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Preparation of nickel foam modified by multiwalled hollow spheres of NiCo_2O_4 as a promising non-enzymatic glucose sensor†

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Nickel foam modified by hollow sphere NiCo_2O_4 particles was successfully prepared via a hydrothermal method using nanosphere SiO_2 particles as the hard template for the hollow structure. Characterisation using SEM-EDX and TEM confirmed the structure as multiwalled hollow spheres with an average size of 270 nm, while characterisation using SEM, XRD, and XPS confirmed that the NiCo_2O_4 particles were attached on the surface of the nickel foam. BET analysis showed that the surface area of the synthesized $\text{NiCo}_2\text{O}_4/\text{Ni}$ foam was nearly three times higher compared to that of the unmodified Ni foam. Investigation of the NiCo_2O_4 -modified nickel foam as an electrode for the detection of glucose in sodium hydroxide solution showed high linearity of the anodic currents ($R^2 = 0.99$) in the concentration range of 0–2.5 μM with sensitivity of 0.060 $\text{mA } \mu\text{M}^{-1}$ and an estimated limit of detection of 0.060 μM . Excellent stability of the current response was also obtained with a relative standard deviation of 1.51% ($n = 10$). Furthermore, the developed sensor demonstrates strong applicability for glucose detection in real samples of human blood plasma, making it highly suitable for practical use. The results indicate that the material is promising for the further development of nickel-based sensors.

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Introduction

Nickel is widely used in catalysts due to its excellent performance as an electrocatalyst.^{1–6} However, nickel has disadvantages due to its high over potential and poor stability.⁷ Combining nickel with cobalt to form spinel NiCo_2O_4 for use as an electrocatalyst has received major attention in many electrochemical applications, such as water splitting, supercapacitor, and chemical sensing.^{8–14} In addition, one of the key factors to obtain a favourable electrocatalyst for use as a working electrode is by modifying its structure and morphology, which could further affect its sensing performance due to the increase of the electrode's surface area.

Meanwhile, glucose is a crucial part in human physiological fluids, playing an important role in human metabolism and being the only main fuel for the brain, except in a state of

prolonged hunger.¹⁵ Strict regulation of glucose metabolism is needed because insufficient glucose intake can disrupt the brain physiology,¹⁶ while high glucose concentrations in human blood can trigger diabetes, a disease which can be caused by genetic factors, insensitivity to insulin, and failed insulin secretion.¹⁷ To manage blood sugar levels in the body, a healthy lifestyle and regular exercise are necessary. In addition, glucose levels in the body should be monitored periodically. Conventional glucose sensors commonly use an enzymatic reaction to promote glucose oxidation.¹⁸ However, loss of biological activity is also often reported due to a change of pH or temperature.^{19,20} Accordingly, the development of the non-enzymatic glucose sensors attracts considerable attention.^{21–23} Such sensors commonly use transition metals, in the forms of metal oxides, bimetal, or layered triple hydroxides,^{24,25} while nickel is the most favourable metal due to its low cost and good reactivity.^{26,27}

Electrochemical detection of glucose based on nickel electrodes has been widely explored. Many types of nickel-based materials have been proposed to be employed as working electrodes for sensors, such as pure nickel metal, oxides, sulfides, and organic frameworks.^{28–30} In addition, the use of alloys or composites is often found to increase the catalytic activity, while minimizing its high overpotential and instability problems.^{31,32} On the other hand, the use of porous materials for sensor applications can provide a high surface area, and accordingly

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accelerate the ion transfer on the electrode's surface, resulting in sensors with high sensitivity.³³

In this work, nickel foam was used as the support for the working electrode due to its porous structure, which provides a high surface area to facilitate good electron and electrolyte transfer during the redox process.³⁴ To solve the high over potential problem, the nickel foam was modified with cobalt. Hollow sphere-structured NiCo_2O_4 was selected for the cobalt source since the multiwalled hollow sphere structure of NiCo_2O_4 can enhance the sensor's surface area and the sensitivity of glucose oxidation. The NiCo_2O_4 was synthesized on the surface of the nickel foam using a hydrothermal method with SiO_2 nanospheres as the hard template. The holes in the NiCo_2O_4 structure were produced by etching the template in an alkaline atmosphere. Confirmation of the hollow nanostructure was obtained by using SEM and TEM characterisation, while the advantage of the hollow structure was employed for the detection of glucose.

The prepared NiCo_2O_4 hollow spheres-modified nickel foam ($\text{NiCo}_2\text{O}_4@\text{Ni}$ foam) was found to have a high surface area. Furthermore, the modified nickel foam showed good linearity for the anodic current with a low limit of detection and high stability of the current response for glucose detection, indicating that the material is suitable for sensor applications.

