a term that was initially trademarked by the Belgian biopharmaceutical firm Ablynx in 2003.¹² In contrast to conventional antibodies (IgG), nanobodies exhibit distinct advantages as detailed in Table 1. Nanobodies are a superior alternative to conventional antibodies (IgG), demonstrating promising potential across a range of applications in structural biology, molecular imaging, disease diagnosis and treatment.

Nanobody development requires the generation of a library of nanobody and using it to identify specific high affinity binders against an antigen. The identification of specific nanobodies that effectively target particular antigens can be accomplished through three distinct methodologies, which are as follows: (i) the conventional naïve or immunization approach, (ii) the utilization of synthetic nanobody (Sybodies) libraries, and (iii) the application of computational techniques in conjunction with artificial intelligence-based modeling that focus on the design and characterization of nanobodies.¹³

Table 1 Comparison between nanobody and conventional antibody^a

Characteristics	Conventional antibodies	Nanobodies
		
Encoded by gene	Two gene fragments (heavy and light chains)	Single-gene fragment (VHH)
Molecular weight	~150 kDa	~15 kDa
Structure	Heteromeric (2 heavy + 2 light chains)	Monomeric (single heavy-chain variable domain)
Mode of binding	Bivalent	Monovalent
Specificity	High	High
Affinity	nM–pM range	nM–pM range
Preferred expression system	Mammalian (CHO, HEK293)	Bacterial (<i>e.g.</i> , <i>E. coli</i>), Yeast (<i>e.g.</i> , <i>Pichia pastoris</i> , <i>Saccharomyces cerevisiae</i>)
Production yield	Moderate to low (complex folding, glycosylation required)	High (simple folding, no glycosylation required)
Solubility	Variable; may aggregate without light chains	Highly soluble (hydrophilic framework)
Stability	sensitive to pH and temperature	High thermal and chemical stability
Ease of manipulation for enhance affinity	Difficult to manipulate at the genetic level	Easily engineered <i>via</i> CDR3 modification
Tissue penetration	Limited due to the Large molecular size	High due to small molecular size
Development cost	High	Low to moderate
Paratope geometry	Concave/flat (fits protruding epitopes)	Convex (fits concave or buried epitopes)

^a Info compiled from multiple sources.^{9,11–13,77,100–102}

Highlight

(i) Library generation

The immunization of camelids involves the injection of purified antigen (Proteins) or whole cells expressing proteins on surface or virus-like particles into them. Typically, the PBMCs (Peripheral blood mononuclear cells) are isolated from the blood collected from the animal. Nanobody libraries are generated using the mRNA from the PBMCs, that are rich in high-affinity, conformationally selective variable heavy-chain domains (VHHs). Conversely, naïve or synthetic libraries, which are distinguished by their intentionally designed complementarity-determining region (CDR) diversity, facilitate a more rapid identification process *in vitro*, eliminating the necessity for animal immunization, and proving to be particularly advantageous in scenarios involving human targets or situations where immunization is not feasible or ethical.¹⁴

(ii) Biopanning to isolate nanobody binders against antigen

The technologies employed for screening and selection play a crucial role in the conversion of VHH repertoires into effective and functional binders that can be utilized for various applications. Among these methodologies, phage display remains the predominant technique for achieving initial enrichment through a series of successive panning processes against antigens that have been immobilized, as seen in enzyme-linked immunosorbent assay (ELISA) formats. Yeast surface display library are panned using magnetic-activated cell sorting (MACS) and fluorescence-activated cell sorting (FACS), both of which allow for the precise differentiation of nanobodies based on key parameters such as binding affinity, specificity, and off-rate kinetics.¹² Ribosome and mRNA display methodologies enable

researchers to explore extensive synthetic repertoires in a completely controlled *in vitro* environment, which proves to be instrumental in the process of affinity maturation that enhances the binding capabilities of the nanobodies.¹⁵

Artificial Intelligence (AI)-Driven technologies have reached a level of sophistication that significantly reduces the expenditure of costly resources and time. AI-Machine Learning (ML) has revolutionized novel protein design field. This topic has been further discussed in the later part of the literature under the section – The Digital Frontier: using AI to design and improve ion channel nanobodies.¹⁶

(iii) Validation of nanobody binders

Upon the identification of promising nanobodies, they can be further evaluated using various biophysical techniques and structural biology to ascertain their affinity and binding sites (Fig. 1).

Structural and mechanistic insights into nanobody-mediated ion channel modulation

High-resolution structures of nanobody-channel complexes have revealed an astonishing diversity of modulatory mechanisms. Rather than simply acting as brute-force pore blockers, nanobodies function as sophisticated molecular machines that can stabilize specific conformational states, allosterically regulate gating, or even act as chaperones to enable structural studies of otherwise intractable targets (Table 2). Here, we

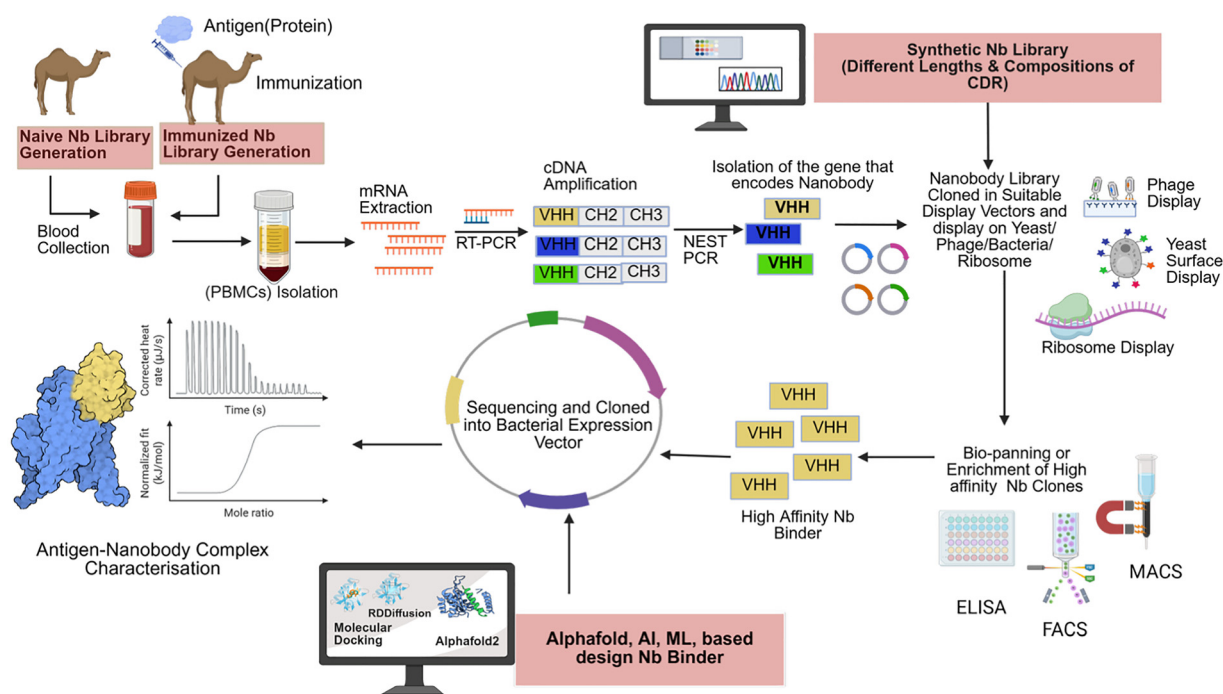


Fig. 1 A flowchart for Nanobody generation strategies and methodologies. The image was created using Biorender.

Table 2 List of nanobodies targeted against ion channels

Nanobody	Target species and ion channel name	Nanobody library	Display platforms for biopanning	EC ₅₀ /affinity (Kd)	Property	PDB structure
13A7	Mouse P2X ₇	Immunized	Phage display	IC ₅₀ = 12 nM	Blocking (prevents gating)	No
14D5	Mouse P2X ₇	Immunized	Phage display	EC ₅₀ = 6 nM	Potentiation	No
Dano1	Human P2X ₇	Immunized	Phage display	IC ₅₀ = 0.2 nM	Blocking (high potency)	No
A0194009G09	human Kv1.3	Immunized	Phage display	IC ₅₀ = 8.2 nM	Blocking (prevents gating)/Suppresses Kv1.3-mediated potassium currents/potent inhibitor	8DFL
Nb.C1	Human ASIC1a	Immunized	Phage display	—	With inhibitor PcTx1 inhibits the gating properties. Nb.C1 stabilizes and prevents aggregation of hASIC1a	7RNN
Nb17, Nb82	Human Nav1.4/Nav1.5	Immunized	Phage display	Nb17: 41.1 ± 9.9 nM (Nav1.4); 60.5 ± 5.80 nM (Nav1.5) Nb82: 50.2 ± 8.87 nM (Nav1.4); 63.2 ± 6.75 nM (Nav1.5) Kd(nb.f3) = 13.2 ± 7.2	Detect Nav1.4 & Nav1.5 channels in live cells and tissue homogenates	No, 7R63 (Nb only), Nb82, (no complex)
nb.E8 & nb.F3	Mouse High-voltage activated calcium channels (HVACCs)	Immunized	Phage display	—	Bind to the auxiliary subunit of HVACCs	8DAM, 8E0E
Nb58	Human TREK-2	Immunized	Phage display	—	Cavβ1, inhibits recombinant Cav1/Cav2 channels reconstituted with Cavβ1	8QZ1
Nb61	Human TREK-2	Immunized	Phage display	Kd = 1110 nM, IC ₅₀ = 685 ± 18 nM	Used immunodetection and immunoassays of TREK2	8QZ2
Nb67	Human TREK-2	Immunized	Phage display	EC ₅₀ = 101 ± 12 nM	Inhibiting channel-gating mechanisms reduces K ⁺ conductance	8QZ3
Biparatropic Nb6158	Human TREK-2	—	—	Kd = 4.1 nM, 16-fold improvement of IC ₅₀ ~40 nM	Channel opening/activation enhances K ⁺ efflux	EMD-19066
Nb76	Human TREK-2	Immunized	Phage display	Not Reported	More inhibitory responses than Nb61	8QZ4
Sb1	Mouse homomeric LRRG8A	Synthetic	Ribosome display	Kd = 23 nM	Channel opening/activation	7P5V
Sb2	Mouse homomeric LRRG8A	Synthetic	Ribosome display	Kd = 48 nM	Channel inhibition	7P5W
Sb3	Mouse homomeric LRRG8A	Synthetic	Ribosome display	Kd = 857 nM	Channel inhibition	7P5Y
Sb4	Mouse homomeric LRRG8A	Synthetic	Ribosome display	Kd = 22 nM	Channel inhibition	7P60
Sb5	Mouse homomeric LRRG8A	Synthetic	Ribosome display	Kd = 173 nM	Channel inhibition	7P6K
Sb1	Mouse heteromeric LRRG8A/C	Synthetic	Ribosome display	—	Channel inhibition, structural stability	8B41
Nb21 (NAM Nb)	Erwinia ligand-gated ion channel (Cys-loop ligand-gated ion channel)	Immunized	Phage display	IC ₅₀ = 0.13 mM	Negative modulation <i>via</i> vestibula binding	6SSP
Nb22 (PAM Nb)	Erwinia ligand-gated ion channel (Cys-loop ligand-gated ion channel)	Immunized	Phage display	EC ₅₀ = 4.2 mM	Positive modulation <i>via</i> vestibular binding	6SSI
Nb72	Erwinia ligand-gated ion channel (Cys-loop ligand-gated ion channel)	Immunized	Phage display	—	—	6HJX
Nb C4	Human alpha7 nicotinic receptor/Neuronal acetylcholine receptor subunit alpha-7	Immunized	Phage display	Kd = 0.2 ± 0.3 nM	Silent allosteric ligand (SAL), showing no effect on ACh-gated currents but inhibiting Nb-E3 elicited potentiation	8C9X
Nb C4	Human alpha7 nicotinic receptor/Neuronal acetylcholine receptor subunit alpha-7	Immunized	Phage display	Kd = 0.2 ± 0.3 nM	With nicotine, Silent Allosteric Modulator	8CAU
Nb E3	Human alpha7 nicotinic receptor/Neuronal acetylcholine receptor subunit alpha-7	Immunized	Phage display	Kd = 1 ± 0.01 nM	Potentiation ACh-gated currents	8CE4

Table 2 (continued)

Nanobody	Target species and ion channel name	Nanobody library	Display platforms for biopanning	EC ₅₀ /affinity (Kd)	Property	PDB structure
Nb E3	Human alpha7 nicotinic receptor/ Neuronal acetylcholine receptor subunit alpha-7	Immunized	Phage display	Kd = 1 ± 0.01 nM	With nicotine potentiates ACh-gated currents	8C11
VHH15	Mouse 5-HT3 receptor	Immunized	Phage display	Kd = 142 nM	Inhibits channel activity	4PIR
Synthetic Nb Sbc2	Human CALHM2	Synthetic	Ribosome display		Structural stabilization for cryo-EM	8RMK
Synthetic Nb Sbc4	Human CALHM2/4 (heteromer)	Synthetic	Ribosome display		Marker for heteromer assembly studies	8RML
Synthetic Nb Sbc4 Nb4	Human CALHM4 (decamer dimer)	Synthetic	Ribosome display		Structural capture of large oligomeric states	8RMN
DN13	Human NMDA (GluN1a–GluN2A–GluN2C)	Immunized	Phage display	Kd = 3.5 ± 0.6 nM with agonist	Reduces structural heterogeneity	8E99
DN1	Human metabotropic glutamate 2 (mGlu2)	Immunized	Phage display	Kd = 2.1 ± 0.4 nM with agonist	suppresses NMDAR gating currents	No
DN13–DN1	Human metabotropic glutamate 2 (mGlu2)	Immunized	Phage display		increase NMDA receptor (NMDAR) currents	No
Nb38	Human metabotropic glutamate 2 (mGlu2) GABA(A)	Immunized	Phage display	Positive allosteric modulator	Precisely regulate NMDAR function	No
Nb25	GABA(A)	Immunized	Phage display	Structural stabilization for cryo-EM		9FFV, 9FFW, 9FFX, 9FFY, 9FFZ, 9FG0, 9FG1, 9FG2, 9FG3 508F, 50JM

classify these interactions based on their primary mechanism of action.

1. Allosteric modulation of channel gating

Many nanobodies function by binding to sites remote from the ion conduction pore, inducing conformational changes that either promote or inhibit channel activity. This allosteric approach offers a powerful route to achieving subtype selectivity.

Targeting extracellular domains: the case of TREK-2 and ASIC1a

TREK-2 is a two-pore domain potassium (K2P) channel that plays a crucial role in stabilizing the resting membrane potential and regulating neuronal excitability. It responds to mechanical, thermal, and chemical stimuli, contributing to neuroprotection and pain modulation, especially under inflammatory or nerve injury conditions. Approaches using nanobodies have been developed to selectively modulate TREK-2 potassium channel activity by targeting its extracellular domains. Twenty-nine nanobodies were identified to bind TREK2, and three of these nanobodies demonstrated significant modulation of the channel properties of TREK2.

Nb61 acts specifically as a negative allosteric modulator for TREK-2, rapidly suppressing TREK-2 currents (IC₅₀ ≈ 685 nM). Notably, this inhibition is highly selective to mouse and human TREK-2, but does not affect related channels like TREK-1 or TASK-3. Structurally, the nanobody operates through a direct, toxin-like mechanism, where its extended CDR3 loop inserts a lysine residue, caps the extracellular ion exit pathway, and decreases potassium currents. However, because the K2P Cap domain of TREK2 restricts direct access to the pore, such a block is unusual, making this finding particularly significant (Fig. 2A). In contrast, Nanobody 67 (Nb67) binds to different extracellular sites and promotes channel opening, enhancing potassium efflux and reducing neuronal hyperexcitability, but also has a weaker affinity to TREK-1, making it partially selective (Fig. 2B). Nb76 binds specifically to the P2-M4 loop of the TREK-2 potassium channel, moves the M4 helix to the open “M4 Up” conformation, thereby allowing the potassium ions to pass. This structural rearrangement closely mirrors the mechanism by which well-established agonists like ML335 activate the channel. By promoting the “M4 Up” conformation, these nanobodies stabilize the selectivity filter in a configuration optimized for maximal potassium ion conductance (Fig. 2C).

