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Bacterial elimination *via* cell membrane penetration by violet phosphorene peripheral sub-nanoneedles combined with oxidative stress†

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The effectiveness of an antibacterial agent is strongly influenced by its antibacterial mechanism, which, in turn, depends on the agent's topological structure. In the natural world, the nanoprotusions on the surface of insect wings give them excellent antimicrobial properties through physical penetration while being compatible with host cells. Inspired by the novel nanostructure of insect wings, violet phosphorus (VP), a new member of the phosphorus family, has antibacterial potential due to the sub-nanoneedle on its edge. Here, we demonstrate that VP and its exfoliated product, violet phosphorene nanosheets (VPNSs), have superior antibacterial capability against pathogens *via* cell membrane penetration induced by peripheral sub-nanoneedles combined with oxidative stress. The results show that VPNSs can inactivate more than 99.9% of two common pathogens (*Escherichia coli* and *Staphylococcus aureus*) and more than 99.9% of two antibiotic-resistant bacteria (*Escherichia coli* pUC19 and methicillin-resistant *Staphylococcus aureus*), while showing almost no toxicity toward normal cells at a high concentration of 2.0 mg mL⁻¹. Moreover, VPNSs can achieve effective treatment of induced skin wound infections and bacterial keratitis (BK) by *Staphylococcus aureus* and methicillin-resistant *Staphylococcus aureus*, respectively, showing promising potential for ocular and skin wound infection theragnostics.

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Introduction

Nature is a versatile designer, sculpting various surprising micro-wonders such as insect wings whose surfaces have antibacterial and antibiofilm properties.^{1–3} These wings have dense surface protrusions at the nano- and micro-levels, which function as natural barriers to combat bacterial pathogens and prevent biofilm formation. The nanoprotusions rupture microbial cells upon contact and lead to bacterial death, which is an effective physical mechanism for protecting insects from bacterial infection.^{4–7} Surprisingly, these nanoprotusions have low toxicity and even promote eukaryotic cell proliferation.^{8,9} Several pieces of evidence suggested that the rigidity of the

bacterial cell wall was significantly greater than that of the eukaryotic cell membrane.^{10–12} Eukaryotic cells could avoid membrane damage and cell death by stretching and twisting the shape to fit the nanostructure.¹³ Researchers inspired by the natural antibacterial structure have created new biomimetic surfaces with special nanostructured morphologies and self-cleaning antibacterial capacity.^{14–17} The nanotopographies and chemical configurations for fabricated biomimetic surfaces show a significant impact on their antibacterial functions. More efficient bactericidal and antibiofilm characteristics have been obtained using specially structured antibacterial surfaces that result in unique mechanisms.^{18,19}

Layered phosphorus and phosphorene have been demonstrated to be effective antibacterial agents, attracting growing interest in related fields due to their high bactericidal efficiency,^{20–24} biosafety,^{25–30} and on-demand degradability.^{31–34} Reactive oxygen species (ROS) are easily produced from phosphorus and phosphorene structures due to the lone pair electrons from phosphorus atoms.^{35–38} Layered phosphorus and phosphorene structures provide more active sites to produce ROS due to their high specific surface areas, which has been well demonstrated for black phosphorus (BP).^{39–42} The nanotopographies and chemical configurations of these layered structures may provide further ways to enhance their antibacterial activity in addition to ROS effects.^{43–46} The special structures of recently produced violet phosphorus (VP) and phosphorene

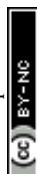
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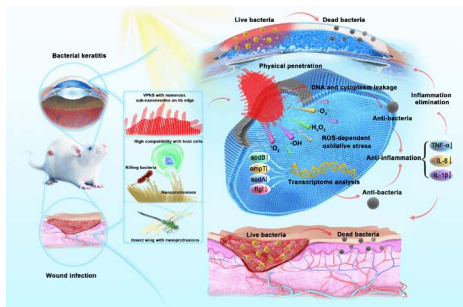
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Scheme 1 The superior antibacterial capability of VPNSs against pathogens via cell membrane penetration induced by peripheral sub-nanoneedles combined with oxidative stress for the treatment of wound infection and bacterial keratitis.

nanosheets (VPNSs) feature numerous sub-nanoneedles on the flake periphery, whose high surface energy favors their interaction with the cell membrane of bacteria. The phenomenon is analogous to protrudes on the surface of an insect wing at the macro-scale, leading to bacterial death.^{47–49} Hence, both ROS-dependent oxidative stress and physical damage are the expected antibacterial mechanisms of VP and VPNSs.

Herein, we report on the antibacterial actions of VP and VPNSs and compare them with the antibacterial mechanism of BP to confirm the additional effects of physical penetration arising from the former structures. Meanwhile, Table S1† compares the antibacterial mechanism of VPNSs with some up-and-coming 2D nanomaterials. Higher antibacterial activity than BP is demonstrated by VP and VPNSs after a series of antibacterial tests against two common pathogens (*Escherichia coli* (*E. coli*) and *Staphylococcus aureus* (*S. aureus*)) and two antibiotic-resistant bacteria (methicillin-resistant *Staphylococcus aureus* (MRSA) and *Escherichia coli* pUC19 (*E. coli* pUC19)). This is determined by the effect of the peripheral sub-nanoneedle induced VP and VPNSs penetrating into the cell membrane combined with oxidative stress to eliminate bacteria. Moreover, *in vivo* mouse experiments prove that VPNSs can achieve effective treatment of induced skin wound infections and bacterial keratitis (BK) by *S. aureus* and MRSA, respectively, showing promising potential for ocular and skin wound infection theragnostics (Scheme 1). This study offers a new 2D antibacterial agent to combat pathogens and proposes a new synergistic mechanism for eradicating pathogens.

Results and discussion

Synthesis and characterization of VPNSs and BPNSs

As illustrated in Fig. 1a and S1,† scanning electron microscopy (SEM) showed that VP has a multilayer structure. Then the VPNSs were obtained by a solvent exfoliation method from bulk VP under mild conditions. An atomic force microscope (AFM) and transmission electron microscope (TEM) showed that VPNSs showed a wide two-dimensional size distribution and their edges were irregular and rough after solution exfoliation (Fig. 1b, S2, and S3†). The structure of the as-obtained VPNSs was also characterized using high-resolution transmission

electron microscopy (HRTEM) and X-ray diffraction (XRD). The HRTEM image showed that the lattice spacing was 0.65 nm and intersected at a 90° angle, corresponding to the (110) crystal planes of VPNSs (Fig. 1c). The selected area electron diffraction (SAED) pattern further revealed the interplanar spacing and angles of VPNSs (Fig. 1c inset). The XRD pattern was coherent with the reported phosphorus crystal structure (Fig. S4†), indicating that VPNSs were successfully synthesized via an exfoliation approach. The dispersivity and turbidity of VPNSs in water were also evaluated as a function of aging time. After standing for 90 min, the dispersed solution was still uniform and only a small part of it had settled, which was conducive to full contact between the bacteria and samples (Fig. S5†).