Materials and methods

Materials

All reagents, including nickel nitrate hexahydrate ($\text{Ni}(\text{NO}_3)_2 \cdot 6\text{H}_2\text{O}$), cobalt nitrate hexahydrate ($\text{Co}(\text{NO}_3)_2 \cdot 6\text{H}_2\text{O}$), sodium hydroxide (NaOH , >98%), urea ($\text{CO}(\text{NH}_2)_2$, 99–100.5%), D-(+) glucose (99.99%), tetraethyl orthosilicate (TEOS, 99.99%), ethanol (99%), and ammonium hydroxide (NH_4OH , 28–32%), were purchased from Sigma-Aldrich, while double distilled water with a maximum conductivity of $0.056 \mu\text{S cm}^{-1}$ was obtained from a Direct-Q® 3 UV Remote Water Purification System (Direct-Q3 UV, Millipore). All chemical reagents used in this experiment were of analytical grade and were used without further purification.

Synthesis of SiO_2 nanospheres

SiO_2 nanospheres were synthesized by slowly dripping 2 mL of TEOS into a mixture of ethanol (50 mL), ammonia (1.5 mL), and water (5 mL). The mixture was then stirred at 60 °C for 24 h. The SiO_2 nanospheres were then obtained by centrifugation and washed with water and ethanol several times, followed by drying under vacuum at 60 °C for 24 h.

Synthesis of NiCo_2O_4 on nickel foam

Prior to use, a piece of nickel foam (dimensions: 10 mm × 10 mm × 1.6 mm) was cleaned with sonication in 3.0 M HCl for 20 min, followed by ethanol and water for 15 min each, then dried at 60 °C for 3 h. Meanwhile, the as-synthesized SiO_2 nanospheres (0.1 g) were placed into 50 mL of water and sonicated for 20 min. $\text{Ni}(\text{NO}_3)_2 \cdot 6\text{H}_2\text{O}$ (0.278 g), $\text{Co}(\text{NO}_3)_2 \cdot 6\text{H}_2\text{O}$ (0.476 g), and urea (1.2 g) were added to the mixture, which was

then stirred to form a homogenous solution before transferring into a 100 mL Teflon-lined stainless-steel autoclave together with the cleaned nickel foam. The autoclave was then heated in an oven at 100 °C for 48 h. After cooling to room temperature, the treated nickel foam was washed with hot NaOH solution in an ethanol–water solvent (1 : 1) to remove the SiO_2 nanosphere template. The characterisation of the treated nickel foam was performed using Fourier-transform infrared spectrometry (FTIR Bruker, LUMOS), X-ray diffraction analysis (XRD Rigaku, Cu-K α radiation), scanning electron microscopy with energy dispersive X-ray analysis (SEM-EDX Hitachi S-4800), and X-ray photoelectron spectroscopy (XPS PHI5000 Versa Probe), while transmission electron microscopy (TEM, JEM-2100F) characterisation was performed for the NiCo_2O_4 particles filtered from the remaining solution in the autoclave.

Electrochemical measurements

The electrochemical measurements were carried out using an eDAQ electrochemical workstation (E-corder 410) with a three-electrode system. The synthesized $\text{NiCo}_2\text{O}_4@\text{Ni}$ was used as the working electrode, with platinum wire as the counter electrode and an Ag/AgCl (saturated KCl) system as the reference electrode. The electrochemical measurements were conducted in 1.0 M NaOH as the electrolyte. Cyclic voltammetry in the potential range of -0.1 – 0.6 V with a scan rate of 25 mV s^{-1} and chronoamperometry at -0.17 V (vs. Ag/AgCl) for 120 s were applied to examine the sensor performance.

The sample measurements were carried out using human blood plasma, obtained from the Faculty of Medicine, University of Indonesia, Jakarta, Indonesia. No preparation or purification were required for the samples prior to the measurements. A total volume of 40 μL of sample was diluted in a 100 mL volumetric flask, then 12.5 mL of it was further diluted in another 100 mL volumetric flask with 1.0 M NaOH. The glucose level in the sample was then measured using the nickel foam electrode modified with NiCo_2O_4 hollow spheres using the CV technique and the results were subsequently validated using a glucose detector (EasyTouch GCU).

Result and discussion

Characterisation of the prepared materials

SiO_2 nanospheres were synthesized from TEOS as a template to form the hollow sphere structure of NiCo_2O_4 . Fig. 1 shows the FTIR and XRD spectra of the synthesized SiO_2 nanospheres. The FTIR spectrum (Fig. 1a) revealed a band at 797 cm^{-1} , attributed to the Si–O bending vibration, while the peak at 961 cm^{-1} is due to the Si–O–(H \cdots H $_2\text{O}$) bending vibration.^{35,36} The absorption band at 1091 cm^{-1} is assigned to the asymmetric vibration of Si–OH. The bands at 1624 cm^{-1} and 3303 cm^{-1} are attributed to the O–H bending vibration and the O–H stretching vibration of adsorbed molecular water, respectively.³⁵ The results indicated that the SiO_2 had been successfully formed.

