



Cite this: *Nanoscale*, 2025, **17**, 7738

Received 7th January 2025,
Accepted 16th February 2025

DOI: 10.1039/d5nr00071h

rsc.li/nanoscale

Characterisation of polymeric nanoparticles for drug delivery

Thomas G. Floyd,^a Pratik Gurnani  ^b and Julia Y. Rho  ^{*c}

Polymeric nanoparticles represent an innovative approach to drug delivery, particularly for addressing complex diseases like cancer. Their nanoscale dimensions facilitate targeted cellular uptake and effective navigation of biological barriers. With a broad range of polymerisation and functionalisation techniques, these nanoparticles can enable precise drug release, enhanced stability, and improved bioavailability while minimising side effects. Compared to conventional carriers, polymeric nanoparticles offer superior stability and versatility. However, despite these beneficial attributes, challenges remain in understanding their dynamic behaviour and interactions within biological systems. This mini-review aims to highlight key characterisation methods for studying polymeric nanocarriers, explore recent advances, and examine current challenges that must be addressed to optimise their therapeutic potential and advance these promising targeted drug delivery systems.

Introduction

Polymeric nanoparticles, typically ranging from 10 to 1000 nanometers, have garnered significant interest as advanced

drug delivery vectors due to their small size, adaptability, and ability to transport and protect therapeutic agents to target sites within the body.¹ Their nanoscale dimensions enable cellular uptake and allow these particles to cross biological barriers, including the challenging blood-brain barrier,^{2,3} which is critical for delivering drugs directly to cells in diseases like cancer.^{2,4-6}

A major advantage of polymeric nanoparticles (PNPs) is their chemical versatility, enabling the creation of a virtually limitless range of polymers with tailored properties through various polymerisation methods (e.g., ring-opening, radical, ionic, etc.), functional groups (e.g., sugars, charged moieties, stimuli-responsive chemistries), and controlled chain length and composition.⁷⁻¹⁸ This versatility supports fine-tuned control over essential delivery parameters, such as release profiles and targeting mechanisms, making polymers ideal for optimised drug delivery.¹⁹ Notably, PNPs can encapsulate drugs, improving the stability and solubility of hydrophobic compounds and protecting sensitive molecules—such as peptides, proteins, and small molecules—from premature degradation to ensuring targeted delivery.²⁰⁻²³ Additionally, polymeric nanoparticles can be engineered for controlled release triggered by stimuli like pH, temperature, or enzyme activity, reducing side effects and enhancing therapeutic outcomes.²⁴⁻³⁰ Importantly, these polymer-based nanomaterials open new avenues for administering drugs previously limited by poor solubility or bioavailability. Additionally, by enhancing drug efficacy at lower doses, polymeric nanoparticles could reduce adverse effects and improve patient outcomes, which is a crucial benefit for administering highly toxic drugs.³¹⁻³⁵

^aAdvanced Drug Delivery, Pharmaceutical Sciences, R&D, AstraZeneca, Macclesfield, UK

^bUCL School of Pharmacy, University College London, 29-39 Brunswick Square, Bloomsbury, London, WC1N 1AX, UK

^cDepartment of Chemistry, University College London, 20 Gordon Street, London, WC1H 0AJ, UK. E-mail: j.rho@ucl.ac.uk



Julia Y. Rho

Julia Rho obtained her MChem (2015) and Ph.D. (2019) from the University of Warwick under Prof. Sébastien Perrier. She then joined the University of Florida as a postdoctoral researcher with Prof. Brent Sumerlin, focusing on cyclic polymers and photo-initiated polymerisation. In 2021, she joined Warwick Medical School to develop sustainable gene delivery vectors before taking on the role of

Group Leader at the University of Birmingham with Prof. Rachel O'Reilly. In 2024, she became a Lecturer in Organic Chemistry at UCL, where her group focuses on using advanced microscopy to investigate polymeric nanoparticles for gene and drug delivery.



In addition to small-molecule drugs, polymers and polymeric nanocarriers have garnered much attention as gene delivery vectors.^{36–38} Compared to traditional gene delivery systems like liposomes, polymeric nanoparticles offer better stability and tunability, facilitating easier storage and broader accessibility for patients worldwide. Their adaptability and cost-effectiveness—particularly their potential to eliminate the need for cryogenic storage—make them appealing alternatives to protein—or lipid-based carriers,³⁹ which often struggle with stability and scalability issues.

Polymer nanoparticles are capable of self-assembly through a variety of motifs, including hydrophobic effects,⁴⁰ hydrogen bonding,^{41–47} crystallisation,^{48,49} and host-guest interactions.^{50–52} These self-assembled structures exhibit a diverse array of properties, such as defined sizes, morphologies, charges, surface chemistries, and functional targeting moieties,^{15,53–55} all of which significantly influence their performance in drug delivery applications.⁵⁶ The characterisation of these features is crucial for understanding their structure–property relationships and typically involves a collection of complementary techniques, including electron microscopy, light scattering, and fluorescence bioimaging.^{57,58} These methods can collectively enable precise tuning of nanoparticle properties to optimise therapeutic outcomes.

Despite their exciting potential, characterising polymeric nanoparticles remains a significant hurdle. Advanced techniques are required to study nanoparticle assembly, stability, and behaviour both *in vitro* and *in vivo*. These methods are essential for evaluating how nanoparticles interact with cells, traverse biological barriers, and function within complex extracellular environments. Understanding the fate of nanoparticles

in circulation, their biodistribution, and their ability to evade the immune system is critical to advancing nanomedicine and achieving targeted delivery.

As polymeric nanoparticles are developed for drug delivery, their performance must be evaluated through *in vivo* studies, including comprehensive pharmacokinetic and pharmacodynamic analyses. These assessments extend beyond nanoscale characterisation, examining critical parameters such as circulation profiles, biocompatibility, toxicity, and therapeutic efficacy. While this article will focus on the nanoscale characterisation of self-assembled polymeric nanostructures for drug delivery, we acknowledge that studying their *in vivo* behaviour and translational potential is equally critical to realising their therapeutic promise for patients. Readers are directed to the excellent reviews cited herein for valuable insights and discussions on these topics.^{59,60}

This mini-review highlights key chemical characterisation techniques for studying organic polymer-based nanoparticles (see Fig. 1), emphasising their strengths, limitations, and recent advancements. By discussing how these techniques deepen our understanding of nanoparticle behaviour in biological systems and the current challenges in the field, we aim to advocate for improved characterisation practices within the field. This mini-review aims to provide a valuable resource for newcomers to the field, encouraging them to explore the wide range of methods available for characterising novel polymeric drug delivery systems. It also seeks to inspire those already working in the field to adopt new analytical approaches to deepen understanding and corroborate insights into the complex polymeric delivery systems being developed. Lastly, we hope this summary may attract researchers from other dis-

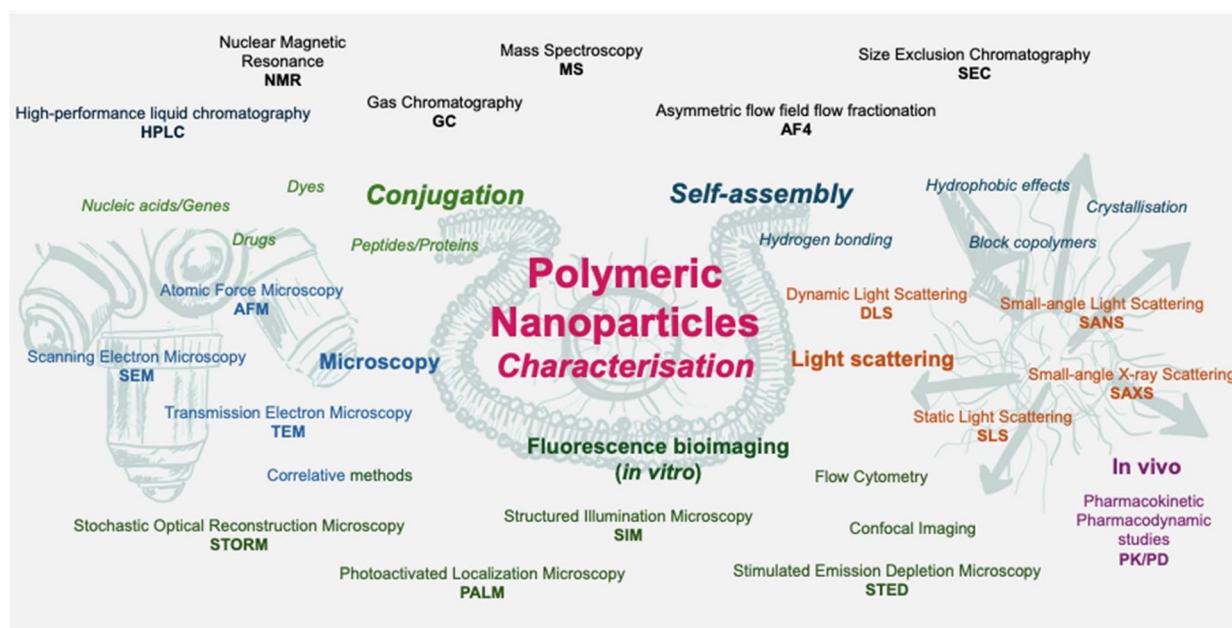


Fig. 1 Summary of polymer and polymer nanoparticle characterisation methods.



ciplines to join us in building innovative approaches that unlock the full therapeutic potential of polymeric nanomedicines and advance the future of targeted drug delivery.

Characterisation methods

Nuclear magnetic resonance (NMR) spectroscopy

Nuclear Magnetic Resonance (NMR) Spectroscopy is an essential tool in polymer chemistry, providing detailed insights into the conversion and kinetics of polymerisation reactions. While less common methods, such as gas chromatography, can also be used to track volatile vinyl monomers, NMR remains the primary method for monitoring the progression of polymerisation reactions. Regardless of the initiation mechanism, the conversion of monomer to polymer, hence polymerisation, is calculated by tracking the appearance of polymer and the disappearance of monomer peaks.

