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# On-demand controlled bidirectional DNAzyme path for ultra-sensitive heavy metal ion detection†

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A bidirectional self-powered biosensor is constructed for the quasi-simultaneous detection of Pb<sup>2+</sup> and Hg<sup>2+</sup> based on MoS<sub>2</sub>@CuS heterostructures as an accelerator and hybridization chain reaction (HCR) as a signal amplification strategy. MoS<sub>2</sub>@CuS heterostructures significantly facilitate electron transfer between glucose and bioelectrodes, thereby greatly improving the detection signal of self-powered biosensors. This novel biosensor employs the unique sequences of DNAzymes to isolate Pb<sup>2+</sup> and Hg<sup>2+</sup> by the cleavage effect and thymine (T)–Hg<sup>2+</sup>–thymine (T) structures, respectively. In the process, Pb<sup>2+</sup> cuts the sequence of DNAzyme at the bioanode to trigger glucose oxidation to monitor Pb<sup>2+</sup>. The as-formed T–Hg<sup>2+</sup>–T structures activate HCR to reduce [Ru(NH<sub>3</sub>)<sub>6</sub>]<sup>3+</sup> to detect Hg<sup>2+</sup> at the biocathode. It is noteworthy that this biosensor not only realizes Pb<sup>2+</sup> or Hg<sup>2+</sup> detection in a single-electrode, respectively, but also can quasi-simultaneously detect both Pb<sup>2+</sup> and Hg<sup>2+</sup> in the bioanode and the biocathode. The novel self-powered biosensor identifies Pb<sup>2+</sup> in the range of 10<sup>6</sup> fM to 10 fM with a limit of detection (LOD) of 3.1 fM and Hg<sup>2+</sup> in the range of 10<sup>6</sup> fM to 1 fM with an LOD of 0.33 fM.

## Introduction

Heavy metal ion pollution is a severe hazard for human health because of the extremely low biodegradability of most heavy metals.<sup>1–4</sup> At present, many novel detection methods are employed to monitor heavy metal ions, such as surface enhanced Raman spectroscopy (SERS),<sup>5</sup> atomic absorption spectroscopy,<sup>6</sup> inductively coupled plasma mass spectrometry,<sup>7</sup> fluorescence spectroscopy,<sup>8–10</sup> colorimetric method,<sup>11</sup> and electrochemical methods.<sup>12,13</sup> For example, an on-site visual approach was designed for toxic Cr(VI) detection based on an

imidazolium-functionalized conjugated polymer;<sup>14</sup> an aptamer-functionalized fluorescent DNA sensor was used to monitor Cu(II) in living tumor cells;<sup>15</sup> an ultra-sensitive and selective electrochemical method was utilized for Cd(II) detection by the synergistic activation of phosphorus and the orbital coupling effect of Fe-doped CoP.<sup>16</sup>

Compared with the above methods, self-powered biosensors are widely used in the detection of biomolecules. In addition to eliminating the need for external power, these sensors exhibit strong anti-interference ability, ultra-sensitive detection capability, and highly identifiable specificity.<sup>17–21</sup> However, there has been no report of self-powered biosensors with the bidirectional detection to monitor heavy metal ions. The major reason is the difficulty in forming double bioelectrodes to simultaneously achieve linear detection.<sup>22–24</sup> Therefore, a bidirectional self-powered biosensor toward multiple heavy metal ions detection is urgently needed.

This work reports a bidirectional self-powered biosensor for the quasi-simultaneous detection of Pb<sup>2+</sup> and Hg<sup>2+</sup> based on MoS<sub>2</sub>@CuS heterostructures as a co-accelerator and a hybridization chain reaction (HCR) as a signal amplification strategy (Scheme 1). Unique sequences of DNAzymes isolate Pb<sup>2+</sup> and Hg<sup>2+</sup> by the cleavage effect and thymine (T)–Hg<sup>2+</sup>–thymine (T) structures, respectively.<sup>25–29</sup> In the process, Pb<sup>2+</sup> cuts the sequence of the DNAzyme at the bioanode to trigger glucose oxidation to monitor Pb<sup>2+</sup>. The as-formed T–Hg<sup>2+</sup>–T structures activate HCR to reduce [Ru(NH<sub>3</sub>)<sub>6</sub>]<sup>3+</sup> to detect Hg<sup>2+</sup> at the biocathode. As a result, this biosensor not only monitors Pb<sup>2+</sup> or Hg<sup>2+</sup> through the current changes caused by the oxidation–

