



Cite this: *J. Anal. At. Spectrom.*, 2025, **40**, 2162

AutoSpect: an all-in-one software solution for automated processing of LA-ICP-TOF-MS datasets†

Andrew M. Crawford, ^{abc} David Z. Zee, ^{abc} Qiaoling Jin, ^d Aaron Sue, ^{abc} Niharika Sinha, ^{abc} Soo Hyun Ahn, ^{ae} Thomas V. O'Halloran ^{abc} and Keith W. MacRenaris ^{abc}

LA-ICP-TOF-MS provides rapid, high resolution elemental analysis of biological and non-biological samples. However, accurate real-time data analysis frequently requires the user to account for several instrumental and experimental variables that can change during data acquisition. AutoSpect is a novel software tool designed to automate the processing and fitting of LA-ICP-TOF-MS data, addressing key challenges such as time-dependent spectral drift, instrument sensitivity drift, calibration inaccuracies, and peak deconvolution, enabling researchers to rapidly and accurately process complex datasets. The tool is optimized to be robustly applicable across scientific fields (e.g., geochemistry, biology, and materials science), providing a streamlined solution for end users seeking to maximize the potential of LA-ICP-TOF-MS for high-resolution elemental mapping and isotopic analysis.

Received 16th April 2025
 Accepted 19th June 2025

DOI: 10.1039/d5ja00145e

rs.c.li/jaas

1. Introduction

Time-of-flight mass spectrometry (TOF-MS) has fast become the technique of choice for analyzing fast transient signals following ionization *via* inductively coupled plasma (ICP) sources due to the dramatic improvement in high-speed detection electronics.¹ This has been especially true for single particle (SP), single cell (SC), and laser ablation (LA) ICP-TOF-MS applications ranging from nanoparticle and microplastic characterization to elemental mapping in geological and biological samples.^{2–4} By combining high frequency LA with ICP-TOF-MS, rapid, high-resolution analyses at scales ranging from microns to millimeters are achievable. Additionally, with recent advancements in benchtop instrumentation, LA-ICP-TOF-MS is now capable of measuring all isotopes at frequencies from 10 Hz up to 1000 Hz helping to move elemental mapping into the realm of more routine, robust, quantitative analysis. These advancements are improving our fundamental understanding of how the distribution and concentration of elements play a role in dynamic processes; and, by combining elemental mapping with complementary imaging modalities

such as matrix assisted laser desorption ionization TOF-MS, near infrared, Raman, histochemistry, immunofluorescence, and brightfield microscopy we can begin to unlock the complexity of a multitude of sample types.^{5–7}

The major advantage of ICP-TOF-MS is the ability to provide near simultaneous detection of all isotopes across the whole mass spectrum which makes it well-suited for the analysis of short transient events such as LA.⁸ However, using TOF-MS for detecting these short transient events generated from single pulse-resolved laser ablation presents challenges, including time-dependent spectral drift, instrument sensitivity drift, and the need for precise calibration and interference correction. Addressing these hurdles is crucial to ensuring accurate data interpretation, particularly for multi-element and isotopic analyses and quantitative elemental mapping. Although there are several software options for mass spectrometry image analysis^{9–11} there remain few commercially available spectral fitting tools for modern ICP-TOF-MS systems that handle spectral post-processing for ICP-TOF-MS datasets including LA.⁹ Each of these tools have independent advantages but sequential application can lead to bottlenecks and inefficiencies in ICP-TOF-MS workflow. Most software^{12–14} requires manual user input to identify optimal peaks for drift correction, mass axis calibration, and peak profile modeling, which can introduce subjectivity and user error. With larger specimens, a laser ablation imaging experiment can require several hours, exposing the spectra to greater possibility of drift due to external factors like temperature changes.^{15,16} While some commercially available software packages can accommodate peak drift up to a user-defined limit, the process is not automatic and can fail to accurately fit peaks that drift beyond that limit. Ideally, users would benefit from inspection of the accuracy of the drift

^aDepartment of Microbiology, Genetics, Immunology, Michigan State University, East Lansing, MI, USA. E-mail: macrenar@msu.edu; ohallor8@msu.edu; crawf472@msu.edu

^bDepartment of Chemistry, Michigan State University, East Lansing, MI, USA

^cElemental Health Institute, Michigan State University, East Lansing, MI, USA

^dDepartment of Physics and Astronomy, Northwestern University, Evanston, IL, USA

^eDepartment of Pathobiology and Diagnostics Investigation, Michigan State University, East Lansing, MI, USA

† Electronic supplementary information (ESI) available. See DOI: <https://doi.org/10.1039/d5ja00145e>



correction process. Overcoming these challenges is particularly important when the goal is a quantitative comparison of dozens of analytes over a broad dynamic range in small regions of interest.

Herein, we describe the workflow of a new integrated and automated software solution called AutoSpect, that integrates multiple stages of data processing, beginning with raw data import, and proceeds through data sorting, peak identification, time dependent peak drift correction, mass-to-charge (m/z , or μ) calibration, peak profile creation, and spectral fitting to generate reliable outputs. Finally, we demonstrate AutoSpect use cases illustrating elemental map generation and data visualization as well as isotope accumulation.

2. AutoSpect workflow

AutoSpect software provides a user-friendly graphical interface for analysis of complex ICP-TOF-MS datasets. This is accomplished through an automated process composed of the following six steps (Fig. 1):

(i) Processing and partitioning raw data: first, LA-ICP-TOF-MS data is imported in the raw hierarchical data format (HDF5), where each component is automatically defragmented to produce three distinct datasets (*i.e.* gas blanks, references, and samples). These three datasets are partitioned into hundreds of independently manageable data chunks with associated metadata (*e.g.*, average integrated mass spectra, acquisition time, and m/z calibration coefficients).

(ii) Measuring peak drift: following processing of raw data, peaks are identified in the integrated spectrum and then tracked across spectral partitions to extract centroid positions. The centroids are modeled as smooth functions of acquisition time and used to characterize drift.

(iii) Drift correction: using a reference set of centroids, partition-specific mass calibration parameters are optimized, modeled over time, and used to interpolate each partition onto the reference mass axis. Finally, a drift-corrected integrated spectrum is computed as a weighted average of the aligned partitions.

(iv) Mass-to-charge (m/z) calibration: the global mass calibration parameters are recalibrated using a refined set of well-isolated peaks with known mass-to-charge (m/z) values. Each is fitted with Gaussian and Lorentzian models to extract centroids and widths. A smooth polynomial model is used to identify and iteratively remove outliers, leaving a final set of peaks for recalibrating the global parameters. The parameters are then refined iteratively until convergence, and the updated calibration parameters are propagated to update drift correction results.

(v) Peak profiling: empirical peak profiles are generated based on isolated peaks that are automatically identified by AutoSpect. These profiles are used to create a look up table (LUT) of all possible peaks contained in the range of the spectra. This ensures accurate representation of spectral features corresponding to the main peak centers. AutoSpect then accounts for instrumental notching effects and models peak tailing.

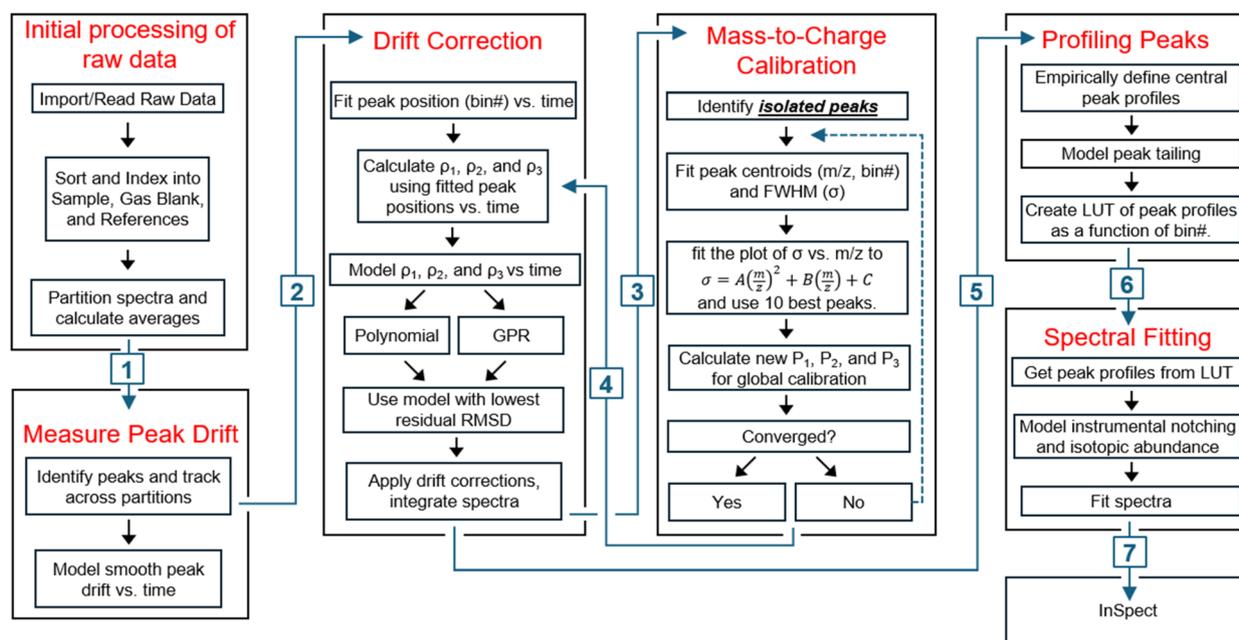


Fig. 1 AutoSpect Workflow AutoSpect was designed as an all-in-one software solution for ICP-TOF-MS datasets that performs many processes automatically. For contextualization, the processes have been broken into six sections. Following initial processing of the raw data, AutoSpect measures the peak drift across all measured spectra. Once peak drift has been measured, the drift correction is calculated and applied. Using the drift corrected integrated spectrum the mass-to-charge axis is recalibrated, and then the drift corrections are updated to the optimized axis. Using the drift corrected and m/z optimized spectra, AutoSpect empirically determines the peak profiles for all possible m/z contained in the data. Finally, AutoSpect performs fitting using linear least squares to deconvolute all peaks and produce elemental mapping data.



(vi) Spectral fitting: the generated peak profiles are applied to fit spectra, resolving overlapping peaks and deconvoluting interferences. Linear optimization algorithms refine the fitting process, ensuring high precision in determining elemental and isotopic abundances. Fitted spectra are saved and a new HDF5 file is generated that can be used in a variety of downstream image processing programs such as *iolite*.^{17–19}

3. Materials and methods for AutoSpect use cases

Datasets to test the key functionality of AutoSpect such as peak fitting and branching were obtained from fresh frozen murine kidney and epididymis as well as sea urchin egg samples. Mice organs were dissected from Balb/c and C57BL/6 mice and were embedded in optimal cutting temperature (OCT) media in a plastic mold and flash frozen using chilled isopentane over liquid nitrogen as described elsewhere.²⁰ Briefly, samples were sectioned at 10 μm using a conventional cryostat (Leica Biosystems) onto SuperFrost charged slides (ThermoFisher Scientific) and stored in $-20\text{ }^\circ\text{C}$ prior to ablation. Sea urchin eggs from *Arbacia punctulata* (Marine Biology Laboratory, Woods Hole, MA, USA) were isolated following standard procedures,²¹ deposited onto Kapton thin film (SPEX SamplePrep) and allowed to air dry at ambient temperature for 8 hours prior to ablation.

Experimental setup begins with outlining the regions of interest on the sample (*i.e.* kidney, epididymis). Additionally, the instrument is set to measure at least 50 seconds of gas blanks throughout a scan for the collection of signals that can be used for background subtraction.

All samples were ablated using the Elemental Scientific Lasers BioImage 266 nm laser ablation system (Elemental Scientific Lasers, Bozeman, MT, USA) equipped with an ultra-fast low dispersion TwoVol3 ablation chamber and a dual concentration injector and connected to icpTOF S2 mass spectrometer (TOFWERK AG, Thune, Switzerland). Elemental content was initially analyzed in real time according to m/z ratio windowing. Tuning was performed using NIST SRM612 glass certified reference material (National Institute for Standards and Technology, Gaithersburg, MD, USA). Torch alignment, lens voltages, and nebulizer gas flow were optimized using ^{140}Ce and ^{55}Mn while maintaining low oxide formation based on the $^{232}\text{Th}^{16}\text{O}^+ / ^{232}\text{Th}^+$ ratio (<0.5). Murine samples were ablated in a raster pattern with a laser repetition rate of 100 Hz using a 10 μm circular spot with a 10 μm spacing and zero raster overlap. Sea urchin samples were ablated in a raster pattern with a laser repetition rate of 100 Hz, a 2 μm circular spot, 2 μm spacing, and zero raster overlap. Scanning data were recorded using ToFPilot 1.3.4.0 (TOFWERK AG) and saved in the HDF5 format v1.8.20.²² Laser ablation images were visualized using *Iolite*.^{17–19}

4. AutoSpect software

4.1 LA-ICP-TOF-MS

Laser ablation works by ablating material from the sample and introducing it to a plasma torch where the material is converted

to positively charged ions. In TOF-MS, these ions are injected between a pair of extraction plates and accelerated toward a detector. For each extraction, the time of collision is recorded for each detection event, culminating in a spectrum of total detected collisions as a function of time. Current elemental mapping *via* LA groups each set of laser shots as a line scan, whereas a single image dataset is represented by as many line scans as there are rasters in the image. Thus, a single image can correspond to the aggregate of thousands of individual line scans each corresponding to hundreds to thousands of individual spectra representing ion extraction events. Furthermore, as an LA-ICP-TOF-MS instrument collects an image, it alternates between segmented scans of sample regions, reference standards, and gas blanks. This results in fragmented, discontinuous data spread across thousands of individual scans that cannot be immediately interpreted and require users to manually assign the identity of each individual line scan, or raster, which is time consuming. AutoSpect software preprocesses this LA-ICP-TOF-MS data in the raw hierarchical data format (HDF5), automatically defragmenting each component, and producing three distinct datasets. These three groups are then partitioned into hundreds of independently manageable data partitions with associated metadata (*e.g.*, average integrated mass spectra, acquisition time, and m/z calibration coefficients, derived below).

