

Cite this: *Mater. Adv.*, 2025,
6, 1364

Assessing dual drug 9-hydroxymethyl noscapine and telmisartan-loaded stearic acid nanoparticles against (H1299) non-small cell lung cancer and their mechanistic interaction with bovine serum albumin†

Snigdha Singh,^{‡*ab} Shubham Sewariya,^{‡acd} Tanya Goel,^{‡ae} Sagar Panchal,^a
Aarushi Singh,^f Shrikant Kukreti,^a Manisha Tiwari^{id e} and Ramesh Chandra^{id *abde}

Solid lipid nanoparticles are appealing to the scientific community owing to their expedient and versatile nature as systems for drug delivery and therefore are being used to treat a variety of illnesses. With parallel line of thought, herein, we have reported the synthesis and characterisation of dual drug stearic acid-loaded solid lipid nanoparticles and screened their efficacy in non-small cell lung cancer. The desired nanoparticles, namely 9-CH₂OH Nos-Tel-SLNs, were prepared using the solvent diffusion method. TEM and AFM images revealed that the nanoparticles have spherical form with a mean size of 36.6 nm. The nanostructures' zeta potential and hydrodynamic size were found to be −36.23 mV and ~406.8 nm, respectively. From RP-HPLC, the noscapine and telmisartan loaded in the nanoparticles were found to be 1.86% and 1.97% respectively. Additionally, we have probed into the interaction of BSA with the synthesized nanocomposite using UV-visible, fluorescence and CD spectroscopic techniques along with computational techniques, namely molecular docking, molecular dynamic simulations and MM-PBSA/GBSA calculations. From the fluorescence quenching of BSA upon interaction with the SLNs, we deduced that a stable ground-state complex between 9-CH₂OH Nos-Tel-SLN and BSA was formed. Similarly, *in silico* evaluation indicated formation of a stable dual drug complex with BSA with telmisartan being more compatible for binding to the protein. To assess further, we also evaluated the anticancer property of 9-CH₂OH noscapine, telmisartan and 9-CH₂OH Nos-Tel-SLN against H1299 lung cancer cell line using MTT assay and the calculated IC₅₀ of 9-CH₂OH Nos-Tel-SLN was 186 µg mL^{−1}. Overall, based on the promising results in this research, such SLNs could be a promising drug delivery tool and can be crucial in the conversion of potential anticancer drugs to marketed anticancer drugs in the near future.

Received 22nd September 2024,
Accepted 6th January 2025

DOI: 10.1039/d4ma00958d

rsc.li/materials-advances

1. Introduction

Of all cancers, lung cancer is particularly deadly having a high mortality rate worldwide accounting for 1.8 million deaths in 2022.¹ One of the underlying reasons for huge death rates due to lung cancer is ineffective drug delivery to the tumor site. In this regard, solid lipid nanoparticles (SLNs) are a class of colloidal drug carriers which hold immense potential for controlled drug delivery systems.^{2,3} They offer many attractive benefits such as good efficacy, low toxicity, targeted drug delivery, high bioavailability upon oral administration, *etc.*^{4,5} The FDA-approved nano-drug named 'Doxil' is doxorubicin-loaded pegylated liposome used in breast and ovarian cancer treatments.⁶ As documented in the literature, biodegradable lipids like stearic acid, palmitic acid and oleic acid found in nanostructured lipid particles (NLPs) are being extensively used

^a Department of Chemistry, University of Delhi, Delhi-110007, India.E-mail: ssingh3@chemistry.du.ac.in, acbrdu@hotmail.com,
rameshchandragroup@gmail.com^b Institute for Nanomedical Sciences (INMS), University of Delhi, Delhi-110007, India^c School of Pharmacy and Biomedical Sciences, University of Central Lancashire, Preston, UK^d Department of Chemistry, Maharaja Surajmal Brij University, Bharatpur, Rajasthan, India^e Dr B.R. Ambedkar Center for Biomedical Research, University of Delhi, Delhi, India^f Ramjas College, University of Delhi, Delhi-110007, India† Electronic supplementary information (ESI) available. See DOI: <https://doi.org/10.1039/d4ma00958d>

‡ These authors have made equal contribution.

in the delivery of drugs to tumor cells.³ Additionally, fatty acids like stearic acid are approved for human consumption by the US FDA.⁷ Also, NLPs can be bulked up in industries due to their high stability.⁸ Nanoparticle-based drug delivery is advantageous due to the improved circulation times, controlled release, and improved efficacy of nanostructures as drug delivery vehicles.^{9–11} Recently, combination drug delivery, co-delivery of medications in conjunction with nanotechnology, has steadily become a preferred approach in research frontiers of modern drug delivery.^{12,13} Within this concept, at least two drugs having different mechanisms of action and different physiochemical properties can be loaded into a combination delivery system that can synergistically inhibit the proliferation of tumor cells compared to the case with free or individual drugs.^{14,15} Importantly, the combination of two or more drugs into the nanoparticles are amalgamated to achieve maximum therapeutic effect and pharmacokinetic properties of therapeutics.^{16,17} The acquisition of multi-drug resistance against a variety of cancers often requires the combination of two or more drugs that can effectively promote cell death by demonstrating a synergistic effect.^{18,19} Guo and co-workers have reported paclitaxel and 5-demethylnobiletin co-loaded cetuximab NLPs with synergistic effects against lung cancer.²⁰ Recently, nanocarriers for concurrent delivery of tariquidar and docetaxel have been documented by Kim *et al.* for drug resistant breast cancer cells.²¹ Solid lipid nanomaterials are usually composed of solid lipids, active drug molecules and surfactants. Thus, we synthesised 9-hydroxymethyl noscapine and telmisartan-loaded stearic acid solid lipid nanoparticles (9-CH₂OH Nos-Tel SLNs), where the lipid moiety in the nanocomposite is used to significantly enhance drug loading into hydrophobic components of carriers which can improve drug loading and stability and the two drugs were chosen due to their therapeutic potential widely documented in the literature.

Noscapine is a naturally occurring compound that was initially extracted from the opium poppy, *Papaver somniferum*, and is recognized as a marketed cough suppressant.^{22,23} Noscapine is a phthalideisoquinoline alkaloid that is non-addictive and non-narcotic in nature. In recent years, its potential as an anticancer agent has gained attention as a result of its inhibitory effects on various tumors. Previous studies showed that noscapine inhibited the growth of cancer cells *in vitro* against the breast cancer cell lines MCF-7 and MDAMB-231, with IC₅₀ values of 29 μ M and 69 μ M, respectively, after 66 hours of treatment.²⁴ Similarly, for lung cancer cell line A549, it showed an IC₅₀ value of 73 μ M.²⁵ Noscapine's anticancer properties are attributed to its ability to bind with tubulin.²⁶ On the other hand, telmisartan is an angiotensin II receptor inhibitor used as a common clinical antihypertensive agent.^{27,28} Several reports have postulated that angiogenesis is crucial for tumor progression and metastasis.²⁹ Further, studies have reported that angiotensin receptor blockers can restrain the growth of various cancer cells. Moreover, studies suggested that treatment with telmisartan leads to apoptosis and it has antiproliferative activity in prostate and renal cancer cells.^{30,31} Also, anticancer effects of telmisartan on various human melanoma

cell lines have been investigated after 72 hours of treatment, with IC₅₀ values for HTB140, FemX, 518a2, and A375 cell lines being 136.7, 116.6, 51.2, and 54.1 μ M respectively.³²

The synthesized 9-CH₂OH Nos-Tel SLNs were extensively characterised *via* various techniques like FE-SEM, TEM, DLS, FT-IR, AFM, XPS *etc.* Also, noscapine and telmisartan drug content/drug loading in the synthesized nanoparticles were estimated using RP-HPLC.

In addition, we have explored the interaction of 9-CH₂OH Nos-Tel SLNs with bovine serum albumin (BSA) using both computational and spectroscopic approaches as the drug-protein interactions are vital and can provide insights into the drug ADMET profile and overall bioavailability. We were inclined towards albumins because they are the most abundant proteins of the circulating system which are involved in binding and transportation of essential nutrients as well as drugs (both exogenous and endogenous) to cells.³³ BSA is an abundant and important plasma protein found in mammals, and is 76% homologous to human serum albumin (HSA).³⁴ BSA is chosen as the model protein to visualize the possible interaction(s) of nanocomposite and albumins due to its structural homology and its cost-effectiveness. BSA has three homologous domains (I–III), further subdivided into two sub-domains, named A and B.³⁵ The two tryptophan residues in BSA are responsible for its characteristic wavelength in UV light and fluorescence. Trp-134 resides in sub-domain IB on the surface of the protein whereas another Trp-212 residue is positioned in the hydrophobic cavity of sub-domain IIA.³⁶

Lastly, we have assessed the dose-dependent cellular toxicity of 9-CH₂OH Nos-Tel SLNs along with 9-CH₂OH Nos and telmisartan in non-small lung cancer cell line H1299 *via* MTT assay. These SLNs could be an interesting target for nanomedicine(s) and warrant further *in vitro* and *in vivo* assays to gain clinical success in the future.

2. Experimental section

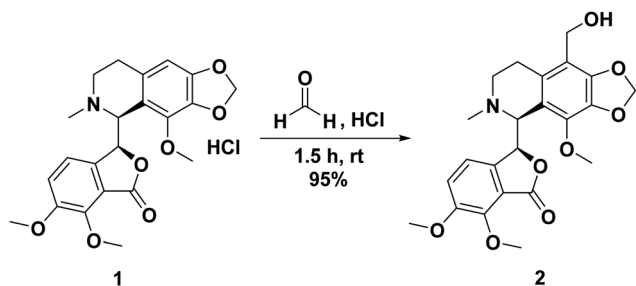
2.1. Materials

Telmisartan (Tel) was procured from TCI, noscapine hydrochloride from Sigma-Aldrich and 9-CH₂OH noscapine was synthesised in the laboratory. Stearic acid (SA) was purchased from Thomas Baker, India and Tween 20 was purchased from Himedia. All the other chemicals procured were of the highest analytical grade. BSA and all other chemicals/reagents were purchased from Sigma-Aldrich, TCI, and Alfa Aesar.

2.2. Synthesis of 9-CH₂OH noscapine

For more than three decades, our team has been diligently engaged in the design and synthesis of noscapinoids, or analogues of noscapine. Noscapine is a 3-substituted phthalide derived pharmacophore that consists of methoxy-containing isoquinoline and benzofuranone rings linked by a C–C chiral bond.³⁷ Over time, the 9'-substituted noscapine analogues have proven to be more effective than other substitutions of the parent compound but selective chemical modification at C-9 is





Scheme 1 Synthesis of 9-hydroxymethyl noscapine (9-CH₂OH Nos).

quite complicated. In this study, '9-hydroxymethyl noscapine' was synthesised using the Blanc reaction wherein noscapine hydrochloride (Scheme 1, **Compound 1**) was treated primarily with paraformaldehyde and HCl. The reaction mixture (RM) was stirred at ambient temperature for 1.5 hours. After confirming the reaction completion using TLC, the RM was quenched using Na₂CO₃. The organic fraction was then extracted using CHCl₃, filtered through dried Na₂SO₄ and the filtrate was concentrated to give crude. The crude was later purified using column chromatography (ethyl acetate/hexane: 30/70) to give the desired product (Scheme 1, **Compound 2**) in 95% yield. The ¹H and ¹³C NMR spectra are given in the ESI.†

2.3. Synthesis of 9-CH₂OH Nos-Tel solid lipid nanoparticles

The 9-hydroxymethyl noscapine telmisartan-loaded nanostructured lipid particles (9-CH₂OH Nos-Tel-SLNs) were prepared using a previously reported solvent diffusion method.^{38,39} Briefly, stearic acid (200 mg), Tween[®] 20, 9-CH₂OH noscapine (30 mg), and telmisartan (30 mg) were dissolved in ethanol and acetone in 1 : 1 ratio. After this, the organic phase was poured into 100 mL of distilled pre-heated water, kept at a temperature of 80 °C. The RM was allowed to stir for 1 hour at the same temperature. Solvent was evaporated under vacuum and then lyophilized to obtain dry product.