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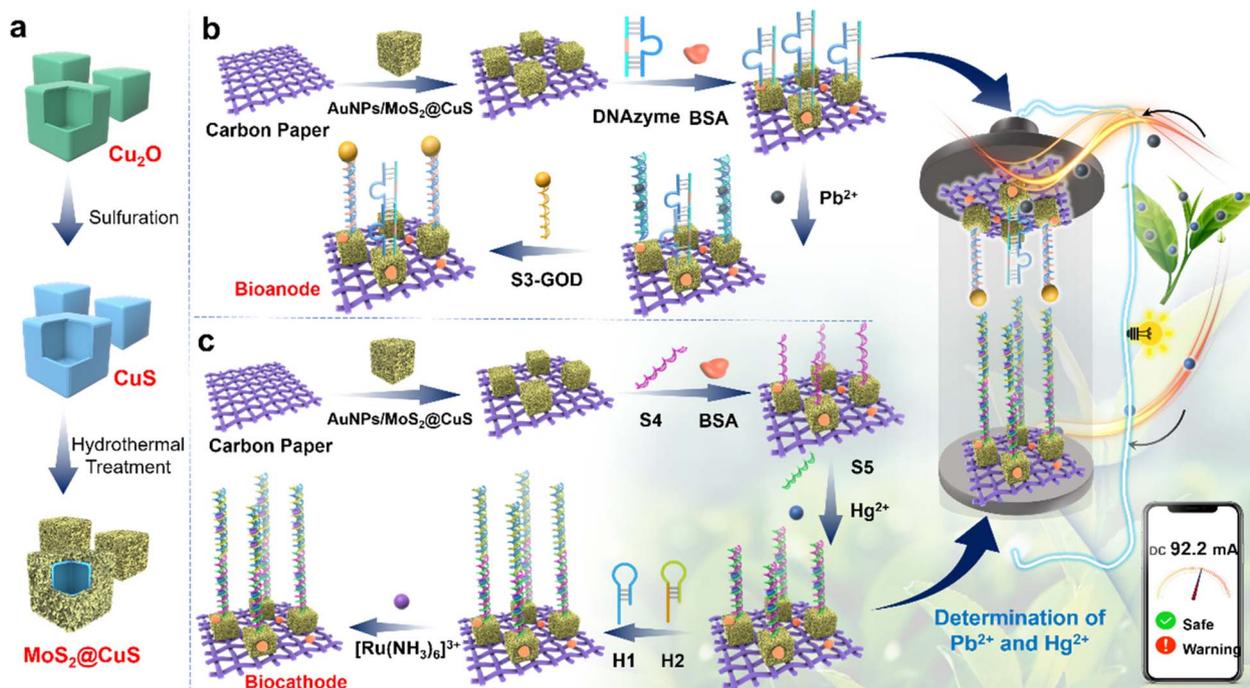
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Scheme 1 (a) The synthetic process of MoS<sub>2</sub>@CuS heterostructures. (b and c) The detection process of Pb<sup>2+</sup> and Hg<sup>2+</sup> of the bidirectional self-powered biosensor.

reduction reactions in a single-electrode, respectively, but also could quasi-simultaneously detect both Pb<sup>2+</sup> and Hg<sup>2+</sup> by observing the open circuit voltage ( $E^{ocv}$ ) in the bioanode and the biocathode. The bidirectional biosensor also exhibits considerable practicability for detecting Pb<sup>2+</sup> and Hg<sup>2+</sup> in tap water.

## Results and discussion

In the TEM images (Fig. 1a and S1<sup>†</sup>), uniform Cu<sub>2</sub>O templates, CuS nanocubes, and MoS<sub>2</sub>@CuS heterostructures (size of ~500 nm) are observed, and there are many small nanosheets on the surface of MoS<sub>2</sub>@CuS heterostructures. The selected area electron diffraction pattern (SAED) confirms the polycrystalline feature (inset, Fig. 1a), which is consistent with the X-ray diffraction (XRD) pattern (Fig. 1b). All peaks are indexed to MoS<sub>2</sub> (JCPDS: 37-1492) and CuS (JCPDS: 06-0462).<sup>30,31</sup> After adding Au nanoparticles (AuNPs, ~20 nm, 5 mM, Fig. S2<sup>†</sup>), many AuNPs are observed on the surface of MoS<sub>2</sub>@CuS heterostructures (Fig. 1c). The elemental mapping images and X-ray photoelectron spectra (XPS) confirm that Au, Cu, Mo, and S are present (Fig. 1d and S3<sup>†</sup>).<sup>32</sup> In addition, UV-vis spectra and FTIR spectroscopy confirmed the successful recombination of heterostructures. For MoS<sub>2</sub>@CuS heterostructures, the FTIR absorption peaks at 1605 and 895 cm<sup>-1</sup> were to the vibration of Mo–O bond and Mo–S bond, respectively (Fig. S4 and S5<sup>†</sup>).<sup>33</sup> Finally, the Brunauer–Emmett–Teller (BET) specific surface of MoS<sub>2</sub>@CuS heterostructures is calculated to be 30.8 cm<sup>2</sup> g<sup>-1</sup> with aperture size of ~5 nm (Fig. S6<sup>†</sup>).

The assembly process of the bioanode and biocathode was explored by cyclic voltammetry (CV) and differential pulse

voltammetry (DPV). Monitoring the maximum current value, the optimal recognition and cleavage time of Pb<sup>2+</sup> on the DNAzyme was 60 min (Fig. 2a). After DNAzyme was cut by Pb<sup>2+</sup>, it was split into two sequences of single strand DNAs: S1 and S2, leaving as-split S2 on the surface of AuNPs/MoS<sub>2</sub>@CuS/CP by Au–S bonding. When S3-GOD is added, the as-split S2 hybridizes with S3-GOD by complementary base pairing to form the bioanode. The optimal hybridization time between S2 and S3-GOD is 50 min (Fig. 2b). In the biocathode, the optimal incubation time among Hg<sup>2+</sup>, S5, and S4 is 30 min to form S5–Hg<sup>2+</sup>/S4/AuNPs/MoS<sub>2</sub>@CuS/CP by the T–Hg<sup>2+</sup>–T structure (Fig. 2c). Finally, the as-formed T–Hg<sup>2+</sup>–T structure further combines with H1 and H2 from the HCR process to generate a multi-duplex structure of H1, H2, and S5 to form H1, H2/S5–Hg<sup>2+</sup>/S4/AuNPs/MoS<sub>2</sub>@CuS/CP.