Next, Raman spectra were used to explore the structural transformation that occurred during exfoliation (Fig. 1d and S6†). The Raman spectra of VPNSs shifted towards higher wavenumbers compared with VP, demonstrating that the thickness decreased after exfoliation.⁵⁰ X-ray photoelectron spectra (XPS) were utilized to examine the degree of VPNS degradation during the exfoliation process. Three peaks located at 129.7, 130.4, and 133.7 eV, respectively, corresponded to 2P_{3/2}, 2P_{1/2}, and PO_x signals (Fig. 1e and S7†). A weak peak at 133.7 eV suggested that VP had no obvious oxidation or chemical degradation during the exfoliation process. Energy dispersive spectroscopy (EDS) and TEM mapping analyses revealed the existence and homogeneous distribution of elemental phosphorus across all samples, further indicating the high purity of the VPNSs (Fig. 1f and S8†). As the newest member in the layered phosphorus allotrope family, the structure of violet phosphorus has been confirmed by single-crystal XRD.^{51,52} The edges of the VPNSs are composed of serious sub-nanoneedles (Fig. 1g), and the sub-nanoneedles were tubular strands composed of $-\text{[P}_2\text{][P}_8\text{][P}_2\text{][P}_9\text{]}-$ (Fig. 1h and i). The sub-nanoneedles were formed at the edges of VPNSs due to bond breakage during solvent exfoliation. The existence of sub-nanoneedles was also simulated for VPNSs (Fig. 1i and S9†). The length of the sub-nanoneedles varies from 2 nm to 8 nm, and each tubular sub-nanoneedle has a diameter of about 0.3–0.4 nm. The distance between each two sub-nanoneedles is about 0.6 nm. A series of sub-nanoneedle bundles help to penetrate the cell membrane. In comparison, each layer of BPNSs was made up of a zigzagging chain of phosphorus atoms, with the linked atoms forming a wrinkled sheet lacking the sub-nanoneedle structures in VPNSs (Fig. S10†). Meanwhile, we report for the first time that these sub-nanoneedle structures cannot be observed in most reported antibacterial two-dimensional materials.^{53–58}

Antibacterial properties of VPNSs and BPNSs

Knowing that the phosphorus allotrope BP and its phosphorene have proven successful at inactivating bacteria by photodynamic therapy (PDT) and photothermal therapy (PTT),^{59–62} we were inspired to examine the possibility of VP and VPNSs serving as antibacterial agents. We first evaluated the antibacterial action of VP against 10⁷ colony-forming units per milliliter (CFU mL⁻¹) of *E. coli* and *S. aureus*, with BP as a comparative



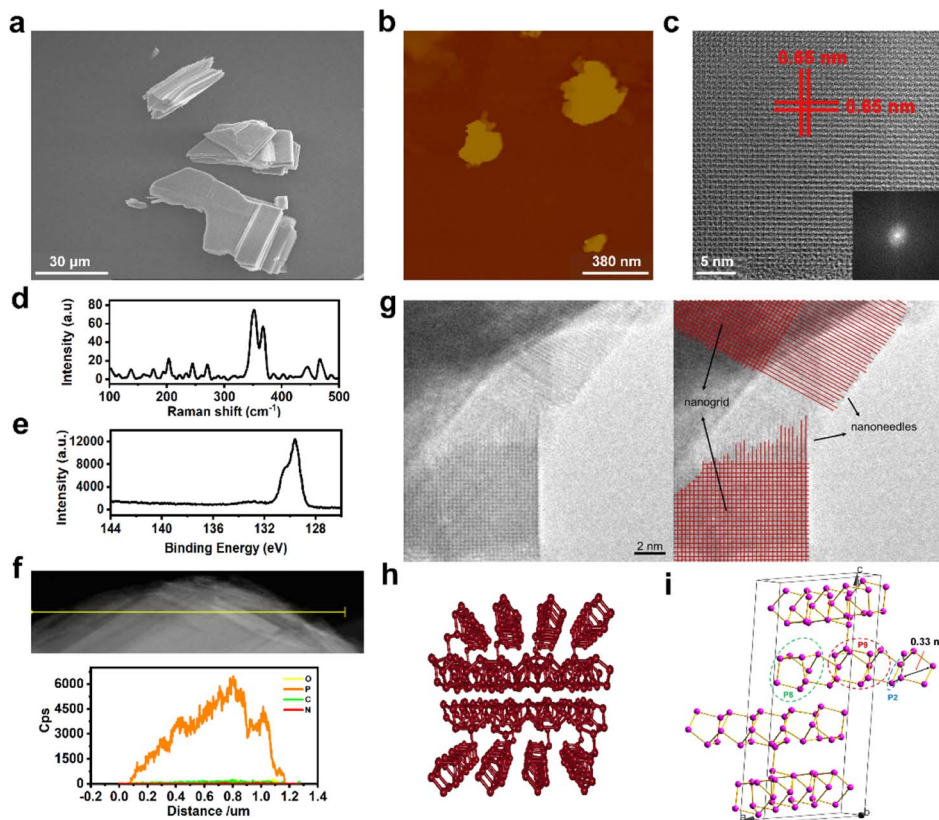


Fig. 1 Characterization of VPNSs. (a) SEM image of bulk VP. (b) AFM image of VPNSs obtained from solvent exfoliation. (c) HRTEM image of VPNSs; (inset) SAED pattern corresponding to the lattice spacing. (d) Raman and (e) XPS spectra of VPNSs. (f) EDS line scanning of VPNSs, including phosphorus, carbon, oxygen, and nitrogen elements. (g) HRTEM image of the VPNS's peripheral sub-nanoneedles. (h) Chemical structure of VPNSs. (i) Layered structure of VPNSs.

using the colony-counting method. As shown in Fig. 2a, after exposure to 1.0 mg mL^{-1} of VP and BP for 3 hours under LED white light irradiation, the survival rate of *E. coli* and *S. aureus* in the presence of BP was significantly higher than in the presence of VP, and the corresponding digital photos further illustrated that VP had excellent antibacterial properties (Fig. S11†). Fig. S12† shows that there was no significant difference in the number of bacteria between the sample exposed to LED light for 180 min and that for 0 min, indicating no effect of long-term light irradiation on bacteria.

We additionally explored the antibacterial properties of VPNSs and BPNSs under the same antibacterial conditions. Unexpectedly, a dramatic difference between the antibacterial effectiveness of VPNSs and BPNSs was observed. The antibacterial percentage of VPNSs reached $>99.9\%$ against *E. coli* and *S. aureus*, compared with 78% for *E. coli* and 85% for *S. aureus* in the presence of BPNSs, and this result illustrated that VPNSs had higher antibacterial activity than BPNSs (Fig. 2b). We also test the minimum inhibitory concentration (MIC) of VPNSs at 0.8 mg mL^{-1} against most of the bacteria and VPNSs can kill all the bacteria in this study efficiently with the MBC at 1.0 mg mL^{-1} (Fig. S13a and b†). As shown in Fig. 2c and d, dynamic testing also revealed that the antibacterial properties of VPNSs against *E. coli* and *S. aureus* were concentration- and time-dependent. Additionally, the

photothermal efficacy of VPNSs was examined as a function of light time. The temperature of VPNSs was $26.2 \text{ }^\circ\text{C}$ even after irradiation for 180 min under LED white light, suggesting that photothermal action could not work on VPNSs (Fig. S14†).

