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High-fidelity imaging of a tumour-associated lysosomal enzyme with an acceptor engineering-boosted near-infrared fluorescent probe†

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To facilitate the understanding of the dynamic distribution and activity of lysosomal enzymes, it is highly desirable to develop high-fidelity near-infrared (NIR) activatable fluorescent probes. Here, we propose a general acceptor engineering strategy to construct NIR probes with lysosome-targeting capability. Upon isosteric replacement and additional functionalization, the β -gal-activatable probe OELysO-Gal exhibited excellent lysosome-targeting capability and favorable responsive performance to the enzyme of interest. Notably, the steric hindrance effect from acceptor engineering is modest, which renders the probe unprecedented affinity to enzymes. Upon the introduction of acceptor engineering, the lysosome-targeting probe became more sensitive to β -gal in cells and tissues, boosting the discrimination of high β -gal-expressing ovarian cancer tumours from low β -gal-expressing tissues. Furthermore, the superiority of OELysO-Gal was validated in real-time visualization of ovarian cancer in tumour-bearing mice. This elegant acceptor engineering strategy provides inspirational insights into the development of customized fluorescent probes for monitoring disease-associated biomarkers within subcellular organelles.

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Introduction

Currently, lysosomes are described as advanced organelles that play critical roles in cellular homeostasis and the mediation of a variety of physiological processes, such as protein degradation and plasma membrane repair.^{1,2} Pieces of evidence have shown that the aberrant activities of hydrolytic enzymes in lysosomes are associated with the pathogenesis of diseases such as storage disorders, cancer, neurodegenerative disorders, and cardiovascular diseases.^{3–5} Among these, β -galactosidase (β -gal) in lysosomes, an exoglycosidase, is involved in the catabolism of sugar conjugates, and its abnormal levels have been associated with the occurrence and progression of primary ovarian cancers, making the lysosomal enzyme a reliable biomarker for the early diagnosis and dynamic imaging of cancer.^{6–10} On-site monitoring of the hydrolytic enzymes in lysosomes in real-time pathways would provide insights into the detailed role of lysosomal enzymes in the progression of diseases, and further aid in the development of early diagnosis and therapeutic strategies.^{11–13}

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Fluorescence imaging has revolutionized fundamental studies in life sciences by enabling the visualization, characterization, and measurement of biological processes at the molecular and cellular levels in living systems.^{14–18} In particular, activatable fluorescent probes in the near-infrared (NIR) window have shown a higher signal-to-noise ratio for *in vivo* imaging.^{19–23} Unfortunately, when it comes to the subcellular dimension, existing NIR activatable probes are prone to dispersing throughout the cell, which largely compromises the fidelity of imaging for biomarkers within specific organelles.^{24–27} In the case of β -gal probes, for example, only a few lysosome-targetable fluorescent probes have been reported for β -gal thus far (Table 1).^{28–32} Most reported lysosome-targeting probes exhibited excitation and/or emission in the ultraviolet-visible region,^{28–30} which largely limits their further application *in vivo*. Recently, a lysosome-targeting probe Lyso-Gal exhibited desirable longer wavelength emission;³¹ however, the proximity of the lysosome-targeting moiety to the enzyme substrate raised concerns about steric hindrance toward the response. Moreover, anti-colocalization with mitochondria was not demonstrated with this probe. Alternatively, the organelle-targeting unit was grafted into the indolium moiety to afford the probe HCYXA- β Gal, which exhibited light-up NIR fluorescence in ovarian cancer cells.³² Nevertheless, the positive charge properties of indolium brought about potential mitochondrial-targeting ability, leading to a bias in the fluorescence signal.^{33,34} In addition, the accessibility of small molecule-based lysosome-targeting probes in living objects



Table 1 Comparison of photophysical and kinetic properties of **OELyso-Gal** and other reported lysosome-targeting probes

Probe	$\lambda_{\text{ex}}/\lambda_{\text{em}}$ (nm)	K_m^a (μM)	Response time ^b	LOD ^c (U/mL)	Pearson's coefficient ^d	Imaging application	Ref.
FC- β gal	360/460; 460/560	—	30 min (150 U/L)	4.0×10^{-5}	—	SKOV-3 cells	28
SRP	495/545	28.0	30 min (0.1 U)	4.19×10^{-7}	—	Senescent vascular cells	29
BMZ-Gal	450/565	78.75	30 min (10 U)	3.6×10^{-2}	0.71	SKOV-3 cells	30
Lyso-Gal	690/725	—	25 min (3 U/mL)	2.2×10^{-2}	0.83	SKOV-3 cells	31
HCyXA- β gal	680/710	68.37	250 s (10 U/mL)	1.2×10^{-2}	0.91	SKOV-3 cells and senescent WI-38 cells	32
OELyso-Gal	610/641	19.06	20 min (1.2 U/mL)	3.2×10^{-3}	0.96	SKOV-3 tumor <i>in vivo</i>	This work

^a K_m , the enzyme kinetic parameter Michaelis–Menten constant, which represents the affinity of the probe to the enzyme. ^b Response time, the time it takes for the probe to reach a plateau in fluorescence signal change (the concentration of the enzyme used). ^c LOD, the limit of detection. ^d The Pearson's co-localization coefficient between the lysosome-targeting probe and commercial lysosome tracker.

remains to be further explored (Table 1), despite the success of nanodevices in mapping lysosomal enzyme activity *in vivo*.^{35–37} Given this, it is still challenging and highly desired to develop novel NIR lysosome-targeting probes for specific detection and visualization of biomarkers *in vivo*.