Next, [Ru(NH<sub>3</sub>)<sub>6</sub>]<sup>3+</sup> inserts into the multi-duplex structure of H1, H2, and S5 on the surface of H1, H2/S5–Hg<sup>2+</sup>/S4/AuNPs/MoS<sub>2</sub>@CuS/CP (Fig. 2d) with optimal concentration of 500 μM [Ru(NH<sub>3</sub>)<sub>6</sub>]<sup>3+</sup>. These assembly processes of the bioanode and biocathode were further verified by gel electrophoresis (Fig. 2e). Line M represents molecular weight standards. For the bioanode, a fading, shallow band with low molecular weight appears when Pb<sup>2+</sup> (lane 2) is incubated with DNAzyme (lane 1). After S3-GOD is added, S3-GOD hybridizes with as-split S2 to form many new bright bands (lane 3). For the biocathode, there is no visible band for S4 (lane 4) or S4 + S5 (lane 5), respectively. When the T–Hg<sup>2+</sup>–T (*i.e.*, S4–Hg<sup>2+</sup>–S5) structure is formed, a higher bright band (lane 6) is observed. Finally, when the T–Hg<sup>2+</sup>–T structure triggers the HCR reaction, a new band is observed (lane 7). These results are consistent with circular dichroic chromatography



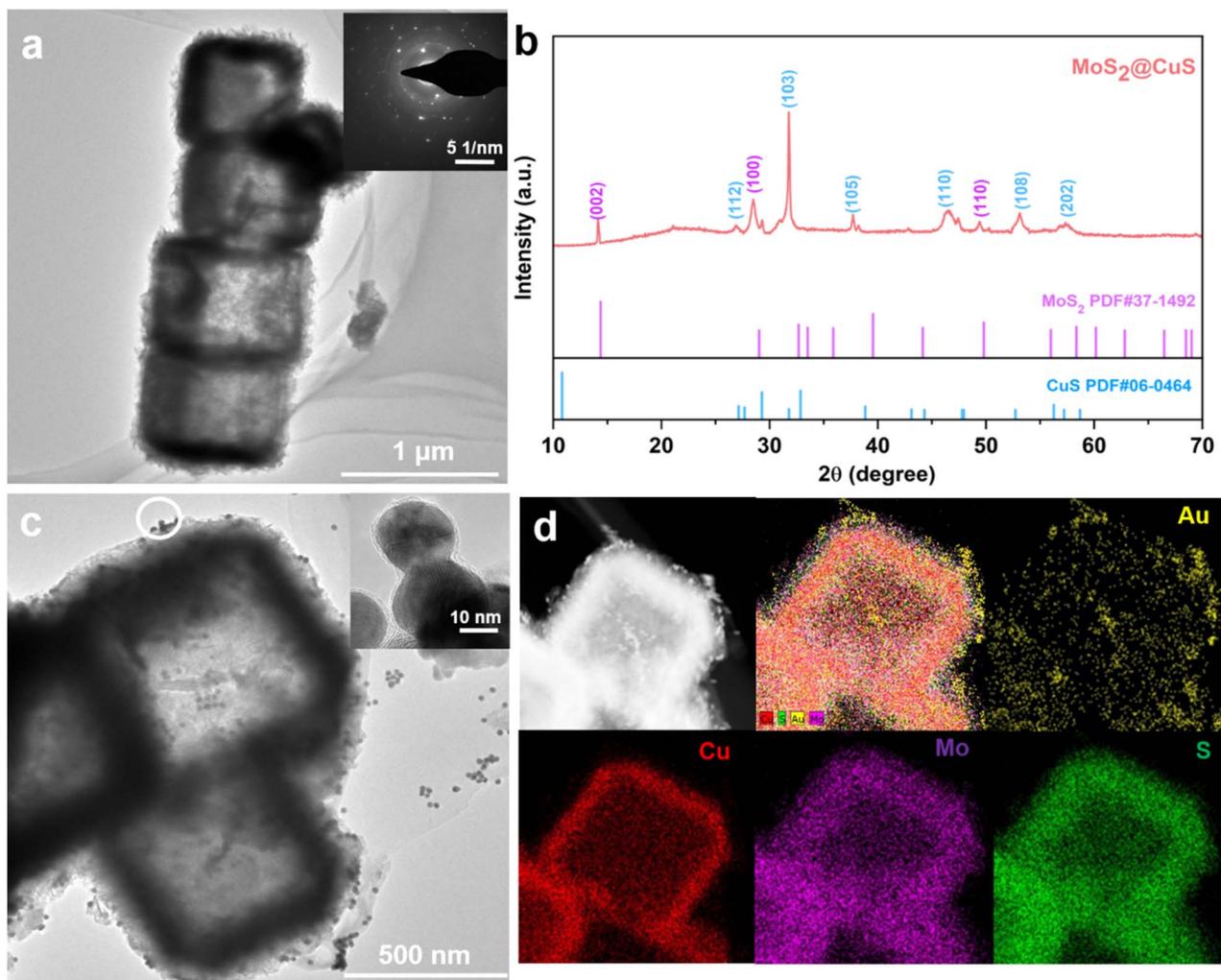


Fig. 1 Characterization of MoS<sub>2</sub>@CuS heterostructures: (a) TEM image and SAED (inset); (b) XRD. (c) TEM image and (d) EDX images of AuNPs/MoS<sub>2</sub>@CuS heterostructures.

(Fig. S7<sup>†</sup>). In the sensing mechanism, the Pb<sup>2+</sup> could cleave the RNA sites and change the DNAzyme structure; the thymine-thymine mismatch base pair (T-T, H1-H2) can capture the Hg<sup>2+</sup> to form a stable neutral T-Hg<sup>2+</sup>-T base pair.