Many self-assembled polymer nanoparticles used for drug delivery are composed of copolymers with distinct block chemistries. These variations drive phase separation into well-defined microdomains, enabling the formation of nanostructures with diverse morphologies. Such nanostructures include spherical and cylindrical micelles, nanofibres, platelets, and vesicles.^{12,32,61-63} It is hoped that tuning the polymeric morphologies may hold the key to addressing significant challenges in drug delivery, such as controlled release.⁶⁴

In block copolymer synthesis, the sequential building of blocks relies on maintaining the “living” polymer chain ends, which allows polymerisation to continue when conditions are suitable (e.g., in the presence of additional monomers, initiators, and typically an oxygen-free environment). NMR is particularly valuable for assessing the “livingness” of controlled polymers, as it can monitor polymer growth and confirm the process remains under controlled conditions. By analysing specific signals in ¹H NMR spectra, researchers can verify consistent chain growth with low levels of termination or side reactions, ensuring the polymerisation retains the characteristics of a living system.

Moreover, NMR becomes a powerful technique when dyes or drugs are conjugated to the polymer structure. Upon conjugation, new characteristic peaks often emerge in the NMR spectrum, or existing peaks may shift due to the formation of new bonds. By examining these changes, it is possible to confirm the successful conjugation of therapeutic agents or fluorescent dyes, which is essential for applications in targeted drug delivery and imaging. Quantifying the success of conjugation is feasible by comparing expected and observed integration values. However, matching the integration of characteristic peaks does not guarantee that all molecules in the solution are conjugated, as unconjugated species may still be present. Therefore, additional characterisation methods are recommended to corroborate conjugation efficiency, such as HPLC and *vide infra*.

Two-dimensional NMR techniques, such as COSY, HSQC, and HMBC, offer powerful insights into the local chemical

environments near the conjugation site. These techniques can reveal interactions between adjacent atoms and identify specific structural features of the polymer. By mapping out spatial relationships and connectivity, 2D NMR can help confirm that conjugation has occurred at the intended site on the polymer chain, thereby ensuring accurate functionalisation. In the context of drug delivery, these complementary methods are invaluable. ¹H NMR enables the confirmation of drug-conjugate linkages, while ¹³C NMR provides detailed structural information about the polymer backbone. Additionally, quantitative NMR facilitates the precise measurement of drug loading or the density of functional groups. For instance, in PEG-PLGA systems, NMR is frequently employed to validate the successful conjugation of a hydrophobic drug to the hydrophilic polymer, enhancing both solubility and release profiles.

Diffusion-ordered (DOSY) NMR has long been a powerful technique for determining the molecular weight of polymers. Its potential was first demonstrated in 1989 by von Meerwall, who showed that pulsed field gradient NMR (PFG NMR) was sufficiently sensitive to detect differences in molecular size and, hence, the molecular weight of polymers.⁶⁵ Subsequent work by Johnson and colleagues expanded this approach, enabling the determination of molecular weight distributions of polymers using constrained regularisation algorithms in diffusion-ordered NMRs.⁶⁶ With the rapid expansion of polymer chemistry, significant efforts were devoted to developing accurate methods for determining molecular weights across a diverse range of polymers. These advancements addressed the challenges posed by varying solution properties, which depended on the choice of polymer and solvent systems. Accurate molecular weight determination became critical for understanding polymer behaviour, optimising synthesis, and tailoring properties for specific applications.⁶⁷⁻⁶⁹

Recent advances in flow chemistry and the development of compact benchtop NMR systems have significantly revitalised the utility of NMR for polymer characterisation.⁷⁰ Notably, the work by the Leibfarth,⁷¹ Warren,⁷² and Junkers groups has demonstrated increasingly efficient,⁷³ solvent-independent,⁷⁴ and universal approaches to molecular weight determination.⁷⁵ With the growing incorporation of AI in data collection, processing, and molecular weight prediction, these high-throughput methodologies are poised to become even more critical, enabling rapid input and feedback loops for polymer development. In a recent article, Gormley discusses the intricate interplay of complex interactions that govern the effectiveness of drug delivery systems.⁷⁶ The article underscores the interconnected nature of key factors such as polymer properties, their behaviour in diverse environments (*in vitro* and *in vivo*), and the mechanisms driving drug release. Referred to as the “curse of dimensionality” in drug delivery, the author points out how interdependent parameters like crystallinity, water absorption/swelling, hydrolysis, and erosion, rely on a broad range of polymer/particles attributes (e.g., molecular weight, size, morphology, porosity) and external conditions (e.g., pH, temperature, osmolarity, location). This highlights



the substantial challenges involved in designing efficient and reliable polymer-based drug delivery systems. However, the author expresses optimism about the potential of machine learning to address these critical issues.

From this, two key parameters to highlight are zeta potential and porosity. Zeta potential, which measures the electrophoretic mobility of particles, is a crucial indicator of nanoparticle surface charge as it affects colloidal stability, aggregation tendencies, and interactions with biological membranes. A high absolute zeta potential (either positive or negative) generally enhances stability by preventing aggregation, while moderate values may be beneficial for controlled interactions with cells and biomolecules. Zeta potential can be measured using instruments such as electrophoretic light scattering (ELS), phase analysis light scattering (PALS), streaming potential instruments, electrokinetic analysers (EKA), and nanoparticle tracking analysis (NTA). It's important to consider that zeta potential is strongly influenced by pH and salt concentration. As nanoparticles are introduced into biologically representative media like blood and plasma, changes in the media, including pH, ions, and proteins (which form the nanoparticle's protein corona), must be considered carefully.

Porosity in nanoparticles plays a crucial role in drug delivery by enhancing drug encapsulation efficiency and enabling controlled or sustained drug release. Additionally, porosity affects density, influencing sedimentation behaviour, diffusion, and transport within biological systems. Together, these physicochemical properties are key to optimising polymeric nanoparticles for targeted, efficient drug delivery. High porosity increases drug loading capacity, improving efficiency and bioavailability. It allows for sustained, targeted release, reducing side effects and improving patient outcomes. Moreover, the porous structure facilitates better drug diffusion and responsiveness to environmental triggers, making porous nanoparticles ideal for precision medicine. Porosity can be measured using techniques such as Brunauer–Emmett–Teller (BET) analysis (for surface area and pore size), mercury intrusion porosimetry (MIP) for pore volume, and electron microscopy (TEM/SEM) for direct imaging. SAXS provides nanostructural details, while TGA assesses porosity through weight loss analysis. Advanced methods like NMR and X-ray tomography offer 3D imaging of porous structures, all helping to optimise drug loading and controlled release in drug delivery applications.

This level of detail is crucial for applications requiring precise polymer architectures, as even small deviations in conjugation sites can alter the material's properties and performance in drug delivery systems.

Size exclusion chromatography (SEC)

Size Exclusion Chromatography (SEC) is a foundational technique in polymer chemistry, providing critical insights into polymer conversion and the evolution of molecular weight. By tracking changes in molecular weight over time, SEC can help monitor the kinetics of polymerisations, offering valuable information about the progress and control of the reaction.

SEC also provides data on the molecular weight distribution, which is important for assessing the uniformity of polymer chains. A narrow symmetrical molecular weight distribution indicates a controlled polymerisation process, where chains start growing at the same time (initiation stage) and grow at a similar rate (propagation stage). In contrast, a broader or asymmetrical distribution may suggest uncontrolled polymerisation and multiple side reactions, leading to variations in chain length.

A double molecular weight peak in the SEC profile can indicate chain–chain coupling, where two polymer chains have joined to form a larger macromolecule. This phenomenon may occur more often during certain polymerisation processes or under specific conditions, such as a high concentration of active polymer chains. Importantly, the degree of chain–chain coupling can influence the uniformity of polymer chains, thereby affecting the properties of the final polymer (e.g. solubility and self-assembly behaviour).

SEC is particularly useful in monitoring chain extension during block copolymerisation, which is essential for designing self-assembling polymers. As mentioned above, the difference in block chemistries is often used in polymer nanoparticle synthesis to generate core–shell nanoparticles. The most common example is a block copolymer with hydrophilic and hydrophobic domains, which self-assembles into nanoparticles. The hydrophobic chains are assembled in the core away from the water, and the hydrophilic chains stabilise the nanoparticles, forming the corona.

Detectors compatible with SEC, such as RI, UV, fluorescence, and viscometry, can be used to assess polymer characteristics. If the polymer contains a UV-active group, such as a conjugated dye or a functional group, it can be monitored as it separates by size. For example, in reversible addition–fragmentation chain-transfer (RAFT) polymerisation, the trithiocarbonate group absorbs at 309 nm and can be detected by coupling SEC with UV detection. This allows for the selective monitoring of polymers with UV-active groups, such as dyes or drugs, which are attached *via* conjugation chemistry. By confirming the presence and distribution of these groups, researchers can verify successful functionalisation and optimise the system for applications requiring precise drug or dye loading.

Due to the increasing complexity of polymeric nanomaterials for drug delivery, molecular weight determination is more complex than for linear polymers. Often, multi-detector SEC (MD-SEC) is required to accurately determine the molecular weight, requiring a concentration detector, such as RI or UV, a light-scattering detector and a viscometer. Working in tandem, these detectors are able to accurately determine the molecular weight of the analyte and other parameters such as concentration, incremental refractive index, size, branching, or, in the case of polymer–drug conjugates, drug loading.⁷⁷ or polymer–drug conjugates, understanding the release rate of the active pharmaceutical ingredient (API) from the nanoparticle is crucial to understanding its efficacy. Whilst SEC is not commonly applied to determine the rate of API release, it



can be used to monitor the release rate by studying the appearance of a peak associated with the API, likely at higher retention volumes, or in the case of APIs with unique UV absorbance from the nanoparticle, monitoring the decrease in UV signal for the nanoparticle.⁷⁸

A further application of SEC to polymeric nanomaterials is to understand their physical stability in aqueous media. SEC is able to reveal the presence of aggregates in a sample, indicated by peaks at lower retention volumes. This is further confirmed by light scattering detectors, where due to the intensity of scattered light being proportional to the size to the power of six, aggregates have a much greater intensity compared to their corresponding intensity determined by a concentration detector, such as RI. Carrying out a complimentary SEC analysis in an organic solvent can be beneficial in confirming if the aggregation is due to non-covalent interactions or caused by covalent coupling.⁷⁹

In drug delivery, GPC is crucial for determining a polymer's molecular weight (M_w) and polydispersity index (PDI), ensuring consistency from batch to batch. It also monitors molecular weight changes during degradation, providing insights into the polymer's stability. For example, in hydrogel-based drug carriers, GPC identified an optimal M_w range that enabled sustained drug release over several weeks, aligning with therapeutic objectives.