Against this backdrop, we developed a general acceptor engineering strategy to construct NIR activatable probes with lysosome-targeting capability (Scheme 1). Upon isosteric replacement and additional functionalization, the electron-acceptor dicyanyl group in **OEN-OH** was replaced by cyanoacetamide with a morpholine ring to afford the fluorophore **OELyso-OH**, which maintained the NIR fluorescence but possessed additional lysosome-targeting ability. As a proof-of-concept, the enzymatic substrate β -galactopyranoside unit was directly grafted onto the fluorophore to afford the lysosome-targeting probe **OELyso-Gal**. By virtue of acceptor engineering, **OELyso-Gal** exhibited the advantages of high affinity ($K_m = 19.06 \mu\text{M}$) as well as fast response (20 min) to β -gal in the docking simulation and enzymatic kinetic investigations. In cell imaging, the fluorescence of **OELyso-Gal** could be activated specifically by lysosomal β -gal in SKOV-3 cells, hence allowing real-time imaging of intracellular β -gal with optimized fidelity. Moreover, the lysosome-targeting probe was found to be more sensitive to β -gal in cells and tissues, which boosted the

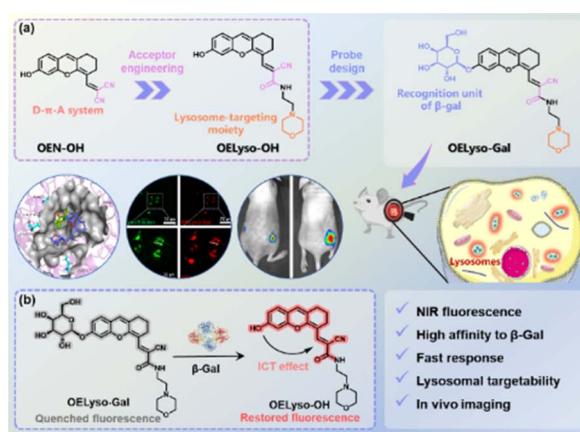
dynamic monitoring of β -gal in ovarian tumour-bearing mice. Importantly, **OELyso-Gal** is the first lysosome-targeting NIR probe for tracking β -gal activity *in vivo*.

Results and discussion

Molecular design and synthesis

The dihydroxanthene-based scaffold **OEN-OH**, characterized as a donor– π –acceptor (D– π –A) system, has been utilized as a precursor for NIR probes with advantages of good photostability and excellent biocompatibility.^{12,38} Herein, the electron-acceptor dicyanyl group in **OEN-OH** was replaced by cyanoacetamide with a morpholine ring to afford the fluorophore **OELyso-OH** (Scheme 1). Considering the rule of isosteric replacement, the obtained **OELyso-OH** was expected to maintain the NIR fluorescence but possess additional lysosome-targeting ability. Moreover, the incorporation of a lysosome-targeting moiety may have minimal impact on the response toward the analyte of interest owing to the distant distribution. As proof of the concept, the enzymatic substrate β -galactopyranoside unit was directly grafted on the fluorophore to afford the lysosome-targeting probe **OELyso-Gal**. Upon substitution with the enzyme-trigger, the NIR fluorescence was expected to be quenched through hindering the intramolecular charge transfer (ICT) effect but intensive NIR fluorescence was observed after exposure toward β -gal. In living cells, the probe **OELyso-Gal** is expected to be preferentially accumulated in lysosomes and continuously activated by lysosomal β -gal, and thus may afford a significant advantage in terms of sensitivity and fidelity.

The dihydroxanthene-based scaffold **OE-OH** was prepared from a previous method,³⁹ followed by Knoevenagel condensation with ethyl cyanoacetate to obtain the precursor **OEE-OH**. To introduce the organelle-targeting unit, the ester intermediately underwent an ammonolysis reaction with 4-(2-aminoethyl) morpholine to afford the lysosome-targeting fluorophore **OELyso-OH**, while the dicyanyl-substituted fluorophore **OEN-OH** was obtained from a Knoevenagel condensation between **OE-OH** and malononitrile.⁴⁰ The two β -gal-activated probes **OELyso-Gal** and **OEN-Gal** were synthesized through a nucleophilic substitution reaction and deacetylation. The detailed synthetic routes are depicted in Schemes S1 and S2,[†] and the structures were characterized by ^1H NMR, ^{13}C NMR and HRMS.



Scheme 1 (a) Schematic illustration of acceptor engineering on the dihydroxanthene-based scaffold and rational design of the probe **OELyso-Gal**. (b) Proposed sensing mechanism of **OELyso-Gal** toward lysosomal β -gal.