To further assess the antibacterial action of VPNSs, *E. coli* and *S. aureus* in the absence and presence of VPNSs were assayed using a LIVE/DEAD Baclight Kit, and live bacteria were stained green with SYTO 9 and dead bacteria were stained red with PI. In Fig. 2e and S15,† intense green dots corresponded to the control group with live *E. coli* and *S. aureus*. After treatment with VPNS for 3 h under LED white light irradiation, intense red dots were detectable, revealing that *E. coli* and *S. aureus* had been killed. These data further verified VPNSs' high toxicity toward pathogens. We then investigated whether VPNSs worked on antibiotic-resistant bacteria using methicillin-resistant *S. aureus* (MRSA) and *E. coli* pUC19 as two models.⁶³ As shown in Fig. 2f, VPNSs at concentrations of 1.0 and 2.0 mg mL^{-1} exhibited an antibacterial percentage of $>99.9\%$ for both models, indicating their effectiveness against drug-resistant bacteria. Additionally, the physical penetration effect of VPNSs on Gram-negative bacteria and Gram-positive bacteria was compared (Fig. S16†). A slightly lower antibacterial activity was observed for VPNSs against *S. aureus* after 3 h under dark conditions due to its thicker and more rigid cell wall compared to *E. coli*.



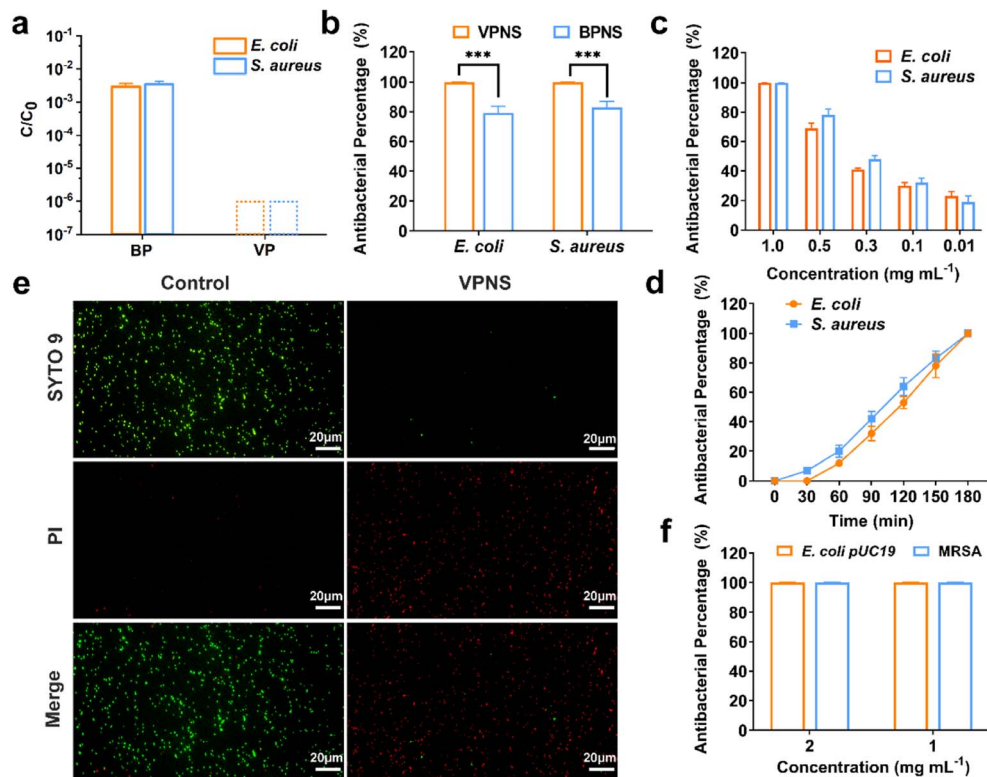


Fig. 2 Antibacterial activity of VP and VPNSs. (a) The survival rate of BP and VP against *E. coli* and *S. aureus* under LED white light irradiation for 3 h. (b) Antibacterial percentage of VPNSs and BPNSs against *E. coli* and *S. aureus* under LED white light irradiation for 3 h. (c) Antibacterial percentage of VPNSs against *E. coli* and *S. aureus* as a function of VPNS concentration (0.01–1.0 mg mL⁻¹) under LED white light irradiation for 3 h. (d) Antibacterial percentage of *E. coli* and *S. aureus* after exposure to 1.0 mg mL⁻¹ of VPNSs for different times under LED white light irradiation. (e) Live/dead staining of *E. coli* bacterial strains treated with VPNSs under LED white light irradiation for 3 h (live bacteria are green and dead ones are red). (f) Antibacterial percentage of VPNSs against *E. coli* pUC19 and MRSA. Data are presented as means \pm SD ($n = 3$). * $p < 0.05$, ** $p < 0.01$, *** $p < 0.001$, **** $p < 0.0001$, and ns, not significant.

Antibacterial mechanism of VPNSs

Given the notable discrepancy between the performance of VPNSs and BPNSs, we sought to explore the VPNS's antibacterial mechanism. First, we examined whether, like BPNSs, VPNSs's performance was affected by light irradiation. We conducted a contrast experiment by testing VPNSs's efficiency against *E. coli* in the dark, under natural light irradiation, and under LED white light irradiation. Fig. 3a showed that VPNS were more toxic under light (especially LED) than in the dark, indicating their light dependency. We therefore considered that VPNS attacked bacteria *via* ROS-dependent oxidative stress induced by PDT, a primary mechanism for BPNSs. Using electron spin resonance (ESR) spectra, we detected whether VPNSs generated ROS in the dark and under light irradiation. As presented in Fig. 3b, VPNSs produced four ROS signals under light irradiation: singlet oxygen (¹O₂), superoxide anion radical ([•]O₂⁻), hydrogen peroxide (H₂O₂), and hydroxyl radical ([•]OH), respectively. On the contrary, no ROS were produced in the dark. Further, the four ROS signals strengthened as a function of light exposure time, suggesting that the generation of ROS depended on light irradiation time. In contrast, BPNSs can only generate ¹O₂, demonstrating that VPNSs produced more ROS species under the same testing conditions.^{64,65} Subsequently, a scavenging

experiment was carried out to discover whether these four ROS species contributed to VPNSs' bactericidal activity under light irradiation.^{66–69} We used four trapping agents: 4-hydroxy-2,2,6,6-tetramethylpiperidinyloxy (TEMPOL) for [•]O₂⁻, isopropyl alcohol (IPA) for [•]OH, ethylenediaminetetraacetic acid ferric sodium salt (Fe(II)) for H₂O₂, and sodium azide (NaN₃) for ¹O₂. As illustrated in Fig. 3c, VPNSs exhibited almost the same antibacterial rates in the presence and absence of TEMPOL, IPA, and Fe(II), demonstrating that neither [•]O₂⁻, [•]OH, nor H₂O₂ accounted for VPNSs' superior antibacterial performance. However, when NaN₃ was used to scavenge ¹O₂, the antibacterial rate decreased to 21%, indicating that ¹O₂ played a key role in eliminating bacteria.

