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Direct measurement of PFAS levels in surface water using an engineered biosensor

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Per- and polyfluoroalkyl substances (PFAS) are a large set of emerging contaminants pervasive in the environment due to amphiphilic properties and strong carbon-fluorine bonds resistant to biodegradation. With an ever-increasing prevalence, the need for precise detection of these chemicals at low levels in drinking water is clear. However, ground and surface water as well as soil and other biosolids have become reservoirs for PFAS at extremely high levels. In fact, PFAS concentrations at part per billion and part per million levels are found in environmental samples taken near high contamination sites including industrial facilities and military bases. In this work, we demonstrate the application of a biosensor based on human liver fatty acid binding protein to detect perfluorooctanoic acid (PFOA) in surface water samples taken near Loring Airforce Base. We show this sensor can detect the high levels of PFOA found in the samples quickly and easily without the use of extensive sample pre-treatment or analytical methods. Therefore, we hope the future of this technology will better assess PFAS detection needs for a multitude of end point users.

Sustainability spotlight

Per and polyfluoroalkyl substances (PFAS, otherwise known as 'forever chemicals') are omnipresent in our lives, where they accumulate in water, soil, crops, animals and us. Currently, PFAS are considered unsafe at any detectable level by the US EPA. We have developed fluorescent biosensors to detect these chemicals in water samples, and in our current study, demonstrate their use in a range of environmental water samples. Approaches such as ours are needed to provide rapid, on-site testing to identify samples that require LC-MS/MS for subsequent, detailed chemical analysis. It also provides key testing to help identify environmental sources of PFAS and mitigate their spread in the environment.

Introduction

PFAS (per-/polyfluoroalkyl substances) are a group of environmental and toxicological contaminants of increasing concern. Since their development in the 1940s, over 3000 variants of PFAS have been manufactured and have entered the global market for use in industrial and consumer applications.[1,2] While their fluorinated carbon chains and polar head moieties impart the oil and water repellence ideal for industrial surfactants as well as consumer goods,[3–6] the unparalleled chemical stability of environmental end products like perfluoroalkyl acids (PFAAs) allow for extreme environmental accumulation.[4,7] Accumulation of these recalcitrant PFAS like perfluorooctanoic acid (PFOA) and perfluorooctane sulfonic acid (PFOS) has become increasingly prevalent in humans[8–10] and has been linked to a variety of health effects including endocrine dysfunction, thyroid, pancreatic, and liver diseases,[9,11–13] as well as a variety of reproductive issues and cancers.[9,14–17]

In recent years many new regulations have been developed and proposed to ensure strict limits on PFAS in drinking water.[18–20] Therefore, detection of these contaminants at the extremely low (part per trillion) levels relevant for drinking water has become a growing priority for researchers. However, it is important to note that human exposure to these chemicals occurs through multiple avenues including food ingestion as well as general contact.[1,4] Specifically, it is becoming increasingly relevant to be able to quickly and easily detect the presence of PFAS in the soil and groundwater around sites with large amounts of these types of contaminants.[21–23] High levels of PFAS pollution are common near manufacturing sites as well as areas utilizing fluorinated AFFFs. In fact, PFOA and PFOS have been found in part per million (ppm) levels in surface and ground water.[22–24]

In this study we aim to show the feasibility of a protein-based biosensor to detect spiked concentrations of PFAS in complex groundwater samples collected in Aroostook County, Maine. Loring Air Force base is located in the town of Limestone within

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Aroostook County and is an EPA Superfunds site known to be contaminated with low levels of PFAS and other common co-contaminants including waste oils, fuels, and spent solvents.[25] Adjacent to this site are the Mi'kmaq Nation Trust Lands as well as the Aroostook National Wildlife Refuge;[26] prior studies have investigated use of phytoremediation to remove PFAS from soils at Loring AFB, and recent testing has detected PFAS in drinking water in Aroostook County.[27,28] Our prior work developing and benchmarking an acrylodan [6-acryloyl-2-dimethylaminonaphthalene] labeled biosensor based on human liver fatty acid binding protein (hLFABP) enabled detection of PFOA and PFOS in spiked creek water samples with limits of detection in the hundreds of parts per billion.[29] In this study we demonstrate the sensor can detect spiked PFOA in complex ground water samples collected adjacent to Loring AFB with minimal sample preparation in agreement with independent LC/MS-MS testing for PFAS using method EPA 1633.[25] These results provide an important initial validation of our biosensor to augment LC/MS-MS testing and demonstrates the use of engineered biosensors for rapid detection of environmental contaminants.