Spectroscopic investigation

Having obtained the fluorophores, the solvatochromic absorption and emission spectra of **OELyo-OH** and **OEN-OH** were recorded in different solvents. As shown in Fig. S13,† the two fluorophores exhibited a bathochromic shift in polar aprotic solvents with increasing orientational polarizabilities, and importantly, **OELyo-OH** exhibited better resistance toward the solvent polarity changes than **OEN-OH**. Such an observation was more evident in the absorption spectra in polar protic solvents (Fig. S14†) as well as the fluorescence spectra in different solvents (Fig. S15†). Of note, the advantage is also distinct in water, in which the fluorescence of **OEN-OH** was almost quenched while the one of **OELyo-OH** remained. To evaluate the efficiency of isosteric replacement, the optical properties of **OELyo-OH** and **OEN-OH** in PBS (10 mM, pH = 7.4, containing 30% DMSO) were investigated (Fig. 1a). Although the absorption spectra varied, both fluorophores exhibited a prominent emission peak at about 640 nm upon excitation at 560 nm, confirming that the fluorescence wavelength was not affected obviously by the introduction of acceptor engineering. A similar conclusion could also be obtained from the consistent wavelength in the solvatochromic investigation.

To further support the idea, density functional theory (DFT) and time-dependent density functional theory (TD-DFT) were implemented using Gaussian 09. As shown in Fig. 1b, both the highest occupied molecular orbital (HOMO) and lowest unoccupied molecular orbital (LUMO) in **OELyo-OH** and **OEN-OH** were located mainly in the whole fluorophore, and a similar

energy gap between HOMO and LUMO could also be found in the two fluorophores, which could contribute to their similar intramolecular charge transfer (ICT) strength and thus similar optical behavior.⁴¹ Furthermore, the calculated vertical excitation and emission wavelengths of **OELyo-OH** and **OEN-OH** were very close, substantiating again the minimal effect of the isosteric replacement on the optical properties.⁴² By contrast, when a block unit was grafted on the hydroxyl group (*e.g.*, a β -galactopyranoside unit to afford **OELyo-Gal**), both the energy gap and the calculated wavelengths changed dramatically. The results manifest that the functionalized fluorophore **OELyo-OH** may provide a robust platform to develop activatable probes with distinct fluorescence changes as well as potential lysosomal targeting capability.

Response mechanisms of **OELyo-Gal**

Inspired by the desired results, the behavior of the probe **OELyo-Gal** in response to β -gal was next characterized. First, the binding mode of **OELyo-Gal** to β -gal was investigated by molecular docking simulation. As shown in Fig. 1c and S16,† the recognition group β -galactopyranoside unit can enter the enzymatic pocket successfully and form hydrogen bonds with the surrounding amino acid residues, which demonstrates the high affinity of **OELyo-Gal** toward β -gal.^{43,44} More importantly, the receptor ends of the fluorophore were stuck outside the pocket as expected, suggesting that the introduction of morpholine rings may have little effect on the binding mode.^{45,46} In addition, the binding mode of **OEN-Gal** (marked in yellow) is highly overlapped with the one of **OELyo-Gal** (marked in blue).