Mass spectrometry (MS)

Mass spectrometry (MS) is a powerful technique for characterising both homopolymers and copolymers, providing valuable insights into their molecular structure. Matrix-assisted laser desorption/ionisation time-of-flight (MALDI-TOF) MS has been commonplace for the characterisation of homopolymers, such as polyethylene glycol. MALDI-TOF is particularly effective for analysing polymers with well-defined end-group functionalisation. This technique allows the identification of the polymer's molecular weight and the detection of end groups, providing crucial information on the degree of polymerisation and ensuring the desired functionalisation at the chain ends.

Due to the number of exponential fragment patterns, characterising copolymers using MS is more challenging. Haddleton and coworkers showed that MALDI, in conjunction with laser-induced dissociation (LID) fragmentation techniques (MALDI-LID-ToF/ToF), could be used to isolate and fragment statistical and diblock polyacrylate copolymers.⁸⁰ Additionally, methods that use two-dimensional or Kendrick mass defect plots to process the mass spectra of polymers have been incredibly powerful.^{81–83} Volmer and coworkers were able to map the genealogical links in mixtures of lignin depolymerisation products using two-dimensional mass defect matrix plots. These tools have the potential to be extended to other classes of polymers (*e.g.* copolymers or terpolymers).⁸³

Since then, double-resonance experiments, using electron capture dissociation (ECD) and Fourier transform ion cyclotron resonance (FT-ICR) tandem mass spectrometry, have been able to characterise acrylamide homo- and block copolymers.⁸³ More recently, polymer MS using two-dimensional method-

ologies has also shown that the precursors that produce independent fragments can be separated *via* modulation frequency. Furthermore, these techniques can be employed to understand and map the specific sequences of random copolymers, gaining insights into how monomers are distributed along a polymer backbone.⁸⁴ These advances allow us to analyse increasingly complex and dispersed polymer samples that have previously not been able to be characterised through MS due to the lack of effective separation through chromatographic or isolation techniques.⁸⁵ In the future, with advances in computation and machine learning, these methods could become more commonplace to differentiate between various copolymer compositions, providing insights into their structural heterogeneity, sequence, and molecular weight distribution.

High-performance liquid chromatography (HPLC)

High-Performance Liquid Chromatography (HPLC), though widely underutilised by the polymer field, is a highly effective technique for polymer characterisation. By optimising solvent composition and selecting appropriate stationary phases, HPLC enables the separation of polymers based on their polarity. This approach is crucial for evaluating the purity, molecular distribution, and structural integrity of polymer products, providing valuable insights into their composition and performance. Notably, Hawker and coworkers utilised the polarity-based separation method (flash chromatography) to successfully isolate polymers with specific degrees of polymerisation (DP).⁸⁶ Though this process may seem laborious and time-consuming, it represents a significant milestone in polymer synthesis by enabling the isolation of individual polymer chain lengths. This advancement is crucial because it allows for the production of polymers with specific, well-defined molecular weights. In applications where uniformity is essential—such as in drug delivery systems—the ability to isolate distinct polymer chain lengths becomes particularly important. Achieving increasingly uniform or even monodisperse polymers can improve consistency, efficacy, and safety, which are critical factors for meeting regulatory standards and ensuring optimal performance in various biomedical applications.

HPLC is also useful for tracking changes in copolymer composition. By monitoring the polymer's retention time (and thus changes in polarity), shifts in composition during polymerisation can be observed. For example, a study by Perrier and Peltier used HPLC to monitor the composition of copolymers (statistical *versus* block), providing detailed insights into how polymer composition and comonomer distribution vary within a specific polymer chain.⁸⁷

Another important application of HPLC is its ability to monitor the conjugation of polymers with dyes, drugs, or peptides, a critical process in drug delivery and diagnostic imaging. With built-in UV and fluorescence detectors, HPLC offers valuable tracking of the conjugation process, providing quantitative insights into both reactants and products before and after conjugation, see Fig. 2.⁸⁸ By analysing the UV absor-



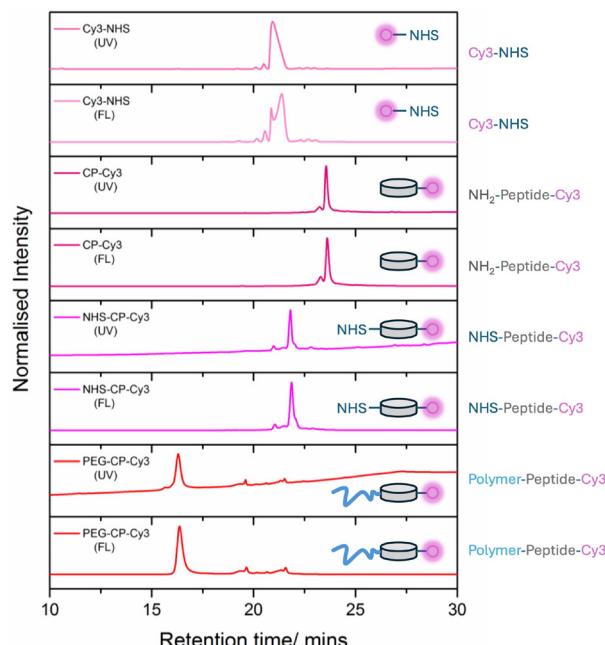


Fig. 2 High-performance liquid chromatography (HPLC) of peptide-polymer-dye conjugate. UV absorption at 280 nm (tryptophan absorption to follow the peptide), fluorescence emission measured at 570 nm upon excitation at 555 nm (to follow the Cyanine 3 dye). Adapted from Rho *et al.*, reproduced with permission from Wiley.⁸⁸

bance or fluorescence emission signals, researchers can assess the efficiency of the conjugation, as well as the progress of the reaction. This allows for precise control over the functionalisation process, ensuring that the desired loading, composition, and overall quality of the conjugates are achieved for optimal performance in their intended application.

As mentioned above, understanding the release of drugs from polymer-drug conjugates is a crucial parameter to understand. Not only can we determine the rate of release in biologically relevant media, but we can also determine the effectiveness of a stimuli-responsive linker. As with SEC, HPLC can be utilised to quantify the release of drugs from the polymeric nanoparticle. Suppose the drug is chemically conjugated to the drug. In that case, this can be straightforward, with the release media containing the nanomaterial and released API directly injected into the HPLC and the peak area calculated. However, for drugs physically encapsulated within a polymeric micelle, this proves more challenging. HPLC will disrupt the encapsulation and will not be able to distinguish between released and encapsulated API. Methods for separation are discussed in detail in the review published by Ghezzi *et al.*⁸⁹ However, the most common procedure involves the employment of dialysis to separate the free API from the micelle. The filtrate is then analysed, and the concentration of the released drug is determined. For both systems, once the API peak area has been determined, it can be plotted *versus* time to understand the release profile of the drug from the nanoparticle.

Microscopy

Transmission electron microscopy (TEM)

Microscopy has significantly advanced nanoparticle characterisation, providing valuable insights into their nanoscopic structures in both solution and cellular environments. Transmission Electron Microscopy (TEM) is particularly useful for visualising nanoparticles due to its high resolution (down to a few nanometers). However, organic polymeric nanoparticles can be challenging to image due to their low electron density, which can reduce contrast and clarity compared to inorganic nanoparticles. Despite this, TEM remains essential for understanding the morphology and behaviour of polymeric nanoparticles. The use of contrast agents or stains, such as phosphotungstic acid (PTA), uranyl acetate, osmium tetroxide (OsO_4), and ruthenium tetroxide (RuO_4), can be used to enhance imaging clarity. However, these stains require careful use and handling due to factors like pH sensitivity and inherent toxicity, which must be managed to ensure accurate and reliable imaging.

A key feature of polymer nanoparticles designed as drug carriers is the reversibility of their self-assembled structures, which are formed through non-covalent interactions. This dynamic property allows the nanoparticles to maintain stability during circulation and drug delivery while also enabling disassembly at the target site to release the therapeutic cargo. These metastable nanostructures require sufficient stability for administration through the bloodstream and into targeted cells but must also dynamically disassemble to release drugs at therapeutic levels without causing significant toxicity or instability during transport. Advanced TEM techniques, such as liquid-cell TEM⁹⁰ and cryo-TEM,^{91,92} are critical for studying these systems under more representative solution-phase or intracellular conditions. These approaches provide invaluable insights into the stability, behaviour, and drug release mechanisms of polymeric nanoparticles, furthering their development as effective drug delivery vectors.

Key contributions to the field include the work of Granick and coworkers, who demonstrated the visualisation of individual macromolecules like polystyrene sulfonate and poly(ethylene oxide) in aqueous solutions using graphene-based liquid-cell TEM. This approach achieved nanometer-resolution imaging without metal-ion labelling.⁹³ It minimises electron-induced damage and background scattering, enabling detailed analyses of polymer sizes, conformational fluctuations, and adsorption-desorption events with standard TEM instruments.

