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## Photoresponsive hydrogel friction†

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Photoresponsive hydrogels are an emerging class of stimuli-responsive materials that exhibit changes in physical or chemical properties in response to light. Previous investigations have leveraged photothermal mechanisms to achieve reversible changes in hydrogel friction, although few have focused on photochemical means. To date, the tribological properties of photoswitchable hydrogels (e.g., friction and lubrication) have remained underexplored. In this work, we incorporated photoresponsive methoxy-spiropyran-methacrylate monomers (methoxy-SP-MA) into a hydrogel network to form a copolymerized system of poly(*N*-isopropylacrylamide-co-2-acrylamido-2-methylpropane sulfonic acid-co-methoxy-spiropyran-methacrylate) (p(NIPAAm-co-AMPS-co-SP)). We demonstrated repeatable photoresponsive changes to swelling, friction, and stiffness over three light cycles. Our findings suggest that volume changes driven by the decreased hydrophilicity of the methoxy-SP-MA upon light irradiation are responsible for differences in the mechanical and tribological properties of our photoresponsive hydrogels. Our results could inform future designs of photoswitchable hydrogels for applications ranging from biomedical applications to soft robotics.

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## 1. Introduction

Stimuli-responsive hydrogels are an important and growing class of hydrogels that change water content, structure, or mechanical and interfacial properties in response to environmental changes such as pH,<sup>1,2</sup> temperature,<sup>3,4</sup> solvent composition,<sup>5</sup> electrostatics,<sup>6,7</sup> and more recently, light.<sup>8–12</sup> This responsive behavior makes such hydrogels attractive materials for 3D printing resins,<sup>13</sup> biomedical applications,<sup>14–16</sup> atmospheric water harvesting,<sup>17,18</sup> and the rapidly emerging field of soft robotics.<sup>19–21</sup> Light-responsive hydrogels take inspiration from biology, which utilizes light in many biological processes such as photosynthesis, phototaxis, and phototropism.<sup>22,23</sup> Light offers bio-orthogonal advantages over other stimuli (e.g., pH, temperature, solvents, *etc.*) by providing non-contacting and precise spatiotemporal control with wavelength specificity. Due to this versatility, there is increasing interest in the development of photoresponsive materials.

One method to form photoresponsive hydrogels is through the utilization of optoproteins, which were first reported in 1973<sup>24</sup> and are a class of light-responsive proteins that control various cell signaling pathways.<sup>25</sup> Their discovery has formed a new field of molecular optogenetics,<sup>26</sup> and when incorporated

into biological hydrogel networks, such as collagen, the elastic modulus can be spatiotemporally controlled and increased due to light-induced dimerization and oligomerization.<sup>27–29</sup> However, one drawback that limits the broad utilization of optoproteins is the time-consuming and low yield purification process.<sup>28</sup> A synthetic analog to optoproteins that are commonly used to form photoresponsive polymeric systems are molecular photoswitches that change conformation and properties upon light irradiation. Photoswitches can be broadly classified by their switching mechanism, where the reversion back to its original state is driven by a thermal process (T-type) or by irradiation with another wavelength of light (P-type). Azobenzene<sup>30,31</sup> (either T- or P-type) and spirobifluorene<sup>32,33</sup> (T-type) photoswitches are commonly utilized and incorporated into liquid crystal elastomers<sup>34–36</sup> and hydrogel networks resulting in light-induced actuation, bending, and locomotion.<sup>8,10,11,30,37–41</sup>

Azobenzene drives macroscopic actuation by undergoing an E/Z isomerization and elongating (*trans* isomer) or contracting (*cis* isomer) the polymer chains to which it is attached.<sup>30,31,42</sup> Conversely, spirobifluorene undergoes pericyclic isomerization in response to light irradiation and exchanges between the spirobifluorene (SP) (ring-closed) and merocyanine (MCH<sup>+</sup>) (ring-open) conformations. The equilibrium and switching kinetics of spirobifluorene molecules are highly dependent on substitution pattern, solvent selection, and solution pH.<sup>32,43–45</sup> In an acidic environment, the hydrophilic MCH<sup>+</sup> form is often stabilized and can be converted to the hydrophobic SP upon irradiation with blue light (Fig. 1). In the absence of light, the SP form undergoes thermal relaxation to the MCH<sup>+</sup> form. This hydrophilicity change drives

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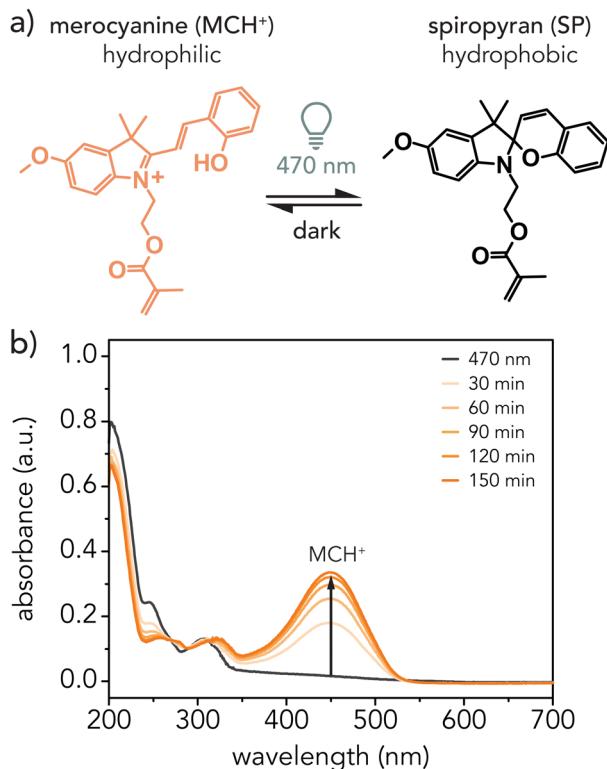
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## Methoxy-Spiropyran-Methacrylate Monomer



**Fig. 1** (a) Chemical structure of methoxy-spiropyran-methacrylate (methoxy-SP-MA) monomer in acidic solution. Under 470 nm irradiation, the monomer isomerizes to the spirobifluorene form. In the dark, it thermally relaxes back to the merocyanine form. (b) UV-vis spectra of 0.02 mM methoxy-SP-MA monomer in acidified methanol ( $\text{pH} \approx 2$ ) at varying intervals in the dark after 1 min of 470 nm light exposure. It took approximately 2.5 h to thermally relax from SP back to  $\text{MCH}^+$  in the dark, as demonstrated by the increased absorbance at  $\lambda \approx 450 \text{ nm}$ .