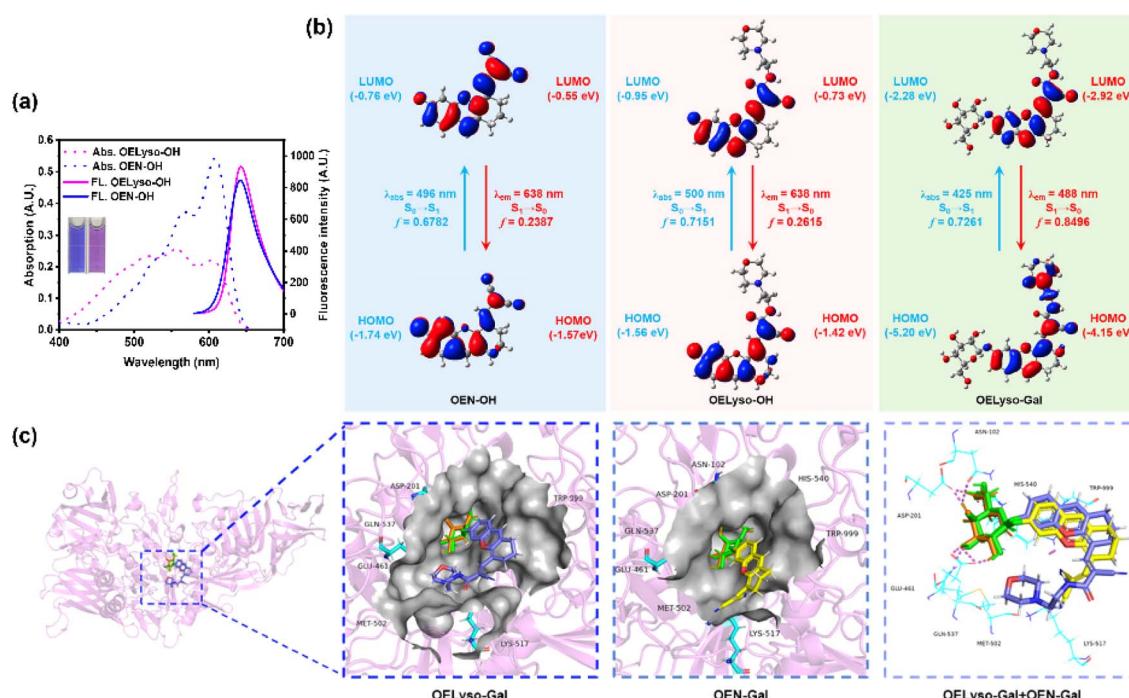


Fig. 1 (a) The absorption and fluorescence spectra of **OEN-OH** (10 μ M) and **OELyo-OH** (10 μ M) in PBS (10 mM, pH = 7.4, containing 30% DMSO). Inset: the corresponding images of **OEN-OH** and **OELyo-OH**. (b) Calculated frontal molecular orbitals involved in the vertical excitation and emission of **OEN-OH**, **OELyo-OH** and **OELyo-Gal**. (c) Molecular docking simulation of the binding mode between **OELyo-Gal** (in blue)/**OEN-Gal** (in yellow) and β -gal (ligand of galactose, in orange).



These results suggest that the acceptor engineering may have a modest effect on the affinity of probes to the enzyme, authenticating the accessibility of **OELyo-Gal** into the β -gal catalytic pocket for subsequent activation.

To validate the enzymatic activation, the absorption and emission spectra of **OELyo-Gal** were inspected in the absence and presence of β -gal. Compared with the initial spectra, **OELyo-Gal** (10 μ M) incubated with β -gal (1.2 U/mL) for 20 min exhibited a significant hypsochromic shift in absorption spectra (Fig. 2a), along with an intensive fluorescence enhancement in emission spectra (Fig. 2b). By contrast, the fluorescence enhancement could be attenuated by the competitive inhibitor D-galactose in a dose-dependent manner (Fig. S17†), proving that the optical changes were triggered specifically by the presence of β -gal. To verify the conclusion, high-performance liquid chromatography (HPLC) analysis was carried out. As shown in Fig. S18b,† **OELyo-Gal** itself exhibited a signal peak at about 5.9 min, but after incubation with β -gal, the peak decreased while another peak appeared at 6.9 min. As the incubation time prolonged, the newly emerged peak dominated in the whole elution, which was attributed to the fluorophore **OELyo-OH** (7.0 min). The further high-resolution mass spectrum (HRMS) analysis (Fig. S18c†) also indicated the hydrolysis

of the β -galactoside bond in **OELyo-Gal** (*m/z*: calc., 570.2452; found, 570.2461) to release the fluorophore **OELyo-OH** (*m/z*: calc., 408.1923; found, 408.1928) after incubation with β -gal. These results supported the allowed enzymatic hydrolysis of the β -galactoside bond in **OELyo-Gal** by the catalysis of β -gal.

Optical response of **OELyo-Gal** to β -gal

Having verified the enzymatic hydrolysis, the spectral response of **OELyo-Gal** to β -gal was characterized in detail. As shown in Fig. 2a, **OELyo-Gal** showed a red color with a broad absorption spectrum ranging from 400 to 600 nm. Upon incubation with β -gal (0–1.2 U/mL) in solution (PBS/DMSO = 7 : 3, V/V, pH 7.4) at 37 °C for 20 min, the absorption peak of **OELyo-Gal** at 525 nm decreased while two peaks emerged at around 567 and 609 nm. This also appeared as the solution color changed from red to violet. Of note, the color change and hypsochromic shift are consistent with the optical properties of the fluorophore **OELyo-OH**. Upon excitation at 560 nm, the fluorescence of the probe **OELyo-Gal** ranging from 580 to 740 nm increased with the concentration of β -gal in the range of 0–1.2 U/mL (Fig. 2b). A good linearity was found between the fluorescence intensity at 641 nm and β -gal concentration, which enables quantitative detection of β -gal ranging from 0 to 0.8 U/mL (Fig. 2c). The limit