Electrochemical impedance spectroscopy (EIS) was used to study the preparation process of the bioanode (Fig. 3a). The resistance ( $R_{et}$ ) value of CP (curve A) is higher than that of AuNPs/MoS<sub>2</sub>@CuS/CP (curve B), confirming the good electrical conductivity of AuNPs/MoS<sub>2</sub>@CuS. After DNAzyme, Pb<sup>2+</sup>, and S3-GOD are sequentially incubated with AuNPs/MoS<sub>2</sub>@CuS/CP, the  $R_{et}$  increases from 14  $\Omega$  to 30  $\Omega$  (Fig. 3a). For the biocathode (Fig. 3b), H1, H2/S5-Hg<sup>2+</sup>/S4/AuNPs/MoS<sub>2</sub>@CuS/CP shows the highest  $R_{et}$  after S4, S5 and Hg<sup>2+</sup>, and H1, H2 are modified the biocathode. In addition, the  $\zeta$ -potential measurements confirmed the successful assembly of the bioanode and biocathode (Fig. S8<sup>†</sup>). CV and linear scanning voltammetry (LSV) were performed to verify the catalytic reaction of GOD on the bioanode. In PBS with 5 mM glucose, a distinct oxidation peak at -0.48 V is observed (blue line), which corresponds to the splitting of DNAzyme to S1 and S2 by Pb<sup>2+</sup>, and the as-split S2

triggers the oxidation of glucose (Fig. 3c and d). The feasibility of the biocathode for Hg<sup>2+</sup> detection was investigated by DPV. In PBS with 500  $\mu$ M [Ru(NH<sub>3</sub>)<sub>6</sub>]<sup>3+</sup>, as-adsorbed [Ru(NH<sub>3</sub>)<sub>6</sub>]<sup>3+</sup> acquires electrons and is reduced to [Ru(NH<sub>3</sub>)<sub>6</sub>]<sup>2+</sup> at the biocathode. When AuNPs/MoS<sub>2</sub>@CuS (black line), S4 (blue line), S5, Hg<sup>2+</sup> (green line), and H1, H2 (red line) are successively coated on the CP surface, H1, H2/S5-Hg<sup>2+</sup>/S4/AuNPs/MoS<sub>2</sub>@CuS/CP exhibits the largest peak current value (Fig. 3e). Finally, the current of DPV was increased when the biocathode combined with the HCR strategy (Fig. S9<sup>†</sup>), which confirmed the signal amplification effect of HCR. These results prove the efficient signal amplification strategy from HCR for the biocathode.

In Fig. 4a and b, there is a linear relationship between the peak current with increasing scan rate in the range of 60 to 200 mV s<sup>-1</sup> (peak potential difference  $\leq$  -20 mV), which proves that the as-prepared bioanode and biocathode exhibit accurate identification ability.<sup>34,35</sup> Here, one biosensor was constructed based AuNPs/CP as the bioanode and the biocathode; the other one was fabricated based on AuNPs/MoS<sub>2</sub>@CuS/CP as the



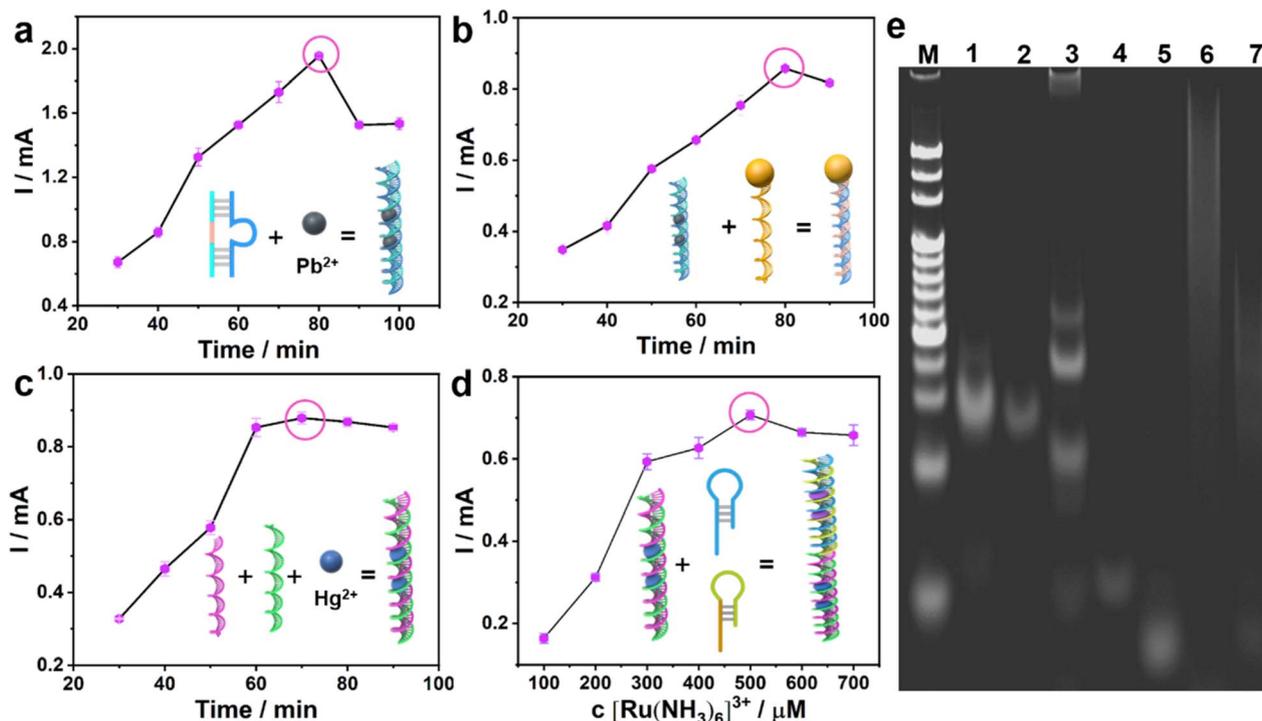


Fig. 2 The optimization of the hybridization reaction times: (a) incubation between  $\text{Pb}^{2+}$  and DNAzyme; (b) incubation between S3-GOD and as-split S2; (c) incubation among S4, S5 and  $\text{Hg}^{2+}$ ; (d) the optimization of  $[\text{Ru}(\text{NH}_3)_6]^{3+}$  concentration. (e) Gel electrophoresis analysis.