4.1.1 Derivation of TOF-MS calibration function. In a time-of-flight mass spectrometer (TOF-MS), ions are accelerated through an electric potential and then travel through a field-free drift region before striking the detector. The time, t , that an ion takes to reach the detector is determined by its mass-to-charge ratio (m/z), and is derived from the classical kinetic energy equation:

$$K_E = \frac{1}{2}mv^2 = qV \quad (1)$$

where m is the ion mass, v is the velocity, q is the ion charge, and V is the accelerating voltage. Solving for v and expressing the time-of-flight as $t = L/V$, where L is the flight path length, gives:

$$t = L\sqrt{\frac{m}{2qV}} = L\sqrt{\frac{m/z}{2V}} \quad (2)$$

This yields a square-root dependence of t on m/z , consistent with the idealized flight model. However, to account for instrumental delays and nonlinearities in practical TOF-MS systems, this relationship is generalized as:

$$t = P_1(m/z)_3^{P_3} - P_2 \quad (3)$$

where P_1 , P_2 , and P_3 are empirical calibration constants determined from known reference peaks. This formulation is used in AutoSpect to interconvert between digital time bins and the corresponding calibrated mass-to-charge values.

Since each ion undergoes the same accelerative force, the more massive an ion is the slower the acceleration it undergoes. This separates the ions in space based on their mass-to-charge ratio (m/z , or μ), such that the corresponding digital spectral



time bin, b_i , for a particular μ_i is given by eqn (4) and the corresponding μ_i for a given time bin, b_i , is given by eqn (5).

$$\text{mz2bin}(\mu_i; P_1, P_2, P_3), b_i = P_1 \times (\mu_i)^{P_3} - P_2 \quad (4)$$

$$\text{bin2mz}(b_i; P_1, P_2, P_3), \mu_i = \left(\frac{b_i + P_2}{P_1} \right)^{-P_3} \quad (5)$$

where P_1 , P_2 , and P_3 are fixed coefficients determined during instrument calibration prior to data collection, and routinely recalibrated after a scan is collected.

4.2 Partitioning and processing raw data

Laser ablation based elemental mapping is acquired using line scans. As such, a single image dataset is represented by as many line scans as there are rasters in the image. Thus, a single image corresponds to the aggregate of thousands of individual line scans. Furthermore, as an LA-ICP-TOF-MS instrument collects an image, it alternates between segmented scans of the sample, reference standards, and gas blanks. As the instrument alternates between segmented scans of the sample, reference standards, and gas blanks, the resulting spectra are fragmented and dispersed across numerous acquisitions. To facilitate structured data handling, spectra from all measurements—sample, gas blank, and references—are sorted accordingly and grouped into smaller partitions, each containing approximately 1600 spectra consisting of 15 616 spectral time points.

For each partition, the average acquisition time and spectrum are computed and stored. The spectral data is structured into a partition matrix, $\mathbf{S} \in \mathbb{R}^{N \times Q}$, where N represents the number of spectral bins, and Q denotes the number of partitions. Each column $\mathbf{S}(:, q)$ in the matrix corresponds to a partition containing the mean spectrum for that subset:

$$\mathbf{S} = \begin{bmatrix} \bar{S}_{1,1} & \bar{S}_{1,2} & \cdots & \bar{S}_{1,Q} \\ \bar{S}_{2,1} & \bar{S}_{2,2} & \cdots & \bar{S}_{2,Q} \\ \vdots & \vdots & \ddots & \vdots \\ \bar{S}_{N,1} & \bar{S}_{N,2} & \cdots & \bar{S}_{N,Q} \end{bmatrix} \quad (6)$$

where each element $\bar{S}_{n,q}$ represents the average intensity at spectral bin n within partition q . The partition-wise averaged spectrum is then computed (eqn (S1)†). The columns of \mathbf{S} are then sorted in ascending order of their mean acquisition times, $\mathbf{t} \in \mathbb{R}^Q$, with the q th entry of \mathbf{t} corresponding to the q th column of \mathbf{S} . Lastly, the integrated spectrum, $\mathbf{s} \in \mathbb{R}^N$, is obtained by averaging over all individual raw pixel spectra.

4.3 Peak identification, tracking peaks, and measuring peak drift

TOF instruments can be sensitive to fluctuations in physical parameters such as temperature.^{15,16} This can lead to time-dependent peak centroid drift of the ions of interest over the course of sample analysis. As such, the peak centroids' positions at the initiation of a scan may not reflect their corresponding positions throughout the scan. Therefore, this time-

dependent peak drift must be accounted for before any processing/fitting of the resultant spectra to produce the most accurate isotope maps. The major drawback for peak fitting is the subjective nature of removing peaks prior to fitting and the time constraints of full spectrum peak fitting. AutoSpect solves these issues through development of an automated process to identify peaks and measure peak drift.

4.3.1 Peak identification. To track and measure peak drift, AutoSpect identifies peaks in the integrated spectrum and then tracks across spectral partitions to extract centroid positions. Using the integrated spectrum, peaks are identified as local maxima where the intensity decreases monotonically to the nine nearest neighboring bins on both sides. The set criteria are satisfied to ensure that the center bin is a true local maximum with symmetrical monotonic decay in intensity over a 19-bin window (see eqn (S2) and (S3)†). Then, this 19-bin window around each peak is used as a search window for each partition, with peaks being identified as local maxima where the intensity decreases monotonically to the nine nearest neighboring bins on both sides.

4.3.2 Tracking peaks across spectral partitions. Each spectral partition, $\mathbf{S}(:, q)$, is analyzed as follows. The intensity values for each peak region in $\mathbf{S}(:, q)$ are extracted and assembled into a matrix $\mathbf{A}_q \in \mathbb{R}^{19 \times J}$, where each column, j , contains the raw

intensity values $\mathbf{S} \left(\begin{bmatrix} \mathbf{x}_{L,j} \\ \vdots \\ \mathbf{x}_{R,j} \end{bmatrix}, q \right)$ such that

$$\mathbf{A}_q = \left[\mathbf{S} \left(\begin{bmatrix} \mathbf{x}_{L,1} \\ \vdots \\ \mathbf{x}_{R,1} \end{bmatrix}, q \right), \mathbf{S} \left(\begin{bmatrix} \mathbf{x}_{L,2} \\ \vdots \\ \mathbf{x}_{R,2} \end{bmatrix}, q \right), \dots, \mathbf{S} \left(\begin{bmatrix} \mathbf{x}_{L,p} \\ \vdots \\ \mathbf{x}_{R,p} \end{bmatrix}, q \right) \right] \quad (7)$$

Here, each column in \mathbf{A}_q represents the 19-bin peak region, centered at \mathbf{x}_j . Similarly, the corresponding bins for the intensity values of the peak regions in $\mathbf{S}(:, q)$ are extracted and assembled into a matrix $\mathbf{A}_{x,i} \in \mathbb{R}^{19 \times J}$, such that

$$\mathbf{A}_{x,q} = \begin{bmatrix} \mathbf{x}_{L,1} & \mathbf{x}_{L,2} & \cdots & \mathbf{x}_{L,p} \\ \vdots & \vdots & \ddots & \vdots \\ \mathbf{x}_{R,1} & \mathbf{x}_{R,2} & \cdots & \mathbf{x}_{R,p} \end{bmatrix} \quad (8)$$

Each peak region $\mathbf{A}_q(:, j)$ is first corrected by subtracting a linear baseline computed using a first-order polynomial fit. The baseline is subtracted from the raw peak region, yielding a corrected peak region. This baseline-corrected region is then fitted to a Lorentzian function. The optimal parameters are determined by minimizing the sum of squared residuals (see Section 3 in ESI†).

From each spectral partition, q , and peak region, j , the fitted centroid, \mathbf{x}_0 , is stored to the q -th and j -th entry of matrix $\hat{\mathbf{x}}_0 \in \mathbb{R}^{J \times Q}$, where J is the number of peaks and Q is the number of spectral partitions (see Fig. 2A, gray lines).



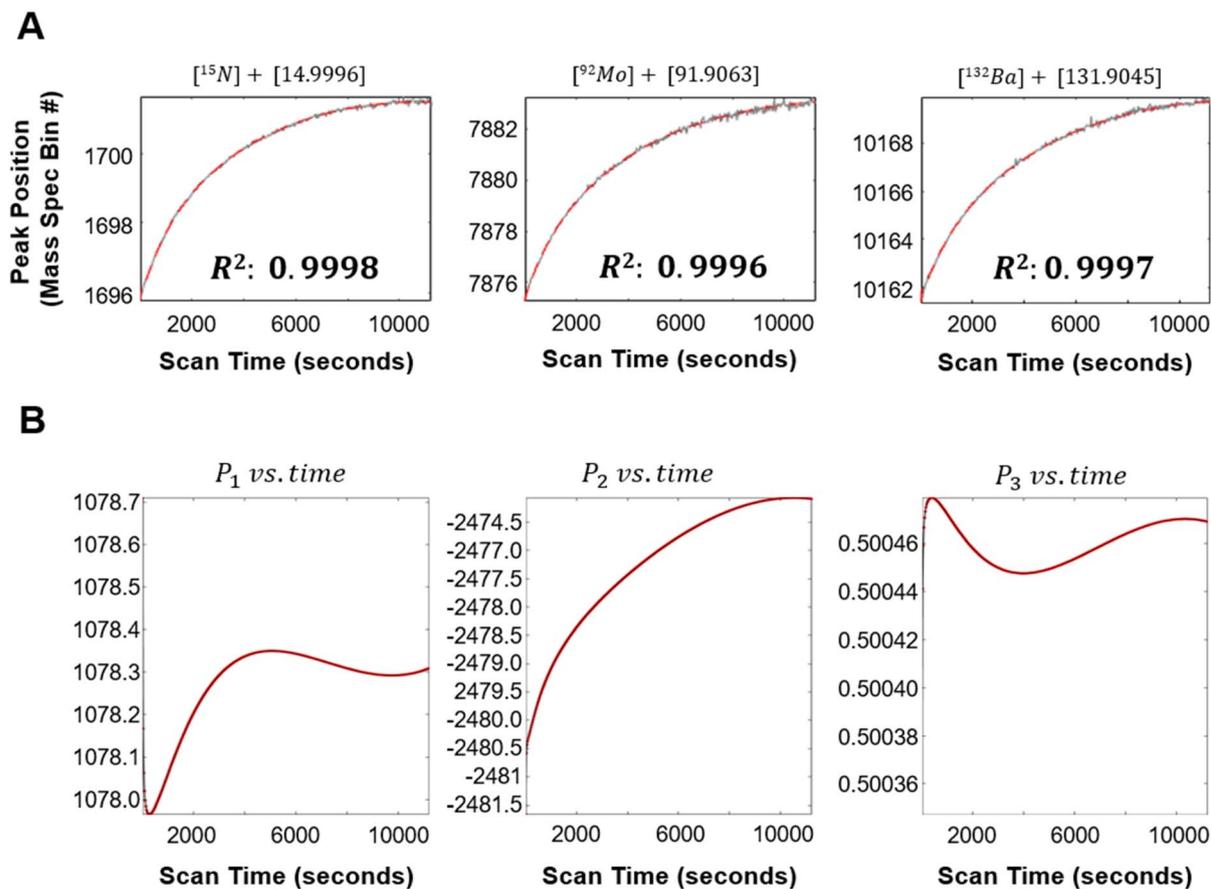


Fig. 2 AutoSpect conducts robust automatic drift correction with error less than 1 ppt. (A) Plots of measured peak centroids for ^{15}N , ^{92}Mo , and ^{132}Ba as a function of time from each partitioned average spectrum showing 3 of the 20+ accepted peaks to be used in calculating drift correction. (B) Following peak tracking and identification, the fitted peak centroids are used to calculate the coefficients for the Thomson calibrations necessary for drift correction. The red dots = fitted/measured centroid; black line = fitted theoretical values for P_1 , P_2 , and P_3 for the whole scan. They are superimposed to one another.