In addition to light-dependent oxidative stress against bacteria, we also found that VPNSs also had a certain antibacterial ability (43%) in the dark and the activity of VPNSs was higher than that of BPNSs (7%) (Fig. 3a). Several other typical 2D nanomaterials can inflict physical damage on the cell membrane, including graphene oxide and graphdiyne.^{70–75} The interaction between VPNSs and bacteria is randomly orientated in solution. The VPNSs contacted with bacteria at all different orientations. The VPNSs with certain angles were able to penetrate the cell membrane of bacteria. This is an important reason to explain why the antimicrobial rate of VPNSs under



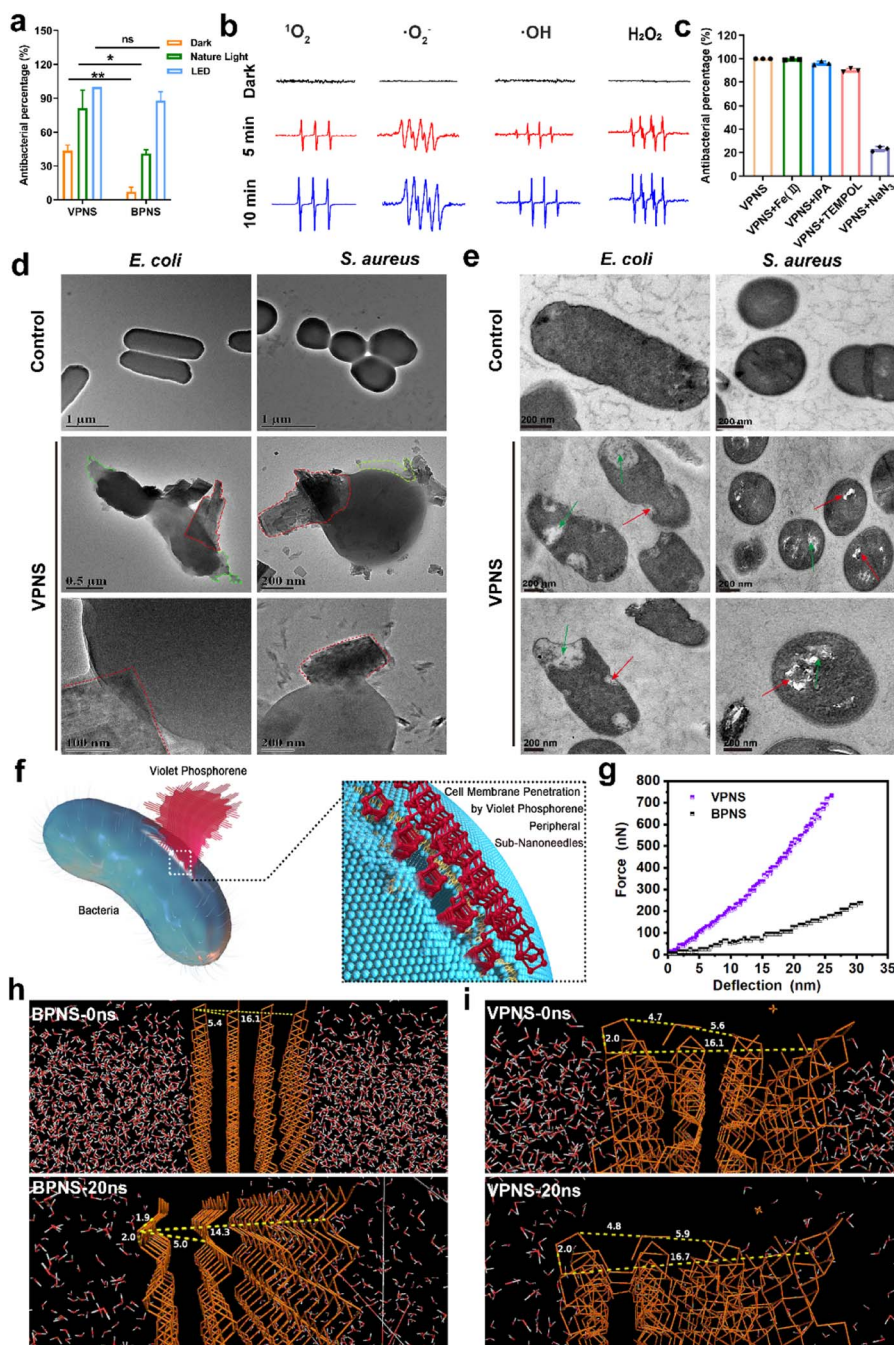


Fig. 3 (a) Antibacterial percentage of VPNSs in the dark, under natural light, and under LED white light against *E. coli*. (b) ESR spectroscopy of $^1\text{O}_2$, O_2^- , $\cdot\text{OH}$, and H_2O_2 in the presence of VPNSs in the dark and under LED white light irradiation. (c) Antibacterial percentage of VPNSs against *E. coli* under LED white light irradiation in the absence and presence of different scavengers. (d) TEM images showing morphological changes in *E. coli* and *S. aureus* before (controls) and after treatment with VPNS samples under LED white light for 3 h (the red and green dotted boxes represent VPNSs that puncture bacteria and bacterial leakage contents, respectively). (e) TEM image of the bacterial section showing morphological changes in *E. coli* and *S. aureus* before (controls) and after treatment with VPNS samples under LED white light for 3 h (the red arrow represents damage to the bacterial cell wall and membrane by VPNSs and the green arrow represents bacterial rupture and disintegration). (f) Schematic illustration of physical penetration induced by VPNS peripheral sub-nanoneedles to kill bacteria. (g) Typical force versus deflection curves of VPNSs and BPNSs. (h) BPNSs and (i) VPNSs in the NPT molecular dynamics simulation (0–20 ns). Data are presented as means \pm SD ($n = 3$). * $p < 0.05$, ** $p < 0.01$, *** $p < 0.001$, **** $p < 0.0001$, and ns, not significant.