Materials and methods

Sample collection

Samples were collected in June of 2021 onsite in Aroostook County, ME and shipped to University of Virginia. Surface water samples were spiked with PFOA and filtered using a 0.2 μm polypropylene filter to remove particulates before biosensor application and shipment to Cyclopure for quantitative analysis through LC-MS-MS.

LC/MS-MS quantification

Filtered samples were diluted as needed in sterile, ultrapure water. PFAS levels in filtered, diluted samples were measured using the Water Test Kit Pro (Cyclopure). The Water Test Kit utilizes DEXSORB® in passive sampling to collect PFAS. After sample application, the filter kits were shipped back to Cyclo-pure for analysis as outlined on their website (**https://www.cyclopure.com/**). Briefly, standard solid-phase extraction was used to recover PFAS, and the eluted samples were analyzed through HPLC-MS-MS (QExactive Orbitrap, ThermoFisher). The lab utilizes isotope dilution for measurement and quantification of 55 PFAS validated to the requirements of EPA methods 533, 537 and 1633. The limit of quantification (LOQ) is 1.0 ng L^{-1} for all PFAS except GenX which is 2.0 ng L^{-1}.

Sensor production

Acrylodan labeled hLFABP (Ac-hLFABP) was produced as previously described.[29] Briefly, the single cysteine containing hLFABP F50C/C69S mutant was expressed *via* the pET28a(+) vector in *E. coli* BL21 (DE3). Cells were grown in LB media with kanamycin (50 μg mL^{-1}) at 37 °C and induced with *via* addition of 1 mM isopropyl β-D-1-thiogalactopyranoside (IPTG). After 18 hours of expression at 20 °C, cells were harvested *via* centrifugation, resuspended in lysis buffer (50 mM Tris–Cl, 100 mM NaCl, 5% v/v glycerol, pH 8), and lysed by sonication. hLFABP F50C/C69S was purified from the clarified lysate by nickel affinity chromatography using Chelating Sepharose Fast Flow resin (Cytiva). Protein was eluted using increasing concentrations imidazole (10–500 mM), and protein containing fractions were dialyzed against PBS (pH 7.5). The N-terminal hexahistidine tag was then cleaved using a Thrombin CleanCleave Kit (Sigma-Aldrich). After cleavage, the protein was conjugated with acrylodan [6-acryloyl-2-dimethylaminonaphthalene] at a 2.5 : 1 fluorophore to protein molar ratio in denaturing conditions (8 M urea) overnight at room temperature with gentle agitation. Removal of unreacted acrylodan and refolding of the denatured protein was performed through an on-column, step-down, urea gradient. Labeled protein was loaded onto nickel charged Chelating Sepharose Fast Flow resin (Cytiva) and washed with 10 column volumes of 50 mM Tris–Cl buffer (pH 8) containing continually decreasing urea concentrations. Properly folded Ac-hLFABP was removed using 500 mM imidazole, and once again dialyzed into PBS (pH 7.6). Protein concentration was found using a BCA protein assay (Pierce), and acrylodan concentration was measured by absorption at 370 nm (extinction coefficient 16 400 M^{-1} cm^{-1}).[30] The degree of labeling for acrylodan conjugated C69S/F50C hLFABP was 1.0.