Nb61-58 is a bi-paratopic nanobody that enhances inhibition of the TREK-2 potassium channel. It links two nanobody units, Nb-Inhibitor-61 and Nb-Binder-58. They bind distinct, non-overlapping sites on the TREK-2 Cap domain. This design significantly increases binding affinity (over 250-fold) compared to the monomeric inhibitor and improves inhibitory potency about 16-fold (IC₅₀ ~ 40 nM). These nanobodies exert their effects allosterically by influencing gating mechanisms

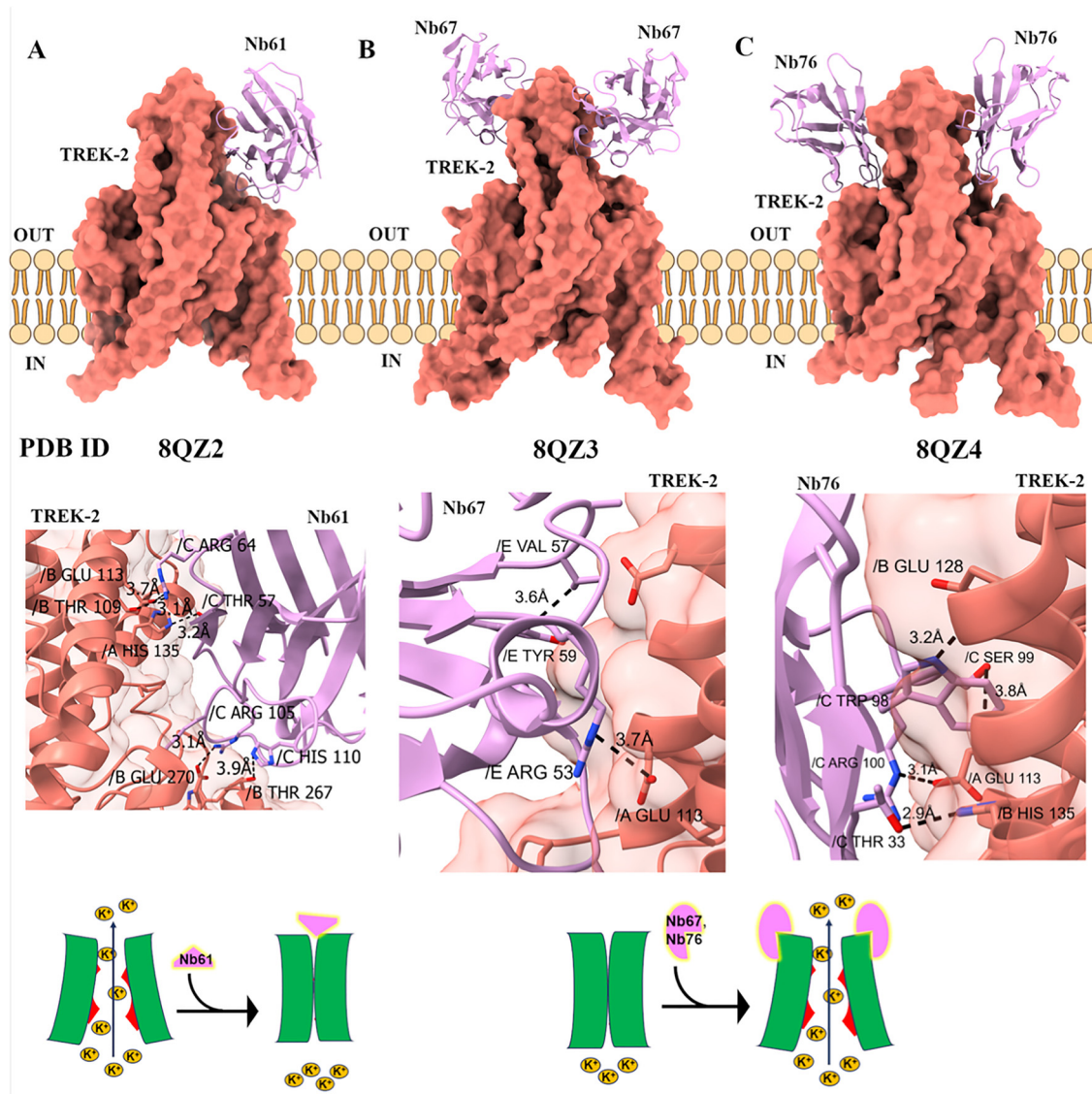


Fig. 2 Allosteric Modulation of the TREK-2 Two-Pore Domain Potassium Channel by Function-Switching Nanobodies. This figure presents a remarkable example of how nanobodies binding to the same general region of an ion channel can elicit opposite functional responses. The panels show crystal structures of the human two-pore domain potassium channel TREK-2 (K2P10.1, salmon) in complex with three distinct nanobodies (plum) that all target the extracellular cap domain but function as either negative or positive allosteric modulators (NAMs or PAMs). (A) The structure of TREK-2 with the inhibitory nanobody (NAM) Nb61, determined by X-ray diffraction at 3.50 Å resolution (PDB ID: 8QZ2). The inset shows the detailed interaction interface, with key contacts involving residues Threonine 57 (Thr-57) and Arginine 105 (Arg-105) of the nanobody and Histidine 135 and Glutamate 270 (Glu-270) from the channel respectively. The binding of Nb61 stabilizes a closed or non-conducting state of the channel. (B) The structure of TREK-2 with the activatory nanobody (PAM) Nb67, determined by X-ray diffraction at 2.4 Å resolution (PDB ID: 8QZ3). In contrast to Nb61, Nb67 potentiates channel activity. The inset highlights interactions with Arginine 53 (Arg-53) of the nanobody and Glutamate 113 (Glu-113) of the channel. (C) The structure of TREK-2 with a second activatory nanobody (PAM), Nb76, determined by X-ray diffraction at 3.2 Å resolution (PDB ID: 8QZ4). The binding mode of Nb76 is similar to that of Nb67, involving interactions with Glutamate 113 (Glu-113) of TREK-2 and Arginine 100 (Arg-100) of the nanobody. The juxtaposition of these structures reveals the subtle structural determinants of functional switching. Minute differences in the binding pose and the specific network of molecular contacts established by each nanobody are sufficient to either stabilize a closed conformation (inhibition) or promote an open conformation (activation) of the channel's gate. This provides an atomic-level roadmap for the rational design of allosteric modulators with precisely tuned activities.

linked to the selectivity filter and conformational changes between functional states. Through this precise modulation of TREK-2 activity, these nanobody tools offer valuable therapeutic potential for neuroprotection and pain management by dampening excessive neuronal excitability.¹⁷

ASIC1a channel

ASIC1a is a proton-gated sodium channel that is primarily involved in pain perception, particularly in conditions like ischemic injury, neuropathic pain, and other forms of nociception. The activation of ASIC1a can lead to the rapid influx of

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sodium ions into cells, contributing to the generation of pain signals.¹⁸ The hASIC1a channel is a trimer with each extracellular domain subunit depicting a palm, thumb, and finger-like architecture.

The cryo-EM structure of human ASIC1a with nanobody Nb.C1 revealed that the nanobody binds to the extracellular thumb domain (D298 and L299), which is an important part of the channel that helps detect acidity and control channel

opening or closing (Fig. 3A). However, Nb.C1 binding to ASIC1a channels did not affect channel dynamics (Fig. 3A). Interestingly, Nb.C1 attaches to a site on ASIC1a that partly overlaps with the binding sites of some snake toxins, such as MitTx1 and Mambalgin-1, which normally activate or modulate the channel. Thus, Nb.C1 binding to ASIC1a was demonstrated to mitigate the effects of MitTx1 on ASIC1a channels. Because of this, Nb.C1 can block toxins like MitTx1 from activating the

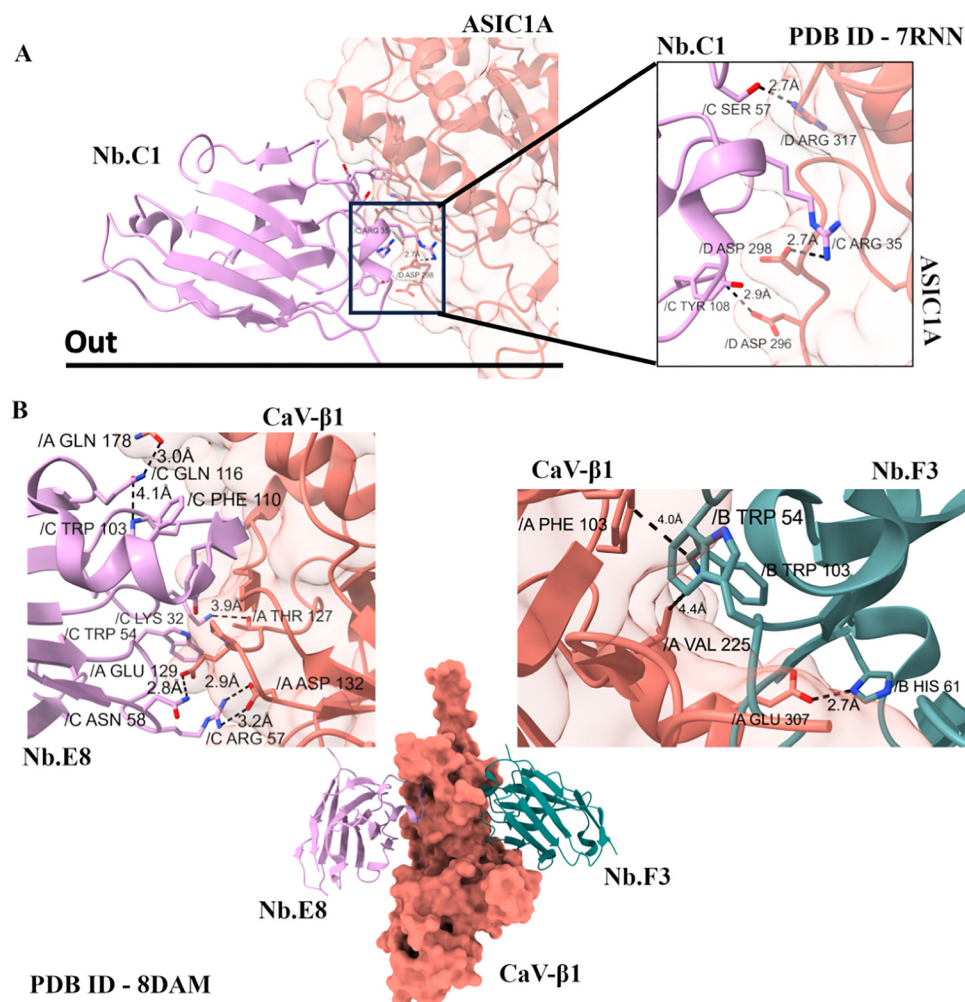


Fig. 3 Nanobody Recognition of Cytoplasmic and Extracellular Epitopes on Voltage-Gated Calcium and Acid-Sensing Ion Channels. (A) Cryo-electron microscopy (Cryo-EM) structure of the trimeric human Acid-Sensing Ion Channel 1a (ASIC1a, salmon) in complex with nanobody Nb.C1 (plum) at a resolution of 2.9 Å (PDB ID: 7RNN). ASIC1a is a proton-gated sodium channel implicated in pain, fear, and ischemia-induced neuronal injury. The structure reveals that Nb.C1 binds to an extracellular epitope that critically overlaps with the binding sites for the Texas coral snake toxin (MitTx1) and black mamba venom Mambalgin-1, but not the inhibitory tarantula toxin psalmotoxin-1 (PcTx1). This specific binding profile establishes Nb.C1 as a molecular tool for dissecting toxin-channel interactions and as a potential antidote. Furthermore, this structural knowledge has enabled advanced protein engineering; fusion of the site-specific but non-inhibitory Nb.C1 to PcTx1 was shown to markedly enhance the toxin's potency, demonstrating the use of nanobodies as delivery modules to increase the effective local concentration of a functional payload at a specific protein surface. (B) Structural details of nanobody binding to the cytoplasmic CaV β auxiliary subunit of a high-voltage activated calcium channel (HVACC). The central panel shows a cartoon representation of the CaV β 1 subunit (salmon) bound by two distinct nanobodies, Nb.E8 (plum) and Nb.F3 (green), which recognize non-overlapping epitopes. Targeting an intracellular auxiliary subunit, rather than the pore-forming subunit, represents a sophisticated allosteric strategy to modulate the function of the entire channel complex from within the cell. The left inset provides a detailed view of the Nb.E8 interface, highlighting a key electrostatic interaction between Arginine 57 (Arg-57) of the nanobody and Aspartate 132 (Asp-132) of CaV β 1, with an interaction distance of 2.9 Å. The right inset details the Nb.F3 interface, showing a hydrogen bond between Histidine 61 (His-61) of the nanobody and Glutamate 307 (Glu-307) of CaV β 1, with a distance of 2.7 Å. Other residues of the nanobody, including Trp-54, Tyr102, Trp-103, and Asp-111, also contribute to the binding interfaces. These structures exemplify how intracellularly expressed nanobodies (intrabodies) can be developed as tools to dissect or modulate channel function *via* their associated proteins.

channel by taking up their binding space. On its own, Nb.C1 does not strongly change the normal activity of ASIC1a. Interestingly, when Nb.C1 is linked with PcTx1, it acts like a “delivery tool.” It places PcTx1 in the perfect position to block ASIC1a more efficiently, making the inhibition stronger. It’s important to note here that this synergy is possible as Nb.C1 does not overlap with the binding site of PcTx1 which is another well-known ASIC inhibitor. Functionally, Nb.C1 has two roles: it acts as an antagonist against toxin-driven activation and as a potentiator when fused with inhibitors.¹⁹ By selectively binding to ASIC1a, nanobody Nb.C1 can fine-tune channel activity without completely shutting it down. Since ASIC1a is strongly linked to pain perception, inflammation, and neurodegeneration, its modulation using nanobodies offers a powerful therapeutic strategy.

Targeting intracellular auxiliary subunits: a strategy for HVACCs

High-voltage-activated calcium channels (HVACCs) are crucial in neurons and cardiac cells, regulating synaptic transmission and heart rhythm. Dysfunctions in HVACCs contribute to disorders like epilepsy, hypertension, and heart failure.

Nb.F3 is a nanobody that does not differentiate between CaV β isoforms and binds to all the isoforms, while Nb.E8 is specific to CaV β_{2a} and CaV β_{1b} . To address these, nanobodies such as nb.F3 have been engineered for isoform-specific inhibition of HVACCs. Nb.F3 interacts with CaV β through complementing aromatic residues on CDR3 of the nanobody and the SH3 domain of CaV β . Differences in Nb.E8 CDR3 regions might be essential in differentiating the CaV β subunits (Fig. 3B). Nb.F3 acts as an allosteric inhibitor by binding the SH3 domain of the CaV β subunit, reducing channel surface expression, lowering open probability, and accelerating inactivation, thereby suppressing CaV β -associated currents. A novel approach fuses nb.F3 with ubiquitin ligases (NEDD4L) to promote targeted degradation of CaV β -bound HVACCs. Nb.F3-NEDD4L inhibited endogenous CaV1/CaV2 channels in mammalian cardiomyocytes, dorsal root ganglion neurons, and pancreatic β cells. Unlike gene knockouts or shRNA, this post-translational method prevents compensatory CaV β isoform reshuffling, allowing precise study of β -subunit roles. This approach is similar to the concept of PROTACs (proteolysis-targeting chimeras), which use bifunctional molecules to promote the degradation of specific proteins. By selectively targeting HVACCs for degradation, this nanobody-based strategy offers a novel way to treat conditions associated with these channels, such as chronic pain, epilepsy, and cardiovascular diseases.^{20,21}

2. Direct gating modification and state stabilization

Some nanobodies act more directly on the channel’s gating machinery, functioning as “gating modifiers” that lock the channel into a specific, often non-conducting, state.