hydrogel dehydration and rehydration, leading to volume changes.<sup>11,32</sup> Due to the significant change in polarity commonly accompanied by the proton release, spirobifluorene/merocyanine-based photoswitches have been used as photoacids<sup>46,47</sup> and photosurfactants.<sup>48,49</sup>

While many groups have investigated the swelling behavior and actuation of spirobifluorene-incorporated hydrogels,<sup>8–11,38,39</sup> the tribological behavior (e.g., friction and lubrication) of light-responsive hydrogels remains largely unexplored. However, several studies over the past decade have investigated related phenomena, including adhesion and surface roughness changes in spirobifluorene-incorporated elastomers<sup>50,51</sup> and hydrogels in response to light.<sup>52</sup> Photocleavable groups have been attached to polymer brushes to control friction<sup>53</sup> while others have demonstrated photoresponsive friction changes of azobenzene-derived hydrogels due to a sol–gel transition.<sup>54</sup> The photothermal effect of thermoresponsive hydrogels has been exploited to tune friction by embedding gold nanoparticles<sup>55,56</sup> or metals<sup>57</sup> into poly(*N*-isopropylacrylamide) (pNIPAAm) networks. In these cases, the main mechanism behind the friction change is driven by the lower critical solution temperature (LCST) of pNIPAAm and the rapid phase transition and network collapse that occurs when the LCST is surpassed.

However, in our work we aimed to synthesize photoresponsive hydrogels with tunable friction coefficients that did not rely on the photothermal effect but rather utilized the photochemical effect of spirobifluorene photoswitches to drive chemical changes within the network that would lead to macroscopic volume changes. Methoxy-spiropyran-methacrylate (methoxy-SP-MA) was synthesized and conjugated with *N*-isopropylacrylamide (NIPAAm) and 2-acrylamido-2-methylpropane sulfonic acid (AMPS) and cross-linked with *N,N'*-methylenebisacrylamide (MBAm) to form the copolymerized hydrogel network (p(NIPAAm-*co*-AMPS-*co*-SP)). AMPS was chosen as the co-monomer for this study to increase the overall hydrophilicity of the system and, as a result, the difference in rehydration/deswelling of hydrogels in aqueous solutions. Previously, Li *et al.* examined different ring substituents of water-soluble spirobifluorenes in various solution pHs and discovered that sulfonated groups led to volume expansion upon light irradiation in acidic environments due to increased net charge.<sup>8</sup> In addition, they demonstrated that to shift the equilibrium to the merocyanine form in the dark, acidic solutions with low pHs ( $\text{pH} \approx 2$ ) are required.<sup>8</sup> To minimize possible hydrolysis of the spirobifluorene/merocyanine moiety commonly associated with the nucleophilic attack of water, we incorporated a methoxy group into the architecture, which has been previously shown to improve hydrolytic stability as well as shift the equilibrium to the merocyanine form.<sup>44,49,58</sup>

Our work was guided by the hypothesis that these hydrogels would exhibit lower friction coefficients in sliding contact with glass hemispherical probes when the methoxy-SP-MA was in the  $\text{MCH}^+$  form and higher friction in the SP form due to an increase in hydrophobicity, leading to hydrogel deswelling. To the authors' knowledge, this is the first instance where volume changes in response to light were used to control friction of bulk hydrogels. We report herein sample volume, friction coefficient, and elastic modulus before and after irradiation. Additionally, the switching kinetics between the  $\text{MCH}^+$  and SP forms was evaluated for the monomers, polymers, and hydrogels.

## 2. Materials and methods

### 2.1 Chemicals

Hydrogel samples were prepared using a combination of commercially available and synthesized constituents. *N*-Isopropylacrylamide 97% (NIPAAm), ammonium persulfate >98% (APS), and *N,N,N',N'*-tetramethylethylenediamine 99% (TEMED) were purchased from Sigma Aldrich. *N,N'*-methylenebisacrylamide 99+% (MBAm) and 1,4-dioxane 99+% were purchased from ThermoFisher Scientific. 2-Acrylamido-2-methylpropane sulfonic acid >98% (AMPS) was purchased from Tokyo Chemical Industry Co., Ltd. All reagents were used as received. 2-(5'-methoxy-3',3'-dimethylspiro[chromene-2,2'-indolin]-1'-yl) ethyl methacrylate (methoxy-SP-MA) (molecular weight: 405.494 g mol<sup>−1</sup>) was synthesized and characterized as detailed in ESI† Section S1 (Fig. S1–S7). Stock solutions of APS (10 wt%) were prepared in ultrapure Milli-Q water (18.2 MΩ cm). Phosphate buffer solution (PBS) ( $\text{pH} \approx 2$ ) was prepared by adding 1 M HCl to 100 mM  $\text{NaH}_2\text{PO}_4$  solution.



The pH of the final solution was measured using the Thermo Scientific Orion Star<sup>TM</sup> A111 Benchtop pH meter.

## 2.2 Light source

Throughout polymerization, swelling experiments, and mechanical testing, the irradiation source was 470 nm collimated LED lights (Thorlabs, Inc. M470L5-C1). Light intensity was measured using a power meter (Thorlabs PM100D) with a standard photodiode power sensor (Thorlabs S121C, 10 mm diameter, 400–1100 nm, 500 nW–500 mW). A light intensity of  $I = 35 \pm 1 \text{ mW cm}^{-2}$  was obtained at 1 A current and maximum power while the blue light source was 35 mm away from the sensor. Similar light intensities and experimental conditions were used for all photoswitching measurements in this study.