Further characterisation with XRD (Fig. 1b) showed a peak at 2θ of 22.75° , which is characteristic of the amorphous SiO_2 . Meanwhile, the SEM image of the synthesized SiO_2



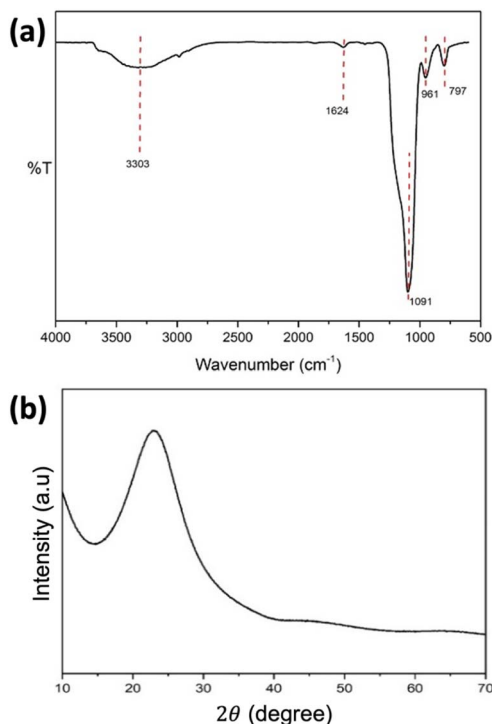


Fig. 1 (a) FTIR and (b) XRD spectra of the synthesized SiO_2 nanospheres.

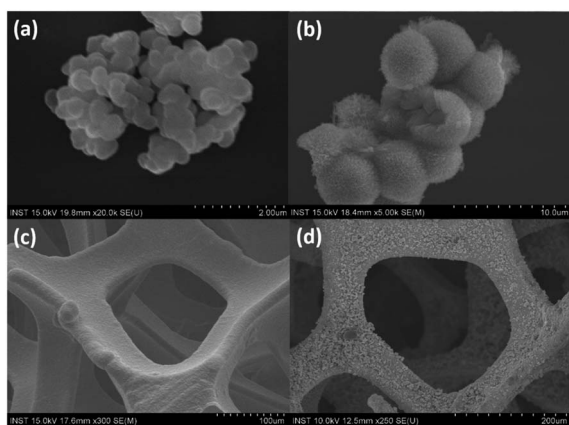
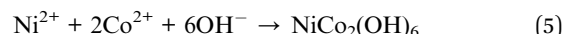
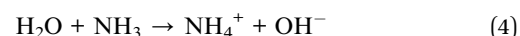
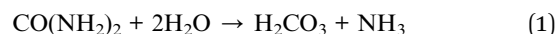


Fig. 2 Typical SEM images of (a) the SiO_2 nanospheres, (b) the NiCo_2O_4 hollow spheres, (c) the unmodified nickel foam, and (d) the NiCo_2O_4 hollow spheres deposited on the nickel foam.

nanospheres (Fig. 2a) shows a spherical shape with the size range from 200 to 300 nm. The EDX characterisation shows ratios of 37.08% and 62.92% for Si and O, respectively, confirming the formation of SiO_2 .

Synthesis of the NiCo_2O_4 hollow spheres was performed using a hydrothermal method in the presence of SiO_2 nanospheres as the hard template. Basically, hydrolysis of urea occurs at a temperature of around 90 °C to form ammonia, providing an alkaline solution to further promote the nucleation process of nickel and cobalt ions to form $[\text{Ni}(\text{NH}_3)_6]^{2+}$ and $[\text{Co}(\text{NH}_3)_6]^{2+}$. This nucleation process takes place on the surface

of the SiO_2 nanospheres. During the heating process, reaction between the excess of ammonia molecules with water molecules generates OH^- to react with nickel and cobalt to form $\text{Ni}(\text{OH})_2$ and $\text{Co}(\text{OH})_2$, which then form NiCo_2O_4 after oxidation, as shown by the following reactions:³⁷



The hollow sphere structure can be seen in the SEM images of the synthesized NiCo_2O_4 hollow spheres (Fig. 2b), which confirmed the morphology of the synthesized material. Meanwhile, the SEM images for the unmodified Ni foam and the hollow spheres-modified NiCo_2O_4 @Ni foam are shown in Fig. 2c and d, respectively. These figures show that the homogeneous NiCo_2O_4 hollow spheres were successfully synthesized covering the surface of the nickel foam. Further confirmation using EDX showed that the NiCo_2O_4 hollow spheres contain 7.92% (w/w) nickel, 16.98% cobalt, 64.37% oxygen, and 10.73% silicon. The nickel : cobalt ratio of 1 : 2 confirms the formation of NiCo_2O_4 . However, the presence of silicon indicated that the template could not be completely removed, which also explains the high oxygen percentage in the structure.