A powerful example of pushing the resolution of these techniques for self-assembled polymeric nanostructures includes work by Manners and coworkers using high-resolution cryo-TEM. In this work, the corona and crystalline core of nanofibres in vitrified solution were directly observed, revealing a 2D pseudo-hexagonal symmetry in the core's packing and a detailed molecular model of polymeric nanofibres. These findings provide unprecedented insight into the structural order of nanofibres with crystalline cores, with implications for



analogous systems, such as π -conjugated block copolymer nanofibers. Moreover, open-source Python libraries have endeavoured to simplify image analysis for TEM and *in situ* TEM.⁹⁴

Recent studies by Wu *et al.* expanded the capabilities of polymer electron microscopy by highlighting advances in TEM instrumentation, including focused ion beams, liquid-phase sample holders, monochromated sources, and direct electron detectors. These reduce radiation sensitivity constraints and promise transformative impacts for imaging soft materials.⁹⁵

Scanning electron microscopy (SEM)

Another invaluable electron microscopy (EM) technique for polymer nanoparticle characterisation is Scanning Electron Microscopy (SEM). While both SEM and TEM are effective for determining particle size, they excel in different areas. TEM is ideal for internal structural analysis, providing detailed insights into nanoparticle morphology, composition, and assembly. In contrast, SEM focuses on surface morphology and particle aggregates, making it particularly useful for studying coatings and overall topology. The choice between TEM and SEM depends on the specific characterisation goals and required resolution. TEM offers sub-nanometer resolution, while SEM typically resolves to tens of nanometers. However, TEM is more sensitive to beam-induced degradation, particularly at higher voltages, making SEM a more robust option for delicate polymer samples.⁹⁶

When analysing polymeric nanoparticles, two critical factors must be considered: the potential for electron beam-induced damage or alteration of the sample, which can affect imaging accuracy, and the difference between experimental conditions and the biological environment, which raises questions about how well *in vitro* studies replicate *in vivo* behaviour. Addressing these challenges, along with advancements in imaging techniques and experimental design, will be crucial for a deeper understanding of how self-assembled polymers behave in living cells and dynamic biological systems.

Atomic force microscopy (AFM)

Atomic Force Microscopy (AFM) complements many of the EM techniques by providing additional insights into the surface morphology, mechanical properties, and three-dimensional topology of polymeric nanostructures. While EM excels in revealing the internal crystalline structure and molecular organisation, AFM offers high-resolution imaging of the nano-fibre surface in real space and under conditions closer to ambient. As with living systems, synthetic supramolecular systems can also 'grow' in a 'living' manner. *In situ* methods to visualise the growth process have been achieved using AFM,⁹⁷ TEM,^{98,99} and iSCAT.¹⁰⁰ Going back to the examples of polymeric nanoparticles assembled through crystallisation, Manners and coworkers were able to use AFM to study the growth of nanofibers on a silicon surface.⁹⁷ The paper also revealed unidirectional growth in certain orientations, where seed alignment restricted growth to one terminus. These insights provide a deeper understanding of BCP nanofiber

growth and its potential for controlled nanoparticle fabrication.

In related work by O'Reilly, Dove, and coworkers, uniform two-dimensional platelets formed through crystallisation-driven self-assembly were effectively characterised using TEM, AFM, and STED, revealing their multilayered structure.¹⁰¹ These multilayered platelets offer significant potential for designing polymeric systems with tailored chemistries, enabling precise control over drug release profiles.¹⁰² In other related areas, the field of artificial cells has advanced significantly, particularly through the use of amphiphilic block copolymers to form vesicular bilayers, often referred to as polymersomes.^{103–108} Structurally analogous to liposomes but composed of polymers, polymersomes provide enhanced stability and tunability, making them ideal candidates for drug delivery and other biomedical applications.¹⁰⁴

All these examples offer valuable insights into the assembly and disassembly processes of polymeric nanoparticles. Gaining a deeper understanding of their dynamic behaviour is crucial for optimising drug delivery systems, ensuring efficient transport, and achieving controlled release from polymer-based nanocarriers.

Fluorescence imaging

Fluorescence imaging is crucial for characterising polymer nanoparticles as it can provide real-time, non-invasive insights into their behaviour and interactions in both solution, *in vitro* and *in vivo*. It enables the tracking of fluorescently labelled nanoparticles in biological systems, elucidating processes such as cellular uptake, biodistribution, and drug release mechanisms.¹⁰⁹ Furthermore, the ability to label specific components of nanoparticles allows for a detailed investigation of core–shell architectures and their dynamic behaviour in complex biological systems.

Fluorescent polymeric nanoparticles (NPs) have proven valuable for *in vivo* applications such as tracking cell fate and tumour development. For example, AIE-based NPs were used to label cancerous cells, enabling their imaging in mice over 21 days, while Rhodamine B-based NPs monitored stem cell implantation in mouse brains.¹¹⁰ Biocompatibility and low toxicity are critical for these applications, with studies showing minimal cytotoxicity for dye-loaded NPs at relevant concentrations. Encapsulation of dyes further reduces toxicity, and biodegradable polymers like PLGA or PCL make these NPs suitable for biomedical use. Emerging applications now leverage dye-loaded NPs not only as labels but also as multifunctional fluorescent probes, paving the way for theranostics and other advanced biomedical technologies. See previous sections on the characterisation of polymer-dye conjugates.

However, the resolution of fluorescence imaging is limited by the diffraction limit of light, approximately 200–250 nm, which can obscure finer structural details at the nanoscale. Recent advancements, such as super-resolution techniques like STED, PALM, and STORM, have extended fluorescence



imaging's capabilities to achieve resolutions down to 20–30 nm, enabling more precise characterisation of polymer nanoparticles.¹¹¹ These innovations bridge the gap between nanoscale resolution provided by electron microscopy and the dynamic, functional insights offered by fluorescence imaging, making it an indispensable tool for nanoparticle research.

Early work by Albertazzi and Meijer showed that homogeneous exchange could be observed in the BTA-based supramolecular polymers using super-resolution imaging (Fig. 3a and b).¹¹² This could be attributed to disordered domains within the ordered hydrogen-bonded structure, where weaker monomer interactions facilitate the exchange process.^{113,114} The STORM technique revealed that this exchange occurs uniformly along the polymer backbone, with no evidence of fragmentation, fusion, or polymerization–depolymerization at the chain ends, suggesting a need to reassess the dynamic behaviour of supramolecular fibres.^{112,115} Cox *et al.* combined AFM and STORM to investigate the self-assembly process of peptide surfactants, revealing the formation of helical fibres ranging from 5 to 10 µm (Fig. 3c and d). Using two-colour STORM, they were able to study the dynamic self-assembly process of these peptides after mixing. Building on this work, Perrier and co-workers demonstrated that dual-labeling strategies with STORM could also visualise the formation of supramolecular block-like structures, where two individual metastable peptide-polymer nanotubes fused together (Fig. 3e).

Similar studies using other super-resolution techniques, such as stimulated emission-depletion (STED) microscopy, have demonstrated the versatility of non-covalent Alexa-488 labelling for imaging cationic self-assembling peptides and peptide-functionalised gold nanoparticles.¹¹⁶ This approach provides a simple and effective method for electrostatically labelling cationic peptide nanostructures, enabling real-time, *in situ* imaging of dynamic processes under physiological conditions.

The success of many super-resolution methodologies hinges on striking a balance between fluorescently labelling biological molecules within cells and the synthetic nanostructures of interest (*i.e.*, your drug-loaded nanoparticle). Albertazzi and colleagues developed a simple, versatile workflow using DNA-PAINT to standardise and enhance the quantification of biological molecule density and distribution on synthetic substrates and cell membranes.^{117–119} This approach improves accuracy, sensitivity, and precision, as demonstrated by the quantification of docking strands on sensor surfaces and PD1 and EGFR receptors on cellular models while effectively filtering out non-specific interactions and artefacts.¹¹⁷

Building on this work, the group also designed nanoparticles functionalised with targeting ligands to selectively deliver therapeutics to cancer cells by exploiting overexpressed receptors. However, moderate receptor expression in healthy cells presents challenges with off-tumour toxicity. To address this, they synthesised a panel of aptamer-functionalised silica-

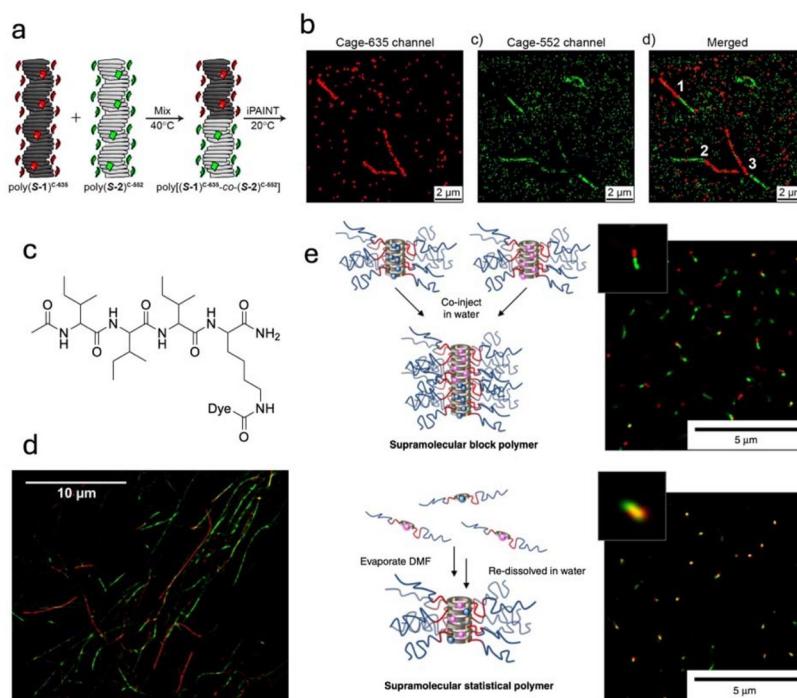


Fig. 3 (a) Schematic representation of copolymerised BTA-based supramolecular polymers, (b) iPANT imaging of the resulting copolymer in channels for Cage-635, Cage-552, and merged (left to right, respectively), (c) Chemical structure and (d) STORM image of self-assembling peptide-dye conjugates that form nanofibers. (e) Schematic representation and STORM images of metastable supramolecular peptide-dye conjugated nanotubes.



supported lipid bilayers (SSLB) to investigate the interplay of valency, aptamer affinity, and epidermal growth factor receptor (EGFR) density on targeting specificity and selectivity.¹²⁰ The study revealed that combining high-affinity aptamers with low-valency SSLBs enhanced selectivity for high-density EGFR cells while minimising accumulation in non-tumour tissues, marking a step forward in the rational design of cancer nanotherapeutics.