Assay

Fluorescence measurements were performed using a Synergy Neo2 Hybrid Multi-Mode Microplate Reader (Biotek) at room temperature and under steady state conditions. Calibration curves and sample data were collected as previously described.[29] Calibration curves were generated by titrating PFOA in deionized water into Ac-hLFABP in PBS (pH 7.6) to a final micromolar ratio of 100 : 1 ligand to sensor respectively. Samples and standards were allowed to equilibrate for 5 minutes before fluorescence spectra were recorded over 400–600 nm after excitation at 360 nm. Signal was quantified as the shift in fluorescence spectra calculated as the change in the average center of mass (Δx_{cm}) from 400 to 460 nm (eqn (1)). Calibration curve data was fit to a four-parameter log dose response model (eqn (2)), and sample PFOA concentrations were interpolated using the obtained fit parameters: Hillslope coefficient (HS), minimum and maximum signal ($\Delta x_{cm,min}$ & $\Delta x_{cm,max}$), and half maximal effective concentration (EC50).

$$x_{cm} = \frac{\sum_{i=l_1}^{l_2} I_i x_i}{\sum_{i=l_1}^{l_2} I_i} \qquad (1)$$

$$\Delta x_{cm} = \Delta x_{cm,min} + \frac{[\text{PFOA}]^{HS} \times (\Delta x_{cm,max} - \Delta x_{cm,min})}{\Delta x_{cm}^{HS} + \text{EC50}^{HS}} \qquad (2)$$

Results and discussion

The developed protein-based biosensor utilizes human liver fatty acid binding protein (hLFABP) as a PFAS-binding scaffold.[29] hLFABP is one of a family of fatty acid binding proteins

expressed cytosolically in various parts of the body with the responsibility of binding and shuttling fatty acids and other hydrophobic ligands.[31] While all fatty acid binding proteins are comprised of hydrophobic β barrel binding regions, hLFABP is the only protein in the family capable of binding two cognate ligands; one in the large binding pocket and one close to an outer binding region as described in detail by others.[32,33]

hLFABP is upregulated in response to PFOA exposure and has also been shown to bind several PFAS variants with moderate affinity due to their structural similarity to endogenous fatty acids.[31,34,35] Furthermore, molecular dynamics and binding studies have concluded that these fluorinated ligands, much like fatty acids, are stabilized through hydrophobic interactions along the inner binding pocket as well as electrostatic interactions with the charged head group of the ligands in a "head-out" mode.[34,36] This mode of binding is further supported as work has shown higher binding affinity of longer chain PFAS indicating increased hydrophobic stabilization.[34,36,37]

We previously described the binding of several PFAS to hLFABP through the introduction of tryptophan into multiple places along the inner binding pocket, and demonstrated the ability of the 50th residue to act as a probe for binding.[29]

By introducing a thiol conjugated solvatochromic fluorophore (acrylodan) at the 50th residue position within the ligand binding pocket, the hLFABP mutant F50C/C69S is capable of binding several PFAS including PFOA while producing a dose dependent blue-shift in acrylodan emission spectra. This shift in emission spectra to higher energy wavelengths occurs due to a polarity change in the acrylodan microenvironment upon ligand binding. The spectral shift is then quantified as the change in peak center of mass (Δx_{cm}).

Aqueous fire-fighting foams (AFFFs), such as those found at Loring AFB, can consist of over 50 different PFAS ranging from C2–C12 in length as well as many fluorotelomers that act as precursors to PFAAs such as PFOA and PFOS.[7,38,39] Wide use of AFFF chemicals at military bases during training, emergency responses, and equipment maintenance make these sites high risk for PFAS contamination.[38,39] In fact, AFFF fluorotelomers as well as perfluorocaboxylates and perfluorosulfonates of varying chain sizes have been found at multiple U.S. military sites, sometimes even reaching part per million levels in groundwater,[21,22,40–42] and are known to have extremely high transport potential.[38,43,44]

Like many other military sites, Loring AFB was a site of known contamination with many hazardous toxins including PFAS, and in the years following the base's deactivation, it remains a EPA Superfunds cleanup site.[25,45] Recently, concerns have been raised about persistent contamination based on PFAS found in drinking water in Aroostook County as well as in agricultural soils on land belonging to the Mi'kmaq; one potential source of this contamination is from overuse of fire-fighting foams that contain PFAS.[27] Over 70 different types of PFAS have been detected in soil samples around the Loring AFB, with sulfonic and carboxylic acids being the primary contaminants at concentrations of up to 150 ppb in soil.[45] A recent test of area schools in Aroostook County show unsafe levels of both lead and PFAS in drinking water.[28,46]

Fig. 1 Illustration of collection sites near (A) Chapman pit and (B) Malabeam Lake. The left panel depicts the area around Loring Airforce Base with an approximation of the Aroostook National Wildlife Refuge overlaid in white.