## 2.3 Hydrogel synthesis

Copolymerized p(NIPAAm-*co*-AMPS-*co*-SP) hydrogel disks were prepared by dissolving 140 mg NIPAAm, 1.4 mg AMPS (0.5 mol% relative to total polymer concentration), 13 mg methoxy-SP-MA (2.5 mol%), and 5.1 mg of MBAm (0.5 mol%) in a solution of 800  $\mu\text{L}$  dioxane, 100  $\mu\text{L}$  DI water, and 7.4  $\mu\text{L}$  TEMED. The precursor solution was bubbled with nitrogen for 30 min. 100  $\mu\text{L}$  of 10 wt% APS was added (forming a 4 : 1 vol/vol solution of 1,4-dioxane : DI water) to initiate polymerization, and the precursor was polymerized between two glass slides with 1.7 mm thick Viton<sup>TM</sup> spacers in a nitrogen-rich environment for 1 h. During polymerization, the samples were irradiated with 470 nm light to drive the monomer equilibrium to the SP form to facilitate more efficient incorporation into the network. Due to the difference in reactivity rate between acrylamide and methoxy-spiropyran-methacrylate, it is important to conduct the polymerization of hydrogels in an oxygen-free atmosphere to ensure complete incorporation of methoxy-SP-MA.<sup>59,60</sup> After polymerization, the gels were sectioned with an 18 mm circular punch (pre-swollen thickness,  $t = 1.6 \text{ mm}$ ) and swollen in 100 mM phosphate buffer solution ( $\text{pH} \approx 2$ ) in the dark for at least 36 h prior to testing to ensure the gels reached equilibrium swelling in the MCH<sup>+</sup> conformation. All mechanical tests and volume measurements were completed two days after synthesis. Control hydrogels of p(NIPAAm-*co*-AMPS) were polymerized in a similar manner as the p(NIPAAm-*co*-AMPS-*co*-SP) hydrogels utilizing the same solvent system of 4 : 1 v/v 1,4-dioxane : DI water, except 144 mg NIPAAm was added to keep the polymer concentration consistent.

## 2.4 UV-vis spectroscopy

UV-vis absorption spectra were measured on Shimadzu UV 3600 UV-vis-NIR Spectrometer using an Absolute Absorbance stage with a working range of 180 to 3600 nm. The photo-induced optical absorption kinetics was measured on a home-built pump-probe setup, as previously reported by our group.<sup>61</sup> For more details, see ESI<sup>†</sup> Section S2.1. UV-vis absorption spectra and kinetics were obtained for methoxy-SP-MA monomer in acidified MeOH (Fig. S8, ESI<sup>†</sup>) and for linear p(NIPAAm-*co*-AMPS-*co*-SP) (Fig. S9, ESI<sup>†</sup>) and p(NIPAAm-*co*-AMPS-*co*-SP) hydrogels (Fig. S10, ESI<sup>†</sup>) in 100 mM phosphate buffer solution

( $\text{pH} \approx 2$ ). For more details about the preparation of the UV-vis samples and detailed characterization of materials, see ESI<sup>†</sup> Section S2.2–S2.5.

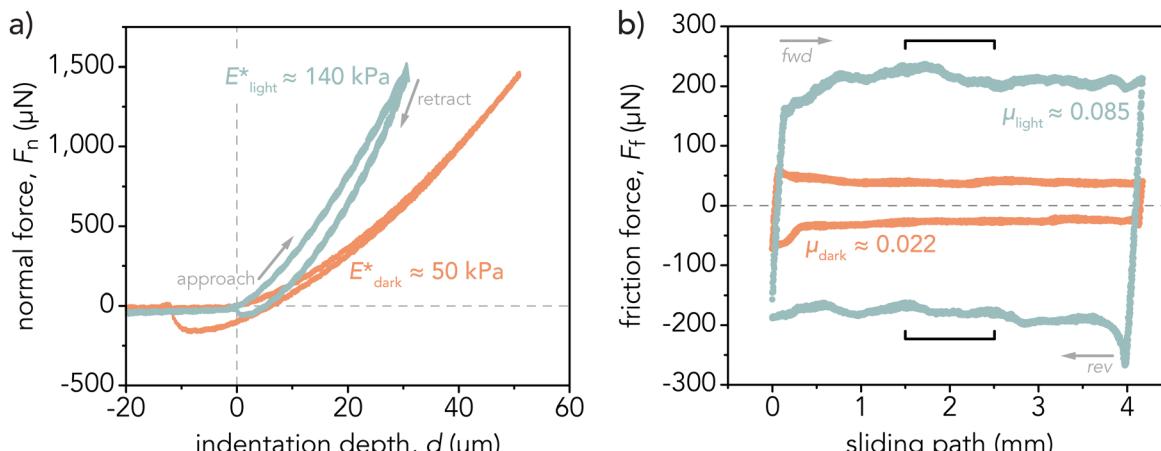
## 2.5 Hydrogel characterization

**2.5.1 Hydrogel swelling.** Hydrogel volume before, during, and after 470 nm light irradiation was recorded from side-view time-lapses using a Nikon D700 DSLR camera (AF Micro-NIKKOR 60 mm f/2.8D lens). The 470 nm light source was mounted 35 mm above the sample ( $I = 35 \pm 1 \text{ mW cm}^{-2}$ ), and hydrogels were irradiated with light for 7 h and equilibrated in the dark for 17 h to ensure enough time elapsed for solution diffusion in and out the network. To record the initial color change upon light irradiation, images were taken every 5 s for the first 1 h and then every 5 min for the remainder of the experiment. Hydrogel volume ( $V$ ) was estimated by assuming a cylindrical geometry and measuring hydrogel diameter and thickness (height) with Fiji.<sup>62</sup> To estimate photo-induced volume changes, calipers were used to measure hydrogel diameter and thickness before blue light irradiation, after 3 h of direct light exposure ( $\lambda = 470 \text{ nm}$ ,  $I = 35 \pm 1 \text{ mW cm}^{-2}$ ), and after 2–5 h of mechanical testing with light irradiation.

**2.5.2 Microindentation measurements.** Microindentation tests were conducted to obtain the reduced elastic modulus,  $E^*$ , of the photoresponsive hydrogels while samples were fully submerged in aqueous solution using a custom-built microtribometer, described previously.<sup>63</sup> Briefly, a hemisphere glass probe (radius of curvature,  $R = 2.6 \text{ mm}$ ) mounted to a double-leaf cantilever with normal and tangential spring constants of  $K_n = 222 \mu\text{N } \mu\text{m}^{-1}$  and  $K_t = 92 \mu\text{N } \mu\text{m}^{-1}$  was used to indent hydrogels to a maximum force of  $F_n = 1.5 \text{ mN}$  at an indentation velocity of  $v_{\text{ind}} = 10 \mu\text{m s}^{-1}$  across three positions along the gel. Hertzian contact mechanics (ESI<sup>†</sup> Section S3) was used to estimate  $E^*$ . Indentation measurements were conducted in the dark to obtain  $E_{\text{dark}}^*$  and in the light after at least 5 h of blue light irradiation ( $\lambda = 470 \text{ nm}$ ,  $I = 35 \pm 1 \text{ mW cm}^{-2}$ ) to determine  $E_{\text{light}}^*$ . Three dark-light cycles were conducted, and gels equilibrated in the dark at least 16 h before further characterization the following day. Representative indentation curves are displayed in Fig. 2a and Fig. S11 (ESI<sup>†</sup>), and the reported  $E^*$  is the average and standard deviation across three separate hydrogels ( $n = 3$  samples, 45 total indentations (Fig. S12, ESI<sup>†</sup>)).