Recent advancements in the field highlight the powerful combination of techniques like correlative light and electron microscopy (CLEM) to study nanoparticle (NP) behaviour. By integrating STORM and TEM, this method enables precise localisation and quantification of NPs within cellular compartments, providing crucial insights into *endo*-lysosomal trafficking and the impact of treatments, such as chloroquine, on endosomal escape and therapeutic efficacy.¹²¹

Light scattering

Light scattering methods are indispensable for characterising polymer nanoparticles, especially in drug delivery, where understanding their size, morphology, and assembly is critical. Techniques like dynamic light scattering (DLS) and static light scattering (SLS) allow researchers to measure particle size, distribution, and molecular weight in solution, offering a non-invasive way to study these aggregates in conditions mimicking physiological environments.

Such analyses go beyond simply determining size and shape, providing insights into the arrangement of polymer chains within the nanoparticle, a critical factor for drug encapsulation and release. While resolving the exact atomic positions within assemblies is currently beyond reach, advancements in scattering methods are progressively enhancing our ability to probe these intricate structures with greater precision. Importantly, light scattering complements other techniques by enabling scalable and reproducible measurements essential for translating polymer nanoparticles from research to therapeutic applications.

A tutorial review by O'Reilly and coworkers serves as an excellent resource for the practical analysis of self-assembled polymer nanoparticles in solution.¹²² It highlights the use of scattering and microscopic techniques to characterise these materials, offering detailed guidance on evaluating their size, morphology, and molecular arrangement. This review bridges the gap between synthetic advances and reliable analytical methodologies, providing valuable insights for researchers aiming to design precise and functional polymer-based nanostructures. This progress mirrors the natural precision found in biological nanostructures like enzymes and viruses, which serve as inspiration for synthetic analogues. By leveraging light scattering alongside microscopic methods, researchers can achieve a detailed understanding of the self-assembly and functional performance of polymer nanoparticles, ultimately advancing their design for drug delivery and other biomedical applications.

A crucial parameter that must be understood for self-assembled nanomaterials is their critical micelle concentration (CMC). The CMC defines the concentration at which unimers self-assemble to form particles. Upon administration of self-assembled particles *in vivo*, they will undergo a dilution effect, which could cause the particles to disassemble if the concentration decreases below the CMC.¹²³ DLS can be utilised to determine this parameter by measuring the scattering intensity as a function of concentration. Particle formation results in a strong increase in scattering intensity, with the inflection point indicating the CMC.¹²⁴ Several other techniques are available to determine CMC, such as conductivity or surface tension measurements or the encapsulation of a hydrophobic fluorophore.¹²⁵

Small-angle X-ray scattering (SAXS) has proven to be an indispensable tool for monitoring polymerization-induced self-assembly (PISA), offering real-time insights into nanostructure evolution during synthesis.^{126–129} Extensive work by Armes and coworkers highlights the use of SAXS to characterise morphological transitions—such as from spheres to worms to vesicles—while providing detailed metrics like particle size, aggregation number, and inter-chain separation. This method also unveils critical formation mechanisms, such as inward growth in vesicle membranes, enhancing the precision of *in situ* characterisation and deepening our understanding of dynamic self-assembly processes.

Small-angle neutron scattering (SANS) is a powerful technique for studying the structural parameters of self-assembled systems, such as size, morphology, and aggregation number, under varying environmental conditions like pH, temperature, or solvent.¹³⁰ By modelling data with appropriate form factors (e.g., Gaussian coil, comb, or hairy cylinder), SANS provides detailed insights into the architecture of conjugated polymer systems, distinguishing between non-assembled and self-assembled species. This approach enables accurate characterisation of supramolecular structures, advancing understanding of their dynamic behaviours in different environments.

Asymmetric flow field-flow fractionation (AF4) has emerged as an exciting characterisation technique for polymeric nanoparticles, offering unique insights into their size, composition, and behaviour under dynamic conditions. By employing multiple detectors, such as refractive index (RI), multi-angle light scattering (MALS), UV, and fluorescence, AF4 provides a comprehensive analysis of self-assembled structures. The technique uses a gentle cross-flow and diffusion to separate polymers, proteins, and nanostructures based on size, enabling the characterisation of self-assembled systems held together by dynamic non-covalent interactions, which are commonly found in polymeric nanoparticles used for drug delivery.

Kariuki *et al.* used AF4 in combination with small-angle neutron scattering (SANS) to analyse cyclic peptide-polymer conjugates, revealing the delicate balance between hydrophobic and hydrophilic forces in nanotube stability and elongation.¹³¹ Similarly, Louie and coworkers demonstrated the power of AF4 with fluorescence detection (AF4-FLD) in studying drug release profiles from PLGA nanoparticles,



showing its superiority over dialysis by resolving temperature-dependent behaviours and enabling size-resolved release profiles.¹³² However, AF4's advantages come with caveats. Significant method optimisation is required, posing a barrier to entry for less-experienced users, and the resulting separation methods may only partially replicate realistic cellular conditions. Furthermore, even with gentle cross-flow, there is a risk of disassembly, particularly in concentration-dependent systems prone to dynamic changes upon dilution. Despite these challenges, AF4 remains a versatile and invaluable technique for advancing our understanding of polymer nanoparticles in drug delivery.

Several of the methods above allow us to obtain particle size distributions. We can use nanoparticle image analysis, which involves acquiring images using TEM, SEM, and AFM to study their size, shape, and distribution. Image processing methods such as contrast enhancement, noise reduction, thresholding, and edge detection help in segmentation and analysis. Quantitative measurements include size distribution, shape analysis, and aggregation detection. Software tools like ImageJ, MATLAB, and Python (OpenCV) are commonly used for automated processing. Alternatively, solution-phase particle analysis methods, like many of the scattering techniques (DLS, SLS, SAXS, SANS), may not necessarily provide particle distribution analyses but important allow us to calculate the average molecular weights and particle sizes in solution. One of the most powerful methods is AF4, as this method will enable us to obtain size and distribution data. However, as mentioned above, the is a highly specialised instrument, not as commonly used or found in most labs, and often requires significant method development before discernible data is obtained.

In summary, materials characterisation plays a crucial role in drug delivery applications by ensuring the proper design and functionality of nanoparticles. Techniques such as electron microscopy, spectroscopy, and porosity measurements allow researchers to assess key properties like size, surface morphology, drug loading capacity, and release profiles. The importance of a diverse range of characterisation methods lies in building a deeper understanding of nanoparticle behaviour, with the power of complementary data helping to validate findings and provide a stronger, more comprehensive picture. Accurate characterisation enables the optimisation of nanoparticle formulations for enhanced stability, biocompatibility, and controlled drug release. By understanding the material's behaviour at the molecular and nanoscale level, researchers can design more effective and targeted drug delivery systems.

Process analytical technologies for polymer nanoparticle drug delivery system manufacture

The characterisation techniques laid out above highlight critical examples to fully assess the properties of polymer nanoparticle drug delivery systems during the discovery research and development phase. However, analytical tools are also heavily integrated with the manufacturing process of modern pharmaceuticals, typically integrated as process analytical

technologies (PATs).¹³³ The goal of PATs is to promote real-time analysis of the critical quality attributes (CQAs) and relate this to the critical process parameters (CPPs) which control said CQAs.¹³⁴ In principle, this can be integrated with quality-by-design risk matrices where analytical feedback loops can adjust the manufacturing process based on the reported quality attributes at each stage of the manufacturing process to ensure the CQA threshold levels are met for batch release.¹³⁵

PATs can be integrated in several different ways depending on the amount of time it takes to receive feedback on the manufacturing process. In the context of polymeric nanomedicines, most of the characterisation techniques described above can be integrated as PATs during various phases of manufacture, polymer synthesis, drug conjugation or the drug formulation stage either online (within the manufacturing path), offline or at-line. Light scattering and spectroscopic techniques (e.g. UV-Vis, fluorescence, Raman) can be easily integrated online with direct feedback of particle size and chemical fingerprints in real-time.^{136,137} In contrast, benchtop techniques such as SEC, NMR, mass spectrometry, imaging techniques, and AF4 can, in principle, be integrated at-line. At the same time, SAXS and SANS, which commonly require specialist facilities, would be fully offline.

As there are no approved polymer nanoparticle drug delivery systems, polymer characterisation PAT approaches would likely be inspired by polymer-conjugate therapies (e.g. PegIntron and Plegridy). On the other hand, nanoparticle characterisation approaches could utilise technologies from approved Adeno-associated virus (AAV) gene therapies (e.g. Luxturna)¹³⁸ or the approved lipid nanoparticle drugs and vaccines (e.g. Doxil, Onpattro, Comirnaty and SpikeVax).¹³⁹ Understanding how these characterisation tools may be implemented and integrated with state-of-the-art digital manufacturing tools such as digital twins and building on underlying polymer-self assembly theory is critical for the translation of these new nanomedicines to the clinic.

Current challenges in polymer nanoparticle delivery

Polymer-based nanoparticles hold significant promise as drug delivery vehicles, but several challenges must be addressed to realise their full potential. A key issue is understanding how the properties of polymeric nanoparticles evolve as they circulate through the body. Their size, shape, surface charge, and the presence of targeting moieties can change due to interactions with biological components such as proteins, lipids, and enzymes. These transformations critically influence systemic delivery, biodistribution, circulation stability, and eventual clearance, as highlighted by a review from Mitchell, Peppas and Langer.⁷ Identifying the final properties of nanoparticles upon reaching their cellular target remains a significant gap in current knowledge. However, it is worth noting that the article also includes some therapies that are FDA-approved nanomedicines, and there are also many promising new therapies that utilise nanoparticles that are currently in the clinic.^{9,140}



The pharmaceutical industry's infrastructure is predominantly tailored for small-molecule drugs and conventional delivery systems. Transitioning to polymer-based drug delivery vectors would necessitate significant investment in new technologies, regulatory frameworks, and manufacturing processes. This structural shift presents logistical and economic barriers, delaying the adoption of these advanced systems. Polymer-based nanoparticles often require intricate designs to achieve precise targeting, controlled release, and stability in physiological conditions. However, this increased complexity comes at a higher cost. A critical question remains: do the improvements in efficacy and efficiency justify the added expense of developing and producing these therapies? Balancing innovation with affordability is essential for making these systems scalable and accessible.