2.4. Characterization of nanoparticles

2.4.1. Microscopy. A Thermo Scientific TALOSTEM was utilised to carry out transmission electron microscopy (TEM) to determine the morphology and size of 9-CH₂OH Nos-Tel-SLNs. For the experiment, Cu grids coated with carbon were used. The sample was dispersed in water and then deposited on the grids using the drop-casting method. The software used to calculate the average size of the nanoparticles was ImageJ. For FE-SEM analysis, a Zeiss Gemini SEM 500 thermal field emission type microscope was used. The surface morphology of 9-CH₂OH Nos-Tel-SLNs was visualized using an atomic force microscopy (AFM) instrument, Park Systems, NX10 using AR5T-NCHR probe. The scanning was done in non-tapping mode. The nanoparticles were dispersed in DMSO and then deposited on a glass electrode which was air-dried for 3 hours at 60 °C before analysis.

2.4.2. Zeta potential and particle size. Samples of nanoparticles were dispersed in sterile water at a concentration of 1 mg mL⁻¹ and then sonicated for 5–10 minutes. Then, 1 mL of

this solution was transferred to a quartz cuvette before analysis. Dynamic light scattering, with a Nanoplus particle size analyzer (Particulate Systems), was used to measure the particle size and a Zetasizer Nano-ZS from Malvern Instruments, UK was employed to measure the surface charge of 9-CH₂OH Nos-Tel-SLNs.

2.4.3. Fourier-transform infrared (FT-IR) spectroscopy. A Shimadzu II FT-IR spectrometer was utilized to record the FT-IR spectra of 9-CH₂OH Nos, telmisartan, stearic acid as well as 9-CH₂OH Nos-Tel-SLNs.

2.4.4. X-ray photoelectron spectroscopy (XPS). The surface analysis to measure elemental composition was conducted using a Thermo Fisher Scientific instrument. The total acquisition time for XPS survey was 25.2 s and the source used was Al K alpha. The standard lens mode was used with a spot size of 400 μm.

2.5. Drug loading using RP-HPLC

The drug loading studies were carried out with a RP-HPLC instrument comprising a PDA detector (SPD-M20A, Shimadzu, Japan PDA) and Rheodyne injector with a 20-μL fixed loop. The solvents used were HPLC-grade acetonitrile and water which were sonicated and passed through a 0.45-μm nylon filter before being used. The stock solutions of 9-CH₂OH noscapine and telmisartan were prepared to be 1000 μg mL⁻¹ from which solutions of 50, 100, 150, 200 and 250 μg mL⁻¹ each were prepared for obtaining the calibration curve. The samples of both drugs and of 9-CH₂OH Nos-Tel-SLNs were run using Phenomenex[®] Kinetica, C₁₈ (250 × 4.6 mm, 5 μm particle size) to be the stationary phase and optimized acetonitrile:water (65 : 35%, v/v) to be the mobile phase. The rate of flow was set to 1 mL minute⁻¹, total run time was 8 minutes per sample and effluents were monitored at 254 nm. The following eqn (1) was used to determine drug loading:

$$\text{Drug loading capacity} = \frac{\text{Amount of drug in 9-CH}_2\text{OH Nos-Tel SLNs}}{\text{Amount of 9-CH}_2\text{OH Nos-Tel SLNs}} \times 100 \quad (1)$$

2.6. Binding studies with BSA and 9-CH₂OH Nos-Tel-SLNs

2.6.1. UV-visible spectroscopy. The instrument used for this study was a UV-visible spectrophotometer (Cary 300) from Varian. A BSA solution of 10 μM concentration was prepared in PBS (pH ~ 7.4), and a stock solution of 9-CH₂OH Nos-Tel-SLNs of 1 mg mL⁻¹ in sterile water was prepared for injection. The absorption spectrum of pure BSA was recorded and then subsequently changes in the BSA absorption spectrum were studied while adding increasing amounts of 9-CH₂OH Nos-Tel-SLNs (12.5–125 μg mL⁻¹). The experiment was performed using 1 × PBS (10 mM) as a reference solution and the spectra were collected over the wavelength range of 200 nm to 400 nm.

2.6.2. Steady-state fluorescence spectroscopy. A Hitachi F-7000 fluorescence spectrophotometer was used for these investigations. The measured spectra ranged in wavelength from 200 to 500 nm while exciting the samples at 280 nm. During the experiment, the scan rate was fixed at 2400 nm min⁻¹ with emission slit width and excitation slit width at 5 nm. We



recorded a spectrum of pure BSA (10 μM) solution at 298 K and then later titrated it with gradually increasing volumes of stock solutions of 9-CH₂OH Nos-Tel-SLNs (12.5–87.5 $\mu\text{g mL}^{-1}$). During fluorescence experiments, we needed to account for the self-quenching effect in typical fluorophores (like BSA) only when the concentration is greater than 10 μM and the path length is 1 cm. Herein, we are using an optimized 10 μM concentration of BSA and do not need to focus on self-quenching of the fluorophore.⁴⁰ For appropriate evaluation of the data, we accounted for the inner filter effect and corrected for it by using eqn (2):

$$F_{\text{corrected}} = F_{\text{observed}} \cdot e^{(A_{\text{ex}} + A_{\text{em}})/2} \quad (2)$$

In equation (2), $F_{\text{corrected}}$ denotes the fluorescence upon correction after considering the inner filter effect; F_{observed} is the fluorescence that was observed for the protein (BSA); A_{ex} is the absorption of the ligand (9-CH₂OH Nos-Tel SLNs) at the excitation wavelength and A_{em} is the absorption of the ligand at the emission wavelength.

Consequent upon obtaining proper emission data, we utilized them to produce a Stern–Volmer plot by noting down the changes in fluorescence intensities and then constructed a double-logarithmic plot (modified Stern–Volmer plot).

2.6.3. Circular dichroism (CD) spectroscopy measurement.

This experiment was conducted with a JASCO J-810 CD spectrophotometer using 1 μM BSA solution at 298 K and a pH of 7.4. We recorded all the spectra from 190 nm to 250 nm at a fixed scan rate of 100 nm min^{−1} under continuous nitrogen flush. We used a quartz cuvette with a 1-cm path length for the experiment. The CD spectra of BSA with and without the presence of 9-CH₂OH Nos-Tel-SLNs were recorded while keeping the concentration of BSA solution constant during addition of different amounts of 9-CH₂OH Nos-Tel-SLNs.

2.7. Computational studies

2.7.1. *In silico* docking and molecular dynamics studies.

Molecular docking was done to visualize the binding poses of the ligands (noscipine and telmisartan) to BSA and to get insights into their binding free energies. The docking was performed using the multi ligand approach⁴¹. To begin with, the 3D crystal structure of BSA (PDB ID: 4OR0) was retrieved from the Protein Data Bank (<https://www.rcsb.org/>) online server directly to Maestro 13.5 (Schrodinger Suite 2023-1).^{42,43} The preparation of protein was done using the in-built protein preparation workflow tab and used default settings but did not delete the ligands as we required the 3D coordinates of the active sites. In this structure there are 4–5 active sites present; thus as a result we have used all the sites and performed docking for the precise and most probable binding sites.⁴⁴ Any missing residue was repaired as it is inbuilt in the preprocess step followed by minimization of all the residues. The structures of drugs telmisartan and noscapiene were drawn and energy minimization step was done with Chem3D 16.0 using the MM2 forcefield and applying a 0.010 RMS gradient. Similarly, the ligand preparation was done using inbuilt module LigPrep using OLPS4 forcefield and used rest settings as

default.^{45,46} Lastly, Glide version 98128 (mmshare version 61128) was used to dock the ligands one by one to all the 5 active sites present on the raw PDB file.^{47–50} Several other tools were also utilized for the visualization and analysis. The final docked ligands were then further used for molecular dynamics (MD) simulation studies using GROMACS-2023.1 with the AMBER99SB-ILDN protein, nucleic AMBER94 forcefield.^{51–56} Antechamber and Acpytype.py were utilized to get the topology of ligands used.⁵⁷ The simulation system was solvated using TIP3P model and then system was neutralised by replacement of the solvent molecules with Na⁺ or Cl[−] as required by the system. The energy was minimized with the MD (Leap-Frog integrator) method followed by 500 000 steps for 1000 ps NVT equilibration at 300 K using V-rescale thermostat and NPT equilibration step at 300 K using Berendsen's pressure coupling algorithm and 1 atm pressure for 500 000 steps for 1000 ps. Lastly, MD simulation was done for a time span of 20 000 ps (20 ns).

2.7.2. Binding free energy calculation with MMPBSA/GBSA.

The final trajectories of the MD simulation were further employed to get the net binding free energy of the system (protein + Nos + Tel). Molecular mechanics Poisson–Boltzmann surface area/generalized-Born surface area (MM-PBSA/GBSA) tools were utilized to get the free energy values of different types of strong or weak interaction of the drugs with the active site.^{58–60} This is one of the most used techniques that allow one to analyse the binding free energy, understand the stability of the structure during MD and measure the role of each individual residue present on the protein by free energy decomposition studies.

In this method, the binding free energy is calculated by using the equations below:

$$\Delta G_{\text{bind}} = \langle G_{\text{COM}} \rangle - \langle G_{\text{REC}} \rangle - \langle G_{\text{LIG}} \rangle \quad (3)$$

$$\langle G_x \rangle = \langle E_{\text{MM}} \rangle + \langle G_{\text{sol}} \rangle - \langle TS \rangle \quad (4)$$

which can also be written as

$$\Delta G_{\text{bind}} = \Delta H - T\Delta S \quad (5)$$

where ΔH is the binding enthalpy and $-T\Delta S$ is the conformational entropy upon binding of drugs with the protein. There are other steps involved but the steps shown above are the most generally used steps to get an idea regarding the output values.

2.8. Cellular experiments

Using the H1299 lung cancer cell line, the cytotoxicity of 9-CH₂OH Nos, telmisartan, and 9-CH₂OH Nos-Tel-SLNs was assessed. The cells were obtained from National Centre for Cell Science (NCCS), Pune, India. H1299 cells were grown in DMEM with 10% FBS along with 5% antibiotic–antimycotic supplement. A stock solution comprising 25 mg mL^{−1} each of 9-CH₂OH Nos, telmisartan, and 9-CH₂OH Nos-Tel-SLNs was prepared in DMSO solvent. A temperature of 37 °C at 5% CO₂ in a CO₂ incubator was set for maintaining the cell lines. After being seeded onto a 96-well plate at a density of 8×10^3 cells per well, the cells were incubated for a day. Following treatment with various drug doses (50, 75, 100, 125, and 150 $\mu\text{g mL}^{-1}$), the cancer cells were cultivated for 48 hours in an incubator.