**2.5.3 Friction measurements.** Friction coefficients were measured using a linear-reciprocating microtribometer, as previously described.<sup>63</sup> Tribological experiments were conducted while the hydrogels were fully submerged in solution at an applied normal force of  $F_n = 2 \text{ mN}$  with a  $v = 0.1 \text{ mm s}^{-1}$  sliding velocity across a path length of 4 mm. Friction coefficients were calculated from friction force loops (Fig. 2b) as discussed in prior work.<sup>64</sup> At least 70 friction cycles were completed, and the last 50 were averaged to obtain friction coefficients in the dark and in the light after 3 h blue light irradiation to determine  $\mu_{\text{dark},c}$  and  $\mu_{\text{light},c}$ , respectively, where c represents the dark-light cycle. Three dark-light cycles were conducted, and the gels reswelled in the dark for at least 16 h before further characterization the following day.





**Fig. 2** Representative (a) indentation curves and (b) friction force loops for p(NIPAAm-*co*-AMPS-*co*-SP) hydrogels in the dark (orange) and after light irradiation (blue). The reduced elastic modulus and friction force both increased in the SP state. Indentations were conducted at an applied force of  $F_n = 1.5 \text{ mN}$  and indentation velocity of  $10 \mu\text{m s}^{-1}$ . The labeled  $E^*$  values are the approximate average elastic moduli across three samples ( $n = 3$  hydrogels, 45 indents) for one cycle in the dark or light respectively. Friction coefficients were measured at an applied force of  $F_n = 2 \text{ mN}$  and sliding velocity of  $v = 0.1 \text{ mm s}^{-1}$  by analyzing the free sliding regime in the middle 25% of the sliding path (indicated by brackets). The labeled  $\mu$  values are the approximate average friction coefficients across three samples ( $n = 3$  hydrogels).

The friction ratio between the light and dark state was calculated as  $f_c = \mu_{\text{light},c}/\mu_{\text{dark},c}$ . A friction ratio  $f_c > 1$  indicates that the gel exhibited increased friction coefficients within the light state.

### 3. Results and discussion

#### 3.1 Switching and swelling kinetics

UV-vis spectroscopy data demonstrated that methoxy-spiropyran-methacrylate monomers photoisomerized from  $\text{MCH}^+$  to SP, within a minute under the application of 470 nm light ( $I = 25 \pm 1 \text{ mW cm}^{-2}$ ) and thermally relaxed in the dark to  $\text{MCH}^+$  within 4 h (Fig. 1b and Fig. S8, ESI<sup>†</sup>). Due to the poor solubility of the methoxy-SP-MA in the phosphate buffer solution ( $\text{pH} \approx 2$ ), the UV-vis spectroscopy experiments were performed in an acidified MeOH solution to mimic the conditions of the phosphate buffer ( $\text{pH} \approx 2$ ) (ESI<sup>†</sup> Sections S2.2 and S2.3). To determine the photo-switching properties of a spiropyran/merocyanine molecule when incorporated into a network, we synthesized linear and crosslinked p(NIPAAm-*co*-AMPS-*co*-SP) (ESI<sup>†</sup> Sections S2.4 and S2.5). Due to the improved solubility, the UV-vis spectroscopy characterization was performed in 100 mM phosphate buffer ( $\text{pH} \approx 2$ ). The photo-switching behavior of the linear p(NIPAAm-*co*-AMPS-*co*-SP) in PBS ( $\text{pH} \approx 2$ ) (Fig. 3) was similar to the methoxy-SP-MA monomer (Fig. 1b) and linear p(NIPAAm-*co*-AMPS-*co*-SP) in acidified methanol (Fig. S9b, ESI<sup>†</sup>). Both systems can be irradiated for several cycles without a loss of photoswitching properties. Characterization of the crosslinked p(NIPAAm-*co*-AMPS-*co*-SP) hydrogel network (Fig. S10, ESI<sup>†</sup>) was challenging due to absorption oversaturation, even when the concentration of methoxy-SP-MA was decreased to 0.5 mol% for UV-vis spectroscopy experiments compared to the 2.5 mol% methoxy-SP-MA used for mechanical testing. Despite that, we were able to observe similar photoswitching properties to the linear p(NIPAAm-*co*-AMPS-*co*-SP).

To demonstrate photoswitchability, p(NIPAAm-*co*-AMPS-*co*-SP) hydrogels were equilibrated in 100 mM PBS ( $\text{pH} \approx 2$ ) for at least 36 h and then irradiated from above with 470 nm light at an intensity of  $35 \text{ mW cm}^{-2}$ . In addition to hydrophilicity changes upon light exposure, methoxy-SP-MA molecules are photochromic, possessing a red color in the ring-open  $\text{MCH}^+$  state and becoming pale-yellow/colorless in the ring-closed SP state.<sup>47,65-67</sup> Within the hydrogel network, this color change was perceived as transitioning from red to light yellow (Fig. 4) with the  $\text{MCH}^+$  quickly converting to SP within seconds of light irradiation (Video S1, ESI<sup>†</sup>). Over 10 min, light penetrated deeper into the bulk of the hydrogel network due to increased transparency at the surface, creating a photobleaching front that propagated through the thickness of the hydrogel. Eventually, the entire hydrogel changed color (Fig. 4b), supporting conversion throughout the bulk of the hydrogel.

#### 3.2 Volume change

The p(NIPAAm-*co*-AMPS-*co*-SP) hydrogels demonstrated repeatable photoswitchable contraction and swelling, as displayed in Fig. 5.

