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Biomedical Frontiers with PVA–chitosan/lignin@CdZnO multifunctional hydrogel

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A nanoparticle-based hydrogel was synthesized and evaluated for advanced biomedical applications including antibacterial, anticancer and wound healing functionalities. The hydrogel was fabricated using polyvinyl alcohol (PVA), chitosan and lignin-mediated nanocomposites as the primary components. The resultant nanocomposites and hydrogel were examined using UV-visible spectroscopy, thermal gravimetric analysis, Fourier transform infrared spectroscopy and XRD techniques to confirm their composition and structural integrity. In the context of antibacterial studies, the PVA–chitosan/lignin@CdZnO (PVA-CS/L@CdZnO) hydrogel exhibited superior bactericidal activity compared with CdZnO and L@CdZnO nanocomposites, effectively inhibiting *Staphylococcus aureus* (*S. aureus*), *Bacillus subtilis* (*B. subtilis*), and *Escherichia coli* (*E. coli*). Antioxidant assays showed remarkable efficacy, with 89% of DPPH (2,2-diphenyl-1-picrylhydrazyl) activity and a reducing power absorbance of 0.68. Furthermore, in wound healing studies conducted on a rat model, the hydrogel achieved 91% wound closure within 10 days, significantly surpassing the 61% closure observed in the control group. Furthermore, against MCF-7 breast cancer cell lines, the hydrogel demonstrated 50% anticancer efficacy, showcasing its potential in oncological applications. These results underscore the multifunctional potential of the PVA–CS/L@CdZnO hydrogel, establishing it as an attractive choice for a wide range of biological applications, including antibacterial, antioxidant, anticancer, and wound healing therapies.

1 Introduction

A wound is a disturbance of the anatomical structure and functional continuity of the surrounding tissues. Wound healing is a complicated biological procedure that involves the restoration of tissue integrity. Physiologically, it may be divided into four separate phases: hemostasis, inflammation, proliferation, and tissue remodeling. It is influenced by a variety of elements, including interactions between the extracellular matrix, different kinds of cells, and growth hormones.[1] The human skin has an intrinsic capacity to encourage self-regeneration after injury; however, this capability can be hampered in certain circumstances, like substantial skin loss, severe burns, chronic wounds, non-healing ulcers, and diabetes. Traditional medicines are becoming more prevalent in a variety of locations, including Africa, Asia, and Latin America, which help to improve healthcare accessibility. Traditional medicines provide primary care for around 80% of the population in Asia and Africa, while they account for 40% of the total healthcare practices in China.[2] Conventional methods such as maggot debridement therapy, larval wound therapy, and herbal-derived substances have been widely employed for wound healing. Aside from their varied applications, all of these traditional treatments have limitations such as the onset of allergic responses, an unclear mechanism of action, the danger of infection, the rapid drying of the wound area, and batch-to-batch fluctuation, among others.[3] Aside from that, many medications have been examined for wound healing, such as glucocorticoids,[4] nonsteroidal anti-inflammatory drugs,[5] and chemotherapeutic drugs,[6] but due to the reduced oxygen flow at the wound when using these drugs, a slow healing process has been recorded. This leads to the exploration of cost-effective and more efficient strategies to heal wounds, especially in the case of diabetic foot wounds.

Nanotechnology has enabled the development of innovative wound-healing strategies, which have been proven to be cost-effective and efficient.[7] In this regard, due to their biodegradability, biocompatibility, and tissue regeneration, more attention

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has been focused on hydrogels in the last few years.[8] In recent research studies, a variety of hydrogels for different kinds of applications have been prepared.[9–12] Hydrogels have been prepared using nanoparticles and macromolecules (hybrid hydrogels) according to the environmental conditions. The structure of hybrid hydrogels is temperature sensitive. Moreover, because of the presence of cations and anions in the hydrogel, environmental pH also influences the hydrogel structure of hybrid hydrogels. The term hybrid hydrogel refers to a structurally integrated network formed by combining three distinct biopolymeric components: cationic starch, carrageenan, and sodium alginate. Unlike conventional hydrogels composed of single or binary polysaccharide systems, the hybrid hydrogel described herein utilizes the complementary charge characteristics of its constituents to achieve enhanced physicochemical performance.[13] Hydrogels are three-dimensional polymeric networks that have been effectively employed in a variety of biological applications. They function as a replacement extracellular matrix, creating a wet environment that promotes wound healing.[14] Hydrogels are widely used in wound healing applications because they are similar to the original extracellular matrix (ECM) and may provide a moist environment. PVA is one of the most common and oldest synthetic polymers used for wound dressings, wound care, and drug delivery systems.[15] The hydrogel's strength can be enhanced by the water-soluble, biocompatible, and biodegradable polymer PVA.[16] The only downside of hydrogels is their weak mechanical stability when swollen. This disadvantage has been overcome by including a composite or hybrid hydrogel system containing more than one polymer in the dressing composition.[17] Synthetic polymers may have limited strength and hydrophobic properties, which limit their applicability. Thus, natural polymers such as chitosan, which is formed by the hydrolysis of chitin's aminoacyl groups,[18] have been utilized to repair wounds. Chitosan is a natural polysaccharide derived from chitin, a biopolymer found in the exoskeleton of crustaceans. This compound not only facilitates the formation of hydrogen bonds with PVA but also enhances the mechanical properties of the hydrogel through electrostatic interactions resulting from dynamic covalent bonds between the amino and carboxyl groups in chitosan.[19] Despite having strong antibacterial and biocompatible qualities, the PVA–chitosan composite hydrogel's limited mechanical strength makes it unsuitable for use as a wound dressing. Moreover, the PVA–chitosan composite hydrogel does not meet the criteria necessary to function as an environmental conditioner that accelerates the wound healing process.[20] The introduction of lignin in the PVA–chitosan hydrogel increases the mechanical strength, and because of its antioxidant and free radical scavenging qualities, the lignin–chitosan–PVA composite hydrogel speeds up healing in mouse skin wound therapy.[21] Lignin, a polyphenolic polymer abundant in nature, contains numerous functional groups that enable hydrogen bonding and electrostatic interactions, thus enhancing the mechanical properties of composite films and hydrogels. Additionally, lignin is effective for modifying inorganic nanomaterials.[22]

Nano-reinforced multifunctional hydrogels represent a possible paradigm change in the area of wound healing.

Biologically active nanoparticles, especially antibacterial and anti-inflammatory nanoparticles (NPs), in combination with biopolymers used in wound dressings, can promote the faster healing of both acute and chronic wounds.[23,24] Metal oxide nanoparticles like CuO, ZnO, MgO, FeO, and CaO are considered to have potential antibacterial activity. It has also been reported that the formation of ZnO NPs and minocycline hydrogel composites significantly enhances the therapeutic and repairing abilities for gingival tissues.[25] Similarly, cadmium oxide (CdO) nanoparticles, because of their antimicrobial qualities, can also be used to develop more valuable composite materials for better biological applications.[26] Another report describes that cadmium (Cd) has the potential to kill cancer cells.[27] Typical reported data reveal that each of PVA, chitosan, lignin, and CdZnO nanomaterials offer valuable biomedical potential. However, alongside their advantageous applications, it is revealed in literature that when these materials are used individually or in binary-combination fashions, they show poor mechanical strength, limited bioactivity, hydrophobicity, agglomeration and cytotoxicity risks.[28] To overcome these challenges, in this research work, we developed a multifunctional hydrogel by integrating all four components, leveraging their complementary properties: PVA provides flexibility, chitosan adds antibacterial activity, lignin enhances the antioxidant capacity and mechanical strength, and CdZnO nanoparticles contribute antimicrobial and anticancer effects. This hybrid matrix, it is hypothesized, will ensure the improvement in biocompatibility and biomedical activities. The fabricated materials were characterized by using UV-vis, FT-IR, TGA, DSC, and XRD techniques. Furthermore, the DPPH free radical scavenging assay and reducing power assay were used to measure the hydrogel's antioxidant activity, while the well diffusion method was used for evaluating its antibacterial activity.