Despite their sophisticated designs, polymer nanoparticles face significant challenges in drug delivery efficiency. Some nanoparticles are so stable that, even after successful cellular internalisation, they fail to effectively release their drug cargo, undermining the system's therapeutic efficacy. Conversely, overly unstable nanoparticles may disassemble before reaching their target, losing the benefits of their nanoscale morphology and protective architecture. Premature disassembly compromises their ability to shield the drug or biologic from degradation, reducing their therapeutic potential.

Addressing these challenges requires a multidisciplinary approach, integrating advances in material science/characterisation, pharmacology, and systems biology. By improving our understanding of nanoparticle transformations, rethinking pharmaceutical infrastructure, and balancing complexity with cost, polymer-based drug delivery systems could overcome inefficiencies and unlock their potential as next-generation therapeutics.

Conclusions: future approaches

To unlock the full potential of polymer-based nanoparticles as drug delivery vehicles, a deeper understanding of their self-assembly and disassembly processes within living cells is crucial. Advanced characterisation techniques capable of monitoring these nanoparticles *in situ* are necessary to correlate their dynamic behaviour with drug delivery outcomes directly. Such insights will provide a clearer picture of how nanoparticles interact with complex cellular environments and release their therapeutic payloads effectively.

The challenge lies in the multivariable nature of biological systems. Parameters such as temperature, pH, concentration, molecular crowding, and dynamic cellular processes continually shift, influencing nanoparticle behaviour in ways that are not yet fully understood. Unlike traditional structure-activity relationships, these multivariant systems require sophisticated analytical methods to untangle the interplay between these factors. For instance, changes in ionic composition resulting from gene regulation could alter the local microenvironment

of the nanoparticle, shifting the kinetics of disassembly and ultimately impacting therapeutic efficacy.

The future of polymer nanoparticle drug delivery depends on our ability to model and predict these complex interactions. Multidisciplinary approaches combining advanced imaging, machine learning, and systems biology will be key to uncovering these relationships. By moving beyond traditional frameworks and embracing the complexity of cellular environments, researchers can develop more effective, reliable, and personalised drug delivery systems, paving the way for a new era of precision medicine.

Author contributions

All authors contributed to the preparation, review and editing of this manuscript.

Data availability

No new data were generated or analysed in this mini-review article. All data referenced are publicly available through the repositories listed in the respective studies, with access details provided in the References section.

Conflicts of interest

There are no conflicts to declare.

Acknowledgements

The authors would like to thank Prof. Sébastien Perrier for inspiring them to explore beyond their immediate fields in pursuit of impactful discoveries.

References

- 1 M. E. Napier and J. M. DeSimone, *Polym. Rev.*, 2007, **47**, 321–327.
- 2 W. Zhang, A. Mehta, Z. Tong, L. Esser and N. H. Voelcker, *Adv. Sci.*, 2021, **8**, 2003937.
- 3 S. Ohta, E. Kikuchi, A. Ishijima, T. Azuma, I. Sakuma and T. Ito, *Sci. Rep.*, 2020, **10**, 18220.
- 4 F. Alexis, E. M. Pridgen, R. Langer and O. C. Farokhzad, in *Drug Delivery*, ed. M. Schäfer-Korting, Springer Berlin Heidelberg, 2010, pp. 55–86.
- 5 S. Wang, K. Cheng, K. Chen, C. Xu, P. Ma, G. Dang, Y. Yang, Q. Lei, H. Huang, Y. Yu, Y. Fang, Q. Tang, N. Jiang, H. Miao, F. Liu, X. Zhao and N. Li, *Nano Today*, 2022, **45**, 101512.
- 6 I. Canton and G. Battaglia, *Chem. Soc. Rev.*, 2012, **41**, 2718–2739.



7 M. J. Mitchell, M. M. Billingsley, R. M. Haley, M. E. Wechsler, N. A. Peppas and R. Langer, *Nat. Rev. Drug Discovery*, 2021, **20**, 101–124.

8 A. B. Cook and S. Perrier, *Adv. Funct. Mater.*, 2019, **30**, 1901001.

9 A. C. Anselmo and S. Mitragotri, *Bioeng. Transl. Med.*, 2019, **4**, e10143.

10 M. C. Arno, J. D. Simpson, L. D. Blackman, R. P. Brannigan, K. J. Thurecht and A. P. Dove, *Biomater. Sci.*, 2023, **11**, 908–915.

11 Y. Bae, S. Fukushima, A. Harada and K. Kataoka, *Angew. Chem.*, 2003, **115**, 4788–4791.

12 K. Bunyamin, E. Lars, T. D. Hien, S. B. Johan, B. Cyrille and P. D. Thomas, *Polym. Chem.*, 2013, **5**, 350–355.

13 W. Chen, S. Ji, X. Qian, Y. Zhang, C. Li, W. Wu, F. Wang and X. Jiang, *Polym. Chem.*, 2017, **8**, 2105–2114.

14 R. Dong, Y. Zhou, X. Huang, X. Zhu, Y. Lu and J. Shen, *Adv. Mater.*, 2015, **27**, 498–526.

15 P. Gurnani and S. Perrier, *Prog. Polym. Sci.*, 2020, **102**, 101209.

16 S. Shukla, F. J. Eber, A. S. Nagarajan, N. A. DiFranco, N. Schmidt, A. M. Wen, S. Eiben, R. M. Twyman, C. Wege and N. F. Steinmetz, *Adv. Healthcare Mater.*, 2015, **4**, 874–882.

17 C. Weizhi, J. Shilu, Q. Xiaoping, Z. Yajun, L. Cheng, W. Wei, W. Fei and J. Xiqun, *Polym. Chem.*, 2017, **8**, 2105–2114.

18 J. Yang, X. Yu, J. I. Song, Q. Song, S. C. L. Hall, G. Yu and S. Perrier, *Angew. Chem., Int. Ed.*, 2022, **61**, e202115208.

19 R. Langer, *Science*, 1990, **249**, 1527–1533.

20 R. M. Broyer, G. N. Grover and H. D. Maynard, *Chem. Commun.*, 2011, **47**, 2212–2226.

21 C. F. N. João, K. G. Michelle, A. R. Daniel, O. F. Alexander, S. John, P. Andrew, B. Caroline, J. S. Christopher and C. Vijay, *Chem. Commun.*, 2019, **55**, 7671–7674.

22 Y. Krishnan, H. A. Rees, C. P. Rossitto, S.-E. Kim, H.-H. K. Hung, E. H. Frank, B. D. Olsen, D. R. Liu, P. T. Hammond and A. J. Grodzinsky, *Biomaterials*, 2018, **183**, 218–233.

23 M. B. Rebecca, N. G. Gregory and D. M. Heather, *Chem. Commun.*, 2011, **47**, 2212–2226.

24 I. Cobo, M. Li, B. S. Sumerlin and S. Perrier, *Nat. Mater.*, 2015, **14**, 143–159.

25 P. Cotanda, D. B. Wright, M. Tyler and R. K. O'Reilly, *J. Polym. Sci., Part A: Polym. Chem.*, 2013, **51**, 3333–3338.

26 G. Vancoillie, W. L. A. Brooks, M. A. Mees, B. S. Sumerlin and R. Hoogenboom, *Polym. Chem.*, 2016, **7**, 6725–6734.

27 M. Hartlieb, S. Catrouillet, A. Kuroki, C. Sanchez-Cano, R. Peltier and S. Perrier, *Chem. Sci.*, 2019, **10**, 5476–5483.

28 S. K. Rajendrakumar, K. Cherukula, H. J. Park, S. Uthaman, Y. Y. Jeong, B.-I. Lee and I.-K. Park, *J. Controlled Release*, 2018, **276**, 72–83.

29 D. Roy, J. N. Cambre and B. S. Sumerlin, *Prog. Polym. Sci.*, 2010, **35**, 278–301.

30 D. Roy, J. N. Cambre and B. S. Sumerlin, *Chem. Commun.*, 2009, 2106–2108.

31 M. Amit, S. Yuran, E. Gazit, M. Reches and N. Ashkenasy, *Adv. Mater.*, 2018, **30**, 1707083.

32 M. Dergham, S. Lin and J. Geng, *Angew. Chem., Int. Ed.*, 2022, **61**, e202114267.

33 S. C. Larnaudie, J. C. Brendel, I. Romero-Canelón, C. Sanchez-Cano, S. Catrouillet, J. Sanchis, J. P. C. Coverdale, J.-I. Song, A. Habtemariam, P. J. Sadler, K. A. Jolliffe and S. Perrier, *Biomacromolecules*, 2017, **19**, 239–247.

34 F. Richter, P. Mapfumo, L. Martin, J. I. Solomun, F. Hausig, J. J. Frietsch, T. Ernst, S. Hoepfener, J. C. Brendel and A. Traeger, *J. Nanobiotechnol.*, 2021, **19**, 70.

35 C. Zhu and J. Nicolas, *Biomacromolecules*, 2022, **23**, 3043–3080.

36 R. Kumar, N. Le, F. Oviedo, M. E. Brown and T. M. Reineke, *JACS Au*, 2022, **2**, 428–442.

37 R. Kumar, C. F. Santa Chalarca, M. R. Bockman, C. V. Bruggen, C. J. Grimm, R. J. Dalal, M. G. Hanson, J. K. Hexum and T. M. Reineke, *Chem. Rev.*, 2021, **121**, 11527–11652.

38 S. T. G. Street, J. Chrenek, R. L. Harniman, K. Letwin, J. M. Mantell, U. Borucu, S. M. Willerth and I. Manners, *J. Am. Chem. Soc.*, 2022, **144**, 19799–19812.