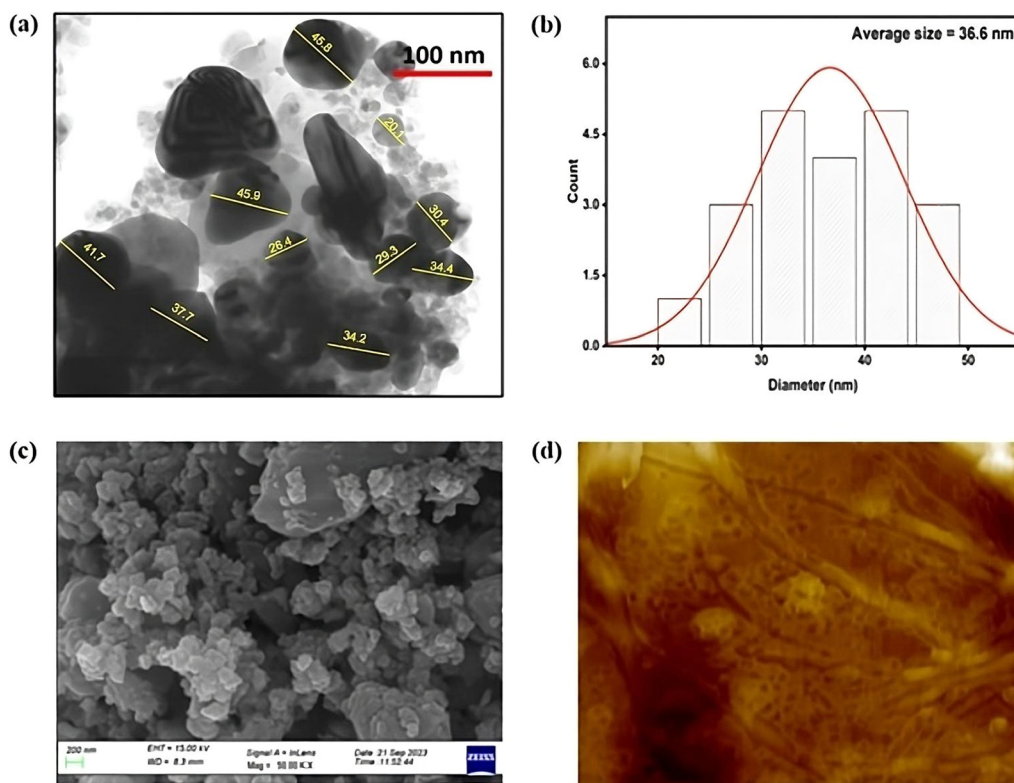


Fig. 1 (a) TEM image at 100 nm; (b) histogram distribution plot depicting size range; (c) FE-SEM image at 200 nm; and (d) AFM image of synthesized 9-CH₂OH Nos-Tel-SLNs.

DMSO-treated cells were used as control. After incubation, 20 μ L of (5 mg mL⁻¹) MTT reagent was added to each well, which was subsequently incubated for another three hours in the CO₂ incubator. The MTT reagent was discarded after the incubation. The formazan crystals formed were dissolved using DMSO (100 μ L). The absorbance was then recorded at 570 nm and reference at 630 nm. The mean \pm SD of quadruplet data of both control and samples was used to represent the final result. To perform statistical comparisons, Student's t-test was utilized. With GraphPad Prism software 8.4.2, the IC₅₀ (inhibitory concentration for 50% cell proliferation) was calculated from graphical plots of the dose-response curve at each concentration.

The following eqn (3) was applied to express the cell viability percentage:

$$\% \text{ Cell Viability} = \frac{\text{OD}(570 - 630)_{\text{treatment}}}{\text{OD}(570 - 630)_{\text{control}}} \times 100\% \quad (6)$$

3. Results and discussion

3.1. Characterization of 9-CH₂OH Nos-Tel-SLNs

3.1.1. Microscopy. The size and morphology of the solid lipid nanoparticle formulation were studied using TEM. First,

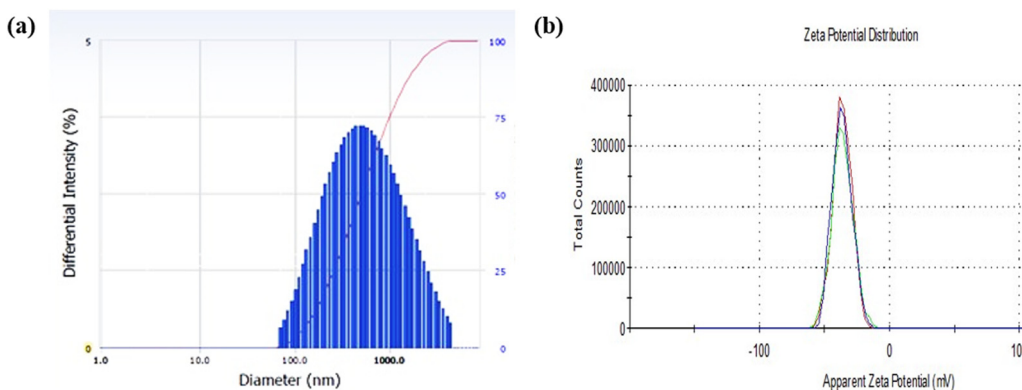


Fig. 2 (a) DLS intensity distribution and (b) zeta potential distribution of synthesized 9-CH₂OH Nos-Tel-SLNs.



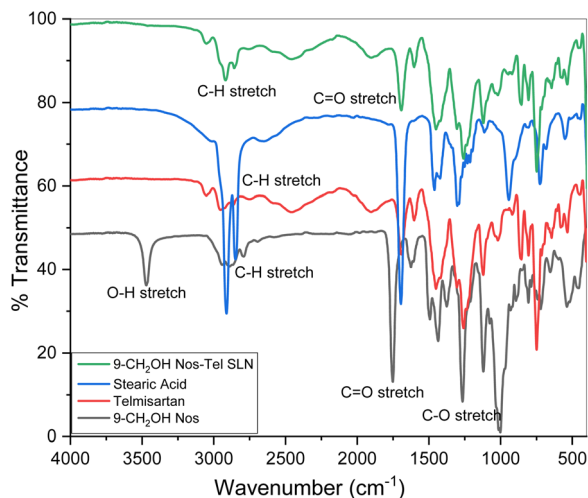


Fig. 3 Comparative FTIR spectra of 9-CH₂OH Nos; telmisartan; stearic acid; and 9-CH₂OH Nos-Tel-SLNs.

1 mg of 9-CH₂OH Nos-Tel SLNs was diluted with sterile water (1 mL) and sonicated for 2 minutes before being placed onto a Cu-r grid coated with carbon. It was then stained with 1% phosphotungstic acid. The sample was dried prior to inspection. In Fig. 1a, the TEM image revealed that the particles were roughly spherical in shape with 36.6 nm as the average size. The nanoparticle size ranged from 20 to 50 nm as seen in the

associated histogram (Fig. 1b). The morphology of the nanoparticles was confirmed using FE-SEM (Fig. 1c). AFM was performed to observe the morphology of the synthesised nanocomposites in more detail. In Fig. 1d, the nanoparticles were seen to be in agglomerated form.

3.1.2. DLS and zeta potential. From this study, we could confirm the formation of 9-CH₂OH Nos-Tel-SLNs as DLS results showed the nanostructure's hydrodynamic size to be ~406.8 nm at 25 °C in sterile water with polydispersity index (PDI) of 0.341 (Fig. 2a). The possible aggregation of 9-CH₂OH Nos-Tel-SLNs in water could be the reason for these values. The difference in the average size of the nanostructures from DLS and TEM analyses might be ascribed to the hydrodynamic diameter with swollen nanostructures in this experiment.^{33,34} The zeta potential came out to be -36.23 mV which might be due to charged groups in both the drugs (Fig. 2b).

3.1.3. FT-IR analysis. The FT-IR stretching frequencies for 9-CH₂OH noscapine, telmisartan, stearic acid as well as 9-CH₂OH Nos-Tel-SLNs have been recorded. The spectrum of 9-CH₂OH Nos exhibited peaks at 3469 cm⁻¹, 2927 cm⁻¹, and 1755 cm⁻¹ representing O-H, aromatic C-H, and C=O stretch respectively. The spectrum of telmisartan exhibited weak bands at 2937 cm⁻¹ (aromatic C-H stretch), 1681 cm⁻¹ (C=O stretching in carboxylic acid), and 1263 cm⁻¹ (C-O stretching in carboxylic acid). The spectrum of stearic acid exhibited peaks at 2926 cm⁻¹ (asymmetric C-H stretch) and 2864 cm⁻¹

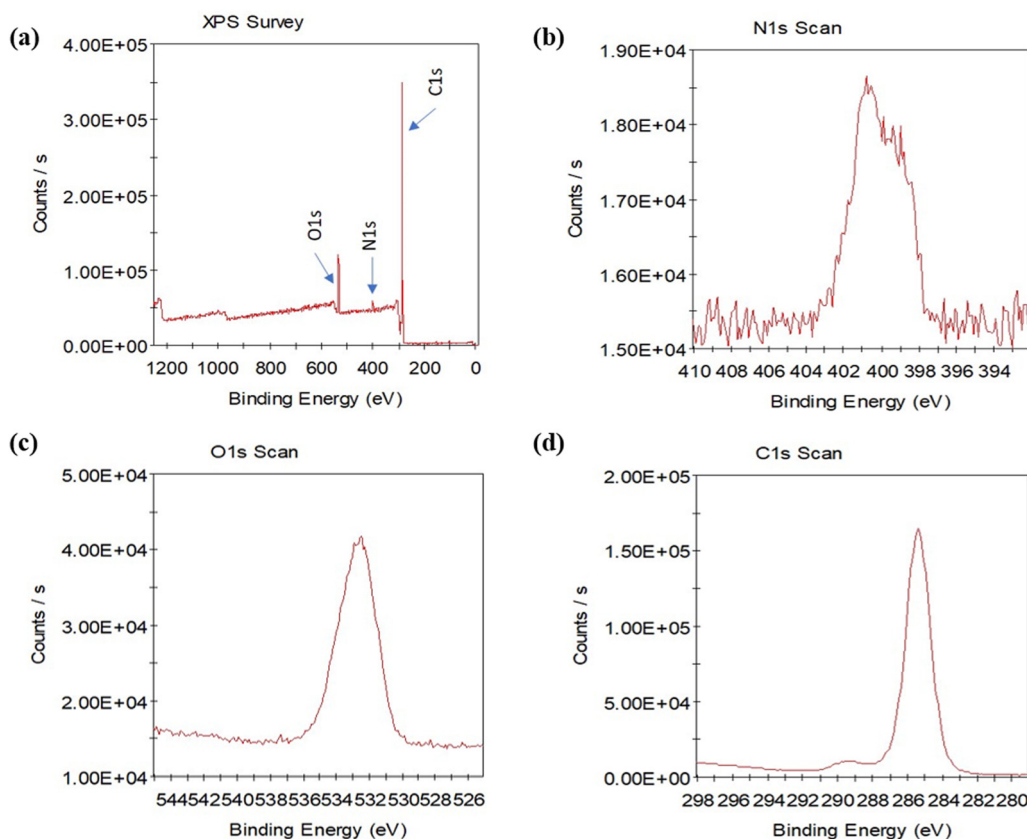


Fig. 4 XPS spectra of 9-CH₂OH Nos-Tel-SLNs: (a) XPS survey spectrum; (b) N 1s scan; (c) O 1s scan; and (d) C 1s scan.