2 Materials and methods

2.1 Chemicals

Zinc chloride ($ZnCl_2$), cadmium chloride ($CdCl_2$), and sodium hydroxide (NaOH) were obtained from Sigma-Aldrich and used without further purification. PVA (M_w = 124–146 kg mol^{-1}, 95% degree of hydrolysis) and 2,2-diphenyl-1-picrylhydrazyl (DPPH) free radical (M_w = 394.32 g mol^{-1}) were also supplied by Sigma-Aldrich and used as received. Chitosan, a low molecular weight product, was purchased from Aldrich. Kraft lignin, a purified commercial polymer, was obtained from Aldrich. Throughout the experiment, ultra-filtered deionized (DI) water was used.

2.2 Preparation of CdZnO NPs

A 1% PVP solution was prepared by dissolving 1 g of PVP in 99 mL of distilled water. Then, 10 mL of this solution was mixed with 2.87 g of $ZnCl_2$ in 100 mL of distilled water and stirred for 30 minutes. Subsequently, 0.056 g of $CdCl_2$ was added to the mixture, and stirring was continued for 1 hour. A NaOH solution was then added dropwise, leading to the formation of white precipitates. The resulting precipitates were washed thoroughly

with methanol and filtered. To eliminate any residual impurities, the filtrate was dried in an oven at 80 °C for 12 hours. After drying, the precipitates were ground into a uniform powder and heated for 4 hours at 550 °C in a muffle furnace.[29]

2.3 Synthesis of L@CdZnO

The L@CdZnO nanocomposite was synthesized using the probe sonication method. In the formulation of solution A, 0.0025 M (0.458 g) $CdCl_2$ and 0.0025 M (0.340 g) $ZnCl_2$ were dissolved in

70 mL of deionized water and stirred until homogeneity was achieved. Solution B was prepared by dissolving 0.013 M (0.6 g) lignin and 0.25 M (0.3 g) NaOH in 30 mL of DI water and stirring constantly until lignin was completely dissolved. Solution B was then gradually introduced into solution A, followed by stirring for an additional 15 minutes. The resultant solution underwent probe sonication for 20 minutes at 60% amplitudes with a 5-second pulse interval. Centrifugation at 8000 rpm for 10 minutes was used to separate the final product, which was then dried in an
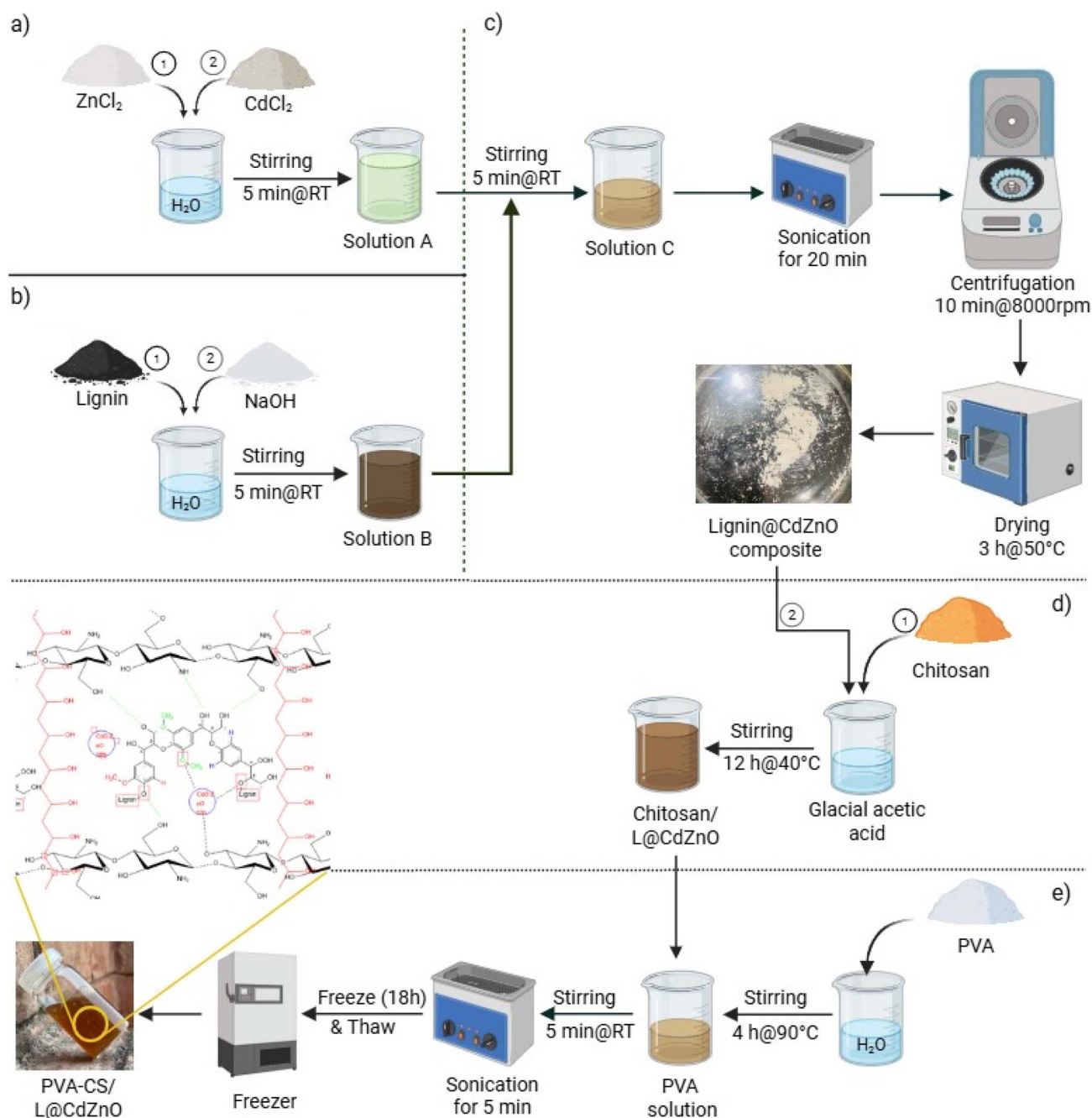
Scheme 1 Fabrication of the PVA–CS/L@CdZnO hydrogel: (a) synthesis of solution A by mixing $CdCl_2$ and $ZnCl_2$; (b) synthesis of solution B by mixing lignin and NaOH; (c) formation of the L@CdZnO composite by mixing solutions A and B; (d) synthesis of CS/L@CdZnO by mixing chitosan in acetic acid and L@CdZnO and (e) finally, the fabrication of the hydrogel by mixing the PVA solution with CS/L@CdZnO to form PVA–CS/L@CdZnO.

oven set at 100 °C for 3 hours.[29] The scheme for the fabrication of L@CdZnO is shown in Scheme 1(c).

2.4 Fabrication of the PVA–CS/L@CdZnO hydrogel

To prepare the PVA–CS/L@CdZnO nanocomposite-based hydrogel, PVA (5 g) was dissolved in 20 mL of DI water under continuous magnetic stirring at 90 °C for 4 hours. Separately, 0.5 g of chitosan was dissolved in 10 mL of glacial acetic acid with magnetic stirring at 40 °C for 12 hours until a homogeneous solution formed. Afterward, 0.05 g of the L@CdZnO nanocomposite was added to the chitosan solution and thoroughly mixed. Both solutions were combined and subjected to sonication for 5 minutes to ensure uniform dispersion. The final mixture was poured into a Petri dish, covered with a Teflon lid, and left to solidify under controlled conditions.[30] The detailed scheme for the fabrication of the PVA–CS/L@CdZnO hydrogel is shown in Scheme 1(a–e).