As  $\text{MCH}^+$  converts to SP upon light irradiation, not only is there a color change but a hydrophilicity change as the molecule becomes more hydrophobic due to the loss of the positively charged nitrogen upon ring-closing, leading to deswelling of the hydrogel mesh (Fig. 5a). Within the first 3 h, sample volume decreased quickly ( $-38 \pm 12\%$ ,  $n = 14$  hydrogels, see Fig. S13, ESI<sup>†</sup>) then slowed over the following 2–4 h ( $-14 \pm 5\%$ ,  $n = 10$  hydrogels). Once the light was turned off, the hydrogel slowly rehydrated over 17 h as the SP started to thermally equilibrate back to the  $\text{MCH}^+$  form. Occasionally, as demonstrated in Fig. 5b, the hydrogel reached its initial volume after the third light cycle. However, most gels in this study only rehydrated to about 80% of the initial sample volume. Similar declines in



## Linear p(NIPAAm-co-AMPS-co-SP)

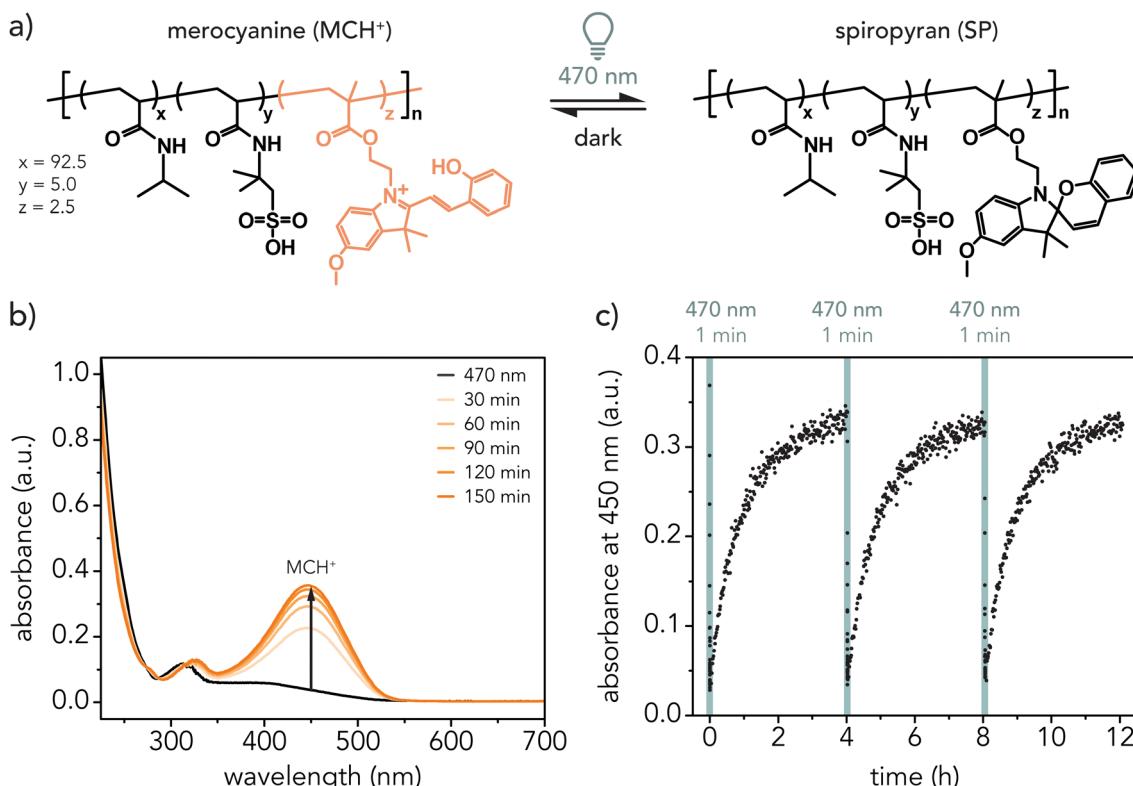


Fig. 3 (a) Chemical structure of linear p(NIPAAm-co-AMPS-co-SP) in the merocyanine and spiropyran forms. (b) UV-vis spectrum of 0.150 mg mL<sup>-1</sup> linear p(NIPAAm-co-AMPS-co-SP) in 100 mM phosphate buffer (pH ≈ 2) with 5 mol% AMPS. The absorbance at  $\lambda \approx 450$  nm increased over time in the dark as the methoxy-SP-MA thermally relaxed from the SP conformation back to the MCH<sup>+</sup> conformation upon removal of 470 nm light. (c) Pump–probe kinetics measurements upon irradiation with 470 nm light for approximately 1 min (Thorlabs, Inc. M470F3,  $I = 25 \pm 1$  mW cm<sup>-2</sup>), followed by the thermal relaxation of the molecule over 4 h in the dark, monitored at the  $\lambda \approx 450$  nm absorbance peak.

rehydration percentage have been observed in other photoresponsive hydrogel systems,<sup>39,68</sup> while others have seen more consistent rehydration.<sup>9,30</sup> This may be caused by inherent sample-to-sample variation compounded by inherent error in volume measurements. Additionally, there may be incomplete conversion between the MCH<sup>+</sup> and SP states between light cycles. However, the underlying mechanism responsible for this effect is not well understood and warrants further study.