4.3.3 Solving a smooth function of peak position vs. time.

Where \hat{x}_0 is the array of fitted centroids from our Lorentzian modeling to the peaks across the spectral partitions, we seek to solve for \hat{x}_f , the smooth temporal trend of the centroids across the partitions. To do this, each row of the peak centroid matrix, \hat{x}_0 , is independently fitted to a smooth function of the mean acquisition time, t , (Fig. 2A, red fitted line, eqn (S10)†). Using the R^2 calculated from the fit to each row (peak centroid as a function of time), only the rows corresponding to the top 20 R^2 values are retained and used in the following section to solve spectral drift as a function of acquisition time. This ensures that the most temporally coherent and well-modeled peaks are used for spectral drift correction.

4.4 Modeling peak drift and applying drift correction

4.4.1 Selecting the basis set or reference spectrum. Since the peak centroids shift as a function of time, each spectral partition has its own unique set of coefficients used for eqn (4) and (5). To account for the drift, AutoSpect models the coefficients for each partition as a function of acquisition time. This creates three new variables, ρ_1 , ρ_2 , and $\rho_3 \in \mathbb{R}^Q$, each

representing a vector of length Q corresponding to the spectral partition specific entries for P_1 , P_2 , and P_3 , respectively (eqn (S11)†).

AutoSpect solves for the coefficients ρ_1 , ρ_2 , and ρ_3 , by first assigning a basis set for comparison. This basis set provides a reference set of peak centroids for comparison with the time-dependent peak centroids derived above. This set of basis peaks is determined by assigning one of the partitions as a reference. To determine the reference partition, total peak region counts per spectral partition are computed and the partition with the fourth-highest total counts is chosen as the reference.

4.4.2 Calculating partition specific mass calibration parameters. To refine the mass calibration parameters, AutoSpect sets about solving the partition specific parameters, stored in the vectors ρ_1 , ρ_2 , and ρ_3 , used for interconverting between bin# and m/z (μ) (eqn (4) and (5)). Using the j th column index of the \hat{x}_f , the peak centroids are converted from bin# to μ (eqn (5)) and become the basis set against which the rest will be compared.

$$\mu_{\text{ref}} = \text{bin2mz}(\hat{x}_f(:,j); P_1, P_2, P_3) \quad (9)$$



$$\mu_q = \text{bin2mz}(\hat{x}_f(:,q); \rho_{1q}, \rho_{2q}, \rho_{3q}) \quad (10)$$

Using the theoretical centroids calculated above, \hat{x}_f , the partition specific calibration parameters (ρ_1 , ρ_2 , and ρ_3) are solved by minimizing the residuals between expected/basis (μ_{ref} , eqn (9)) and fitted (μ_q , eqn (10)) values.

Following optimization of the ρ_1 , ρ_2 , and ρ_3 calibration parameters, each parameter is fitted as a function of the mean acquisition time, t , using polynomial fitting, Gaussian Process Regression fitting, or a simple cubic spline interpolation. The resulting root-mean-squared-deviations from each approach for all three parameters are compared and the approach with the corresponding lowest value is used going forward (Fig. 2B).

Once the spectra of S are drift corrected, the integrated spectrum is recalculated (Fig. 3 bottom row, Fig. 6A and 8 bottom row) as the weighted mean of the drift corrected spectral partitions.

4.4.3 Drift correction of spectral partitions. Each spectral partition $S(:,q)$ is corrected for time-dependent drift using the optimized partition-specific calibration parameters $\rho_1(q)$, $\rho_2(q)$, and $\rho_3(q)$ for each spectral partition $q = 1, \dots, Q$. Each partition is first converted to its corresponding mass axis, μ_q , using eqn (10), with subsequent interpolation from μ_q onto the reference axis μ_{ref} using a shape-preserving cubic Hermite operator (eqn (11)).

$$\begin{aligned} \hat{S}(:,q) &= \mathcal{I}_{\mu_q \rightarrow \mu_{\text{ref}}}(S(:,q)), \text{ where } \mu_q \\ &= \text{bin2mz}(\mathbf{b}_0; \rho_1(q), \rho_2(q), \rho_3(q)) \end{aligned} \quad (11)$$

Here: \mathbf{b}_0 is the uniformly spaced vector $1, \dots, N$, corresponding to bins of μ_{ref} , μ_q is the mass axis computed from \mathbf{x}_0 using eqn (5) for partition q , $\mathcal{I}_{\mu_q \rightarrow \mu_{\text{ref}}}$ is the interpolation operator, implemented using a piecewise cubic Hermite interpolation polynomial, that maps the spectrum from the local axis μ_q to the global reference axis μ_{ref} , $\hat{S}(:,q)$ is the drift-corrected spectrum matrix for partition q .

An overlay of the various spectral partitions following drift correction can be seen in Fig. 3A and B, which show drift correction of low, mid, and high range m/z regions. This can be seen by the top and middle rows. Where the top rows show noticeable peak drift in the centroid positions, the middle row shows that the drift corrected spectra are perfectly aligned.

4.4.4 Recomputing the integrated spectrum. Peak drift results in blurred features from the integrated spectrum. To correct for this blurring, the integrated spectrum must be recalculated following drift correction. Since each partition is derived from a known number of raw spectra, the drift-corrected integrated spectrum is then computed as a weighted average of the columns of \hat{S} , with weights proportional to the number of contributing spectra (Section 8, ESI†).

The deblurring of spectra following drift correction can be seen in Fig. 3 (and later in the bottom row of Fig. 8) by looking at the bottom row of plots and comparing the original integrated spectrum with the integrated spectrum from drift correction. Although the peaks are narrower for all three regions, the impact, at least in this example, is most noticeable for m/z of 18,

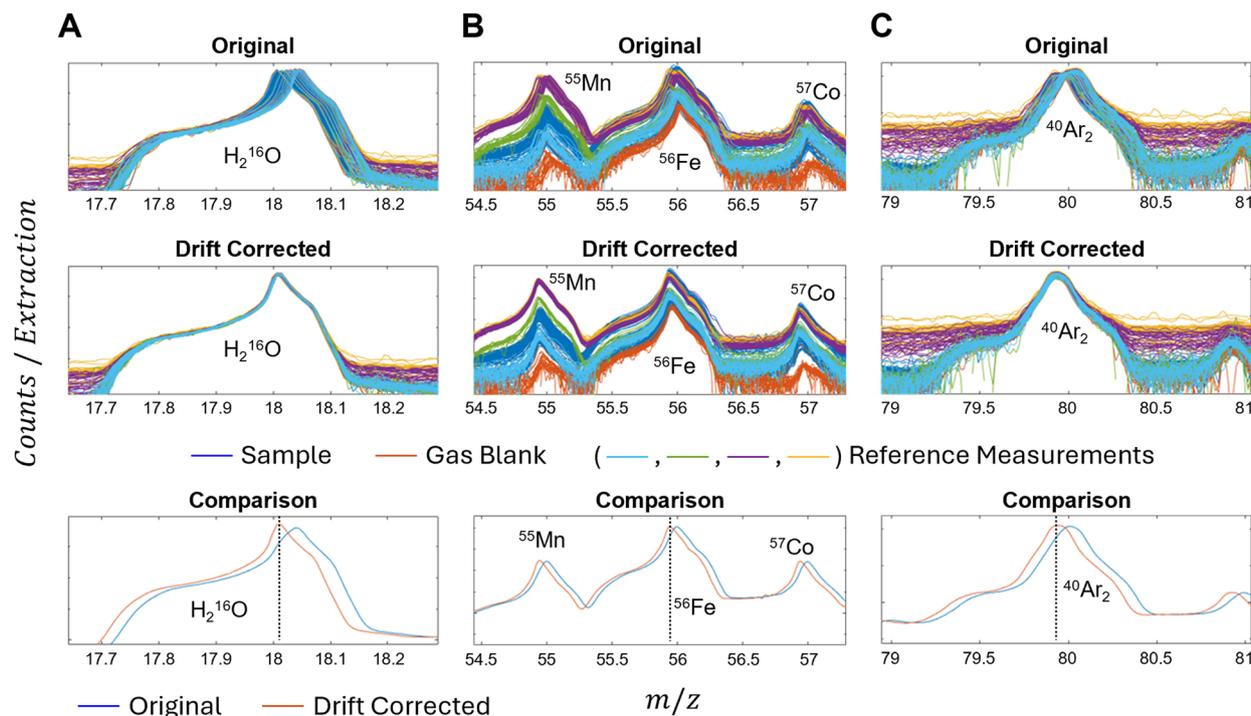


Fig. 3 Time dependent instrument drift correction. AutoSpect automatically corrects for drift, which is applied to the whole dataset. Here we show drift correction for five masses (A) H_2^{16}O , (B) ^{55}Mn , ^{56}Fe , ^{57}Co , and (C) $^{40}\text{Ar}_2$. The top panel shows the original uncorrected spectra, and the middle panel shows drift corrected spectra. The various colors denote the different partition groups from the sample, gas blanks, and various reference standards used for the scan. The bottom panel shows a comparison of the average of both the original (blue) and drift corrected (red) spectra from all partitions. Both plots show significant changes to the apparent peak position and peak morphology post AutoSpect.



where it is easily seen that the peak is much more clearly defined.

4.5 Optimizing mass spectrum calibration

The global mass calibration parameters are recalibrated using a refined set of well-isolated peaks with known m/z values. Each is fitted with Gaussian and Lorentzian models to extract centroids and widths. A smooth polynomial model is used to identify and iteratively remove outliers, leaving a final set of peaks for recalibrating the global parameters. The parameters are then refined iteratively until convergence, and the updated calibration parameters are propagated to update drift correction results.

4.5.1 Identifying isolated peaks for global mass spectrum calibration. Following drift correction, the global variables P_1 , P_2 , and P_3 are recalibrated using actual mass peaks, *i.e.*, both a peak exists and the corresponding value of its μ is known (rather than assumed) with very high confidence to be a specific ion (*e.g.* ^{55}Mn). This is different from drift correction where only the presence of the peak and its apparent μ according to reference spectrum and the suboptimal mass calibration coefficients P_1 , P_2 , and P_3 set by the instrument were used.

This begins by using the preset integration windows for the 315 ions in the LUT available from TofWare. All peaks that have integration windows that do not overlap with any other window are considered isolated peak regions. For the icpTOF S2 instrument, of the 315 available peak regions in the LUT, 118 peaks are considered isolated. Then in a process similar to peak identification above (Section 4.3), each peak region of the drift corrected weighted integral spectrum, \hat{s} , is checked to verify two things.

- (1) The highest point (peak) is contained in the window but not at the boundaries of the window.
- (2) The spectral intensities are monotonically decreasing to the left and right (similar to eqn (S2) and (S3)†).

4.5.2 Fitting isolated peak regions to obtain the centroids and peak widths. Following initial identification, the isolated peak regions are analyzed using Gaussian and Lorentzian fitting approaches. For each peak region, the raw intensity values, y_i , and corresponding indices, x_i , are extracted along with the corresponding m/z values for the corresponding ion, μ_i^{LUT} , from the LUT. The region defined by the index corresponding to the point of maximum intensity and a window of ± 4 is fitted to a single Gaussian and the R^2 calculated. Then only peak regions with $R^2 > 0.7$ are carried forward for further analyses.

Next, the fitted centroid and width from the Gaussian fitting are used as initial values for fitting the same region to a Lorentzian function (eqn (S17), ESI†). From this, the centroids (x_{fitted}) and peak widths (σ_{fitted}) are saved. To avoid spurious fits, the x_{fitted} is verified to be contained within the windowed region. If it is not, then the peak region and its associated x_{fitted} and σ_{fitted} are discarded. Using the R^2 from the Lorentzian fitting, all fitted peak regions with $R^2 > 0.75$ are carried forward. Using eqn (5), the x_{fitted} is converted to μ_{fitted} . Then x_{fitted} , μ_{fitted} , and σ_{fitted} are stored into column vectors for further refinement (eqn (S18), ESI†).

4.5.3 Solving for peak broadening as a function of m/z . Using μ_{fitted} along with σ_{fitted} , the list of isolated peaks is further refined to determine the optimal peaks to be used for recalibrating the global coefficients, P_1 , P_2 , and P_3 . The peak widths (σ) follow a smooth trend as a function of the mass-to-charge ratio (μ).¹⁴ Since individual peaks may not always be fully isolated, *i.e.* some may be broadened due to overlap with neighboring peaks, a filtering process is applied to iteratively remove peaks with broadened widths. If a peak overlaps with another, the fitting process may incorrectly attribute a broader width to what is a combination of multiple peaks. Removing outliers with excessive width improves confidence that the remaining peaks are truly isolated and that their widths accurately reflect instrumental resolution and physical broadening effects.