2.5 Characterizations

The synthesized materials were thoroughly characterized using Fourier transform infrared (FT-IR) spectroscopy, UV-visible spectroscopy, X-ray diffraction (XRD), and thermogravimetric analysis (TGA) following the reported protocols.[31] FT-IR analysis was performed using a Thermo-Nicolet 6700 spectrometer (USA) to identify the functional groups present in the CdZnO nanoparticles (NPs), L@CdZnO NPs, and PVA–CS/L@CdZnO hydrogel, covering a spectral range from 400 to 4000 cm^{-1}. The optical properties of the CdZnO NPs, L@CdZnO, and PVA–CS/L@CdZnO hydrogel were investigated using UV-visible spectroscopy with a LAMBDA 25 spectrophotometer, scanning in the wavelength range of 200–800 nm. The phase composition and crystalline structure were determined via XRD utilizing CuKα radiation in a 2θ range from 0° to 90°. To examine the thermal stability and decomposition behavior, TGA was conducted using an SDT Q600 instrument.

2.6 Antibacterial activity

The antibacterial activity of CdZnO, L@CdZnO, and PVA–CS/L@CdZnO hydrogel was assessed using a slightly modified version of the well diffusion method described previously.[32] The Department of Microbiology at the GCUF provided one Gram-negative strain, i.e., E. coli, and two Gram-positive strains, i.e., S. aureus and B. subtilis, for the antibacterial evaluation. For the test medium, 3.8 g of Mueller–Hinton agar was dissolved in 100 mL of distilled water and sterilized in an autoclave at 121.7 °C for 20 minutes. Bacterial cultures were equally distributed on the surface of Petri dishes after the sterilised media had been added and allowed to solidify. Stock solutions of the test samples were prepared in dilute acetic acid, followed by serial dilutions of 3 mg mL^{-1}, 1.5 mg mL^{-1}, 0.75 mg mL^{-1}, and 0.375 mg mL^{-1}. Acetic acid (30 μg mL^{-1}) was used as a negative control, while CFR 30 (30 μg mL^{-1}) served as a positive control. Five wells were made in each plate, and 40 ppm from each dilution was added to the corresponding wells, with CFR 30 positioned at the center. The plates were incubated at 37 °C for 24 hours, after which the bacterial growth was measured as zone of inhibition (ZOI) in mm. Triplicate measurements were performed for each sample to ensure the accuracy and precision of the results.

2.7 Antioxidant study

2.7.1 DPPH free radical scavenging activity.
DPPH is a stable free radical frequently used to evaluate the radical scavenging activity of the antioxidant components. The DPPH free radical scavenging activity of CdZnO, L@CdZnO, and the hydrogel was assessed by using a previously reported protocol with slight modifications.[33] Briefly, methanol solutions of CdZnO, L@CdZnO, and PVA–CS/L@CdZnO hydrogel samples at varying concentrations (1000 μg, 500 μg, 250 μg, and 125 μg) were individually mixed with 4 mL of a 0.2 mM methanol DPPH free radical solution. After keeping the mixture in the dark for 30 minutes at room temperature, the absorbance was measured at 517 nm using methanol as a blank. To ensure the accuracy, assay was carried out three times. The DPPH free radical scavenging potential was measured by the following eqn (1):

$$\% \text{ of inhibition} = \frac{\text{absorbance Dpph} - \text{absorbance sample}}{\text{absorbance Dpph}} \times 100 \quad (1)$$

The DPPH radical scavenging activity increases with decreasing absorbance.

2.7.2 Reducing power assay.
The antioxidant activity of CdZnO, L@CdZnO, and the hydrogel was determined according to the previously reported methods.[34] Specifically, 2.5 mL of the samples (CdZnO, L@CdZnO, and PVA–CS/L@CdZnO hydrogel) at varying concentrations (62.5 μg mL^{-1}, 125 μg mL^{-1}, 250 μg mL^{-1}, 500 μg mL^{-1}, and 1000 μg mL^{-1}) was mixed with 2.5 mL of 200 mmol L^{-1} sodium phosphate (pH 6.6) and 2.5 mL of a potassium ferricyanide solution. The mixture was incubated at 50 °C for 20 minutes in an incubator. Next, 2.5 mL of 10% w/v trichloroacetic acid was added after incubation, and centrifugation was performed for 10 minutes at 650 rpm. Five millilitres of the obtained supernatant were taken and combined with 1.0 mL of 0.1% ferric chloride and 5 mL of distilled water. Ascorbic acid was used as the reference standard for measuring the final solution's absorbance at 700 nm. Greater absorption resulted in an increased reducing power.

2.8 Wound healing potential

The wound healing potential of the prepared hydrogels was evaluated in white Albino rats weighing 250–300 g. A total of four rats were used in the study, and they were divided into two groups: Group 1 served as the control group, while Group 2 received the treatment. The animal study for wound healing was approved by the Department of Pharmaceutics, Government College University, Faisalabad, Pakistan. Briefly, to induce wounds, the rats were anesthetized with chloroform, and their backs were shaved using a hair trimmer. Using sterile surgical tools, a full-thickness excisional incision with a 5-mm diameter was created on the dorsal surface. The treatment was then directly applied to the wounds. Images of

components. In the hydrogel spectrum, a new and distinct band appears at 1596 cm^{-1}, which is not present in the spectra of individual components. This band is attributed to the C=N stretching vibration, indicating the formation of imine (Schiff base) linkages. Imine bonds typically arise from a condensation reaction between a primary amine (–NH$_2$) and a carbonyl group (aldehyde or ketone, –C=O). In this system, the –NH$_2$ groups are contributed by chitosan, a biopolymer known for its primary amine functionality. The carbonyl groups are likely derived from oxidized lignin, which contains aldehyde and ketone moieties as a result of depolymerization or chemical modification. This type of crosslinking enhances the structural integrity and stability of the hydrogel network. The imine bond is formed by the condensation reaction between the amine group from chitosan and aldehyde or the ketone group from the oxidized or cross-linked lignin PVA.[39] In addition to the FT-IR peaks obtained in case of L@CdZnO IR spectra, the hydrogen bonding peak, likely between the hydroxyl and carbonyl groups in lignin and chitosan, confirms the formation of PVA-CS/L@CdZnO hydrogel. Additionally, the peak at 968 cm^{-1}, attributed to CdZnO NPs, further verifies the successful synthesis of the hydrogel.

3.3 TGA analysis

The thermal stability of lignin, CdZnO NPs, L@CdZnO, and PVA–CS/L@CdZnO hydrogel was assessed through TGA, as
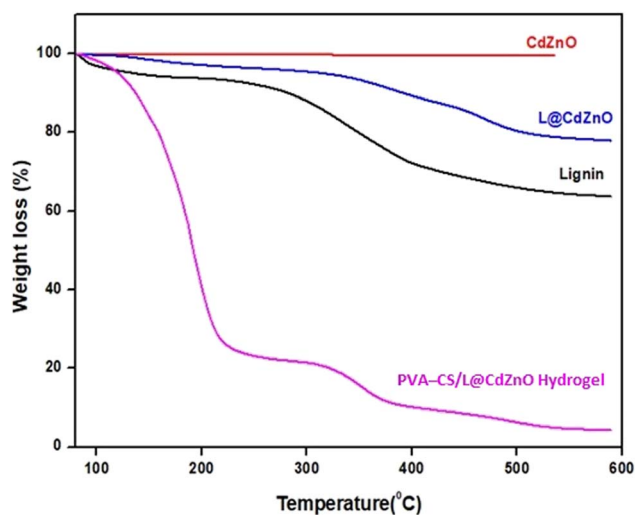

Fig. 3 TGA spectra of lignin, CdZnO NPs, L@CdZnO, and the PVA–CS/L@CdZnO hydrogel.

shown in Fig. 3. The TGA curve of CdZnO showed a minimal weight loss of 2%, indicating a negligible amount of bound water or impurities, confirming the high purity of the nanocomposite. The thermal degradation of lignin occurred in three stages. The evaporation of absorbed and bonded water was the cause of the initial 6.2% weight loss between 80 and 160 °C. The primary cause of the 26% weight loss between 160 and 470 °C was the breakdown of lignin into volatile chemicals, while the slower degradation in the third stage, from 470 to 600 °C, produced char, leaving approximately 63% of the sample remaining at 600 °C.