The Kv1.3 channel plays a critical role in the activation of T-cells, which are key components of the immune system. This channel is often overexpressed in various autoimmune diseases, contributing to inappropriate T-cell activation and the progression of conditions such as multiple sclerosis and rheumatoid arthritis.²²

The A0194009G09 nanobody is a highly selective and potent modulator of the human Kv1.3 potassium channel. The cryo-EM structure revealed that four nanobody molecules bind to the tetramer’s voltage-sensing domains (VSDs) and the adjacent pore domain (Fig. 3A). Unlike conventional channel blockers that physically obstruct the pore-forming EL3 loop, A0194009G09 binds to an allosteric site and inhibits the Kv1.3 channel activity.²³ A0194009G09 specifically interacts with Kv1.3 residues Y417 and A421 – G427. This interaction triggers structural rearrangements in a critical part of the channel known as the selectivity filter, focusing on amino acid residues between Tyr436 and Asp449 (Fig. 4). These changes stabilize the channel in a C-type inactivated state, a conformation in which the channel remains closed and unable to conduct potassium ions despite not being physically occluding the channel pore.²⁴ This specificity and prolonged inhibition make Kv1.3-targeting nanobodies a promising therapeutic tool for modulating the immune response and treating autoimmune diseases.

P2X7 ion channel

Similarly, nanobodies targeting the P2X7 receptor, an ATP-gated ion channel critical for inflammation, cell death, and immune responses, demonstrate both inhibitory and potentiating effects. This channel is known to mediate the release of pro-inflammatory cytokines, including IL-1 β , which contribute to neuroinflammation, pain, and a variety of other inflammatory diseases.²⁵ When P2X7 is activated, it forms a large pore in the membrane, allowing the passage of ions and other molecules that trigger further inflammatory responses.

P2X7-blocking nanobodies offer precise and rapid modulation of the ATP-gated P2X7 ion channel. Nanobody 13A7 (IC₅₀ – 12 nM) efficiently inhibits P2X7 channel activity by preventing the conformational changes triggered by ATP binding in mouse macrophages and T cells. In contrast, nanobody 14D5 (EC₅₀ – 6 nM) enhances P2X7 channel function. These nanobodies act specifically on the P2X7-mediated inflammation pathway. An albumin-binding nanobody fused with 13A7 or 14D5 dimeric nanobodies increased their half-life and prolonged the effects of these nanobodies. Mouse models further verified the binding and modulation of 13A7 and 14D5. Dano1 (IC₅₀ – 0.2 nM), a human-specific nanobody that surpasses traditional small-molecule antagonists by 1000-fold in inhibiting the release of IL-1 β by monocytes in LPS and ATP-treated human blood. This superior potency arises from the ability of the nanobody to bind functional epitopes on P2X7 that conventional antibodies and drugs cannot reach.²⁶ While detailed structural data for these nanobodies is still pending, their ability to modulate P2X7 function makes them invaluable tools in studying inflammation and immune responses. As a result, P2X7-targeting nanobodies represent a promising advancement in

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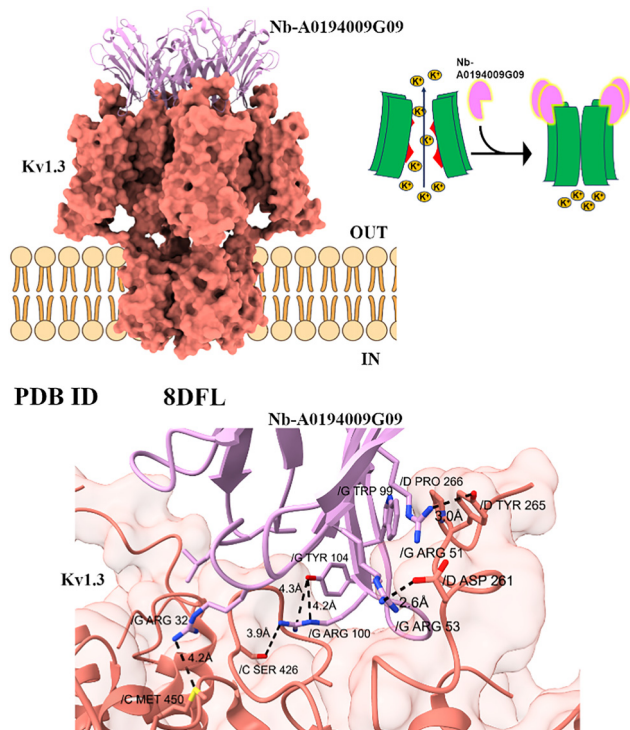


Fig. 4 Structural Basis of Nanobody Binding to Kv1.3 Channels. Cryo-EM structure of the tetrameric human Kv1.3 potassium channel (salmon) bound by four copies of the inhibitory nanobody Nb-A0194009G09 (plum), resolved to 3.25 Å (PDB ID: 8DFL). Kv1.3 is highly expressed on activated T cells, making it a prime therapeutic target for immunomodulation. This structure reveals a sophisticated allosteric mechanism of inhibition. Rather than acting as a simple pore blocker, the nanobody binds to the channel's voltage-sensing domains (VSDs) and adjacent pore domain, acting as a "gating modifier" that stabilizes an inactive, non-conducting conformation of the pore. The inset highlights a specific interaction between Arginine 100 (Arg-100) of the nanobody and Serine 426 (Ser-426) of Kv1.3, with a distance of 3.0 Å. This mechanism represents a powerful paradigm for developing highly selective channel inhibitors that modulate the gating machinery itself.

immunomodulation, with the potential to improve therapies for inflammatory and autoimmune diseases through their speed, selectivity, and enhanced efficacy.

3. Isoform, subunit, and heteromer-specific recognition

A key advantage of nanobodies is their ability to recognize unique epitopes with surgical precision, enabling the differentiation between closely related channel isoforms or specific subunit compositions within a larger complex.

Targeting specific oligomeric assemblies: CALHM and NMDA receptors

Calcium homeostasis modulator (CALHM). Calcium homeostasis modulator (CALHM) channels are large-pore, non-selective ion channels that facilitate ATP release and play essential roles in neuronal signaling, taste perception, and metabolic regulation.

CALHM1, CALHM2, and CALHM6 form homo- and hetero-oligomers, demonstrating flexible stoichiometry (such as tetramers, octamers, decamers, or dimer-of-decamer assemblies). Synthetic nanobodies Sb-C2 and Sb-C4 bind specifically to the cytoplasmic LRR-like domains of CALHM2 and CALHM4 subunits, respectively, regions that are critical for oligomer assembly and gating regulation. Structurally, the SbC2 epitope includes residues at the intracellular end of transmembrane helix TM3, the region after TM4, and part of the C-terminal loop connecting short helices CT2H and CT3H on the CALHM2 subunit. A key feature is that SbC2 binding stabilizes the C-terminus of the adjacent CALHM2 subunit, which is otherwise unstructured. This extensive binding interface ($\sim 2200 \text{ \AA}^2$) results in strong, specific recognition of CALHM2. The interaction is predominantly mediated *via* hydrophobic interactions and CH- π bonds²⁷ (Y110 of the nanobody and P322 of the receptor) (Fig. 5A). SbC4 specifically binds to the extracellular regions of CALHM4 subunits, which were not clearly delineated in the structure to pinpoint residue-level interactions (Fig. 5B). By enabling atomic-level mapping of CALHM assemblies, nanobodies pave the way for drug design targeting CALHM-mediated ATP release in conditions like Alzheimer's disease, ischemia, and taste disorders.²⁸

NMDA (*N*-methyl-D-aspartate) receptor. This principle is extended to the highly complex *N*-methyl-D-aspartate (NMDA) receptors, which are heterotetramers crucial for synaptic plasticity. *N*-methyl-D-aspartate receptors (NMDARs) are glycine- and glutamate-gated ion channels. Under physiological conditions, they function as heterotetramers, typically composed of two essential GluN1 subunits paired with two GluN2 (A-D) and/or GluN3 (A-B) subunits. The GluN1 subunits bind glycine, while the GluN2 subunits bind glutamate. Functionally, NMDARs are crucial for synaptic plasticity, learning, and memory by mediating calcium influx upon activation. Nb4 binds specifically to the extracellular domain of the GluN2A subunit, probably near the ligand-binding domain, but does not act as an agonist; instead, it serves as a modulator or stabilizer of receptor conformation (Fig. 6A and B).²⁹

Distinguishing between isoforms: NaV1.4 and NaV1.5 channels. NaV1.4 and NaV1.5 are voltage-gated sodium channels found in skeletal muscle and cardiac tissue, respectively. The nine human voltage-gated sodium channel isoforms (NaV1.1–1.9) mediate rapid sodium ion influx, essential for action potential generation in excitable tissues such as skeletal muscle, heart, and nerves. Mutations in the cytoplasmic C-terminal domain of these channels are linked to genetic disorders, including epilepsy, periodic paralysis, myotonia, and cardiac arrhythmias.³⁰

While many nanobodies are functional modulators, others serve as high-fidelity detection tools. Nanobodies Nb17 and Nb82 were developed to bind the C-terminal domains of the skeletal muscle (NaV1.4) and cardiac (NaV1.5) voltage-gated sodium channels, respectively. They bind with nanomolar affinities ($\sim 40\text{--}60 \text{ nM}$) and minimal cross-reactivity to other isoforms. Although they do not modulate channel gating or ion conductance, they serve as powerful molecular tools for

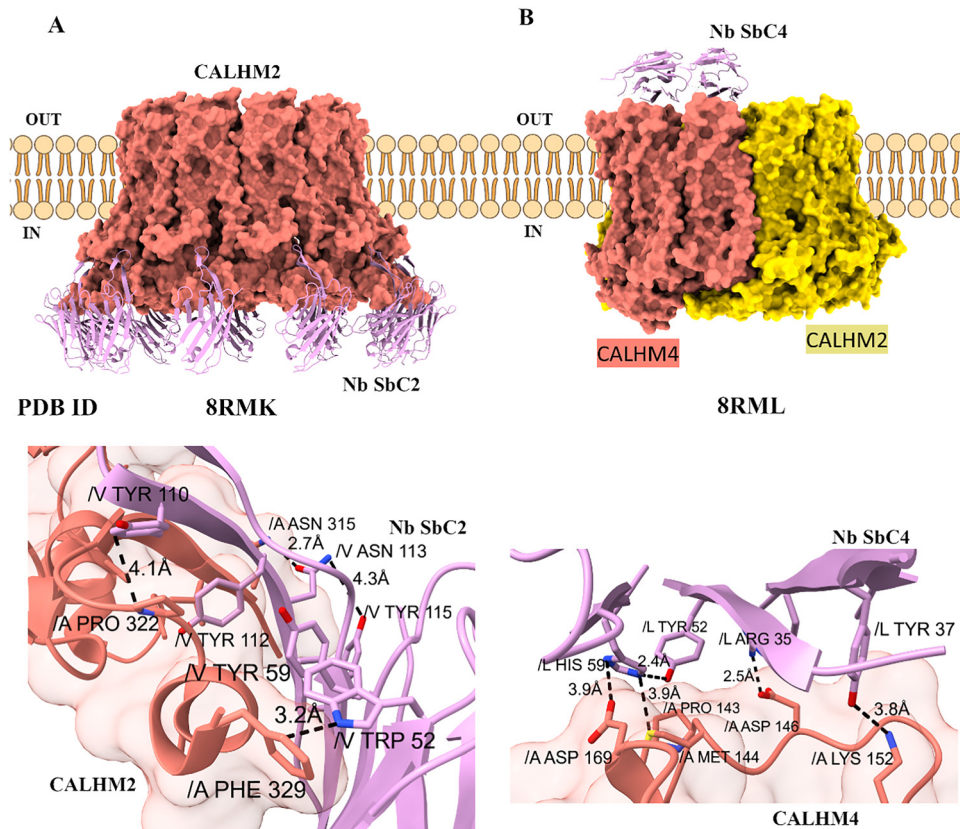


Fig. 5 Structural Basis of Nanobody Binding to Oligomeric CALHM channels. (A) Cryo-EM structure of the homomeric human Calcium Homeostasis Modulator 2 (CALHM2) channel (salmon) in complex with the synthetic nanobody Sbc2 (plum), resolved to 3.07 Å (PDB ID: 8RMK). CALHM2 is a pore-forming subunit of a voltage-gated ion channel. The inset shows a detailed view of the interaction interface, highlighting key contacts contributed by Tyrosine 59 (Tyr-59), Tyrosine 110 (Tyr-110), and Asparagine 113 (Asn-113) from the nanobody's complementarity-determining regions (CDRs). (B) Cryo-EM structure of the heteromeric human CALHM2/4 channel in complex with the synthetic nanobody Sbc4 (plum), resolved to 3.84 Å (PDB ID: 8RML). This structure provides a compelling example of heteromer-specific recognition. The nanobody binds to a "neo-epitope" formed at the interface between the CALHM2 subunit (gold) and the CALHM4 subunit (salmon). The inset reveals that the interaction is mediated by contacts between CALHM4 and Sbc4, including Aspartate 146 (Asp-146) from CALHM4 and Arginine 35 (Arg-35) from Sbc4, with a representative interaction distance of 2.5 Å shown. The ability to target a unique chemical and topographical landscape present only in a specific subunit combination is a hallmark of nanobody selectivity and provides a blueprint for designing biologics that can differentiate between closely related heteromeric channel assemblies.

isoform-specific detection, imaging, and biochemical isolation. The specificity and high affinity of Nb17 and Nb82 provide valuable reagents for dissecting the biology of NaV channels and hold promise for developing targeted diagnostics or therapeutic tools, particularly for skeletal and cardiac muscle disorders linked to NaV dysfunction.³¹

4. Nanobodies as structural chaperones and probes of Cys-loop receptors

The Cys-loop receptor superfamily of pentameric ligand-gated ion channels (pLGICs) has been a particularly fertile ground for nanobody development, where they have served as both functional modulators and indispensable tools for structural biology.

Probing a Conserved Allosteric Vestibule: From ELIC to 5-HT₃.

Cys-loop receptors

Cys-loop receptors constitute a family of pentameric ligand-gated ion channels, encompassing both cation-selective members such as serotonin 5-HT₃ and nicotinic acetylcholine (nACh) receptors, the zinc-activated (ZAC) receptor, as well as anion-selective types including GABA and glycine receptors. The characteristic "Cys-loop" is a conserved disulfide-bonded loop in the extracellular domain essential for structural integrity and function. These receptors mediate fast synaptic transmission by opening their ion channels in response to neurotransmitter binding, allowing selective flow of ions across the membrane for excitatory or inhibitory signalling. Dysfunction in these receptors has been linked to a variety of neurological and psychiatric disorders, including epilepsy, schizophrenia, and neurodegenerative diseases. Therapeutic nanobodies against Cys-loop receptors may be developed to modulate neurological diseases associated with dysfunctional inhibitory or excitatory signaling.³² The prokaryotic channel ELIC serves as an excellent model for its human counterparts.