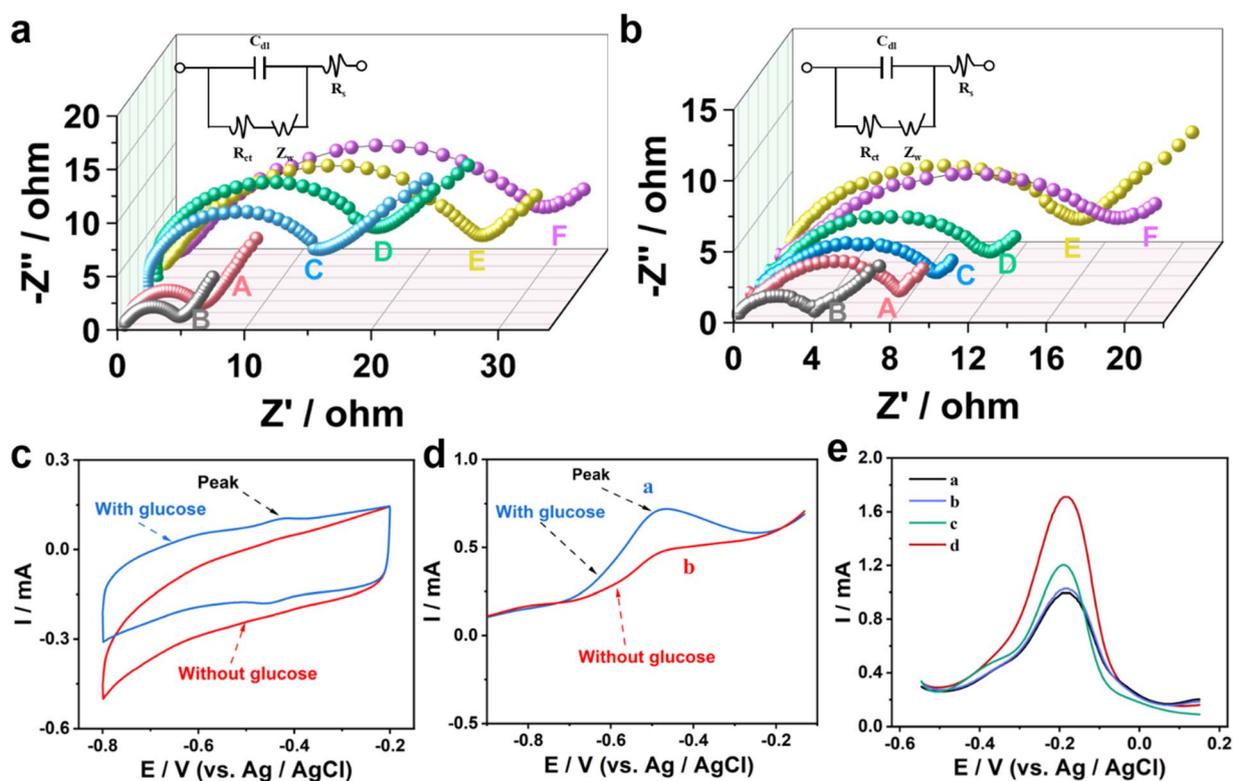


Fig. 3 (a) EIS of the bioanode: bare CP (A), AuNPs/ $\text{MoS}_2$ @CuS/CP (B), DNAzyme/AuNPs/ $\text{MoS}_2$ @CuS/CP (C), DNAzyme/AuNPs/ $\text{MoS}_2$ @CuS/CP (D),  $\text{Pb}^{2+}$ /BSA/DNAzyme/AuNPs/ $\text{MoS}_2$ @CuS/CP (E), S3-GOD/ $\text{Pb}^{2+}$ /DNAzyme/AuNPs/ $\text{MoS}_2$ @CuS/CP (F) (inset: the circuit diagram). (b) EIS of the biocathode: bare CP (A), AuNPs/ $\text{MoS}_2$ @CuS/CP (B), S4/AuNPs/ $\text{MoS}_2$ @CuS/CP (C), BSA/S4/AuNPs/ $\text{MoS}_2$ @CuS/CP (D), S5- $\text{Hg}^{2+}$ /S4/AuNPs/ $\text{MoS}_2$ @CuS/CP (E), H1, H2/S5- $\text{Hg}^{2+}$ /S4/AuNPs/ $\text{MoS}_2$ @CuS/CP (F) (inset: the circuit diagram). (c) CV and (d) LSV curves of the bioanode in PBS (pH 7.4) without glucose and with 5 mM glucose in the presence of  $\text{Pb}^{2+}$ . (e) DPV curves of the assembly process of the biocathode in PBS (pH 7.4) with  $[\text{Ru}(\text{NH}_3)_6]^{3+}$ .