As a previous Superfunds site, the Loring base was identified as having soil and groundwater containing contaminates including volatile organic compounds (VOCs), polychlorinated biphenyls (PCBs), polyaromatic hydrocarbons (PAHs), pesticides, metals, and other petroleum related compounds. Therefore, we believe it to be important to show feasibility of PFAS detection using this biosensor in complex samples containing other co-contaminants.[25] Even among AFFFs, formulations include various hydrocarbon surfactants, polymers, and organic solvents amongst the fluorinated chemicals.[47–49] To demonstrate our biosensor's utility in this type of application setting, we measured total signal for PFAS binding in spiked samples collected adjacent to the Loring AFB as well as in major waterways such as the Aroostook River. Fig. 1 illustrates the sites where samples were collected. Based on LC/MS-MS analysis, all samples contained primarily PFOA as expected accounting for ~93 and ~60% of the total PFAS measured for sites A and B respectively. PFHxS was also found at high levels and accounted for ~37% of total PFAS measured at site B. PFHxS was commonly used in AFFF, and PFOA is one of the most abundant PFAS found in the environment, and often is a breakdown product formed from higher molecular weight PFAS. The results of the LC/MS-MS data are summarized in Table 1. Our previous

Table 1 Results of surface water samples from LC/MS-MS. Verified concentrations are in ng L^{-1} with LOQ defined as limit of quantification

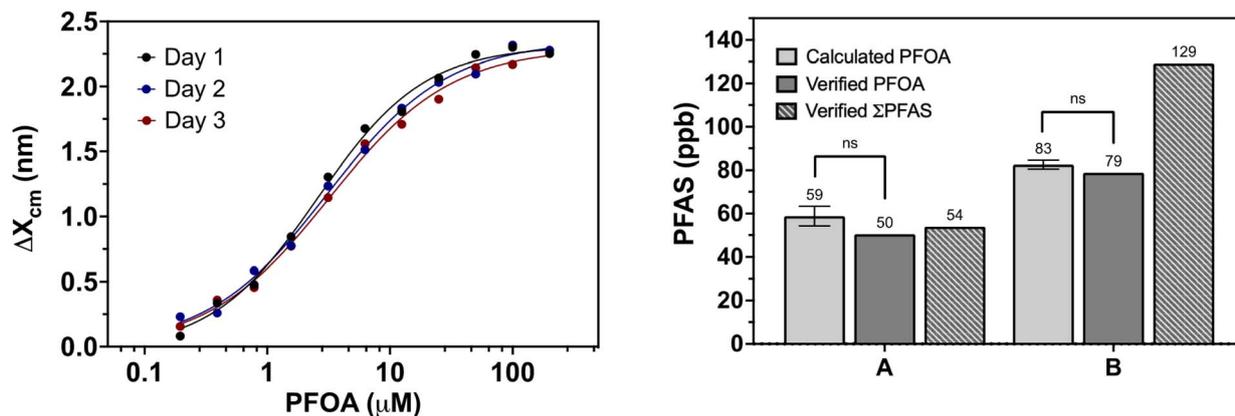| PFAS (ng L^{-1})	Chapman pit (A)	Malabeam lake (B)
PFBA	<LOQ	<LOQ
PFPeA	112.50	<LOQ
PFHxA	183.75	47.73
PFHpA	1417.50	202.27
PFOA	50 477.50	78 840.91
PFNA	<LOQ	<LOQ
PFDA	86.25	<LOQ
HFPO-DA (GenX)	<LOQ	<LOQ
PFBS	268.75	831.82
PFHxS	581.25	47 920.45
PFOS	881.25	1379.55
∑PFAS	54 008.75	129 222.73