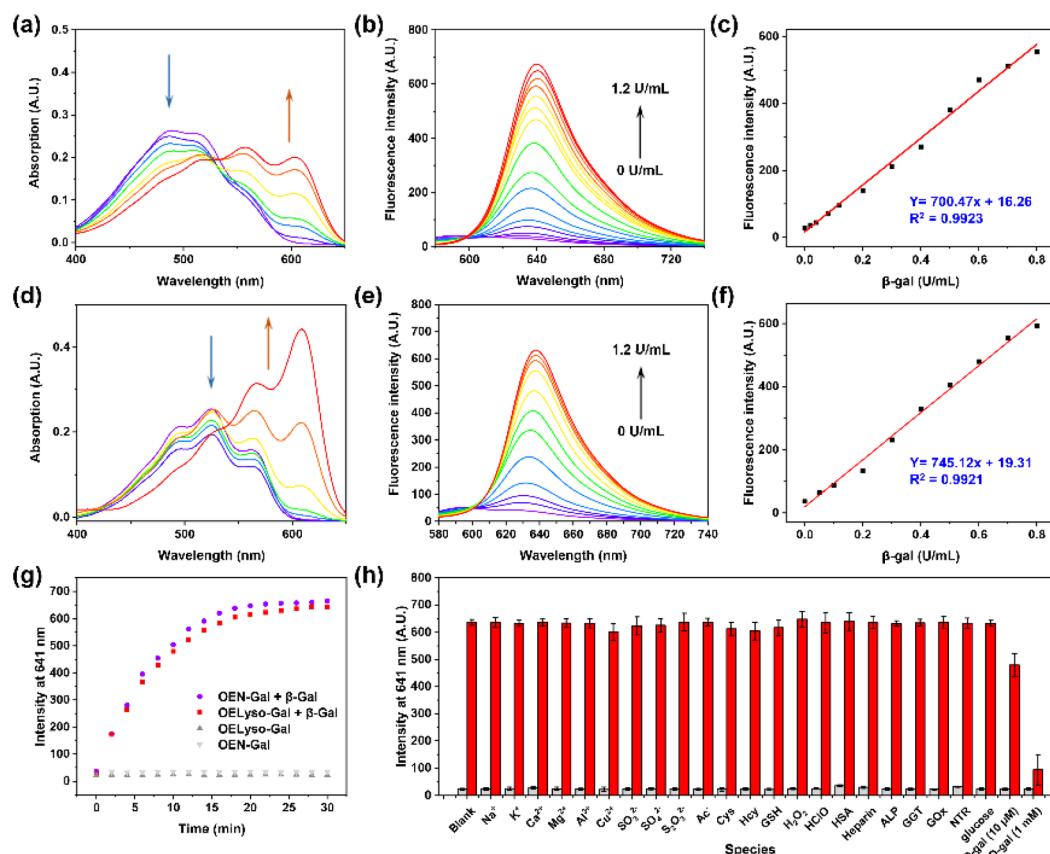


Fig. 2 Spectral profiles of **OELyo-Gal** (10 μ M) and **OEN-Gal** (10 μ M) incubated with β -gal for 20 min. (a–c) Absorption spectra (a), fluorescence spectra (b) and fluorescence intensity (c) of **OELyo-Gal** incubated with β -gal. (d–f) Absorption spectra (d), fluorescence spectra (e) and fluorescence intensity (f) of **OEN-Gal** incubated with β -gal. (g) Time-dependent fluorescence intensity of **OELyo-Gal** (red blocks) and **OEN-Gal** (purple dots) in the presence of β -gal (1.2 U/mL). (h) Fluorescence intensity of **OELyo-Gal** at 641 nm upon incubation with β -gal in the absence or presence of various interferents.



of detection (LOD) of **OELyo-Gal** was calculated to be 3.2×10^{-3} U/mL, a high value of sensitivity comparable with most of the probes. The optical titration experiment of **OEN-Gal** toward β -gal activities was also carried out. As depicted in Fig. 2d and e, a similar hypsochromic shift was observed in absorption spectra and a consistent fluorescence enhancement at 639 after incubation with β -gal (0–1.2 U/mL) for 20 min at 37 °C. The LOD of **OEN-Gal** was determined to be 3.0×10^{-3} U/mL (Fig. 2f).

After incubation with potentially interfering biological substances including cations, reduction anions, reactive oxygen species, amino acids, and enzymes with **OELyo-Gal** (10 μ M) for 20 min, negligible fluorescence was observed, indicating that **OELyo-Gal** has excellent selectivity toward β -gal over other relevant interferents (Fig. 2h). Furthermore, the competitive experiment demonstrated that the presence of other interferents has a negligible effect on the fluorescence enhancement of **OELyo-Gal** except for the groups containing α -galactose (competitive inhibitor of β -gal). The pH effects also exhibited a desirable fluorescence response to β -gal in the pH range from 6.0 to 8.6 (Fig. S19†), which is also consistent with the good catalytic activity of β -gal in this range. These results demonstrate that **OELyo-Gal** exhibits the desired performance for sensitive detection of β -gal in biological matrices.

To further understand the enzymatic kinetics of probes, the fluorescence intensities of **OELyo-Gal** and **OEN-Gal** as a function of time were compared upon incubation with β -gal (1.2 U/mL). As depicted in Fig. 2g and S20,† the fluorescence increased quickly in 15 min, which reached a plateau at 20 min, indicative of the fast response of both probes to β -gal. Of note, the signal

enhancement of **OELyo-Gal** (25.2 folds) was higher than that of **OEN-Gal** (18.3 folds). Furthermore, the Michaelis–Menten and Lineweaver–Burk equations were constructed.^{40,45} As shown in Fig. S21,† the kinetic parameter Michaelis constant (K_m) of **OELyo-Gal** was calculated to be 19.06 μ M, the lowest value reported for probes with lysosomal targetability (Table 1). The result indicates the favorable affinity of **OELyo-Gal** to β -gal, which could be attributed to the minimal steric hindrance of the probe to the enzymatic pocket by virtue of acceptor engineering, while the K_m of **OEN-Gal** was determined to be 16.24 μ M. These results were consistent with the above molecular docking results (Fig. 1c). More importantly, **OELyo-Gal** with superior affinity to β -gal could be an ideal candidate for the fast detection and high-fidelity imaging of the enzyme in biological scenarios.