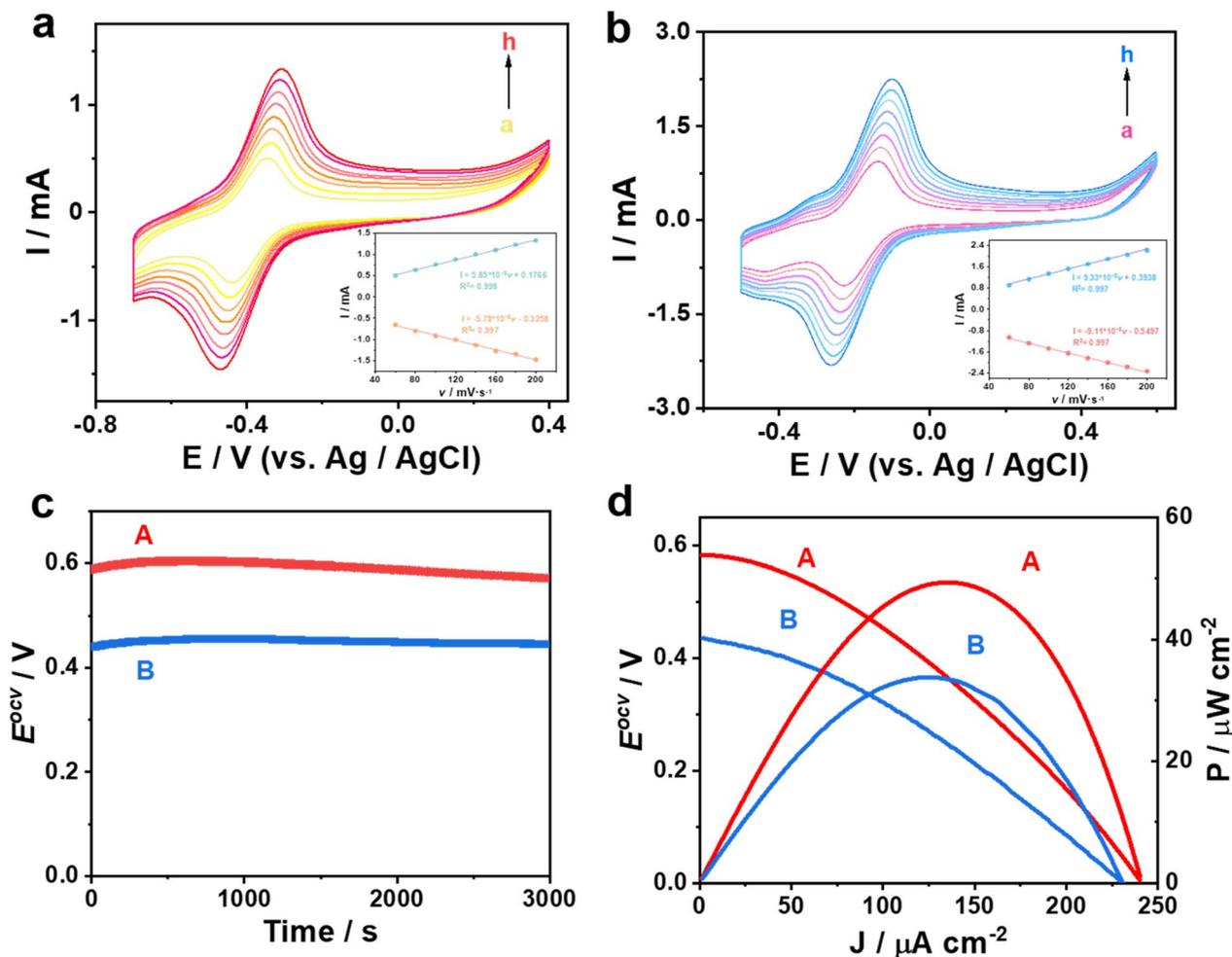


Fig. 4 (a and b) CV of S3-GOD/Pb<sup>2+</sup>/DNAzyme/AuNPs/MoS<sub>2</sub>@CuS/CP (*i.e.*, bioanode) (yellow to red lines) and H1, H2/S5 Hg<sup>2+</sup>/S4/AuNPs/MoS<sub>2</sub>@CuS/CP (*i.e.*, biocathode) (pink to blue lines) with different scan rates ( $\nu$ ): (a–h) 60, 80, 100, 120, 140, 160, 180, 200 mV s<sup>-1</sup>. (c) E<sup>ocv</sup> and (d) power output of the self-powered biosensor constructed of: (A) both S3-GOD/Pb<sup>2+</sup>/DNAzyme/AuNPs/MoS<sub>2</sub>@CuS/CP (the bioanode) and H1, H2/S5-Hg<sup>2+</sup>/S4/AuNPs/MoS<sub>2</sub>@CuS/CP (the biocathode), and (B) both S3-GOD/Pb<sup>2+</sup>/DNAzyme/CP (the bioanode) and H1, H2/S5-Hg<sup>2+</sup>/S4/CP (the biocathode).

bioanode and the biocathode. The  $E^{\text{ocv}}$  of the biosensor based on AuNPs/MoS<sub>2</sub>@CuS/CP is about 0.58 V, which is 0.13 V higher than that of the biosensor based on AuNPs/CP (Fig. 4c). Similarly, the maximum power output of the biosensors based on AuNPs/MoS<sub>2</sub>@CuS/CP and AuNPs/CP is 49.5 μW cm<sup>-2</sup> and 33.2 μW cm<sup>-2</sup>, respectively (Fig. 4d), which proves high-efficiency conduction of MoS<sub>2</sub>@CuS heterostructures.

For the single detection of Pb<sup>2+</sup>, the peak intensity of glucose oxidation at -0.48 V increases with increasing Pb<sup>2+</sup> concentration under optimal conditions in a CV test at the bioanode (Fig. S10†). Moreover, there is a good linear relationship between the logarithm of Pb<sup>2+</sup> concentration and current intensity in the range of 10 fM ~1 nM. The equation is:  $I = 0.01 \times \log C_{\text{Pb}^{2+}} + 0.20$  (correlation coefficient,  $R^2 = 0.995$ ), and the detection of limit (LOD) is calculated to be 3.1 fM ( $S/N = 3$ ). Analogously, the current response at -0.18 V is attributed to the reduction of [Ru(NH<sub>3</sub>)<sub>6</sub>]<sup>3+</sup> in the DPV test at the biocathode, which gradually increases with increasing Hg<sup>2+</sup> concentration (Fig. S11†). A linear correlation between the logarithm of Hg<sup>2+</sup>

concentration and current intensity in the range of 1 fM to 1 nM was fitted by the regression equation:  $I = 0.1 \times \log C_{\text{Hg}^{2+}} + 2.4$  ( $R^2 = 0.995$ ), and LOD is calculated to be 0.32 pM ( $S/N = 3$ ).