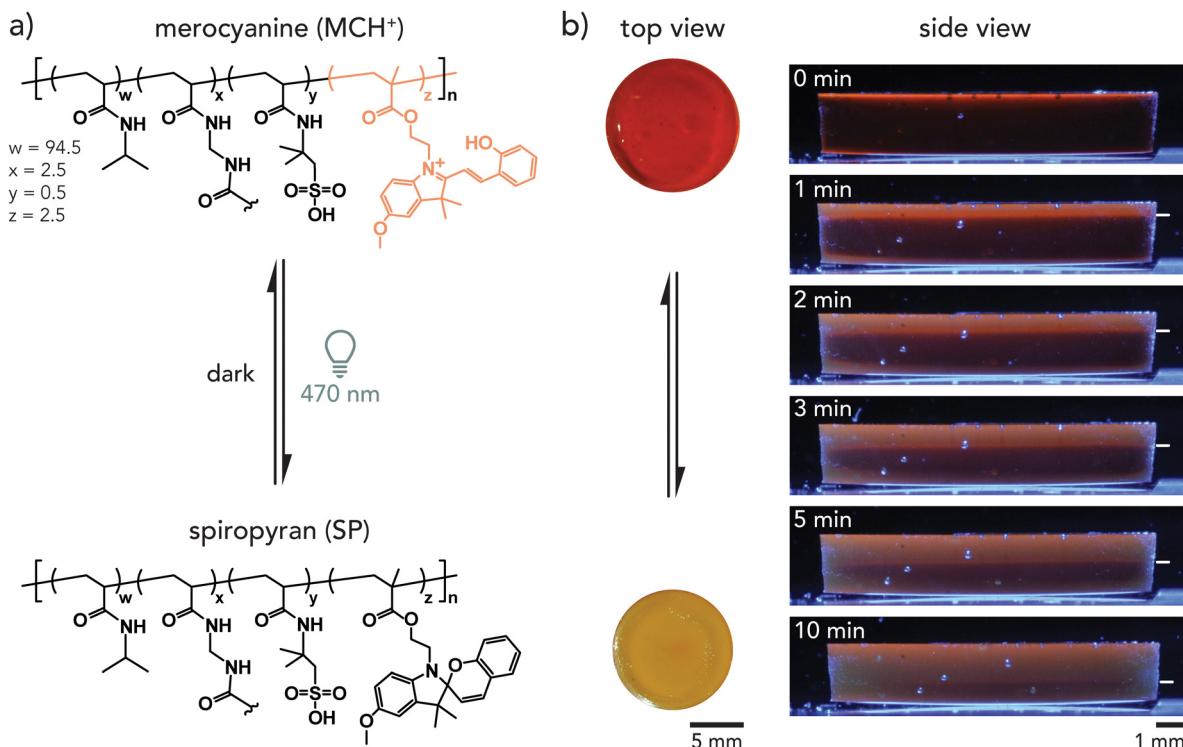
### 3.3 Photoresponsive lubricity

The friction coefficients of p(NIPAAm-co-AMPS-SP) hydrogels were measured before and after illumination with 470 nm light. Hydrogels were equilibrated in 100 mM phosphate buffer solution (pH ≈ 2) for at least 36 h before mechanical characterization. Fig. 6a and c demonstrate a representative friction experiment: friction coefficients and hydrogel volumes were obtained while the gels were in the dark and after direct irradiation ( $\lambda = 470$  nm,  $I = 35 \pm 1$  mW cm<sup>-2</sup>) for 3 h. Hydrogel volumes were measured again after mechanical testing, and gels were left to equilibrate in the dark for at least 16 h before the next cycle began to account for the slow rehydration times. Fig. 6a demonstrates that friction repeatedly increased at least 5 times the initial value after light irradiation for a representative gel. Fig. 6b shows the average

friction coefficients and standard deviations in the dark and light state across three hydrogel samples for three dark–light cycles. For friction coefficient values for each hydrogel, see Fig. S14 and S15 (ESI†). The average initial friction coefficient in the dark was  $\mu_{\text{dark},1} = 0.022 \pm 0.002$ . After direct light irradiation for 3 h, the friction coefficient almost quadrupled to  $\mu_{\text{light},1} = 0.085 \pm 0.039$  leading to a friction ratio ( $\mu_{\text{light},1}/\mu_{\text{dark},1}$ ) of  $f_1 = 3.9$ . However, the friction ratio increased with each dark–light cycle ( $\mu_{\text{dark},2} = 0.023 \pm 0.003$ ,  $\mu_{\text{light},2} = 0.170 \pm 0.010$ ,  $\mu_{\text{dark},3} = 0.019 \pm 0.003$ ,  $\mu_{\text{light},3} = 0.160 \pm 0.030$ ), with  $f_2 = 7.4$  and  $f_3 = 8.5$  for the second and third light cycles, respectively. This indicates that the friction increase with light irradiation is repeatable. The friction ratios reported herein surpass other pNIPAAm-based systems that depend on the combined effects of temperature and light for photoresponsive hydrogel friction.<sup>56,57</sup>

Representative hydrogel swelling behavior corresponding with friction measurements for a single hydrogel sample is depicted in Fig. 6c, which shows normalized volume ( $(V/V_{\text{dark},1}) \times 100\%$ ) over time. For this experiment, hydrogel volume decreased after the first light cycle and reswelled to approximately 50% of the initial volume overnight. The sample deswelled and rehydrated to similar volumes during the second and third light cycles.

## p(NIPAAm-co-AMPS-co-SP) Hydrogel



**Fig. 4** (a) Chemical structure of p(NIPAAm-co-AMPS-co-SP) hydrogel. (b) Top- and side-view of hydrogel demonstrating the photobleaching front propagating through the thickness of the hydrogel over 10 min with image of hydrogel before and after photobleaching. Black arrows and white lines are used to guide the eye to indicate the photobleaching front.

Fig. 6d demonstrates the average normalized volume ( $(V/V_{\text{dark},1}) \times 100\%$ ) for three hydrogels across the dark-light cycles. On average, gels only reached about 75% of their initial volume after the first cycle but consistently deswelled to 50% of their initial volume ( $V_{\text{dark},1}$ ) after 3 h of irradiation for all the light cycles. This may indicate that not all the methoxy-SP-MA fully converted back to the  $\text{MCH}^+$  form after the first light cycle. This is consistent with previous results, where poly(*N*-isopropylacrylamide-*co*-acrylic acid) hydrogels also did not reach full volume recovery after the first light cycle but were able to achieve consistent recovery in subsequent cycles.<sup>39</sup>

In addition to friction and volume changes, the elastic modulus also changed with light.  $E_{\text{light}}^*$  was consistently 2 to 3 times greater than  $E_{\text{dark}}^*$  for each dark-light cycle and across three hydrogel samples (Fig. S12, ESI†). According to rubber elasticity theory, modulus is dependent on the density of elastically active polymer chains ( $\rho_{\text{el}}$ ) within a network, with greater density leading to higher moduli.<sup>69–71</sup> For hydrogels, mesh size ( $\xi$ ), which can be defined as the average spacing between polymer chains in a network, is inversely proportional to  $\rho_{\text{el}}$ .<sup>72</sup> Therefore, a higher density of chains often indicates a smaller mesh. And an increase in elastic modulus due to hydrogel deswelling, as was observed in our photoresponsive gels, may indicate decreases in  $\xi$ . Based on de Gennes' elastic modulus scaling relationship of  $E \propto \xi^{-3}$ ,<sup>70</sup> if  $E_{\text{light}} \approx 2E_{\text{dark}}$ , then  $\xi_{\text{light}} \approx 0.79 \xi_{\text{dark}}$ . Therefore, mesh size may decrease roughly 20 to 30%

depending on the elastic modulus increase with light. This estimation is also supported by the volume change that occurs upon light irradiation.

While de Gennes' scaling concepts link the elastic modulus with hydrogel mesh size,<sup>70</sup> friction coefficients have also been shown to scale with mesh size for Gemini hydrogel (gel-on-gel) sliding configurations with larger mesh sizes leading to lower friction coefficients.<sup>73</sup> Similarly, others have demonstrated that mesh size increases with water content.<sup>74,75</sup> Therefore, we postulate that friction increased upon light irradiation due to decreasing mesh size – indicated by hydrogel deswelling and increased elastic modulus – associated with the increased hydrophobicity of the methoxy-SP-MA molecules.