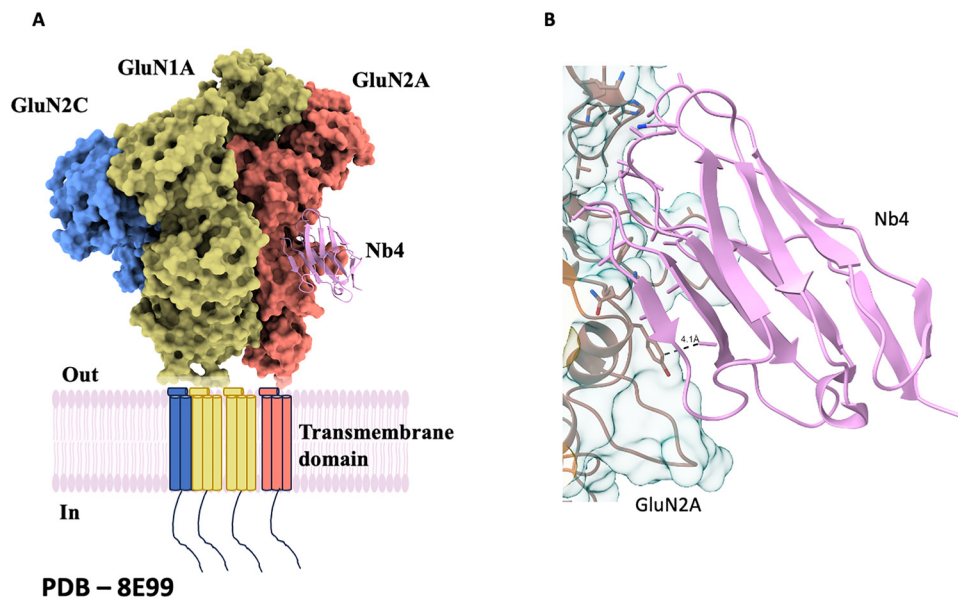


Fig. 6 Subunit-Specific Targeting of a Tri-heteromeric NMDA Receptor Complex. (A) A structural model of a tri-heteromeric N-methyl-D-aspartate (NMDA) receptor, composed of one GluN1 subunit (gold), one GluN2A subunit (salmon), and one GluN2C subunit (blue). The nanobody Nb4 (plum) is shown binding with exquisite specificity to the GluN2A subunit. The binding site is located at the critical interface between the amino-terminal domain (ATD) and the ligand-binding domain (LBD) of the GluN2A subunit. This ATD-LBD interface is a well-established allosteric hub that controls the gating of the ion channel pore. By targeting a region that differs between GluN2 isoforms, the nanobody achieves its remarkable subunit selectivity. (B) A detailed view of the molecular contacts at the interaction interface between the GluN2A subunit and Nb4. A representative interaction distance of 4.1 Å is indicated. The ability to selectively modulate the function of only those NMDA receptors containing a specific subunit (e.g., GluN2A) is of immense therapeutic interest, as it could allow for the treatment of neurological disorders with greater precision and fewer side effects compared to non-selective channel blockers. This structure provides an atomic-level blueprint for an isoform-specific pharmacological strategy.

Nanobodies targeting its large extracellular vestibule have revealed a conserved modulatory hotspot.

(a) ELIC (Erwinia ligand-gated ion channel). The *Erwinia* ligand-gated ion channel (ELIC) is a prokaryotic member of the Cys-loop receptor family that serves as a structural and functional model for human pentameric ligand-gated ion channels. Two nanobodies, Nb21 (Negative Allosteric modulator) and Nb22 (Positive Allosteric modulator), have been developed against ELIC. Both nanobodies bind to the extracellular domain (ECD) of ELIC but stabilize the receptor in distinct functional conformations. Nb22 is a positive allosteric modulator that interacts with every subunit of the pentameric receptor on the extracellular domain. The CDR1 loop of the nanobody interacts between the $\beta 8$ – $\beta 9$ strands. The CDR1 loop forms an anti-parallel β -sheet-like conformation with the receptor's β -strands. In contrast, Nb21 functions as a negative allosteric modulator; the CDR3 α -helix binds to the top of the extracellular domain at the entry site, blocking the channel pore at the top.³³ Nb72 binding to ELIC is similar to Nb22-ELIC interaction. It interacts with the $\beta 9$ – $\beta 10$ strands of the orthosteric site and also with the N-terminal $\beta 6$ – $\beta 7$ loop. These inter-subunit interactions likely restrict subunit movements, thereby stabilizing the receptor in a particular conformational state (Fig. 7A and B).³⁴

These nanobodies with improved stability, blood–brain barrier penetration, and pharmacokinetics could be used to treat neurological disorders, including epilepsy, schizophrenia,

chronic pain, and addiction, offering receptor-specific therapies with high precision and minimal off-target effects.

(b) Serotonin 5-HT₃ receptor. The 5-hydroxytryptamine type 3 (5-HT₃) receptor is a cation-selective ion channel belonging to the Cys-loop superfamily. When serotonin binds to the 5-HT₃ receptor, it induces a conformational change that quickly opens the ion channel. This allows sodium (Na⁺), potassium (K⁺), and calcium (Ca²⁺) ions to enter the neuron. The resulting cation influx depolarizes the cell membrane, producing a rapid excitatory signal in neurons of both the central and peripheral nervous systems. During brain development, the 5-HT₃ receptor plays a critical role in regulating neuronal circuit formation, dendritic growth, and synaptic organization. Disruption of 5-HT₃ receptor signaling, whether through genetic variations or environmental factors such as stress or drug exposure, can lead to altered brain wiring and cognitive deficits. Such dysfunctions have been associated with neurodevelopmental disorders, including autism spectrum disorders (ASD), schizophrenia, bipolar disorder, and anxiety-like behaviors.³⁵

As in ELIC, the vestibule site where nanobody binds is conserved. In the mouse serotonin 5-HT₃ receptor, VHH15 binds to the equivalent site. Functional analysis demonstrates that this binding inhibits the channel activation by serotonin. This indicates that the receptor adopts a conformation corresponding to an inhibited, non-conducting state, preventing ion flow through the channel despite the presence of the

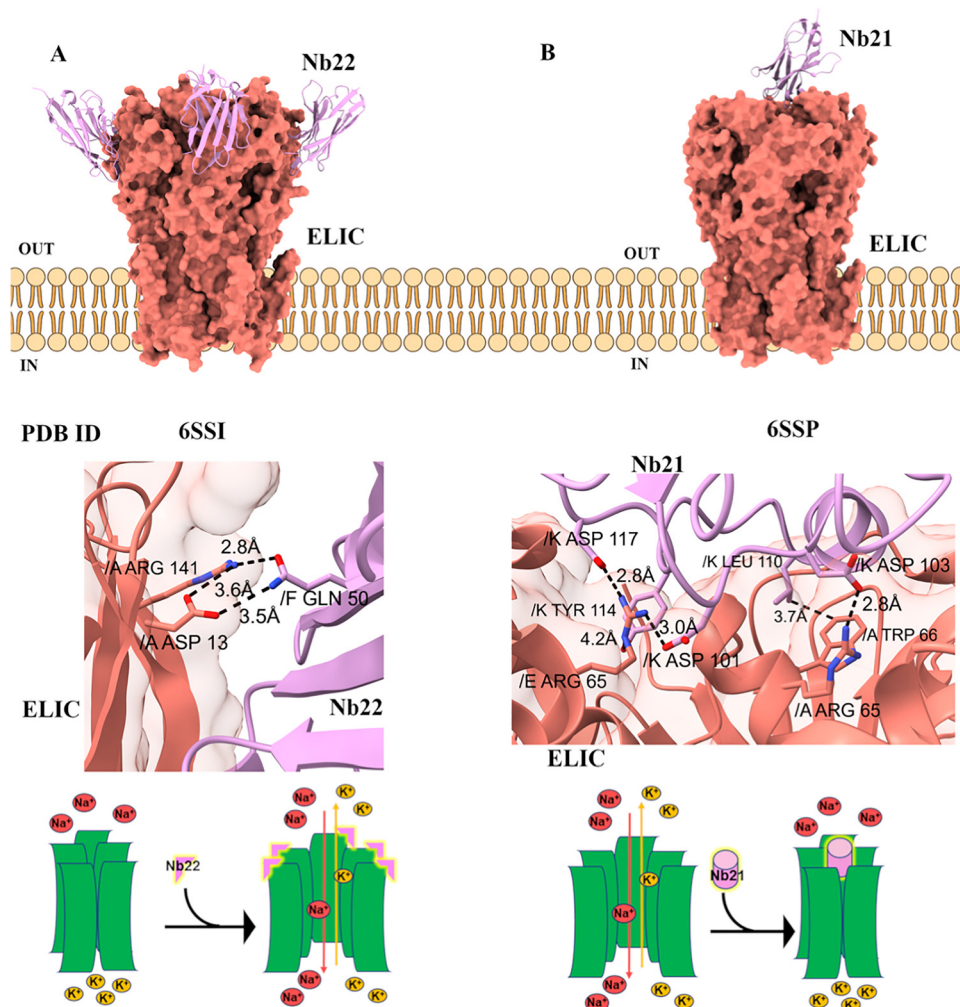


Fig. 7 Nanobody Targeting of a Conserved Vestibule Site in Cys-Loop Receptors – ELIC receptors. This figure illustrates the targeting of a conserved allosteric modulatory site within the extracellular vestibule of pentameric ligand-gated ion channels (pLGICs), bridging a prokaryotic channel homolog with a pharmacologically important eukaryotic receptor. (A) X-ray crystal structure of the pLGIC from *Dickeya chrysanthemi*, ELIC (salmon), in complex with the Positive allosteric modulator (PAM) Nb22 (plum), resolved to 2.59 Å (PDB ID: 6SSI). The top panel shows Nb22 binding within the large extracellular vestibule of the pentameric channel. The bottom panel provides a detailed view of the interface, highlighting a key salt bridge between Arginine 141 (Arg-141) of ELIC and Glutamine 50 (Gln-50) of Nb21, with a distance of 2.8 Å. (B) X-ray crystal structure of ELIC (salmon) with the negative allosteric modulator (NAM) Nb21 (plum), resolved to 3.25 Å (PDB ID: 6SSP). Nb21 binds to a partially overlapping site within the same vestibule, demonstrating that this region can accommodate modulators with opposing functional effects. The detailed view highlights interactions utilizing Arginine 65 (Arg-65) from two different domains of ELIC and several residues within the CDRs of Nb21, including Asp-101, Asp-103, and Asp-117.

neurotransmitter. Nanobody binding to the 5-HT₃ receptor can influence neurotransmitter recognition by stabilizing the extracellular ligand-binding domain, particularly the flexible loops that form the orthosteric binding site. By capping or interacting with regions such as the C-loop and adjacent structural elements, nanobodies restrict the conformational dynamics necessary for efficient serotonin binding and receptor activation. This stabilization may either lock the receptor in a resting, inactive state or modulate its transition states, thereby altering the affinity and efficacy of neurotransmitter binding (Fig. 8).³⁶ Numerous functional modulator nanobodies (activating and inhibiting) have been generated against 5-HT₃AR and m5-HT₃AB receptors. These nanobodies were found to have a

strong affinity for the receptors, with K_d values ranging from low nanomolar to submicromolar concentrations.³²

Diverse mechanisms in human pLGICs: nAChR and GABAARs

Human $\alpha 7$ nicotinic acetylcholine receptor (nAChR). The human $\alpha 7$ nicotinic acetylcholine receptor (nAChR) is a pentameric ligand-gated ion channel crucial for neuronal communication. In human Cys-loop receptors, nanobodies display an even wider range of actions. The cryo-EM structure of the human $\alpha 7$ nicotinic acetylcholine receptor (nAChR) in complex with nanobody E3 reveals a pentameric receptor capped by five E3 nanobodies at the extracellular domain (ECD). E3 binds at the apical inter-subunit site, stabilizing an agonist-like

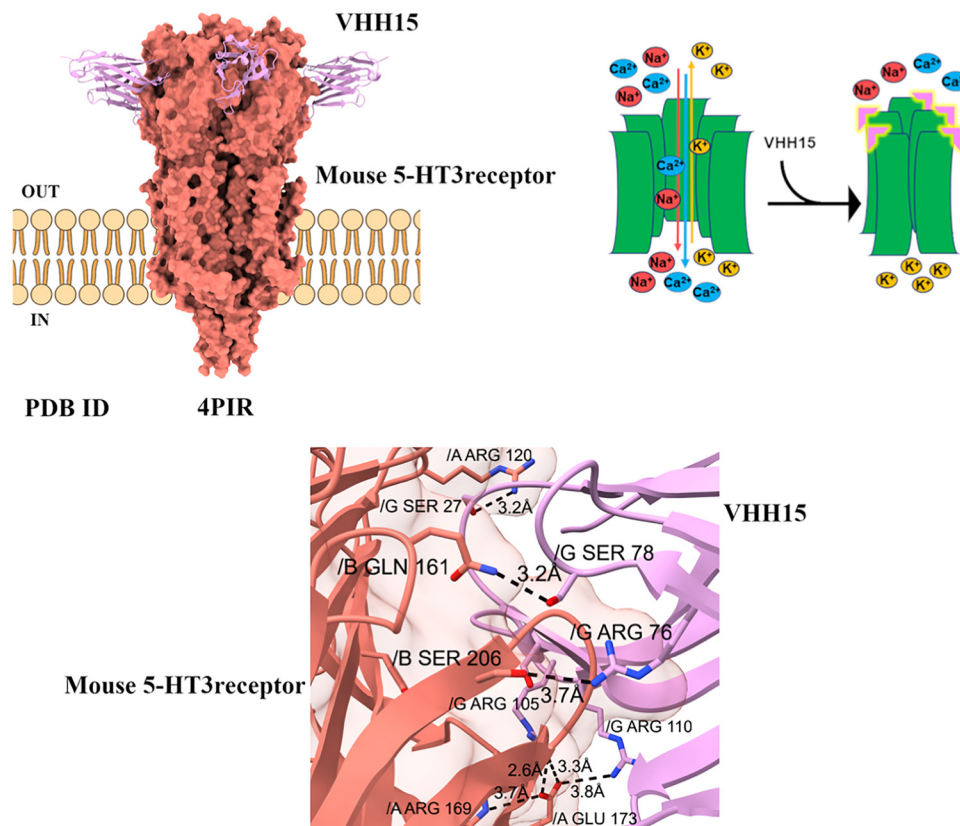


Fig. 8 Nanobody Targeting of a Conserved Vestibule Site in Cys-Loop Receptors – 5-HT₃ receptor. X-ray structure of the eukaryotic mouse serotonin 5-HT₃ receptor (salmon) in complex with nanobody VHH15 (plum), resolved to 3.5 Å (PDB ID: 4PIR). Functional studies have shown that the vestibule binding site identified in ELIC is conserved and functionally relevant in the human 5-HT₃ receptor. The bottom panel shows two key interactions at this site: a 3.2 Å interaction between Arginine 120 (Arg-120) of the receptor and Serine 27 (Ser-27) of the nanobody, and a 3.3 Å interaction between Arginine 105 (Arg-105) of the receptor and Glutamate 173 (Glu-173) of the nanobody. Together, these structures suggest that the extracellular vestibule is an evolutionarily conserved allosteric “hotspot”, validating the use of prokaryotic homologs like ELIC as robust platforms for discovering and characterizing modulators of their more complex human counterparts.

conformation even without the presence of an agonist. This interaction extends the extracellular domain and involves contacts with an N-linked sugar moiety of receptor Asn23 and Arg56 of the nanobody. The nanobody binding induces conformational changes that promote channel activation by allosterically stabilizing an active-like state (Fig. 9A). In contrast, Nanobody C4 binds to the same apical inter-subunit epitope on the human $\alpha 7$ nicotinic acetylcholine receptor as Nanobody E3 but functions as a silent allosteric ligand. Unlike E3, C4 does not significantly alter receptor gating or promote channel activation. Its binding stabilizes the receptor without inducing the conformational changes necessary for enhanced ion flow. But C4 binding to nAChR inhibits the E3-induced potentiating effect. The differences in the modulations of the two nanobodies probably stem from the fact that the CDR3 residues and their interacting residues in the receptor are different.^{37,38}