For the bidirectional detection of Pb<sup>2+</sup> and Hg<sup>2+</sup>,  $E^{\text{ocv}}$  of the novel biosensors was investigated at the double electrodes (Fig. 5). For instance, Hg<sup>2+</sup> concentration is determined to be 1 nM at the biocathode in a tap water sample (Fig. 5a and b). A good linear relationship between  $E^{\text{ocv}}$  and the logarithm of Pb<sup>2+</sup> concentration is calculated:  $E^{\text{ocv}} = 0.078 \log C_{\text{Pb}^{2+}} + 1.21$  ( $R^2 = 0.994$ ) with the LOD of 3.1 fM ( $S/N = 3$ ) in the range of 10 fM to 10<sup>6</sup> fM. Here, the  $E^{\text{ocv}}$  increases with the increment of Pb<sup>2+</sup> concentration at the bioanode. In another example, Pb<sup>2+</sup> concentration is determined to be 1 nM at the bioanode in the same tap water sample (Fig. 5c and d). There is a linear relationship between  $E^{\text{ocv}}$  and the logarithm of Hg<sup>2+</sup> concentration in the range of 1 fM to 10<sup>6</sup> fM:  $E^{\text{ocv}} = 0.083 \log C_{\text{Hg}^{2+}} + 1.34$  ( $R^2 = 0.995$ ), and the LOD is calculated to be 0.33 fM ( $S/N = 3$ ). Here, the  $E^{\text{ocv}}$  increases with the increment of Hg<sup>2+</sup> concentration at the biocathode. Compared with previously reported



sensors (Tables S2 and S3<sup>†</sup>), the bidirectional self-powered biosensor shows wider detection ranges and lower LODs for Pb<sup>2+</sup> and Hg<sup>2+</sup> detection. In order to further visualize the on-site detection of Pb<sup>2+</sup> and Hg<sup>2+</sup>, our capacitor amplification strategy was explored by smart Bluetooth data transfer with a smartphone for real-time read-out of test results (Fig. S12 and see Movie S1<sup>†</sup>).<sup>36–38</sup> In the test process, the mobile phone reads out the instantaneous current when different concentrations of Pb<sup>2+</sup> and Hg<sup>2+</sup> are in an unknown water sample, further realizing on-site and real-time detection (Fig. S13 and S14<sup>†</sup>).

The signal responses of the self-powered biosensor toward Pb<sup>2+</sup> and Hg<sup>2+</sup> detection remained at 83.5% and 82.1% of

original signal after the biosensors were stored at 4 °C for 15 days, further confirming the long-time stability (Fig. S15<sup>†</sup>). The recyclability of one as-designed biosensor was tested by analyzing different concentrations of Pb<sup>2+</sup> and Hg<sup>2+</sup>. All test results maintained within 5% of the error, which confirmed good recyclability for the biosensor (Fig. S16<sup>†</sup>). To confirm the specificity, there was no  $E^{\text{ocv}}$  signal when six possible interferences, *i.e.*, Na<sup>+</sup>, K<sup>+</sup>, Mg<sup>2+</sup>, Cu<sup>2+</sup>, Co<sup>2+</sup>, and blank water sample, were detected by the as-designed biosensor. The solution with Pb<sup>2+</sup> or Hg<sup>2+</sup> showed significantly high  $E^{\text{ocv}}$ , thus verifying the good specificity of the bidirectional biosensor (Fig. S17<sup>†</sup>). In addition, the relative standard deviations (RSDs) were