To model the expected smooth dependence of σ_{fitted} on the corresponding fitted centroid positions μ_{fitted} , a second-order polynomial model is constructed using non-negative least squares regression. In addition, the expected peak width for each centroid is then estimated using a fitted polynomial model, the most extreme outlier is then removed, and the polynomial fit is recomputed with the remaining peaks. This process is repeated until only 10 peaks remain (Fig. 4A and ESI Section 10†).

From these 10 peaks, the associated x_{fitted} and μ_{fitted} are used to optimize the coefficients P_1 , P_2 , and P_3 . The optimization problem is solved using nonlinear least squares (eqn (S20), ESI†). The associated σ_{expected} from the ten peaks are used to calculate the expected peak centroid width for all spectral bins for use in Sections 4.6 and 4.7.

4.5.4 Iterative refinement of mass-to-charge axis recalibration. Post calibration of drift correction parameters, the m/z axis for the detected spectra needs to be recalibrated. The recalibration can be conducted from the integrated spectrum, but the peaks are blurred because the integrated spectrum is the average of drifted peaks. Mass-to-charge axis recalibration is performed after drift correction using the highly resolved peaks. Refinement of mass calibration is an iterative process. Each iteration begins with the mass axis (M_i) determined by the initial values for the coefficients P_{1i} , P_{2i} , and P_{3i} , and ends with optimized values for the coefficients (P_{1i+1} , P_{2i+1} , and P_{3i+1}) and M_{i+1} . At the end of each iteration, the unique values from M_i and M_{i+1} are taken combined and the combined bin positions using the previous and current parameters are computed. Then, recalibration is considered converged when the population becomes self-consistent (ESI Section 11†). Fig. 4B shows how various regions of the spectra can shift, and that recalibration of the m/z axis is not always just a simple translation. As can be seen in Fig. 4B, around both m/z of 19 and 203, both regions required a corrective shift to higher m/z , while around m/z of 60 required a corrective shift to lower m/z .

4.5.5 Post recalibration optimization of drift correction. The global calibration coefficients P_1 , P_2 , and P_3 are used in drift correction as the basis set for calculating the m/z axis into which the peaks from all the spectral partitions are aligned. Post-drift-correction optimization of these parameters means the spectral partition coefficients for ρ_1 , ρ_2 , and ρ_3 (eqn (S11),



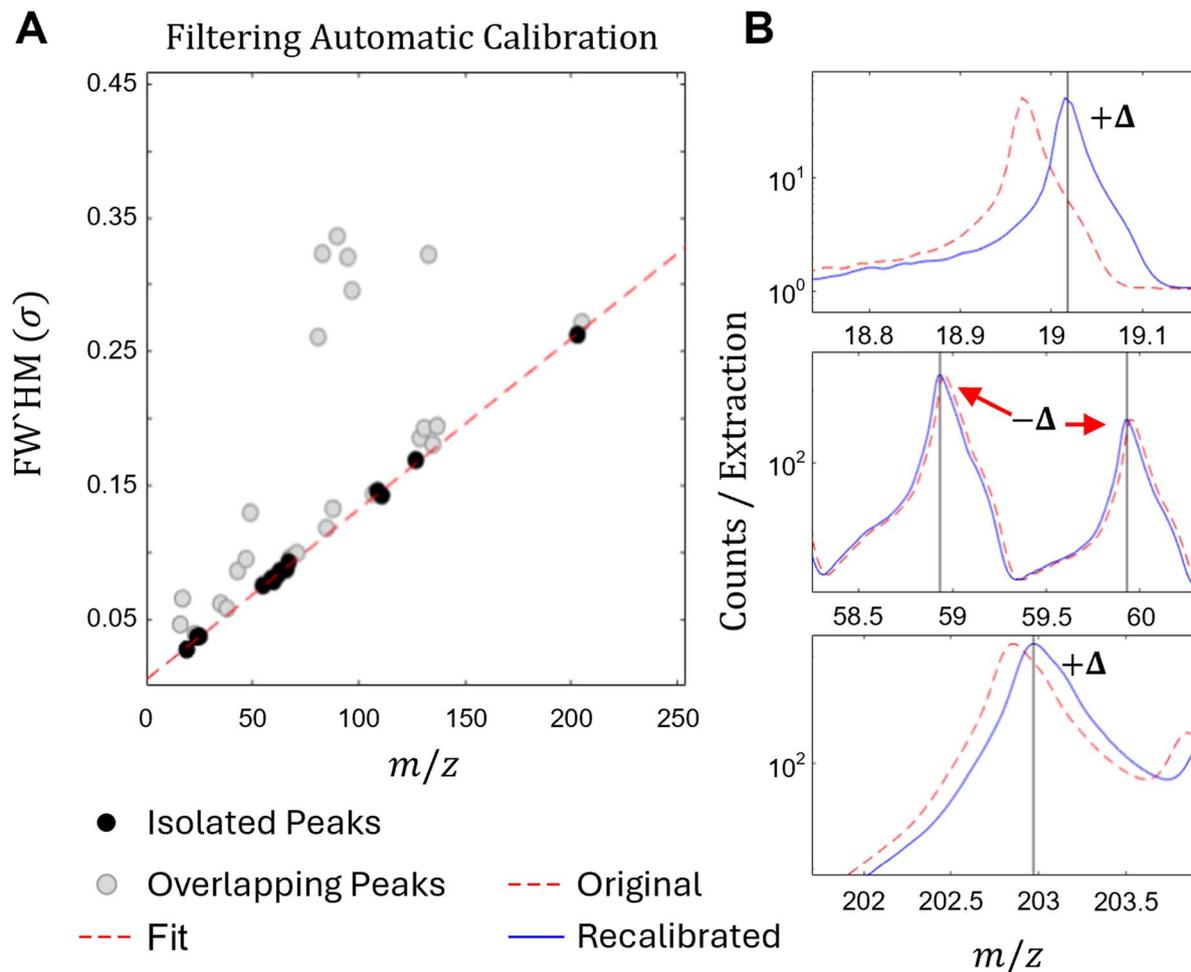


Fig. 4 Final mass calibration. (A) Fitted peak widths are modeled as a function of m/z because isolated ions (in black) should exhibit narrower peak widths than isobars (in grey). This relationship is used to recalibrate the spectra post collection. Using nonlinear optimization with non-negativity constraints, the plot of σ vs. μ is fit to the equation $\sigma = a\mu^2 + b\mu + c$. The peaks used for fitting are black dots with light grey representing peaks that were rejected during analysis. (B) Four different peaks from three different spectral regions (m/z 18.8–19.1, 58.5–60, 202–203.5) comparing the average spectrum pre (red, dashed line) and post drift correction (blue, solid line).

ESI[†]) must also be updated. Therefore, the optimization procedures performed in Section 4.4 are repeated using the new set of P_1 , P_2 , and P_3 .

4.6 Peak profile calculations

4.6.1 Dilation of isolated peak regions. The 10 isolated peak regions, identified in Section 4.5 are adaptively diluted. The left boundary (x_L) of the integration window is initially set at the starting index assigned by the LUT for each identified peak. To adjust this boundary, AutoSpect iteratively examines the mean intensity in a forward window (x_L to x_{L+3}) and a backward window (x_{L-3} to x_L). If the mean intensity in the forward window exceeds that of the backward window, the boundary is shifted leftward by one unit, *i.e.*, $x_L \rightarrow x_{L-1}$. This process continues until the intensity trend reverses or the boundary approaches the lower limit of the spectrum, at which point further shifting is halted, and the final x_L is assigned. Similarly, the right boundary (x_R) is initially set by the LUT and adjusted dynamically. If the mean intensity in the forward

window (x_R to x_{R+3}) is lower than that in the backward window (x_{R-3} to x_R), the boundary is shifted rightward by one unit, *i.e.*, $x_R \rightarrow x_{R+1}$. This adjustment continues until the trend reverses, or the boundary reaches the upper spectrum limit, at which point further shifting ceases, and x_R is set (ESI Section 12[†]).

4.6.2 Constructing an empirical peak center profile look up table. The isolated peak regions spanning the full m/z range are each normalized to an intensity range spanning from 0 to 1. The peaks are then transformed from m/z space into standard deviation space, centered at the fitted centroid μ_0 and scaled by the fitted Gaussian peak width σ :

$$s = \frac{\mu - \mu_0}{\sigma} \quad (12)$$

Each transformed peak is then interpolated onto a fixed standard deviation grid, $s \in [-20, 20]$, with k uniformly spaced points. The peak profiles corresponding to a centroid positioned anywhere on the mass-axis are interpolated across all detector bins using first-order polynomial regression at each s .



coordinate, forming a continuous 2D surface of peak shape profiles. This creates the empirical LUT used below:

- $LUT_y \in \mathbb{R}^{k \times N}$: empirical peak profile intensities in standard deviation space, with each column corresponding to the measured profile at each of the N integer value digital spectral bins.

- $LUT_x \in \mathbb{R}^{(k \times N)}$: empirical peak profile spectral bin indices in standard deviation space, with each column corresponding to the bin coordinate of the corresponding intensity value in LUT_y .

This LUT facilitates accurate, calibration-driven construction of empirical peak shapes during fitting.

4.6.3 Empirical peak center profile *via* LUT interpolation.

Given a desired centroid m/z denoted as $\mu_0 \in \mathbb{R}^m$, for each of m peaks, the corresponding empirical peak shape is retrieved *via* interpolation from the precomputed LUTs. This process involves several variables, an interpolation operator, and a series of transformation steps (ESI Section 13†).

4.6.4 Interpolation procedure.

The empirically determined peak profiles are determined from our LUTs as follows. First, m/z is converted to fractional bin index, \bar{b}_i , using the calibration parameters using eqn (4) and global calibration coefficients (P_1 ,

P_2 , and P_3). Since \bar{b}_i will only extremely rarely be a whole integer (*i.e.*, an exact match to a column of LUT_x and LUT_y), the two nearest corresponding integer bins are blended to generate the intermediate profile corresponding to \bar{b}_i . Then, using x_i and y_i , the peak shape y_i , defined over non-integer spectral bin coordinates x_i , in standard deviation space, is mapped onto the uniform detector bin grid *via* interpolation and then normalized to unit area. This yields $G \in \mathbb{R}^{N \times m}$, the empirical core peak shapes for each centroid $\mu_{0,i}$.

4.6.5 Asymmetric tailing functions.

Visual inspection of the peaks in mass spectra show long tails that extend to low and high m/z by tens of m/z units (Fig. 5B–D). Fig. 6 shows the result of accounting for these tails and the impact they can have on very distant m/z peaks (Table 1). To account for these low and high m/z extended tails, each peak's core shape is extended with asymmetric leading and trailing tails functionally similar to those modeled in X-ray fluorescence microscopy.^{23–25}

Let:

- $\mu \in \mathbb{R}^{N \times 1}$: m/z evaluation points.
- $\sigma \in \mathbb{R}^{1 \times m}$: peak widths.
- $\beta \in \mathbb{R}^{1 \times m}$: tail widths.