Type A γ -aminobutyric acid receptors (GABA_ARs). GABA_A receptors (GABA_ARs) are pentameric ligand-gated ion channels that mediate the majority of fast inhibitory neurotransmission in the brain. The GABA_A receptor family comprises 19 different types of subunits, designated as $\alpha 1$ -6, $\beta 1$ -3, $\gamma 1$ -3, δ , ϵ , θ , π , and $\rho 1$ -3. In the brain, specific subunits are formed in

certain neurons and tend to assemble in particular ways. Most GABA_A receptors in the human brain are made up of 2 α subunits, 2 β subunits, and 1 γ subunit. Among these, the $\alpha 1$, $\beta 2$, $\beta 3$, and $\gamma 2$ subunits are the most commonly found and often appear together in the same areas. Each receptor is composed of five subunits arranged around a central pore, typically assembled from combinations of α , β , and γ subunits, with $\alpha 1\beta 2\gamma 2$ being a common adult isoform. Dysfunction of the GABA_A receptor (GABAAR) is linked to various neurological and psychiatric disorders due to its central role in inhibitory neurotransmission.^{39,40}

Nanobody38 (Nb38) that specifically binds to the $\alpha 1$ subunit of the GABA_A receptor. Structural and functional studies show that Nb38 binds at the extracellular domain interfaces involving the $\alpha 1$ principal face and the complementary faces of neighbouring $\beta 3$ and $\gamma 2$ subunits. This binding stabilizes the receptor in an activated conformation, as evidenced by an approximately 6.5-fold increase in Nb38 binding affinity in the presence of GABA. Functionally, Nb38 strongly potentiates GABA-induced currents, increasing receptor activity by up to 480% in $\alpha 1\beta 3\gamma 2$ engineered receptors and about 290% in wild-type receptors. This potentiation is selective for receptors

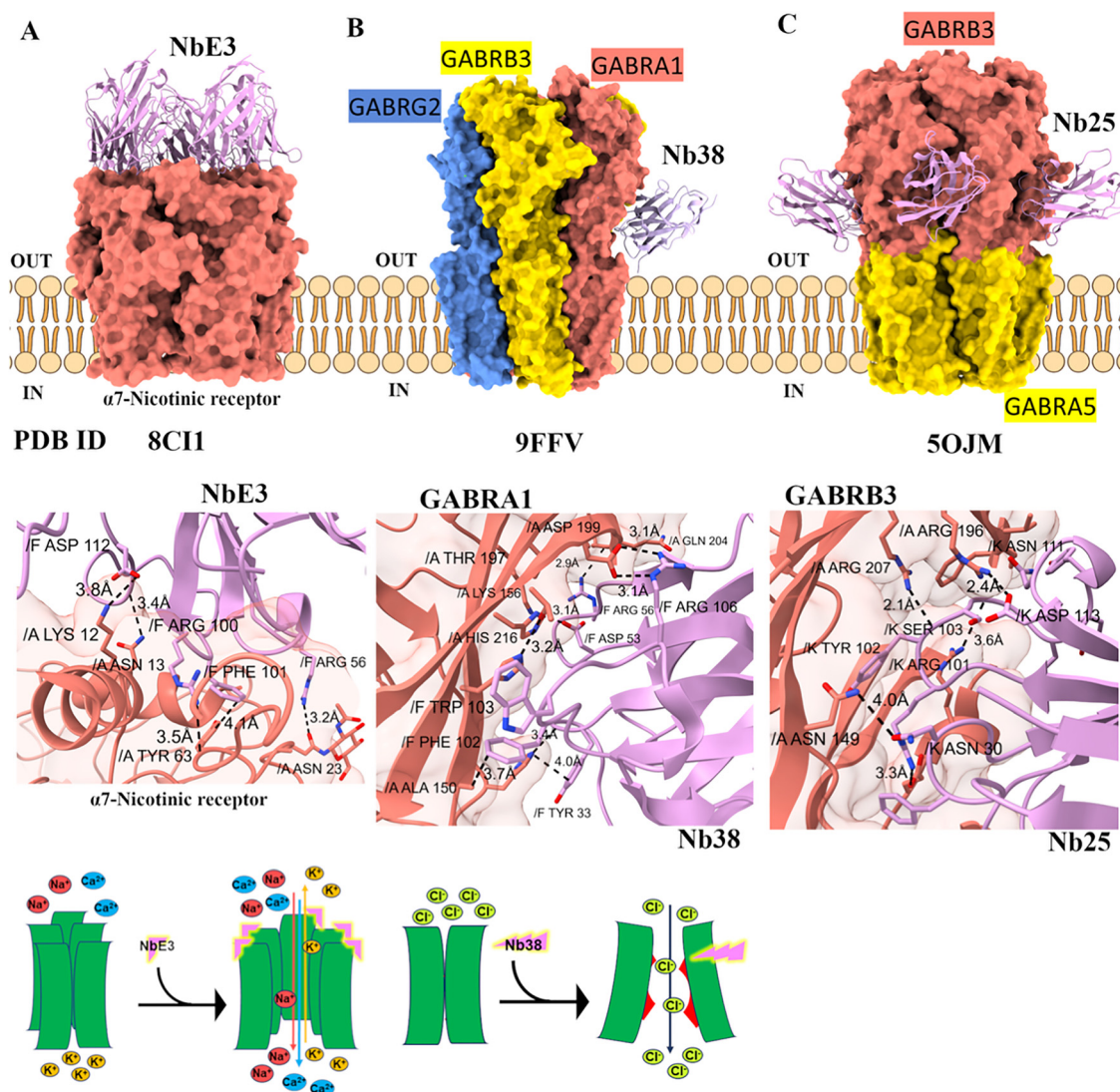


Fig. 9 Diverse Modulatory Mechanisms of Nanobodies Targeting Human Cys-Loop Receptors. We highlight the remarkable versatility of nanobodies in modulating the function of major human pLGICs and in facilitating their structural determination. (A) Cryo-EM structure of the human $\alpha 7$ nicotinic acetylcholine receptor (nAChR, salmon) in complex with the positive allosteric modulator (PAM) NbE3 (plum), resolved to 2.8 Å (PDB ID: 8CI1). NbE3 employs a novel modulatory mechanism: five nanobody molecules bind at the apex of the pentameric receptor, at the interfaces between subunits, forming their own pentameric assembly that extends the extracellular domain. This binding remotely drives the receptor into an agonist-bound conformation even in the absence of an orthosteric agonist, effectively acting as a “surrogate agonist”. The bottom panel details interactions involving Arginine 56 (Arg-56) of the nanobody and Asparagine 23 (Asn-23) of the receptor, with a distance of 3.2 Å. (B) Cryo-EM structure of the human $\alpha 1\beta 3\gamma 2$ GABAA receptor ($\alpha 1$ – salmon, $\beta 3$ – gold, and $\gamma 2$ – blue) with Nb38 (plum), resolved to 2.8 Å (PDB ID: 9FFV). In this context, Nb38 functions as a conformational stabilizer, trapping the receptor in a “long-lived symmetric resting state”. Such conformational locking is invaluable for high-resolution structural studies of large, flexible membrane proteins. The bottom panel shows the extensive interaction network, involving Lys-156, Asp-199, and Gln-204 from the receptor and Asp-53 and Arg-106 from the nanobody. (C) X-ray structure of a chimeric $\beta 3$ - $\alpha 5$ GABAA receptor ($\beta 3$ – salmon, $\alpha 5$ – gold) with Nb25 (plum), resolved to 3.3 Å (PDB ID: 5OJM). Similar to Nb38, Nb25 was employed as a crystallization chaperone, providing a rigid scaffold that stabilized the receptor and enabled the determination of its structure in the presence of neurosteroids. The bottom panel highlights a tight, 2.4 Å interaction between Arginine 196 (Arg-196) of the receptor’s $\beta 3$ subunit and Aspartate 113 (Asp-113) of Nb25. These examples demonstrate that nanobodies are not only modulators but also indispensable tools that enable fundamental discoveries by stabilizing specific functional states of ion channels for structural analysis.

containing the $\alpha 1$ subunit and is more effective than the benzodiazepine diazepam in amplifying GABA responses. Additionally, Nb38 increases the amplitude and prolongs the decay time of spontaneous inhibitory postsynaptic currents (sIPSCs) in neurons, thereby enhancing inhibitory neurotransmission. The gating mechanism involves Nb38 stabilizing the receptor’s

activated state without acting as a direct agonist itself. By binding near the ligand-binding site interfaces, Nb38 likely promotes conformational changes that favor channel opening and prolonged activity, enhancing the inhibitory function of GABA_A receptors containing the $\alpha 1$ subunit. Nb38 interacts with the GABA_A receptor *via* aromatic residues on opposite

Highlight

faces of the binding interface, leading to π - π stacking interactions. Hydrogen bonds between a few polar residues further stabilize the interaction (Fig. 9B).⁴¹ Nb25 is a nanobody that specifically binds to the β 3 extracellular domain (ECD) of the GABA_A receptor. Structural studies using cryo-EM revealed that three Nb25 molecules bind between adjacent ECD interfaces of the α 5 β 3 GABA_A receptor, particularly at interfaces involving β 3 subunits. This binding helps to identify and distinguish β 3 subunits in receptor assemblies, which is especially useful because α 5 and β 3 subunits have similar sequences and structures that make them hard to differentiate at lower resolution (Fig. 9C). Functionally, Nb25 binds at the interfaces between β subunits, and although it binds tightly, it does not show significant potentiation effects like Nb38. Nb25 has been used as a tool in structural studies to facilitate receptor crystallization and improve classification of receptor particles in cryo-EM analysis.⁴²

Stabilizing elusive domains: the case of volume regulated anion channels (VRACs). Homomeric LRRC8A channels, a core component of the volume-regulated anion channel (VRAC), are essential for cellular osmotic balance. These channels are activated during cell swelling, allowing chloride and other solutes to exit and restore normal cell volume. Beyond this basic role, LRRC8A has been linked to important physiological and pathological processes, including insulin secretion, glucose regulation, tumor progression, and central nervous system disorders such as cerebral ischemia.⁴³ Recently, synthetic nanobodies known as sybodies have been developed to specifically target the cytoplasmic leucine-rich repeat (LRR) domain of LRRC8A. Biophysical and cryo-EM analyses demonstrate that sybodies (synthetic nanobodies) Sb1 to Sb5 bind to the proteins with an affinity in the order of nanomolar range to the LRR domain of LRRC8A, while they do not show any binding to the LRR domains of LRRC8C and LRRC8D. The sybodies stabilize the channel in specific conformations of LRRC8A. The Cryo-EM structure of LRRC8A/Sb1 complex shows that sybody binding stabilizes the flexible cytoplasmic LRR domains, enabling the determination of the structural feature of these regions, which are poorly defined in the apo form of LRRC8A. Sb1 interacts with the LRR repeats 8–11 through all three CDR regions. The sybody interacts with a hydrophilic region of the LRR repeats, mediated by a majority of aromatic residues (~10 residues) in the sybody that form hydrogen-bonded contacts and cation- π and anion- π interactions. Sybodies Sb2 and Sb3 target the same epitope on the LRR domain despite different binding modes because the epitope is a structurally accessible and conserved site near the transmembrane region. Their distinct sequences and binding kinetics result in variations in their interaction, yet both recognize repeats 3–6 on the convex face of the LRR domain. Although Sb2 and Sb3 bind similarly to the same epitope, the significant difference in their dissociation constants is mainly due to Sb3 having an approximately 20-fold faster off-rate than Sb2.

Contrary to the interactions observed in sybody Sb1, the interaction interface of sybodies Sb2 and Sb3 contains fewer aromatic residues and more hydrophilic residues. All three

nanobodies inhibit the LRRC8A by restricting the LRR domain (Sb1) or inducing conformational changes in the LRR domain and pore region (Sb2 and Sb3). Sybodies Sb4 and Sb5 potentiate channel activity by binding to alternate subunits of the LRR domain and are buried in the dimer interfaces of the domains, specifically engaging repeats 2–14 (Sb4) and 2–7 (Sb5). These sites are accessible only in specific subunit positions due to the arrangement of subunits within the channel. Functionally, Sb4 and Sb5 serve as allosteric activators, increasing VRAC channel activity by enhancing LRR domain mobility and triggering conformational changes that likely promote channel opening.⁴⁴ Beyond mechanistic importance, these findings link LRRC8A modulation to physiological roles such as insulin secretion, glucose control, tumor progression, and ischemic brain injury, highlighting sybody-channel complexes as a promising therapeutic target.

5. Indirect modulation of ion channels via GPCRs: the mGluR2/NMDAR axis

Nanobodies can also modulate ion channels indirectly by targeting associated signaling proteins. Metabotropic glutamate receptors (mGluRs), which are G protein-coupled receptors (GPCRs), form a well-known functional complex with NMDARs. They are known to play crucial roles in modulating excitatory neurotransmission in the brain. Nanobodies DN10 and DN13 were developed as selective positive allosteric modulators of the mGluR2 receptor.

These nanobodies bind to the intracellular domain of the receptor, close to the G protein-coupling interface, where they stabilize specific conformations of the receptor. DN13 binds specifically to agonist-bound mGlu2 homomers and enhances their activity. DN1 nanobody demonstrated binding to both homomer and heteromer conformations of mGlu2, without affecting receptor function.⁴⁵ A DN1–DN13 biparatopic nanobody enhanced the affinity to mGlu2. The DN1–DN13 nanobody improved working memory in GluN1 knockdown mice models.⁴⁶ By fine-tuning the conformational states of mGluR2, these nanobodies provide a powerful means to probe receptor function, dissect mGluR2–NMDA receptor cross-talk, and inspire novel therapeutic strategies for neurological disorders such as schizophrenia, anxiety, and excitotoxic neurodegeneration. This highlights a sophisticated strategy where a nanobody targeting a GPCR can precisely regulate the function of a downstream ion channel (Fig. 10).

Breaking down the fortress: delivering nanobody across the blood–brain barrier

The blood–brain barrier (BBB) is a selective permeability barrier that protects the brain from harmful substances while regulating the passage of essential nutrients and molecules. However, this selective barrier also presents a significant challenge in delivering therapeutics to the central nervous system (CNS), particularly for large molecules such as antibodies. Nanobodies, with their small size and high stability, offer a promising solution

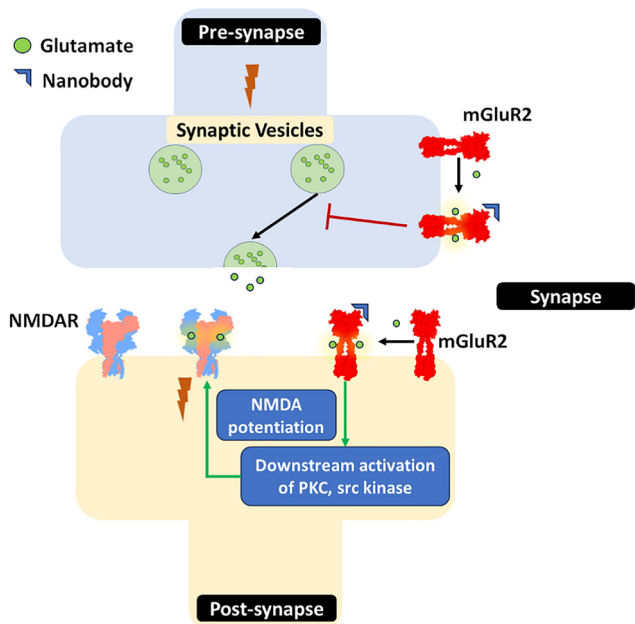


Fig. 10 Schematic diagram depicting mGluR2-mediated regulation of NMDA receptors.

to this challenge, as they can more easily cross the BBB compared to larger antibody constructs.⁴⁷

Delivery of therapeutic or diagnostic nanobodies can be achieved *via* several mechanisms (Fig. 11). BBB can be breached by several methods, including passive diffusion, Carrier-mediated Transport (CMT), Receptor-mediated transcytosis (RMT), and Adsorptive-mediated transcytosis (AMT).⁴⁸ It is important to measure how well BBB transport works in order to figure out how useful it might be for treatment. Although data is still limited, a few important studies offer useful benchmarks.