Real-time fluorescence imaging of lysosomal β -gal in living cells

Inspired by the favorable performance of **OELyo-Gal** *in vitro*, its applicability for visualization of the endogenous β -gal in living cells was assessed. Before that, the cytotoxicity of **OELyo-Gal** against SKOV-3 cells was evaluated using MTT assay. No distinct effect was found on the cell viability (>90%) at concentrations less than 80 μ M (Fig. 3b), indicating the excellent biocompatibility of **OELyo-Gal**. Another determinant requirement for the practical applications in long-term monitoring is the high photostability toward high-energy lasers.^{38,47} The photostability of **OELyo-Gal** was evaluated under the excitation of a 150 W xenon lamp. As shown in Fig. 3a, the signal intensities at 641 nm before and after β -gal incubation were relatively stable

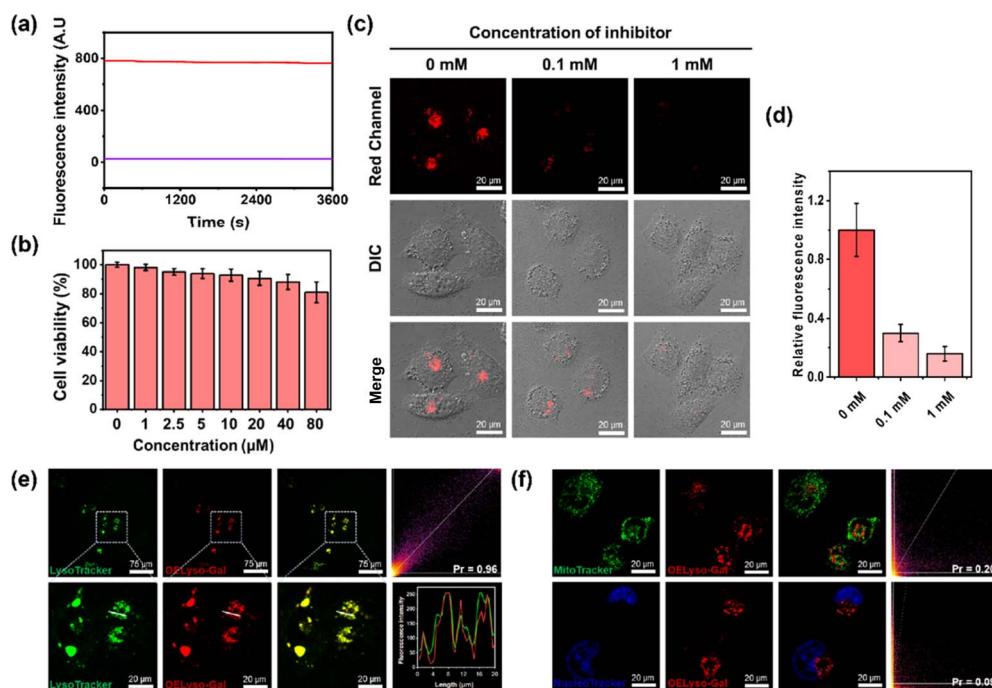


Fig. 3 (a) The photostability of **OELyo-Gal** and **OEN-Gal** incubated with β -gal. (b) Cell viability of SKOV-3 cells incubated with **OELyo-Gal**. (c and d) Fluorescence images and relative fluorescence intensity of **OELyo-Gal** (10 μ M)-staining SKOV-3 cells treated with inhibitors (α -galactose, 100 μ M or 1 mM). (e and f) Fluorescence imaging of SKOV-3 cells incubated with **OELyo-Gal** (10 μ M) for 30 min and then stained with LysoTracker-Green (5 μ M), MitoTracker-Green (1 μ M), or Hoechst (1 μ M) for another 30 min.



during the scanning period of 60 min, indicating the desirable resistance to photobleaching. Next, the probe was applied for tracking endogenous β -gal in SKOV-3 cells, a cell line of primary ovarian cancer with high expression of β -gal.^{7,48} As shown in Fig. S22,[†] red fluorescence was observed in SKOV-3 cells, in which the signals intensified with increasing concentration of the probe. Considering the fidelity of the signals, the working concentration of the probe is determined to be 10 μ M. Later, to elucidate the specificity of the probe in cells, a competitive inhibition experiment was carried out in SKOV-3 cells. The red fluorescence weakened gradually with increasing concentration of D-galactose (Fig. 3c and d), substantiating that the fluorescence enhancement is highly specific to the activity of intracellular β -gal.