The TGA curve of L@CdZnO also comprised three stages. In the first stage, due to the elimination of moisture, there was a 3.81% weight loss between 80 and 130 °C. In the second stage, between 250 and 400 °C, lignin decomposed, with a reduced weight loss of 9.02%, attributed to the incorporation of nanoparticles, which enhanced thermal stability. The final stage showed continued slow degradation, leaving about 76% of the sample remaining at 600 °C. The hydrogel's TGA curve also showed degradation in three stages. In the first stage from 30 to 120 °C, the major weight loss (74%) was due to the evaporation of water and acetic acid in the hydrogel. In the second stage from 200 to 350 °C, the decomposition of polyvinyl alcohol and chitosan resulted in a 13% weight loss. In the third stage, degradation ranged from 350 to 550 °C, and weight loss (5.96%) occurred due to the degradation of the saccharide rings and the DE polymerization of the acylated and deacylated units, with approximately 4% of the sample remaining at 600 °C, as shown in Table 1. TGA was performed to assess the thermal stability of the PVA–CS/L@CdZnO hydrogel, a parameter of significance for biomedical applications. Thermal stability is a critical consideration in the context of sterilization procedures (such as autoclaving or dry heat treatment), storage conditions, and the material's *in vivo* performance, particularly where exposure to physiological or elevated temperatures may occur. These characteristics enhance the hydrogel's suitability for biomedical applications such as drug delivery systems, wound dressings, or implantable scaffolds, where predictable thermal behavior is essential.

3.4 XRD analysis

The XRD spectra of lignin, CdZnO, L@CdZnO, and PVA–CS/L@CdZnO hydrogel show crystallographic structures, showing atomic arrangement in the octahedral configuration in Fig. 4. Lignin shows diffraction peaks at 31.87°, 34.16°, 37.99°, 46.27°, and 52.51°, corresponding to the diffraction planes 100, 002,

Table 1 TGA results of lignin, CdZnO NPs, L@CdZnO, and the PVA–CS/L@CdZnO hydrogel

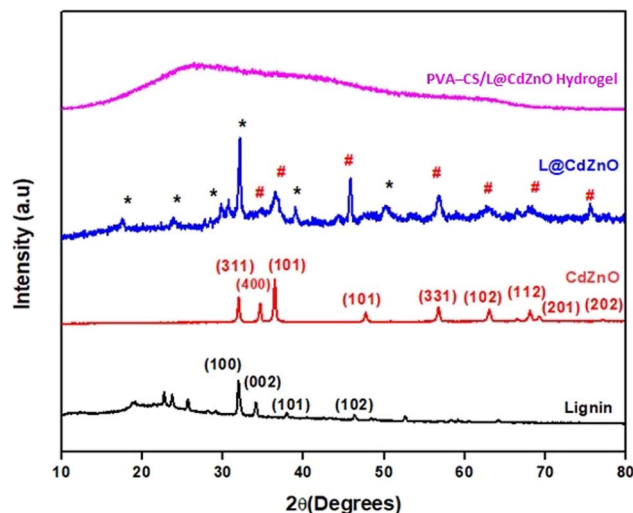| Material | T_{onset} (°C) | Peak 1 | | | Peak 2 | | Peak 3 | | Residues at 600 °C |
		T_{max} (°C)	Wt%		T_{max} (°C)	Wt%	T_{max} (°C)	Wt%	
Lignin	81	160	6.2		470	26	588	5	63
CdZnO	52	550	2		—	—	—	—	98
L@CdZnO	50	130	3.81		400	9.02	550	10	76
PVA–CS/L@CdZnO	29	120	74		350	13	550	5.96	4

Fig. 4 XRD spectra of lignin, CdZnO NPs, L@CdZnO, and the PVA–CS/L@CdZnO hydrogel.

101, 102, and 110, respectively.[29] Previous studies also confirm the diffraction peaks of lignin at these planes to confirm the purity of lignin 29. In the diffraction spectrum of the CdZnO, the sharp peaks at 2θ values of 32.16, 34.64, 47.65, and 56.72 correspond to (311), (400), (101), and (331), respectively, indicating the reflection planes of CdO NPs (JCPDS card no. 005-0628),[40] and other peaks values such as 2θ values of 36.44, 63.02, 68.06, 69.34, and 77.02 are associated with (101), (102), (112), (201), and (202), respectively, reflection planes of ZnO NPs (JCPDS no. 75-1526).[41] The average crystalline size of the CdZnO NPs was calculated by Debye–Scherer's formula, as shown in the following eqn (4):

$$D = \frac{K\lambda}{\beta \cos \theta} \quad (4)$$

where K denotes the form factor (0.94), λ is the X-ray wavelength of radiation for CuKα (1.54056 Å), β is the full width at the half-maximum intensity (FWHM), θ is the Bragg diffraction angle, and D is the crystallite size. Based on this equation, the estimated average size of the CdZnO is 19.05 nm. The XRD spectrum of L@CdZnO was confirmed against the standard of lignin and CdZnO NPs. The reflection planes at 2θ values of 31.87 (100), 34.16 (002), 37.99 (101), and 46.27 (102) confirm the presence of lignin in the L@CdZnO.[29]

The remaining peaks at 2θ values of 32.16 (311), 34.64 (400), 47.65 (101), and 56.72 (331) can be related to the crystal planes of CdZnO NCs (JCPDS card no. 005-0628).[40] The estimated mean particle size of the L@CdZnO nanocomposite is 24.61 nm. CdZnO and L@CdZnO particles exhibit hexagonal wurtzite shapes with the sizes of 19.05 nm and 24.61 nm, respectively, while the hydrogel displays an amorphous structure. Hydrogel formation was confirmed by the characteristic peaks of the PVA and chitosan when L@CdZnO was added to it. The two diffraction peaks at 20° and 22° are the characteristic peaks of PVA and chitosan, respectively.[42] The hydrogel exhibits a broad peak at a 2θ value of 27°, indicating the presence of a significant

amount of an amorphous material, likely lignin. The XRD pattern of the PVA–CS/L@CdZnO hydrogel confirms the absence of crystalline morphology of CdZnO NP, *i.e.*, a homogenous dispersion of CdZnO NP in PVA-CS/L hydrogel either through hydrogen bonding or electrostatic forces of attraction. This suggests that the presence of PVA and chitosan reduces the crystallinity of the L@CdZnO nanoparticles. This behavior is attributed to the significant hydrogen bonding among PVA, chitosan, and L@CdZnO, confirming the successful formulation of PVA–CS/L@CdZnO hydrogel.[43]

3.5 Antibacterial activity

The antibacterial activity of CdZnO, L@CdZnO and PVA–CS/L@CdZnO hydrogel was evaluated towards *S. aureus*, *B. subtilis*, and *E. coli* using the well diffusion method, as shown in Fig. 5. Results indicated that the nanocomposites at a concentration of 3 mg mL^{-1} expressed the largest zone of inhibition against all three kind of bacterium.

Specifically, CdZnO at 3 mg mL^{-1} achieved the highest ZOI against *S. aureus* (12 mm), *B. subtilis* (9.5 mm), and *E. coli* (9 mm), while the maximum ZOIs expressed by L@CdZnO were 11 mm, 9 mm, and 5 mm against *S. aureus*, *B. subtilis*, and *E. coli*, respectively. Promising antibacterial activity of PVA–CS hydrogel (without nanoparticles) has already been reported against *S. aureus* and *E. coli*.[30] In our study, the PVA–CS/L@CdZnO hydrogel demonstrated the most significant antibacterial effect, with the ZOIs of 18 mm, 13 mm, and 11 mm against *B. subtilis*, *S. aureus*, and *E. coli*, respectively. Current reported studies also reveal the effectiveness of different hydrogels against bacterial infections, but we found quite encouraging results.[44] The bactericidal effect of ZnO NPs is effective against Gram-positive as well as Gram-negative bacteria because of their increased surface area relative to microparticles, which enhances antibacterial efficacy.[45] The CdZnO exerts antibacterial effects primarily by the release of metal ions and reactive oxygen species (ROS), which disrupt bacterial cell membranes and high protein transport and ultimately cause cell death.[37,46] Furthermore, the antimicrobial potential of chitosan has also been reported in different formulations, particularly in acidic environments (pH < 6.5) where deacetylated C_2 amino groups in chitosan become protonated and positively charged. These positive charges interact with the negatively charged microbial cell walls and membranes, leading to increased cell permeability, osmotic damage, and the leakage of cytoplasmic contents, including essential proteins and ions.[47,48]