### 3.4 Challenges and opportunities for photoresponsive hydrogels

This study presents, to the authors' knowledge, the first instance that photoswitchable friction relying on a photochemical effect rather than photothermal<sup>56,57</sup> or a sol-gel transition<sup>54</sup> has been demonstrated in bulk hydrogel materials. Zhu *et al.* demonstrated friction changes for gold nanoparticle-incorporated pNIPAAm hydrogels about 1 mm thick. A green light with  $3.5 \text{ W cm}^{-2}$  intensity, which is an order of magnitude greater than what was used here ( $I = 35 \pm 1 \text{ mW cm}^{-2}$ ), was able to locally increase the temperature within the pNIPAAm network and surpass the LCST, leading to a rapid collapse of the gel.

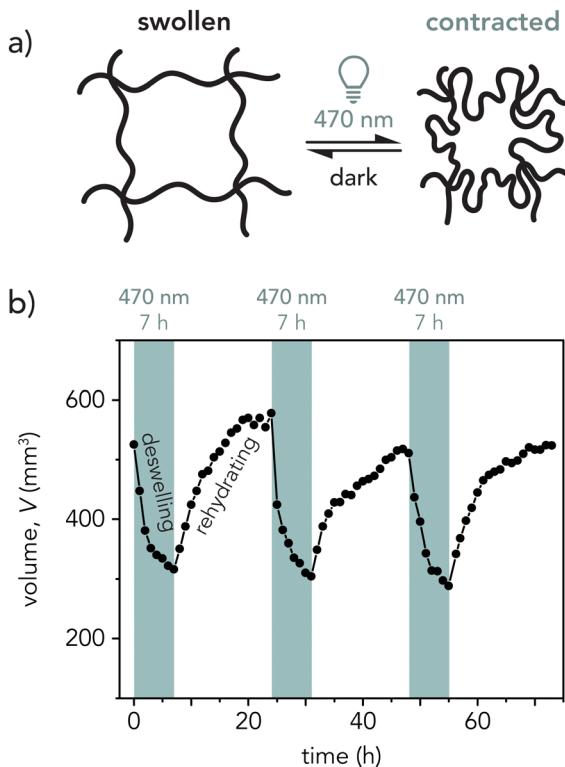


Fig. 5 (a) Hydrogel schematic depicting the possible microstructural change within the hydrogel mesh upon light irradiation. (b) Representative plot of volume as a function of time for three light–dark cycles (7 h blue light on, 17 h off).

They reported that the friction coefficient increased from approximately  $\mu \approx 0.25$  to  $\mu \approx 0.7$  ( $f = 2.8$ ) within 10 s and decreased within 30 s.<sup>56</sup> Similarly, Wu *et al.* demonstrated photothermal friction changes for MXene-p(NIPAAm-*co*-AMPS) hydrogels irradiated with near-infrared light ( $I = 1 \text{ W cm}^{-2}$ ). In their study, they observed that friction increased from  $\mu \approx 0.02$  to  $\mu \approx 0.13$  ( $f = 6.5$ ) within 5 min and decreased within 1 min.<sup>57</sup> However, both hydrogel systems relied on the LCST behavior of pNIPAAm to drive the change in friction behavior. Here, we demonstrated photoresponsive friction due to the hydrophilic transition of SP-MA which led to light-induced deswelling and repeatable higher friction ratios.

It is worth noting that NIPAAm, which is thermoresponsive, was required for our studies due to its solubility in both water and dioxane. This solvent mixture was necessary to dissolve monomers and the photochromic material for these studies. Additionally, AMPS was chosen as the comonomer to increase swelling within aqueous solutions and to add a source of internal protons.<sup>39</sup> It has been demonstrated that the incorporation of AMPS with NIPAAm leads to an increased lower critical solution temperature (LCST), but homogeneous pNIPAAm hydrogels can shrink under irradiation due to a slight temperature increase even several degrees below the LCST,<sup>39</sup> which was something also observed herein (Fig. S13 and S16, ESI†). Even though there was a small volume change ( $-8 \pm 7\%$ ,  $n = 6$  hydrogels), there was no significant change in friction

coefficient after 3 h of 470 nm light irradiation ( $I = 35 \pm 1 \text{ mW cm}^{-2}$ ) (Fig. S16, ESI†), indicating that the driving force behind the friction change for our p(NIPAAm-*co*-AMPS-*co*-SP) hydrogels is most likely the methoxy-SP-MA incorporated monomers.