Passive diffusion of any material prerequisites a small size (<400 Da), fat solubility, a less polar surface, and fewer hydrogen bonds (<6) forming residues. 89Zr-nanobody shows a very low level of non-specific, passive diffusion into the brain in rats, approximately ~0.02% injected dose per gram (% ID per g) after 1 hour. PET imaging studies confirm that without BBB disruption, brain uptake remains minimal, supporting the use of this baseline for assessing targeted delivery strategies in brain imaging and therapy.⁴⁹

Nbs can traverse the BBB through RMT, a process in which molecules bind to specific receptors on the endothelial cells of

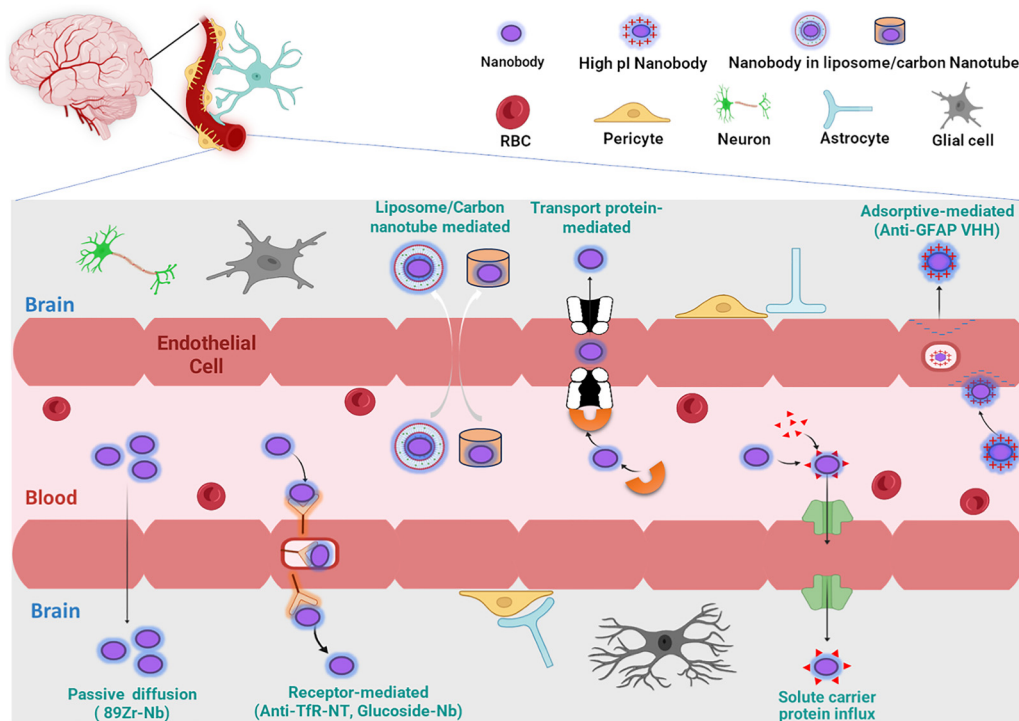


Fig. 11 Schematic of strategies for nanobody delivery across the blood–brain barrier (BBB). This schematic illustrates the cellular architecture of the BBB comprising brain endothelial cells, pericytes, and astrocytes and summarizes current strategies being explored to facilitate nanobody transcytosis from the blood into the brain parenchyma. Several distinct mechanisms are depicted: (1) adsorptive-mediated transcytosis, which relies on electrostatic interactions between a cationic nanobody (e.g., one with a high isoelectric point, pI) and the negatively charged endothelial cell surface; the example of an anti-GFAP VHH suggests targeting of astrocytes after crossing. (2) Receptor-mediated transcytosis (RMT), a “Trojan horse” approach where the nanobody is fused to a ligand (e.g., another nanobody) that binds an endogenous transporter, such as the transferrin receptor (TfR), exemplified by “Anti-TfR-NT”. (3) Carrier-mediated transport, involving the encapsulation of nanobodies within delivery vehicles like liposomes or carbon nanotubes. (4) Passive diffusion, which is generally inefficient for biologics but may be feasible for small, modified nanobodies, such as the radiolabeled “89Zr-Nb” used for PET imaging. Other potential routes include influx *via* endogenous transport proteins or solute carrier proteins. Overcoming the “delivery problem” is the final frontier for neuro-biologics, and the most promising future therapeutics will likely be multi-functional molecules that combine a high-potency channel-modulating domain with a dedicated BBB-shuttling domain. The image was created using Biorender.

Highlight

the BBB, such as the transferrin receptor or insulin-like growth factor receptors. These receptors facilitate the transport of nanobodies across the BBB, allowing them to reach their target in the CNS. This ability to target the brain with high specificity opens new avenues for the treatment of neurological diseases, including Alzheimer's disease, Parkinson's disease, and glioblastoma. RMT is currently the most widely used method for the delivery of nanobodies through the BBB. FC5 and FC44 are two sdAbs that enter the BBB through RMT.^{50,51} FC5 specifically binds to the luminal $\alpha(2,3)$ -sialoglycoprotein receptor TMEM30A on brain endothelial cells, an interaction that initiates clathrin-mediated endocytosis of FC5 and its subsequent RMT across the BBB. *In vitro* studies using Brain Microvascular Endothelial Cells (BMEC) monolayers show that FC5 achieves approximately $4.0 \pm 0.56\%$ translocation at 6 hours and $42.0 \pm 3.35\%$ at 24 hours, significantly outperforming unrelated single-domain or control antibodies in both specificity and translocation rate. *In vivo*, FC5 brain uptake ranges from 0.1% to 1% of the injected dose per gram of tissue (% ID per g), with enhanced versions—such as dimerized or Fc-fused constructs—achieving up to $\sim 0.8\%$ ID per g to 2% ID per g, depending on the experimental model and configuration, reflecting up to a 20-fold increase in delivery efficiency.⁵² Nbs developed against the extracellular domain of the human insulin-like growth factor 1 receptor (IGF1R), when fused to either mouse or human Fc regions, are capable of crossing the BBB *via* receptor-mediated transcytosis. These constructs not only achieve brain uptake levels ranging from 5 to 11% ID per g in rats, but have also been shown to deliver non-BBB-penetrant therapeutic small molecules into the CNS.^{53,54}

The transferrin receptor is also a target for RMT.⁵⁵ Nanobodies targeting the transferrin receptor (TfR) have been employed to deliver neurotensin (NT) into the CNS. One notable construct is the engineered M1 nanobody, particularly its triple histidine mutant M1(His). When combined with other nanobody domains—such as 13A7–13A7 (targeting P2X7 receptor) and Nb80 (binding to albumin)—this multi-domain fusion efficiently crosses the BBB after intravenous administration. Quantitatively, brain uptake reached 13.4% ID per g at 1 nmol kg^{-1} and 8.8% at 3 nmol kg^{-1} , while a higher dose of 30 nmol kg^{-1} resulted in 3.5% ID per g, indicating a dose-dependent saturation effect. Incorporating an albumin-binding nanobody extended systemic half-life from 21 minutes to 2.6 hours, significantly enhancing delivery.^{56–58} Nb targeting a cytosolic prion protein PrPc was capable of crossing the BBB *in vitro* and *in vivo*, and it was hypothesized to transmigrate *via* RMT.⁵⁹ Bi-specific Nanobodies conjugated with nanobodies targeting RMT fused with human FC region could provide a multipronged approach to overcome the limitations in pharmacokinetics (faster renal clearance of sdAbs) and crossing the BBB. VHH-E9-SCFv8D3 is a bispecific nanobody that uses RMT (scFv8D3 targets transferrin) to deliver a nanobody (VHH-E9) against glial fibrillary acidic protein (GFAP) overexpressed by astroglial cells in regions affected by Alzheimer's disease. VHH-E9 nanobody reached brain concentrations of 0.15% ID per g, while VHH-E9-SCFv8D3 attained 0.44% ID per g 2 hours

post-injection.⁶⁰ Glycosylated nanobodies (Glucoside-Nb) have shown much better ability to cross the BBB and accumulate in glioblastoma tumors in mice. Using RMT, they delivered about 2.9 times more to the brain compared to unmodified nanobodies. In a mouse model of glioma, brain delivery increased by 5.7 times, as confirmed by fluorescence imaging 24 hours after injection. This enhancement is attributed to glycosylation-mediated engagement of the GLUT1 transporter, which is highly expressed on the BBB and glioblastoma cells and is crucial for glucose uptake and tumor metabolism. Quantitatively, glycosylated nanobodies achieve up to about 6% ID per g of brain tissue (ID per g-brain), outperforming unmodified analogues, which typically show less than 2% ID per g-brain.⁶¹

The transmigration of Nb's through the BBB by AMT has been demonstrated in a few cases where the pI of the Nb's is high. For instance, Nb R3QV (pI > 8.3) targets A β 42, Nb A2 (pI > 9.5) targets phosphorylated Tau protein,⁶² and an Nb that targets GFAP (pI = 9.4).^{63–65} Alternatively, Nbs have been delivered into the CNS using agents that can transmigrate through the BBB, such as glutathione-targeted PEGylated liposomes, multi-walled carbon nanotubes (MWCNTs), or Fe₃O₄ nanoparticles.^{66–69}

The study of the bivalent mGlu2-targeting nanobody, DN13-DN1, provides the most complete data. After a single intraperitoneal injection in mice, radiolabeling studies showed that brain uptake peaked at 4 hours, with 0.08% of the injected dose (%ID) was found in total brain extracts. Although this level of penetration appears low, it was sufficient to achieve a therapeutically relevant brain concentration of approximately 9.2 nM, which is significantly higher than the nanobody's binding affinity for its target. Importantly, the nanobody was detectable in the brain for a minimum of 7 days (at approximately 1.5 nM), a duration that directly corresponded with enduring behavioral enhancements in mouse models of schizophrenia. The brain uptake of 0.08% ID is similar in quantity to the 0.01–0.4% reported for the passive diffusion of conventional IgG antibodies.⁴⁶ However, the pharmacological implications are very different. IgGs have a long serum half-life (days to weeks), while unmodified nanobodies are cleared from circulation within 1 hour. The fact that DN13-DN1 can get IgG-like brain exposure even though it has a short peripheral half-life means that a much more efficient transport mechanism is at work. For context, in the field of PET imaging, a brain uptake of more than 0.1% of the injected dose per cubic centimeter (% ID per cc) is often seen as a benchmark for a successful CNS tracer, which means that the levels achieved by DN13-DN1 are within a functionally significant range.⁶⁰

The development of these innovative strategies for crossing the BBB holds great promise for advancing nanobody-based treatments for a wide range of CNS disorders.

From bench to bedside: the clinical progression of ion channel-targeting nanobodies

Preclinical studies have shown that nanobodies have a lot of potential, but a close look at their clinical development shows that there is a big gap between proving the technology platform and using it on a specific type of ion channel.

The nanobody platform has been very successful in both clinical and business settings. So far, four nanobody-based drugs have been approved by major agencies like the FDA and EMA. These include Caplacizumab (Cabliivi[®]), a bivalent nanobody targeting von Willebrand factor for acquired thrombotic thrombocytopenic purpura;⁷⁰ Ozoralizumab (Nanozora[®]), a trivalent, bispecific nanobody targeting TNF α for rheumatoid arthritis (approved in Japan);^{71–73} Envafolimab, a PD-L1-targeting nanobody fused to an Fc domain for solid tumors (approved in China);^{74,75} and Ciltacabtagene autoleucel (Carvykti[®]), a CAR-T cell therapy utilizing two B-cell maturation antigen-targeting nanobodies for multiple myeloma.⁷⁶ A thorough examination of clinical trial databases uncovers a substantial array of nanobody candidates, featuring numerous active trials, predominantly in oncology and inflammatory diseases.⁷⁷ Nonetheless, a notable finding arises from this analysis: None of the approved nanobody drugs or candidates in late-stage clinical development targets an ion channel. The antigens that have been successfully targeted are primarily soluble proteins (vWF, TNF α) or highly expressed cell surface markers on immune or cancer cells (PD-L1, BCMA). This disparity highlights the unique difficulties associated with ion channel targets. Monoclonal antibodies targeting ion channels such as P2X7 and Orai-1 have commenced clinical trials; however, this advancement is yet to be mirrored in the nanobody domain.

Nanobodies are versatile, small and modular for targeting proteins nevertheless, there are a few limitations to the use of nanobodies to study ion channels. Nanobodies are generated using proteins expressed in a heterologous system. The lack of pivotal regulatory and interacting partners of the receptor in the heterologous system may hinder the efficiency of the nanobody in the native or physiological conditions of the ion channel, since the receptors are known to exist in different conformational states in the presence of auxiliary proteins and other interacting proteins. The ability of a nanobody to trap receptors in specific conformational states might be useful in certain aspects, while it may not be useful to study aspects pertaining to receptor modulation.

Problems that make ion channel targets hard to translate to clinical use

The notable lack of ion channel-targeting nanobodies in the clinical pipeline indicates a substantial translational gap, stemming from the intrinsic biochemical difficulties associated with this category of membrane proteins.

First and foremost is the “antigen challenge”. The generation of high-affinity nanobodies typically begins with the immunization of a camelid, which requires substantial quantities of pure, stable, and conformationally correct antigen. Ion channels are notoriously difficult to produce in this manner. They are frequently expressed at low levels in native tissues, and recombinant overexpression may result in misfolding and aggregation.⁷⁸ Various detergents have been used traditionally to purify membrane proteins. The choice of detergents depends on the membrane protein and might have effect the stability and functionality of membrane proteins. In order to provide a more

conducive environment, detergent-purified membrane proteins can be further stabilized by incorporating amphipols, nanodiscs or reconstituting the receptors in liposomes. A recent report comparing nanodiscs and liposome-based purification of ELIC receptor identified that liposomes provided a more native environment to the protein, thereby reducing artefactual conformations as observed in nanodiscs. Such strategies may be adopted for the purification and/or stabilization of challenging membrane protein targets.⁷⁹

Second, the process of screening is much more complicated. High-throughput ELISA-based tests can help find binders for soluble targets like TNF α . To find functional modulators of an ion channel, on the other hand, you need specialized, low-throughput, and technically challenging tests, like patch-clamp electrophysiology, to see how the channel current changes. This makes the process much more complicated, meaning fewer candidates can be effectively screened, making discovery campaigns take longer and cost more. Finally, the high structural similarity among ion channel subtypes means that very specific nanobodies need to be made to avoid possibly harmful off-target effects. This is a high standard for safety and regulatory approval. The main challenge that must be overcome to move from preclinical promise to clinical reality for ion channel-targeting nanobodies is solving these fundamental problems in antigen production and functional screening. The development of computational tools to identify specific nanobodies against proteins is gaining traction in the field, and the following are some of the AI and ML methods used for this purpose (Table 3).

The digital Frontier: using AI to design and improve ion channel nanobodies

Integrating artificial intelligence (AI) and machine learning (ML) is transforming the traditional, hands-on, and time-consuming process of discovering nanobodies. These computational methods allow for fast and accurate identification, design, and optimization of nanobodies by utilizing advanced deep learning architectures, structural modeling, and large-scale data analysis. This is especially promising for addressing the challenges associated with hard targets, such as ion channels, because of the structural complexity, low expression yields, and the subtle differences among channel subtypes.