After that, to elucidate the subcellular organelle-targeting ability of **OELysO-Gal**, the co-localization imaging experiment was conducted. The SKOV-3 cells were incubated with **OELysO-Gal** for 30 min and then stained with the commercial tracker for lysosome (LysoTracker-Green), mitochondria (MitoTracker-Green), and nucleus (Hoechst 33342), respectively, for another 30 min. As shown in Fig. 3e, the red fluorescence produced by **OELysO-Gal** overlapped well with the green fluorescence rendered by LysoTracker Green. The fluorescence intensity profiles of **OELysO-Gal** and LysoTracker-Green in the regions of interest (ROI, given by a white line) were well-fitting, revealing the excellent lysosome-targeting ability of **OELysO-Gal**. Moreover, Pearson's co-localization coefficient between **OELysO-Gal** and LysoTracker-Green was calculated to be 0.96, a value higher than that of the reported lysosome-targeting probes for β -gal (Table 1). The result confirms the effectiveness of acceptor engineering in the targeting of organelles. By contrast, Pearson's co-localization coefficient between **OELysO-Gal** and MitoTracker-Green (0.20) or Hoechst 33342 (0.09) was much smaller (Fig. 3f). These results verify that the probe **OELysO-Gal** could be accumulated in the lysosomes and activated specifically by lysosomal β -gal in SKOV-3 cells.

To further substantiate the idea, the dynamic activation process of **OELysO-Gal** was illustrated in SKOV-3 cells pre-stained with LysoTracker-Green. As depicted in Fig. 4a and b, the fluorescence of **OELysO-Gal** exhibited persistent light-up at specific organelles. The red fluorescence was observed within 5 min and gradually intensified with prolonged incubation. More importantly, the time-lapsed red fluorescence derived from activated **OELysO-Gal** merged well with lysosomes labeled by LysoTracker-Green, which was consistent with the fact of lysosomal distribution of β -gal reported in previous research studies.^{31,49} The result demonstrates that the fluorescence of **OELysO-Gal** is indeed activated by lysosomal β -gal in ovarian cancer cells, allowing real-time fluorescence imaging of intracellular β -gal with optimal fidelity.

Evaluation of β -gal activities in cells and tumour-bearing mice

Having demonstrated the success in specific imaging of lysosomal β -gal with **OELysO-Gal**, the significance of lysosomal targeting for β -gal detection in cells was revealed by comparing with the control probe **OEN-Gal**. Although no obvious difference

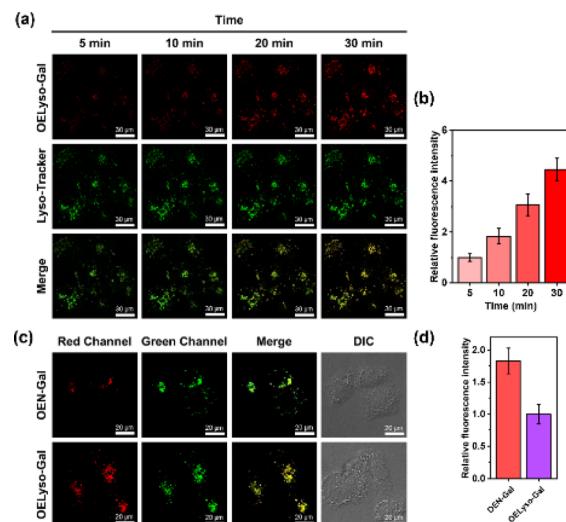


Fig. 4 (a and b) Real-time fluorescence images and relative fluorescence intensity of **OELysO-Gal** (10 μ M) in SKOV-3 cells pretreated with LysoTracker-Green (5 μ M). Scale bar: 30 μ m. (c and d) Fluorescence images and relative fluorescence intensity of LysoTracker-Green (5 μ M)-staining SKOV-3 cells incubated with **OEN-Gal** (10 μ M) or **OELysO-Gal** (10 μ M), respectively. Scale bar: 20 μ m.

was found in the optical response *in vitro*, a probe that could locate and accumulate in lysosomes is expected to provide higher signal intensities for lysosomal β -gal. As expected, upon the introduction of acceptor engineering, the fluorescence enhancement of **OELysO-Gal** was almost twice as large as that of **OEN-Gal** without lysosome-targeting ability (Fig. 4c and d). Similarly, their fluorescence signals overlapped well with those of LysoTracker-Green. The result suggests that the lysosome-targeting probe is more sensitive to imaging β -gal in cells, substantiating the role of the acceptor-engineering strategy proposed herein. Given its higher efficiency for endogenous β -gal detection, **OELysO-Gal** was utilized to evaluate the β -gal levels in different cells. **OELysO-Gal** was incubated with SKOV-3, HeLa, Hepa 1-6 and HepG2 cells for 30 min at 37 °C and then the fluorescence images were recorded. As shown in Fig. S24,[†] intensive fluorescence was found in SKOV-3 cells but faint fluorescence signals were observed in other cells, which have been found to have low β -gal levels.^{19,40} These results suggest that the probe **OELysO-Gal** could be an edge tool for discriminating β -gal-overexpressing ovarian cancer cells from other cells.