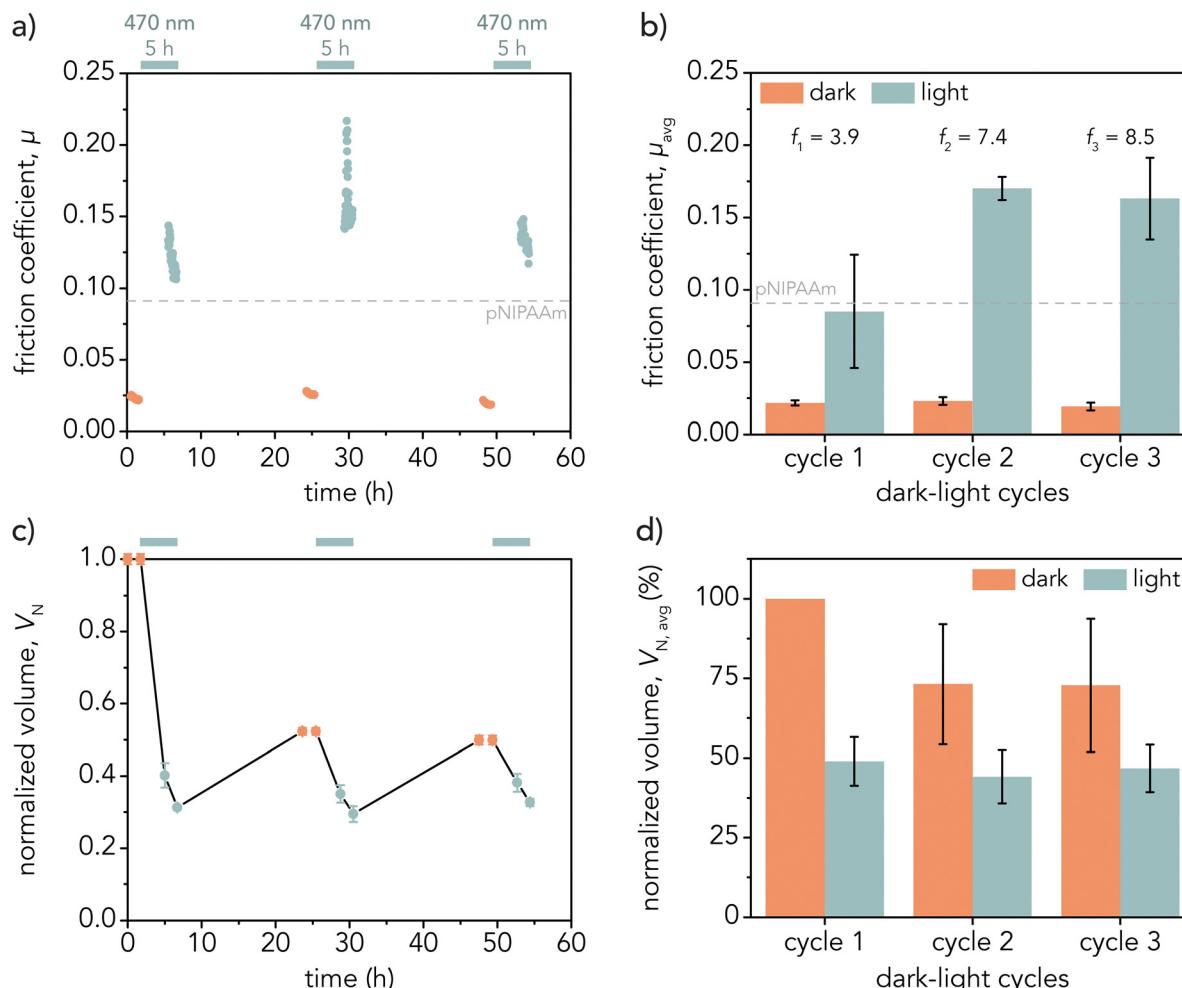
One limitation in our experiments is that the deswelling and rehydration of the hydrogels are diffusion-controlled, which limits the rate at which friction can change due to diffusion of solution in and out of the network. One way to potentially accelerate this process is by reducing the dimensions of the hydrogel, which is why smaller and thinner (typically  $< 0.5 \text{ mm}$ ) hydrogels are often used, leading to deswelling and swelling times on the order of minutes rather than hours.<sup>10</sup> Intentionally synthesizing porous hydrogels can also decrease swelling times from hours to seconds but may sacrifice strength.<sup>76</sup> In contrast, the gels herein are approximately 2 mm thick and 20 mm in diameter when fully swollen. These thicknesses are required for friction and indentations using our existing microtribometer configuration to ensure that we remain within the small strain limit ( $d/t \leq 0.1$ ) and to avoid any substrate effects. Additionally, thicker substrates help reduce bending or wrinkling effects during light penetration that often occur due to gradients in light intensity and strain.

The photoresponsive behavior demonstrated herein is not limited to bulk hydrogels but can be applied to thin ( $< 1 \text{ mm}$ ) hydrogel coatings as well. Thin layers of p(NIPAAm-*co*-AMPS-*co*-SP) were covalently attached to glass (see Section S8 for synthesis details, ESI†) to constrain the gels from swelling in the radial direction. Despite this restriction, there were still noticeable volume changes that occurred upon irradiation due to deswelling in the vertical direction, and both the friction coefficient and elastic modulus increased (Fig. S17, ESI†). These results indicate that bulk volume changes are not necessary to increase friction. However, to fully explore whether volume change is needed to drive photoresponsive friction changes or if the hydrophilicity change of the methoxy-SP-MA is enough, polymer brushes of p(NIPAAm-*co*-AMPS-*co*-SP) could be synthesized to eliminate any volume changes due to hydrogel swelling. This interesting topic will be left to future studies.

The rich and vast design space of our photoswitchable hydrogel platform offers opportunities to achieve more controlled friction behavior by tuning parameters such as light intensity, methoxy-SP-MA concentration, AMPS concentration, polymer concentration, and solution pH. This work demonstrates a new route to control friction coefficients of hydrogels using light, which could lead to the design of new photoresponsive materials and coatings for soft robotics and biomedical applications to control underwater locomotion or object manipulation.

## 4. Conclusion

While the tribological behavior of hydrogels responsive to other stimuli such as temperature,<sup>77,78</sup> solvent,<sup>79,80</sup> and pH<sup>81,82</sup> have been explored, there are fewer studies on



**Fig. 6** Representative (a) friction coefficient and (c) normalized volume ( $(V/V_{dark,1}) \times 100\%$ ) as a function of time for a p(NIPAAm-co-AMPS-co-SP) hydrogel sample. Friction and volume measurements were recorded after the gel underwent 3 dark-light cycles, during which gels equilibrated in the dark for about 16 h and were irradiated with 470 nm light for 3 h. Upon irradiation, friction increased 5 times while the volume of the gel decreased 60% due to increased hydrophobicity upon conversion to the SP state. Multiple dark-light cycles demonstrate the repeatability of the friction change between the  $MCH^+$  and SP states. (b) Bar plot demonstrating the average friction coefficient and standard deviation for 3 individual hydrogels in the dark and under 470 nm light with the friction ratio ( $f = \mu_{light}/\mu_{dark}$ ) labeled for each light cycle. (d) Bar plot of average normalized volume ( $(V/V_{dark,1}) \times 100\%$ ) across 3 hydrogels for each dark-light cycle. Gels generally recovered about 75% of their initial volume after the first light cycle.

light-induced interfacial changes. Our findings demonstrate that light-tunable friction repeatedly was achieved with p(NIPAAm-*co*-AMPS-*co*-SP-MA) hydrogels across three light cycles. Hydrogels with low friction ( $\mu_{dark} \approx 0.02$ ) were formed when the gels were in the dark (primarily  $MCH^+$ ) while high friction ( $\mu_{light} > 0.08$ ) was achieved in the light (primarily SP), indicating that the friction coefficient increased at least  $4\times$  upon light irradiation. Elastic moduli ( $E_{light}^* \approx 2E_{dark}^*$ ) and volume changes ( $V_{light} \approx 0.5V_{dark}$ ) were also observed upon light irradiation. The underpinning mechanism may be linked to photo-induced reduction in mesh size due to decreased hydrophilicity of methoxy-SP-MA monomers. Photoswitchable gels offer an exciting new arena to investigate the fundamental mechanisms of hydrogel surface physics and their programmable and reversible tribological properties and could have far-reaching impacts from biomedicine to soft robotics.

## Data availability

The original data for all the figures in the main text and Supplementary Information are available at Data Dryad, a free and searchable digital repository (<https://doi.org/10.5061/dryad.280gb5mzv>).

## Conflicts of interest

There are no conflicts to declare.

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