The structural information of the synthesized NiCo_2O_4 hollow spheres was confirmed by TEM characterisation of the precipitated NiCo_2O_4 particles of the remaining solution from the autoclave. Fig. 3 shows the TEM images of the NiCo_2O_4 particles on three different scales. An average diameter of

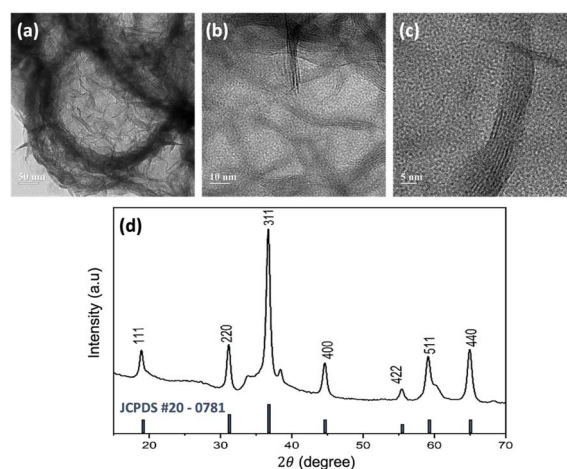


Fig. 3 (a–c) Typical TEM images of the NiCo_2O_4 hollow spheres in different magnifications, and (d) XRD spectra for the NiCo_2O_4 hollow spheres in comparison with the NiCo_2O_4 JCPDS card, shown as the black lines, as the reference.

around 270 nm for the NiCo_2O_4 hollow spheres was estimated using ImageJ software. Besides, a contrasting colour difference observed between the shells and the inner space confirmed the formation of the hollow structure. The figure also shows that the hollow spheres have multiple walls with thickness of around 5 nm (Fig. 3c).

Fig. 3d shows the XRD peak pattern of the synthesized NiCo_2O_4 hollow spheres. Diffraction peaks were observed at 2θ of 18.95° , 31.15° , 36.7° , 44.65° , 55.45° , 59.15° , and 64.95° , which were attributed to the characteristic peaks of the inverse cubic spinel phase of NiCo_2O_4 .³⁸ This result was confirmed with the JCPDS card no. #20-0781, as shown in the black lines in the figure. The inverse spinel structure of NiCo_2O_4 consists of two sites, tetrahedral and octahedral. Nickel is distributed at the octahedral site while cobalt is located at both the octahedral and tetrahedral sites. The multi-valency of cobalt makes the electrical conductivity of NiCo_2O_4 twice as high as those of the monometallic nickel oxide (NiO) or cobalt oxide (Co_3O_4), which further contributes to accessible electron transfer.³⁹

XPS characterisation was further conducted to determine the composition of the elements present on the surface of the electrodes. The XPS spectrum of the synthesized $\text{NiCo}_2\text{O}_4/\text{Ni}$ foam in Fig. 4a shows the main peaks of Ni, Co, and O. In addition, the peaks of C and Si are also observed as a result of the remaining template used in the synthesis of the $\text{NiCo}_2\text{O}_4/\text{Ni}$ foam. The deconvolution of the peak spectra of Ni 2p, Co 2p, and O 1s by using Gaussian fitting is shown in Fig. 4a–c, respectively. The characteristic peaks of Ni $2p_{1/2}$ and Ni $2p_{3/2}$ were detected at the binding energies of 856.28 eV and 873.88 eV, respectively (Fig. 4b). In addition, two shake-up satellites for Ni $2p_{1/2}$ and Ni $2p_{3/2}$ were also detected, resulting in a spin energy difference of 17.58 eV, confirming the formation of the nickel hydroxide phase.⁴⁰

Meanwhile, Fig. 4c shows the XPS spectra of Co 2p atoms with two peaks at binding energies of 781.52 and 798.06 eV, which characterise Co $2p_{3/2}$ and Co $2p_{1/2}$. Typical peaks of $\text{Co}^{2+} 2p_{3/2}$ and $\text{Co}^{2+} 2p_{1/2}$ are shown at the binding energies of

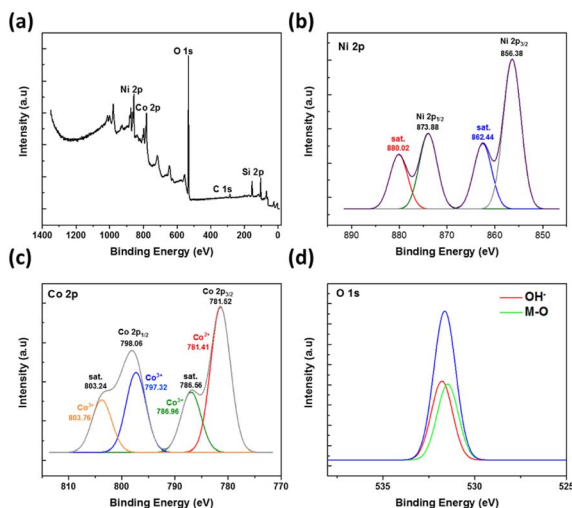


Fig. 4 (a) The XPS spectra of the synthesized $\text{NiCo}_2\text{O}_4/\text{Ni}$ foam together with (b–d, respectively) the related deconvolution peaks of Ni 2p, Co 2p, and O 1s.