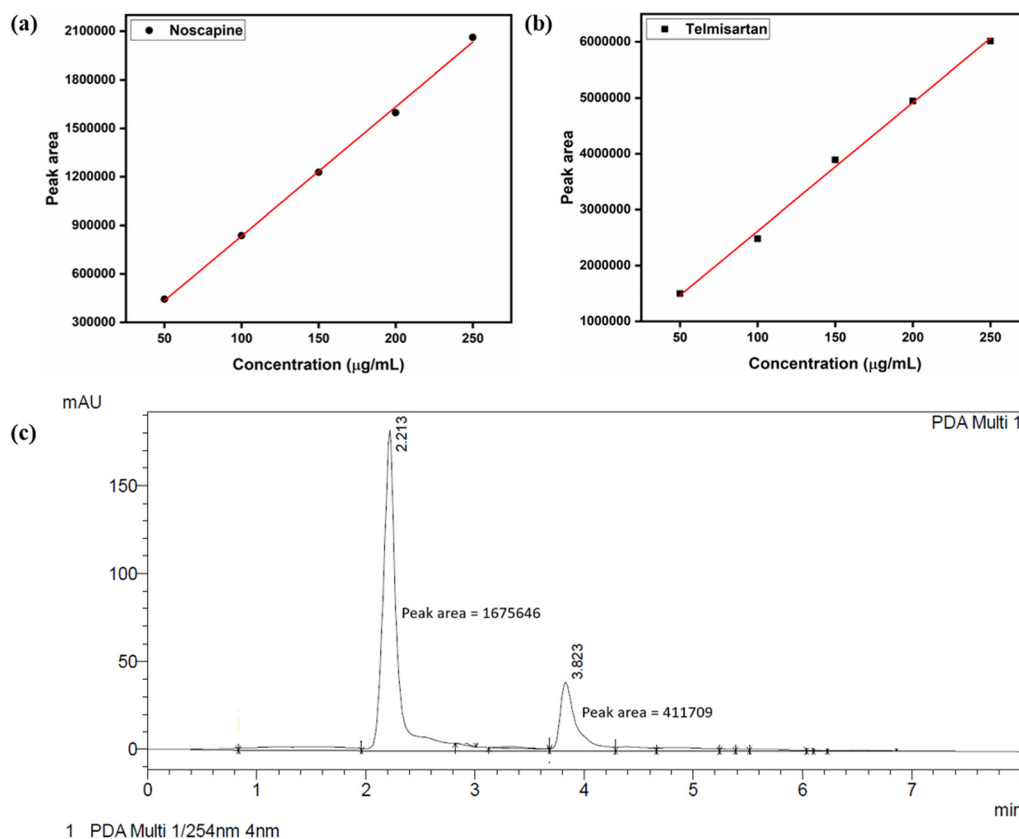


Fig. 5 Calibration curves of (a) 9-CH₂OH noscapine and (b) telmisartan. (c) HPLC chromatogram of 9-CH₂OH Nos-Tel SLNs depicting retention times and peak areas of the two loaded drugs.

(symmetric C-H stretching/methylene CH₂ stretching).³ The 9-CH₂OH Nos-Tel-SLNs spectrum displayed peaks at 3061 cm⁻¹ (aliphatic C-H stretch), 2926 cm⁻¹ and 2864 cm⁻¹ (C-H stretch in CH₃/CH₂ groups), 1697 cm⁻¹ (C=O stretch), and 1251 cm⁻¹ (C-O stretch). The comparative IR spectral analysis indicated that Nos and Tel preserved their characteristics in the lipid matrix (Fig. 3).

3.1.4. X-ray photoelectron spectroscopy (XPS). To determine the chemical state and composition of different elements in the nanocomposite, we have performed XPS analysis. The spectra in Fig. 4 confirm the presence of O, N, and C in the nanocomposite. The sharp peak at 286 eV corresponds to C-C; however, the C spectrum has a broad binding energy peak at 289 eV indicating O-C=O components. The chemical states for C=O and C-O binding energy were observed around 530–536 eV for O 1s. However, for N 1s the binding energy was around 400 eV.⁶¹

3.2. Estimation of 9-CH₂OH noscapine and telmisartan drug loading in 9-CH₂OH Nos Tel SLNs

RP-HPLC is a conventional technique which is used for estimation of loaded drugs content or encapsulation efficiency in nanoparticles. Herein, we used this technique to calculate the drug loading of 9-CH₂OH noscapine as well as telmisartan in the synthesized nanoparticles. The retention times for

telmisartan and 9-CH₂OH noscapine were found to be 2.21 and 3.82 minutes respectively. The obtained calibration curves of 9-CH₂OH noscapine (Fig. 5a) and telmisartan (Fig. 5b) were found to be linear with R² = 0.9986 and 0.9971, respectively, in concentrations ranging from 50 to 250 µg mL⁻¹. The obtained equation for 9-CH₂OH noscapine was Y = 7987.35X – 35 362.7 and that for telmisartan was Y = 22 986.16X + 317 787.9. Using these equations and the peak areas in the chromatogram of the nanoparticles shown in Fig. 5c, the loadings of noscapine and telmisartan were found to be 1.86% and 1.97%, respectively, in 9-CH₂OH Nos-Tel SLNs.

3.3. Biophysical studies

3.3.1. UV-visible spectroscopy. UV-visible absorption spectroscopy is a widely established technique to get an insight into ligand-protein interactions (9-CH₂OH Nos-Tel SLNs and BSA, in our case). It also tells us about the conformational changes in the protein ensuing upon possible complex formation between nanocomposite and protein. The absorption spectrum of BSA^{62,63} has characteristic peaks at 198 nm and 278 nm. The peak at λ_{max} = 198 nm represents the carbonyl group (n to π*) transitions in the backbone of BSA whereas that at λ_{max} = 278 nm corresponds to aromatic amino acid (π to π*) transitions. The absorption spectra of BSA with and without 9-CH₂OH Nos-Tel-SLNs are shown in Fig. 6d. Upon successive



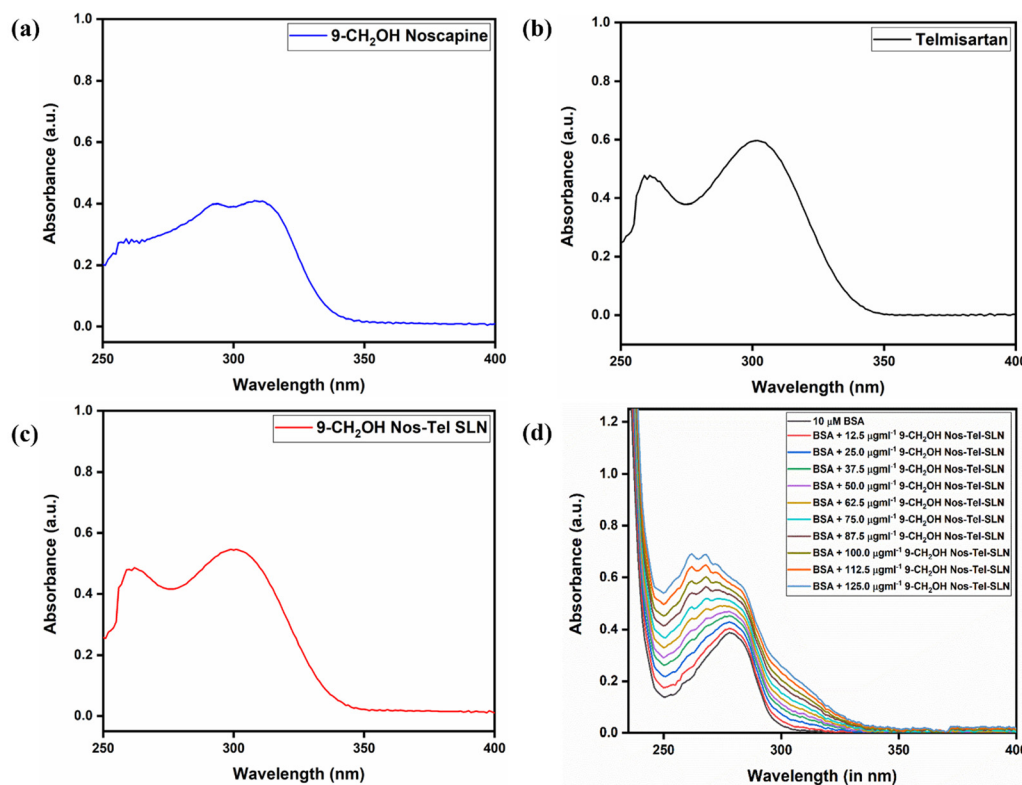


Fig. 6 Absorption spectra of (a) 9-CH₂OH noscapine; (b) telmisartan; (c) 9-CH₂OH Nos-Tel SLNs; and (d) BSA against varying amounts of 9-CH₂OH Nos-Tel SLNs.

addition of 9-CH₂OH Nos-Tel SLNs to BSA, we observed a hyperchromic shift, *i.e.*, enhancement in the peak intensity of BSA suggesting interaction between the nanoparticles and the protein. It can be inferred that due to possible complex formation between nanoparticles and BSA, there are conformational changes in BSA which lead to increased aromatic amino acid exposure in the hydrophobic region.⁶⁴

3.3.2. Steady-state fluorescence spectroscopy. Fluorescence or emission spectroscopy is an effective technique, being utilized to gain a deeper comprehension of ligand-protein interactions and to probe into the mechanism of complex formation between protein (BSA) and nanocomposite.⁶⁵ Proteins like BSA have intrinsic fluorescence due to the presence of aromatic amino acid residues like phenylalanine, tryptophan, and tyrosine.⁶⁶ Amongst these, tryptophan is the most liable to be influenced by any structural changes and thus contributes majorly towards fluorescence quenching of the protein.^{67,68} The fluorescence spectra of BSA with and without 9-CH₂OH Nos-Tel-SLNs are shown in Fig. 7a. In the absence of the nanoparticles, BSA showed maximum emission at 344 nm when excited at 280 nm wavelength.⁶⁹ In line with our absorption spectroscopy results, we noted that there was a decrease in the emission intensity of BSA (fluorescence quenching) due to stepwise addition of 9-CH₂OH Nos-Tel-SLNs along with a bathochromic shift ($\Delta\lambda = 5$ nm). The fluorescence quenching upon addition of the nanoparticles is evidence of the interaction between BSA and 9-CH₂OH Nos-Tel-SLNs.