dark conditions is only about 40%. The SEM and TEM images were taken to examine the morphology and membrane integrity of bacteria in the presence of VPNSs under LED irradiation conditions (Fig. 3d). The bacterial cells in control groups were

observed to have smooth and intact cell membranes, without cytomembrane destruction or cytoplasmic leakage. However, significant wrinkles and depressions were observed to appear on the cytomembranes in the presence of VPNSs. Some VPNSs



were also found to penetrate the cells (red dotted box in Fig. 3d), causing cytoplasm (green dotted box in Fig. 3d) and DNA (Fig. S17†) leakage and killing the bacteria. The damage of *E. coli* (Video 1†) and *S. aureus* (Video 2†) was also observed after VPNS treatment due to VPNS puncture combined with oxidative stress from TEM. The untreated bacteria were observed to have normal morphology and a dense intracellular matrix (Fig. 3e), while the VPNS-treated bacterial sections were observed to have bacterial rupture and disintegration (green arrow Fig. 3e) as well as cell wall and membrane damage caused by VPNS puncture (red arrow Fig. 3e). The morphology of bacteria treated with VPNSs has been demonstrated to show depressions, folds, and damage compared to the smooth and flat bacterial surface in the control group, indicating the death of bacteria of treated ones (SEM, Fig. S18†). Additionally, the morphology of bacteria treated with VPNSs under dark conditions was also determined to evaluate the physical destruction effect of VPNSs on bacteria. The VPNSs were observed to penetrate bacteria under the induction of sub-nanoneedles (Fig. S19†), resulting in bacterial death. The bacteria were observed to have many holes and damage on the cell wall and membrane after treatment of VPNSs (Fig. S20†). The VPNSs have been demonstrated to puncture bacteria and cause bacterial death under the induction of sub-nanoneedles. The length of sub-nanoneedles is usually shorter than the thickness of the phospholipid bilayer. The cell wall or membrane could not be pieced by the sub-nanoneedles from the edge of VPNSs alone. However, the sub-nanoneedles with sharp tips are favored to penetrate the bacteria like 'gears', driving entire VPNSs into the bacteria and eventually killing the bacteria (Fig. 3f). In addition, the dynamic light scattering (DLS) results demonstrated that the size of VPNSs was close to that of bacteria, which was conducive to sufficient contact between them for cell membrane penetration induced by the VPNS's peripheral sub-nanoneedles (Fig. S21†). The interaction between VPNSs and bacteria was further explored to understand the penetration of VPNSs to bacteria. A strong peak at 1032 cm^{-1} corresponding to the stretching vibration of P–OC and peaks at 2925 and 2857 cm^{-1} corresponding to the stretching vibrations of the CH_2 and CH_3 groups were detected from the Fourier transform infrared spectroscopy (FTIR) spectrum of VPNSs (Fig. S22†). The dangling phosphorus bonds of VPNSs have been demonstrated to be functionalized by the exfoliation solvent (anhydrous ethanol) to form stable $-\text{P}-\text{OCH}_2\text{CH}_3$ groups. The contact angle of VPNSs with water was also measured to be 92.8° , suggesting the hydrophobic feature of functionalized alkyl chains to VPNSs (Fig. S23†). Therefore, the hydrophobic chain of VPNSs has been demonstrated to further promote its insertion into bacteria through hydrophobic interaction with hydrophobic bacteria due to the presence of polysaccharides in the cell wall and phospholipids in the membrane.

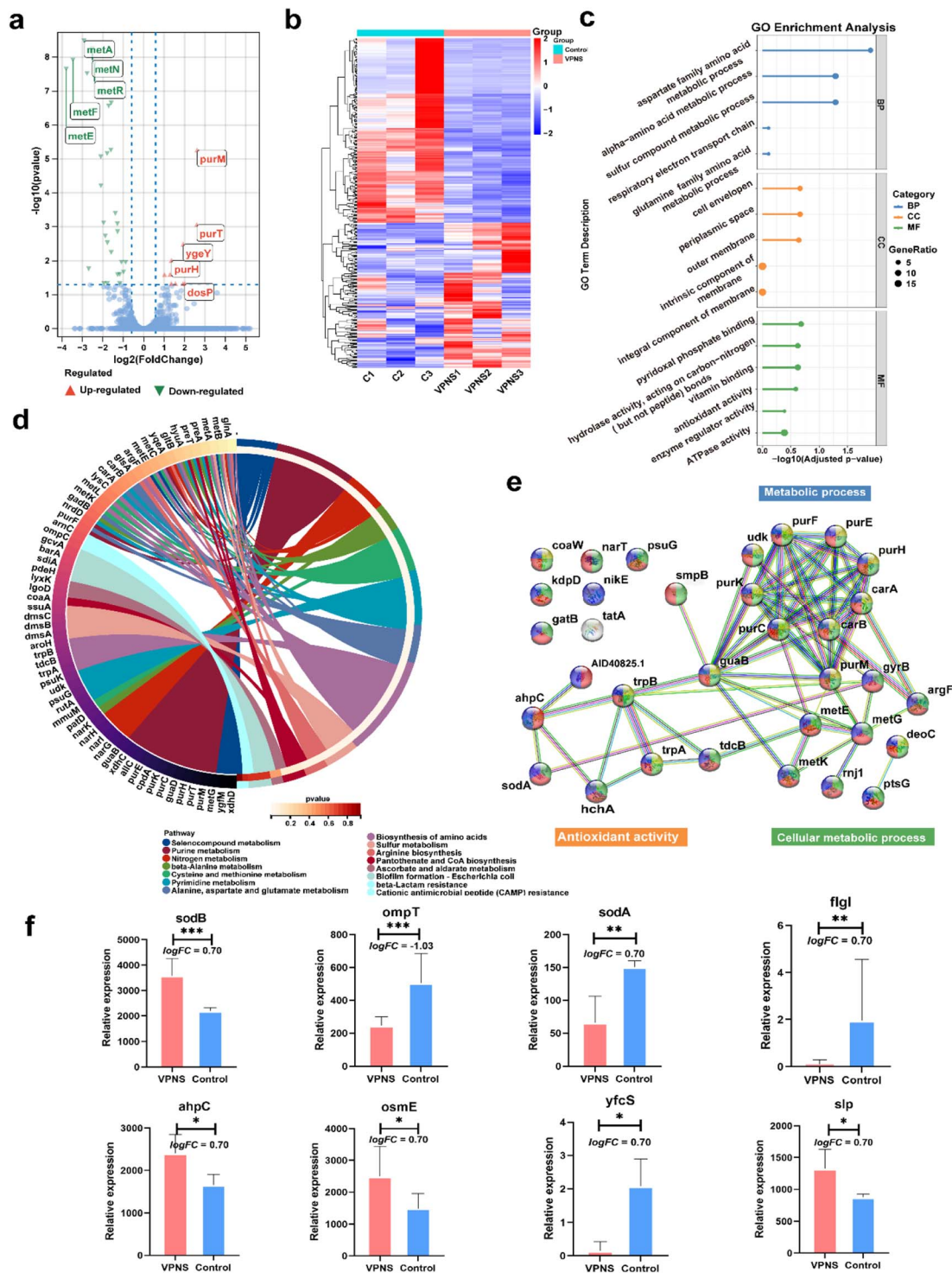
The cell membrane was easily penetrated induced by the peripheral sub-nanoneedles due to the extremely high 2D Young's modulus of VPNSs (Fig. 3g). The 2D Young's modulus of monolayer violet phosphorene ($1512 \pm 76\text{ N m}^{-1}$) has been deduced to be 4.4 times as high as that of graphene (340 N m^{-1}) and much higher than that of BPNSs (214 N m^{-1}).⁷⁶ The