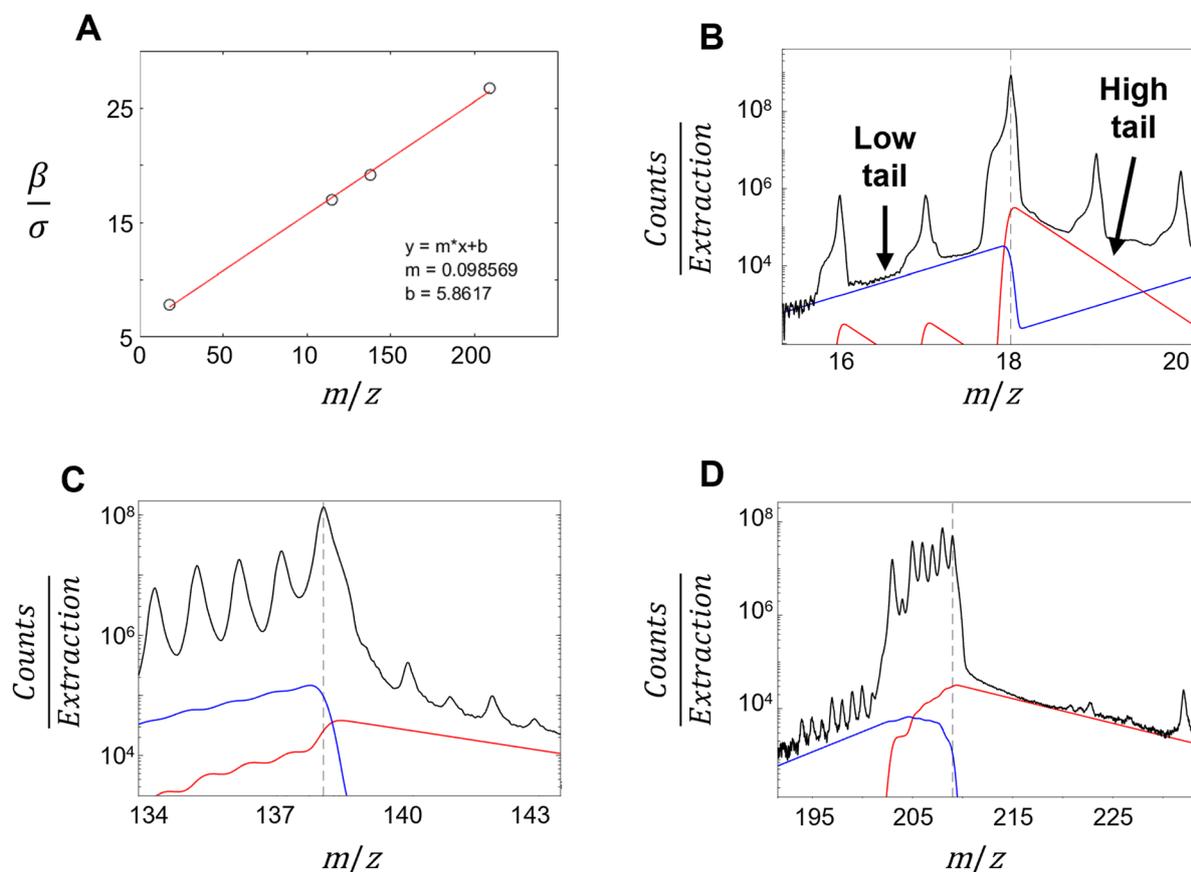


Fig. 5 Peak tailing. (A) High and low peak tails are fitted to an error function and the width (β) is constrained to a ratio of the centroid peak width (σ) fitted by a Lorentzian. The ratio β/σ is constrained to a smooth function of m/z (here we show a 1st order polynomial). (B–D) Shows the calculated high and low peak tails for $^{16}\text{H}_2^{16}\text{O}^+$ (B), $^{138}\text{Ba}^+$ (C), and $^{208}\text{Pb}^+$. Of note, this is the same equation used in X-ray fluorescence to model low energy tailing of the fluorescence peaks caused by inefficient electron capture in the detector, or residual energy. For LA, there is a very steep low m/z but a long trailing high m/z tail. The high m/z is where expected detector or focusing inefficiencies manifest since higher masses arrive later.



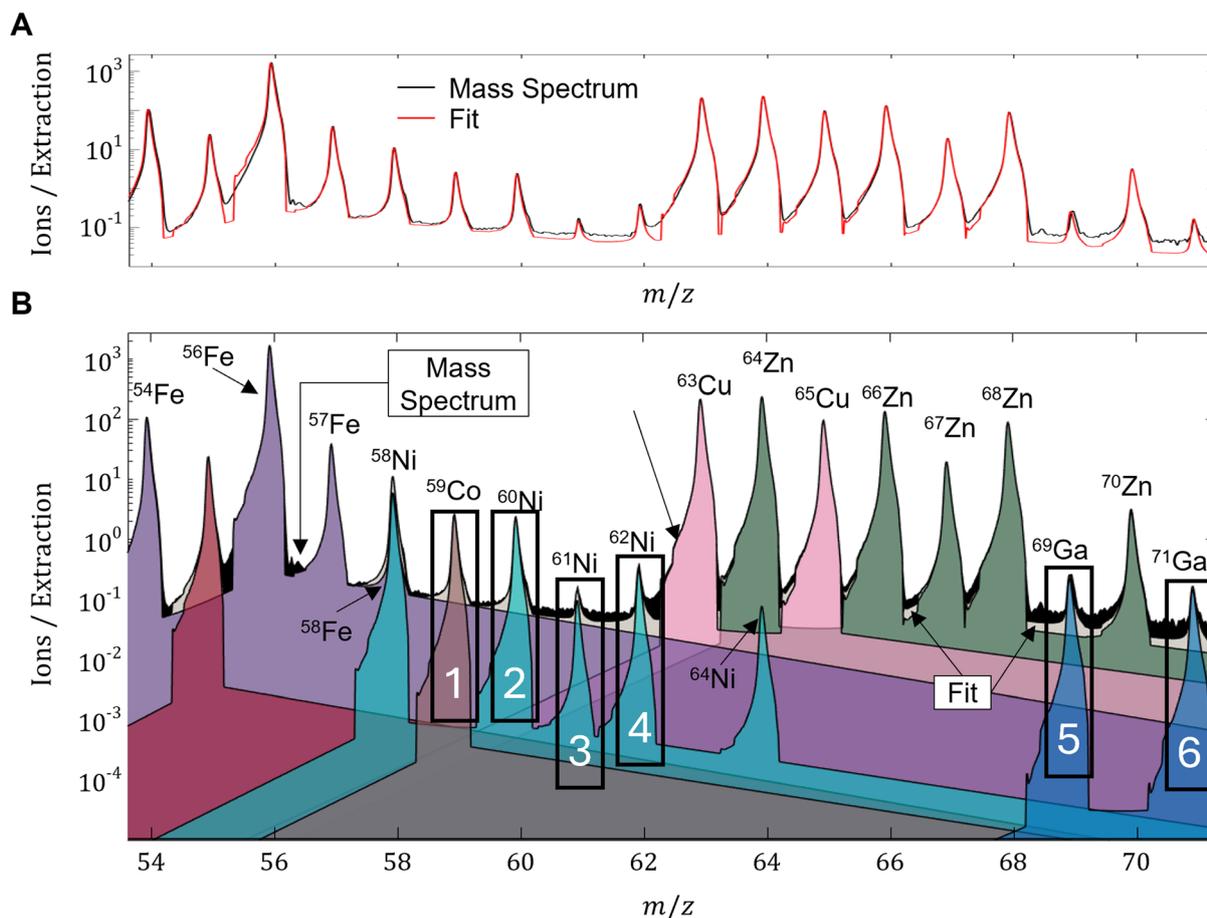


Fig. 6 The importance of tailing in accurately fitting peaks across the spectra. (A) The integrated spectrum fit of a murine brain tissue section. (B) An area plot of the overlapping mass spectrum isotopes from m/z 54 to 71 displayed on a log intensity scale. The spectra were corrected by gas blank measurement and the residual fitted to the parameterized peak profiles automatically determined in AutoSpect. The fit to the empirically determined profiles with isotope ratio branching are shown for Mn, Fe, Co, Ni, Cu, Zn, and Ga. The peak centroids are not fully empirically determined which is why they drop to the low and high m/z tails.

The tails are defined as:

$$T_{\text{low}} = \frac{1}{2} \exp\left(\frac{\mu - \mu_0}{\beta}\right) \operatorname{erfc}\left(\frac{\mu - \mu_0}{\sigma\sqrt{2}} + \frac{\sigma}{\beta\sqrt{2}}\right), \quad T_{\text{high}} = \frac{1}{2} \exp\left(\frac{\mu_0 - \mu}{\beta}\right) \left[\operatorname{erfc}\left(\frac{\mu_0 - \mu}{\sigma\sqrt{2}} + \frac{\sigma}{\beta\sqrt{2}}\right) \right] \quad (13)$$

Each tail matrix is normalized column-wise (eqn (S34), ESI†).

4.6.6 Tail widths constrained by peak width. Tailing widths, β , follow a smooth dependence on peak resolution across the mass range. As such, tail widths are not free parameters; rather, they are scaled by the peak widths according to a first-order polynomial in centroid m/z (ESI Section 15†).

Table 1 The contribution of the various tails to the separate isotope peaks are calculated for six regions identified in Fig. 6. Although the area of any tail negligibly contributes to the quantitative estimates of its parent isotope, these tails have very far-reaching impacts across the data. This can be seen by comparing the relative amplitudes of the various tails with the total peak amplitude for the various isotopes

Region	Peaks Isotope	Intensity	Tails			Percentage of peak intensity		
			Intensity			Percentage of peak intensity		
			Fe	Cu	Zn	Fe	Cu	Zn
0	^{56}Fe	1526	0.2408	—	—	0.02%	—	—
1	^{59}Co	2.526	0.0998	—	—	3.95%	—	—
2	^{60}Ni	2.291	0.0725	—	—	3.16%	—	—
3	^{61}Ni	0.1542	0.0520	0.0027	—	33.74%	1.76%	—
4	^{62}Ni	0.3078	0.0380	0.0092	—	12.33%	2.99%	—
5	^{69}Ga	0.2553	0.0039	0.0106	0.0283	1.52%	4.15%	11.08%
6	^{71}Ga	0.1671	0.0020	0.0063	0.0175	1.22%	3.76%	10.45%



This relationship between β and σ and the strong adherence to a first order relationship can be seen in Fig. 5A which shows the ratio of β/σ as a function of m/z .

4.6.7 Mass-to-charge dependent tail amplitude scaling.

The amplitude of the low- and high- m/z tails are on the order of 0.0001 of the intensity of the parent peak and vary smoothly across the spectrum (ESI Section 16†). This scaling function is applied independently to the low- and high-energy tails to produce the vectors r_{low} and r_{high} , which are then used below during peak shape assembly.

4.6.8 Peak shape combination and normalization. After empirical peak shapes and asymmetric tails have been defined, they are combined into a final asymmetric model, G_T , for each elemental signal. This step ensures that each modeled peak incorporates core instrument resolution and realistic tailing. After combining the core peak with the asymmetric tails, each resulting peak shape $G_T(:,i)$ is normalized such that its total area integrates to one (eqn (S34), ESI†). The resulting matrix $G_T \in \mathbb{R}^{N \times m}$ contains the asymmetric, resolution-constrained, and normalized peak shapes for each spectral signal prior to application of instrumental notching and isotopic branching.

4.6.9 Correction for instrumental notching (Tofwerk-specific). AutoSpect includes an optional correction mechanism specific to Tofwerk TOF-MS instruments, which employ inverse quadrupole filtering, referred to as notching, to reduce the transmission of extremely abundant background ions, such as those arising from argon, nitrogen, water vapor, and other atmospheric components, which would otherwise cause serious detector saturation. This filtering alters the transmission efficiency at selected m/z values, artificially suppressing the observed intensities of certain isotopes and thereby distorting their natural abundance ratios.

To correct for this effect, AutoSpect uses the stored notching parameters from the raw data file to automatically optimize and account for these changes. These values are used to compute a set of scaling factors, referred to as FLOAT, which are applied to the branching ratios of affected isotopes.

4.6.10 Isotopic ratio branching application. Since the isotopes of given elements have very well documented natural abundances, the ratios of the various isotopes for a given element can be used to combine the equations for individual isotopes of a given species into a single equation accounting for the split probabilities of each isotope. If a sample contains isotopic enrichment, that isotope can be disconnected from branching and fitted individually.

To model isotopic structure, each elemental peak in G_T is condensed into one or more isotopic peaks using the notch-corrected branching ratio matrix \tilde{B}_{iso} .

Let:

- $G_T \in \mathbb{R}^{N \times m}$: asymmetric, tailed, normalized elemental peak profiles,
- $\tilde{B}_{\text{iso}} \in \mathbb{R}^{m \times \gamma}$: corrected branching ratio matrix,
- $G_{\text{br}} \in \mathbb{R}^{N \times \gamma}$: final modeled isotope-resolved asymmetric, tailed peak profiles.

Then, the isotopic peak shapes are computed as:

$$G_{\text{br}} = G_T \times \tilde{B}_{\text{iso}} \quad (14)$$

Each column of \tilde{B}_{iso} contains fractional contributions from isotopes of a given element. These are derived from known natural abundances and adjusted to account for notching. Each column is then normalized to unit area (eqn (S34), ESI†). This step allows each species to be represented by a single equation, incorporating all isotopes and correcting for instrument-induced artifacts. It improves both interpretability and robustness in spectral deconvolution, particularly for peaks that are partially resolved or overlapping (Fig. 6).

4.7 Spectral fitting and peak deconvolution

In the final steps of AutoSpect, using the drift calibration and the branched equations defined in the previous sections, the spectra for the samples, gas blanks, and reference standards are fitted to deconvolute peak overlap. Typically, with LA data, the individual pixel spectra are sparsely populated where most of the spectral bins contain zeros. This is especially the case with biological tissues. Because of this, interpolating the pixel spectra into a common grid for drift correction can result in significant errors. To avoid such potential errors, the composite model matrix G_{br} is interpolated to the local drift-corrected mass axis for each partition. Then, prior to spectral fitting, background correction is applied using either measured gas blanks or an automated SNIP-based background estimation algorithm.²⁶ Once the spectra are background corrected and the model matrix is aligned with the measured data, the corrected spectra are deconvolved using standard linear least squares:

$$C_q(:,k) = (\tilde{G}_q^T \tilde{G}_q)^{-1} \tilde{G}_q^T (F_q(:,k) - B_q(:,k)) \quad (15)$$

This yields C_q , a matrix of coefficients for all components (columns of \tilde{G}_q) across all spectra in partition q . Since each column of \tilde{G}_q is normalized to unit area, the resulting coefficients in C_q represent the total extracted counts for each modeled peak component, and no additional normalization or post-processing is required (ESI Section 19†).