39 C. Zylberberg, K. Gaskill, S. Pasley and S. Matosevic, *Gene Ther.*, 2017, **24**, 441–452.

40 N. J. W. Penfold, J. Yeow, C. Boyer and S. P. Armes, *ACS Macro Lett.*, 2019, **8**, 1029–1054.

41 L. Brunsved, B. J. B. Folmer, E. W. Meijer and R. P. Sijbesma, *Chem. Rev.*, 2001, **101**, 4071–4098.

42 M. K. Henk, P. S. Rint and E. W. Meijer, *Eur. J. Org. Chem.*, 2004, 2553–2555, DOI: [10.1002/ejoc.200300752](https://doi.org/10.1002/ejoc.200300752).

43 T. F. A. De Greef, M. M. J. Smulders, M. Wolffs, A. P. H. J. Schenning, R. P. Sijbesma and E. W. Meijer, *Chem. Rev.*, 2009, **109**, 5687–5754.

44 M. R. Ghadiri, J. R. Granja, R. A. Milligan, D. E. McRee and N. Khazanovich, *Nature*, 1993, **366**, 324–327.

45 G. J. t. C. Mattijs and G. B. Hans, *Macromol. Chem. Phys.*, 2007, **208**, 1437–1446.

46 I. W. Hamley, *Angew. Chem., Int. Ed.*, 2014, **53**, 6866–6881.

47 J. Y. Rho and S. b. Perrier, *ACS Macro Lett.*, 2021, **10**, 258–271.

48 M. Inam, G. Cambridge, A. Pitto-Barry, Z. P. L. Laker, N. R. Wilson, R. T. Mathers, A. P. Dove and R. K. O'Reilly, *Chem. Sci.*, 2017, **8**, 4223–4230.

49 L. MacFarlane, C. Zhao, J. Cai, H. Qiu and I. Manners, *Chem. Sci.*, 2021, **12**, 4661–4682.

50 J. Zhang, H. Sun and P. X. Ma, *ACS Nano*, 2010, **4**, 1049–1059.

51 C. Stoffelen and J. Huskens, *Small*, 2016, **12**, 96–119.

52 Q.-D. Hu, G.-P. Tang and P. K. Chu, *Acc. Chem. Res.*, 2014, **47**, 2017–2025.

53 C. A. Stevens, K. Kaur and H.-A. Klok, *Adv. Drug Delivery Rev.*, 2021, **174**, 447–460.



54 P. Gurnani, A. B. Cook, R. A. E. Richardson and S. Perrier, *Polym. Chem.*, 2019, **10**, 1452–1459.

55 P. Gurnani, C. Sanchez-Cano, H. Xandri-Monje, J. Zhang, S. H. Ellacott, E. D. H. Mansfield, M. Hartlieb, R. Dallmann and S. Perrier, *Small*, 2022, **18**, 2203070.

56 R. X. Zhang, T. Ahmed, L. Y. Li, J. Li, A. Z. Abbasi and X. Y. Wu, *Nanoscale*, 2017, **9**, 1334–1355.

57 J. Tang, J. M. Li, G. Li, H. T. Zhang, L. Wang, D. Li and J. S. Ding, *Int. J. Nanomed.*, 2017, **12**, 6687–6704.

58 P. Das and N. R. Jana, *ACS Appl. Polym. Mater.*, 2021, **3**, 4791–4811.

59 R. Ferrari, M. Sponchioni, M. Morbidelli and D. Moscatelli, *Nanoscale*, 2018, **10**, 22701–22719.

60 N. Kamaly, Z. Xiao, P. M. Valencia, A. F. Radovic-Moreno and O. C. Farokhzad, *Chem. Soc. Rev.*, 2012, **41**, 2971–3010.

61 N. M. Amanda and D. H. Jeffrey, *Acc. Chem. Res.*, 2017, **50**, 714–722.

62 Y. Mai and A. Eisenberg, *Chem. Soc. Rev.*, 2012, **41**, 5969–5985.

63 H.-A. Klok and S. Lecommandou, *Adv. Mater.*, 2001, **13**, 1217–1229.

64 A. Rösler, G. W. M. Vandermeulen and H.-A. Klok, *Adv. Drug Delivery Rev.*, 2012, **64**, 270–279.

65 E. D. von Meerwall, *J. Magn. Reson.*, 1982, **50**, 409–416.

66 A. Chen, D. Wu and C. S. Johnson Jr., *J. Am. Chem. Soc.*, 1995, **117**, 7965–7970.

67 N. Cherifi, A. Khoukh, A. Benaboura and L. Billon, *Polym. Chem.*, 2016, **7**, 5249–5257.

68 C. Chamignon, D. Duret, M.-T. Charreyre and A. Favier, *Macromol. Chem. Phys.*, 2016, **217**, 2286–2293.

69 K. Ute, R. Nagao and K. Watanabe, in *NMR Methods for Characterization of Synthetic and Natural Polymers*, ed. R. R. Zhang, T. Miyoshi and P. Sun, The Royal Society of Chemistry, 2019, ch. 5, pp. 80–100.

70 O. Tooley, W. Pointer, R. Radmall, M. Hall, T. Swift, J. Town, C. Aydogan, T. Junkers, P. Wilson, D. Lester and D. Haddleton, *ACS Polym. Au*, 2024, **4**, 311–319.

71 M. Reis, F. Gusev, N. G. Taylor, S. H. Chung, M. D. Verber, Y. Z. Lee, O. Isayev and F. A. Leibfarth, *J. Am. Chem. Soc.*, 2021, **143**, 17677–17689.

72 S. T. Knox, S. Parkinson, R. Stone and N. J. Warren, *Polym. Chem.*, 2019, **10**, 4774–4778.

73 P.-J. Voorter, M. Wagner, C. Rosenauer, J. Dai, P. Subramanian, A. McKay, N. R. Cameron, J. J. Michels and T. Junkers, *Polym. Chem.*, 2023, **14**, 5140–5146.

74 P. J. Voorter, A. McKay, J. Dai, O. Paravagna, N. R. Cameron and T. Junkers, *Angew. Chem., Int. Ed.*, 2021, **61**, e202114536.

75 I. W. F. Silva, A. McKay, A. Sokolova and T. Junkers, *Polym. Chem.*, 2024, **15**, 1303–1309.

76 A. J. Gormley, *J. Controlled Release*, 2024, **373**, 23–30.

77 A. M. Striegel, *Anal. Bioanal. Chem.*, 2008, **390**, 303–305.

78 N. Akhtar, M. B. Ashford, L. Beer, A. Bowes, T. Bristow, A. Broo, D. Buttar, S. Coombes, R. Cross, E. Eriksson, J.-B. Guilbaud, S. W. Holman, L. P. Hughes, M. Jackman, M. J. Lawrence, J. Lee, W. Li, R. Linke, N. Mahmoudi, M. McCormick, B. MacMillan, B. Newling, M. Ngeny, C. Patterson, A. Poulton, A. Ray, N. Sanderson, S. Sonzini, Y. Tang, K. E. Treacher, D. Whittaker and S. Wren, *J. Pharm. Sci.*, 2023, **112**, 844–858.

79 S. Sonzini, F. Caputo, D. Mehn, L. Calzolai, S. E. F. Borgos, A. Hyldbakk, K. Treacher, W. Li, M. Jackman, N. Mahmoudi, M. J. Lawrence, C. Patterson, D. Owen, M. Ashford and N. Akhtar, *Int. J. Pharm.*, 2023, **637**, 122905.

80 J. S. Town, G. R. Jones and D. M. Haddleton, *Polym. Chem.*, 2018, **9**, 4631–4641.

81 K. Ishitsuka, T. Kakiuchi, H. Sato and T. N. J. Fouquet, *Rapid Commun. Mass Spectrom.*, 2020, **34**, e8584.

82 E. Kendrick, *Anal. Chem.*, 1963, **35**, 2146–2154.

83 T. E. Morgan, S. H. Ellacott, C. A. Wootton, M. P. Barrow, A. W. T. Bristow, S. Perrier and P. B. O'Connor, *Anal. Chem.*, 2018, **90**, 11710–11715.

84 T. E. Morgan, T. G. Floyd, B. P. Marzullo, C. A. Wootton, M. P. Barrow, A. W. T. Bristow, S. Perrier and P. B. O'Connor, *Polym. Chem.*, 2022, **13**, 4162–4169.

85 T. E. Morgan, C. A. Wootton, B. Marzullo, J. Paris, A. Kerr, S. H. Ellacott, M. A. van Agthoven, M. P. Barrow, A. W. T. Bristow, S. Perrier and P. B. O'Connor, *J. Am. Soc. Mass Spectrom.*, 2021, **32**, 2153–2161.

86 J. Lawrence, S.-H. Lee, A. Abdilla, M. D. Nothling, J. M. Ren, A. S. Knight, C. Fleischmann, Y. Li, A. S. Abrams, B. V. K. J. Schmidt, M. C. Hawker, L. A. Connal, A. J. McGrath, P. G. Clark, W. R. Gutekunst and C. J. Hawker, *J. Am. Chem. Soc.*, 2016, **138**, 6306–6310.

87 R. Peltier, A. Bialek, A. Kuroki, C. Bray, L. Martin and S. Perrier, *Polym. Chem.*, 2018, **9**, 5511–5520.

88 J. Y. Rho, J. C. Brendel, L. R. MacFarlane, E. D. H. Mansfield, R. Peltier, S. Rogers, M. Hartlieb and S. Perrier, *Adv. Funct. Mater.*, 2018, **28**, 1704569.

89 M. Ghezzi, S. Pescina, C. Padula, P. Santi, E. Del Favero, L. Cantù and S. Nicoli, *J. Controlled Release*, 2021, **332**, 312–336.

90 W. Gibson, J. T. Mulvey, S. Das, S. Selmani, J. G. Merham, A. M. Rakowski, E. Schwartz, A. I. Hochbaum, Z. Guan, J. R. Green and J. P. Patterson, *ACS Nano*, 2024, **18**, 11898–11909.