In summary, our fabricated PVA–CS/L@CdZnO hydrogel demonstrated enhanced antibacterial efficacy due to the multiple antibacterial hydrogel components, which trigger the generation of ROS, and the release of metallic ions, dominantly Zn^{2+} and Cd^{2+} in biological system.[37] Further, deacetylated C_2 amino groups of chitosan molecules,[48] and the presence of phenolic hydroxyl and methoxy groups on the surface of lignin also play effective role in antibacterial activities.[49] These factors collectively contributed to the PVA–CS/L@CdZnO hydrogel's strong antibacterial potential. Hence, PVA–CS/L@CdZnO hydrogels are proposed to be used for the treatment of
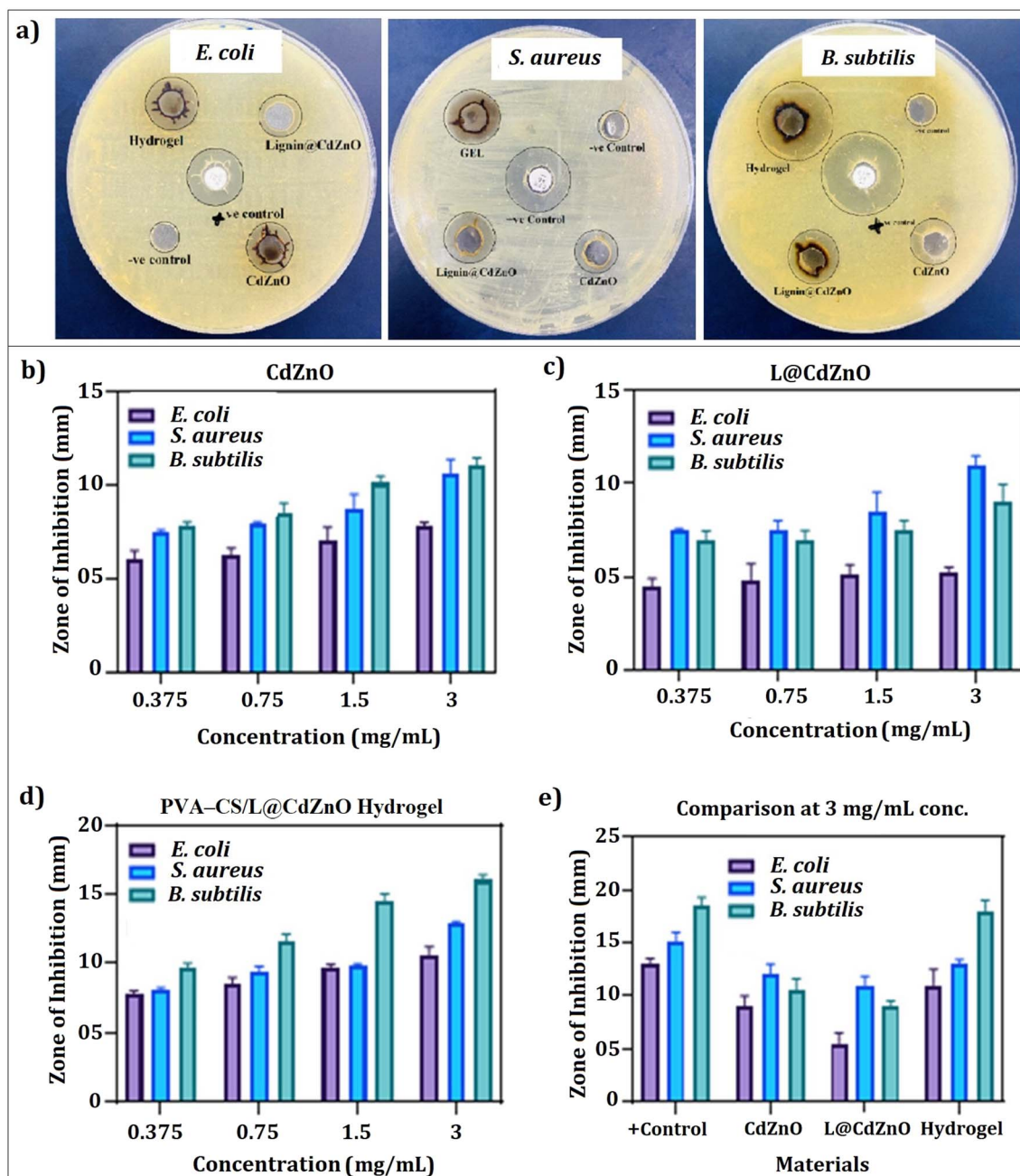
Fig. 5 Antibacterial activity observed using the disc diffusion process (a), results of the antibacterial effect of CdZnO NPs (b), L@CdZnO (c), and the PVA–CS/L@CdZnO hydrogel composite (d) at different concentrations, and a comparative evaluation among all the materials of 3 mg mL^{-1} concentration using *E. coli*, *S. aureus* and *B. subtilis* bacterial strains (e).

periodontal disease due to their inhibitory effects. The mechanistic interaction of the hydrogel composite with the bacterial cell wall and the resulting fate of the bacterial cell are shown in Fig. 6.

3.6 Antioxidant activities

3.6.1 DPPH scavenging activity. The antioxidant activity of CdZnO, L@CdZnO, and PVA–CS/L@CdZnO hydrogel composite was assessed using the DPPH free radical scavenging activity, as shown in Fig. 7(a). This activity relies on the capacity of

antioxidants to neutralize the stable free radical, DPPH, leading to a decrease in absorbance detectable by the UV spectrophotometer. Antioxidants change the purple color of DPPH into a yellow color. At a concentration of 1000 μg mL^{-1}, the synthesized L@CdZnO had a better antioxidant activity of 81%, whereas CdZnO showed a higher reducing scavenging activity of 70% at 1000 μg mL^{-1}. The PVA–CS/L@CdZnO hydrogel expressed the highest DPPH activity of 89% at 1000 μg mL^{-1}. After modifying CdZnO with lignin, the DPPH scavenging activity increased from 70% to 80% at a 1000 μg mL^{-1}
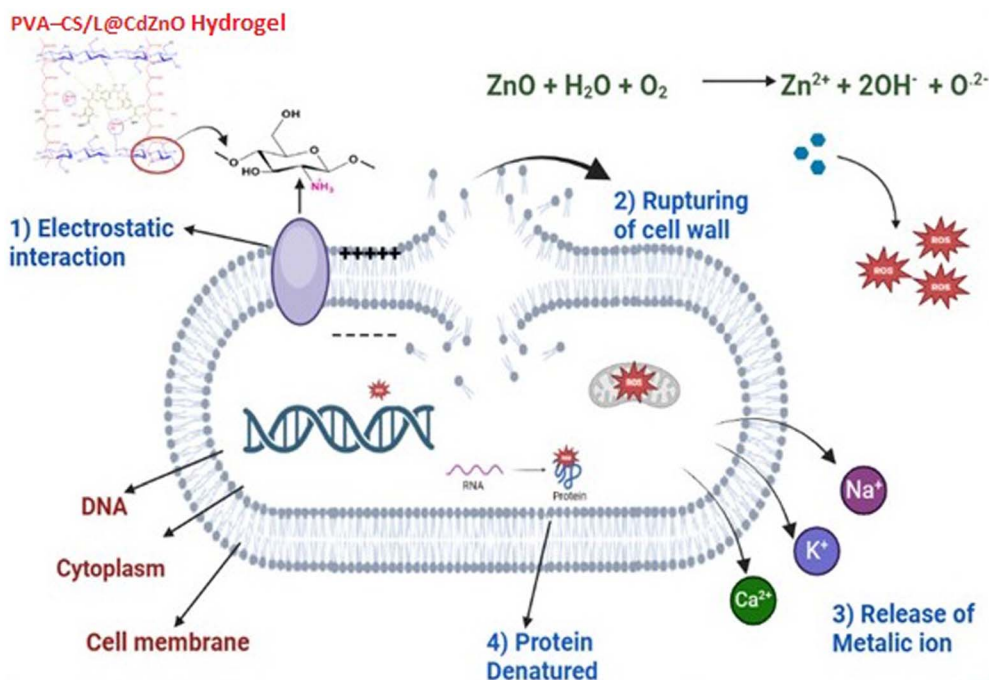
Fig. 6 Antibacterial mechanistic action of the PVA–CS/L@CdZnO hydrogel.

concentration. The highest DPPH scavenging activity was expressed by the hydrogel, which was formed *via* the fabrication of L@CdZnO onto PVA/CS. According to the formulation of the hydrogel, the increasing scavenging potential of PVA–CS/L@CdZnO hydrogel was likely due to the addition of chitosan with the antioxidant potential. The scavenging effect of chitosan is based on the free amino (NH_2) groups' ability to bind with free radicals and form stable macromolecule radicals. After that, NH_2 groups take up hydrogen ions from the mixture, producing ammonium (NH^{3+}) groups.