To assess the nature of the interaction, *i.e.*, static, dynamic or mixed quenching, we utilized the Stern–Volmer eqn (7) mentioned below. Static quenching occurs when a ground-state complex is formed between a drug molecule and protein, whereas dynamic quenching refers to when collisional encounters occur between protein and drug(s). Mixed quenching is an outcome of both collisions and formation of complex between the protein and drug(s) simultaneously.^{70,71} The relations between F_0/F and $[Q]$ in all three cases are given as:

$$\frac{F_0}{F} = 1 + K_{sv}[Q] = K_q\tau_0[Q] \quad (7)$$

$$\frac{F_0}{F} = 1 + K_s[Q] \quad (8)$$

$$\frac{F_0}{F} = (1 + K_D[Q])(1 + K_s[Q]) \quad (9)$$

In the above equations, F_0 is BSA's fluorescence without the nanoparticles; F is BSA's fluorescence with the nanoparticles; $[Q]$ corresponds to the drug's concentration, K_{sv} is the Stern–Volmer constant, K_q is the biomolecular quenching constant, K_s is the association constant, K_D is the dynamic quenching constant and τ_0 ($\sim 10^{-8}$ seconds)⁷² corresponds to the protein's lifetime in the absence of quencher. From the equations, it is clear that a plot of F_0/F against $[Q]$ is a straight line (linear) in the case of static quenching (Fig. 7b, eqn 7) and dynamic quenching (eqn 8) whereas it is non-linear for mixed quenching



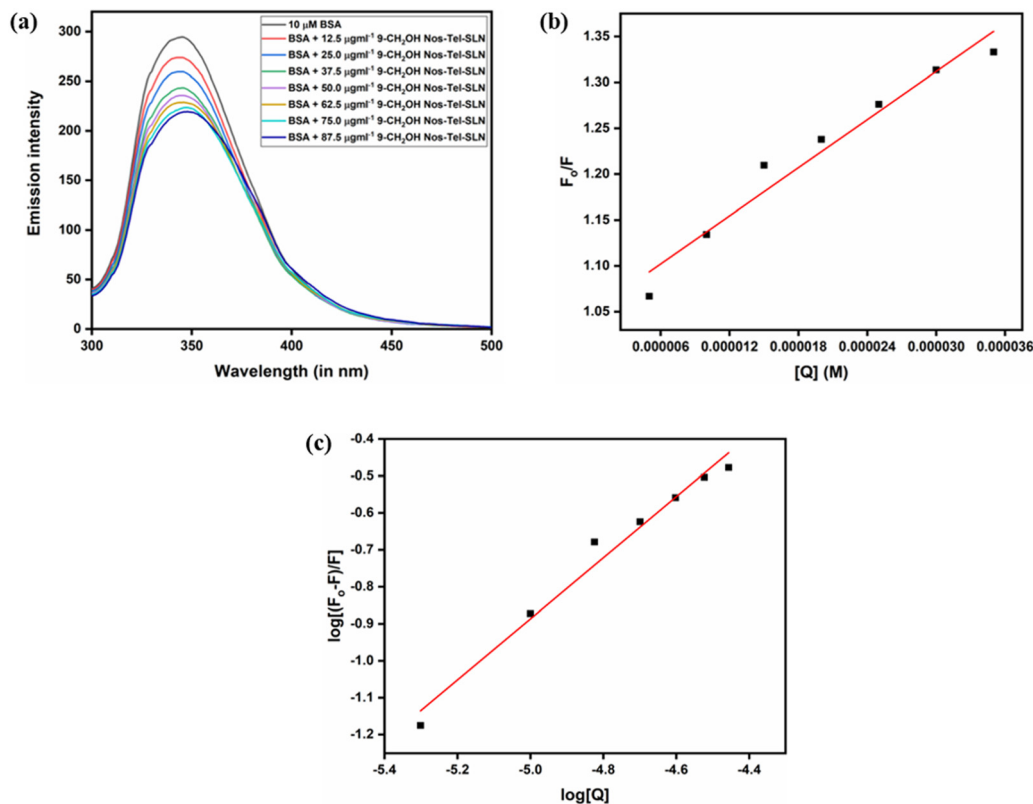


Fig. 7 (a) Fluorescence/emission spectra of BSA against different amounts of 9-CH₂OH Nos-Tel SLNs. (b) Stern–Volmer plot. (c) Modified Stern–Volmer plot.

Table 1 Quenching constants and binding parameters for 9-CH₂OH Nos-Tel SLN binding with BSA

Temperature (K)	$K_{sv} (M^{-1}) \times 10^4$	$K_q (M^{-1} s^{-1}) \times 10^{12}$	$K_b (M^{-1}) \times 10^4$	n
298	0.874	0.874	0.1752	0.82

(eqn 9). In our study, the plot was found to be linear, for which K_{sv} and K_q are mentioned in Table 1. From K_q value of $\sim 0.874 \times 10^{12} M^{-1} s^{-1}$, we concluded that BSA follows the static mode of quenching forming a stable ground-state complex with 9-CH₂OH Nos-Tel SLNs (K_q is of the order of 10^{12} , i.e., higher than $2 \times 10^{10} M^{-1} s^{-1}$ or the maximum scattering collisional quenching constant).⁷³

Furthermore, we used the modified Stern–Volmer equation (Fig. 7c, eqn 10) to measure the binding constant and also the number of binding sites:

$$\log\left(\frac{F_0 - F}{F}\right) = \log K_b + n \log[Q] \quad (10)$$

In the above equation, K_b is the binding constant and n represents the number of binding sites. From Table 1, we can see that 9-CH₂OH Nos-Tel SLN and BSA bind in a 1 : 1 stoichiometric ratio with $0.17 \times 10^4 M^{-1}$ as the value of the binding constant.

3.2.3. Circular dichroism spectroscopy. CD is an important and robust technique used to analyse any changes in the

conformation of a protein upon binding with any ligand/drug.⁷⁴ At 298 K, the spectrum of pure BSA solution exhibits a negative absorption peak at 208 nm due to the $n \rightarrow \pi^*$ transition and another maximum at ~ 222 nm attributed to the $\pi \rightarrow \pi^*$ transition, which are characteristic bands that represent α -helices of BSA.⁷⁵ From Fig. 8, we can see that the intensity of the peaks increased upon adding the nanoparticles to BSA. The secondary structure alterations in the protein were determined *via* BeStSel online server⁷⁶ and the results are shown

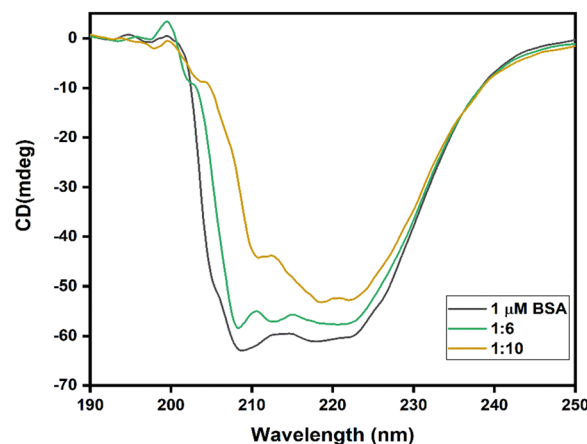


Fig. 8 CD spectra of free BSA and with addition of different molar ratios of BSA:9-CH₂OH Nos-Tel-SLNs (1 : 6 and 1 : 10).



Table 2 Evaluation of secondary structure of BSA

Secondary structure	Details of secondary structure	Percentage content of secondary structure		
		BSA	1 : 6	1 : 10
Helix		24.8	24.6	10.1
Antiparallel	Anti 1 (left-twisted)	0.0	5.9	0.0
	Anti 2 (relaxed)	0.0	0.0	8.0
	Anti 3 (right-twisted)	17.3	12.7	7.3
Parallel		0.1	3.0	17.9
Turns		17.5	17.6	12.2
Others		40.4	36.2	44.5

in Table 2. We determined that the α -helix content in BSA decreased from 24.8% to 10.1% upon binding.

3.4. Computational studies

3.4.1. Molecular docking and MD studies. We performed *in silico* assessments via molecular docking and MD simulation studies to verify our experimental observations and visualize the binding affinity of the drugs (noscipine and telmisartan) in 9-CH₂OH Nos-Tel SLNs and to further investigate the stability of the formed complex. We performed the docking using Glide (an inbuilt module to the Schrodinger Suite 2023-1). As seen, there are 5 active sites present in the PDB file of BSA (PDB ID: 4OR0). We docked the drug one by one to all the active sites and compared the affinity of binding for both drugs on the bases of their respective docking scores. In Table 3, we show the details of all five active sites and the docking values to the corresponding sites. As we can see from Table 3, the best binding scores were found to be at NSP 601 for both drugs.

We noted that the docking score of telmisartan was significantly better relative to that of noscapiene; thus we decided to use the docking score of the best pose for Tel, *i.e.*, $-6.568 \text{ kcal mol}^{-1}$ (best result), and the docking score for Nos, *i.e.*, $-4.506 \text{ kcal mol}^{-1}$ (second-best result), for further simulations. The respective interactions of the system/complex containing both drugs at different sites in BSA are displayed in Fig. 9a. The individual interactions of noscapiene at NSP 603 and telmisartan at NSP 601 are exhibited in Fig. 9b and c. Also, Fig. 9d displays the 2D interactions of both drugs with BSA. The obtained 3D coordinates of the drugs from docking were

Table 3 Docking scores of both drugs (Nos and Tel) at different active sites in BSA

Ligand present on the active site	Drug	Docking score (kcal mol^{-1})	Glide score
NSP 601	Nos	-5.893^a	-6.070
	Tel	-6.568^a	-8.356
NSP 602	Nos	-4.135	-4.937
	Tel	-5.676^b	-5.967
NSP 603	Nos	-4.506^b	-4.683
	Tel	-5.520	-5.810
PEG 604	Nos	-3.096	-3.274
	Tel	-4.458	-6.512
PEG 605	Nos	-3.826	-4.003
	Tel	-3.670	-3.960

^a Best docking score. ^b Second best docking score.

further utilized for molecular dynamics calculations to check the associated conformational changes to the structure of the protein when binding with the two drugs at an atomic level. Gromacs is the most frequently used tool for MD and other computational studies. Here, we did a 20-ns calculation of final complex which we obtained from molecular docking and used different inbuilt modules of Gromacs to analyse the drug and protein interactions at an atomic level. After completion of the calculations, the final trajectories were investigated to obtain the changes in conformation that occurred during simulation.

Using the final trajectories, the root mean square fluctuation (RMSF) and root mean square deviation (RMSD) values were evaluated to get information about the conformational flexibility of the protein structure when both the drugs were bound to it. It is clear from Fig. 10a that the RMSF ranged between 0.1 and 0.4 nm indicating the stabilization of the protein structure during the simulation. From Fig. 10b, we see that the RMSD of Nos bound to BSA was initially stabilized until 9 ns but then momentarily increased to almost 3 nm and then later attained equilibrium with RMSD fluctuating between 2.5 and 3 nm for the remaining span of the simulation. On the other hand, RMSD for Tel bound to BSA was almost constant at around 0.25 nm throughout the simulation (Fig. 10b). This indicated that the binding affinity of Tel to BSA is higher and this interaction was more compatible compared to Nos-BSA binding. To confirm these observations, we further did hydrogen bond numbers analysis (H-bond analysis) of both drugs. From Fig. 10c, we note that the number of H-bonds for Tel-BSA interactions was almost thrice relative to Nos-BSA interactions during the simulation. The average number of H-bonds per time frame for Nos was found to be 1.030 out of 668 347 and for Tel it was 2.806 out of 688 370. This analysis strengthened the earlier compatibility results and at the same time also validated the higher RMSD of Nos-BSA binding.