91 J. Kuntsche, J. C. Horst and H. Bunjes, *Int. J. Pharm.*, 2011, **417**, 120–137.

92 P. Renz, M. Kokkinopoulou, K. Landfester and I. Lieberwirth, *Macromol. Chem. Phys.*, 2016, **217**, 1879–1885.

93 K. H. Nagamanasa, H. Wang and S. Granick, *Adv. Mater.*, 2017, **29**, 1703555.

94 G. Ing, A. Stewart, G. Battaglia and L. Ruiz-Perez, *PLoS One*, 2023, **18**, e0285691.

95 H. Wu, H. Sun, R. A. J. F. Oerlemans, S. Li, J. Shao, J. Wang, R. R. M. Joosten, X. Lou, Y. Luo, H. Zheng, L. K. E. A. Abdelmohsen, H. H. P. Garza, J. C. M. van Hest and H. Friedrich, *Adv. Mater.*, 2024, 2402987.



96 C. I. C. Crucho and M. T. Barros, *Mater. Sci. Eng., C*, 2017, **80**, 771–784.

97 R. L. Harniman, S. Pearce and I. Manners, *J. Am. Chem. Soc.*, 2022, **144**, 951–962.

98 M. A. Touve, C. A. Figg, D. B. Wright, C. Park, J. Cantlon, B. S. Sumerlin and N. C. Gianneschi, *ACS Cent. Sci.*, 2018, **4**, 543–547.

99 G. M. Scheutz, M. A. Touve, A. S. Carlini, J. B. Garrison, K. Gnanasekaran, B. S. Sumerlin and N. C. Gianneschi, *Matter*, 2021, **4**, 722–736.

100 Y. Guo, T. Xia, V. Walter, Y. Xie, J. Y. Rho, L. Xiao, R. O. O'Reilly and M. Wallace, *ChemRxiv*, 2024, DOI: [10.26434/chemrxiv-2024-d1gd3](https://doi.org/10.26434/chemrxiv-2024-d1gd3).

101 T. Xia, Z. Tong, Y. Xie, M. C. Arno, S. Lei, L. Xiao, J. Y. Rho, C. T. J. Ferguson, I. Manners, A. P. Dove and R. K. O'Reilly, *J. Am. Chem. Soc.*, 2023, **145**, 25274–25282.

102 M. Khan, T. R. Guimarães, R. P. Kuchel, G. Moad, S. Perrier and P. B. Zetterlund, *Angew. Chem., Int. Ed.*, 2021, **60**, 23281–23288.

103 K. T. Kim, J. J. L. M. Cornelissen, R. J. M. Nolte and J. C. M. van Hest, *Adv. Mater.*, 2009, **21**, 2787–2791.

104 R. J. R. W. Peters, M. Marguet, S. Marais, M. W. Fraaije, J. C. M. v. Hest and S. Lecommandoux, *Angew. Chem., Int. Ed.*, 2014, **53**, 146–150.

105 D. D. Lane, F. Y. Su, D. Y. Chiu, S. Srinivasan, J. T. Wilson, D. M. Ratner, P. S. Stayton and A. J. Convertine, *Polym. Chem.*, 2014, **6**, 1255–1266.

106 S. Varlas, R. Keogh, Y. Xie, S. L. Horswell, J. C. Foster and R. K. O'Reilly, *J. Am. Chem. Soc.*, 2019, **141**, 20234–20248.

107 H. Che and J. C. M. van Hest, *ChemNanoMat*, 2019, **5**, 1092–1109.

108 C. G. Palivan, L. Heuberger, J. Gaitzsch, B. Voit, D. Appelhans, B. B. Fernandes, G. Battaglia, J. Du, L. Abdelmohsen, J. C. M. van Hest, J. Hu, S. Liu, Z. Zhong, H. Sun, A. Mutschler and S. Lecommandoux, *Biomacromolecules*, 2024, **25**, 5454–5467.

109 A. Reisch and A. S. Klymchenko, *Small*, 2016, **12**, 1968–1992.

110 K. Li, W. Qin, D. Ding, N. Tomczak, J. Geng, R. Liu, J. Liu, X. Zhang, H. Liu, B. Liu and B. Z. Tang, *Sci. Rep.*, 2013, **3**, 1150.

111 W. Li, G. S. Kaminski Schierle, B. Lei, Y. Liu and C. F. Kaminski, *Chem. Rev.*, 2022, **122**, 12495–12543.

112 L. Albertazzi, D. van der Zwaag, C. M. A. Leenders, R. Fitzner, R. W. van der Hofstad and E. W. Meijer, *Science*, 2014, **344**, 491–495.

113 L. Albertazzi, D. v. d. Zwaag, C. M. A. Leenders, R. Fitzner, R. W. v. d. Hofstad and E. W. Meijer, *Science*, 2014, **344**, 491–495.

114 M. H. Bakker, C. C. Lee, E. W. Meijer, P. Y. W. Dankers and L. Albertazzi, *ACS Nano*, 2016, **10**, 1845–1852.

115 R. M. P. da Silva, D. van der Zwaag, L. Albertazzi, S. S. Lee, E. W. Meijer and S. I. Stupp, *Nat. Commun.*, 2016, **7**, 11561.

116 M. Kumar, J. Son, R. H. Huang, D. Sementa, M. Lee, S. O'Brien and R. V. Ulijn, *ACS Nano*, 2020, **14**, 15056–15063.

117 R. Riera, E. Archontakis, G. Cremers, T. de Greef, P. Zijlstra and L. Albertazzi, *ACS Sens.*, 2023, **8**, 80–93.

118 M. M. E. Tholen, B. J. H. M. Rosier, R. T. Vermathen, C. A. N. Sewnath, C. Storm, L. Woythe, C. Izquierdo-Lozano, R. Riera, M. van Egmond, M. Merkx and L. Albertazzi, *ACS Nano*, 2023, **17**, 11665–11678.

119 M. M. E. Tholen, R. P. Tas, Y. Wang and L. Albertazzi, *Chem. Commun.*, 2023, **59**, 8332–8342.

120 L. Woythe, D. Porciani, T. Harzing, S. van Veen, D. H. Burke and L. Albertazzi, *J. Controlled Release*, 2023, **355**, 228–237.

121 T. Andrian, Y. Muela, L. Delgado, L. Albertazzi and S. Pujals, *Nanoscale*, 2023, **15**, 14615–14627.

122 J. P. Patterson, M. P. Robin, C. Chassenieux, O. Colombani and R. K. O'Reilly, *Chem. Soc. Rev.*, 2014, **43**, 2412–2425.

123 S. C. Owen, D. P. Y. Chan and M. S. Shoichet, *Nano Today*, 2012, **7**, 53–65.

124 Q. Yu, R. M. England, A. Gunnarsson, R. Luxenhofer, K. Treacher and M. B. Ashford, *Macromolecules*, 2022, **55**, 401–412.

125 R. Wu, M. Tian, C. Shu, C. Zhou and W. Guan, *Soft Matter*, 2022, **18**, 8920–8930.

126 E. E. Brotherton, F. L. Hatton, A. A. Cockram, M. J. Derry, A. Czajka, E. J. Cornel, P. D. Topham, O. O. Mykhaylyk and S. P. Armes, *J. Am. Chem. Soc.*, 2019, **141**, 13664–13675.

127 M. J. Derry, L. A. Fielding, N. J. Warren, C. J. Mable, A. J. Smith, O. O. Mykhaylyk and S. P. Armes, *Chem. Sci.*, 2016, **7**, 5078–5090.

128 R. Takahashi, S. Miwa, F. H. Sobotta, J. H. Lee, S. Fujii, N. Ohta, J. C. Brendel and K. Sakurai, *Polym. Chem.*, 2020, **11**, 1514–1524.

129 S. K. Filippov, J. M. Franklin, P. V. Konarev, P. Chyttil, T. Etrych, A. Bogomolova, M. Dyakonova, C. M. Papadakis, A. Radulescu, K. Ulbrich, P. Stepanek and D. I. Svergun, *Biomacromolecules*, 2013, **14**, 4061–4070.

130 E. D. H. Mansfield, M. Hartlieb, S. Catrouillet, J. Y. Rho, S. C. Larnaudie, S. E. Rogers, J. Sanchis, J. C. Brendel and S. Perrier, *Soft Matter*, 2018, **14**, 6320–6326.

131 M. Kariuki, J. Y. Rho, S. C. L. Hall and S. Perrier, *Macromolecules*, 2023, **56**, 6618–6632.

132 H. Wu, A. Homawoo, S. Shariati, C. E. Astete, D. F. Rodrigues, C. M. Sabliov, E. H. Fini and S. M. Louie, *RSC Pharm.*, 2024, **1**, 994–1007.

133 G. Gerzon, Y. Sheng and M. Kirkitadze, *J. Pharm. Biomed. Anal.*, 2022, **207**, 114379.

134 N. Aguiam, L. I. F. Moura, M. Oliveira, H. Florindo and J. A. Lopes, in *Artificial Intelligence for Drug Product Lifecycle Applications*, ed. A. Pais, C. Vitorino, S. Nunes and T. Cova, Academic Press, 2025, pp. 169–203.

135 S. Cunha, C. P. Costa, J. N. Moreira, J. M. Sousa Lobo and A. C. Silva, *Nanomed.: Nanotechnol. Biol. Med.*, 2020, **28**, 102206.



136 X. Feng, G. Huang, J. Qiu, L. Peng, K. Luo, D. Liu and P. Han, *Opt. Commun.*, 2023, **531**, 129225.

137 G. Gkogkos, L. Panariello, E. Grammenou, M. A. Cornwell, A. Afrashtehpour, A. J. MacRobert, I. P. Parkin and A. Gavriilidis, *Chem. Eng. J.*, 2023, **467**, 143350.

138 T. Dobrowsky, D. Gianni, J. Pieracci and J. Suh, *Curr. Opin. Biomed. Eng.*, 2021, **20**, 100353.

139 Z. Kis, R. Shattock, N. Shah and C. Kontoravdi, *Biotechnol. J.*, 2019, **14**, 1800376.

140 A. C. Anselmo and S. Mitragotri, *Bioeng. Transl. Med.*, 2021, **6**, e10246.