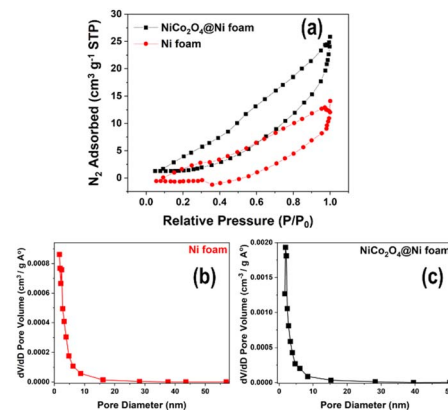


Fig. 5 (a) N_2 adsorption/desorption isotherms of the unmodified Ni foam and the $\text{NiCo}_2\text{O}_4/\text{Ni}$ foam; and (b and c) the pore size distributions of the unmodified Ni foam and the $\text{NiCo}_2\text{O}_4/\text{Ni}$ foam, respectively.

781.41 eV and 797.32 eV, while typical peaks of $\text{Co}^{3+} 2p_{3/2}$ and $\text{Co}^{3+} 2p_{1/2}$ are shown at the binding energies of 786.96 eV and 803.76 eV, respectively.⁹ These results confirmed the existence of multi-valence cobalt in the synthesized material.

In the case of the XPS O 1s spectra, two fitting peaks are shown at the binding energy of around 531.66 eV (Fig. 4d), deconvoluted to the metal–oxygen bond at the binding energy of 531.42 eV and the defects, impurities, and a range of surface species, including hydroxyls, chemisorbed oxygen, uncoordinated lattice oxygen, or species intrinsic to the surface of spinel, at the binding energy of 531.77 eV.⁹

The surface area of the unmodified Ni foam and the synthesized $\text{NiCo}_2\text{O}_4/\text{Ni}$ foam was examined by BET analysis. Fig. 5a depicts the N_2 adsorption/desorption isotherms and Barrett-Joyner-Halenda (BJH) pore-size-distribution plots (Fig. 5b and c) for the electrodes. The isotherms of the unmodified Ni foam and the $\text{NiCo}_2\text{O}_4/\text{Ni}$ foam sample can be categorized as typical type IV with an H_3 hysteresis loop, indicating the existence of a mesoporous structure in the materials.^{41–44} As shown in Fig. 5, Ni foam exhibits a surface area and a pore volume of $10.294 \text{ m}^2 \text{ g}^{-1}$ and $0.026 \text{ cm}^3 \text{ g}^{-1}$, respectively, while $\text{NiCo}_2\text{O}_4/\text{Ni}$ foam shows an increase in both the surface area and pore volume to $17.944 \text{ m}^2 \text{ g}^{-1}$ and $0.045 \text{ cm}^3 \text{ g}^{-1}$, respectively. Moreover, the pore size distribution, derived from desorption data and calculated from the BJH model (Fig. 5b and c), shows that the average pore radii of the Ni foam and the $\text{NiCo}_2\text{O}_4/\text{Ni}$ foam are 2.431 nm and 1.889 nm, respectively.

In comparison to the unmodified Ni foam, the synthesized $\text{NiCo}_2\text{O}_4/\text{Ni}$ foam has a greater surface area and pore volume, as well as smaller pore radius, which is believed to be advantageous for the diffusion of the electrolyte to the electrode's active sites and will improve its electrochemical performance for glucose sensing.

Electrochemical behaviour of glucose at the prepared $\text{NiCo}_2\text{O}_4/\text{Ni}$ foam

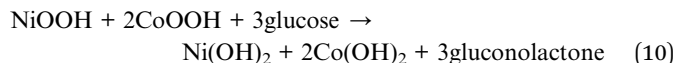
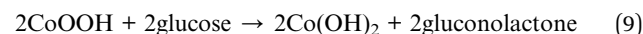
Cyclic voltammetry of a 1.0 M NaOH solution in the presence (solid line) and absence (dashed line) of glucose was performed



to study its electrochemical behaviour at the prepared $\text{NiCo}_2\text{O}_4\text{@Ni}$ foam (red line) compared to the unmodified Ni foam (black line) (Fig. 6a). The prepared $\text{NiCo}_2\text{O}_4\text{@Ni}$ foam shows a significantly higher current density compared to the unmodified Ni foam, both in the presence and absence of glucose, which is in line with the BET analysis results. Signal-to-background current (S/B) ratios of 0.10 and 0.28 were achieved for the unmodified Ni foam and the $\text{NiCo}_2\text{O}_4\text{@Ni}$ foam, respectively, which is nearly three times higher than the unmodified Ni foam.