mechanical properties were further confirmed using theoretical calculations, as shown in Fig. 3h, i, and S24.† Molecular dynamics (MD) simulation of the *NPT* (normal pressure and temperature) ensemble was employed to investigate the system changes under a pressure of 1.0 atm within 20 ns of simulation. The P–P bond lengths and layer distances in BPNSs and VPNSs were monitored during MD processing. At the starting point (0 ns), the distances between two layers and four layers of BPNSs were 5.4 angstroms and 16.1 angstroms, respectively, decreasing to 5.0 angstroms and 14.3 angstroms after 20 ns in the MD system. The conditions were different in the VPNS system. The distance from the top side to the bottom side and the distance between two layers changed slightly during 20 ns of MD processing, demonstrating that due to their 2D crisscross structure, VPNSs had a higher deformation resistance than BPNSs, making them more physically destructive toward bacteria. This effect of VPNSs on *E. coli* based on contact-triggered action was further confirmed by inhibition zone testing in the dark. As shown in Fig. S25,† unlike AgNO_3 , which exhibited an obvious inhibition ring due to the release of Ag^+ ions, neither VPNSs nor BPNSs showed an aseptic area, confirming their antibacterial mechanism including physical penetration of the bacteria.

The above experiments demonstrated that VPNSs showed a significant inhibitory effect on bacterial growth. To further explore the molecular mechanism by which VPNSs inhibit bacterial growth, we attempted to assess the specific response at the mRNA level using RNA sequencing (RNA-Seq) (Fig. 4). The correlation of gene expression levels between samples, an important index to test the reliability of the experiment and the reasonableness of sample selection, was also conducted. The R^2 values of both inter-group and intra-group samples were found to be greater than 0.8 (Fig. S26†), indicating a good biological repeatability. 4901 genes were identified, of which 374 were differentially expressed ($|\log_2(\text{fold change})| > 1$ and P value < 0.05), including 210 upregulated genes and 164 downregulated genes. The top 5 most differentially upregulated and downregulated genes are displayed in the volcano plot (Fig. 4a and b). To further investigate the molecular mechanisms of differentially expressed genes, gene ontology (GO) enrichment analysis was performed. As shown in Fig. 4c, a total of 330 GO terms were enriched, including 183 biological process (BP), 21 cellular component (CC), and 126 molecular function (MF) terms. The following were noteworthy BP terms: aspartate family amino acid metabolic process (GO:0009066) and sulfur compound metabolic process (GO:000679). The periplasmic space (GO:0042597), cell envelope (GO:0030313), and outer membrane (GO:0019867) were the main distributed terms in CC ontology. With regard to the ontology of MF, the important categories were pyridoxal phosphate binding (GO:0030170), vitamin binding (GO:0019842), and hydrolase activity, acting on carbon–nitrogen (but not peptide) bonds (GO:0016810).

Subsequently, the Kyoto Encyclopedia of Genes and Genome (KEGG) enrichment analysis was employed to explore the possible molecular regulation pathways (Fig. 4d). In the ontology of KEGG, the main categories were gathered at terms: seleno-compound metabolism, purine metabolism, nitrogen





interaction (PPI) network was constructed (Fig. 4e). The majority of the identified DEGs were enriched by KEGG. The most interacted proteins were mainly concentrated in the following pathways: purine metabolism, biosynthesis of amino acids, and cellular anatomical entity. Based on the above result, the regulated genes associated with antimicrobial mechanisms are shown in Fig. 4f as bar graphs individually. All *sodB*, *sodA*, and *ahpC* were associated with oxidative stress and *ompT*, *flgI*, *osmE*, *yfcS*, and *slp* associated with membrane destruction were up-regulated or down-regulated compared with the control group.

In addition to antibacterial activity, it is essential to evaluate the biocompatibility of VPNSs before the material can be applied *in vivo*. First, the cell viability and cytotoxicity of VPNSs were assessed using CCK-8 and MTT assays (Fig. S27 and S28†). The VPNSs showed no toxicity toward NIH 3T3 cells, Raw 264.7 cells, or L02 cells within a concentration range of 0.125–2.0 mg mL⁻¹, suggesting that VPNSs have good biocompatibility. Hence, it was potential for use in clinical applications. In addition, Fig. S29 and S30† show that compared with PEI25K, L02 cells treated with different concentrations of VPNSs emitted strong green fluorescence and blue fluorescence, respectively, in live/dead cell staining and TUNEL cell staining assays, indicating that the majority of the cells remained viable. The results showed that no cytotoxicity or apoptosis was induced in the concentration range of 0.125–2.0 mg mL⁻¹. The toxicity of VPNSs to human corneal epithelial cells (HCECs) associated with the eyeball has also been measured (Fig. S31†). Strong green fluorescence was detected in both live and dead HCECs after treating with VPNSs with different concentrations, indicating no toxicity of VPNSs in the concentration range of 0.125–2.0 mg mL⁻¹ to HCECs.

In addition, we also performed hemolysis testing to further evaluate the erythrocyte compatibility of VPNSs, using Triton X-100 as the positive control. As shown in Fig. S32,† after incubation with the VPNSs, followed by centrifugation, the supernatants were transparent, indicating that no disruption of the erythrocytes had occurred and no hemoglobin was released. The hemolysis rate of the VPNSs was only 1.7% at 2.0 mg mL⁻¹, much lower than the ASTM standard (ASTM F756-2008) for the hemolysis ratio of biomaterials (<5%). VPNSs showed high antibacterial activity and low cytotoxicity to normal cells may be due to the rigidity difference between bacterial and eukaryotic cell membranes. It was reported that Young's modulus of human mesenchymal stem cells was in the region of 0.09–49 kPa compared to 50–200 kPa for certain bacterial cell envelopes.^{77–79} Eukaryotic cells are able to avoid membrane damage and cell death by stretching and twisting to fit the subnanoneedle shape of VPNSs.⁸⁰

In vivo wound infection treatment

Encouraged by the excellent *in vitro* antibacterial properties of VPNSs, coupled with their biosafety, we then investigated *in vivo* antibacterial effectiveness of VPNSs in skin or soft tissue-related infections that induced severe inflammation. A wound-infection model in mice was established using *S. aureus*, and the efficiency of wound healing was observed before and after

treatment with VPNSs and BPNSs (Fig. 5a). The infected mice were randomly divided into five groups and then treated with PBS (control), BPNSs, VPNSs, BPNSs with LED irradiation (BPNS + L), and VPNSs with LED irradiation (VPNS + L) within 7 days. As shown in Fig. 5b and c, the wounds treated with VPNSs and BPNSs exhibited significantly faster healing than those in the control group. Especially, those treated with VPNS + L healed the fastest and were almost completely gone within 7 days, whereas the wound area in the control group was still about 55% ± 7.3% of the original size. We also used the colony-counting method to evaluate bacterial survival at the infection site on day 7. Fig. 5d and e show that the bacterial survival numbers in wounds treated with VPNS + L and BPNS + L groups were obviously lower than for the other groups, with the VPNS + L group showing the lowest survival and thereby demonstrating that the material was active *in vivo*.