Lastly, analysis of radius of gyration (R_g) was done to get information about overall dimensions of the protein. In Fig. 10d, we can clearly see that the protein stability persisted throughout the simulation along with both the drugs. In the case of Tel, the value was a little higher than that for Nos which can be due to the overall large size of the drug. The large drug interactions resulted in slight loosening of the compactness or slight increase in flexibility of the secondary structure of BSA.

3.4.2. MM-PBSA/GBSA calculations. Poisson-Boltzmann surface area (PBSA) and generalized Born surface area (GBSA) is a conventional computational tool based on molecular mechanics which is used for calculation of binding free energy of a complex formed during simulation. The trajectories obtained from the MD simulation were required to perform these calculations. The results of these calculations, *i.e.*, the details of different energy components and their respective values, are given in Table 4 for PBSA and Table 5 for GBSA. In docking followed by simulations, we already noted that Tel binding is better with BSA compared to that of No. Here, a similar trend was followed as the net ΔG_{bind} for Tel-BSA binding showed significantly higher values of $-43.7 \text{ kcal mol}^{-1}$ (MM-PBSA analysis; Table 4) and $-59.97 \text{ kcal mol}^{-1}$ (MM-GBSA



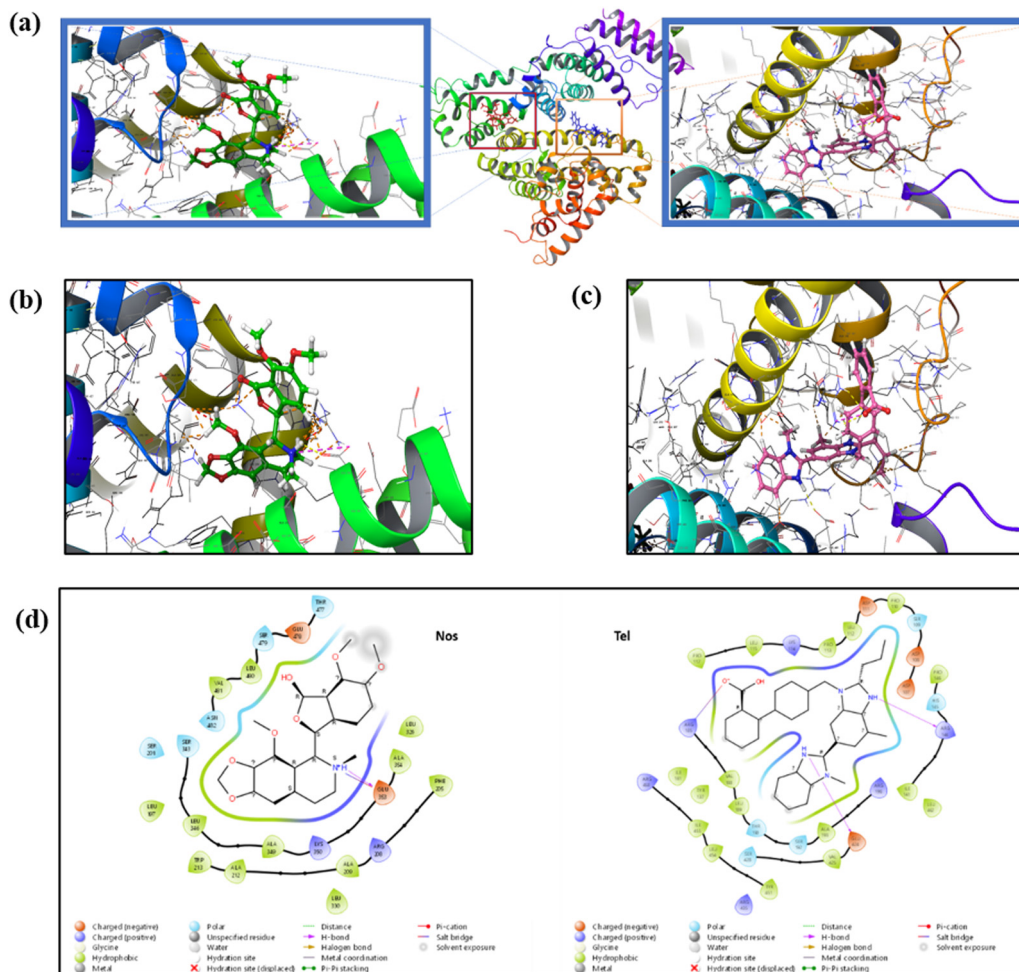


Fig. 9 (a) Final complex of Nos and Tel with BSA. (b) 3D interaction pose of Nos with BSA at NSP 603. (c) 3D interaction pose of Tel with BSA at NSP 601. (d) 2D interaction poses of both the drugs with BSA.

analysis; Table 5). The net negative change in binding free energy (ΔG_{bind}) indicated the formation of a stable complex when both the drugs are bound to the protein.

3.5. *In vitro* cytotoxicity assay

The cytotoxicity of 9-CH₂OH Nos, telmisartan and 9-CH₂OH Nos-Tel-SLNs to lung cancer cells was screened by using the 3-(4,5-dimethylthiazol-2-yl)-2,5-diphenyltetrazolium bromide (MTT) cell proliferation assay. We analyzed the reduction of MTT reagent by metabolically active cells to its insoluble formazan crystal form. Dimethyl sulfoxide (DMSO) was employed to dissolve the formazan crystals that form during the process. When dissolved in an appropriate solvent, they become purple in colour. The intensity of the colour can be measured spectrophotometrically and this yields a proportionate relationship with the number of live cells. The cytotoxic effects of 9-CH₂OH Nos, telmisartan and 9-CH₂OH Nos-Tel-SLNs at 50, 75, 100, 125, and 150 $\mu\text{g mL}^{-1}$ were assessed *in vitro* and the IC₅₀ values were determined to be 282.5, 155.7, and 186 $\mu\text{g mL}^{-1}$, respectively, after 48 h of treatment. The concentration-dependent cytotoxicity profiles of all compounds can be seen in Fig. 11. 9-CH₂OH Nos-Tel-SLNs were successfully

able to deliver drugs into the lung cells substantially inhibiting the proliferation of H1299 cancer cells as shown in Fig. 12. Based on *in vitro* experiments, the combination of 9-CH₂OH Nos and telmisartan in 9-CH₂OH Nos-Tel SLNs demonstrates a positive effect. The combination approach enhances the therapeutic potential by allowing the use of lower doses of each drug, potentially minimizing the side effects associated with high doses of a single drug. Telmisartan alone exhibits higher cytotoxicity at high doses, which could also be influenced by experimental conditions, such as differences in bioavailability or delivery in the assay. Overall, the nanoparticle formulation provides a controlled and sustained release of both drugs, which is advantageous for long-term therapeutic strategies.^{77,78}

4. Conclusion

In the present era of evolving nanotechnology, solid lipid nanoparticles are being explored for their uses in drug delivery and clinical medicine. Also, dual-drug systems, also known as combinatorial systems, for drug delivery offer a viable way to combat drug resistance by simultaneously delivering two or



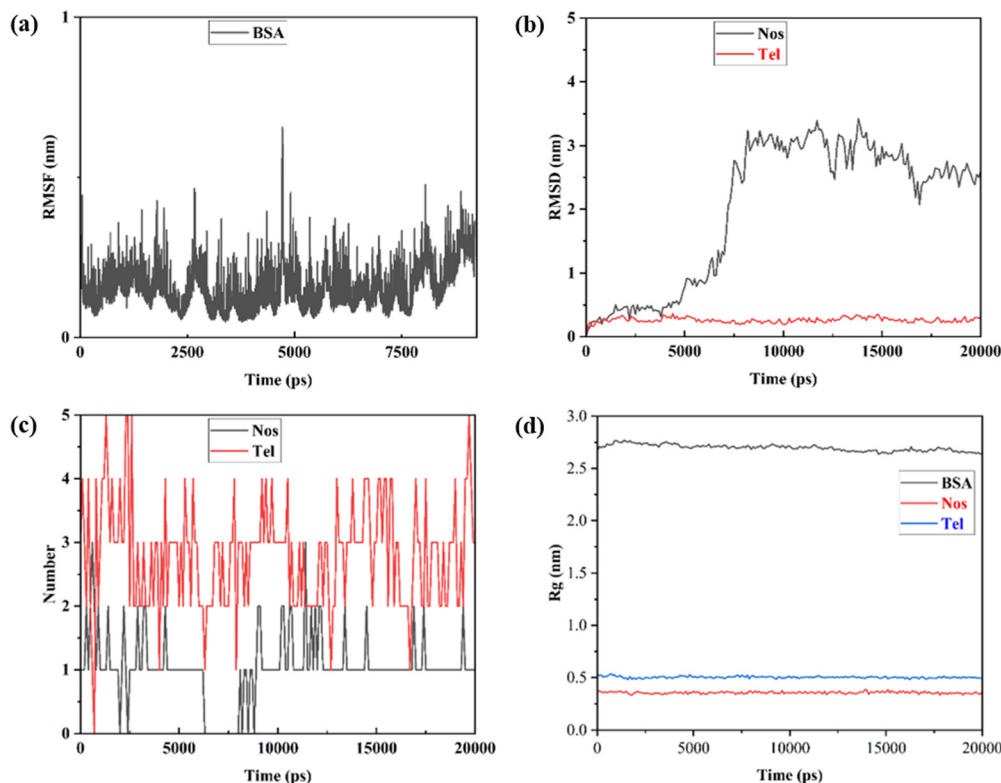


Fig. 10 (a) RMSF analysis of BSA. (b) RMSD analysis of BSA when both drugs are bound to it. (c) Hydrogen bond analysis of Nos and Tel with BSA. (d) Radius of gyration (R_g) analysis.