Furthermore, chronoamperometry was conducted to validate the performance of the developed sensors (Fig. 6b), showing a similar trend of the current responses to the CV data. A significant increase of the glucose oxidation currents was observed when using the modified Ni foam. A signal-to-background current (S/B) ratio of 1.025 and 1.25 was achieved for the unmodified Ni foam and $\text{NiCo}_2\text{O}_4\text{@Ni}$ foam, respectively. The results confirmed that the higher surface area of the $\text{NiCo}_2\text{O}_4\text{@Ni}$ foam helps to enhance the number of catalytic active sites, which further increase its current density.

Anodic and cathodic peak couple at the potentials of +0.45 V and +0.1 V (vs. Ag/AgCl) were observed, respectively, corresponding to the binary intrinsic-state reduction-oxidation peak couples of $\text{Ni}^{3+}/\text{Ni}^{2+}$ and $\text{Co}^{3+}/\text{Co}^{2+}$ ions in NiCo_2O_4 .^{45,46} These peaks were overlapped to form larger shoulder peak due to the similar reduction-oxidation potentials of $\text{Ni}^{3+}/\text{Ni}^{2+}$ and $\text{Co}^{3+}/\text{Co}^{2+}$.⁴⁶ When glucose was present in the solution, a significant increase of the oxidation peak currents was observed. This result indicates that NiCo_2O_4 could be a promising catalyst for glucose electrooxidation, and hence could be an excellent glucose sensor. The possible mechanism of glucose oxidation by NiCo_2O_4 is through each intrinsic-state reduction-oxidation couple of $\text{Ni}^{3+}/\text{Ni}^{2+}$ and $\text{Co}^{3+}/\text{Co}^{2+}$ ions, as follows:^{46,47}



The influence of scan rate was studied to investigate the electron transfer kinetics and optimise the scan rate for glucose detection. Fig. 6b shows the cyclic voltammogram for $\text{NiCo}_2\text{O}_4\text{@Ni}$ foam in 1.0 M NaOH solution in the presence of glucose at 0.5 μM . A shift in the anodic peak to a more positive potential was observed, whereas the cathodic peak shifted to a more negative potential. This result indicates that a quasi-reversible electron transfer reaction occurs.⁴⁸ Plots of the square root of the scan rate *versus* the peak current (I_p) (Fig. 6c), showing a linear fit with the $R^2 = 0.999$, indicate that the electron transfer on the prepared electrode surface is a diffusion-controlled process.^{49,50} Furthermore, determination of the optimum scan rate is based on the largest signal-to-background ratio $[(S - B)/B]$, where S and B are the anodic peak currents in the presence and absence of glucose, respectively. Based on this calculation, the optimum scan rate of 25 mV s^{-1} was fixed and used for further experiments.

The performance of the prepared $\text{NiCo}_2\text{O}_4\text{@Ni}$ foam as the working electrode in the quantitative detection of glucose was then assessed. Fig. 7a reveals that the peak current increases proportionally with the concentration of glucose. The oxidation currents of glucose electrocatalysis by $\text{NiCo}_2\text{O}_4\text{@Ni}$ foam fell into a linear curve in the concentration range of 0 to 2.5 μM ($R^2 \geq 0.99$) with the linear equation of $y \text{ (mA)} = 0.0173[\text{glucose} \text{ (}\mu\text{M)}] - 0.0002$ (Fig. 2b). From the linear curve, the prepared electrode can provide sensitivity of 0.018 $\text{mA } \mu\text{M}^{-1}$.

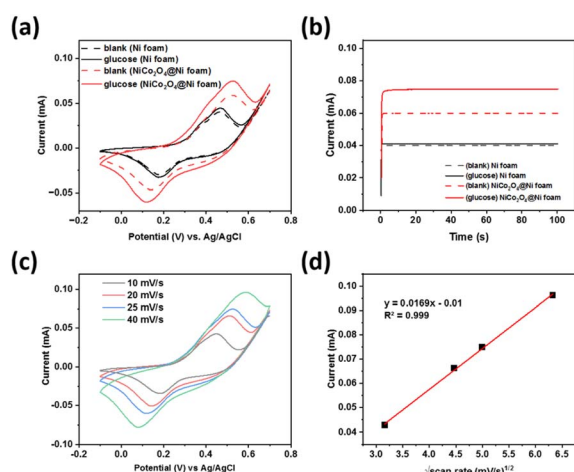


Fig. 6 (a) Cyclic voltammograms at a scan rate of 25 mV s^{-1} and (b) chronoamperograms with the prepared $\text{NiCo}_2\text{O}_4\text{@Ni}$ foam as the working electrode in comparison with the unmodified Ni foam in 1.0 M NaOH solution with and without the presence of 0.5 μM glucose. (c) Cyclic voltammograms for the prepared $\text{NiCo}_2\text{O}_4\text{@Ni}$ foam at various scan rates and (d) the related peak currents plots as a function of the square root of the scan rate.