3.6.2 Reducing power assay. The reducing power assay, used to investigate the antioxidant activity, measures the reduction of ferric ions into ferrous ions in the presence of an antioxidant, resulting in a color shift from yellow to green or blue. This change is detected as an intense blue Prussian

complex at 700 nm, with ascorbic acid serving as the standard. The CdZnO showed absorbance values of 0.053, 0.089, 0.097, 0.147, and 0.258, whereas L@CdZnO showed absorbance values of 0.141, 0.254, 0.317, 0.451 and 0.591. The hydrogel showed absorbance values of 0.201, 0.298, 0.419, 0.598, and 0.685, and ascorbic acid, which was used as the standard, had absorbance values of 0.195, 0.300, 0.460, 0.683, and 0.851, as shown in Fig. 7(b). The CdZnO showed slight antioxidant activity due to metal oxide nanoparticles. A study revealed that with increasing nanoparticle concentration, the reducing power also increases.[50] However, when lignin was attached to the nanoparticles, the reducing power increased from 0.258 to 0.591 with increasing absorbance. Interestingly, the reducing potential of L@CdZnO was significantly higher than that of native lignin by several orders of magnitude.[51] As was stated earlier, the
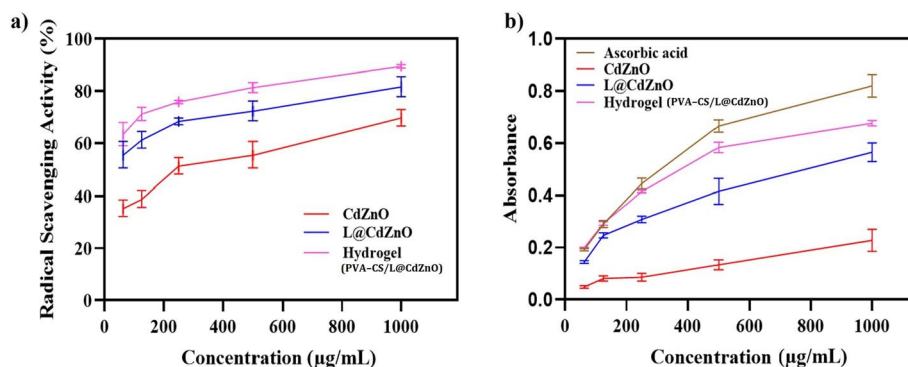

Fig. 7 Antioxidant activity study: (a) DPPH scavenging activity of CdZnO NPs, L@CdZnO, and the PVA–CS/L@CdZnO hydrogel and (b) reducing power of ascorbic acid, CdZnO NPs, L@CdZnO, and the PVA–CS/L@CdZnO hydrogel composite.

phenolic hydroxyl groups are the primary component that governs the redox activity of lignin.[52] The PVA–CS/L@CdZnO hydrogel showed a strong reducing power because it contains lignin and chitosan as additional factors. A prior investigation demonstrated the antioxidant effects of chitosan.[53] Because chitosan chains may chelate ferrous ions and are therefore a source of antioxidants, they also contain active hydroxyl and amino groups, which give chitosan its antioxidant potential. Therefore, the PVA–CS/L@CdZnO hydrogel could be a novel candidate for antioxidant activities.

3.7 Wound healing potential

In vivo wound healing studies were conducted to assess the effectiveness of the PVA–CS/L@CdZnO hydrogel in accelerating wound closure. Fig. 8 shows the control group and the treatment group using the hydrogel, which adhered directly to the wounds without additional preparation. The gel-like consistency of the hydrogel created a protective layer over the wound, supporting antimicrobial defense. Results indicated that wounds treated with the hydrogel healed significantly faster than those in the control group. Observations noted early re-epithelialization and the formation of new blood vessels under the hydrogel, with complete wound closure by day 10. The statistical analysis highlighted a notable reduction in the healing time for hydrogel-treated wounds, with marked improvements observed on days 6, 8, and 10. Initially, both groups showed similar wound statuses up to day 3, but by day 6, the hydrogel-treated wounds demonstrated considerably faster healing, with complete closure by day 10. Wound healing typically progresses through the phases of hemostasis, PVA–CS/L@CdZnO inflammation, proliferation, and maturation. The enhanced healing observed in the hydrogel group was attributed to the active antioxidant components from the lignin and chitosan within the hydrogel matrix. Previous research supports the use of lignin-based hydrogels as effective antioxidant wound dressings, underscoring the hydrogel's potential as an advanced wound treatment option.

3.8 Anticancer activities

The anticancer activity of the PVA–CS/L@CdZnO hydrogel was assessed against MCF7 cell lines. Results revealed that the PVA–CS/L@CdZnO hydrogel, L@CdZnO, and CdZnO exhibited anticancer activity against the MCF7 cancerous cell line, where the IC50 values were 100.01, 100.34, and 99.78, respectively. Moreover, the anticancer activity of the PVA–CS/L@CdZnO hydrogel, L@CdZnO, and CdZnO towards MCF7 at a concentration of 100 μg mL^{-1} was 50.3%, 41.93%, and 25%, respectively, as shown in Fig. 9. CdZnO-, L@CdZnO-, and hydrogel-based systems generate free radicals that cause the formation of reactive oxygen species (ROS). By disrupting cellular
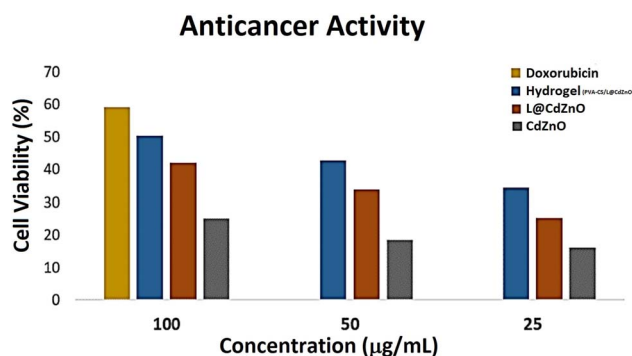