Routine blood analysis was conducted on the treated mice, as shown in Fig. 5f. Compared with the control group, the experimental groups showed fewer white blood cells (WBCs) and lymphocytes (Lymph), demonstrating that VPNSs and BPNSs had anti-infection activity *in vivo*. Notably, the blood values of the VPNS + L-treated mice had almost returned to normal levels, showing that VPNSs were the most effective material. Finally, hematoxylin–eosin (H&E) staining of wound tissues revealed the wound-healing process in different treatment groups at the histological level. As shown in Fig. 5g, the control group presented obvious inflammatory cells, whereas none were found after treatment with BPNS, VPNS, VPNS + L, and BPNS + L groups and the wounds were filled with granulation tissue. Among the four sample types, the granulation tissue treated with VPNS + L was the most mature, indicating that VPNSs had the most positive impact on wound healing. Upon comparison, the VPNS + L group demonstrated greater healing efficiency than the other groups.

In vivo bacterial keratitis treatment

Based on the good therapeutic effect of VPNSs on skin wounds and their excellent antibacterial properties, a keratitis model of MRSA-infected SD rats was also established in this study to evaluate the therapeutic effect of VPNSs *in vivo* (Fig. 6a). The rats were randomly divided into five groups: (1) control (PBS), (2) VPNS, (3) BPNS with LED irradiation (BPNS + L), (4) VPNS with LED irradiation (VPNS + L), and (5) levofloxacin (LVFX), respectively. Then slit-lamp images were captured on the following 9 days to monitor the apparent morphology and inflammatory response characteristics of corneas (Fig. 6b and c). On day 0, similar corneal infiltrates and abscesses were observed in all groups, indicating the same infection level at the beginning of treatment. In the PBS-treated group, the eyes presented obvious corneal edema, inflammatory infiltration in the anterior chamber, and persistent infection. As a control, the development of corneal infections in VPNS and BPNS + L was well controlled, but the symptoms were not eliminated until day 9, leading to a longer recovery time. Surprisingly, the inflammation and infection were significantly reduced in the VPNS + L group on day 3, and the treatment efficiency of the VPNS + L



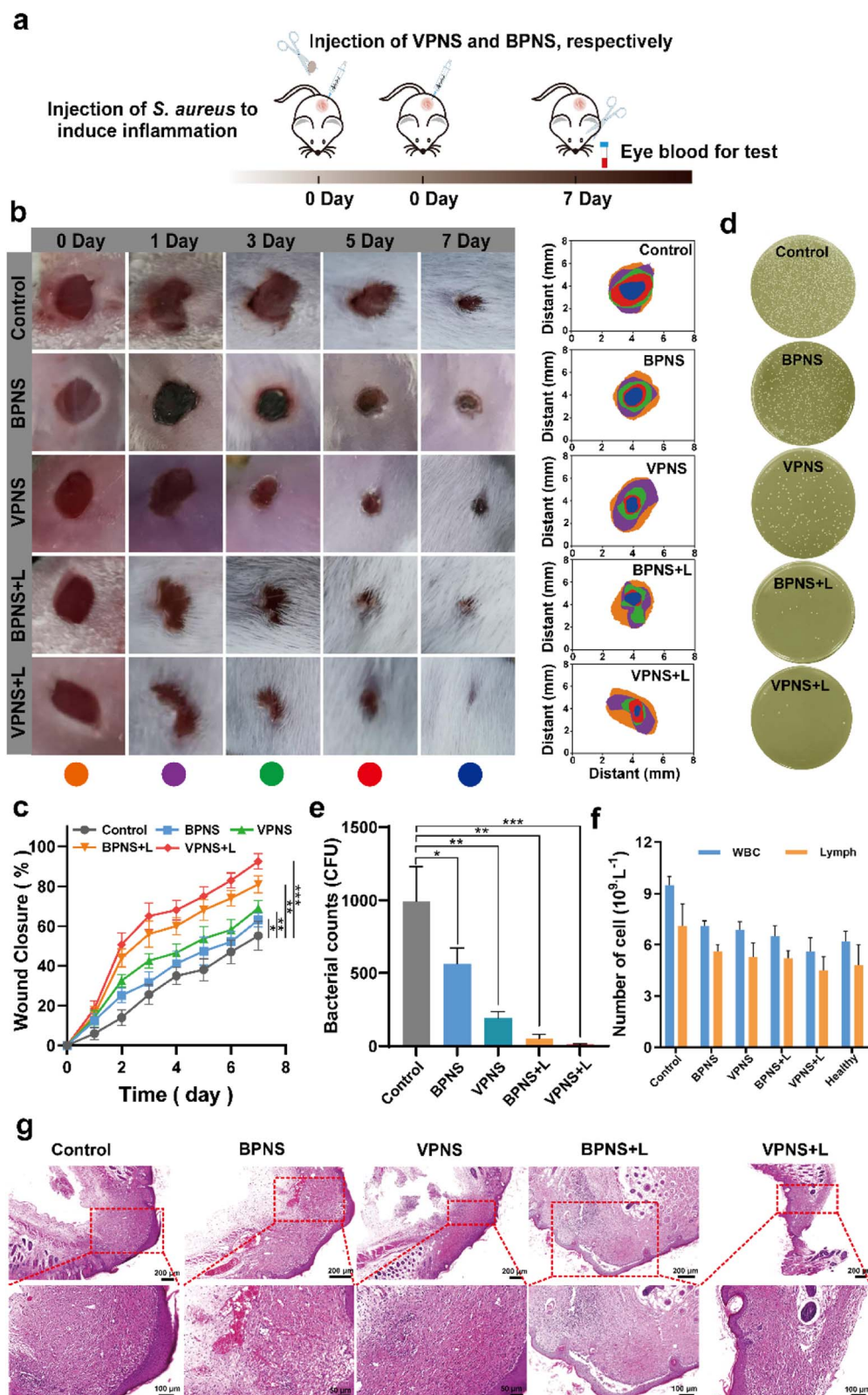


Fig. 5 Validation of the antibacterial effect and potentially accelerated wound healing of VPNSs and BPNSs. (a) Schematic illustration of the *in vivo* infectious animal model using *S. aureus*. (b) Visual observation of mice wounds and (c) wound closure rates in the presence of VPNSs and BPNSs as a function of aging time. (d) Bacterial survival culture plates and (e) corresponding bacterial counts at wound sites treated with VPNSs and BPNSs, on day 7. (f) WBC and lymph levels for treated mice and healthy mice on day 7. (g) Histological microscopy images of wound tissue samples on day 7. Data are presented as means \pm SD ($n = 6$). * $p < 0.05$, ** $p < 0.01$, and *** $p < 0.001$.



group was even better than that of the levofloxacin group, which could be attributed to the rapid sterilization of VPNS-producing more ROS under LED irradiation. Correspondingly, the clinical scores of the eyes in PBS, VPNS, and BPNS + L groups showed no significant decrease over time. As a comparison, the eyes in the

VPNS + L group showed the lowest clinical score on day 9 and the total clinical score was no higher than 1 (Fig. 6d). Furthermore, the increased corneal thickness revealed the lack of therapeutic effects of the VPNS group and BPNS + L group in treating refractory keratitis. It was also worth noting that the corneal thickness remained unchanged in the VPNS + L group compared with the healthy rats on day 9 (Fig. 6e).