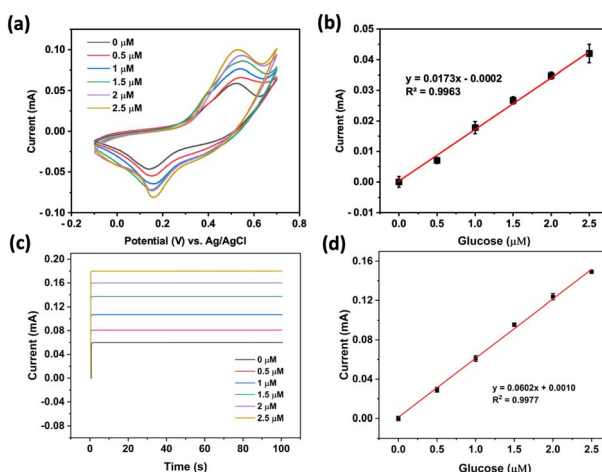


Fig. 7 (a and b) Cyclic voltammograms at a scan rate of 25 mV s^{-1} and the related calibration curve, respectively. (c and d) Chronoamperograms at +0.56 V (vs. Ag/AgCl) and the related calibration curve, respectively. The applied working electrode was $\text{NiCo}_2\text{O}_4\text{@Ni}$ foam and the electrolytes were various concentrations of glucose in 1.0 M NaOH.



Table 1 Comparison of the current work against other literature studies using various electrodes for the electrochemical detection of glucose

Electrode	Concentration range (μM)	LOD (μM)	Ref.
$\text{NiCo}_2\text{O}_4/\text{GCE}$	10–200	0.6	46
CuO/TiO_2	10–2000	0.39	51
CoWO_4	0–4500	0.7	52
c- $\text{Ni}(\text{OH})_2/\text{HR}$	2–3800	0.6	53
Cu_2O MSs/S–MWCNTs	4.95–7000	1.46	54
$\text{NiCo}_2\text{O}_4/\text{Ni foam}$	0.06–2.5	0.06	This work

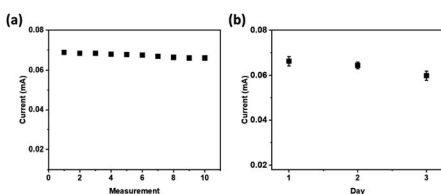
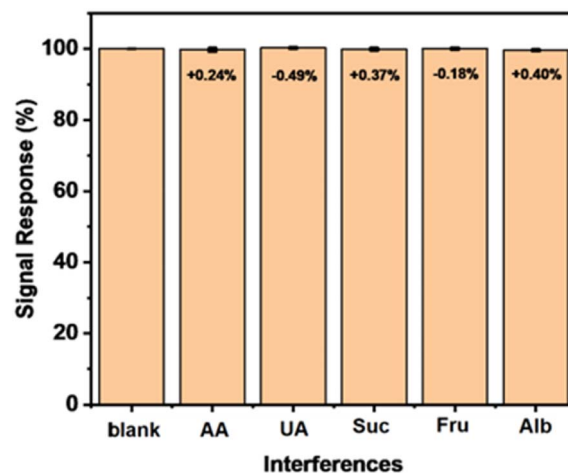
Furthermore, an estimated limit of detection (LOD) of $0.173 \mu\text{M}$ could be determined by employing the formula of $\text{LOD} = 3(S_y/S)$, where S_y represents the standard deviation of the response curve and S denotes the slope of the calibration curve.

Further investigation using chronoamperometry at an applied potential of $+0.56 \text{ V}$ (vs. Ag/AgCl) in the same concentration range as that using cyclic voltammetry also showed excellent linearity ($R^2 \geq 0.99$) with the linear equation of $y \text{ (mA)} = 0.0602[\text{glucose } (\mu\text{M})] - 0.0010$ (Fig. 2a and b). A sensitivity of $0.060 \text{ mA } \mu\text{M}^{-1}$ with an estimated LOD of $0.060 \mu\text{M}$ could be achieved.

The analytical performance of the developed sensor in comparison with other related glucose detection methods is displayed in Table 1, showing that the use of $\text{NiCo}_2\text{O}_4/\text{Ni foam}$ as the electrode for glucose sensing is favourable among the other reported sensors, with a lower limit of detection than the other electrodes.

A repeatability test was performed to evaluate the precision level of the developed sensor using the prepared electrode. The tests were conducted ten times with cyclic voltammetry technique using a solution of $0.5 \mu\text{M}$ glucose in 1.0 M NaOH. The developed sensor showed excellent repeatability of the current responses, as confirmed by the relative standard deviation (RSD) of 1.51% (Fig. 8a).