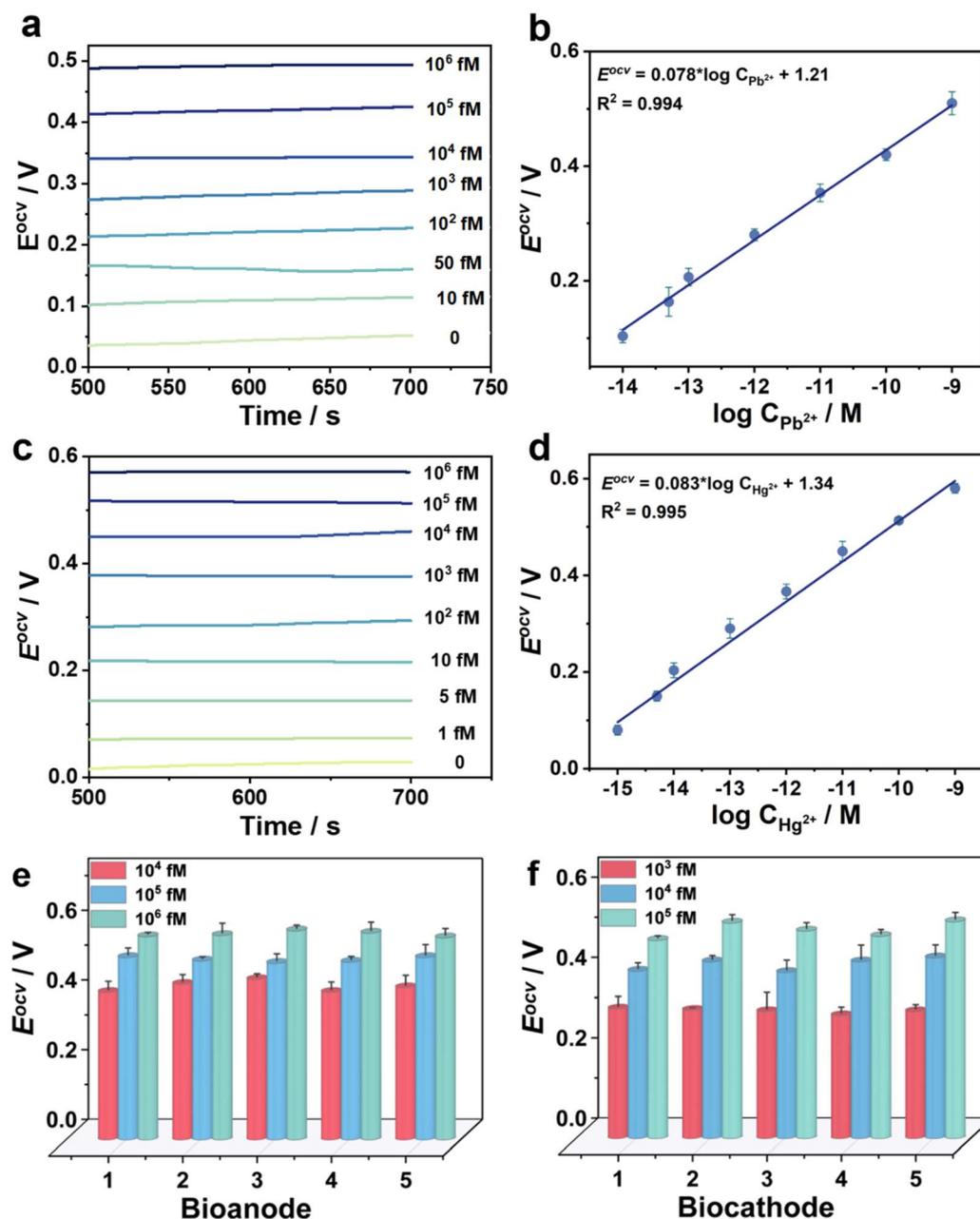


Fig. 5 (a)  $E^{\text{ocv}}$  of different concentrations of Pb<sup>2+</sup> and (b) relationship between  $E^{\text{ocv}}$  and Pb<sup>2+</sup> concentration; (c)  $E^{\text{ocv}}$  of different concentrations of Hg<sup>2+</sup> and (d) relationship between  $E^{\text{ocv}}$  and Hg<sup>2+</sup> concentration. (e and f) The repeatability of the self-powered biosensor.



measured to be  $\leq 5\%$  in five parallel experiments, indicating the good repeatability of the novel biosensor (Fig. 5e and f). To further test the practical application,  $\text{Pb}^{2+}$  and  $\text{Hg}^{2+}$  with the concentrations of 1, 10, 50, and 100 nM in tap water and lake water were prepared to perform a labelled recovery experiment. The RSDs values were calculated to be the range from 3.7% to 5.3% for  $\text{Pb}^{2+}$  and 2.1% to 5.9% for  $\text{Hg}^{2+}$ ; and the recovery rates were in the range from 96.4% to 105.0% for  $\text{Pb}^{2+}$  and 97.0% to 104.8% for  $\text{Hg}^{2+}$  (Tables S4 and S5†). These results demonstrate that the bidirectional self-powered biosensor possesses good selectivity, stability, and reproducibility, and could be used for practical sample detection.

## Conclusions

In summary, a bidirectional self-powered biosensor is designed to simultaneously monitor  $\text{Pb}^{2+}$  at the bioanode and  $\text{Hg}^{2+}$  at the biocathode. Here, the  $\text{MoS}_2@\text{CuS}$  heterostructures are successfully prepared to accelerate the electron transfer between glucose and the bioelectrode to increase the power output. Moreover, the novel biosensor realizes  $\text{Pb}^{2+}$  detection by the cutting effect of  $\text{Pb}^{2+}$  toward DNAzyme to trigger glucose oxidation at the bioanode, and monitors  $\text{Hg}^{2+}$  by forming unique T- $\text{Hg}^{2+}$ -T structures to activate HCR for the reduction of  $[\text{Ru}(\text{NH}_3)_6]^{3+}$  at the biocathode. The self-powered biosensor could not only perform linear detection of  $\text{Pb}^{2+}$  at the bioanode or  $\text{Hg}^{2+}$  at the biocathode, but also quasi-simultaneously realizes linear detection for both  $\text{Pb}^{2+}$  and  $\text{Hg}^{2+}$  at the bioanode and the biocathode. The bidirectional biosensor exhibits wide detection ranges of  $10^6$  fM  $\sim 10$  fM toward  $\text{Pb}^{2+}$  and  $10^6$  fM  $\sim 1$  fM toward  $\text{Hg}^{2+}$ , respectively; and the LODs of  $\text{Pb}^{2+}$  and  $\text{Hg}^{2+}$  are as low as 3.1 fM and 0.33 fM, respectively. This biosensor possesses highly efficient, ultra-sensitive, highly selective, and good reproducible detection of  $\text{Pb}^{2+}$  and  $\text{Hg}^{2+}$ . Meanwhile, smart and portable mobile phones and capacitors are well used for on-site direct reading detection. This work opens a new direction for designing novel bidirectional biosensors to detect multiple heavy metal ions.

## Data availability

All underlying data are available in the published article itself and its ESI.†

## Author contributions

J. X., F. W., X. L., W. Z., and H. Y. directed the project. Y. L performed the main experimental work. F. L provided experimental equipment. R. C., and W. T. provided some constructive suggestions for the experiments. All the authors discussed the experimental results.

## Conflicts of interest

There are no conflicts to declare.

## Acknowledgements

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