Furthermore, H&E staining and histological analysis were performed on the corneal tissues after 9 days of treatment. As shown in Fig. 6f, H&E staining images showed that the corneal structures of rats treated in PBS groups were destroyed with significant inflammatory cell infiltration and corneal edema. Compared with the PBS group, a decrease in corneal edema and infiltration of inflammatory cells was observed in the VPNS and BPNS + L groups. Only in VPNS + L and levofloxacin groups that showed uniform corneal layers without obvious inflammatory cell infiltration and corneal edema, the corneal epithelial cells regenerated well and were closely arranged. Next, immunofluorescence staining was also conducted to investigate the expression of proinflammatory factors IL-1 β , IL-6, and TNF- α associated with keratitis treatment. As seen in Fig. 6g, the lowest red fluorescence signal levels were observed in rats treated with the VPNS + L group, indicating much fewer inflammatory mediators expressed in this group. The above results fully demonstrated that VPNSs under LED irradiation had excellent antibacterial ability and good inflammatory mitigation ability, which provided new insight into healing refractory keratitis.

Conclusions

In summary, we reported the antibacterial activities of VP and VPNSs, which are able to inactivate more than 99.9% of common pathogens (*E. coli* and *S. aureus*) and antibiotic-resistant bacteria (*E. coli* pUC19 and MRSA). VPNSs were demonstrated to have higher antibacterial activity than BPNSs owing to the unique two-layer structure of crisscrossed rods that form a nanogrid with numerous sub-nanoneedles along the edge, which led to the extremely high deformation resistance of VPNSs and made the cell membrane easily penetrated. Given their excellent ability to inactivate bacteria *via* physical penetration of the cell membrane, combined with oxidative stress, VPNSs have also shown the potential to accelerate wound healing in mice and bacterial keratitis in rats. This study not only presents an emerging 2D antibacterial agent but also offers encouragement for future studies on different biomedical applications of VPNSs.

Data availability

All the data supporting this article have been included in the main text and the ESI.†

Author contributions

Q. S., J. K., and A. D. designed the research plan. Q. S., X. Z., W. L. and B. Z. performed all of the experiments and analyzed the data. Q. S., J. K., Z. L., and A. D. worked on the figures. Q. S. contributed to the writing of the manuscript. J. K., B. W., and A. D.

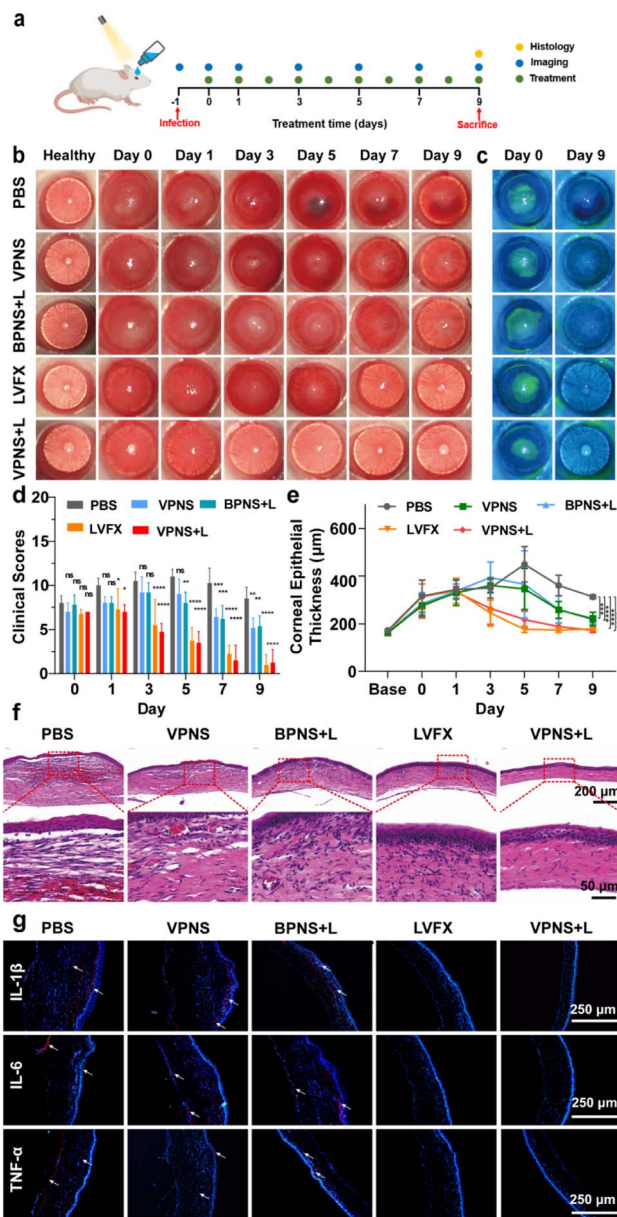


Fig. 6 (a) Schematic illustration of the *in vivo* bacterial keratitis rat mode using MRSA. (b) Representative slit-lamp images of bacteria-infected rats after different treatments on days 0, 1, 3, 5, 7, and 9. (c) Representative images of corneal fluorescein staining on 0 and 9 days after different treatments. (d) Corneal clinical score of bacteria-infected rats after different treatments on days 0, 1, 3, 5, 7, and 9. (e) Corneal thickness values of bacteria-infected rat eyes after different treatments. (f) H&E staining of infected corneas after diverse treatments on day 9. (g) Immunofluorescence images of cytokines (IL-1 β , IL-6, and TNF- α) after different treatments, and the cell nucleus and cytokines exhibited blue and red fluorescence colors. Data are presented as means \pm SD ($n = 3$). * $p < 0.05$, ** $p < 0.01$, *** $p < 0.001$, **** $p < 0.0001$, and ns, not significant.



refined the draft. J. Z. and L. Z. provided technical support and conceptual advice. All authors discussed the results and implications and edited the manuscript at all stages.

Conflicts of interest

There are no conflicts to declare.

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