A stability test was carried out for 3 days at one-day intervals to study the stability of the prepared $\text{NiCo}_2\text{O}_4/\text{Ni foam}$ for glucose oxidation. Good stability of the current responses was obtained with a slight decrease of the current response of around 2.7% after the 3rd day. The results indicated that the hollow spheres of NiCo_2O_4 were stably attached on the surface of nickel foam, and therefore the prepared $\text{NiCo}_2\text{O}_4/\text{Ni foam}$ is promising for application in a real glucose sensor.

**Fig. 8** The current peaks of the voltammograms for $0.5 \mu\text{M}$ glucose in 1.0 M NaOH at $\text{NiCo}_2\text{O}_4/\text{Ni foam}$ (a) for ten consecutive measurements, and (b) on three different measurement days.**Fig. 9** Comparison of the signal responses for $0.5 \mu\text{M}$ glucose in 1.0 M NaOH at $\text{NiCo}_2\text{O}_4/\text{Ni foam}$ performed in the absence (blank) and in the presence of $0.25 \mu\text{M}$ ascorbic acid, uric acid, sucrose, fructose, and albumin. The error bars represent the standard deviations from three independent measurements.**Table 2** Comparison of glucose content obtained from the blood plasma sample measurements employing the developed method and the commercial glucose detector

Methods	Glucose (mg dL^{-1})
CV	173.28 ± 2
EasyTouch glucose detector	176

The selectivity of the developed sensor using the prepared $\text{NiCo}_2\text{O}_4/\text{Ni foam}$ electrode was investigated by performing an interference study in the presence of possible interferents, including ascorbic acid, uric acid, sucrose, fructose, and albumin. As displayed in Fig. 9, the addition of the compounds at concentrations up to 50 percent analyte did not significantly change the peak currents. The results suggest the high selectivity of the developed sensor towards glucose in the presence of ascorbic acid, uric acid, sucrose, fructose, and albumin.

The performance of the developed sensor was evaluated by measuring the glucose content in blood plasma sample obtained from the Faculty of Medicine, Universitas Indonesia, Jakarta, Indonesia. Ethical clearance was obtained from the Health Research Ethics Committee, Faculty of Medicine Universitas Indonesia No. 878//UN2.F1/ETIK/PPM.00.03/2020. The diluted blood plasma was electrochemically analysed under the optimised conditions. The current, obtained as an average of three measurements, yielded a value of 0.0664 mA (ESI S1†). Data processing was conducted using the equation derived from the linear calibration curve, indicating a glucose content of $173.28 \text{ mg dL}^{-1}$ in the blood plasma sample (ESI S2†). The electrochemical measurement results were subsequently validated using a glucose detector (EasyTouch GCU), confirming a glucose level of 176 mg dL^{-1} in the blood plasma sample (ESI S3†). This validates that the detection result using the $\text{NiCo}_2\text{O}_4/\text{Ni foam}$ electrode is comparable to the result obtained



from the glucose detector. Thus, the prepared NiCo₂O₄@Ni foam electrode demonstrates promising potential as a detection tool (Table 2).

Conclusions

Multiwalled hollow spheres of NiCo₂O₄ were successfully attached on the inner surface of nickel foam with a hydrothermal method with an estimated sphere size of 270 nm. The NiCo₂O₄ contains 7.92% (w/w) nickel, 16.98% cobalt, 64.37% oxygen, and 10.73% silicon. The nickel-to-cobalt ratio of 1 : 2 confirms the formation of NiCo₂O₄, whereas the observed silicon indicates that the template could not be completely removed, which also explains the high oxygen percentage in the structure. Investigation of the modified nickel foam for non-enzymatic-based electrochemical detection of glucose provided a linear calibration curve in the glucose concentration range from 0 to 2.5 μM . A detection limit of 0.060 μM with a sensitivity of 0.060 mA μM^{-1} could be achieved with excellent repeatability, stability, and selectivity towards glucose in the presence of ascorbic acid, uric acid, sucrose, fructose, and albumin. Furthermore, the developed sensor was effectively utilized for the detection of glucose in a blood plasma sample.

Author contributions

N. E.: data curation, formal analysis, investigation, and writing; T. A. H. P.: data curation, formal analysis, and investigation; A. R. S.: data curation, formal analysis, and investigation; R. K. P.: data curation, formal analysis, and investigation; Y. M. T. A. P.: electrochemical investigation, and writing-review and editing; I. R.: investigation, and writing-review and editing; Y. K. K.: material preparation supervision, validation, and writing-review and editing; H. C.: conceptualization, supervision, and validation; T. A. I.: conceptualization, supervision, validation, funding acquisition, and writing-review and editing. All authors have given approval to the final version of the manuscript.

Conflicts of interest

There are no conflicts to declare.

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