Fig. 9 Anticancer activity of CdZnO NPs, L@CdZnO, and the PVA–CS/L@CdZnO hydrogel composite.
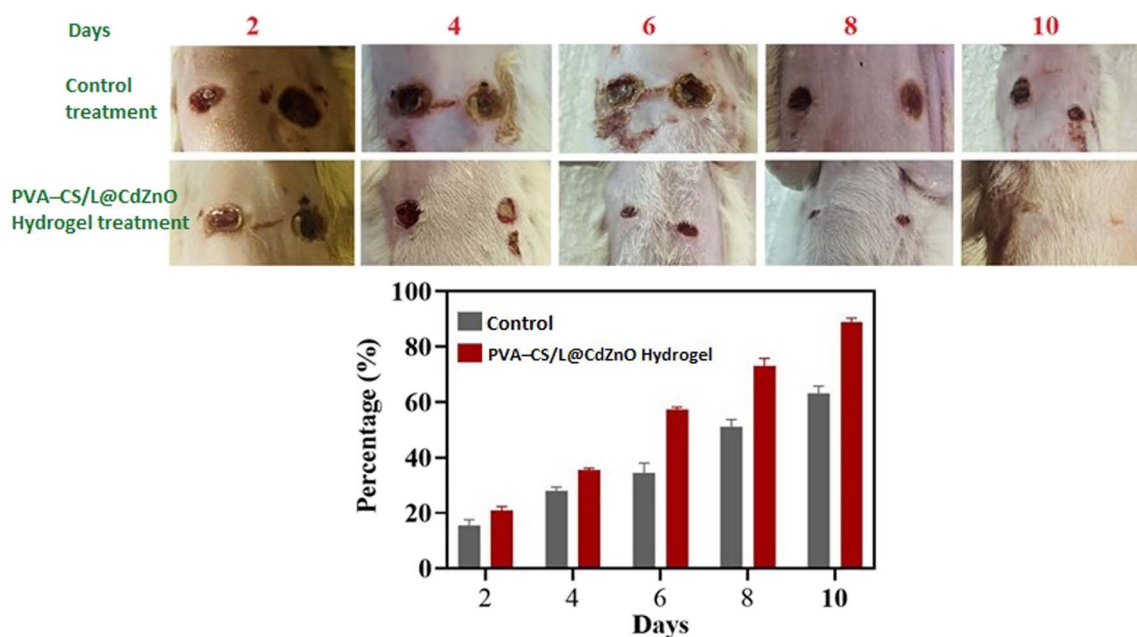

Fig. 8 Quantitative wound healing analysis of PVA–CS/L@CdZnO hydrogel in comparison with positive cotrol drug in rats.

metabolic processes and damaging DNA, proteins, and lipids, these ROS cause oxidative stress in cancer cells, which in turn causes apoptosis.[41,54] On the basis of the reported evidences, Cd and Zn of PVA–CS/L@CdZnO hydrogel, specifically disrupt mitochondrial proteases, activating caspases to induce apoptosis and halting the cell cycle, thereby preventing further cancer cell proliferation.[55] Recent studies more effectively present the smart hydrogel concept for effective cancer therapy.[56]

4 Conclusion

This study developed an eco-friendly and cost-effective approach for the synthesis of L@CdZnO and PVA–CS/L@CdZnO hydrogel using lignin, PVA and chitosan. The fabricated nanocomposites and hydrogel were characterized by UV-visible, FTIR, XRD, and TGA analyses, confirming their high purity. CdZnO and lignin@CdZnO particles exhibited hexagonal wurtzite shapes with sizes of 19.05 nm and 24.61 nm, respectively, while PVA–CS/L@CdZnO hydrogel displayed an amorphous structure. Antibacterial studies revealed that CdZnO, L@CdZnO, and the hydrogel had the potential for *S. aureus*, *E. coli*, and *B. subtilis* bacterial growth inhibition at 12 mm, 11 mm, and 18 mm, respectively. Regarding the antioxidant activities, the hydrogel showed the maximum of 89% free radical scavenging potential at the concentration of 1000 μg mL^{-1}, while all other materials showed less free radical scavenging activity. In the *in vivo* study of wound healing, the hydrogel showed significant results, with 91% healing of the wound on day 10 compared with the control, which healed the wound by almost 61% on day 10. The biocompatibility and protective nature of PVA–CS/L@CdZnO hydrogel make it a suitable scaffold for wound healing, tissue engineering, and anticancer activities. The novelty and inexpensiveness of the method make it more attractive.

Author contributions

H. A., S. A. R. N., and S. U. H. contributed equally in all fields of this research work such as conceptualization, methodology, supervision, writing original – draft, investigation, formal analysis, and supervision. X. F., Y. S., and M. S. N. contributed in conceptualization, investigation, resources, and writing – review and editing. A. R. and N. A. L. contributed in methodology, formal analysis, data interpretation, writing – review and editing. All authors have approved the manuscript for submission.

Conflicts of interest

All the authors declare no conflict of interest.

Data availability

Data will be made available on request.

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References

1 A. Shamloo, *et al.*, Fabrication and evaluation of chitosan/gelatin/PVA hydrogel incorporating honey for wound healing applications: An in vitro, in vivo study, *Int. J. Pharm.*, 2021, **592**, 120068.

2 R. F. Pereira and P. J. Bartolo, Traditional therapies for skin wound healing, *Adv. Wound Care*, 2016, **5**(5), 208–229.

3 F. Jurczak, *et al.*, Randomised clinical trial of Hydrofiber dressing with silver versus povidone–iodine gauze in the management of open surgical and traumatic wounds, *Int. Wound J.*, 2007, **4**(1), 66–76.

4 F. A. Saddique, *et al.*, Identification of Cyclic Sulfonamides with an N-Arylacetamide Group as α-Glucosidase and α-Amylase Inhibitors: Biological Evaluation and Molecular Modeling, *Pharmaceuticals*, 2022, **15**(1), 106.

5 Z. Varga, S. rafay ali Sabzwari and V. Vargova, Cardiovascular risk of nonsteroidal anti-inflammatory drugs: an under-recognized public health issue, *Cureus*, 2017, **9**(4), e1144.

6 S. U. Rizvi, *et al.*, Antimicrobial and antileishmanial studies of novel (2E)-3-(2-chloro-6-methyl/methoxyquinolin-3-yl)-1-(aryl)prop-2-en-1-ones, *Chem. Pharm. Bull.*, 2010, **58**(3), 301–306.

7 K. Kalantari, *et al.*, Chitosan/PVA hydrogels incorporated with green synthesized cerium oxide nanoparticles for wound healing applications, *Eur. Polym. J.*, 2020, **134**, 109853.

8 H. Du, *et al.*, Fabrication of recoverable Bi2O2S/Bi5O7I/ZA hydrogel beads for enhanced photocatalytic Hg0 removal in the presence of H2O2, *Sep. Purif. Technol.*, 2025, **359**, 130597.

9 S. Cheng, *et al.*, A motion-responsive injectable lubricative hydrogel for efficient Achilles tendon adhesion prevention, *Mater. Today Bio*, 2025, **30**, 101458.

10 Y. Liu, *et al.*, Fabrication of temperature and pH dual-sensitive semi-interpenetrating network hydrogel with enhanced adhesion and antibacterial properties, *Polymer*, 2025, **326**, 128343.

11 H. Qi, *et al.*, Electrospun green fluorescent-highly anisotropic conductive Janus-type nanoribbon hydrogel array film for multiple stimulus response sensors, *Composites, Part B*, 2025, **288**, 111933.

12 W. He, *et al.*, Sealing the Pandora's vase of pancreatic fistula through entrapping the digestive enzymes within a dextrorotary (D)-peptide hydrogel, *Nat. Commun.*, 2024, **15**(1), 7235.

13 Z. Cai, *et al.*, Preparation and properties of cationic starch-carrageenan-sodium alginate hydrogels with pH and temperature sensitivity, *Food Chem.*, 2024, **459**, 140272.

14 Y. Ye, et al., Multifunctional DNA hydrogels with light-triggered gas-therapy and controlled G-Exos release for infected wound healing, Bioact. Mater., 2025, 52, 422–437.

15 J. K. Li, N. Wang and X. S. Wu, Poly (vinyl alcohol) nanoparticles prepared by freezing–thawing process for protein/peptide drug delivery, J. Contr. Release, 1998, 56(1–3), 117–126.

16 Q. Zeng, et al., Preparation and properties of polyvinyl alcohol/chitosan-based hydrogel with dual pH/NH3 sensor for naked-eye monitoring of seafood freshness, Int. J. Biol. Macromol., 2024, 263, 130440.

17 E. A. Kamoun, E.-R. S. Kenawy and X. Chen, A review on polymeric hydrogel membranes for wound dressing applications: PVA-based hydrogel dressings, J. Adv. Res., 2017, 8(3), 217–233.

18 E. Fakhri, et al., Chitosan biomaterials application in dentistry, Int. J. Biol. Macromol., 2020, 162, 956–974.

19 T. Wang, et al., PVA/chitosan-based multifunctional hydrogels constructed through multi-bonding synergies and their application in flexible sensors, Carbohydr. Polym., 2025, 350, 123034.