Once fitted, AutoSpect copies the original data file and then updates fitted peak data. Since AutoSpect outputs the data in the native TofWerk format, the fitted data can be seamlessly incorporated to any of the existing data reduction pipelines currently in the field using the TofWerk hdf5 structure.

5. AutoSpect use case examples

5.1 Single cell and tissue section imaging

AutoSpect functionality was tested on freshly isolated sea urchin eggs from *Arbacia punctulata*, which have an average diameter of 70 μm . This dataset required \sim around 4.5 hours per sample and exhibited noticeable signal drift resulting from observed peak position drift with potentially contributing factors from instrument drift, ablation drift and transport drift (Fig. 7). For ^{24}Mg , ^{31}P , and ^{66}Zn , the peak drift was quantified as $\frac{m/z}{\Delta(m/z)}$ yielding values of 480, 344, and 507, respectively. This is on the order of 50% the instrument specified resolution. Additional datasets were collected from 10 μm thick sections of epididymis and kidney tissues, which respectively showed low



and high localized abundance of molybdenum, an essential enzymatic cofactor.

AutoSpect was compared to currently existing software for spectral analysis, Tofware, to benchmark performance. A laser ablation dataset of sea urchin eggs was analyzed using both Autospect and Tofware to compare their workflows, speed, and performance. This dataset was chosen due to its large file size, with 987 raster lines of 1305 spots, each 2 μm in size, giving a field of 2610 $\mu\text{m} \times 1974 \mu\text{m}$, and a file size of 9.08 GB. The Tofware workflow totaled 53 min and 24 s, comprising peak shape optimization and peak fitting across 315 masses ranging from $^6\text{Li}^+$ to $^{238}\text{U}^+$ (see Table 2). The analogous peak fitting by Autospect was accomplished in 41 min 50 s. The Autospect workflow took 10 min 14 s to complete drift correction, and an additional 27 s to perform peak profiling, totaling 52 min 31 s for all operations. The resulting fitted laser ablation images and

the original, uncorrected data are shown in Fig. 7. Notably, this dataset has fluctuating $^{24}\text{Mg}^+$, $^{31}\text{P}^+$, $^{66}\text{Zn}^+$ signals arising from time dependent peak centroid drift. The decrease in $^{24}\text{Mg}^+$ for Tofware is a result of the imperfect calibration of the mass axis. This can be seen in Fig. 8 with the spectral partitions projected onto the Tofware mass axis, where the peak centroid for $^{24}\text{Mg}^+$ is shifted further out of focus to higher apparent m/z . For $^{66}\text{Zn}^+$, Tofware improved the mass axis calibration for the latter *ca.* 70% of the image, improving the bottom of the map, but worsening the top. For $^{31}\text{P}^+$, peak broadening in Tofware leads to an inability to separate the $^{31}\text{P}^+$ intensity from that of an apparent unknown satellite gas peak. None of the pitfalls in Tofware are a reflection of the software, rather these reflect the need for a robust and automated mass axis drift correction. As can be seen, when mass axis drift correction is robustly

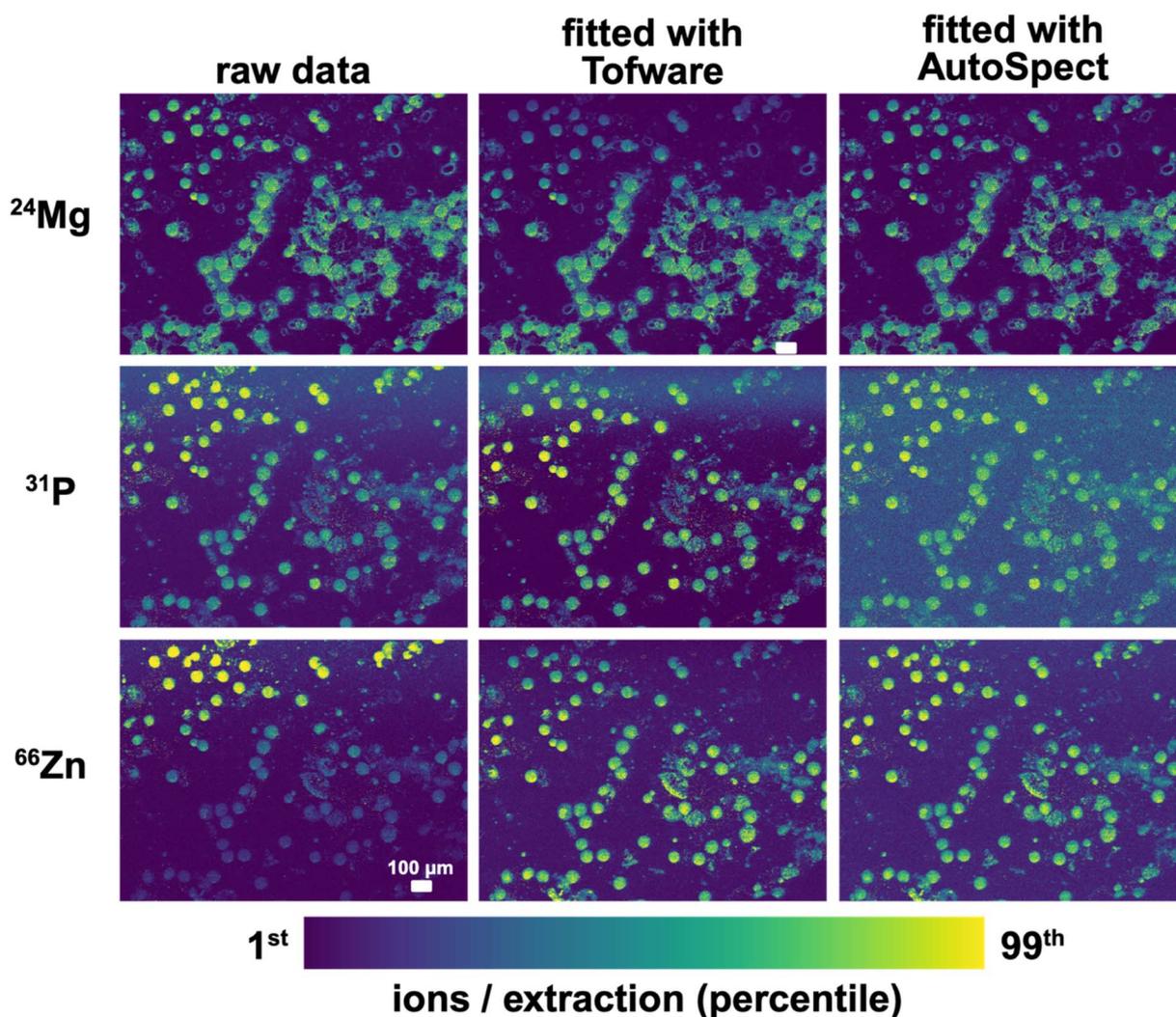


Fig. 7 Comparison of peak fitting and drift correction by AutoSpect *versus* Tofware. Sea urchin eggs were deposited onto Kapton thin film and analyzed by LA-ICP-TOF-MS. The ^{24}Mg , ^{31}P , and ^{66}Zn data are visualized from the 1st to 99th percentile. The resulting, unprocessed data showed localization of ^{24}Mg , ^{31}P , and ^{66}Zn in the eggs (first column). Notably, the ^{31}P and ^{66}Zn signals fluctuate during 4.5 hours of acquisition. When fitted with Tofware, the eggs have better contrast from background in the ^{31}P and ^{66}Zn channels, but all three mass channels show fluctuation (second column). Fitting with AutoSpect can eliminate these artifacts and give a stable response over the course of the experiment (third column).



Table 2 Comparing the data processing tasks and the times needed by AutoSpect and Tofware to complete those tasks. Spectral data processing with AutoSpect and Tofware were performed on the same machine

Data processing task	Time taken by AutoSpect (mm:ss)	Time taken by Tofware (mm:ss)
Dataset 1: sea urchin eggs (experimental scan time = 4:37:15)		
Peak fitting ^a	41:50	53:24
Drift correction	10:14	— ^b
Peak profiling	00:27	— ^b
Total	52:31	53:24
Dataset 2: tissue slide 2 (experimental scan time = 1:10:02)		
Peak fitting ^a	05:17	07:18
Drift correction	03:11	— ^b
Peak profiling	00:15	— ^b
Total	08:43	07:18
Dataset 3: tissue slide 3 (experimental scan time = 1:10:04)		
Peak fitting ^a	06:09	09:12
Drift correction	03:25	— ^b
Peak profiling	00:22	— ^b
Total	09:56	09:12
Dataset 4: tissue slide 5 (experimental scan time = 1:20:54)		
Peak fitting ^a	08:33	11:06
Drift correction	03:42	— ^b
Peak profiling	00:22	— ^b
Total	12:37	11:06

^a Includes data loading and writing tasks. ^b Function not available.

performed, as in AutoSpect, it eliminates these fluctuations and gives a stable response over the course of the experiment.

Another demonstration for AutoSpect involves showing the effectiveness of isotope ratio branching in revealing spatial localization of low isotopic abundance elements such as molybdenum in biological tissues (Fig. 9). Molybdenum acts as an essential metal cofactor to enzymes that participate in redox reactions due to its ability to shuttle between three oxidation states.²⁷ Therefore, detection of molybdenum in biological samples most likely indicate the presence of these enzymes. While molybdenum was detectable using Iolite software, the isotope ratio branching capability of AutoSpect improved signal to noise, allowing for increased accurate assessment of localization within the sample.

6. Discussion

AutoSpect provides an approach that is useful at many levels to LA-ICP-TOF-MS analysis, addressing longstanding challenges in data processing. By automating drift correction and peak profile determination, profiling low and high peak tailing, and fitting spectra, it improves both accuracy and efficiency of analysis. AutoSpect's flexible design allows for adaptation to other fields requiring high-resolution elemental and isotope analyses. Future updates will incorporate additional functionality, such as advanced multiply charged species handling and enhanced matrix-matching algorithms.

The approach employed in AutoSpect, and many of the underlying algorithms, were directly borrowed from or built upon ideas and algorithms developed for X-ray fluorescence

microscopy (XFM).^{28–31} In particular, the implementation of branching ratios, introduction of the low and high m/z tailing, use of directly subtracting the gas blank, and the partitioning and chunking of spectra were adapted from the M-BLANK program used for fitting XFM spectra.

Recalibration of the mass axis: when identifying isolated peaks to calculate the smooth function of peak broadening as a function of m/z , the field largely supports the use of a first order polynomial. However, a second order polynomial was used rather than a first order (ESI Section 10†) as it was found that allowing for subtle curvature adhering to a square component yielded peaks that aligned with their tabulated m/z values across the dynamic range of individual atoms to a much better degree than a slope component alone (Fig. 4A).

Automatic generation of peak profiles: empirical peak profiles are generated based on isolated peaks that are automatically identified by the software and used to create a LUT of all possible peaks contained in the range of the spectra. This ensures accurate representation of spectral features corresponding to the main peak centers. AutoSpect then accounts for instrumental notching effects and models peak tailing. The incorporation of peak tailing and accounting for these tails is quantitatively important, especially concerning the high m/z tailing which persists for tens of m/z . This explains the difficulty of fitting an isotope neighboring another isotope with an intensity that is greater than 4 orders of magnitude larger.

Peak tailing: peak tailing is a new feature that has not been implemented into peak shape modeling of mass spectra. The functional forms have been adapted from XFM for modeling inefficient electron capture in energy-dispersive detectors. In XFM and related XRF systems, only a low-energy tail is observed, corresponding to post-detection charge dissipation—an effect analogous to the high m/z tail observed in TOF. In the context of TOF mass spectrometry, however, an additional low m/z tail emerges, requiring a new physical interpretation. Despite the differing origins, both tails are modeled using mirrored functional forms, and distinct interpretations are warranted for each side of the peak.

High m/z tailing is hypothesized to result from residual charge persisting on the detector, which dissipates over time, analogous to charge retention artifacts in energy dispersive X-ray detectors.^{23–25} This leads to a slowly decaying signal that extends tens of m/z units beyond the peak and must be modeled to avoid misattributing ion counts.