Fig. 2 (Left) Sensor calibration curves for varying PFOA concentrations spiked in water. Data from these spiked standards were fit to a four-parameter log−dose response model, and water sample concentrations were calculated using the parameters obtained from the non-linear regression for each day the analysis was performed. (Right) Comparison of predicted and verified concentrations of PFOA and total PFAS in parts per billion (ppb) for surface water samples. The calculated concentrations are mean values $\pm$ SE with $n = 3$.

work showed the biosensor is most sensitive to PFOA at <1 ppm levels unlike PFHxS at greater than >1 ppm levels.[29] Therefore, we prepared standards containing solely PFOA to calibrate the biosensor, determine apparent signal from PFAS binding in environmental samples, and compare to LC/MS-MS results.

The left panel of Fig. 2 shows the calibration curves of the assay replicates utilized for sample PFOA quantification. These data were fit to four-parameter log-dose response models where Hillslope coefficient (HS), minimum and maximum signal ($\Delta x_{cm,min}$ & $\Delta x_{cm,max}$), and half maximal effective concentration (EC50) constants were derived. Three separate sets of derived constants were used for quantifying PFOA concentration in the water samples rather than an average amongst the replicates to gauge concentrations more accurately in lower PFOA containing samples and reduce day to day error.

The results of LC/MS-MS indicated samples A and B contained 50 and 79 ppb PFOA respectively. Based on our calibration curve using PFOA, from our biosensor measurements we obtained values of 59 $\pm$ 5 ppb and 83 $\pm$ 2 ppb for these samples. One sample *t*-tests were conducted to determine statistical similarity between the calculated PFOA concentration and verified analytical value for both samples. Obtained *p*-values were 0.208 and 0.206 for samples A and B respectively showing differences in PFOA concentrations obtained through biosensor measurements and HPLC/MS-MS analysis are not statistically significant. This provides further evidence that the biosensor is robust to environmental testing and can be used for direct determination of PFOA.

PFOA was the main contaminant found in sample A which was taken from Chapman Pit. Along with PFOA, sample B, taken from Malabeam Lake, also contained 48 ppb PFHxS, a 6-carbon sulfonated perfluoroalkyl acid. The ability of the biosensor to detect PFOA in this sample with relative accuracy but not PFHxS indicates a selectivity for the 8-carbon chain carboxylic acid contaminant. This is consistent with prior work that suggests shorter chain PFAS like PFHxS, when bound to the inner binding pocket of hLFABP, provides less available contact area for specific interactions and stabilization.[29,37]

It is important to note challenges with sample variability; for surface water, constituents including organic matter and other co-contaminants can interfere with PFAS detection. Our prior work demonstrated that representative surfactants such as SDS which bind hLFABP do not interfere with PFAS detection.[29] Furthermore, this testing on complex spiked field samples with limited sample pre-processing generated results consistent with independent LC/MS-MS detection. Future applications of this biosensor will focus on further analysis of how other pollutants or compounds might interfere with PFAS detection beyond those tested to date.

Conclusions

Overall, this study provides evidence that an engineered, protein-based biosensor can be used to detect PFAS in field samples using fluorescence readout with minimal pre-processing. With recent studies indicating widespread and significant PFAS levels in soils, water, agricultural products, food, consumer products and the human body, a multi-faceted approach to PFAS detection is needed. As illustrated in this work, biosensors have the advantage of straightforward implementation with reduced sample pre-processing; as such, they can serve as a useful initial screen for contamination to augment more sophisticated, detailed detections methods such as LC/MS-MS. As more studies show that PFAS levels in surface water and soils can reach levels greater than parts per trillion (ppt), it is also important to develop testing methods able to give reliable results in this concentration range that are cost-effective and readily available. As mentioned above, our current efforts are focused on understanding how other pollutants or environmental compounds impact detection, as well as extending detection to other compounds often found where PFAS contamination is present.

Data availability

The data supporting this article has been included in the manuscript.

Author contributions

Conflicts of interest

There are no conflicts to declare.

Acknowledgements

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