Table 4 Poisson Boltzmann surface area analysis of Tel and Nos with BSA

Energy component	Telmisartan				Noscapine			
	Complex ^a	Protein ^a	Drug ^a	ΔG_{bind}^a (complex - (protein + drug))	Complex ^a	Protein ^a	Drug ^a	ΔG_{bind}^a (complex - (protein + drug))
BOND	1766.89	1751.71	15.18	0	1765.44	1751.71	13.74	0
ANGLE	4739.5	4683.72	55.78	0	4723.82	4683.72	40.1	0
DIHED	6176.91	6149.75	27.15	0	6176.66	6149.78	26.88	0
VDWAALS	-4821.63	-4745.3	-9.04	-67.29	-4769.97	-4745.3	-7.06	-17.61
EEL	-43 391.4	-43 339.5	-12.89	-38.96	-43 557.3	-43 339.5	7.69	-225.46
1-4 VDW	2190.43	2177.01	13.42	0	2185.83	2177.02	8.81	0
1-4 EEL	27 683.46	27 681.1	2.36	0	27 734.01	27 681.12	52.89	0
EPB	-8783.21	-8753.49	-98.63	68.91	-8587.44	-8753.56	-61.92	228.04
ENPOLAR	142.96	145	4.31	-6.35	146.07	145	3.05	-1.98
EDISPER	0	0	0	0	0	0	0	0
GGAS	-5655.81	-5641.52	91.96	-106.26	-5741.51	-5641.49	143.05	-243.07
GSOLV	-8640.25	-8608.48	-94.32	62.56	-8441.36	-8608.56	-58.87	226.06
TOTAL	-14 296.1	-14 250	-2.36	-43.7	-14 182.9	-14 250.1	84.18	-17.01

^a All values are reported in kcal/mol, unless stated otherwise.

more drugs to a tumor site. According to the findings presented in this study, 9-CH₂OH Nos-Tel-SLNs were successfully synthesized through the solvent diffusion method. TEM and FE-SEM results reveal the formation of nanostructures that are spherical in shape having a mean size of 36.6 nm. RP-HPLC studies indicate that loaded noscapine and telmisartan content in the nanoparticles is 1.86% and 1.97% respectively. The expanding use of nanoparticles in drug delivery and cancer therapeutics

necessitates a thorough examination of their interactions with blood proteins. Therefore, interaction studies were performed using spectroscopic and computational techniques, both of which unveiled a stable complex formation between 9-CH₂OH Nos-Tel-SLNs and BSA. Furthermore, the H1299 cell line was used to study the *in vitro* anticancer activities of 9-CH₂OH Nos, telmisartan and 9-CH₂OH Nos-Tel-SLNs. For 9-CH₂OH Nos, telmisartan and 9-CH₂OH Nos-Tel-SLNs, the corresponding



Table 5 Generalized Born surface area analysis of Tel and Nos with BSA

Energy component	Telmisartan				Noscapine			
	Complex ^a	Protein ^a	Drug ^a	ΔG_{bind}^a (complex – (protein + drug))	Complex ^a	Protein ^a	Drug ^a	ΔG_{bind}^a (complex – (protein + drug))
BOND	1766.89	1751.71	15.18	0	1765.44	1751.71	13.74	0
ANGLE	4739.5	4683.72	55.78	0	4723.82	4683.72	40.1	0
DIHED	6176.91	6149.75	27.15	0	6176.66	6149.78	26.88	0
VDWAALS	–4821.63	–4745.3	–9.04	–67.29	–4769.97	–4745.3	–7.06	–17.61
EEL	–43 391.4	–43 339.5	–12.89	–38.96	–43 557.3	–43 339.5	7.69	–225.46
1-4 VDW	2190.43	2177.01	13.42	0	2185.83	2177.02	8.81	0
1-4 EEL	27 683.46	27 681.1	2.36	0	27 734.01	27 681.12	52.89	0
EGB	–8604.64	–8565.01	–93.95	54.32	–8400.33	–8565.02	–62.29	226.98
ESURF	207.04	210.36	4.7	–8.03	211.61	210.36	3.5	–2.25
GGAS	–5655.81	–5641.52	91.96	–106.26	–5741.51	–5641.49	143.05	–243.07
GSOLV	–8397.61	–8354.65	–89.24	46.28	–8118.71	–8354.65	–58.79	224.73
TOTAL	–14 053.4	–13 996.2	2.72	–59.97	–13 930.2	–13996.1	84.26	–18.34

^a All values are reported in kcal/mol, unless stated otherwise.

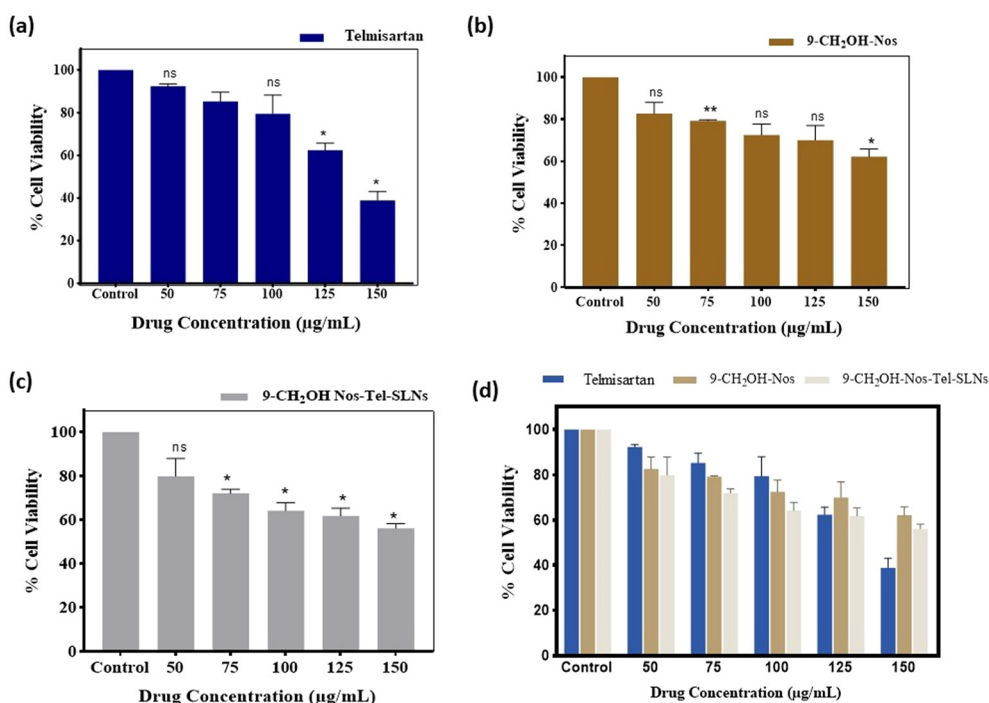


Fig. 11 *In vitro* dose-dependent cytotoxicity profiles of (a) telmisartan, (b) 9-CH₂OH Nos and (c) 9-CH₂OH Nos-Tel-SLNs. (d) Cell viability comparison among telmisartan, 9-CH₂OH Nos, and 9-CH₂OH Nos-Tel-SLNs against H1299 cells. Data represent mean \pm SD and * $p \leq 0.05$ was considered statistically significant.

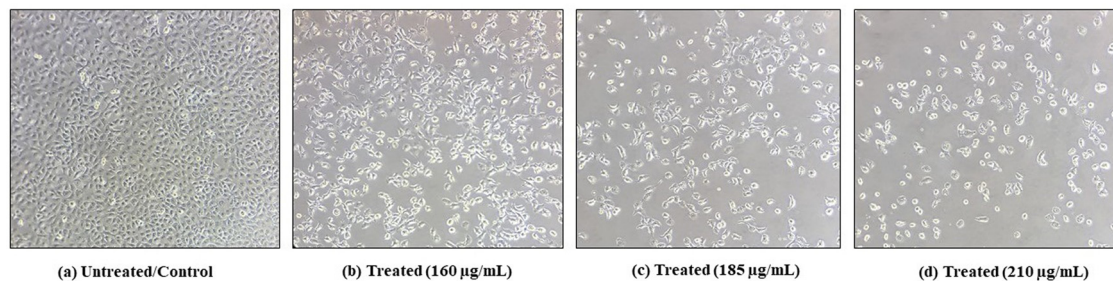


Fig. 12 Morphological changes and decline in cell viability of H1299 cells due to treatment with different concentrations of 9-CH₂OH-Nos-Tel-SLNs for 48 hours.



values of IC₅₀ are 282.5, 155.7, and 186 µg mL⁻¹. Therefore, the synthesized novel 9-CH₂OH Nos-Tel-SLN formulation developed as a dual-drug delivery system can offer significant advantages in the treatment of lung cancer.

Data availability

The authors confirm that the data supporting the findings of this study are available within the article and/or its ESI.†

Conflicts of interest

The authors have no conflict of interest.

Acknowledgements

S. Singh is grateful to ICMR (45/102/2018/Nan-BMS) for providing her SRF fellowship. S. Singh and R. Chandra are grateful to Indo-Russia (DST-RFBR: INT/RUS/RFBR/389) grant. S. Sewariya is grateful to CSIR (09/045(1739)/2019-EMR-I) for senior research fellowship. T. Goel is grateful for DST-INSPIRE fellowship (IF200339). The authors are grateful to the Department of Chemistry, University of Delhi for facilities and support.