The emergence of highly precise protein structure prediction tools, particularly AlphaFold, has revolutionized structural biology.⁸⁰ Advanced structure prediction models like AlphaFold3 have significantly improved nanobody-antigen complex modelling, achieving high-accuracy docking success rates of 8.9% for antibodies and 13.4% for nanobodies.⁸¹ While exact binding epitope prediction remains challenging with accuracy below 50%, confidence scores such as ipTM (interface predicted TM-score) reliably distinguish near-native from incorrect models. The prediction quality heavily depends on the nanobody CDR3 loop characteristics, with simple, stretched conformations and shorter loops being modeled more accurately than kinked and longer loops due to their inherent flexibility. Despite these limits, such tools provide a valuable starting point for structure-guided design and candidate selection.⁸²

Table 3 List of computational tools for the development of nanobodies

Contribution area	Exemplary tools/models	Model type/ approach	Key applications in nanobody development
Structure prediction	AlphaFold2, AlphaFold3, IgFold, NanoNet, ImmuneBuilder, RoseTTAFold, NanoBodyBuilder2	Transformer, ResNet, GNN, AntiBERTy	Accurate modeling of nanobody (VHH) 3D structures, with focus on variable CDR loops (esp. CDR3/H3)
Sequence & epitope design	ProteinMPNN, RFDiffusion, JAM, ParaAntiProt, AlphaProteo, BindCraft, Evolvex	Generative AI, transformer, CNN	De novo design of nanobody sequences for specific antigens, identification of strong binding sites.
Affinity & developability	DeepAb, ML classifiers, NanoBERTa-ASP & NbX	RNN, ResNet, decision Tree	Predict binding affinity and filter high-affinity candidates; assess developability, solubility, and stability
Humanization & immunogenicity	AbNatiV (deep learning) + ML pipelines	Deep learning, ML classifiers	Predict and minimize immunogenicity, improve resemblance to human antibodies
High-throughput screening	ML-based interaction models	ML classifiers, CNN	Screening vast protein-antibody interaction datasets, sifting for leads rapidly
Generative design	Generative AI platforms, RFDiffusion	Generative AI, transformer	Create diverse <i>in silico</i> nanobody variants targeting multiple or “undruggable” sites
Paratope/epitope prediction	Parapred, ParaAntiProt	RNN (LSTM), CNN, transformer	Paratope and epitope prediction to identify binding interfaces

Complementary deep learning models like IgFold and NanoNet enable precise 3D structure prediction of nanobodies directly from sequences, with IgFold achieving a median CDR3 RMSD accuracy of 2.2 Å for nanobodies and operating at remarkable speed (under 25 seconds). These tools have made large-scale structural analysis feasible, with researchers successfully predicting structures for over 1.4 million paired antibody sequences.^{83,84}

Affinity maturation of nanobodies is an important aspect after discovery implies improving their binding strength to specific target antigens through repeated cycles of design and refinement of their sequences or structures. While this was traditionally done using random mutagenesis followed by experimental screening, recent advances in computational approaches have streamlined and expedited the affinity maturation process.⁸⁵ Computational affinity maturation platforms like ADAPT and EvolveX combine physics-based models with machine learning to screen millions of virtual mutants, achieving dramatic improvements and selecting top candidates. These approaches have achieved dramatic changes—for example, an anti-CD47 nanobody was computationally optimized using homology modeling combined with ADAPT, resulting in mutants with up to an 87-fold increase in binding affinity and improved thermostability.⁸⁶ Even more dramatically, another pipeline improved the affinity of a VHH against the immune checkpoint protein Vsig4 by over 1000-fold, transforming a weak binder into a potent nanomolar-affinity molecule.⁸⁷

Machine learning models for binding prediction have achieved remarkable performance in nanobody-antigen interaction forecasting, with advanced algorithms reaching prediction accuracies exceeding 80%.⁸⁸ NABP-BERT, a specialized language model developed by Google, represents a breakthrough in sequence-based binding prediction, achieving very high scores in the benchmarks while focusing on surrounding amino acid contexts.^{89,90} These models leverage extensive datasets of nanobody-protein binding interactions and utilize sophisticated architectures to predict binding purely from sequence data.^{91,92} Machine learning analyzes large datasets

of nanobody-antigen interactions and identifies patterns in sequence, structure, and noncovalent interactions (*e.g.*, hydrogen bonds, aromatic stacking) that govern binding affinity. Feature analysis reveals that hydrogen bonding and aromatic-associated interactions are key mechanistic determinants of binding affinity, with hydrogen bond descriptors accounting for 51.9% of important predictive features and aromatic interactions contributing 29.6%. This enables prediction of new epitopes and the nanobody features critical for strong, specific binding.⁸⁸

Generative models, including AlphaProteo, BindCraft, and RFDiffusion, further expand capabilities by designing novel sequences targeting challenging epitopes, with BindCraft leveraging AlphaFold2's trained weights to generate nanomolar binders without requiring high-throughput screening.^{16,93} These comprehensive AI-driven pipelines integrate reinforcement learning, ensemble meta-predictors, and *in silico* mutagenesis to refine nanobody candidates by predicting how sequence changes affect binding affinity, stability, and developability, thereby accelerating discovery cycles while enhancing success rates against previously difficult targets.⁹⁴

AI and machine learning continue to reshape the future of nanobody discovery for ion channels by providing powerful capabilities such as structure-guided virtual design, rapid and accurate epitope mapping, and data-driven mutational optimization, where the generation of large amounts of antigen is challenging. These technologies integrate seamlessly with experimental workflows to establish a robust, cutting-edge discovery pipeline tailored for the unique challenges posed by ion channel targets. By combining precise structural modeling with intelligent library selection and functional impact prediction, AI and ML streamline the identification and optimization of high-affinity, specific nanobodies.^{95–97} This convergence not only accelerates development timelines but also enhances the precision and efficacy of nanobody candidates, paving the way for innovative therapeutics and diagnostics targeting ion channels and other complex membrane proteins.

Future outlook

The field of ion channel-targeted nanobodies stands at a fascinating inflection point. The preclinical evidence is strong, showing that these biologics can change how channels work with unmatched precision and through new allosteric mechanisms. However, the way to use this in the clinic is still mostly unexplored. The future of this field will likely be defined by progress in three key areas: tackling new targets, innovating delivery strategies, and integrating intelligent design. In addition, the need for developing strategies for the administration of nanobodies, increasing the half-life of nanobodies, and generating a large repertoire of nanobodies against multiple ion channels to target very specific diseased states are probably the challenges that lie ahead in this field.

A significant gap in the current research landscape is the lack of nanobodies that target ionotropic glutamate receptors (iGluRs), including AMPA, Kainate, NMDA, and Delta receptors.⁹⁸ This deficiency is particularly notable given their critical role in central nervous system (CNS) physiology and pathology, alongside the recent achievement in creating a brain-penetrating nanobody for their G protein-coupled counterparts, the metabotropic glutamate receptors (mGluRs). The difficulties in targeting iGluRs stem from their considerable structural complexity. Unlike the dimeric mGluRs, iGluRs are large, heavily glycosylated heterotetramers with a complex “dimer-of-dimers” architecture in their extracellular domains.⁹⁸ This complexity makes them exceptionally difficult to produce as stable antigens for immunization and complicates the identification of functional epitopes. Interestingly, the lack of nanobodies against the structurally simpler Glycine receptor has been attributed to the fact that its structure could be readily solved by other means, suggesting the field has prioritized targets where nanobodies provide a unique enabling advantage. As cryo-EM continues to unravel iGluR structures, the next frontier will be to move beyond structural chaperones and develop functional nanobody modulators, which remain a major untapped therapeutic opportunity.

Author contributions

The manuscript was conceptualized, designed, and written by MS, SB, SAM, IM and supervised by JK.

Conflicts of interest

No conflict of interest

Data availability

No primary research results, software or code have been included and no new data were generated or analysed as part of this review.

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References

- M. J. Ackerman and D. E. Clapham, *N. Engl. J. Med.*, 1997, **336**, 1575–1586.
- F. Bezanilla, *Neuron*, 2008, **60**, 456–468.
- C. A. Hübner and T. J. Jentsch, *Hum. Mol. Genet.*, 2002, **11**, 2435–2445.
- K. Bohmwald, N. M. S. Gálvez, C. A. Andrade, V. P. Mora, J. T. Muñoz, P. A. González, C. A. Riedel and A. M. Kalergis, *Front. Physiol.*, 2021, **12**, 736681.
- W. Wu, J. Zheng, R. Wang and Y. Wang, *Biochem. Pharmacol.*, 2023, **218**, 115863.
- L. He, M. Ahmad and N. Perrimon, *Exp. Cell Res.*, 2019, **374**, 259–265.
- T. Kamei, T. Kudo, H. Yamane, F. Ishibashi, Y. Takada, S. Honda, Y. Maezawa, K. Ikeda and Y. Oyamada, *Biochem. Biophys. Res. Commun.*, 2024, **721**, 150126.
- E. Y. Yang and K. Shah, *Front. Oncol.*, 2020, **10**, 1182.
- C. Hamers-Casterman, T. Atarhouch, S. Muyldermans, G. Robinson, C. Hamers, E. B. Songa, N. Bendahman and R. Hamers, *Nature*, 1993, **363**, 446–448.
- S. S. Rizk, D. M. Moustafa, S. A. ElBanna, H. T. Nour El-Din and A. S. Attia, *World J. Microbiol. Biotechnol.*, 2024, **40**, 209.
- S. Muyldermans, *Annu. Rev. Biochem.*, 2013, **82**, 775–797.
- J. Yong Joon Kim, Z. Sang, Y. Xiang, Z. Shen and Y. Shi, *Adv. Drug Delivery Rev.*, 2023, **195**, 114726.
- S. Muyldermans, *FEBS J.*, 2021, **288**, 2084–2102.
- C. McMahon, A. S. Baier, R. Pascolutti, M. Wegrecki, S. Zheng, J. X. Ong, S. C. Erlandson, D. Hilger, S. G. F. Rasmussen, A. M. Ring, A. Manglik and A. C. Kruse, *Nat. Struct. Mol. Biol.*, 2018, **25**, 289–296.
- Q. Su, W. Shi, X. Huang, S. Yin, X. Yang and X. Lu, *MedComm: Biomater. Appl.*, 2023, **2**, e54.
- J. L. Watson, D. Juergens, N. R. Bennett, B. L. Trippe, J. Yim, H. E. Eisenach, W. Ahern, A. J. Borst, R. J. Ragotte, L. F. Milles, B. I. M. Wicky, N. Hanikel, S. J. Pellock, A. Courbet, W. Sheffler, J. Wang, P. Venkatesh, I. Sappington, S. V. Torres, A. Lauko, V. De Bortoli, E. Mathieu, S. Ovchinnikov, R. Barzilay, T. S. Jaakkola, F. DiMaio, M. Baek and D. Baker, *Nature*, 2023, **620**, 1089–1100.
- K. E. J. Rödröm, A. Cloake, J. Sörmann, A. Baronina, K. H. M. Smith, A. C. W. Pike, J. Ang, P. Proks, M. Schewe, I. Holland-Kaye, S. R. Bushell, J. Elliott, E. Pardon, T. Baukowitz, R. J. Owens, S. Newstead, J. Steyaert, E. P. Carpenter and S. J. Tucker, *Nat. Commun.*, 2024, **15**, 4173.
- S. Gründer and X. Chen, *Int. J. Physiol., Pathophysiol. Pharmacol.*, 2010, **2**, 73–94.
- Y. Wu, Z. Chen, F. J. Sigworth and C. M. Canessa, *eLife*, 2021, **10**, e67115.
- T. J. Morgenstern, J. Park, Q. R. Fan and H. M. Colecraft, *eLife*, 2019, **8**, e49253.