In contrast, the low m/z tail appears to reflect a phenomenon that precedes the actual arrival of the ion at the detector. While it may seem counterintuitive to detect a signal before the particle arrives, electrostatics provides a rationale. As a charged ion approaches the detector, its electric field induces a mirror charge within the conductive surface of the detector, an effect that can be understood using the method of image charges from electrostatics. This induced field, and the resulting current, could plausibly begin to rise before the ion physically reaches the detector. Notably, the slope of this low- m/z tail would depend on ion velocity: heavier ions (higher m/z) move more slowly, resulting in a more gradual leading slope. This



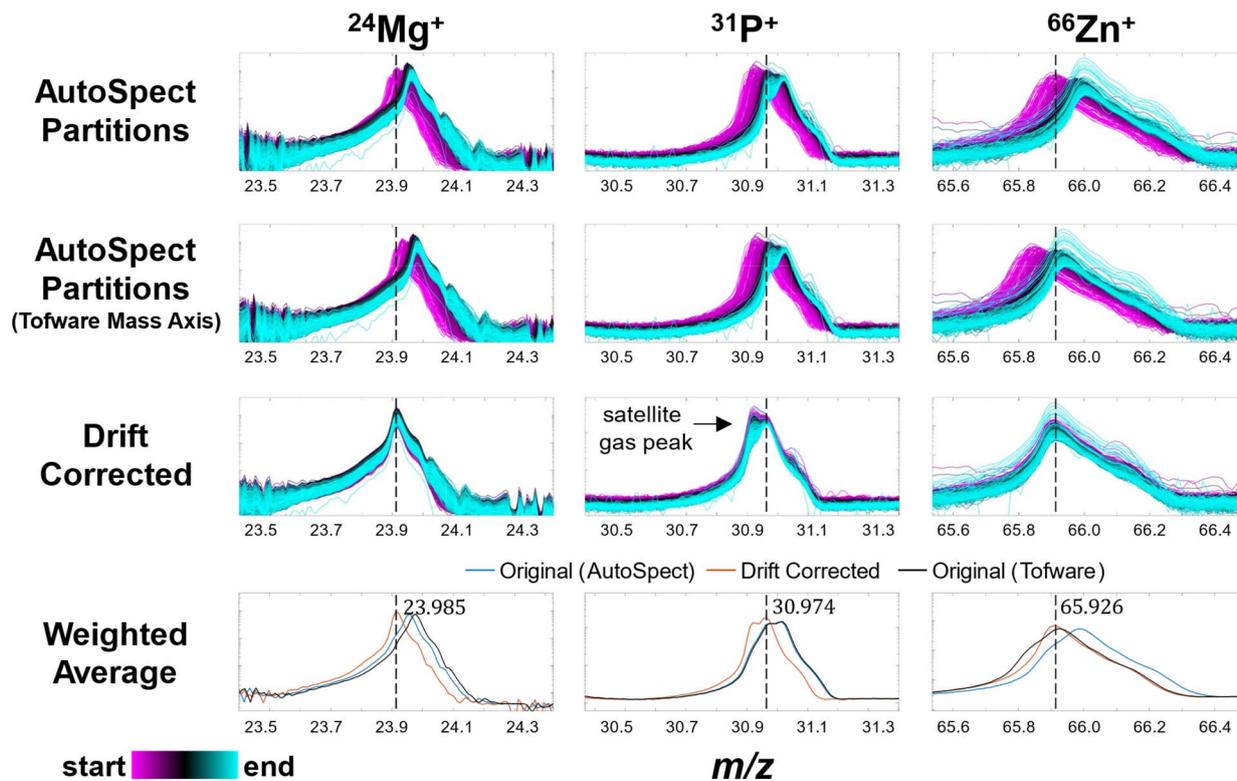


Fig. 8 Spectral analysis of peak fitting and drift correction by AutoSpect and Tofware. The average spectrum for each of the 806 spectral partitions determined in AutoSpect from the sea urchin eggs from Fig. 7 are shown for the three masses $^{24}\text{Mg}^+$, $^{31}\text{P}^+$, and $^{66}\text{Zn}^+$. Row 1 shows the original spectra prior to any drift correction. Row 2 shows the scan partitions from AutoSpect projected onto the mass axis calibration from Tofware. Row 3 shows the spectra from the partitions after drift correction. Row 4 shows the average of the uncorrected spectra projected to the mass axis from AutoSpect (blue) and Tofware (black), along with the average spectrum from the drift corrected (red) spectra from AutoSpect, showing significant changes to the apparent peak position and peak morphology post AutoSpect drift correction.

matches observations from empirical fits, which show shallower low-side tailing for higher masses.

Thus, the peak tailing model captures both a post-arrival dissipation component (high m/z tail) and a pre-arrival induction component (low m/z tail). While both features are needed to accurately model the observed peaks asymmetry, and failure to account for them can significantly impact spectral deconvolution especially in dense or overlapping regions, the proposed explanation should be viewed as speculative at this time.

In TOF-MS it is difficult to reliably quantify a weaker peak that is positioned near a much more intense peak differing by four or more orders of magnitude in intensity. For example, if ^{55}Mn is present at 10 000 counts and ^{56}Fe is only 10 counts, the ^{56}Fe signal is traditionally considered unreliable due to interference from the more intense neighboring peak. Notably, such quantitation has never invoked tailing, as tails had not previously been modeled or recognized as a source of interference in TOF-MS. The identification and modeling of peak tails in AutoSpect represents a new advancement that helps explain and correct this increased noise in the weaker neighboring peak. With the inclusion of explicit tail modeling in AutoSpect, such weaker peaks can now be meaningfully quantified even in the presence of nearby intense signals, challenging this long-standing assumption and extending the quantifiable dynamic range of TOF-MS. This assumption likely stems from historical

limitations in peak modeling that failed to incorporate tailing behavior. The inclusion of accurate tail models in AutoSpect directly challenges this assumption by enabling quantification even in cases of extreme dynamic range and overlap, thereby extending the practical limits of spectral resolution and trace detection.

Building on this, we can examine how tail contributions manifest in real datasets. For example, the contribution from the peak tail for ^{56}Fe is *ca.* 0.02% the amplitude of the main centroid contributing negligibly to the quantitative estimate of ^{56}Fe . However, because LA exists across a dynamic range of 8 to 10 orders of magnitude, these tails can have significant non-negligible impacts on neighboring peaks near and far in unpredictable manners that are sample dependent. For example, comparing the amplitudes of the raw peak and tails present for ^{61}Ni (region 3), 35.5% of the peak amplitude corresponds to the combined contributions from the Cu and Fe tails (Fig. 6). Similarly, 15.32% of the peak amplitude for ^{62}Ni (region 4) corresponds to these two tails. For ^{69}Ga (region 5) and ^{71}Ga (region 6), 16.76% and 15.43% of the peak amplitudes correspond to the combined contributions of the Fe, Cu, and Zn tails. By comparison, the 3.95% and 3.16% contributions to ^{59}Co (region 1) and ^{60}Ni (region 2), are less significant.

Spectral fitting: AutoSpect applies background correction using either gas blanks or a SNIP-based algorithm, with the



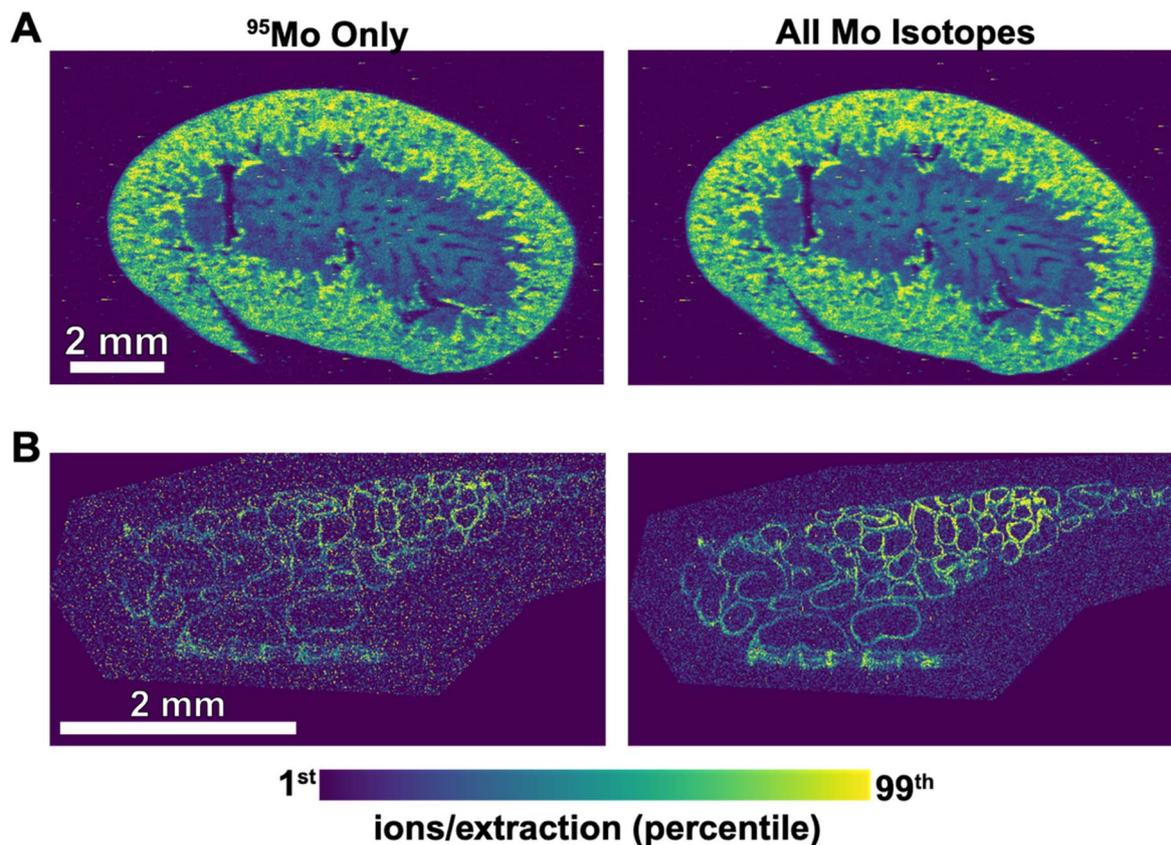


Fig. 9 Isotope ratio branching improves signal to noise for low abundance elements in biological tissue samples. (A) LA-ICP-TOF-MS molybdenum map of a 20 μm thick mouse kidney section. Kidney has naturally high concentrations of Mo and does not benefit as much from isotope ratio branching. However, (B) LA-ICP-TOF-MS of a 20 μm thick mouse epididymis, a male reproduction organ, which has naturally low concentrations of molybdenum shows how mapping using a single isotope (^{95}Mo) has lower signal to noise than if isotope ratio branching (combining other isotopes of Mo with variable abundance), improves signal to noise allowing accurate localization of the element within the tissue.

residual spectra fitted using the generated peak profiles to resolve overlapping peaks and deconvolute interferences. The fitted peak intensities are then saved in the native HDF5 format for compatibility with existing data pipelines allowing further analysis and reporting.

7. Conclusion

AutoSpect represents a significant advancement in the field of LA-ICP-TOF-MS, providing researchers with a robust, automated tool for spectral fitting and data reduction. Case use studies indicate that AutoSpect supports:

- (1) Enhanced spectral deconvolution, resolving interferences with high precision.
- (2) Accurate drift corrections, ensuring consistent results across extended analytical sessions.
- (3) Efficient handling of complex datasets, reducing analysis times significantly compared to manual methods.

By streamlining workflows and addressing critical analytical challenges, AutoSpect empowers users to fully leverage the capabilities of this powerful analytical technique, paving the

way for new discoveries in fields from geology to biology, from medicine to material sciences.

Ethical statement

All animal procedures were conducted in compliance with National Institutes of Health's Guide for the Care and Use of Laboratory Animals³² and were approved by the Institutional Animal Care and Use Committee at Michigan State University (protocol approval number: 202200021). Mice were maintained on a 12 h light/dark cycle with chow and water available *ad libitum*.

Data availability

Data and software are available upon request and can be found at <https://qemap.ehi.msu.edu/resources>.

Author contributions

AMC conceived, designed, developed, wrote, and validated all software, including AutoSpect, InSpect, and affiliated



subroutines, and performed testbed analyses with input from KWM, DZZ, and TVO. AMC also contributed to the interpretation of results and preparation of the methods description. AMC, DZZ, SHA, KWM, TVO wrote the manuscript. DZZ performed software comparisons, isolated samples, collected and analyzed results for the sea urchin data sets. Mouse kidneys were harvested by QJ. KWM, DZZ, SHA, NS, and AS sectioned murine tissues and collected data.

Conflicts of interest

The authors have no conflicts to declare aside from the Auto-Spec copyright which is held by AMC, KWM and TVO at Michigan State University.

Acknowledgements

Metal analysis and quantitative elemental mapping was performed at the Michigan State University Quantitative Bio Element Analysis and Mapping (QBEAM) Center generously supported by the MSU Office for Research and Innovation, the National Institute of General Medical Sciences of the National Institutes of Health award for the resource entitled “Quantitative Elemental Mapping for the Life Sciences” (QE-Map, P41 GM135018) and by the Office of The Director, National Institutes of Health (S10OD026786). D. Z. Z. thanks the National Institute of General Medical Sciences of the National Institutes of Health for a Ruth L. Kirschstein NRSA postdoctoral fellowship (F32GM139401). SHA acknowledges support from National Institute of Child Health and Disease R01 HD100832 for supporting acquisition of mouse epididymal tissue, and TVO acknowledges R01 GM038784 for supporting sea urchin samples. The content of this publication is solely the responsibility of the authors and does not necessarily represent the official views of the National Institutes of Health. The authors thank Dr Andy Drews for suggesting image charge induction as a possible mechanism for low m/z tailing in TOF-MS.