As a case in point, the practical feasibility of **OELysO-Gal** for real-time *in vivo* visualization of β -gal activity was evaluated in tumour-bearing mice. Before that, *in vitro* hemolysis assay was carried out. As shown in Fig. S25,[†] no significant hemolysis occurred at a concentration of **OELysO-Gal** up to 100 μ M. Then, SKOV3 subcutaneous xenograft nude mice were treated with **OELysO-Gal** *via* intra-tumoural injection. As shown in Fig. 5a, distinct NIR fluorescence was collected specifically in the tumour region within 10 min, and gradually increased to the maximum within 120 min, indicating the quick activation of **OELysO-Gal** *in situ*. According to the intensity measurements in



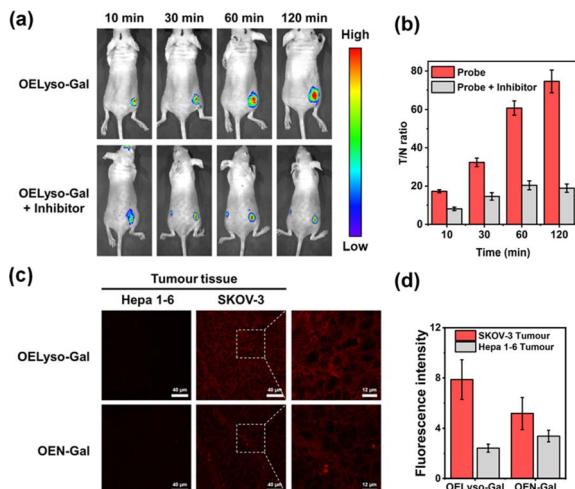


Fig. 5 (a) Time-dependent fluorescence images of β -gal in the SKOV3 tumor-bearing mice intratumorally injected with OELysogal (100 μ M) or OELysogal (100 μ M) + D-galactose (1 mM). (b) Signal ratio between the tumor and normal site (T/N) in animals at different times. (c and d) Fluorescence images (c) and relative fluorescence intensity (d) of OELysogal (10 μ M)/OEN-Gal (10 μ M) in Hepa 1-6 and SKOV-3 tumour tissue. Scale bar: 40 mm.

the region of interest, the signal ratio between the tumour and normal site (T/N) reached 74.6, indicating successful tumour identification (Fig. 5b). To further validate the finding that NIR signals were indeed activated by β -gal in ovarian tumours, the mice were preinjected with D-galactose for 30 min and then treated orthotopically with OELysogal. The NIR fluorescence in the ovarian tumour attenuated a lot compared with that in the absence of inhibitors (T/N value decreased to 18.9), verifying that the increased fluorescence signals at the tumour site came from β -gal activated OELysogal. Collectively, these results implied the potential of the probe OELysogal as a promising tool for monitoring ovarian cancer *in vivo*.

Finally, to illustrate the early detection capability, we tested the accessibility of OELysogal in tissue imaging. As shown in Fig. 5c, high-contrast fluorescence was observed in ovarian tumour slices while no fluorescence was observed in low β -gal-expressing liver tumour slices. The result demonstrates the capability of OELysogal for discriminating between high and low β -gal-expressing tissues *in situ*. Moreover, the fluorescence intensity of OELysogal in ovarian tumour tissue was found to be higher than that of OEN-Gal (Fig. 5d), which is consistent with the cell imaging in Fig. 4c. The result validates the observation that lysosomal specificity improves sensitivity in tissues and, more importantly, demonstrates the promise of OELysogal in early detection in clinical scenarios.

Conclusions

In summary, we successfully designed and constructed a lysosome-targeting dihydroxanthene-based NIR activatable probe, OELysogal, for imaging disease-associated enzymes in lysosomes. OELysogal exhibited high affinity and fast response to β -gal in the enzymatic kinetic investigations, revealing minimal

steric hindrance effects from acceptor engineering. Notably, the K_m of OELysogal was found to be 19.06 μ M, the lowest value reported for probes with lysosomal targetability. Moreover, OELysogal had a higher co-localization coefficient with the lysosome tracker than other reported probes, and such excellent lysosomal specificity was found to enhance the sensitivity of OELysogal in living ovarian cancer cells and in an ovarian tumour section. Furthermore, the superiority of OELysogal was demonstrated in real-time visualization of ovarian cancer in tumour-bearing mice, which is the first *in vivo* implementation with a lysosome-targeting probe activated by β -gal. We believe that this design strategy of acceptor engineering will provide inspirational insights into the development of customized fluorescent probes for monitoring disease-associated biomarkers within subcellular organelles.

Data availability

Synthetic procedure, characterization, photophysical measurements, calculation results and fluorescence imaging can be found in the main text or the ESI.†

Author contributions

B. Feng and F. Chu wrote and reviewed the manuscript. B. Feng synthesized the compounds. F. Chu performed biochemical experiments. Y. Fang performed the calculation experiments. M. Liu and X. Feng performed imaging experiment. J. Dong, and F. Chen reviewed and commented the manuscript. W. Zeng supervised the entire project.

Conflicts of interest

The authors declare that they have no competing financial interests.

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