20 F. Islam, et al., Assessment of Chitosan-PVA Hydrogels Infused with Marine Collagen Peptides for Potential Wound Healing Applications, Compos., Part C: Open Access, 2024, 100528.

21 Y. Zhang, et al., Novel lignin–chitosan–PVA composite hydrogel for wound dressing, Mater. Sci. Eng., C, 2019, 104, 110002.

22 X. Zhang, et al., Chitosan/PVA composite film enhanced by ZnO/lignin with high-strength and antibacterial properties for food packaging, Int. J. Biol. Macromol., 2025, 141658.

23 N. Alipoormazandarani, S. Ghazihoseini and A. M. Nafchi, Preparation and characterization of novel bionanocomposite based on soluble soybean polysaccharide and halloysite nanoclay, Carbohydr. Polym., 2015, 134, 745–751.

24 M. Yar, et al., Synthesis, in vitro lipoxygenase inhibition, docking study and thermal stability analyses of novel indole derivatives: Non-isothermal kinetic study of potent LOX inhibitor N'-(diphenylmethylene)-2-(1H-indole-3-yl) acetohydrazide, J. Iran. Chem. Soc., 2014, 11(2), 369–378.

25 S. Zhang, et al., Antimicrobial properties of metal nanoparticles and their oxide materials and their applications in oral biology, J. Nanomater., 2022, 2022(1), 2063265.

26 S. Balamurugan, et al., Synthesis of CdO nanopowders by a simple soft chemical method and evaluation of their antimicrobial activities, Pacific Sci. Rev. A: Nat. Sci. Eng., 2016, 18(3), 228–232.

27 A. Z. Skheel, M. H. Jaduaa and A. N. Abd, Green synthesis of cadmium oxide nanoparticles for biomedical applications (antibacterial, and anticancer activities), Mater. Today: Proc., 2021, 45, 5793–5799.

28 K. G. Nathan, K. Genasan and T. Kamarul, Polyvinyl Alcohol-Chitosan Scaffold for Tissue Engineering and Regenerative Medicine Application: A Review, Mar. Drugs, 2023, 21, 304.

29 B. Bilal, et al., Fabrication of guided tissue regeneration membrane using lignin-mediated ZnO nanoparticles in biopolymer matrix for antimicrobial activity, Front. Chem., 2022, 10, 837858.

30 W. Yang, et al., Polyvinyl alcohol/chitosan hydrogels with enhanced antioxidant and antibacterial properties induced by lignin nanoparticles, Carbohydr. Polym., 2018, 181, 275–284.

31 T. A. Sherazi, et al., Zwitterionic analog structured ultrafiltration membranes for high permeate flux and improved anti-fouling performance, J. Membr. Sci., 2022, 643, 120060.

32 S. A. R. Naqvi, et al., Antimicrobial and Antihypercholesterolemic Activities of Pulicaria gnaphalodes, Dose Response, 2020, 18(1), 1559325820904858.

33 Z. A. Khan, et al., Antioxidant and antibacterial activities of Hibiscus Rosa-sinensis Linn flower extracts, Pak. J. Pharm. Sci., 2014, 27(3), 469–474.

34 A. Abbas, et al., Phytochemical Analysis, Antioxidant and Antimicrobial Screening of Seriphidium Oliverianum Plant Extracts, Dose Response, 2021, 19(1), 15593258211004739.

35 A. Khan, et al., Aloe vera and ofloxacin incorporated chitosan hydrogels show antibacterial activity, stimulate angiogenesis and accelerate wound healing in full thickness rat model, J. Biomed. Mater. Res., Part B, 2023, 111(2), 331–342.

36 S. A. R. Naqvi, et al., Antioxidant, Antibacterial, and Anticancer Activities of Bitter Gourd Fruit Extracts at Three Different Cultivation Stages, J. Chem., 2020, 2020, 7394751.

37 N. M. Al-Hada, et al., Down-top nanofabrication of binary (CdO) x (ZnO) 1–x nanoparticles and their antibacterial activity, Int. J. Nanomed., 2017, 8309–8323.

38 L. M. Jose, S. Kuriakose and S. Thomas, Fabrication, characterization and in vitro antifungal property evaluation of biocompatible lignin-stabilized zinc oxide nanoparticles against selected pathogenic fungal strains, BioNanoScience, 2020, 10, 583–596.

39 J. Preet, et al., A lignin-based biocomposite hydrogel for antimicrobial and wound healing applications, Mater. Adv., 2024, 5(23), 9445–9457.

40 M. Asghar, et al., Synthesis and characterization of microbial mediated cadmium oxide nanoparticles, Microsc. Res. Tech., 2020, 83(12), 1574–1584.

41 A. Rafique, et al., Chia seed-mediated fabrication of ZnO/Ag/Ag2O nanocomposites: structural, antioxidant, anticancer, and wound healing studies, Front. Chem., 2024, 12, 1405385.

42 H. Kweon, I. C. Um and Y. H. Park, Structural and thermal characteristics of Antheraea pernyi silk fibroin/chitosan blend film, Polymer, 2001, 42(15), 6651–6656.

43 X. Ji, et al., Synthesis and characterization of alkali lignin-based hydrogels from ionic liquids, BioResources, 2017, 12(3), 5395–5406.

44 J. Zhou, et al., Remineralization and bacterial inhibition of early enamel caries surfaces by carboxymethyl chitosan lysozyme nanogels loaded with antibacterial drugs, J. Dent., 2025, 152, 105489.

45 Y. Xie, *et al.*, Antibacterial activity and mechanism of action of zinc oxide nanoparticles against Campylobacter jejuni, *Appl. Environ. Microbiol.*, 2011, **77**(7), 2325–2331.

46 L. Zhang, *et al.*, ZnO nanofluids–A potential antibacterial agent, *Prog. Nat. Sci.*, 2008, **18**(8), 939–944.

47 R. Y. Pelgrift and A. J. Friedman, Nanotechnology as a therapeutic tool to combat microbial resistance, *Adv. Drug Deliv. Rev.*, 2013, **65**(13–14), 1803–1815.

48 A. J. Friedman, *et al.*, Antimicrobial and anti-inflammatory activity of chitosan–alginate nanoparticles: a targeted therapy for cutaneous pathogens, *J. Invest. Dermatol.*, 2013, **133**(5), 1231–1239.

49 A. Alzagameem, *et al.*, Antimicrobial activity of lignin and lignin-derived cellulose and chitosan composites against selected pathogenic and spoilage microorganisms, *Polymers*, 2019, **11**(4), 670.

50 B. N. Singh, *et al.*, Biosynthesis of stable antioxidant ZnO nanoparticles by Pseudomonas aeruginosa rhamnolipids, *PLoS One*, 2014, **9**(9), e106937.

51 F. M. Freitas, *et al.*, Green synthesis of lignin nano-and micro-particles: Physicochemical characterization, bioactive properties and cytotoxicity assessment, *Int. J. Biol. Macromol.*, 2020, **163**, 1798–1809.

52 L. R. C. Barclay, F. Xi and J. Q. Norris, Antioxidant properties of phenolic lignin model compounds, *J. Wood Chem. Technol.*, 1997, **17**(1–2), 73–90.

53 A. Aradmehr and V. Javanbakht, A novel biofilm based on lignocellulosic compounds and chitosan modified with silver nanoparticles with multifunctional properties: Synthesis and characterization, *Colloids Surf., A*, 2020, **600**, 124952.

54 S. A. Shahzad, *et al.*, Synthesis, thymidine phosphorylase inhibition and molecular modeling studies of 1,3,4-oxadiazole-2-thione derivatives, *Bioorg. Chem.*, 2015, **60**, 37–41.

55 M. Roshani, *et al.*, Metal nanoparticles as a potential technique for the diagnosis and treatment of gastrointestinal cancer: a comprehensive review, *Cancer Cell Int.*, 2023, **23**(1), 280.

56 L. Guo, *et al.*, Smart hydrogel: A new platform for cancer therapy, *Adv. Colloid Interface Sci.*, 2025, **340**, 103470.