References

- 1 A. Gundlach-Graham, Chapter Three - Multiplexed and Multi-Metal Single-Particle Characterization with ICP-TOFMS, in *Comprehensive Analytical Chemistry*, ed. Milačić R., Ščančar J., Goenaga-Infante H. and Vidmar J., Elsevier, 2021, vol 93, pp. 69–101, DOI: [10.1016/bs.coac.2021.01.008](https://doi.org/10.1016/bs.coac.2021.01.008).
- 2 B. Paul, K. Kysenius, J. B. Hilton, M. W. M. Jones, R. W. Hutchinson, D. D. Buchanan, C. Rosty, F. Fryer, A. I. Bush, J. M. Hergt, J. D. Woodhead, D. P. Bishop, P. A. Doble, M. M. Hill, P. J. Crouch and D. J. Hare, An Integrated Mass Spectrometry Imaging and Digital Pathology Workflow for Objective Detection of Colorectal Tumours by Unique Atomic Signatures, *Chem. Sci.*, 2021, **12**, 10321–10333, DOI: [10.1039/D1SC02237G](https://doi.org/10.1039/D1SC02237G).
- 3 B. Paul, D. J. Hare, D. P. Bishop, C. Paton, V. T. Nguyen, N. Cole, M. M. Niedwiecki, E. Andreozzi, A. Vais, J. L. Billings, L. Bray, A. I. Bush, G. McColl, B. R. Roberts, P. A. Adlard, D. I. Finkelstein, J. Hellstrom, J. M. Hergt, J. D. Woodhead and P. A. Doble, Visualising Mouse Neuroanatomy and Function by Metal Distribution Using Laser Ablation-Inductively Coupled Plasma-Mass Spectrometry Imaging, *Chem. Sci.*, 2015, **6**, 5383–5393, DOI: [10.1039/c5sc02231b](https://doi.org/10.1039/c5sc02231b).
- 4 C. Neff, P. Keresztes Schmidt, P. S. Garofalo, G. Schwarz and D. Günther, Capabilities of Automated LA-ICP-TOFMS Imaging of Geological Samples, *J. Anal. At. Spectrom.*, 2020, **35**, 2255–2266, DOI: [10.1039/DOJA00238K](https://doi.org/10.1039/DOJA00238K).
- 5 D. Z. Zee, K. W. MacRenaris and T. V. O'Halloran, Quantitative imaging approaches to understanding biological processing of metal ions, *Curr. Opin. Chem. Biol.*, 2022, **69**, 102152, DOI: [10.1016/j.cbpa.2022.102152](https://doi.org/10.1016/j.cbpa.2022.102152).
- 6 S. A. Iakab, P. Ràfols, X. Correig-Blanchar and M. García-Altres, Perspective on Multimodal Imaging Techniques Coupling Mass Spectrometry and Vibrational Spectroscopy: Picturing the Best of Both Worlds, *Anal. Chem.*, 2021, **93**, 6301–6310, DOI: [10.1021/acs.analchem.0c04986](https://doi.org/10.1021/acs.analchem.0c04986).
- 7 P. Niehaus, R. Gonzalez de Vega, M. T. Haindl, C. Birkel, M. Leoni, A. M. Birkel-Toegelhofer, J. Haybaeck, S. Ropele, M. Seeba, W. Goessler, U. Karst, C. Langkammer and D. Clases, Multimodal analytical tools for the molecular and elemental characterisation of lesions in brain tissue of multiple sclerosis patients, *Talanta*, 2024, **270**, 125518, DOI: [10.1016/j.talanta.2023.125518](https://doi.org/10.1016/j.talanta.2023.125518).
- 8 L. Hendriks, A. Gundlach-Graham, B. Hattendorf and D. Günther, Characterization of a new ICP-TOFMS instrument with continuous and discrete introduction of solutions, *J. Anal. At. Spectrom.*, 2017, **32**, 548–561, DOI: [10.1039/C6JA00400H](https://doi.org/10.1039/C6JA00400H).
- 9 R. Weiskirchen, S. Weiskirchen, P. Kim and R. Winkler, Software solutions for evaluation and visualization of laser ablation inductively coupled plasma mass spectrometry imaging (LA-ICP-MSI) data: a short overview, *J. Cheminf.*, 2019, **11**, 16, DOI: [10.1186/s13321-019-0338-7](https://doi.org/10.1186/s13321-019-0338-7).
- 10 T. E. Lockwood, L. Schlatt and D. Clases, SPCal – an open source, easy-to-use processing platform for ICP-TOFMS-based single event data, *J. Anal. At. Spectrom.*, 2025, **40**, 130–136, DOI: [10.1039/D4JA00241E](https://doi.org/10.1039/D4JA00241E).
- 11 H. B. Andrews, L. Hendriks, S. B. Irvine, D. R. Dunlap and B. T. Manard, TOFHunter—unlocking rapid untargeted screening of inductively coupled plasma-time-of-flight-mass spectrometry data, *J. Anal. At. Spectrom.*, 2025, **40**, 910–920, DOI: [10.1039/D4JA00331D](https://doi.org/10.1039/D4JA00331D).
- 12 M. J. Cubison and J. L. Jimenez, Statistical precision of the intensities retrieved from constrained fitting of overlapping peaks in high-resolution mass spectra, *Atmos. Meas. Tech.*, 2015, **8**, 2333–2345, DOI: [10.5194/amt-8-2333-2015](https://doi.org/10.5194/amt-8-2333-2015).
- 13 H. Stark, R. L. N. Yatavelli, S. L. Thompson, J. R. Kimmel, M. J. Cubison, P. S. Chhabra, M. R. Canagaratna, J. T. Jayne, D. R. Worsnop and J. L. Jimenez, Methods to extract molecular and bulk chemical information from series of complex mass spectra with limited mass resolution, *Int. J. Mass Spectrom.*, 2015, **389**, 26–38, DOI: [10.1016/j.ijms.2015.08.011](https://doi.org/10.1016/j.ijms.2015.08.011).



- 14 H. Timonen, M. Cubison, M. Aurela, D. Brus, H. Lihavainen, R. Hillamo, M. Canagaratna, B. Nekat, R. Weller, D. Worsnop and S. Saarikoski, Applications and limitations of constrained high-resolution peak fitting on low resolving power mass spectra from the ToF-ACSM, *Atmos. Meas. Tech.*, 2016, **9**, 3263–3281, DOI: [10.5194/amt-9-3263-2016](https://doi.org/10.5194/amt-9-3263-2016).
- 15 V. A. Petyuk, N. Jaitly, R. J. Moore, J. Ding, T. O. Metz, K. Tang, M. E. Monroe, A. V. Tolmachev, J. N. Adkins, M. E. Belov, A. R. Dabney, W.-J. Qian, D. G. Camp and R. D. Smith, Elimination of Systematic Mass Measurement Errors in Liquid Chromatography–Mass Spectrometry Based Proteomics Using Regression Models and a Priori Partial Knowledge of the Sample Content, *Anal. Chem.*, 2008, **80**, 693–706, DOI: [10.1021/ac701863d](https://doi.org/10.1021/ac701863d).
- 16 I. V. Chernushevich, A. V. Loboda and B. A. Thomson, An introduction to quadrupole–time-of-flight mass spectrometry, *J. Mass Spectrom.*, 2001, **36**, 849–865, DOI: [10.1002/jms.207](https://doi.org/10.1002/jms.207).
- 17 C. Paton, J. Hellstrom, B. Paul, J. Woodhead and J. Hergt, Iolite: Freeware for the visualisation and processing of mass spectrometric data, *J. Anal. At. Spectrom.*, 2011, **26**, 2508–2518, DOI: [10.1039/C1JA10172B](https://doi.org/10.1039/C1JA10172B).
- 18 B. Paul, C. Paton, A. Norris, J. Woodhead, J. Hellstrom, J. Hergt and A. Greig, CellSpace: A module for creating spatially registered laser ablation images within the Iolite freeware environment, *J. Anal. At. Spectrom.*, 2012, **27**, 700–706, DOI: [10.1039/C2JA10383D](https://doi.org/10.1039/C2JA10383D).
- 19 B. Paul, J. Petrus, D. Savard, J. Woodhead, J. Hergt, A. Greig, C. Paton and P. Rayner, Time resolved trace element calibration strategies for LA-ICP-MS, *J. Anal. At. Spectrom.*, 2023, **38**, 1995–2006, DOI: [10.1039/D3JA00037K](https://doi.org/10.1039/D3JA00037K).
- 20 S. H. Ahn, K. Halgren, G. Grzesiak, K. W. MacRenaris, A. Sue, H. Xie, E. Demireva, T. V. O'Halloran and M. G. Petroff, Autoimmune regulator deficiency causes sterile epididymitis and impacts male fertility through disruption of inorganic physiology, *bioRxiv*, 2025, preprint, 2025.2001.2011.632558, DOI: [10.1101/2025.01.11.632558](https://doi.org/10.1101/2025.01.11.632558).
- 21 V. D. Vacquier, Laboratory on sea urchin fertilization, *Mol. Reprod. Dev.*, 2011, **78**, 553–564, DOI: [10.1002/mrd.21360](https://doi.org/10.1002/mrd.21360).
- 22 M. Folk, G. Heber, Q. Koziol, E. Pourmal and D. Robinson, An overview of the HDF5 technology suite and its applications, in *Proceedings of the EDBT/ICDT 2011 Workshop on Array Databases*, Association for Computing Machinery, Uppsala, Sweden, 2011, pp. 36–47.
- 23 B. Vekemans, K. Janssens, L. Vincze, F. Adams and P. Van Espen, Analysis of X-ray spectra by iterative least squares (AXIL): New developments, *X-Ray Spectrom.*, 1994, **23**, 278–285, DOI: [10.1002/xrs.1300230609](https://doi.org/10.1002/xrs.1300230609).
- 24 J. L. Campbell and J. A. Maxwell, A cautionary note on the use of the Hypermet tailing function in X-ray spectrometry with Si(Li) detectors, *Nucl. Instrum. Methods Phys. Res., Sect. B*, 1997, **129**, 297–299, DOI: [10.1016/S0168-583X\(97\)00229-2](https://doi.org/10.1016/S0168-583X(97)00229-2).
- 25 J. L. Campbell, A. Perujo and B. M. Millman, Analytic description of Si(Li) spectral lineshapes due to monoenergetic photons, *X-Ray Spectrom.*, 1987, **16**, 195–201, DOI: [10.1002/xrs.1300160503](https://doi.org/10.1002/xrs.1300160503).
- 26 C. G. Ryan, E. Clayton, W. L. Griffin, S. H. Sie and D. R. Cousens, SNIP, a statistics-sensitive background treatment for the quantitative analysis of PIXE spectra in geoscience applications, *Nucl. Instrum. Methods Phys. Res., Sect. B*, 1988, **34**, 396–402, DOI: [10.1016/0168-583X\(88\)90063-8](https://doi.org/10.1016/0168-583X(88)90063-8).
- 27 G. Schwarz, R. R. Mendel and M. W. Ribbe, Molybdenum cofactors, enzymes and pathways, *Nature*, 2009, **460**, 839–847, DOI: [10.1038/nature08302](https://doi.org/10.1038/nature08302).
- 28 A. M. Crawford, N. J. Sylvain, H. Hou, M. J. Hackett, M. J. Pushie, I. J. Pickering, G. N. George and M. E. Kelly, A comparison of parametric and integrative approaches for X-ray fluorescence analysis applied to a Stroke model, *J. Synchrotron Radiat.*, 2018, **25**, 1780–1789, DOI: [10.1107/S1600577518010895](https://doi.org/10.1107/S1600577518010895).
- 29 A. M. Crawford, A. Deb and J. E. Penner-Hahn, M-BLANK: a program for the fitting of X-ray fluorescence spectra, *J. Synchrotron Radiat.*, 2019, **26**, 497–503, DOI: [10.1107/S1600577519000651](https://doi.org/10.1107/S1600577519000651).
- 30 A. M. Crawford, B. Huntsman, M. Y. Weng, O. Ponomarenko, C. D. Kiani, S. J. George, G. N. George and I. J. Pickering, Abridged spectral matrix inversion: parametric fitting of X-ray fluorescence spectra following integrative data reduction, *J. Synchrotron Radiat.*, 2021, **28**, 1881–1890, DOI: [10.1107/S1600577521008419](https://doi.org/10.1107/S1600577521008419).
- 31 A. M. Crawford, X-Ray Fluorescence Data Analysis Using A Blank Correction Approach, in *Advances in X-Ray Analysis (AXA)*, Lombard IL, United States; 2019, vol 63, pp. 180–193.
- 32 National Research Council (US) Committee for the Update of the Guide for Care and Use of Laboratory Animals, *Guide for the Care and Use of Laboratory Animals: Eighth Edition*, The National Academies Press, Washington DC, United States, 8th edn, 2011, DOI: [10.17226/12910](https://doi.org/10.17226/12910).