- 21 T. J. Morgenstern, N. Nirwan, E. O. Hernández-Ochoa, H. Bibollet, P. Choudhury, Y. D. Laloudakis, M. Ben Johny, R. A. Bannister, M. F. Schneider, D. L. Minor and H. M. Colecraft, *Nat. Commun.*, 2022, **13**, 7556.
- 22 S. Cheng, D. Jiang, X. Lan, K. Liu and C. Fan, *Biomed. Pharmacother.*, 2024, **175**, 116651.
- 23 US1149086B2 - KV1.3 binding immunoglobulins - Google Patents, [https://patents.google.com/patent/US1149086B2/en?q=\(ion+channels+AND+nanobodies+AND+current\)&dq=+ion+channels+AND+nanobodies+AND+current](https://patents.google.com/patent/US1149086B2/en?q=(ion+channels+AND+nanobodies+AND+current)&dq=+ion+channels+AND+nanobodies+AND+current), (accessed December 9, 2024).
- 24 P. Selvakumar, A. I. Fernández-Mariño, N. Khanra, C. He, A. J. Paquette, B. Wang, R. Huang, V. V. Smider, W. J. Rice, K. J. Swartz and J. R. Meyerson, *Nat. Commun.*, 2022, **13**, 3854.
- 25 M. L. Cotrina and M. Nedergaard, *Purinergic Signalling*, 2009, **5**, 223–232.
- 26 W. Danquah, C. Meyer-Schwesinger, B. Rissiek, C. Pinto, A. Serracant-Prat, M. Amadi, D. Iacenda, J.-H. Knop, A. Hammel, P. Bergmann, N. Schwarz, J. Assunção, W. Rotthier, F. Haag, E. Tolosa, P. Bannas, E. Boué-Grabot, T. Magnus, T. Laeremans, C. Stortelers and F. Koch-Nolte, *Sci. Transl. Med.*, 2016, **8**, 366ra162.
- 27 H. K. Ganguly, M. B. Elbaum and N. J. Zondlo, *Biochemistry*, 2025, **64**, 2848–2866.
- 28 K. Drodźdyk, M. Peter and R. Dutzler, *eLife*, 2024, **13**, RP96138.
- 29 T.-H. Chou, H. Kang, N. Simorowski, S. F. Traynelis and H. Furukawa, *Mol. Cell*, 2022, **82**, 4548–4563.e4.
- 30 G. Loussouarn, D. Sternberg, S. Nicole, C. Marionneau, F. Le Bouffant, G. Toumaniantz, J. Barc, O. A. Malak, V. Fressart, Y. Péréon, I. Baró and F. Charpentier, *Front. Pharmacol.*, 2016, **6**, 314.
- 31 L. Srinivasan, V. Alzogaray, D. Selvakumar, S. Nathan, J. B. Yoder, K. M. Wright, S. Klinke, J. N. Nwafor, M. S. Labanda, F. A. Goldbaum, A. Schön, E. Freire, G. F. Tomaselli, L. M. Amzel, M. Ben-Johny and S. B. Gabelli, *J. Biol. Chem.*, 2022, **298**, 101763.
- 32 World Intellectual Property Organization, WO2015189162A1, 2015.
- 33 M. Brams, C. Govaerts, K. Kambara, K. L. Price, R. Spurny, A. Gharpure, E. Pardon, G. L. Evans, D. Bertrand, S. C. Lummis, R. E. Hibbs, J. Steyaert and C. Ulens, *eLife*, 2020, **9**, e51511.
- 34 C. M. Hénault, C. Govaerts, R. Spurny, M. Brams, A. Estrada-Mondragon, J. Lynch, D. Bertrand, E. Pardon, G. L. Evans, K. Woods, B. W. Elbersson, L. G. Cuello, G. Brannigan, H. Nury, J. Steyaert, J. E. Baenziger and C. Ulens, *Nat. Chem. Biol.*, 2019, **15**, 1156–1164.
- 35 N. M. Barnes, T. G. Hales, S. C. R. Lummis and J. A. Peters, *Neuropharmacology*, 2009, **56**, 273–284.
- 36 G. Hassaine, C. Deluz, L. Grasso, R. Wyss, M. B. Tol, R. Hovius, A. Graff, H. Stahlberg, T. Tomizaki, A. Desmyter, C. Moreau, X.-D. Li, F. Poitevin, H. Vogel and H. Nury, *Nature*, 2014, **512**, 276–281.
- 37 M. S. Prevost, N. Barilone, G. Dejean de la Bâtie, S. Pons, G. Ayme, P. England, M. Gielen, F. Bontems, G. Pehau-Arnaudet, U. Maskos, P. Lafaye and P.-J. Corringer, *Nat. Commun.*, 2023, **14**, 5964.
- 38 Q. Li, A. Nemezc, G. Aymé, G. D. de la Bâtie, M. S. Prevost, S. Pons, N. Barilone, R. Baachaoui, U. Maskos, P. Lafaye and P.-J. Corringer, *Cell. Mol. Life Sci.*, 2023, **80**, 164.
- 39 A. Ghit, D. Assal, A. S. Al-Shami and D. E. E. Hussein, *J. Genet. Eng. Biotechnol.*, 2021, **19**, 123.
- 40 S. Masiulis, R. Desai, T. Uchański, I. Serna Martin, D. Laverty, D. Karia, T. Malinauskas, J. Zivanov, E. Pardon, A. Kotecha, J. Steyaert, K. W. Miller and A. R. Aricescu, *Nature*, 2019, **565**, 454–459.
- 41 P. S. Miller, S. Masiulis, T. Malinauskas, A. Kotecha, S. Rao, S. Chavali, L. D. Colibus, E. Pardon, S. Hannan, S. Scott, Z. Sun, B. Frenz, G. Klesse, S. Li, J. M. Diprose, C. A. Siebert, R. M. Esnouf, F. DiMaio, S. J. Tucker, T. G. Smart, J. Steyaert, M. M. Babu, M. S. P. Sansom, J. T. Huisken and A. R. Aricescu, *bioRxiv*, 2018, preprint, DOI: [10.1101/338343](https://doi.org/10.1101/338343).
- 42 P. S. Miller, S. Scott, S. Masiulis, L. D. Colibus, E. Pardon, J. Steyaert and A. R. Aricescu, *Nat. Struct. Mol. Biol.*, 2017, **24**, 986.
- 43 S. Rutz, D. Deneka, A. Dittmann, M. Sawicka and R. Dutzler, *Nat. Struct. Mol. Biol.*, 2023, **30**, 52–61.
- 44 D. Deneka, S. Rutz, C. A. J. Hutter, M. A. Seeger, M. Sawicka and R. Dutzler, *Nat. Commun.*, 2021, **12**, 5435.
- 45 P. Scholler, D. Nevoltris, D. De Bundel, S. Bossi, D. Moreno-Delgado, X. Rovira, T. C. Møller, D. El Moustaine, M. Mathieu, E. Blanc, H. McLean, E. Dupuis, G. Mathis, E. Trinquet, H. Daniel, E. Valjent, D. Baty, P. Chames, P. Rondard and J.-P. Pin, *Nat. Commun.*, 2017, **8**, 1967.
- 46 M. Oosterlaken, A. Rogliardo, T. Lipina, P.-A. Lafon, M. E. Tsitokana, M. Keck, H. Cahuzac, P. Prieu-Sérandon, S. Diem, C. Derieux, C. Camberlin, C. Lafont, D. Meyer, P. Chames, F. Vandermoere, P. Marin, L. Prêzeau, D. Servent, A. Salahpour, A. J. Ramsey, C. Bécamel, J.-P. Pin, J. Kniazeff and P. Rondard, *Nature*, 2025, 1–9.
- 47 E. Ruiz-López and A. J. Schuhmacher, *Biomolecules*, 2021, **11**, 1131.
- 48 F. Zheng, Y. Pang, L. Li, Y. Pang, J. Zhang, X. Wang and G. Raes, *Front. Immunol.*, 2022, **13**, 978513.
- 49 W. G. Lesniak, C. Chu, A. Jablonska, B. Behnam Azad, O. Zwaenepoel, M. Zawadzki, A. Lisok, M. G. Pomper, P. Walczak, J. Gettemans and M. Janowski, *Eur. J. Nucl. Med. Mol. Imaging*, 2019, **46**, 1940–1951.
- 50 A. Muruganandam, J. Tanha, S. Narang and D. Stanimirovic, *FASEB J.*, 2002, **16**, 240–242.
- 51 G. K. Farrington, N. Caram-Salas, A. S. Haqqani, E. Brunette, J. Eldredge, B. Pepinsky, G. Antognetti, E. Baumann, W. Ding, E. Garber, S. Jiang, C. Delaney, E. Boileau, W. P. Sisk and D. B. Stanimirovic, *FASEB J.*, 2014, **28**, 4764–4778.
- 52 A. Abulrob, H. Sprong, P. V. B. En Henegouwen and D. Stanimirovic, *J. Neurochem.*, 2005, **95**, 1201–1214.
- 53 W. Alata, A. Yogi, E. Brunette, C. E. Delaney, H. van Faassen, G. Hussack, U. Iqbal, K. Kemmerich, A. S. Haqqani, M. J. Moreno and D. B. Stanimirovic, *FASEB J.*, 2022, **36**, e22208.
- 54 A. Yogi, G. Hussack, H. Van Faassen, A. S. Haqqani, C. E. Delaney, E. Brunette, J. K. Sandhu, M. Hewitt, T. Sulea, K. Kemmerich and D. B. Stanimirovic, *Pharmaceutics*, 2022, **14**, 1452.
- 55 Y. Wouters, T. Jaspers, B. De Strooper and M. Dewilde, *Fluids Barriers CNS*, 2020, **17**, 62.
- 56 T. J. Esparza, S. Su, C. M. Francescutti, E. Rodionova, J. H. Kim and D. L. Brody, *Fluids Barriers CNS*, 2023, **20**(1), 64.
- 57 S. Su, T. J. Esparza and D. L. Brody, *PLoS One*, 2022, **17**, e0276107.
- 58 Y. Wouters, T. Jaspers, L. Rué, L. Serneels, B. De Strooper and M. Dewilde, *Fluids Barriers CNS*, 2022, **19**, 79.
- 59 D. R. Jones, W. A. Taylor, C. Bate, M. David and M. Tayebi, *PLoS One*, 2010, **5**, e9804.
- 60 Y. Li and J. Wang, *J. Labelled Compd. Radiopharm.*, 2023, **66**, 444–451.
- 61 S. Zhou, X. Fang, Y. Luo, Y. Yang, W. Wei, G. Huang, X. Zhang and C. Wu, *Bioconjugate Chem.*, 2025, **36**, 291–301.
- 62 R. Abskharon, H. Pan, M. R. Sawaya, P. M. Seidler, E. J. Olivares, Y. Chen, K. A. Murray, J. Zhang, C. Lantz, M. Bentzel, D. R. Boyer, D. Cascio, B. A. Nguyen, K. Hou, X. Cheng, E. Pardon, C. K. Williams, A. L. Nana, H. V. Vinters, S. Spina, L. T. Grinberg, W. W. Seeley, J. Steyaert, C. G. Glabe, R. R. Ogorzalek Loo, J. A. Loo and D. S. Eisenberg, *Proc. Natl. Acad. Sci. U. S. A.*, 2023, **120**, e2300258120.
- 63 T. Li, J.-P. Bourgeois, S. Celli, F. Glacial, A.-M. Le Sourd, S. Mecheri, B. Weksler, I. Romero, P.-O. Couraud, F. Rougeon and P. Lafaye, *FASEB J.*, 2012, **26**, 3969–3979.
- 64 S. R. Meier, D. Sehlin and S. Syvänen, *Nucl. Med. Biol.*, 2022, **114–115**, 128–134.
- 65 Canada, CA2962275C, 2019.
- 66 M. Rotman, M. M. Welling, A. Bunschoten, M. E. Backer, J. Rip, R. J. A. Nabuurs, P. J. Gaillard, M. A. van Buchem, S. M. van der Maarel and L. van der Weerd, *J. Controlled Release*, 2015, **203**, 40–50.
- 67 U. Iqbal, H. Albaghdadi, M.-P. Nieh, U. I. Tuor, Z. Mester, D. Stanimirovic, J. Katsaras and A. Abulrob, *Nanotechnology*, 2011, **22**, 195102.
- 68 U. Iqbal, H. Albaghdadi, Y. Luo, M. Arbabi, C. Desvaux, T. Veres, D. Stanimirovic and A. Abulrob, *Br. J. Cancer*, 2010, **103**, 1606–1616.
- 69 S. Zhu, A.-G. Huang, F. Luo, J. Li, J. Li, L. Zhu, L. Zhao, B. Zhu, F. Ling and G.-X. Wang, *ACS Appl. Mater. Interfaces*, 2019, **11**, 19006–19016.
- 70 M. Scully, S. R. Cataland, F. Peyvandi, P. Coppo, P. Knöbl, J. A. K. Hovinga, A. Metjian, J. de la Rubia, K. Pavenski, F. Callewaert, D. Biswas, H. D. Winter and R. K. Zeldin, *N. Engl. J. Med.*, 2019, **380**, 335–346.
- 71 S. Oyama, K. Ebina, Y. Etani, M. Hirao, M. Kyuuma, Y. Fujii, K. Iwata, B. Ogawa, T. Hasegawa, S. Kawano, Y. Nakanishi, S. Okada and K. Nakata, *Sci. Rep.*, 2022, **12**, 18102.

- 72 Y. Tanaka, *Expert Opin. Biol. Ther.*, 2023, **23**, 579–587.
- 73 S. J. Keam, *Drugs*, 2023, **83**, 87–92.
- 74 M. Chen, M. Jiang, X. Wang, L. Shen and J. Li, *Expert Opin. Biol. Ther.*, 2022, **22**, 1227–1232.
- 75 A. Markham, *Drugs*, 2022, **82**, 235–240.
- 76 T. Martin, S. Z. Usmani, J. G. Berdeja, M. Agha, A. D. Cohen, P. Hari, D. Avigan, A. Deol, M. Htut, A. Lesokhin, N. C. Munshi, E. O'Donnell, A. K. Stewart, J. M. Schecter, J. D. Goldberg, C. C. Jackson, T.-M. Yeh, A. Banerjee, A. Allred, E. Zudaire, W. Deraedt, Y. Olyslager, C. Zhou, L. Pacaud, D. Madduri, A. Jakubowiak, Y. Lin and S. Jagannath, *J. Clin. Oncol.*, 2023, **41**, 1265–1274.
- 77 I. Jovčevska and S. Muyldermans, *BioDrugs*, 2020, **34**, 11–26.
- 78 C. J. Hutchings, P. Colussi and T. G. Clark, *mAbs*, 2018, **11**, 265.
- 79 V. Dalal, B. K. Tan, H. Xu and W. W. Cheng, *eLife*, 2025, **14**, RP106728.
- 80 M. Sánchez-Marin, M. Giulini and A. M. J. J. Bonvin, Combining AI structure prediction and integrative modelling for nanobody-antigen complexes, *bioRxiv*, 2025, preprint, DOI: [10.1101/2025.07.01.662355](https://doi.org/10.1101/2025.07.01.662355).
- 81 F. N. Hitawala and J. J. Gray, What does AlphaFold3 learn about antigen and nanobody docking, and what remains unsolved?, *bioRxiv*, 2025, preprint, DOI: [10.1101/2024.09.21.614257](https://doi.org/10.1101/2024.09.21.614257).
- 82 F. Eshak and A. Goupil-Lamy, 2024.
- 83 T. Cohen, M. Halfon and D. Schneidman-Duhovny, *Front. Immunol.*, 2022, **13**, 958584.
- 84 J. A. Ruffolo, L. S. Chu, S. P. Mahajan and J. J. Gray, *Nat. Commun.*, 2023, **14**(1), 2389.
- 85 L. Wang, X. He, G. Guo, X. Qian and Q. Huang, Computational nanobody design using graph neural networks and Metropolis Monte Carlo sampling, *bioRxiv*, 2025, preprint, DOI: [10.1101/2025.06.08.658414](https://doi.org/10.1101/2025.06.08.658414).
- 86 X. Cheng, J. Wang, G. Kang, M. Hu, B. Yuan, Y. Zhang and H. Huang, *Int. J. Mol. Sci.*, 2019, **20**, 4187.
- 87 Z. Zhang, R. Van Der Kant, I. Marković, D. Vizarraga, T. Garcia, K. Maragkou, J. Delgado Blanco, D. Cianferoni, G. Orlando, G. Cia, N. Geukens, C. Carolis, A. N. Volkov, S. N. Sawides, M. Dewilde, J. Schymkowitz, L. Serrano Pubul and F. Rousseau, In silico design of stable single-domain antibodies with high affinity, *bioRxiv*, 2024, preprint, DOI: [10.1101/2024.04.22.589762](https://doi.org/10.1101/2024.04.22.589762).
- 88 H. Feng, X. Sun, N. Li, Q. Xu, Q. Li, S. Zhang, G. Xing, G. Zhang and F. Wang, *ACS Omega*, 2024, **9**, 47893–47902.
- 89 F. S. Ahmed, S. Aly and X. Liu, *Briefings Bioinf.*, 2024, **26**(1), bbae518.
- 90 J. T. Hadsund, T. Saława, B. Janusz, L. Shan, L. Zhou, R. Röttger and K. Krawczyk, *Bioinf. Adv.*, 2024, **4**(1), vbae033.
- 91 S. Dandibhotla, M. Samudrala, A. Kaneriyana and S. Dakshanamurthy, *Pharmaceuticals*, 2025, **18**(3), 329.
- 92 Y. Zhang, Z. Wang, F. Ge, X. Wang, Y. Zhang, S. Li, Y. Guo, J. Song and D. J. Yu, *Briefings Bioinf.*, 2024, **25**(6), bbae489.
- 93 M. Pacesa, L. Nickel, C. Schellhaas, J. Schmidt, E. Pyatova, L. Kissling, P. Barendse, J. Choudhury, S. Kapoor, A. Alcaraz-Serna, Y. Cho, K. H. Ghamary, L. Vinué, B. J. Yachnin, A. M. Wollacott, S. Buckley, A. H. Westphal, S. Lindhoud, S. Georgeon and B. E. Correia, *Nature*, 2025, **646**(8084), 483–492.
- 94 V. Dewaker, V. K. Morya, Y. H. Kim, S. T. Park, H. S. Kim and Y. H. Koh, *Biomark. Res.*, 2025, **13**(1), 52.
- 95 N. S. El Salamouni, J. H. Cater, L. M. Spenkelink and H. Yu, *FEBS Open Bio*, 2025, **15**, 236–253.
- 96 J. Liu, L. Wu, A. Xie, W. Liu, Z. He, Y. Wan and W. Mao, *J. Nanobiotechnol.*, 2025, **23**(1), 87.
- 97 H. Zhu and Y. Ding, *Biology*, 2025, **14**(5), 547.
- 98 E. Karakas, M. C. Regan and H. Furukawa, *Trends Biochem. Sci.*, 2015, **40**, 328–337.
- 99 E. F. Pettersen, T. D. Goddard, C. C. Huang, E. C. Meng, G. S. Couch, T. I. Croll, J. H. Morris and T. E. Ferrin, *Protein Sci.*, 2021, **30**, 70–82.
- 100 E. Pardon, T. Laeremans, S. Triest, S. G. F. Rasmussen, A. Wohlkönig, A. Ruf, S. Muyldermans, W. G. J. Hol, B. K. Kobilka and J. Steyaert, *Nat. Protoc.*, 2014, **9**, 674–693.
- 101 M. Arbabi-Ghahroudi, *Front Immunol.*, 2017, **8**, 1589.
- 102 K. A. Henry and C. R. MacKenzie, *Front. Immunol.*, 2018, **9**, 41.