References

- 1 F. Bray, M. Laversanne, H. Sung, J. Ferlay, R. L. Siegel, I. Soerjomataram and A. Jemal, *Ca-Cancer J. Clin.*, 2024, **74**, 229–263.
- 2 O. A. Madkhali, *Molecules*, 2022, **27**, 1543.
- 3 J. Akbari, M. Saeedi, F. Ahmadi, S. M. H. Hashemi, A. Babaei, S. Yaddollahi, S. S. Rostamkalaei, K. A. Addo and A. Nokhodchi, *Pharm. Dev. Technol.*, 2022, **27**, 525–544.
- 4 K. Mo, A. Kim, S. Choe, M. Shin and H. Yoon, *Pharmaceutics*, 2023, **15**, 2065.
- 5 R. A. Paun, S. Jurchuk and M. Tabrizian, *Bioeng. Transl. Med.*, 2024, **9**, e10601.
- 6 B. Yechezkel, *J. Controlled Release*, 2012, **160**, 117–134.
- 7 M. A. Liebert, *J. Am. Coll. Toxicol.*, 1987, **6**, 321–401.
- 8 S. Das and A. Chaudhary, *AAPS PharmSciTech*, 2011, **12**, 62–76.
- 9 X. Letao, W. Xing, L. Yun, Y. Guangze, J. F. Robert and Z. Chun-Xia, *Adv. NanoBiomed Res.*, 2022, **2**, 2100109.
- 10 D. Lombardo, M. A. Kiselev and M. T. Caccamo, *J. Nanomater.*, 2019, **3702518**, 1–26.
- 11 S. Singh, T. Goel, A. Singh, H. Chugh, N. Chakraborty, I. Roy, M. Tiwari and R. Chandra, *Artificial Cells, Nanomed., Biotechnol.*, 2024, **52**, 46–58.
- 12 S. S. Qia, J. H. Suna, H. H. Yuc and S. Q. Yua, *Drug Delivery*, 2017, **24**, 1909–1926.
- 13 S. Fumoto and K. Nishida, *Chem. Pharm. Bull.*, 2020, **68**, 603–612.
- 14 H. Zhang, Q. Xue, Z. Zhou, N. He, S. Li and C. Zhao, *Front. Pharmacol.*, 2023, **14**, 1176232.
- 15 C. H. Kim, S. Lee, J. Y. Choi, M. J. Lyu, H. M. Jung, Y. T. Goo, M. J. Kang and Y. W. Choi, *Pharmaceutics*, 2023, **16**, 349.
- 16 Y. Guo, W. He and S. Yang, *et al.*, *Colloids Surf., B*, 2017, **151**, 119–127.
- 17 G. Garg, S. Garg, P. Patel, G. D. Gupta and B. D. Kurmi, *Int. J. Polym. Mater. Polym. Biomater.*, 2024, 1–15.
- 18 T. B. Emran, A. Shahriar, A. R. Mahmud, T. Rahman, M. H. Abir, M. F. Siddiquee, H. Ahmed, N. Rahman, F. Nainu, E. Wahyudin, S. Mitra, K. Dhama, M. M. Habiballah, S. Haque, A. Islam and M. M. Hassan, *Front. Oncol.*, 2022, **12**, 891652.
- 19 C. Pi, W. Zhao, M. Zeng, J. Yuan, H. Shen, K. Li, Z. Su, Z. Liu, J. Wen, X. Song, R. J. Lee, Y. Wei and L. Zhao., *Drug Delivery*, 2022, **29**, 1878–1891.
- 20 S. Guo, Y. Zhang, Z. Wu, L. Zhang, D. He, X. Li and Z. Wang, *Biomed. Pharmacother.*, 2019, **118**, 109225.
- 21 C. H. Kim, S. Lee, J. Y. Choi, M. J. Lyu, H. M. Jung, Y. T. Goo, M. J. Kang and Y. W. Choi, *Pharmaceutics*, 2023, **16**, 349.
- 22 P. C. Rida, D. LiVecche, A. Ogden, J. Zhou and R. Aneja, *Med. Res. Rev.*, 2015, **35**, 1072–1096.
- 23 X. Chen, T. T. T. Dang and P. J. Facchini, *Phytochemistry*, 2015, **111**, 7–13.
- 24 C. Kocak, F. E. Kocak, B. Ozturk, G. Tekin and H. Vatansev, *Bratisl. Lek. Listy*, 2020, **121**, 43–50.
- 25 A. Awasthi, N. Kumar, A. Mishra, R. Ravi, A. Dalal, S. Shankar and R. Chandra, *ACS Pharmacol. Transl. Sci.*, 2022, **5**, 1292–1304.
- 26 V. Tomar, S. Kukreti, S. Prakash, J. Madan and R. Chandra, *Curr. Top. Med. Chem.*, 2017, **17**, 174–188.
- 27 M. Sharpe, B. Jarvis and K. L. Goa, *Drugs*, 2001, **61**, 1501–1529.
- 28 S. Zhang and Y. Wang, *Oncol. Lett.*, 2018, **15**, 5859–5864.
- 29 T. Matsui, *et al.*, *Int. J. Mol. Sci.*, 2019, **20**, 3197.
- 30 K. Tascilar, L. Azoulay, S. Dell’Aniello, D. B. Bartels and S. Suissa, *Am. J. Hypertens.*, 2016, **29**, 1358–1365.
- 31 E. Samukawa, S. Fujihara, K. Oura, H. Iwama, Y. Yamana, T. Tadokoro, T. Chiyo, K. Kobayashi, A. Morishita and M. Nakahara, *et al.*, *Int. J. Oncol.*, 2017, **51**, 1674–1684.
- 32 J. Grahovac, T. Srdić-Rajić, J. F. Santibañez, M. Pavlović, M. Čavić and S. Radulović, *Cancer Biol. Med.*, 2019, **16**, 247–263.
- 33 B. Carlo and E. Domenici, *Curr. Med. Chem.*, 2002, **9**, 1463–1481.
- 34 H. Chugh and R. Chandra, *J. Biomol. Struct. Dyn.*, 2019, **37**, 35–36.
- 35 S. Gandhi and I. Roy, *J. Mol. Liq.*, 2019, **296**, 111871.
- 36 P. Szymaszek, *et al.*, *J. Mol. Liq.*, 2022, **347**, 118262.
- 37 A. Awasthi, M. Singh, G. Rathee and R. Chandra, *RSC Adv.*, 2020, **10**, 12626–12652.
- 38 R. M. Shah, F. Malherbe, D. S. Eldridge, E. A. Palombo and I. H. Harding, *J. Colloid Interface Sci.*, 2014, **428**, 286–294.
- 39 R. M. Shah, D. Rajasekaran, M. Ludford-Menting, D. S. Eldridge, E. A. Palombo and I. H. Harding, *Colloids Surf., B*, 2016, **140**, 204–212.
- 40 W. Bae, T. Y. Yoon and C. Jeong, *PLoS One*, 2021, **16**, e0247326.



- 41 S. Raghavendra, S. J. Aditya Rao, V. Kumar and C. K. Ramesh, *Comput. Biol. Chem.*, 2015, **59**, 81–86.
- 42 H. M. Berman, The Protein Data Bank, *Nucleic Acids Res.*, 2000, **28**, 235–242.
- 43 A. Bujacz, K. Zielinski and B. Sekula, *Proteins*, 2014, **82**, 2199–2208.
- 44 G. M. Sastry, M. Adzhigirey, T. Day, R. Annabhimoju and W. Sherman, *J. Comput.-Aided Mol. Des.*, 2013, **27**, 221–234.
- 45 C. Lu, C. Wu, C. D. Ghoreishi, W. Chen, L. Wang, W. Damm, G. A. Ross, M. K. Dahlgren, E. Russell, C. D. Von Bargen, R. Abel, R. A. Friesner and E. D. Harder, *J. Chem. Theory Comput.*, 2021, **17**, 4291–4300.
- 46 R. C. Johnston, K. Yao, Z. Kaplan, M. Chelliah, K. Leswing, S. Seekins, S. Watts, D. Calkins, J. Chief Elk, S. V. Jerome, M. P. Repasky and J. C. Shelley, *J. Chem. Theory Comput.*, 2023, **19**, 2380–2388.
- 47 R. A. Friesner, J. L. Banks, R. B. Murphy, T. A. Halgren, J. J. Klicic, D. T. Mainz, M. P. Repasky, E. H. Knoll, M. Shelley, J. K. Perry, D. E. Shaw, P. Francis and P. S. Shenkin, *J. Med. Chem.*, 2004, **4**, 1739–1749.
- 48 T. A. Halgren, R. B. Murphy, R. A. Friesner, H. S. Beard, L. L. Frye, W. T. Pollard and J. L. Banks, *J. Med. Chem.*, 2004, **47**, 1750–1759.
- 49 R. A. Friesner, R. B. Murphy, M. P. Repasky, L. L. Frye, J. R. Greenwood, T. A. Halgren, P. C. Sanschagrin and D. T. Mainz, *J. Med. Chem.*, 2006, **49**, 6177–6196.
- 50 Y. Yang, K. Yao, M. P. Repasky, K. Leswing, R. Abel, B. K. Shoichet and S. V. Jerome, *J. Chem. Theory Comput.*, 2021, **17**, 7106–7119.
- 51 M. J. Abraham, T. Murtola, R. Schulz, S. Páll, J. C. Smith, B. Hess and E. Lindahl, *SoftwareX*, 2015, **1–2**, 19–25.
- 52 S. Páll, M. J. Abraham, C. Kutzner, B. Hess and E. Lindahl, Tackling Exascale Software Challenges in Molecular Dynamics Simulations with GROMACS, *Solving Software Challenges for Exascale: International Conference on Exascale Applications and Software, EASC 2014, Stockholm, Sweden, April 2–3, 2014, Revised Selected Papers 2*, 2015, pp. 3–27.
- 53 S. Pronk, S. Páll, R. Schulz, P. Larsson, P. Bjelkmar, R. Apostolov, M. R. Shirts, J. C. Smith, P. M. Kasson, D. van der Spoel, B. Hess and E. Lindahl, *Bioinformatics*, 2013, **29**, 845–854.
- 54 Y. Liu, F. Ji and R. Liu, *Nanotoxicology*, 2013, **7**, 97–104.
- 55 D. Van Der Spoel, E. Lindahl, B. Hess, G. Groenhof, A. E. Mark and H. J. C. Berendsen, *J. Comput. Chem.*, 2005, **26**, 1701–1718.
- 56 E. Lindahl, B. Hess and D. van der Spoel, *J. Mol. Model.*, 2001, **7**, 306–317.
- 57 A. W. Sousa da Silva and W. F. Vranken, *BMC Res Notes*, 2012, **5**, 367.
- 58 M. S. Valdés-Tresanco, M. E. Valdés-Tresanco, P. A. Valiente and E. Moreno, *J. Chem. Theory Comput.*, 2021, **17**, 6281–6291.
- 59 S. Genheden and U. Ryde, *Expert Opin. Drug Discovery*, 2015, **10**, 449–461.
- 60 E. Wang, H. Sun, J. Wang, Z. Wang, H. Liu, J. Z. H. Zhang and T. Hou, *Chem. Rev.*, 2019, **119**, 9478–9508.
- 61 T. Goel, N. Deshwal, S. Gusain, R. Chandra, M. Tiwari and S. Singh, *Int. J. Biol. Macromol.*, 2024, **283**, 137532.
- 62 B. Hess, C. Kutzner, D. van der Spoel and E. Lindahl, *J. Chem. Theory Comput.*, 2008, **4**, 435–447.
- 63 Z. Chi, R. Liu, Y. Teng, X. Fang and C. Gao, *J. Agric. Food Chem.*, 2010, **58**, 10262–10269.
- 64 Y. Li, W. He, J. Liu, F. Sheng, Z. Hu and X. Chen, *Biochim. Biophys. Acta, Gen. Subj.*, 2005, **1722**, 15–21.
- 65 J. R. Lakowicz, *Principles of Fluorescence Spectroscopy*, Springer, 3rd edn, 2006, p. 278.
- 66 V. D. Suryawanshi, L. S. Walekar, A. H. Gore, P. V. Anbhule and G. B. Kolekar, *J. Pharm. Anal.*, 2016, **6**, 56–63.
- 67 A. Biswas, R. K. Swarnkar, B. Hussain, S. K. Sahoo, P. I. Pradeep, G. N. Patwari and R. Anand, *J. Phys. Chem. B*, 2014, **3**, 10035–10042.
- 68 G. Sekar, M. Haldar, D. T. Kumar, C. G. P. Doss, A. Mukherjee and N. Chandrasekaran, *J. Mol. Liq.*, 2017, **241**, 793–800.
- 69 S. Sewariya, H. Sehrawat, N. Mishra, M. B. Singh, P. Singh, S. Kukreti and R. Chandra, *Int. J. Biol. Macromol.*, 2023, **247**, 125791.
- 70 S. Gandhi and I. Roy, *J. Mol. Liq.*, 2019, **296**, 111871.
- 71 N. Singh, N. Kumar and G. Rathee, *et al.*, *ACS Omega*, 2020, **5**, 2267–2279.
- 72 Q. Wang, C. R. Huang, M. Jiang, Y. Y. Zhu, J. Wang, J. Chen and J. H. Shi, *Spectrochim. Acta, Part A*, 2016, **156**, 155–163.
- 73 F. F. Tian, F. L. Jiang, X. L. Han, C. Xiang, Y. S. Ge, J. H. Li, Y. Zhang, R. Li, X. L. Ding and Y. Liu, *J. Phys. Chem. B*, 2010, **114**, 14842–14853.
- 74 K. Phopin, W. Ruankham, S. Prachayasittikul, V. Prachayasittikul and T. Tantimongkolwat, *Int. J. Mol. Sci.*, 2020, **21**, 249.
- 75 M. Voicescu and D. G. Angelescu, *J. Nanopart. Res.*, 2012, **14**, 1174.
- 76 A. Micsonai, F. Wien, E. Bulyaki, J. Kun, E. Moussong, Y. H. Lee, Y. Goto, M. Refregiers and J. Kardos, *Nucleic Acids Res.*, 2018, **46**(W1), W315–W322.
- 77 B. Gupta, C. S. Yong and J. O. Kim, *J. Pharm. Invest.*, 2017, **47**, 461–473.
- 78 R. R. Lala, A. S. Shinde and N. Y. Nandvikar, *J. Pharm. Invest.*, 2018, **10**, 17–22.

